

Online Submissions: http://www.wjgnet.com/esps/ wjg@wjgnet.com doi:10.3748/wjg.v19.i30.4841 World J Gastroenterol 2013 August 14; 19(30): 4841-4849 ISSN 1007-9327 (print) ISSN 2219-2840 (online) © 2013 Baishideng, All rights reserved.

EDITORIAL

Acoustic radiation force impulse of the liver

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Telephone: +39-45-8124140 Fax: +39-45-8277808 Received: January 8, 2013 Revised: April 15, 2013 Accepted: July 17, 2013

Published online: August 14, 2013

Abstract

Acoustic radiation force impulse (ARFI) imaging is a new and promising ultrasound-based diagnostic technique that, evaluating the wave propagation speed, allows the assessment of the tissue stiffness. ARFI is implemented in the ultrasound scanner. By short-duration acoustic radiation forces (less than 1 ms), localized displacements are generated in a selected region of interest not requiring any external compression so reducing the operator dependency. The generated wave scan provides qualitative or quantitative (wave velocity values) responses. Several non-invasive methods for assessing the staging of fibrosis are used, in order to avoid liver biopsy. Liver function tests and transient elastography are non-invasive, sensitive and accurate tools for the assessment of liver fibrosis and for the discrimination between cirrhotic and non-cirrhotic liver. Many published studies analyse ARFI performance and feasibility in studying diffuse liver diseases and compare them to other diagnostic imaging modalities such as conventional ultrasonography and transient elastography. Solid focal liver lesions, both benign and malignant, are common findings during abdominal examinations. The accurate characterization and differential diagnosis are important aims of all the imaging

modalities available today. Only few papers describe the application of ARFI technology in the study of solid focal liver lesions, with different results. In the present study, the existing literature, to the best of our knowledge, about ARFI application on diffuse and focal liver pathology has been evaluated and results and statistical analyses have been compared, bringing to the conclusion that ARFI can be used in the study of the liver with similar accuracy as transient elastography in diagnosing significant fibrosis or cirrhosis and has got some advantages in respect to transient elastography since it does not require separate equipment, better displays anatomical structures and measurements can be successfully carried out almost in every patient.

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Key words: Acoustic radiation force impulse imaging; Sonoelastography; Diffuse liver pathology; Focal liver lesion

Core tip: In the present study, the existing literature, to the best of our knowledge, about acoustic radiation force impulse (ARFI) application on diffuse and focal liver pathology has been evaluated and results and statistical analyses have been compared, bringing to the conclusion that ARFI can be used in the study of the liver with similar accuracy than transient elastography in diagnosing significant fibrosis or cirrhosis and has got some advantages in respect to transient elastography since it does not require separate equipment, better displays anatomical structures and measurements can be successfully carried out almost in every patient.

D'Onofrio M, Crosara S, De Robertis R, Canestrini S, Demozzi E, Gallotti A, Pozzi Mucelli R. Acoustic radiation force impulse of the liver. *World J Gastroenterol* 2013; 19(30): 4841-4849 Available from: URL: http://www.wjgnet.com/1007-9327/full/v19/ i30/4841.htm DOI: http://dx.doi.org/10.3748/wjg.v19.i30.4841



INTRODUCTION

Acoustic radiation force impulse (ARFI) imaging is a new and promising ultrasound-based diagnostic technique that, evaluating the wave propagation speed, allows the assessment of the tissue stiffness^[1-3]. ARFI is implemented in the ultrasound scanner and by using a conventional probe, without any need for external compression so reducing the operator dependency, it evaluates deep tissues stiffness providing complementary informations potentially useful for the diagnosis^[1-6]. By short-duration acoustic radiation forces (less than 1 ms), it generates localized displacements in a selected region of interest (ROI; a box with dimension of $1 \text{ cm} \times 0.5 \text{ cm}$, identified on a conventional B-mode (Figure 1) image^[7,8]. Depending on the interactions with the transducer^[8,9], the generated wave scan provides qualitative (imaging) or quantitative (wave velocity values, measured in m/s) responses, by Virtual Touch Tissue Imaging and Virtual Touch Tissue Quantification, respectively (Siemens, Erlangen, Germany).

DIFFUSE LIVER DISEASES

Biopsy provides an extremely valuable contribution to the assessment of liver status in the case of chronic disease, offering information both on fibrosis and necroinflammatory activity. However, not only the risk of complications, which have been reported with a frequency of 5%-20% for minor complications and 0.3%-0.5% for major complications^[10] including also exceptional cases of death, but also contraindications, such as coagulopathy, poor patients cooperation or lack of consent, tend to limit its use, especially for repeated use over time. Furthermore, insufficient sampling and inter-observer variability may occur^[11].

