

# Pharmacokinetics of a Multipurpose Pod-Intravaginal Ring Simultaneously Delivering Five Drugs in an Ovine Model

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Multipurpose technologies that simultaneously protect from sexually transmitted infections and unintended pregnancy are urgently needed. Pod-intravaginal rings (IVRs) formulated with the antiretroviral agents (ARVs) tenofovir, nevirapine, and saquinavir and the contraceptives etonogestrel and estradiol were evaluated in sheep. Steady-state concentrations were maintained for 28 days with controlled, sustained delivery. This proof-of-principle study demonstrates that pod IVRs can deliver three ARVs from different mechanistic classes and a progestin-estrogen combination over the wide range needed for putative preventative efficacy.

Unprotected sex can result in unintended pregnancy as well as sexually transmitted infections (STIs) and represents a major health problem worldwide. Multipurpose technologies (MPTs) (1, 2) for simultaneous protection of individuals from sexual HIV infection and unintended pregnancy may save development time and reduce costs in addressing this global health priority. Topical delivery of one or more antiretroviral (ARV) agents in combination with one or more hormonal contraceptives from intravaginal rings (IVRs) holds significant potential as a female-controlled strategy, especially in resource-limited countries (3, 4). In this approach, the active pharmaceutical ingredients (APIs) are administered in a coitally independent, sustained-release formulation that significantly reduces adherence issues compared to daily-pill, ARV vaginal-gel, and coitally dependent regimens.

Multipurpose IVRs need to simultaneously deliver API combinations at independently controlled rates (5). In some cases, multiple drugs will be needed for a single prevention modality. Conventional IVR technologies-i.e., matrix and reservoir rings (3)—contain the API(s) homogeneously dispersed, either in solution or as a suspension, in the elastomer backbone that makes up the ring. This approach complicates the development of combination IVRs, which partially explains why, to date, all IVRs have delivered one or two APIs (3, 4). With the above parameters in mind, we have developed a novel IVR platform (referred to as "pod IVR") that can simultaneously deliver multiple drugs in a modular fashion (6). The polymer-coated drug cores, referred to as pods, are embedded in an unmedicated ring. This approach leads to a number of important benefits, discussed in detail elsewhere (6, 7). In the context of combination IVRs as an MPT, the pod IVR design readily enables the delivery of 3 or more drugs from a single device, as described below.

The primary purpose of this proof-of-concept study is to demonstrate that 3 ARV drugs from different mechanistic classes can be delivered in tandem with a progestin-estrogen combination from a novel multipurpose IVR at independently controlled release rates.

## MATERIALS AND METHODS

**Production of intravaginal rings.** Silicone pod IVRs (Fig. 1) were produced according to published methods (6) and contained two pods of

each drug per ring: tenofovir (TFV), nevirapine (NVP), saquinavir (SQV), and estradiol (E2) at 16 mg API per pod (32 mg drug per ring) and etonogestrel (ETG) at 10 mg API per pod (20 mg drug per ring). The pod membrane consisted of poly(vinyl alcohol), and three 2-mm delivery channels per pod were mechanically fashioned in the IVR (6).

**Study design.** *In vivo* studies were performed with 3 sheep according to methods described previously (5, 8) at the University of Texas Medical Branch (UTMB) in Galveston, TX, with approval from the Institutional Animal Care and Use Committee. Note that the sheep estrus cycle likely was suppressed by the simultaneous administration of E2 and ETG from the IVR. No significant changes in the weight of the animals or unusual vaginal discharges were observed over the course of the study.

