

SYMPOSIUM REVIEW

Skeletal muscle vasodilatation during maximal exercise in health and disease

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Abstract Maximal exercise vasodilatation results from the balance between vasoconstricting and vasodilating signals combined with the vascular reactivity to these signals. During maximal exercise with a small muscle mass the skeletal muscle vascular bed is fully vasodilated. During maximal whole body exercise, however, vasodilatation is restrained by the sympathetic system. This is necessary to avoid hypotension since the maximal vascular conductance of the musculature exceeds the maximal pumping capacity of the heart. Endurance training and high-intensity intermittent knee extension training increase the capacity for maximal exercise vasodilatation by 20–30%, mainly due to an enhanced vasodilatory capacity, as maximal exercise perfusion pressure changes little with training. The increase in maximal exercise vascular conductance is to a large extent explained by skeletal muscle hypertrophy and vascular remodelling. The vasodilatory capacity during maximal exercise is reduced or blunted with ageing, as well as in chronic heart failure patients and chronically hypoxic humans; reduced vasodilatory responsiveness and increased sympathetic activity (and probably, altered sympatholysis) are potential mechanisms accounting for this effect. Pharmacological counteraction of the sympathetic restraint may result in lower perfusion pressure and reduced oxygen extraction by the exercising muscles. However, at the same time fast inhibition of the chemoreflex in maximally exercising humans may result in increased vasodilatation, further confirming a restraining role of the sympathetic nervous system on exercise-induced vasodilatation. This is likely to be critical for the maintenance of blood pressure in exercising patients with a limited heart pump capacity.

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Introduction

During low intensity exercise muscle blood flow increases proportionally to the oxygen demand and experiments manipulating arterial oxygen concentration (C_{aO_2}) have demonstrated that, in general, muscle blood flow is regulated to match O_2 delivery with O_2 demand (Saltin *et al.* 1998; Roach *et al.* 1999; Gonzalez-Alonso *et al.* 2006). This is achieved by increasing vasodilatation when C_{aO_2} is reduced by hypoxia (Koskolou *et al.* 1997a; Calbet *et al.* 2003), isovolaemic anaemia (Koskolou *et al.* 1997b), hypervolaemic haemodilution (Calbet *et al.* 2004b) or carbon monoxide breathing (Gonzalez-Alonso *et al.* 2001) while at the same time essentially maintaining perfusion pressure with increasing cardiac outputs. Conversely, when C_{aO_2} is increased by erythrocytic autologous transfusion (Gonzalez-Alonso *et al.* 2006) or hyperbaric hyperoxia (Casey *et al.* 2011), muscle blood flow is reduced during submaximal exercise and thus leaves convective O_2 delivery unaffected. In some circumstances, the blood flow response to exercise may be influenced by O_2 diffusive limitations, which have been extensively treated elsewhere (Wagner, 1988; Calbet & Lundby, 2009; Calbet *et al.* 2009). When during submaximal exercise both acute isovolaemic anaemia and hypoxia are combined to reduce arterial C_{aO_2} by $\sim 60\%$, muscle blood flow is increased by almost $\sim 45\%$ and the muscular \dot{V}_{O_2} is maintained by increasing O_2 extraction (Roach *et al.* 1999). However, in humans with a limited heart pumping capacity, as for example in patients with heart failure, vasodilatation may be restrained by a sympathetically mediated mechanism to avoid hypotension (Piepoli *et al.* 1996; Crisafulli *et al.* 2007), which may be mediated by muscle mechanoreceptors (Middlekauff & Chiu, 2004; Amann *et al.* 2010). Another exception to this mechanism is observed in patients with mitochondrial or metabolic myopathies. In these patients $\dot{V}_{O_{2,max}}$ is reduced and the anaerobic contribution to energy production is high already with low intensity exercise, and muscle blood flow and cardiac output are increased disproportionately to the oxygen demand (Taivassalo *et al.* 2003; Jeppesen *et al.* 2012). Consequently the degree of vasodilatation per work load is greater in patients with mitochondrial myopathies than in healthy controls. However, maximal exercise vasodilatation is also restrained in these patients (Jeppesen *et al.* 2012). Therefore, the magnitude of muscular vasodilatation during submaximal exercise results from the interplay between oxygen delivery, oxygen demand, muscle metabolism, the pumping capacity of heart, and sympathetic activity. The same factors combined with the maximal conductance permitted by the vascular structure when fully vasodilated may contribute to limit maximal muscular hyperaemia in humans.

