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Optimized gold nanoshell ensembles for biomedical applications

Debabrata Sikdar¹, Ivan D Rukhlenko^{1*}, Wenlong Cheng^{2,3} and Malin Premaratne¹

Abstract

We theoretically study the properties of the optimal size distribution in the ensemble of hollow gold nanoshells (HGNS) that exhibits the best performance at *in vivo* biomedical applications. For the first time, to the best of our knowledge, we analyze the dependence of the optimal geometric means of the nanoshells' thicknesses and core radii on the excitation wavelength and the type of human tissue, while assuming lognormal fit to the size distribution in a real HGN ensemble. Regardless of the tissue type, short-wavelength, near-infrared lasers are found to be the most effective in both absorption- and scattering-based applications. We derive approximate analytical expressions enabling one to readily estimate the parameters of optimal distribution for which an HGN ensemble exhibits the maximum efficiency of absorption or scattering inside a human tissue irradiated by a near-infrared laser.

Keywords: Hollow gold nanoshells, Lognormal distribution, Absorption, Scattering, Biomedical applications

Background

The biocompatibility of gold nanoparticles, along with their tunable plasmon resonances and the ability to accumulate at targeted cancer sites, has proven them to be very effective agents for absorption-based photothermal therapy and scattering-based imaging applications [1-8]. Amongst the commonly used gold nanoparticles, silica-core gold nanoshells exhibit larger photothermal efficiency as compared to gold nanorods of equal number densities [1], whereas hollow gold nanoshells (HGNS) absorb light stronger than the silica-core gold nanoshells do [9,10]. Furthermore, HGNS are comparatively less harmful to healthy tissues neighboring a cancer site [9], which makes them prospective for both photothermal and imaging applications. Although different tissue types and excitation wavelengths were analyzed before to determine the optimal dimensions of a nanoshell [10,11], no optimization has ever been performed for a nanoshell ensemble with a real size distribution. In this Letter, we fill this gap by conducting the first theoretical study of the distribution parameters of the lognormally dispersed HGNS

exhibiting peak absorption or scattering efficiency. In particular, we comprehensively analyze the dependence of these parameters on the excitation wavelength and optical properties of the tissue, giving clear design guidelines.

Methods

Despite a significant progress in nanofabrication technology over the past decade, we are still unable to synthesize large ensembles of almost identical nanoparticles. The nanoparticle ensembles that are currently used for biomedical applications exhibit broad size distributions, which are typically lognormal in shape [12-15]. In an ensemble of single-core nanoshells, both the core radius R and the shell thickness H are distributed lognormally [15], with their occurrence probabilities given by the function [16]

$$f(x; \mu_X, \sigma_X) = \frac{1}{x\sigma_X\sqrt{2\pi}} \exp\left(-\frac{(\ln x - \mu_X)^2}{2\sigma_X^2}\right), \quad (1)$$

where $x = r$ or h is the radius or thickness of the nanoshell, $\mu_X = \ln(\text{Med}[X])$ and σ_X are the mean and standard deviation of $\ln X$, respectively, and $\text{Med}[X]$ is the geometric mean of the random variable $X = R$ or H .

*Correspondence: ivan.rukhlenko@monash.edu

¹Advanced Computing and Simulation Laboratory (ACS), Department of Electrical and Computer Systems Engineering, Monash University, Clayton 3800, Victoria, Australia

Full list of author information is available at the end of the article

The efficiencies of absorption and scattering by a nanoparticle ensemble are the key characteristics determining its performance in biomedical applications. In estimating these characteristics, it is common to use a number of simplifying assumptions. First of all, owing to a relatively large interparticle distance inside human tissue (typically constituting several micrometers [17]), one may safely neglect the nanoparticle interaction and the effects of multiple scattering at them [18,19]. Since plasmonic nanoparticles can be excited resonantly with low-intensity optical sources, it is also reasonable to ignore the nonlinear effects and dipole–dipole interaction between biomolecules [20]. The absorption of the excitation light inside human tissue occurs on a typical length scale of several centimeters, within the near-infrared transparency window of 650 to 1000 nm [21]. However, the attenuation of light does not affect the efficiencies of scattering and absorption by the ensemble, and is therefore neglected in the following analysis. These simplifications allow us to relate the average absorption and scattering efficiencies (S_{abs} and S_{sca}) of the nanoshell ensemble embedded in a tissue to the corresponding efficiencies (Q_{abs} and Q_{sca}) of individual plasmonic nanoshells as