Considerable efforts have been made to develop noninvasive methods for assessing the staging of fibrosis, in order to avoid liver biopsy. In this setting the ideal method should be simple, inexpensive, easily available, repeatable and accurate.

Liver function tests [alanine aminotransferase (ALT), aspartate aminotransferase (AST), total proteins, serum albumin, gamma-globulins, gamma glutamyl transpeptidase (GGT), total bilirubin, alkaline phosphatase, prothrombin time/international normalized ratio] can be performed prior to the liver biopsy. The 2 main scoring systems used to predict and evaluate liver fibrosis are AST-platelet ratio index (AST level and platelet count) and FIBROMAX (Biopredictive, France) that combines the measurement of 10 indirect parameters adjusted for age, sex, weight and height: α 2-macroglobulin, haptoglobin, apolipoprotein A1, total bilirubin, GGT, ALT, AST, fasting glucose, triglycerides and total cholesterol.

Transient elastography (TE) (Fibroscan, Echosense, Paris, France) has proved to be a non-invasive, sensitive and accurate tool for the assessment of liver fibrosis and particularly for the discrimination between cirrhotic and non-cirrhotic liver and its use is rapidly spreading. However, since it requires separate equipment, it means that

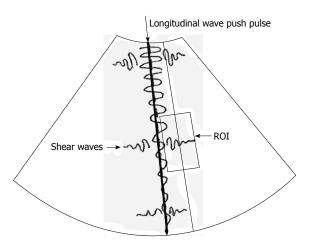


Figure 1 Acoustic radiation force impulse virtual touch tissue quantification technical scheme. ROI: Region of interest.

at least one other examination is necessary in addition to conventional ultrasonography (US) of the liver, requiring additional time and costs after B-mode ultrasonography. Moreover, during TE examination, only A-mode imaging is displayed on the screen in order to select the area of scanning and, consequently, ligaments, vascular structures or even lesions, may inadvertently be included in the ROI, possibly affecting the final results.

ARFI imaging offers the possibility of performing a quantitative measurement of the elasticity of the hepatic parenchyma during conventional US evaluations, without requiring additional transducers or other equipment^[7].

Many studies analyse ARFI performance in studying diffuse liver diseases. Piscaglia *et al*^[12] show that Virtual Touch Tissue Quantification is able to identify the presence of cirrhosis with good accuracy and produces results correlated with those obtained by transient elastography with Fibroscan. They performed measurement in the right lobe, by means of an intercostal scan, a condition which offers high inter-observer reproducibility (r = 0.874 in their series^[12]).

The great advantage of fibrosis assessment using Virtual Touch Tissue Quantification is the fact that it can be performed at the same time as conventional US investigation. US is routinely used worldwide in the management of patients with chronic liver disease and is the first imaging technique employed when liver disease is suspected. With conventional US, certain features are highly specific for predicting severe fibrosis or cirrhosis (surface nodularity: specificity 95%; caudate lobe hypertrophy: 91%), but are not very sensitive (sensitivity of 54% and 41% respectively)^[13]. Piscaglia *et al*^{12]} affirm that results in performing ARFI imaging have found to be similar to those of other works, all of which showed an area under the receiver operating characteristic curve (AUROC) above 0.9 for the diagnosis of cirrhosis with a cut-off value of 1.77 m/s (sensitivity 93%, specificity 85.1%). This cut-off value is very similar to those reported by Friedrich-Rust et al^[7] (1.75 m/s), Sporea et al^[14] and Takahashi et $al^{[15]}$, but differs from the ones obtained

