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ORIGINAL ARTICLE Glucose modulation of spreading depression susceptibility

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Spreading depression of Leão is an intense spreading depolarization (SD) wave associated with massive transmembrane ionic, water, and neurotransmitter shifts. Spreading depolarization underlies migraine aura, and occurs in brain injury, making it a potential therapeutic target. While susceptibility to SD can be modulated pharmacologically, much less is known about modulation by systemic physiological factors, such as the glycemic state. In this study, we systematically examined modulation of SD susceptibility by blood glucose in anesthetized rats under full physiological monitoring. Hyperglycemia and hypoglycemia were induced by insulin or dextrose infusion (blood glucose ~40 and 400 mg/dL, respectively). Spreading depolarizations were evoked by direct cortical electrical stimulation to determine the intensity threshold, or by continuous topical KCl application to determine SD frequency. Hyperglycemia elevated the electrical SD threshold and reduced the frequency of KCl-induced SDs, without significantly affecting other SD properties. In contrast, hypoglycemia significantly prolonged individual and cumulative SD durations, but did not alter the electrical SD threshold, or SD frequency, amplitude or propagation speed. These data show that increased cerebral glucose availability makes the tissue resistant to SD.

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INTRODUCTION

Spreading depression of Leão is an intense spreading depolarization (SD) wave associated with massive ionic, water, and neurotransmitter fluxes typically lasting less than a minute in normal brain. Spreading depolarization is believed to be the electrophysiological substrate of migraine aura and a trigger for headache. Moreover, SDs occur in ischemic, hemorrhagic, or traumatic brain injury, and worsen tissue outcome by increasing the metabolic burden and diminishing the perfusion.¹ Therefore, SD is a potential therapeutic target in migraine and brain injury.²

Genetic and pharmacological modulation of SD susceptibility is well recognized;³⁻⁶ however, modulation by systemic physiological factors is poorly understood. Glycemic status in particular is clinically relevant and modifiable factor in the manaа gement of brain injury and migraine. Spreading depolarization rapidly stimulates glucose consumption, leading to a lasting depletion of tissue glucose, and hypoglycemia delays SD recovery, suggesting that glucose is an important immediate source of energy required to restore the transmembrane ionic gradients after SD.^{7–9} Indeed, hyperalycemia suppresses peri-infarct SDc^{10–12} Indeed, hyperglycemia suppresses peri-infarct SDs.^{10–12} However, it is not clear whether this is because of improved energy status in ischemic penumbra stabilizing the polarization state, or because tissue glucose availability directly modulates SD susceptibility. In support of the latter, hypoglycemia appears to lower topical KCl concentrations required to trigger a SD,¹³ and hyperglycemia has been reported to markedly reduce the amplitude of KCI-induced SDs.¹¹ However, there has never been a systematic analysis of the impact of blood and cerebrospinal fluid (CSF) glucose levels on SD susceptibility. Therefore, using electrical and KCl stimulation as two independent but complementary methods for SD induction, we tested the hypothesis that blood glucose is inversely related to SD susceptibility.

MATERIALS AND METHODS

National and institutional guidelines for animal care and use for research purposes were strictly followed, and study protocol was approved by the institutional review board.

Surgical Preparation

A total of 28 rats (Sprague–Dawley, male, 275 to 400 g) were fasted overnight, anesthetized with urethane (1.3 to 1.5 g/kg, intraperitoneal), and intubated for mechanical ventilation (70% N₂O/30% O₂; SAR-830, CWE, Ardmore, PA, USA). Femoral vein and artery were cannulated for drug infusions, continuous mean arterial blood pressure recording (PowerLab, ADInstruments, Colorado Springs, CO, USA), and arterial blood gas and pH measurements every 15 to 30 minutes to maintain arterial pCO₂ around 35 mm Hg (Rapidlab 248 blood gas/pH analyzer, Siemens HealthCare, Eschborn, Germany). Arterial blood pressure, pH, pCO_2 , and pO_2 were comparable among different glycemic states (Table 1). Rectal temperature was kept at 37°C using a thermostatically controlled heating pad (Harvard Apparatus, Holliston, MA, USA). Rats were placed in a stereotaxic frame (Stoelting, Wood Dale, IL, USA) and three burr holes were drilled under saline cooling on each hemisphere at the following coordinates (mm from bregma): (1) posterior 7, lateral 2 (parieto-occipital cortex) for direct electrical stimulation (2 mm diameter), or topical KCl application (1 mm diameter); (2) posterior 5, lateral 2 (fronto-parietal cortex) for proximal recording site; (3)