$$S_{\alpha} = \iint Q_{\alpha}(r, h) f(r; \mu_R, \sigma_R) f(h; \mu_H, \sigma_H) dr dh, \quad (2)$$

where $Q_{\alpha}(r, h)$ is expressed through Mie coefficients for a coated sphere [9,22,23], which are the functions of the excitation wavelength, refractive index of the tissue, and permittivities of the nanoshell constituents.

It is seen that the average absorption and scattering efficiencies of a nanoshell ensemble, excited at a fixed wavelength, are functions of the four parameters: $\text{Med}[R]$, $\text{Med}[H]$, σ_R , and σ_H . This poses the problem of finding, and studying the properties of, the optimal distribution parameters for which the nanoshell ensemble exhibits the maximum absorption or scattering efficiency.

Results and discussions

We focus on HGNs with gold permittivity described by the size-dependent model from Ref. [9], and begin by evaluating their average absorption and scattering efficiencies inside a tissue of refractive index $n = 1.55$. Figures 1(a) and 1(b) show these efficiencies in the parametric space of $\text{Med}[R]$ and $\text{Med}[H]$ for $\sigma_R = \sigma_H = 0.5$ and excitation wavelength $\lambda = 850$ nm. Each dependency is seen to exhibit a distinct peak in the form of a flat plateau, which arise predominantly due to the resonant interaction of light with the localized symmetric plasmon modes of the HGNs [9]. The absorption peaks for $\text{Med}[R] \approx 44$ nm and $\text{Med}[H] \approx 9$ nm, while the scattering reaches its maximum for larger and much thicker nanoshells, with $\text{Med}[R] \approx 54$ nm and $\text{Med}[H] \approx 26$ nm. The broadness of the peaks and the associated high tolerance of the