Maximal muscle hyperaemia

The first measures of muscle blood flow during exercise yielding peak values between 50 and 60 ml (100 g) $^{-1}$ min $^{-1}$ were based on xenon clearance or venous occlusion plethysmography (Grimby *et al.* 1967), which both underestimate the actual values (Saltin, 2007). In the 1980s, the development of the knee extension model by Andersen and Saltin allowed the measurement of quadriceps muscle blood flow in humans in response to incremental exercise (Andersen & Saltin, 1985). The observed values of 250 ml (100 g tissue) $^{-1}$ min $^{-1}$ were later confirmed using the ultrasound Doppler methods to measure the arterial inflow (Rådegran *et al.* 1999). Even higher levels of muscle hyperaemia were reported in elite cyclists with values up to ~ 400 ml (100 g tissue) $^{-1}$ min $^{-1}$ (Richardson *et al.* 1993). Thus, human skeletal muscle may reach peak levels of perfusion similar to those reported in other mammals including athletic species (Parks & Manohar, 1983; Armstrong & Laughlin, 1985; Manohar, 1986; Musch *et al.* 1987; Poole & Erickson, 2011).

The real levels of peak hyperaemia for the human quadriceps muscle during one leg knee extension exercise may, however, be slightly lower (80–90% of the previously reported values) than initially claimed, once the perfusion of the inactive muscle mass of the leg (about 5.5 kg) during knee extension exercise (~ 5 –7 ml (100 g tissue) $^{-1}$ min $^{-1}$ (Heinonen *et al.* 2012), the skin, and other leg tissues are discounted. Since each leg of a healthy young male has a muscle mass of ~ 8 kg (Wang *et al.* 1999), if all leg muscles were to accommodate as much blood flow as the quadriceps muscle during maximal knee extension exercise, the maximal theoretical blood flows would range between 32 and 50–60 l min $^{-1}$ in physically active men and elite athletes, respectively (Andersen & Saltin, 1985). This level of perfusion is impossible since the maximal cardiac output in physically active men ranges between 20 and 25 l min $^{-1}$ (Asmussen & Nielsen, 1955; Åstrand *et al.* 1964; Calbet *et al.* 2007) and the maximal values reported for elite athletes are just above 40 l min $^{-1}$ (Ekblom & Hermansen, 1968).

However, the previous calculation did not account for the fact that blood flow is proportional to the perfusing pressure, and the latter is about 20–30% greater during knee extension than during upright exercise (Hermansen *et al.* 1970; Andersen & Saltin, 1985; Calbet *et al.* 2004a). With intra-arterial infusion of adenosine or ATP at doses that cause maximal vasodilatation, peak leg blood flow in the supine position ranges between 6 and 8 l min $^{-1}$ (0.75–1.00 l min $^{-1}$ kg $^{-1}$), with a mean arterial pressure close to 80 mmHg (Rådegran & Calbet, 2001; Rosenmeier *et al.* 2004; Calbet *et al.* 2006). Thus, increasing the mean arterial pressure to 120–130 mmHg and assuming a similar pressure gradient between the femoral artery and the

femoral vein, the maximal leg blood flow attainable with a mean arterial pressure (MAP) of 120 mmHg, as often observed at peak exercise while bicycling, should lie in between 9 and 12 l min⁻¹ (1.13–1.50 l min⁻¹ kg⁻¹), for untrained men. Then, with a perfusion pressure similar to that observed during knee extension exercise, the mean muscle blood flow for the full leg should be below 150 ml (100 g tissue)⁻¹ min⁻¹ in physically active men (12 l min⁻¹ per leg, assuming 8 kg of muscle mass and that muscle vasodilatation is maximal and similar during peak knee extension and bicycling).

How does this lower value reconcile with the much higher perfusions observed during maximal knee extension exercise? The main explanation is that there are regional differences in hyperaemia between muscle fibres, as reported in rodents (Armstrong & Laughlin, 1985) and foxhounds (Musch *et al.* 1987) with microspheres, and in humans with positron emission tomography (Kalliokoski *et al.* 2000) (Fig. 1). In fact, peak values in deep regions of the quadriceps muscle of up to 400 ml (100 g tissue)⁻¹

min⁻¹ have been reported during isometric intermittent knee extensions using positron emission tomography in physically active men (Heinonen *et al.* 2010). However, the observed mean values for the whole quadriceps were ~40 ml (100 g tissue)⁻¹ min⁻¹, reflecting marked heterogeneity in the regional distribution of blood flow in the exercising quadriceps muscle in humans (Heinonen *et al.* 2010).

Another mechanism that has been suggested to contribute to enhance muscle hyperaemia is ‘the muscle pump’ (Laughlin, 1987). The most prominent explanation for how this theoretical construct may facilitate blood flow is by reducing the venous hydrostatic pressure in dependent limbs (for review see Laughlin, 1987; Tschakovsky & Sheriff, 2004). In addition to this, muscle contractions generate a small arterial retrograde flow, whilst at the same time facilitating venous blood to be propelled towards the heart. In the drained venous segments negative pressures may be generated when the muscles relax and return to their original length, facilitating the inflow of blood from arteries, since retrograde flow from more proximal venous segments is impeded by venous valves. It has also been suggested that the muscle pump may increase the kinetic energy of blood, though the mechanism is unclear. According to Tschakovsky & Sheriff (2004), contraction frequency constitutes a major determinant of muscle pump efficacy, but this contrasts with the observation of no effect of contraction frequency on muscle perfusion at a given exercise intensity in humans (Hoelting *et al.* 2001; Osada & Radegran, 2002). Moreover, the effect of a muscle pump should be proportional to the mechanical work of the pump, i.e. to exercise intensity. However, once peak leg blood flow has reached its maximum value, increasing exercise intensity (which must enhance the action of the pump) does not result in higher perfusion. Similar conclusions have been achieved by others (Gonzalez-Alonso *et al.* 2008).

