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Effects of pentobarbital on upper airway patency during sleep

M. Eikermann^{*,#,¶}, D.J. Eckert^{#,+}, N.L. Chamberlin^{#,§}, A.S. Jordan^{#,+}, S. Zaremba^{#,§}, S. Smith^{#,+}, C. Rosow^{*,#}, and A. Malhotra^{#,+}

^{*}Dept of Anesthesia, Massachusetts General Hospital, Beth Israel Deaconess Medical Center, Boston, MA, USA.

[#]Harvard Medical School, Beth Israel Deaconess Medical Center, Boston, MA, USA.

⁺Divisions of Sleep Medicine and Pulmonary/Critical Care, Brigham and Women's Hospital, Beth Israel Deaconess Medical Center, Boston, MA, USA.

[§]Dept of Neurology, Beth Israel Deaconess Medical Center, Boston, MA, USA.

[¶]Universitätsklinikum Essen, Klinik fuer Anästhesie und Intensivmedizin, Essen, Germany.

Abstract

We hypothesised that pentobarbital would improve upper airway mechanics based on an increase in latency to arousal and amplitude of the phasic genioglossus electromyogram (EMG), and a decrease in the active upper airway critical closing pressure (P_{crit}).

12 healthy subjects received pentobarbital (100 mg) or placebo in a double-blind, crossover protocol. During wakefulness, we measured the genioglossus reflex response to negative pressure pulses. During sleep, carbon dioxide was insufflated into the inspired air. Airway pressure was then decreased in a stepwise fashion until arousal from sleep.

With basal breathing during sleep: flow rate was lower in volunteers given pentobarbital; end-tidal CO_2 concentration and upper airway resistance were greater; and P_{crit} was unaffected (pentobarbital mean \pm_{sD} -11.7 \pm 4.5 *versus* placebo -10.25 \pm 3.6 cmH₂O; p=0.11). Pentobarbital increased the time to arousal (297 \pm 63s *versus* 232 \pm 67 s; p<0.05), at which time phasic genioglossus EMG was higher (6.2 \pm 4.8% maximal *versus* 3.1 \pm 3%; p<0.05) as were CO₂ levels. The increase in genioglossus EMG after CO₂ administration was greater after pentobarbital *versus* placebo. Pentobarbital did not affect the genioglossus negative-pressure reflex.

Pentobarbital increases the time to arousal and stimulates genioglossus muscle activity, but it also increases upper airway resistance during sleep.

Keywords

Airway; arousal threshold; lung; obstructive sleep apnoea/hypopnoea syndrome; sleep-disordered breathing

Obstructive sleep apnoea (OSA) is a common disorder [1], characterised by repetitive pharyngeal collapse during sleep [2]. Arousal from sleep is traditionally believed to be an

STATEMENT OF INTEREST

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CORRESPONDENCE M. Eikermann Dept of Anesthesia and Critical Care Massachusetts General Hospital 55 Fruit St Boston, MA 02114-2696 USA meikermann@partners.org.

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important mechanism for reestablishing airway patency in OSA. However, recent data suggest that an excessively low arousal threshold may predispose an individual to recurrent arousals, and the hyperventilation that occurs following arousal may produce hypocapnia during subsequent sleep [3].

Reduced carbon dioxide values may lead to either central or obstructive apnoea, depending on the prevailing upper airway mechanics [4, 5]. Thus, a low arousal threshold may contribute to sleep apnoea, at least in some individuals [3, 6, 7]. Premature arousal during an obstructive event may prevent adequate upper airway muscle recruitment because there is inadequate accumulation of respiratory stimuli (i.e. CO2 and negative intrapharyngeal pressure). Recent data suggest that treatment with certain hypnotics may not be deleterious and may even improve this condition in certain patients [8–11]. A number of medications have been demonstrated to raise the arousal threshold, and recent data suggest that treatment with some hypnotics and antidepressants may improve OSA manifestations [8-11]. Triazolam and ethanol have been shown to increase the arousal threshold in response to airway occlusion in normal subjects [12, 13], and the antidepressants mirtazipine and trazodone may improve manifestations of sleep apnoea [8]. It has been shown that trazodone co-administered with L-tryptophan can treat sleep-disordered breathing in an animal model of OSA [14]. In humans, trazodone may improve airway mechanics by raising the arousal threshold [10] and potentially allowing both negative airway pressure and CO₂ to increase, thereby activating pharyngeal dilator muscles. The upper airway dilator muscles (e.g. genioglossus) are known to respond during sleep to combinations of negative pressure and hypercapnia better than to either stimulus alone [15].