Ref.	Value (m/s)
The right lobe of healthy liver	
Eiler <i>et al</i> ^[33]	1.16
Sporea <i>et al</i> ^[48]	1.19
Karlas et al ^[49]	1.19
Jaffer <i>et al</i> ^[50]	1.12
Marginean <i>et al</i> ^[51]	1.18 ± 0.27
Crespo et al ^[52]	1.06
Kircheis <i>et al</i> ^[53]	1.09 ± 0.13
Yoon <i>et al</i> ^[54]	1.06
Colombo <i>et al</i> ^[18]	1.40
Sporea <i>et al</i> ^[55]	1.28 ± 0.43
Noruegas <i>et al</i> ^[56]	1.11
Rizzo et al ^[57]	0.99
Karlas et al ^[58]	1.15 ± 0.17
Sporea <i>et al</i> ^[59]	0.97 ± 0.19
Son <i>et al</i> ^[60]	1.07 ± 0.11
Rifai <i>et al</i> ^[61]	1.10 ± 0.17
Kuroda <i>et al</i> ^[62]	0.99 ± 0.21
Popescu <i>et al</i> ^[63]	1.15 ± 0.21
Piscaglia et al ^[12]	1.13
Toshima <i>et al</i> ^[64]	1.15
Horster <i>et al</i> ^[65]	1.19
Goertz <i>et al</i> ^[66]	1.16 ± 0.11
Goertz et al ^[35]	1.09
D'Onofrio <i>et al</i> ^[32]	1.56
Fierbinteanu-Braticevici <i>et al</i> ^[17]	< 1.185 (cut-off)
Friedrich-Rust <i>et al</i> ^[7]	1.10
A liver with severe fibrosis (> F3)	
Ye <i>et al</i> ^[67]	1.69
Sporea <i>et al</i> ^[48]	1.43
Karlas <i>et al</i> ^[49]	1.43
Chen <i>et al</i> ^[68]	2.43 ± 0.13
Sporea <i>et al</i> ^[69]	1.60 ± 0.49 HBV; 1.55 ± 0.63 HCV
Crespo et al ^[52]	1.77
Kircheis <i>et al</i> ^[53]	1.44 + 0.26
Yoon <i>et al</i> ^[54]	1.89
Friedrich-Rust <i>et al</i> ^[70]	1.55
Colombo <i>et al</i> ^[18]	1.44
Sporea <i>et al</i> ^[55]	1.64 ± 0.51
Noruegas <i>et al</i> ^[56]	1.48
Rizzo <i>et al</i> ^[57]	1.70
Karlas <i>et al</i> ^[58]	1.70 if non-viral
Sporea <i>et al</i> ^[59]	1.71 ± 0.52
Kuroda <i>et al</i> ^[62]	1.61 ± 0.79 F3; 2.35 ± 1.11 F4
Toshima <i>et al</i> ^[64]	1.88
Sporea <i>et al</i> ^[21]	1.78 ± 0.77
Fierbinteanu-Braticevici <i>et al</i> ^[17]	> 1.54 (cut-off)
Takahashi <i>et al</i> ^[15]	2.57 ± 0.52 mean value for F4
	(cut-off > F3 = 1.44)
Lupsor <i>et al</i> ^[16]	1.520 ± 0.575
Friedrich-Rust <i>et al</i> ^[7]	1.64

Table 1 Mean wave propagation velocity values

HBV: Hepatitis B virus; HCV: Hepatitis C virus.

in other studies^[16,17] that reported slightly higher thresholds. In their series the good performance of the ARFI technique with the previously reported cut-off value was also confirmed by the testing in a population with cirrhosis proven by biopsy as the reference standard.

Other works compare ARFI imaging to TE by means of Fibroscan, such as the one from Colombo *et al*^[18]. They similarly found that TE and ARFI are both highly effective in diagnosing cirrhosis, but they came to the conclusion that TE is probably more accurate in predict-

ing significant fibrosis (AUROC of TE 0.897, AUROC of ARFI 0.815), although they could not demonstrate a statistically significant difference between the two curves. Their results were consistent with Boursier *et al*^[19] and Lupsor *et al*^[16] who found the same diagnostic accuracy for cirrhosis, but better performance of TE in predicting significant fibrosis (F2 or higher), but were at variance with three studies which instead found similar accuracies of TE and ARFI in diagnosing significant fibrosis^[7,20,21].

Another interesting finding was that Virtual Touch Tissue Quantification measurements could be successfully carried out in all patients enrolled^[12], while TE was unsuccessful in 7% of cases (*e.g.*, in patients with narrow intercostal spaces and in those with morbid obesity), as reported also in literature^[22-26]. A possible explanation for this is that Virtual Touch Tissue Quantification may not be limited by narrow intercostal spaces or even by moderate excess weight, as it only requires the visible liver is not deeper than a fixed distance from the skin surface (in order to put the ROI in the parenchyma), while with TE the liver must not be more than 25 mm from the skin.

Regarding steatosis and inflammatory changes in diffuse liver disease, there is no agreement in the possible use of ARFI in diagnosing these parenchymal changes and in the effects of these changes themselves on ARFI measurements^[20,27,28]. It seems unlikely that changes that minimally affect the parenchymal stiffness will be at this moment accurately depicted and diagnosed by using this non invasive technique.

NORMAL AND PATHOLOGICAL VALUES

Mean normal values and mean values indicating severe fibrosis (Table 1) range about 0.8-1.7 m/s (Figure 2A) and about 1-3.4 m/s (Figure 2B) respectively.

Fierbinteanu-Braticevici *et al*^[17] demonstrated that ARFI elastography could predict fibrosis of F2 META-VIR stage or higher with a validity of 90.2%. They calculated the optimal cut-off point between stages F1 and F2 to be 1.21 m/s. At this value, ARFI elastography had a sensitivity of 89.4% and a specificity of 100%. In their work, they also demonstrated that ARFI can predict even better F3 and F4 stage fibrosis. The optimal cut-off value to identify fibrosis stage F3 or higher was 1.54 m/s, with sensitivity and specificity of 97% and 100% respectively. The optimal cut-off value in predicting cirrhosis (stage F4) was 1.94 m/s with a sensitivity of 100% and a specificity of 98.1%.