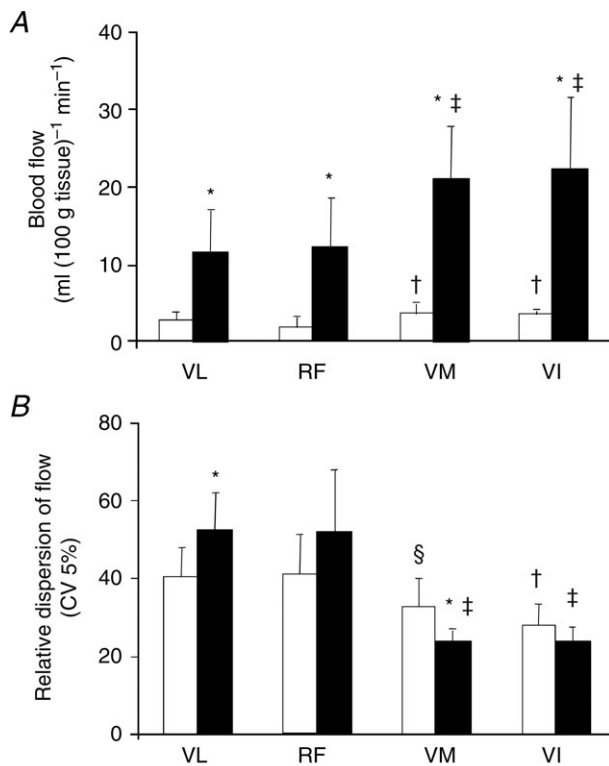


Figure 1. High heterogeneity of skeletal muscle blood flow in humans

Mean blood flow (A) and relative dispersion of blood flow (B) in the different portions of the quadriceps femoris muscle measured with positron emission tomography and H₂¹⁵O during intermittent leg extension isometric contractions (Kalliokoski *et al.* 2000). **P* < 0.01 rest versus exercise, †*P* < 0.001 versus resting RF and VL, ‡*P* < 0.001 versus exercising RF and VL, §*P* < 0.001 versus resting VL. VL: vastus lateralis; RF: rectus femoris; VM: vastus medialis; VI: vastus intermedius.

Is there a functional reserve in muscle vasodilatory capacity during maximal exercise in humans?

In general, during maximal dynamic exercise with either a small muscle mass (one- or two-legged knee extension exercise) similar levels of muscle hyperaemia are reached regardless of C_{aO_2} , P_{O_2} , venous muscle pH, femoral vein blood temperature, haemoglobin desaturation or acclimatization to altitude in healthy humans (Koskolou *et al.* 1997b; Roach *et al.* 1999; Mourtzakis *et al.* 2004; Calbet & Lundby, 2009). This could indicate that during exercise engaging a small muscle mass vasodilatation is already maximal in the active regions of the muscle, implying that to even further increase muscle blood flow perfusion pressure must be increased. To test if there is

some residual vasodilatory capacity during small muscle mass exercise, Barden *et al.* (2007) infused adenosine intra-arterially during maximal knee extension exercise performed with hyperoxia ($F_{IO_2} = 1$). In the four subjects from whom maximal data were obtained, peak vascular conductance was not increased by adenosine (Barden *et al.* 2007). Although this study is in agreement with a lack of vasodilatory reserve at maximal exercise in humans, there are two limitations that preclude any definitive conclusion. First, only the quadriceps muscle was recruited during the exercise but the adenosine was infused into the common femoral artery, and this causes massive vasodilatation in the hamstrings and other leg tissues (Heinonen *et al.* 2010). Second, adenosine increases muscle sympathetic activity when infused at rest and is not as potent as for example ATP as a sympatholytic agent, leaving open the possibility of some vasodilator reserve in the active muscles not revealed by the infusion of adenosine, due to some sympathetic vasoconstriction still remaining during the adenosine infusion (Rosenmeier *et al.* 2004).