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Table 1. Systemic physiological parameters							
Group	Ν	BP (mm Hg)	pН	pCO₂ (mm Hg)	pO_2 (mm Hg)	Blood glucose (mg/dL)	CSF glucose (mg/dL)
Hypoglycemia	6	104 ± 4	7.38 ± 0.01	36±1	181 ± 9	39±1	21 ± 3
Normoglycemia	12	100 ± 4	7.41 ± 0.01	35 ± 1	185 ± 9	128 ± 7	98 ± 10
Hyperglycemia	10	104 ± 3	$\textbf{7.41} \pm \textbf{0.01}$	37 ± 1	177 ± 10	425 ± 16	228 ± 12
RP blood pressure: CSE cerebrospinal fluid							

3P, blood pressure; CSF, cerebrospinal fluid.



Figure 1. Glycemic state and electrical stimulation threshold for spreading depolarization (SD) induction. Representative DC potential recordings show the timing and intensity of cathodal stimulation in the three glycemic groups, and the threshold intensity that triggered an SD. The graph shows the median (horizontal line), mean (+), 25% to 75% range (box), and 10% to 90% range (whisker) in each group. *P < 0.01 versus both hypoglycemic and normoglycemic groups. Vertical calibration bar = 25 mV. μ C, microCoulomb.

posterior 1, lateral 2 mm (frontal cortex) for distal recording site. Dura was gently removed at the KCl site, and care was taken to avoid bleeding. Following surgical preparation, the cortex was allowed to rest for 10 minutes under saline irrigation and dura was covered with mineral oil to prevent drying.

Electrophysiology

The extracellular steady (DC) potential and electrocorticogram were recorded with glass micropipettes (150 mmol/L NaCl), $300 \,\mu$ m below the dural surface (EX1 differential amplifiers, Dagan Corporation, Minneapolis, MN, USA). Ag/AgCl reference electrode was placed subcutaneously in the neck.

Spreading Depolarization Susceptibility

Spreading depolarization susceptibility was determined using two distinct but complementary methods. On one hemisphere, electrical threshold for SD induction was determined by direct cortical stimulation using a constant current unit (WPI, Sarasota, FL, USA), a bipolar stimulation electrode placed on the cortical pial surface (400 μ m tip diameter, 1 mm tip separation; Frederick Haer Company, Bowdoin, ME, USA), and a Ag/AgCl ground electrode placed subcutaneously in the neck, as described previously. Cathodal pulses of increasing intensity (100 to 4,000 μ C) were applied at 4-minute intervals by adjusting the stimulus current and duration until an SD was observed. At 1 mA current, pulses of 100, 200, 300, and 400 milliseconds were applied followed by 2 mA current of 300, 400, and 500 milliseconds. If SD was not evoked, additional stimuli of 3 mA, 400 milliseconds, and 4 mA, 400, 500, 1,000 milliseconds then were applied. After the completion of threshold determination, the other hemisphere was surgically prepared in the same manner. A cotton ball (2 mm diameter) soaked with 1 M KCl was placed on the pial surface and replaced every 30 minutes. The number of KCl-induced SDs was counted for 1 hour. Small amplitude shifts in extracellular DC potential (<5 mV) were not included in the SD count.