Recent data show that pentobarbital can increase genioglossus phasic activity in the rat [11, 16]. However, pentobarbital also produces some less desirable effects on airway physiology in the rat: it causes a dose-dependent reduction in both diaphragmatic activity and tonic (expiratory) genioglossus activity [16]. Large doses of pentobarbital can also impair the genioglossus negative-pressure reflex (*i.e.* reflex activation in response to a sudden decrease in pressure) [16], which may adversely affect upper airway patency.

Based on preclinical data, we hypothesised that pentobarbital would delay arousal in human subjects following a standardised negative-pressure stimulus and that this delay would augment genioglossus muscle activity and improve upper airway closing pressure. To test these hypotheses, we performed a randomised, double-blind, placebo-controlled, crossover study comparing 100 mg pentobarbital to placebo.

MATERIALS AND METHODS

The protocol was approved by the Institutional Review Board of Brigham and Women's Hospital (Boston, MA, USA). 12 healthy adult volunteers (ages 18–48 yrs; body mass index $<25 \text{ kg} \cdot \text{m}^{-2}$) were recruited to participate in the study. We excluded people with concurrent cardiopulmonary disease, including untreated hypertension, kidney disease, liver disease, neuromuscular disease, sleep disorders and psychiatric disease. We also excluded those taking medication known to affect sleep, upper airway muscles or respiratory function (*e.g.* oral contraceptives, hormone replacement therapy, theophylline, acetazolamide, stimulants, sedatives, thyroxine and antidepressants). Finally, we excluded those with a history of lidocaine or barbiturate allergy, or acute intermittent porphyria. Subjects were recruited through posted flyers, e-mail and newspaper advertisements.

Protocol

Subjects were studied twice, once with pentobarbital 100 mg (diluted in cherry syrup) and once with placebo treatment (cherry syrup alone) in a randomised, double-blind fashion, with 10 days between treatments (fig. 1).

On study days, subjects were admitted into our Clinical Research Center (Beth Israel Deaconess Medical Center, Boston, MA, USA) at approximately ~20:00 h. Pre-menopausal females underwent a urinary pregnancy test prior to medication administration. After the study procedures were explained, adhesive surface electrodes were attached to the scalp (electroencephalogram (EEG)), face (electrooculogram), and chin (electromyogram (EMG)). Following this, both nostrils were decongested (oxymetazoline HCl), and one nostril and the back of the throat were anaesthetised with ~0.5 mL of topical 4% lidocaine (20–40 mg). Airway pressure was monitored at the level of the epiglottic (epiglottic pressure) using a pressure-tipped Millar catheter that was inserted through the anaesthetised nostril and secured with tape. Three surface electrocardiogram electrodes were placed on the chest and shoulders.

The area under the tongue (3–4 mm lateral to the frenulum on each side) was topically anaesthetised with lidocaine for insertion of genioglossus muscle electrodes. Two needles (25-gauge) containing 30-gauge stainless steel recording electrodes were inserted into the genioglossus muscle. The needles were then quickly removed leaving the recording electrodes in place. Recordings were bipolar with a forehead ground. The subject was instructed to perform several manoeuvres to determine maximal activity of the genioglossus muscle (maximal tongue protrusion, swallowing, negative inspiratory force).

A nasal continuous positive airway pressure (CPAP) mask placed over the subject's nose and held in place with a head strap permitted measurement of breathing rate, inspired volume (integrated inspiratory flow signal from a pneumotachograph), mask pressure and CO_2 levels. An arterial oxygen saturation probe was attached to one of the subject's fingers or earlobes to monitor oxygenation.

Before and 60 min after administration of the study drug, baseline data were collected during a 10-min period of normal breathing while the subject was awake (fig. 1). In addition, ~40 brief pulses of negative airway pressure (200 ms) were delivered during early inspiration every two to eight breaths to measure the genioglossus negative pressure reflex as described previously [17, 18].

Subjects were then allowed to fall asleep while breathing room air at atmospheric pressure. When breathing was stable for a period of 5 min, the respiratory response to CO_2 was assessed. Sufficient CO_2 (10% balanced with nitrogen) was added to the inspired air to produce stable elevations of end-tidal CO_2 that were first 5, then 10 mmHg higher than baseline.