Theoretical calculations by Saltin (1985) indicated that the combined maximal vasodilatory capacity of the arm and leg muscles would be of such a magnitude, that in order to maintain MAP during maximal whole body exercise, cardiac output would have to be increased 2- to 3-fold higher than that achievable at peak exercise. This also implies that to prevent hypotension during whole body exercise and to avoid insufficient oxygen delivery to the heart, brain and respiratory muscles, which may require between 3 and 5 l min^{-1} of blood flow, vasodilatation in the active muscles must be restrained and precisely controlled. The regulating mechanism(s) should respond to changes in arterial pressure and must integrate signals from the other vascular beds also in order to ensure sufficient oxygen supply. There is strong evidence suggesting that the sympathetic nervous system plays this role by restraining muscle vasodilatation during whole body exercise, or in exercise conditions for which there is risk of hypotension (Marshall *et al.* 1961; Secher *et al.* 1977; Lang *et al.* 1997; Dela *et al.* 2003; Schrage *et al.* 2004). For example, Marshall *et al.* (1961) reported that blood pressure was reduced during supine exercise in a man who had undergone surgical thoracolumbar sympathectomy for essential hypertension.

Similarly, MAP drops during electrostimulation-induced exercise on the cycle ergometer in paraplegics who lack functional sympathetic innervation in the legs (Dela *et al.* 2003). In chronic heart failure (CHF) patients sympathetic inhibition with clonidine results in greater leg vascular conductance during peak exercise on the cycle ergometer (Lang *et al.* 1997). Several exercise models during which blood flow demand beyond the main active muscles was increased by superimposing intense arm exercise on leg exercise (Secher *et al.* 1977) or vice versa (Volianitis & Secher, 2002), or by increasing the work of

the respiratory muscles (Harms *et al.* 1997), have reported a subsequent vasoconstriction on the main active muscles, which is likely to be mediated by the sympathetic nervous system. Conversely, unloading the respiratory muscles during exercise resulted in greater quadriceps muscle blood flow in chronic obstructive pulmonary disease (COPD) patients (Vogiatzis *et al.* 2011).

Thus, indirect evidence suggests that during whole body exercise muscle vasodilatation must be restrained to maintain MAP. More definitive evidence for such a mechanism was obtained by studying a group of elite cross-country skiers in which maximal cardiac output, and leg and arm blood flows were assessed while skiing using different techniques involving various combinations of arm and leg exercise (Calbet *et al.* 2004a). It was observed that during maximal diagonal skiing, where arms and legs are strongly engaged simultaneously, that the vasodilatory response was restricted to values below the maximal attainable to maintain MAP (Fig. 2).

To determine if counteracting ongoing sympathetic vasoconstriction during whole body cycle exercise

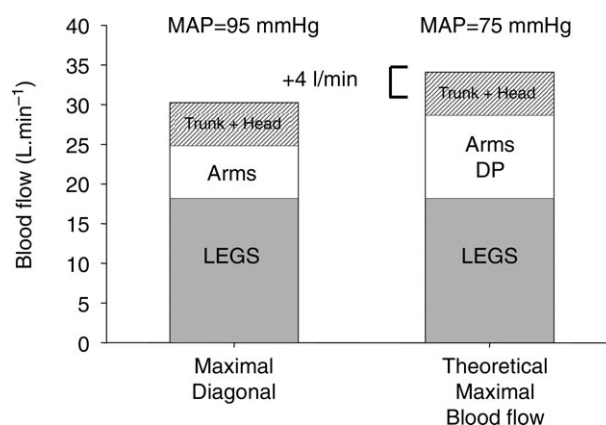


Figure 2. The combined vasodilatory capacity of the arm and leg muscles exceeds the pumping capacity of the heart (Calbet *et al.* 2004a)

Cross-country skiers were studied during submaximal (76% $\dot{V}_{O_{2max}}$) skiing while using arm and legs (diagonal technique), only arm (double poling technique) and leg skiing (like skating). They were also studied during maximal exercise with the diagonal technique. Trunk and head perfusion at maximal diagonal was calculated by subtracting peak leg and arm blood flows from peak cardiac output. The maximal theoretical cardiac output was calculated by adding the maximal values that were observed for leg blood flow (during maximal diagonal), the peak arm blood flow (observed during double poling) and the 5 l min^{-1} of blood flow necessary to perfuse the head and trunk. The latter gave 4 l min^{-1} more cardiac output than actually measured, implying that in humans with well trained arm and leg muscles the combined peak perfusion of the head trunk and arm muscle exceeds the pumping capacity of the heart. This also implies that during maximal upright arm and leg combined exercise, muscle vasodilatation must be restrained to avoid hypotension. (Figure from Calbet & Joyner, 2010.)