Sample collection, processing, and analysis. Vaginal rings were inserted on day 0, and cervicovaginal lavage (CVL) samples were collected at predetermined time points (days 7, 14, 21, and 28) (Fig. 2) using published methods (5). Briefly, CVL was collected by gently infusing phosphate-buffered saline solution (10 ml) into the vaginal vault via a sterile 10-ml syringe attached to a sterile pediatric Foley catheter (size, 5 or 8 French units) of adjusted length. The resulting CVL fluid was drawn out with the same device. Vaginal tissue samples were obtained by biopsy on day 14. Samples were processed, stored, and transported as described previously (5). Bioanalysis was performed by liquid chromatographymass spectrometry (LC-MS), and detailed methods are given in the supplemental material. For CVL, the lower limits of quantitation (LLOQs) were as follows: TFV, 17 nM (5 ng ml<sup>-1</sup>); NVP, 9 nM (2.5 ng ml<sup>-1</sup>); SQV, 8 nM (5 ng ml<sup>-1</sup>); ETG, 31 nM (10 ng ml<sup>-1</sup>); and E2, 2 nM (0.5 ng ml<sup>-1</sup>). For tissue, the LLOQs were as follows: TFV,  $2 \text{ nM} (0.5 \text{ ng g}^{-1})$ ; NVP, 4 nM(1 ng g $^{-1}$ ); SQV, 8 nM (5 ng g $^{-1}$ ); ETG, 3 nM (1 ng g $^{-1}$ ); and E2, 2 nM  $(0.5 \text{ ng g}^{-1})$ . The run-to-run coefficient of variation (9) for all methods

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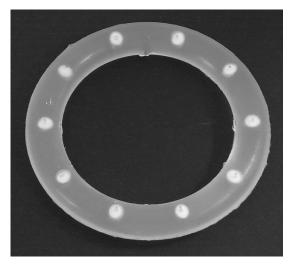


FIG 1 Photograph of a 10-pod IVR sized for use in humans (outer diameter, 56 mm; inner diameter, 40 mm; cross-section, 8 mm).

was below 10%. A total of 75 measurements were made (3 sheep  $\times$  5 samples per sheep  $\times$  5 drug levels).

#### RESULTS

Cervicovaginal lavage (CVL) concentrations (Fig. 2) were constant over the 28 days, indicating that steady state had been maintained and that sustained release of all five drugs was achieved in a controlled fashion over the length of the study. Tenofovir (TFV) CVL levels  $(7.7 \times 10^3 \pm 6.1 \times 10^3$  nM [median  $\pm$  standard deviation]) were the highest of the five drugs, as expected based on their aqueous solubilities. Nevirapine (NVP) and saquinavir (SQV) CVL concentrations (93  $\pm$  141 nM and 36  $\pm$  79 nM, respectively; 28-day median  $\pm$  standard deviation) were qualitatively similar for the duration of the study (Fig. 2). Median etonogestrel (ETG) CVL levels (13  $\pm$  6.9 nM) were 8 times higher than the corresponding estradiol (E2) levels (1.6  $\pm$  1.2 nM). These steady-state drug levels span nearly four orders of magnitude.

Vaginal tissue drug levels measured on day 14 are compared with the corresponding CVL drug concentrations in Table 1. The drugs partitioned from the lumen into the vaginal tissues accord-

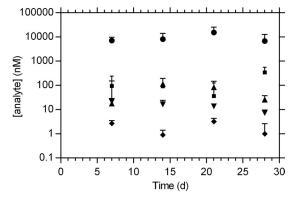


FIG 2 Cervicovaginal lavage concentrations (median + SD) of 5 drugs delivered simultaneously via combination pod IVRs over 28 days in sheep (n = 3). Circles, TFV; squares, NVP; triangles, SQV; inverted triangles, ETG; diamonds, E2.

TABLE 1 Day 14 drug distribution and concentrations across key
pharmacokinetic compartments in sheep $(n = 3)$ following
simultaneous administration from combination 5-drug pod IVRs

Drug	Concn (nM) <sup><i>a</i></sup>		Tissue-to-CVL
	Cervicovaginal lavage	Vaginal tissue <sup>b</sup>	ratio
Tenofovir (TFV)	$8.2\times10^3\pm5.9\times10^3$	$20\times10^3\pm9.4\times10^3$	2.4
Nevirapine (NVP)	92 ± 14	$92\times10^3\pm20\times10^3$	$1.0 \times 10^3$
Saquinavir (SOV)	$0.11\times 10^3\pm 78$	$8.1\times10^3\pm4.1\times10^3$	71
Etonogestrel (ETG)	$17 \pm 7.2$	$1.1\times10^3{\pm}~1.6\times10^3$	65
Estradiol (E2)	$0.87\pm0.55$	$1.1\times10^3\pm6.5\times10^3$	$1.2 \times 10^3$

<sup>*a*</sup> Median  $\pm$  standard deviation.