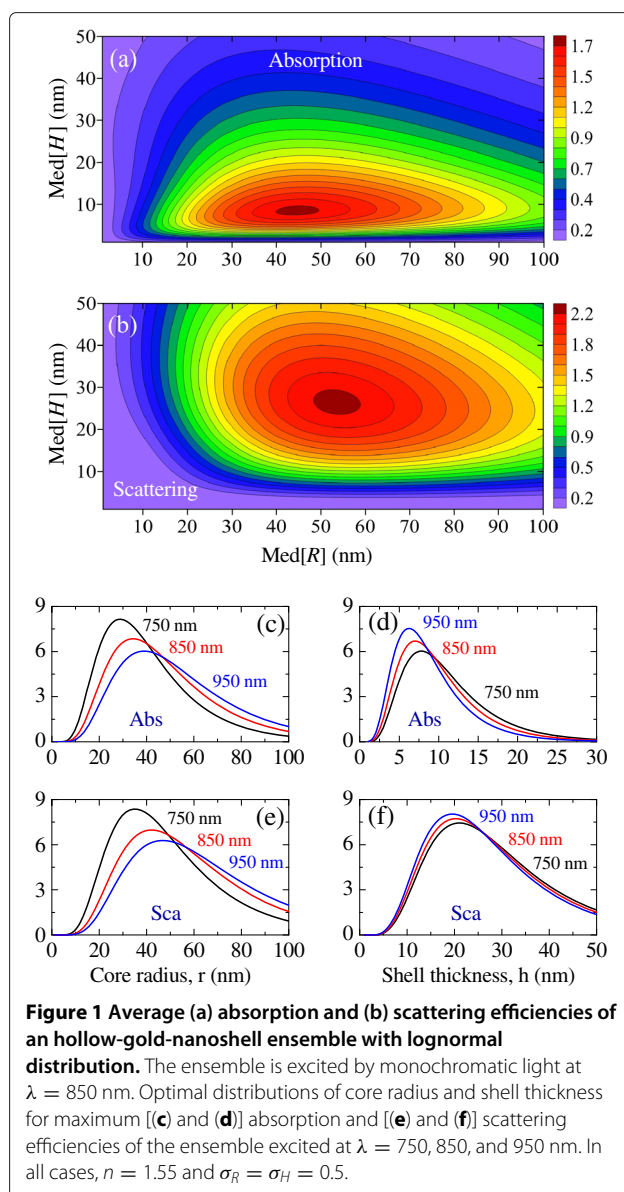


Figure 1 Average (a) absorption and (b) scattering efficiencies of an hollow-gold-nanoshell ensemble with lognormal distribution. The ensemble is excited by monochromatic light at $\lambda = 850$ nm. Optimal distributions of core radius and shell thickness for maximum [(c) and (d)] absorption and [(e) and (f)] scattering efficiencies of the ensemble excited at $\lambda = 750, 850,$ and 950 nm. In all cases, $n = 1.55$ and $\sigma_R = \sigma_H = 0.5$.

nanoshell ensemble to the fabrication inaccuracies are the consequences of size distribution.

The effects of the excitation wavelength on the optimal distributions of the core radius and shell thickness are shown in Figures 1(c)–1(f). Equal σ_R and σ_H ($\sigma_R = \sigma_H = \sigma$) correspond to the situation of similar (scalable) shapes of the two distributions. It is seen that the increase in the excitation wavelength shifts the optimal distribution $f(r; \mu_R, \sigma)$ towards larger radii for both absorption [Figure 1(c)] and scattering [Figure 1(e)]. This trend is opposite to the behavior of the optimal distributions $f(h; \mu_H, \sigma)$ in Figures 1(d) and 1(f), which shifts towards thinner shells with λ . Since the increase in $\text{Med}[R]$ is larger than the reduction in $\text{Med}[H]$, the optimal excitation

of ensembles with larger HGNs require lower-frequency sources.

The optimal geometric means of HGNs' dimensions crucially depend on the shape of size distribution determined by the parameter σ . Figure 2 shows how the optimal distributions of R and H are transformed when σ is increased from 0.1 to 1. As expected, larger σ results in broader distributions that maximize the absorption and scattering efficiencies of the nanoshell ensemble. It also leads to the right skewness of the distributions, thus increasing the fabrication tolerance. At the same time, the increase in σ from 0.1 to 1 reduces the peak values of S_{abs} and S_{sca} by about a factor of 3.5 each. This indicates the need of a compromise between the performance of an HGN ensemble and the fabrication tolerance. Regardless of σ , the ensemble exhibiting the maximum absorption efficiency comprises of HGNs with core radii smaller than those required for maximizing the scattering efficiency. A similar trend exists for the optimal distribution $f(h; \mu_H, \sigma)$, with absorbing nanoshells being much thinner than the scattering ones.

The dependencies of the peak absorption and scattering efficiencies on the excitation wavelength are plotted in Figure 3(a) for $n = 1.55$. The efficiencies are seen to monotonously decrease with λ , which makes shorter-wavelength near-infrared lasers preferable for both absorption- and scattering-based applications. Figures 3(b) and 3(c) show the dispersion of the geometric means for the optimal nanoshell distributions. One can see that the best performance is achieved for the nanoshells of smaller sizes, excited at shorter wavelengths. These results are summarized in the following polynomial fittings of the theoretical curves: $\text{Med}[R] \approx \lambda(21\sigma^2 -$