would enhance muscle blood flow and oxygen delivery, and thereby exercise performance, ATP was infused intra-arterially at near maximal and maximal exercise under control conditions (at sea level) (Calbet *et al.* 2006) and after 8–12 days at high altitude (4559 m above sea level) (Lundby *et al.* 2008). At sea level, ATP increased maximal exercise leg vascular conductance by 17% (Calbet *et al.* 2006). MAP was not affected by the infusion of ATP due to a small (6%) but significant elevation of cardiac output. About half of the increase in cardiac output was directed to the ATP-infused leg, which showed a trend ($P=0.08$) for 0.8 l min^{-1} higher LBF (8% more than under control conditions). However, the infusion of ATP reduced the a-vO₂ difference, likely to be due to a deviation of some blood flow to less active muscle fibres and other tissues of the leg. After 8–12 days of residence at altitude the resting MAP was elevated by ~ 20 mmHg, likely to be due to increased sympathetic activity mediated in part an increased chemoreflex response in chronic hypoxia (Calbet, 2003; Hansen & Sander, 2003). At the same time maximal cardiac output and peak leg blood flow were reduced by $\sim 20\%$, indicating that at maximal exercise in hypoxia there was a functional reserve (about 5 l min^{-1}) to increase cardiac output and, hence leg blood flow, in response to the ATP infusion. Similar to at sea level, maximal exercise leg vascular conductance was increased, whereas leg blood flow was not. The latter was likely to be the consequence of a reduction of maximal exercise MAP with ATP. O₂ extraction across the leg was reduced with ATP at altitude confirming that unselective vasodilatation at maximal exercise may cause $\dot{V}_{\text{O}_2}/\dot{Q}$ mismatch in normoxic conditions or when sympathetic activity is increased, as for example in chronic hypoxia.

Muscle fibre type, training and reduced physical activity

Regional differences in peak exercise hyperaemia have been attributed to differences in fibre type composition and training. In rodents, peak muscle hyperaemia may be 2- to 4-folds greater in red (type I) than in predominantly white (type II) muscles (Armstrong & Laughlin, 1985). Cross-sectional studies in humans indicate that endurance trained muscles may have a 30–60% higher peak hyperaemic responses to exercise than untrained muscles (Andersen & Saltin, 1985; Snell *et al.* 1987; Richardson *et al.* 1993). There are few longitudinal studies in humans where the effect of training on peak exercise muscle hyperaemia has been examined (Juel *et al.* 2004; Mourtzakis *et al.* 2004; Blomstrand *et al.* 2011). Blomstrand *et al.* (2011) studied 14 recreationally active subjects who performed one-legged knee extension exercise for 5–7 weeks, 3–5 days per week (~ 1 h per session), while the

other leg remained untrained (Fig. 3). Five of the subjects trained at approximately 70% of their pre-determined one-legged peak work rate (5 days week⁻¹), four others performed 40 bouts each consisting of 1 min exercise at approximately 100% of maximal single leg oxygen uptake, separated by 30 s rest periods (aerobic intermittent training; 3 days week⁻¹), and five subjects performed 15×1 min bouts of exercise at 150% of the maximal single leg oxygen uptake, separated by 3 min rest periods (anaerobic intermittent training; 4 days week⁻¹). The three groups all improved their peak leg \dot{V}_{O_2} by $\sim 32\%$, and this improvement was related to a 30% increase in leg blood flow, i.e. oxygen delivery. Since the muscle mass was increased by 5.8%, the normalized peak quadriceps muscle hyperaemia was increased by 22%, from 216 to $265\text{ ml (100 g)}^{-1}\text{ min}^{-1}$ (Blomstrand *et al.* 2011). In six subjects, Juel *et al.* (2004) reported an increase of peak quadriceps muscle blood flow of 25% after 7–8 week of one-legged knee extension high-intensity interval training with (15×1 min bouts at 150% of $\dot{V}_{\text{O}_{2\text{max}}}$, with 3 min rest periods). Aerobic one-legged knee extension training (1 h day^{-1} at 70% maximum workload for 5 days week⁻¹) in six subjects resulted in a $\sim 27\%$ greater leg blood flow and vascular conductance (Mourtzakis *et al.* 2004). Interestingly, the level of maximal hyperaemia after training was almost identical when tested in normoxia and hyperoxia ($F_{\text{I}\text{O}_2}: 0.6$), indicating that during exercise engaging only a small muscle mass peak muscle blood flow reaches the same value regardless of C_{aO_2} (Mourtzakis *et al.* 2004).

The effect of training on maximal exercise hyperaemia during whole body exercise, as for example during bicycling in the semi-recumbent position, was studied by Roca *et al.* (1992). In nine non-active men, 9 weeks of

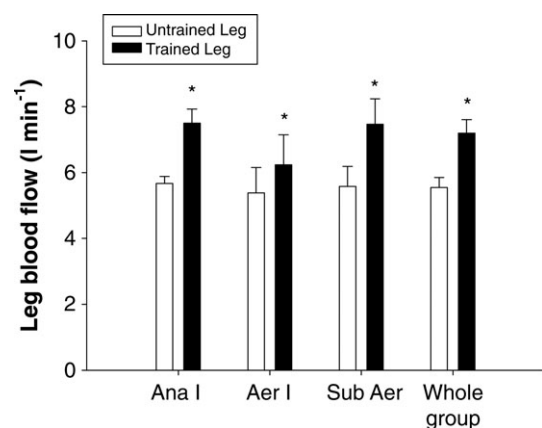


Figure 3. Changes in peak leg blood flow after three different knee extension training programs: anaerobic intervalic (Ana I), aerobic intervalic (Aer I), and submaximal aerobic (Sub A)