<sup>b</sup> Based on the assumption that vaginal tissue has a density of 1 g ml<sup>-1</sup> (24).

ing to the following trend (i.e., tissue-to-CVL ratios): E2  $\sim$  NVP > SQV  $\sim$  ETG > TFV.

#### DISCUSSION

One of the primary challenges associated with developing an MPT for the prevention of both sexual HIV infection and unintended pregnancy is that multiple APIs need to be incorporated into a single product. The challenge is further compounded if multiple APIs per prevention modality are required for it to be efficacious. In the case of contraception using IVRs, progestin-estrogen combinations have demonstrated superior clinical efficacy over devices delivering only progestin (10). Several large multicenter trials evaluating a matrix IVR delivering the progestin levonorgestrel found pregnancy rates at 12 months between 3.7% (11) and 5.1% (12). In contrast, the NuvaRing, which delivers a combination of ETG and ethinyl estradiol, demonstrated clinical efficacy in excess of 99% in Europe and in the United States (13–15).

A combination of multiple ARV agents, preferably targeting different phases in the HIV infection cycle, is likely to provide more efficient protection than a single drug (16, 17). As a result, an efficacious multipurpose IVR for female-controlled prevention of HIV infection and unintended pregnancy requires delivery of at least four APIs.

Matrix and reservoir IVR technologies have demonstrated that up to two APIs can be delivered from a single device (3, 4). The technical hurdles in developing and manufacturing IVRs based on these technologies, including segmented designs (4), that deliver five APIs simultaneously and at individually controlled rates appear daunting. To this end, we have developed a novel pod IVR technology where solid API drug cores are coated with biocompatible polymer membranes to afford the so-called pods, which are subsequently embedded an inert elastomer ring (6). An IVR sized for human use can support up to 10 pods, and each pod can theoretically contain a different API being released at an independently controlled rate.

In this proof-of-principle study, we developed a 5-drug pod IVR containing two pods of each API and evaluated the device in sheep. Three ARV agents from different mechanistic classes were used in combination, including TFV, a nucleoside reverse transcriptase inhibitor (NRTI) under clinical evaluation in a vaginal gel for HIV prevention (18, 19); NVP, a non-NRTI in the same class as dapivirine, which is being evaluated as an IVR formulation in a large multinational clinical trial (http://www .mtnstopshiv.org/news/studies/mtn020); and SQV, a protease inhibitor that has not been used previously in a topical vaginal formulation but that has shown promise as a microbicide by blocking viral maturation and transmission of HIV-1 at mucosal surfaces (20). The remaining two APIs in our novel IVR were ETG and E2 for contraception.

Here we have demonstrated that our pod IVR released five drugs at the approximate relative rates hypothesized for an effective device, affording CVL levels in the following decreasing order: TFV > NVP  $\sim$  SQV > ETG > E2. High intraluminal TFV levels are known to be required for effective HIV prevention (21). Median TFV CVL levels over the course of this study were  $7.7 \times 10^3$ nM ( $2.2 \times 10^3$  ng ml<sup>-1</sup>). A previous study in the same breed of sheep using an identical CVL collection method found that drug concentration measured in CVL is diluted approximately  $10 \times$  to  $50 \times$  relative to cervicovaginal fluid (CVF) levels (5). Based on this dilution range, we estimate that the median 2.2 imes10<sup>3</sup> ng ml<sup>-1</sup> CVL levels measured in sheep are comparable to the 10<sup>5</sup> ng ml<sup>-1</sup> median 24-h CVF concentrations observed in women following exposure to 4 ml 1% TFV gel (22), shown to be protective clinically (18). Median 24-h TFV tissue levels in a 1% TFV gel clinical study were  $24 \times 10^3$  nM (7 × 10<sup>3</sup> ng ml<sup>-1</sup>) (22), while the median day 14 vaginal tissue TFV concentration in our sheep study was  $20 \times 10^3$  nM (5.6  $\times 10^3$  ng ml<sup>-1</sup>). The 50% inhibitory concentrations (IC<sub>50</sub>s) of NVP (10 to 100 nM) (http://www.accessdata.fda.gov/drugsatfda\_docs/label/2005/2 0636s025,20933s014lbl.pdf) and SOV (1 to 30 nM) (http: //www.accessdata.fda.gov/drugsatfda\_docs/label/2003/20828s 015ppi.pdf) are similar and several orders of magnitude lower than those of TFV (0.04 to  $8.5 \times 10^3$  nM) (23), suggesting that the observed tissue levels for all three ARV agents are an appropriate starting point in developing a safe and effective MPT product. Vaginal lumen levels of ETG were 8 times higher than the corresponding E2 concentrations, in agreement with the relative daily release rates of ETG and EE from the NuvaRing (120  $\mu$ g day<sup>-1</sup> and 15  $\mu$ g day<sup>-1</sup>, respectively) (14).