$61\sigma + 106) - 44\sigma^2 + 72\sigma - 48$ and $\text{Med}[H] \approx \lambda^2(-58\sigma^2 + 65\sigma + 44) + \lambda(103\sigma^2 - 127\sigma - 78) - 56\sigma^2 + 77\sigma + 39$ for absorption, and $\text{Med}[R] \approx \lambda(281\sigma^2 - 409\sigma + 225) - 266\sigma^2 + 376\sigma - 146$ and $\text{Med}[H] \approx \lambda^2(-966\sigma^3 + 1921\sigma^2 - 1150\sigma + 244) + \lambda(1731\sigma^3 - 3439\sigma^2 + 2046\sigma - 430) - 803\sigma^3 + 1607\sigma^2 - 967\sigma + 231$ for scattering. Here λ is expressed in micrometers, $0.1 \leq \sigma \leq 1$, and the accuracy of the geometric means is about ± 1 nm.

The parameters of the optimal lognormal distribution also vary with the type of human tissue. Figures 3(d)–3(f) show such variation for the entire span of refractive indices of human cancerous tissue [9,19], $\lambda = 850$ nm, and three typical shapes of the distribution. It is seen that the peak efficiencies of absorption and scattering by an HGN ensemble grow with n regardless of the shape parameter σ . The corresponding geometric mean of the core radii reduces with n and may be approximated as $\text{Med}[R] \approx n(-51\sigma^2 + 87\sigma - 65) + 72\sigma^2 - 136\sigma + 147$ for absorption, and as $\text{Med}[R] \approx n(-94\sigma^2 + 142\sigma - 87) + 114\sigma^2 - 179\sigma + 178$ for scattering. In contrast, the optimal geometric mean of the shell thicknesses is almost independent of n and approximated by the polynomial $\text{Med}[H] \approx 2\sigma^2 - 3\sigma + 10$ in the case of absorption, and as $\text{Med}[H] \approx 26\sigma^2 - 41\sigma + 40$ in the case of scattering. These expressions allow estimation (with an accuracy of about ± 1 nm) of the optimal distribution parameters of an HGN ensemble excited at $\lambda = 850$ nm for $0.1 \leq \sigma \leq 1$ and $1.35 \leq n \leq 1.7$. Numerical calculations show that the optimal dependencies $\text{Med}[R](n)$ and $\text{Med}[H](n)$ have almost constant slopes for $650 \text{ nm} \leq \lambda \leq 1000 \text{ nm}$. This feature allows one to use Figure 3 to roughly estimate the optimal lognormal distributions of HGNs to be delivered to any human tissue illuminated by a near-infrared laser.

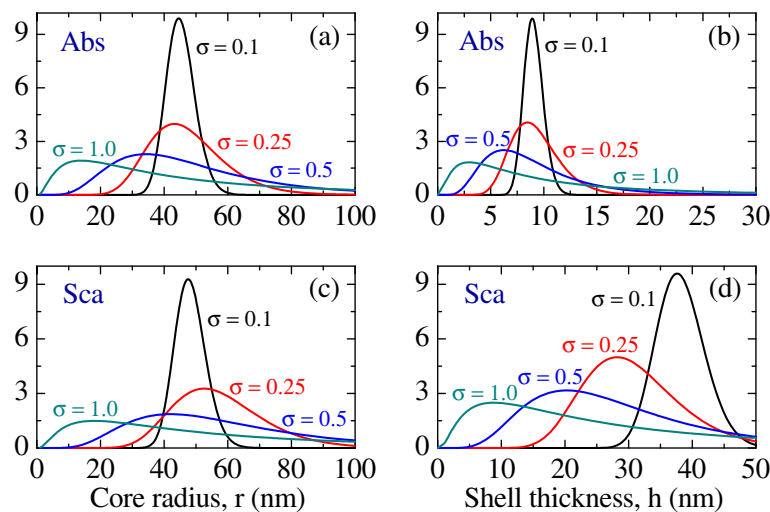


Figure 2 Optimal lognormal distributions of core radius and shell thickness in an ensemble of hollow gold nanoshells exhibiting maximum average [(a) and (b)] absorption and [(c) and (d)] scattering efficiencies for $\sigma = \sigma_R = \sigma_H = 0.1, 0.25, 0.5$, and 1.0 . The simulation parameters are the same as in Figures 1(a) and 1(b).