The three groups improved similarly their peak leg \dot{V}_{O_2} by 32%, and this improvement was due to a 30% increase in leg blood flow (Whole group) (Blomstrand *et al.* 2011).

endurance training increased peak leg blood flow by $\sim 27\%$ in normoxia and hypoxia ($F_{I_{O_2}}$: 0.12) (Roca *et al.* 1992). The effect of training on the leg blood flow response to submaximal exercise at the same absolute work load remains controversial, with some studies reporting a small reduction after training (Kiens *et al.* 1993; Proctor *et al.* 2001; Nyberg *et al.* 2012b) or no change at low intensities but increases at near-maximal exercise intensity (Krustrup *et al.* 2004). Consequently, submaximal haemodynamic responses to exercise cannot be used to infer the response at maximal exercise.

Overall, these studies demonstrate that in a relatively short time maximal muscle hyperaemia during small or large muscle mass exercise may be increased by 20–30%, without concomitant changes in MAP. A more prolonged training stimulus may cause even greater increases of peak vascular conductance, as suggested by the study of Sinoway *et al.* (1986), who showed that post-ischaeamic forearm maximal vascular conductance was 42% higher in the dominant compared to the contralateral arm of tennis players (Fig. 4). The increase in perfusion may be explained by two main mechanisms, (a) increased vasodilatation (functional cross-sectional area) or (b) increased anatomical vascular cross-sectional area, or a combination of both. The first mechanism would imply that before training there is a functional vasodilator reserve not utilized even at peak exercise, which is made available with training. The second mechanism requires vascular remodelling leading to widening of conduit arteries and

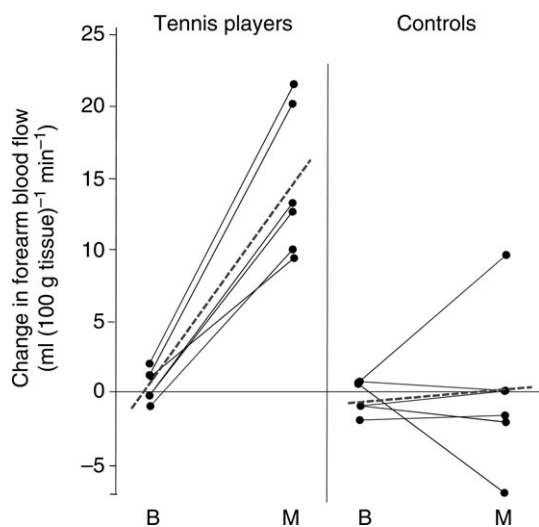


Figure 4. Maximal post-ischaeamic vasodilatation in the dominant and non-dominant arms of tennis players and control subjects with similar $\dot{V}_{O_{2\max}}$, measured with plethysmography after 5 min of arterial occlusion coupled with 1 min of exercise

In the tennis players maximal forearm hyperaemia was 42% higher in the dominant than in the non-dominant forearm (Sinoway *et al.* 1986).

arteriogenesis in response to training (increasing the capillary bed alone does not enhance the cross-sectional area of the resistance vessels).

Vascular remodelling increases the cross-sectional area of the capillary bed (Andersen & Henriksson, 1977; Duscha *et al.* 1999; Blomstrand *et al.* 2011; Esposito *et al.* 2011) and conduit arteries (Schmidt-Trucksass *et al.* 2000; Naylor *et al.* 2006), by a mechanism involving shear stress and NO (Tinken *et al.* 2010; Green *et al.* 2012). For example, the internal diameter of the femoral artery is wider in cyclists, middle-distance runners and triathletes, while that of the carotid artery is similar in athletes and controls (Schmidt-Trucksass *et al.* 2000). Moreover, increases in brachial artery diameter have been shown following training resumption in elite rowers (Naylor *et al.* 2006).

Interestingly, if shear stress is attenuated in one arm during bilateral handgrip training by cuff inflation the training-induced improvement of peak reactive hyperaemia is completely blunted in the cuffed arm (Tinken *et al.* 2010) (Fig. 5). In this study, no increase was observed in the cuffed arm brachial artery resting diameter after training, while in the non-cuffed arm the brachial artery diameter was increased by 0.2 mm. Although this change was non-statistically significant it accounted for one-third of the increase in peak reactive hyperaemia after training in the non-cuffed arm. This is due to the great impact that the radius of the vessels have on the vascular conductance (conductance = $\pi r^4/8\eta L$, where η represents the viscosity and L the length of the vessel). Consequently, a small error of only 0.1–0.2 mm in the assessment of the diameter of the brachial artery has a major impact on the calculations of blood flow and vascular conductance.