Subjects were then awoken and placed on $3 \text{ cmH}_2\text{O}$ CPAP. Once they had reached stable nonrapid eye movement sleep again, we increased the CPAP level to alleviate any degree of flow limitation. When steady state stage-II sleep without flow limitation was achieved, we reduced airway opening pressure in 2-cmH₂O steps, and subjects were monitored for arousal (*i.e.* presence of α wave activity on the EEG). If the subject did not have an arousal for 1 min we proceeded to the next step. Continuous negative airway pressure was used if subatmospheric pressures were required. This titration procedure (hereafter called a negative pressure ramp) was repeated up to a maximum of 15 times throughout the night. Following data collection, all equipment was removed and the subjects were allowed to recover in the General Clinical Research Center for 8 h after drug ingestion and until they felt alert

enough to go home. Discharge readiness was confirmed by a licensed physician who was not involved in the study.

Data analysis

A single experienced, registered sleep technician, blinded to the experimental manipulations, defined the presence of arousal and sleep stage according to standard criteria [19]. For analysis of arousability, we have only included data in the analysis that occurred >30 s after onset of a pressure reduction.

The effect of pentobarbital and placebo on the excitation component of the genioglossus negative pressure reflex was compared within subjects pre *versus* post administration according to methods that have been previously described [17, 18]. Analysis was performed blinded to the study condition. Briefly, the genioglossus (GG)-EMG signal was rectified and averaged for all negative pressure pulses that were free from movement and swallow artefact. The amplitude of the initial GG-EMG peak was expressed as a percentage of the baseline activity. Reflex latency was defined as the time to peak GG-EMG from time zero (the last point preceding the sudden decrement in the ensemble-averaged pressure signal).

Wakefulness, phasic and tonic GG-EMG, airflow, upper airway resistance and end-tidal CO₂ were measured during quiet breathing before and 60 min after study drug. Maximal genioglossus activation manoeuvres allowed an EMG scale to be created for each subject between electrical 0 and the single highest value encountered (100%) [20]. During sleep, GG-EMG just prior to arousal was calculated by averaging the value during three breaths immediately before arousal.

A standardised protocol for assessing the active P_{crit} was implemented as previously described (fig. 2) [21]. When inspiratory flow limitation was stable, nasal pressure and maximum inspiratory flow were obtained from three breaths at the end of a 2-min period of stable stage 2 sleep. Flow limitation was defined as: unchanged inspiratory flow despite a further decrease in pharyngeal (epiglottic) pressure. Mask pressure was then plotted *versus* maximum flow for the flow limited breaths and fitted using a linear regression model.

Time to arousal was defined as the time from onset of the negative pressure ramp to an arousal as detected by EEG α -wave activity.

Upper airway resistance (epiglottic catheter to mask) was measured at a flow of $0.2 \text{ L} \cdot \text{s}^{-1}$, which is generally on the linear portion of the pressure/flow curve.

Statistical analysis

The primary dependent variable was time to arousal. We also tested the hypothesis that time to arousal is significantly longer in subjects following pentobarbital 100 mg compared with placebo. We tested the secondary hypothesis that phasic GG-EMG just prior to arousal would be significantly higher in volunteers given pentobarbital compared with placebo. Finally, we tested the exploratory hypothesis that active upper airway closing pressure would be lower (more negative) in volunteers given pentobarbital *versus* placebo.

Based on the observations of BERRY and co-workers [12, 13] who observed a longer time to arousal from sleep in volunteers given alcohol and triazolam, we anticipated a 30% difference and a sD of 10%. Based on the data of YOUNES *et al.* [11], who observed a higher phasic genioglossus activity at the time of arousal in rats given pentobarbital compared with placebo, we expected a 50% difference between groups in phasic genioglossus activity (SD 10%). Finally, based on the association of phasic genioglossus activity and upper airway closing pressure in humans, we expected a 10% difference (SD 10%) in *P*_{crit} between groups

[22]. We calculated that a total sample size of 10 volunteers would provide sufficient power to detect a significant difference in the primary and secondary hypotheses (power=0.8, α <0.05). Paired t-tests were used for testing the main hypotheses. We used a general linear model (mixed model) to analyse the GG-EMG response to CO₂. We used GG-EMG as the dependent variable and drug (pentobarbital *versus* placebo), respiratory phase (phasic *versus* tonic), and CO₂ level (baseline, +5 mmHg and +10 mmHg) as independent variables.