Spreading Depolarization Attributes

In addition to the electrical SD threshold and KCI-induced SD frequency, the amplitude of DC shift, and its duration at half maximal amplitude were measured. The duration of first SD upon KCI application, as well as the average and cumulative duration of all SDs during continuous KCI application were calculated. Spreading depolarization propagation speed was measured based on its latency and the distance between the proximal and distal recording electrodes. In addition, propagation block between the two recording sites (%) was calculated as: $100 \times (1 - (number of SDs detected at the distal site/proximal site))$.

Experimental Protocol

Three cohorts of rats were studied in alternating order. Hypoglycemia was induced by combined insulin and glucose (10%) infusion. After an initial bolus of 3 mU/g, insulin infusion was maintained at 1.5 mU per kg per minute. Blood glucose was initially monitored every 5 to 10 min, and then every 30 min to adjust the infusion rate for a target blood glucose of 40 mg/dL. Hyperglycemia was induced by intravenous 20% dextrose infusion for 1 hour; an additional dose (1 to 2 ml) of 40% dextrose was given intraperitoneally to achieve target blood glucose (\sim 400 mg/dL). Saline infusion served as time control in normoglycemic group. Once target blood glucose was achieved, glycemic condition was



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Figure 2. Glycemic state and susceptibility to KCI-induced spreading depolarization (SD). (**A**) Representative DC potential recordings show repetitive SDs during continuous topical KCI (1 M) application in the three glycemic groups. Box and whisker plots show SD frequency (**B**), duration of first SD upon initial topical KCI application (**C**), total cumulative and average SD durations during 1 hour continuous topical KCI application (**D**, **E**), propagation speed of first SD upon initial topical KCI application (**F**), and SD amplitude (**G**). Hypoglycemia prolonged the SDs, so that although SD frequency was not increased, total cumulative depolarization duration was significantly longer. In contrast, hyperglycemia reduced SD frequency, and the duration of first SD. [†]*P* < 0.05 versus normoglycemia; [‡]*P* < 0.05 versus hypoglycemia; ^{*}*P* < 0.01 versus both hyperglycemia and normoglycemia. Vertical calibration bar = 25 mV.

maintained for 1 hour before SD susceptibility assessment and continued throughout the experiment. At the end of each experimental protocol, cerebrospinal fluid (CSF) was sampled via cisternal puncture and glucose concentrations were measured. Cerebrospinal fluid glucose levels showed excellent correlation with blood glucose in each cohort ($R^2 = 0.83$; Table 1).

Data Analysis

Data are expressed as mean \pm s.d. One-way analysis of variance or Kruskal–Wallis tests were used to determine statistically significant differences in parametric and nonparametric datasets, respectively (GraphPad Prism 5, La Jolla, CA, USA).

RESULTS

Hyperglycemia elevated the electrical threshold for SD induction (Figure 1), and suppressed KCI-induced SD frequency (Figures 2A

and 2B). The duration of first SD triggered upon initial KCl application also tended to be shorter compared with normoglycemic rats (Figure 2C). However, in normoglycemic rats, SD durations quickly decreased after the first SD (subsequent SDs 32% shorter lasting compared with first SD, P < 0.01). Therefore, the average and total cumulative duration of all SDs triggered during 1 hour KCl application did not significantly differ between normoglycemic and hyperglycemic groups (Figures 2D and 2E).

In contrast to hyperglycemia, hypoglycemia did not alter SD threshold (Figure 1) or frequency (Figures 2A and 2B). As expected, SD durations were significantly prolonged (Figure 2C). Indeed, the average and total cumulative depolarization durations during 1 hour topical KCI application were more than doubled in hypoglycemic rats (Figures 2D and 2E).

Glycemic state did not impact SD propagation speed or amplitude (Figures 2F and 2G), or the incidence of propagation block between the two recording sites $(23\% \pm 13\%, 23\% \pm 18\%,$

and 9% \pm 27% in hypoglycemic, normoglycemic, and hyperglycemic groups, respectively; $P\!>\!0.05$).