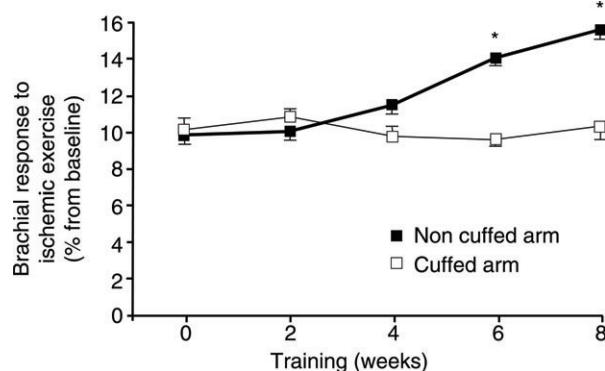


Figure 5. Relative change in brachial artery flow mediated dilatation from baseline in response to ischaemic exercise across the 8-week handgrip exercise training in healthy young men

One arm was trained with a cuff around the arm inflated at 60 mmHg to prevent shear stress. Error bars represent SEM.

* $P < 0.05$ between the cuffed and non-cuffed arm (Tinken *et al.* 2010).

Maximal exercise vascular conductance is reduced with ageing by unknown mechanism(s) (Proctor *et al.* 2003, 2004). Animal studies have reported arteriolar rarefaction (reduced number of arterioles) in rodent muscle with ageing (Behnke *et al.* 2006). This may be facilitated by a combination of factors including reduced physical activity (Sugawara *et al.* 2004; Rakobowchuk *et al.* 2011), endothelial dysfunction (Taddei *et al.* 2001) and lower nitric oxide bioavailability (Nyberg *et al.* 2012a), leading to remodelling of the vascular tree (rarefaction). Other mechanisms, like altered sympatholysis, may also play a role (see below).

Sympathetic overactivity may limit exercise vasodilatation in patients

Excessive sympathetic activation is involved in both initiation and progression of chronic heart failure (CHF) (Hasking *et al.* 1986; Brunner-La Rocca *et al.* 2001). This sympathetic overactivity has been attributed to an impairment of baroreflex control of sympathetic activity (Grassi *et al.* 1995) and increased peripheral chemoreflex sensitivity (Despas *et al.* 2012). Although forearm vascular resistance is increased in patients with sympathetic overactivity (Roveda *et al.* 2003) and intense sympathoexcitation during exercise contributes to a reduced exercise capacity in CHF (Piepoli *et al.* 1996; Notarius *et al.* 2001; Crisafulli *et al.* 2007), it remains unknown whether the increased sympathetic overactivity may play a role in limiting maximal exercise induced vasodilatation. In chronic heart failure maximal cardiac output is reduced and hence the capacity to perfuse the active muscles (Magnusson *et al.* 1997). These patients have a rather limited capacity to perform exercise on the cycle ergometer in part due to the reduced oxygen delivery; however, they can reach a peak skeletal muscle perfusion and a leg oxygen uptake similar to that of healthy individuals when only a sufficiently small muscle mass is activated (Magnusson *et al.* 1997).

Increasing the active muscle mass in heart failure patients results in lower peak leg blood flow and leg vascular conductance accompanied by increased noradrenaline spillover (an indirect measure of sympathetic activation). This sympathoactivation is likely to be necessary to limit the exercise-induced skeletal muscle vasodilatation and thereby preserve a minimal degree of perfusion levels for the brain, heart and respiratory muscles (Poole *et al.* 2012).

Exercise training decreases muscle sympathetic nerve activity (MSNA) in CHF (Roveda *et al.* 2003) and hypertensive patients (Laterza *et al.* 2007). The reduction in sympathetic overactivity has been associated with improved baroreflex control of MSNA and heart rate (HR) during increases and decreases in MAP (Laterza

et al. 2007). Moreover, in CHF exercise training elicits a marked increase of maximal exercise hyperaemia, although this does not seem related to a reduced exercise sympathetic activation (Esposito *et al.* 2010). However, exercise capacity and quality of life of these patients is improved with cycle training by several mechanisms which may include enhanced maximal cardiac output and O₂ extraction capacity (independent or in combination) (Cattadori *et al.* 2011).

It has been reported that training one leg at a time with knee extensions (8 weeks of endurance training, 3 times a week, 50 min session⁻¹ leg⁻¹) resulted in 38% increase in peak leg blood flow (+1.2 l min⁻¹) during single knee extension exercise and 19% (+1.8 l min⁻¹) during exercise on the cycle ergometer (Esposito *et al.* 2011), despite the fact that maximal cardiac output (measured during cycling) was increased only by 5% (not statistically significant). The corresponding improvements for leg $\dot{V}_{O_{2peak}}$ during bike and single leg exercise were 40 and 54%, respectively. The increase in peak muscle perfusion was explained by a 40 and 53% greater peak vascular conductance. Interestingly, this increase in vascular conductance was not associated with lower calculated noradrenaline spillover values, but was accompanied by increased muscle fibre cross-sectional area, capillary-to-fibre ratio, number of capillaries around each fibre, and mitochondrial volume (Esposito *et al.* 2011).