The results are expressed as the mean \pm_{sD} , unless otherwise indicated. SPSS Version 11.0 and Sigma Stat Version 3.0 (both SPSS, Inc., Chicago, IL, USA) were used for statistical analysis.

RESULTS

One volunteer was excluded during the first study night due to inability to sleep, leaving data from 11 volunteers (three males and eight females) aged 35 ± 10 yrs (height 173 ± 8 cm, weight 67 ± 8 kg) for analysis.

Effects of pentobarbital during wakefulness

During wakefulness, pentobarbital did not affect breathing or genioglossus muscle function. There was no significant difference in minute ventilation, tidal volume (V_T), end-tidal CO₂, duty cycle (time taken for inspiration (t)/total time of respiratory cycle (t_{tot})), flow-rate (V_T /t), phasic and tonic GG-EMG (table 1).

Negative pressure reflex activation of the GG-EMG was robust with pentobarbital and placebo (more than two-fold increase, table 2). Amplitude and latency of the genioglossus reflex activation did not differ before and after pentobarbital administration. Similarly, reflex properties did not differ before *versus* after placebo.

Effects of pentobarbital during sleep

Respiratory function during normal breathing—During normal stage II sleep (atmospheric mask pressure), flow rate was significantly lower in volunteers given pentobarbital, while end-tidal CO₂ concentration, and upper airway resistance were significantly greater compared with both baseline (same study day) and placebo. Duty cycle was significantly greater after pentobarbital compared with baseline (table 2). $V_{\rm T}$ and respiratory frequency did not differ between treatments.

Responses to pressure drops

<u>**Time to respiratory-induced arousal from stage II sleep:**</u> For each subject, we decreased CPAP an average of 10 ± 3 times during stage II sleep. Onset of flow limitation occurred at -3.6 ± 2.5 versus -3.4 ± 3.2 cmH₂O in the placebo and pentobarbital night, respectively, without differences between groups (p=0.8).

There was no difference in the number of pressure drops prior to arousal between placebo and pentobarbital trials. However, arousal from stable stage II sleep occurred significantly later with pentobarbital ($297\pm63 \ versus 232\pm67 \ s$ after stimulus; p<0.05), and mask pressure was therefore lower (-2.9±3.2 versus -0.5±2.3 cmH₂O; p<0.05).

<u>Genioglossus function and upper airway pressure flow relationship just prior to</u> <u>arousal from sleep:</u> Phasic genioglossus activity during flow-limited breathing just prior to arousal was significantly higher after pentobarbital compared with placebo (fig. 3). End-tidal CO₂ concentration (first breath after termination of pressure drop) was modestly but significantly higher, with pentobarbital *versus* placebo (45.6 ± 4.6 *versus* 42 ± 1.1 mmHg; p<0.05).

The range of mask pressure values used for assessment of P_{crit} was 1–-17 cmH₂O. The change in P_{crit} (pentobarbital -1.7±4.5 *versus* placebo -10.25±3.6 cmH₂O; p=0.11; fig. 4) and the increase in tonic genioglossus activity with pentobarbital compared with placebo did not reach statistical significance (p=0.082). In assessing whether genioglossus activation was mechanically effective, we found that the rise in tonic (but not phasic) GG-EMG was predictive of the improvement in airway mechanics (*i.e.* active P_{crit}) (r= -0.66; p=0.03; fig. 5).

Genioglossus function and peak airflow measured at the same time after starting the <u>negative pressure ramp as at the placebo night</u>. We analysed genioglossus activity and peak airflow at a standardised time $(260\pm100 \text{ s} \text{ after onset of negative pressure drop})$, defined as the lowest level of mask pressure (at $-5.45\pm2.78 \text{ cmH}_2\text{O}$) that we were able to apply under both placebo and pentobarbital conditions. Both flow-limited and no flow-limited breaths were included in this analysis. Phasic genioglossus activity was significantly higher $(3.9\pm6.6\% \text{ versus } 1.3\pm1.96\%$ of maximum activation; p=0.08), but tonic genioglossus activity ($0.68\pm1.2\% \text{ versus } 0.49\pm0.85\%$ of maximum; p=0.3) and peak inspiratory airflow ($0.33\pm0.1 \text{ versus } 0.3\pm0.13 \text{ L}\cdot\text{s}^{-1}$; p50.17) did not differ between groups.