DISCUSSION

Our data demonstrate that glycemic state and cerebral glucose availability are important modulators of SD susceptibility and duration in otherwise normal rat brain. Hyperglycemia rendered the cortex more resistant to SD initiation and hastened SD recovery, whereas hypoglycemia had the opposite effect on SD durations. More severe hyperglycemia was reported to greatly diminish the occurrence and duration of peri-infarct SDs and decrease the amplitude of KCI-induced SDs, although SD frequency and duration did not appear to differ from normoglycemic controls.¹¹ In another study, hyperglycemia delayed and hypoglycemia hastened the onset of anoxic depolarization.¹⁴ This was later confirmed using diffusion-weighted MRI, which also showed that hyperglycemia shortened the duration of peri-infarct SDs in ischemic penumbra, but interestingly not in nonischemic cortex.¹⁵ The latter may reflect better preservation of the tissue glucose pool, and therefore, membrane stability. Data from isolated retina preparations also suggest that glucose availability is an important physiological regulator of SD occurrence and properties.¹⁶

The mechanism of hyperglycemic suppression of SD susceptibility is not known. In both experimental animals and in humans, SD is associated with a rapid surge in glucose utilization that leads to a marked decrease in tissue glucose levels within minutes, ^{7,9,17-22} which can be stepwise cumulative upon repeated exposure.23 Hyperglycemia does increase cerebral glucose availability and diminish the drop in tissue glucose during SD.^{19,24} It is therefore possible that hyperglycemic increase in glucose availability provides an immediate source of substrate for rapidly stimulated glycolysis to help the ATP-dependent pumps guell the stimulus-induced rises in extracellular $[K^+]$, preventing them from reaching the SD threshold. Hyperglycemia may also augment lactate production and lower the tissue pH, thereby suppressing the membrane excitability.9,25 It is unlikely that changes in plasma or tissue osmolarity play a role since mannitol was reportedly ineffective.²⁶ A vascular mechanism is also unlikely because hyperglycemia does not alter the resting blood flow or the hemodynamic response to SD.27

In general, hypoglycemia has been reported to have the opposite effect. For example, insulin-induced hypoglycemia reportedly reduced the KCl concentration threshold for SD by half in rats.¹³ However, glucose levels were not reported, and the increase in SD susceptibility developed a couple of hours after a single dose of insulin, and thus did not appear to temporally correspond to the transient hypoglycemia induced by this method. In another study, hypoglycemia (<75 mg/dL) was associated with higher frequency of peri-infarct SDs in cats.¹⁰ Although in our study hypoglycemia did not appear to enhance SD susceptibility in nonischemic brain, it is possible that depleted glucose pool makes ischemic penumbra more sensitive to hypoglycemia to facilitate peri-infarct SD occurrence. We did not observe spontaneous SD events analogous to anoxic depolarization in any of the hypoglycemic animals,²⁸ but hypoglycemia did delay SD recovery as blood glucose levels were generally below 50 mg/dL.¹² Therefore, the absence of an increase in KCI-induced SD frequency in hypoglycemic rats should be interpreted with caution, because prolonged SDs are expected to limit the SD repetition rate presumably by extending the absolute refractory period during which a subsequent SD could not be triggered. Indeed, the cumulative depolarization duration was significantly prolonged in hypoglycemic rats, suggesting that hypoglycemia can be detrimental in brain injury.

In summary, the inverse relationship between plasma glucose and peri-infarct SD occurrence^{10,11} appears to be at least in part due to a general suppression of SD susceptibility by higher plasma glucose levels, which is observed even in nonischemic brain. Our data suggest that the optimal normoglycemic range in the management of brain injury may be higher than previously targeted. However, hyperglycemia can also be detrimental for injury outcome via unrelated mechanisms,²⁹ and thus cannot be endorsed solely based on these data. Lastly, it is interesting to note that fasting is a commonly quoted trigger for migraine, and diabetes has been reported to abolish or reduce the frequency and severity of migraine attacks.^{30–32} The mechanism of these clinical associations may be plasma glucose modulation of SD susceptibility.

DISCLOSURE/CONFLICT OF INTEREST

The authors declare no conflict of interest.

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