In heart failure patients with an haematocrit below 35%, erythropoietin treatment increasing [Hb] from 11 to 14 g dl⁻¹ increased $\dot{V}_{O_{2peak}}$ during cycle ergometer exercise by 15% (from 11 ± 0.8 to 12.7 ± 2.8 ml kg⁻¹ min⁻¹) and the 6 min walking distance by 12%, without significant changes in post-ischaemic forearm vascular conductance (Mancini *et al.* 2003). Altogether, these studies indicate that in heart failure patients peak exercise hyperaemia is limited to a great extent by the reduced leg flow conductance due to structural factors (a smaller vascular tree).

Altered sympatholysis could contribute to reduce maximal exercise vasodilatation

Sympathetic nerve activity increases with central command and exercise intensity (Victor *et al.* 1995), and may be enhanced by muscle afferent feedback from mechanoreceptors, venous distension (Cui *et al.* 2011) and the peripheral chemoreceptors (Stickland *et al.* 2011). The increase of sympathetic nerve activity restricts muscle blood flow (O'Leary *et al.* 1997) through α -adrenoreceptor stimulation at the feed arteries (VanTeeffelen & Segal, 2003). Muscle contractions cause the release of vasodilator substances that initiate a conducted vasodilatation signal that travels along the vessel wall retrogradely up to the

feed arteries, counteracting the vasoconstrictor action of the sympathetic nerves (VanTeeffelen & Segal, 2006). This process is named functional sympatholysis (Remensnyder *et al.* 1962).

Moore *et al.* (2010) have demonstrated that the conducted vasodilatation is increased by phentolamine (which blocks the α -adrenergic receptors) even in response to an isolated muscle contraction lasting 0.1 s. This implies that some constitutive sympathetic tone at rest is necessary to avoid unwanted conducted vasodilatation spreading to neighbouring non-contracting muscle regions. Insufficient sympatholysis due to either increased sympathetic tone or reduced sympatholytic activity could explain the reduced maximal exercise vasodilatation observed with ageing (Jackson *et al.* 2010) and in conditions accompanied by increased sympathetic activity such as CHF, chronic kidney failure, preeclampsia and COPD. In this regard, enhanced activation of α -adrenoreceptors restricting conducted vasodilatation has been shown in ageing mice (Jackson *et al.* 2010) and combined with the exercise induced enhancement of sympathetic neural activity, this could explain the reported limited maximal exercise vasodilatation observed in old men and women (Koch *et al.* 2003; Proctor *et al.* 2004).

Interestingly, Kirby *et al.* (2012) have reported that old compared to young men have blunted increase of plasma venous ATP concentration and reduced effluent ATP values during forearm exercise due to impaired ATP release from the erythrocytes in response to haemoglobin deoxygenation (see Ellsworth & Sprague (2012) for review). Impaired functional sympatholysis has been observed after 2 weeks of muscle immobilization (Mortensen *et al.* 2012) and in hypertensive patients (Vongpatanasin *et al.* 2011). Nitric oxide (NO) bioavailability is also reduced with ageing in humans, however improving NO bioavailability with an intra-arterial infusion of the antioxidant *N*-acetylcysteine did not increase leg blood flow in exercising men (Nyberg *et al.* 2012a). The influence that changes in circulating or interstitial putative sympatholytic signals (K^+ , ATP, NO, etc.) and responsiveness to these sympatholytic agents in health and disease on peak exercise vasodilatation deserves future study.

Conclusions

Human skeletal muscle may reach similar levels of peak hyperaemia during exercise to those observed in other mammals, including athletic species. Exercise elicits heterogeneous muscle hyperaemia, reflecting differences in vascular structure and motor unit recruitment. Maximal muscle vasodilatation in exercising humans depends on the active muscle mass, is likely to be restrained by sympathetic nervous system during whole

body exercise, increases with training, whilst it is reduced with ageing and in diseases accompanied by increased sympathetic overactivity or reduced pumping capacity of the heart. It remains unknown if a reduction of the sympathetically mediated vasoconstriction during maximal exercise plays a role in the training-induced increase of peak muscle vasodilatation in healthy humans. In patients with chronic heart failure, hypertension and probably other conditions accompanied by sympathetic overactivity, or limited maximal cardiac output, peak skeletal muscle vasodilatation may be limited by the sympathetic system, even during exercise with a small muscle mass. Exercise training may normalize sympathetic overactivity and enhance maximal exercise vascular conductance and thereby increase the quality of life and prognosis of these patients.

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