Upstream resistance (mask pressure (P_{mask})/peak airflow (V_{max})) taken at the same time tended to be lower under pentobarbital (19±14 cmH₂O·L⁻¹·s) compared with placebo (24±19 cmH₂O·L⁻¹·s (p=0.066).

Respiratory response to CO_2—In one pentobarbital trial, and in two placebo trials, awakening from sleep was observed before steady state hypercapnic stimulation could be achieved. Measurements of the respiratory response to CO_2 are therefore reported from nine volunteers.

Increased inspired CO₂ augmented the GG-EMG, and the amplitude of this effect was significantly dependent on drug (pentobarbital>placebo) and state (phasic>tonic; table 3). Administration of CO₂ significantly increased upper airway resistance by $145\pm18\%$ (placebo) and $147\pm17\%$ (pentobarbital). Flow rate measured at an end-tidal CO₂ 10 mmHg above baseline was not significantly different between groups ($198\pm76\%$ of baseline for placebo *versus* $196\pm68\%$ for pentobarbital).

DISCUSSION

Our study found that in healthy volunteers, pentobarbital (100 mg orally) had no effect on respiratory function during wakefulness and did not impair genioglossus muscle function during the awake or sleep states. During stage II sleep, pentobarbital had a mild respiratory depressant effect, manifested as a decrease in peak inspiratory flow, and a rise in end-tidal CO_2 and upper airway resistance. However, the hypercapnic responsiveness of the genioglossus muscle improved. Active P_{crit} did not significantly change following pentobarbital. However, lower Pcrit values were associated with increased tonic GG-EMG, suggesting clinical relevance of the observed muscle recruitment, *i.e.* that it was mechanically effective. These results confirm and extend those of YOUNES *et al.* [11] as well as our own preclinical studies in rats [16].

An interesting finding of our study is that in humans, pentobarbital increased time to arousal and genioglossus activation preceding arousal. This particular constellation of effects could be useful for OSA patients with low arousal thresholds, ventilatory control instability, or

both. YOUNES *et al.* [3] as well as WELLMAN *et al.* [23] have suggested that ventilatory control instability can contribute to the pathogenesis of OSA. Concomitant increases in phasic genioglossus activity and time to arousal should help stabilise breathing patterns by allowing the necessary physiological responses to obstructive events to stabilise the airway, without producing arousals and subsequent ventilatory overshoot that cause ventilatory oscillation in susceptible patients. In support of this idea, <u>Younes *et al.*</u> [24] observed that even patients with severe sleep apnoea have some periods of stable breathing, and we have recently observed that these stable breathing periods are associated with high levels of upper airway dilator muscle activity [25], suggesting that these muscles are necessary and sufficient to protect pharyngeal patency when adequate respiratory stimulation is present for sufficient duration. However, delaying arousal is theoretically deleterious for patients with a high

In our study, upper airway closing pressure was stable at 100 mg pentobarbital, a dose that promotes sleep in humans [26, 27], without affecting normal breathing or the ventilatory response to CO_2 [28]. However, pentobarbital increased upper airway resistance during sleep, leading to decreased peak inspiratory flow rate and mild hypercapnia. In theory, an elevated upper airway resistance may actually be beneficial in those with unstable ventilatory control [29], if the accumulation of respiratory stimuli allows important recruitment of upper airway muscle activity [15, 30].

arousal threshold in whom substantial hypoxaemia and hypercapnia could develop.

Interestingly, respiratory depression may contribute to upper airway-stabilising effects of pentobarbital. We previously observed a dissociation of pentobarbital's respiratory effects on the genioglossus activation and breathing (inhibition of diaphragmatic activity and consequent hypercapnia) of rats [16]. We therefore speculate that hypercapnia plays a role in mediating pentobarbital's activating effects on the genioglossus, which we observed at the time of arousal [31, 32]. To the extent that chemoreflex activation of the genioglossus muscle may occur independently of ventilatory drive, it is possible that elevated CO_2 may partially account for the increase in genioglossus activity observed in parallel with decreased ventilatory drive [31]. Another possibility is that, when negative effort dependence is present, flow may actually improve with reduced ventilatory drive. However, pentobarbital's narrow therapeutic index makes pentobarbital a problematic candidate agent for use as a treatment for OSA. Further work is required to determine whether a pharmacological approach to sleep apnoea therapy is viable using either different agents or by carefully selecting patients for treatment.