The flexible design of the pod IVR platform has been discussed in detail in terms of accelerated development as well as ease and cost effectiveness of manufacturing (6, 7). Multiple degrees of freedom in the control of delivery (i.e., pod polymer membrane, number of pods, delivery channel number, and cross-sectional area) allow release rates to be rapidly titrated to target levels, and established *in vitro-in vivo* correlation models (5, 7, 8) minimize the number of required animal studies in preclinical development. Here, proof of principle for an MPT based on a 5-drug IVR was demonstrated. Future studies will need to rationally select the most appropriate drug combinations and target pharmacokinetic parameters (target drug levels in key anatomic compartments) that will lead to favorable health outcomes.

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### REFERENCES

- Friend DR, Doncel GF. 2010. Combining prevention of HIV-1, other sexually transmitted infections and unintended pregnancies: development of dual-protection technologies. Antiviral Res. 88:S47–S54.
- Friend DR. 2012. Drug delivery in multiple indication (multipurpose) prevention technologies: systems to prevent HIV-1 transmission and unintended pregnancies or HSV-2 transmission. Expert Opin. Drug Deliv. 9:417–427.
- Malcolm RK, Edwards KL, Kiser P, Romano J, Smith TJ. 2010. Advances in microbicide vaginal rings. Antiviral Res. 88:S30–S39.
- Kiser PF, Johnson TJ, Clark JT. 2012. State of the art in intravaginal ring technology for topical prophylaxis of HIV infection. AIDS Rev. 14:62–77.
- Moss JA, Malone AM, Smith TJ, Kennedy S, Kopin E, Nguyen C, Gilman J, Butkyavichene I, Vincent KL, Motamedi M, Friend DR, Clark MR, Baum MM. 2012. Simultaneous delivery of tenofovir and acyclovir via an intravaginal ring. Antimicrob. Agents Chemother. 56:875–882.
- Baum MM, Butkyavichene I, Gilman J, Kennedy S, Kopin E, Malone AM, Nguyen C, Smith TJ, Friend DR, Clark MR, Moss JA. 2012. An intravaginal ring for the simultaneous delivery of multiple drugs. J. Pharm. Sci. 101:2833–2843.
- Moss JA, Malone AM, Smith TJ, Butkyavichene I, Cortez C, Gilman J, Kennedy S, Kopin E, Nguyen C, Sinha P, Hendry RM, Guenthner P, Holder A, Martin A, McNicholl J, Mitchell J, Pau C-P, Srinivasan P, Smith JM, Baum MM. 2012. Safety and pharmacokinetics of intravaginal rings delivering tenofovir in pig-tailed macaques. Antimicrob. Agents Chemother. 56:5952–5960.
- Moss JA, Baum MM, Malone AM, Kennedy S, Kopin E, Nguyen C, Gilman J, Butkyavichene I, Willis R, Vincent KL, Motamedi M, Smith TJ. 2012. Tenofovir and tenofovir disoproxil pharmacokinetics from intravaginal rings. AIDS 26:707–710.
- 9. Snyder LR, Kirkland JJ, Glajch JL. 1997. Practical HPLC method development, 2nd ed. John Wiley & Sons, Inc., New York, NY.
- Brache V, Faundes A. 2010. Contraceptive vaginal rings: a review. Contraception 82:418-427.