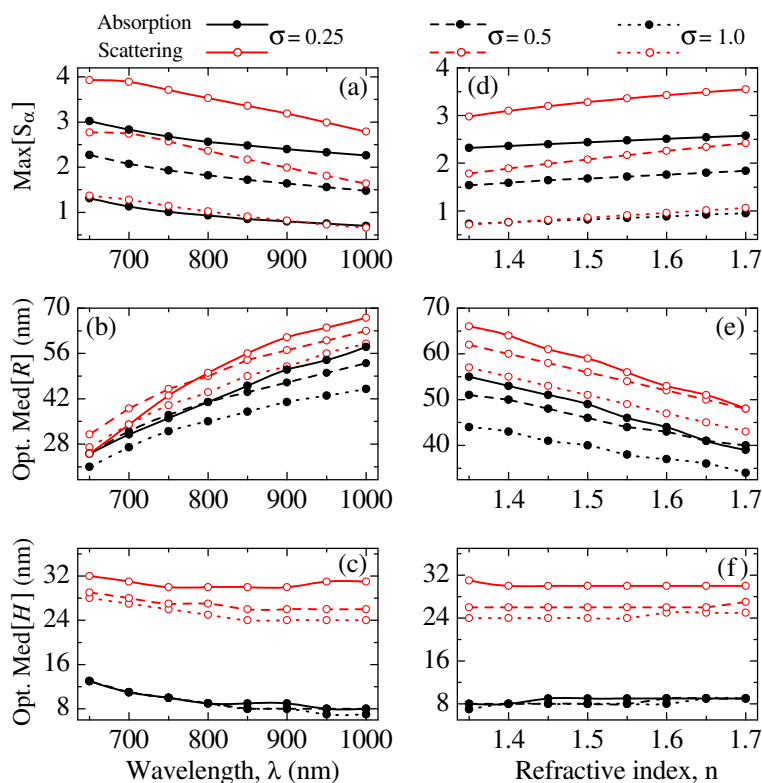


Figure 3 [(a) and (d)] Optimal average absorption (filled circles) and scattering (open circles) efficiencies, and parameters [(b) and (e)] Med[R] and [(c) and (f)] Med[H] of the corresponding optimal distributions as functions of excitation wavelength and tissue refractive index. In (a)–(c), $n = 1.55$; in (d)–(f), $\lambda = 850$ nm. Solid, dashed, and dotted curves correspond to $\sigma = 0.25, 0.5$, and 1.0 , respectively.

Conclusions

In summary, we have studied the optimal distributions of lognormally dispersed hollow gold nanoshells for different excitation wavelengths and human tissues. Shorter-wavelength, near-infrared sources were found to be most effective for *in vivo* biomedical applications. The analytical expressions obtained may be used to estimate the optimal distribution of the nanoshells providing the maximum efficiency of their absorption or scattering of near-infrared radiation inside human tissue.

Abbreviations

HGN: Hollow Gold Nanoshell; Med[X]: Median of the random variable X.

Competing interests

The authors declare that they have no competing interests.

Authors' contributions

IDR, WC, and MP jointly suggested the study conducted by DS. DS conceived the model, performed the simulations, and prepared the manuscript. IDR, WC, and MP supervised the study, participated in the analysis of the results, helped DS to interpret and present the obtained result, and thoroughly edited the manuscript. All authors read and approved the final manuscript.

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Author details

¹Advanced Computing and Simulation Laboratory (A_{CS}L), Department of Electrical and Computer Systems Engineering, Monash University, Clayton 3800, Victoria, Australia. ²Department of Chemical Engineering, Faculty of Engineering, Monash University, Clayton 3800, Victoria, Australia. ³The Melbourne Centre for Nanofabrication, 151 Wellington Road, Clayton 3168, Victoria, Australia.

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