An increase in genioglossus activity, as has been observed in our volunteers during the pentobarbital night prior to arousal from sleep, does not necessarily translate to mechanical improvement. Recently we have observed that pharmacologically evoked genioglossus muscle weakness (partial neuromuscular transmission block) explains only 20% of the variance of the evoked increase in upper airway closing pressure [33]. Moreover, OSA patients may even have significantly greater basal genioglossal activity compared to controls during wakefulness [20]. Other nonmuscular factors, such as decreases in lung volume [34–36], and fluid displacement into nuchal and peripharyngeal soft tissues [37], could contribute to narrowing and increased airflow resistance of the pharynx, and predispose to pharyngeal collapse in humans.

In the present study, upper airway resistance increased during sleep, and the magnitude of the effect was higher when pentobarbital was given. The respiratory duty cycle was significantly increased by pentobarbital, suggesting that higher resistance was partially offset by an increase in inspiratory time. Our data cannot explain why upper airway resistance during normal breathing was increased, while genioglossal mechano- and chemoresponses were normal or even augmented. Upper airway resistance is influenced by a

variety of mechanisms including airflow pattern, mandibular and body position, respiratory timing, as well as end-expiratory lung volume. We speculate that pentobarbital's deleterious effects on upper airway resistance might in part be explained by its reduction of lung volume. In pentobarbital-anaesthetised dogs, phasic electrical activity increases over time in the expiratory muscles, whereas electrical activity of the inspiratory muscles is unchanged [38], which might decrease end-expiratory lung volume.

In our study, the pentobarbital-induced change in tonic but not phasic genioglossus activity correlated with improved P_{crit} values. Tonic upper airway muscle activity is critical for maintenance of airway patency [39]. The impact of tonic genioglossus activity on airway patency in OSA patients has been emphasised in a recent study reported from our laboratory [40]. In OSA, reductions in tonic genioglossus activity during rapid eye movement are associated with hypopnoea events and therefore have been suggested to contribute to the higher severity of OSA in that stage [40]. In addition, our recent research in single motor units in the genioglossus has highlighted the importance of tonic motor neurons in affecting overall genioglossal activity and airway mechanics [41]. Ostensibly, the genioglossus phasic activity may be more mechanically effective when influencing a stiffened airway.

Limitations

We made a comparison between pentobarbital and placebo. Accordingly, our data cannot address whether the observed effects are specific to pentobarbital or a class effect of barbiturates or even γ -aminobutyric acid A agonists.

The increases in GG-EMG at the end of the negative pressure ramp may be secondary to the prolonged latency to arousal (with lower mask and pharyngeal pressures and an increase in CO_2) and increased resistance, but may also include a specific barbiturate stimulatory effect. The greater increase in the genioglossus response to evoked hypercapnia during the pentobarbital compared with placebo may provide some evidence for a primary stimulatory effect of the barbiturate on genioglossus EMG. Moreover, genioglossus activity measured at a standardized time after onset of a pressure ramp, revealed higher values of phasic genioglossus activity during the pentobarbital compared with placebo, suggesting that barbiturates may have some stimulatory effects on genioglossus muscle.

At the end of the pressure ramps, the volunteers showed considerable flow-limited breathing (even at a fixed flow of $0.2 \text{ L} \cdot \text{s}^{-1}$), which complicates resistance determinations. As the pharyngeal tissues collapse, the epiglottic pressure is no longer the downstream pressure, and thus airflow resistance is not simply a function of the pressure drop from the mask to the epiglottic catheter. While we have included peak-flow during the ramps, we do not know an ideal way of reporting the resistance at the end of the pressure ramps during flow limitation.

We believe more OSA research should address arousability, a variable that is associated with sleepiness and may have therapeutic implications [42]. We assessed arousability by the arousal response time during step reduction of the airway pressures. During OSA, arousal could be caused by various factors, such as hypercapnia, hypoxaemia, intrathoracic pressure, and by interaction among these. The arousal response examined in this study is one aspect of the responses in normal subjects and may not reflect arousability during OSA.

In summary, in healthy volunteers given pentobarbital, time to arousal and phasic genioglossus activity immediately prior to arousal were increased and genioglossus reflex activation was maintained. However, pentobarbital increased upper airway resistance during sleep leading to decreased peak flow and mild hypercapnia while active upper airway closing pressure was stable. These findings make it difficult to predict whether or not manipulating arousal threshold with pentobarbital may be a viable therapeutic strategy for

subsets of sleep apnoea patients. Its narrow therapeutic index makes pentobarbital a problematic candidate agent. Further work will be required to determine whether a pharmacological approach to sleep apnoea therapy is viable using either different agents or by carefully selecting patients for treatment.