- 11. Koetsawang S, Ji G, Krishna U, Cuadros A, Dhall GI, Wyss R, Rodriquex la Puenta J, Andrade ATL, Khan T, Kononova ES, Lawson JP, Parekh U, Elstein M, Hingorani V, Na-ning W, Zhong-beng Y, Landgren B-M, Boukhris R, Li-lan L, Boccard S, Machin D, Pinol A, Rowe PJ. 1990. Microdose intravaginal levonorgestrel contraception: a multicenter clinical trial. 1. Contraceptive efficacy and side-effects. Contraception 41:105–124.
- Sahota J, Barnes PMF, Mansfield E, Bradley JL, Kirkman RJE. 1999. Initial UK Experience of the levonorgestrel-releasing contraceptive intravaginal ring. Adv. Contracept. 15:313–324.
- 13. Roumen F. 2002. Contraceptive efficacy and tolerability with a novel combined contraceptive vaginal ring, NuvaRing. Eur. J. Contracept. Reprod. Health Care 7:19–24.
- Oddsson K, Leifels-Fischer B, de Melo NR, Wiel-Masson D, Benedetto C, Verhoeven CHJ, Dieben TOM. 2005. Efficacy and safety of a contraceptive vaginal ring (NuvaRing) compared with a combined oral contraceptive: a 1-year randomized trial. Contraception 71:176–182.
- Madden T, Blumenthal P. 2007. Contraceptive vaginal ring. Clin. Obstet. Gynecol. 50:878–885.
- Garcia-Lerma JG, Otten RA, Qari SH, Jackson E, Cong ME, Masciotra S, Luo W, Kim C, Adams DR, Monsour M, Lipscomb J, Johnson JA, Delinsky D, Schinazi RF, Janssen R, Folks TM, Heneine W. 2008. Prevention of rectal SHIV transmission in macaques by daily or intermittent prophylaxis with emtricitabine and tenofovir. PLoS Med. 5:291–299.
- Balzarini J, Van Damme L. 2007. Microbicide drug candidates to prevent HIV infection. Lancet 369:787–797.
- Karim QA, Karim SSA, Frohlich JA, Grobler AC, Baxter C, Mansoor LE, Kharsany ABM, Sibeko S, Mlisana KP, Omar Z, Gengiah TN, Maarschalk S, Arulappan N, Mlotshwa M, Morris L, Taylor D. 2010. Effectiveness and safety of tenofovir gel, an antiretroviral microbicide, for the prevention of HIV infection in women. Science 329:1168– 1174.
- 19. Karim SSA, Karim QA. 2011. Antiretroviral prophylaxis: a defining moment in HIV control. Lancet 378:e23–e25.

- 20. Stefanidou M, Herrera C, Armanasco N, Shattock RJ. 2012. Saquinavir inhibits early events associated with establishment of HIV-1 infection: potential role for protease inhibitors in prevention. Antimicrob. Agents Chemother. 56:4381–4390.
- 21. Karim SSA, Kashuba ADM, Werner L, Karim QA. 2011. Drug concentrations after topical and oral antiretroviral pre-exposure prophylaxis: implications for HIV prevention in women. Lancet 378:279–281.
- 22. Schwartz JL, Rountree W, Kashuba ADM, Brache V, Creinin MD, Poindexter A, Kearney BP. 2011. A multi-compartment, single and multiple dose

pharmacokinetic study of the vaginal candidate microbicide 1% tenofovir gel.
PLoS One 6:e25974. doi:10.1371/journal.pone.0025974.
23. Gilead Sciences, Inc. 2012. Product monograph. <sup>Pr</sup>Viread<sup>®</sup> (tenofovir

- Gilead Sciences, Inc. 2012. Product monograph. <sup>Pr</sup>Viread<sup>®</sup> (tenofovir disoproxil fumarate tablets) 300 mg antiretroviral agent. Gilead Sciences, Inc., Foster City, CA.
- 24. Nuttall J, Kashuba A, Wang R, White N, Allen P, Roberts J, Romano J. 2012. The pharmacokinetics of tenofovir following intravaginal and intrarectal administration of tenofovir gel to rhesus macaques. Antimicrob. Agents Chemother. 56:103–109.