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FIGURE 1.

Study protocol. Subjects were studied twice: during placebo and during pentobarbital treatment. Each study day, measurements were performed during wakefulness (before and after test-drug application) and sleep. During sleep, subjects were studied at atmospheric pressure first, to measure normal breathing and the respiratory response to inspiratory carbon dioxide insufflation. Subjects were then put on continuous positive airway pressure (CPAP) (3 mmHg) to avoid flow limitation, and negative-pressure ramps were performed until arousal. GG-EMG: genioglossus electromyography; *P*_{crit}: critical closing pressure.

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FIGURE 2.

Method of calculation of upper airway critical closing pressure (P_{CRTT}) during stage II sleep by linear regression in one volunteer. Peak air flow during flow-limited breathing is plotted as a function of mask pressure. Throughout the study night, 12 negative-pressure ramps were performed, while flow limitation was observed. Values derived from 31 flow-limited breaths were used for analysis and extrapolated to P_{CRTT} (mask pressure at zero flow) by linear regression. Note that, at a given mask pressure, peak flow during flow-limited breathing varied throughout the overnight study, suggesting that the balance between the collapsing and dilating forces acting at the upper airway varied throughout the night. Eikermann et al.



FIGURE 3.

Effect of pentobarbital () and placebo () on genioglossus activity during negative pharyngeal pressure challenges. Average values of genioglossus (GG) electromyogram (EMG) just prior to arousal are shown. Phasic genioglossus activity was significantly higher after pentobarbital (100 mg) compared with the control night, and tonic genioglossus activity tended to be higher. % max: % maximal. *: p<0.05 *versus* placebo; [#]: p<0.1 *versus* placebo.



FIGURE 4.

Effect of pentobarbital on active upper airway critical closing pressure (P_{CRIT}) during sleep. The figure shows the average P_{CRIT} values in 11 subjects during the pentobarbital night compared with the placebo night. Vertical bars represent mean±sp. Note that P_{CRIT} tended to be more negative during the pentobarbital night compared with the placebo night. #: p=0.11 *versus* placebo.

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FIGURE 5.

Difference in active upper airway critical closing pressure (P_{CRIT}) during the pentobarbital night and control night *versus* the difference in tonic genioglossus activity (as % of maximum (max) value). Measurements during negative pharyngeal pressure challenges during sleep. Average values from all pressure drops. r= -0.66, p=0.03.

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TABLE 1

		Wakefulnes	s		Slee	
	Before test drug applic	cation (baseline)	After test drug	application	During stage	e II sleep
	Pentobarbital	Placebo	Pentobarbital	Placebo	Pentobarbital	Placebo
Upper airway resistance CMH ₂ O·L ⁻¹ ·s	2.9 ± 4.4	2.3 ± 3.4	5.2 ± 4.8	1.6 ± 0.9	$7.1\pm8.3^{*,+}$	2.5 ± 2.6
End-tidal CO ₂ mmHg	41.6 ± 2.7	40.1 ± 2.6	42.4 ± 3.2	40.9 ± 1.9	44.5 ± 3.4 *,+	42.3 ± 2.3
$V_{ m E}{ m L}\cdot{ m min}^{-1}$	6.8 ± 1.9	6.9 ± 1.2	7.0 ± 1.5	6.8 ± 1.5	6.6 ± 1.7	6.4 ± 1.1
$V_{ m T}$ L min ⁻¹	0.40 ± 0.15	0.37 ± 0.06	0.37 ± 0.09	0.38 ± 0.07	0.42 ± 0.15	0.40 ± 0.11
Duty cycle [#]	0.43 ± 0.03	0.41 ± 0.03	0.46 ± 0.06	0.43 ± 0.09	$0.47\pm0.07^+$	0.44 ± 0.09
Flow rate ¶ mL·s ⁻¹	0.36 ± 0.29	0.3 ± 0.29	0.34 ± 0.19	0.29 ± 0.04	$0.23\pm0.06^{\$}$	0.29 ± 0.07
Phasic GG-EMG activity % max	1.9 ± 2.4	2.1 ± 4.9	2.2 ± 2.9	1.9 ± 1.9	4.6 ± 7.9	2.1 ± 4.9
Tonic GG-EMG activity % max	1.2 ± 2.6	0.7 ± 2.2	1.5 ± 4.0	0.8 ± 3.8	2.4 ± 6.3	0.64 ± 2.2
Peak GG-EMG activity % max	3.1 ± 4.8	2.7 ± 5.9	3.6 ± 6.7	2.7 ± 5.1	6.1 ± 11.6	2.7 ± 5.9
Data are presented as mean \pm sd. <i>V</i> E: minut	te ventilation; VT: tidal vo	olume; GG-EMG: ¿	genioglossus elect	romyogram.		

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measured as time taken for inspiration (η)/total time of respiratory cycle

 $_{\rm p<0.05}^{*}$ versus place bo treatment, sleep values

 $^+$ p<0.05 versus baseline, same study day

 $\$_{p<0.1}$ versus place bo treatment, sleep values.

TABLE 2

Negative pressure pulse data collected during wakefulness

Pressure reflex and stimulus characteristics	Pre-pentobarbital	Post-pentobarbital	Pre-placebo	Post-placebo
Excitation onset latency ms	27 ± 5	28 ± 3	26 ± 5	21 ± 2
Excitation peak amplitude % baseline	224 ± 30	227 ± 34	236 ± 34	242 ± 28
Excitation peak latency ms	36 ± 4	38 ± 3	42 ± 8	34 ± 4
Minimum mask pressure cmH ₂ O	$\text{-16}\pm2$	-17 ± 2	-19 ± 2	-17 ± 1
Number of artefact-free pulse presentations	39 ± 3	35 ± 3	41 ± 2	34 ± 3

Data are presented as mean \pm sem. There were no significant differences between conditions for genioglossus reflex characteristics or stimulus magnitudes. n=10.

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	Room	air	P _{ET} , co ₂ 5 mmHg a	bove baseline	PET, CO2 10 mmHg	above baseline
	Pentobarbital	Placebo	Pentobarbital	Placebo	Pentobarbital	Placebo
Upper airway resistance cmH ₂ O·L ⁻¹ ·s	$6.4\pm8.5^+$	2.3 ± 2.5	7.0 ± 11.1	2.7 ± 2.1	$9.4\pm16^{\$,f}$	$3.3 \pm 3.2^{\$}$
$V_{ m E}{ m L}{ m min}^{-1}$	6.0 ± 2.3	5.3 ± 1	9.6 ± 3.8	7.9 ± 2.5	$12.1\pm 6.5^{\$}$	$12.1\pm3.5^{\$}$
$V_{ m T}{ m L}\cdot{ m min}^{-1}$	0.41 ± 0.15	0.37 ± 0.07	0.61 ± 0.19	0.53 ± 0.17	$0.87\pm0.33^{\$}$	$0.79\pm2.4^{\$}$
Duty cycle [#]	0.43 ± 0.13	0.41 ± 0.04	0.44 ± 0.23	0.42 ± 0.05	0.50 ± 0.30	0.42 ± 0.03
Flow rate [¶] mL·s ⁻¹	0.27 ± 0.08	0.27 ± 0.05	0.38 ± 0.10	0.36 ± 0.08	$0.52\pm0.22^{{\it S}}$	$0.53\pm0.15^{\$}$
Phasic GG-EMG activity % max	4.6 ± 7.9	2.1 ± 4.9	5.8 ± 9.9	2.1 ± 1.9	$14\pm24^{f,\#\#}$	3.3 ± 7.7
Tonic GG-EMG activity % max	2.4 ± 6.3	0.64 ± 2.2	3.8 ± 10.4	0.8 ± 3.8	$5.2 \pm 13.8^{\#\#}$	1.0 ± 3.4
Data are presented as mean \pm sp. <i>P</i> ET, CO ₂	2: end-tidal carbon	ı dioxide tensic	on; VE: minute ventil	ation; <i>V</i> T: tidal	volume; GG-EMG: ge	nionglossus electrom
# measured as time taken for inspiration (4)/	/total time of respi	ratory cycle				

iyogram.

 $\sqrt[n]{measured as } V_{T/t_1}$.

+ p<0.05 for drug effect, *i.e.*, higher GG-EMG during pentobarbital *versus* placebo (all GG-EMG data during carbon dioxide insufflation, general linear model (mixed model)),

§ p<0.05 versus placebo treatment (Wilcoxon)

 $f_{p<0.05 \ versus}^{f}$ baseline, same study day

p<0.1 versus placebo treatment.