In chronic viral hepatitis, the knowledge of the stage of liver fibrosis is important for prognosis and for decisions about antiviral treatment^[29]. Fibrosis staged higher than F2 is an indicator for antiviral treatment, hence the great therapeutic value of a highly accurate diagnostic test. Moreover, early detection of significant fibrosis (F3 or higher) is essential since patients with significant fibrosis are at high risk of developing complications, such as portal hypertension or hepatocellular carcinoma, and consequently need specific follow-up^[17]. D'Onofrio M et al. Acoustic radiation force impulse of the liver



Figure 2 Acoustic radiation force impulse imaging of the liver. A: Normal value in healthy liver. B: Cirrhosis. C: Outlier value in healthy liver.

At present, it's difficult to determine the real impact of ARFI in the early diagnosis of hepatic fibrosis^[17,27]. According to Fierbinteanu-Braticevici *et al*^[17], in fact, there is a values overlap between F0-F1 and F2 fibrosis stages. The increase in liver propagation velocity has been demonstrated to be more important between stages F2 and F3 than between F1 and F2. This is consistent with the fact that the increase in fibrous tissue is more important between stages F2 and F3 than between F1 and F2. This limit of ARFI was overcome by the fact that fibrosis staged F2 or higher is considered a hallmark of progressive liver disease, therefore these are the patients in which there is a stronger indication for treatment as compared with patients with no or mild fibrosis^[30,31].

There is in fact a range of variability of normal and pathological values in the Literature (Table 1). So what is important is to give the correct task to this new technique at present. The correct use of this technique has to be based on the true possibility of this system to detect changes in liver stiffness related to the development of different amount of fibrosis. The risk that absolutely should be avoided is to overestimate pathology and to look for inconsistent diseases. Therefore, in conclusion, the normal cut-off values must not be too strict but perhaps they also have to be adapted from time to time in relation to clinical and technical setting and from measurement to measurement.

In example, variability in the normal value is reported in literature^[32] with a mean value of about 1.5 m/s in healthy subjects. This result can be considered an outlier^[33] but however possible (Figure 2C). Moreover higher values can be obtained measuring in the left lobe^[12,32] and in the superficial part of the right lobe^[32]. This last aspect can be contrarily absent in child^[33] due to a lower agerelated fibrosis in the superficial liver parenchyma. Also in other published series Virtual Touch Tissue Quantification results in the right and left liver lobes did not appear to be strictly similar and, on average, the stiffness values were found to be higher in the left lobe than in the right lobe, at least in patients with chronic hepatitis (68% of patients had higher values in the left lobe than in the right lobe). Furthermore the diagnostic capacity to establish the histological degree of liver fibrosis (with a reference biopsy taken in the right lobe) was lower in Vir-

tual Touch Tissue Quantification measurements from the left lobe than from the right lobe. These data, however, are not to be considered as a limitation of Virtual Touch Tissue Quantification to date, since they may perhaps more correctly reflect real differences and heterogeneity in the disease progression rates between the two lobes. It was in fact demonstrated that when two biopsies were taken in the two lobes during laparoscopy, a difference in one fibrosis stage between the two lobes occurred in up to 33% of cases^[34]. However since our reference standard for the assessment of fibrosis in chronic liver disease is biopsy of the right lobe of the liver, it is recommended to measure liver stiffness by Virtual Touch Tissue Quantification in this lobe. Moreover, an approach with multiple measurements in various liver sites is worthy of further investigation as it may lead to interesting and original diagnostic results. In addition, Goertz et al^[35] suggest to perform Virtual Touch Tissue Quantification via intercostal access in order to minimize invalid measurements and standard deviation. In their series, in fact, values taken subcostally were slightly higher than those measured through an intercostal approach.

Also some technical aspects need to be taken into account because they may explain some variability among published data. In example, the new release of the system is based on two acoustic pulses laterally to the ROI one by one at both sides and the maximum depth of the system nowadays achievable is 8 cm. Based on these considerations, the data published in the more recent papers should be more indicative of what can be obtainable with the new systems.

A recent study by Han *et al*^{36]}, compares ARFI performance to Doppler parameters and describes a weak but significant relationship between liver stiffness, measured by ARFI, and the parameters related to the portal pressure, as measured by Doppler US in patients with liver cirrhosis at different Child-Pugh stages, but having no oesophageal varices. The study demonstrates a positive correlation between the median ARFI sonoelastographic velocity, which reveals liver stiffness, and the flow parameters of Doppler US, which reflects portal hypertension. All these features, however, appear in advanced stage of disease.

Regarding the possible role of ARFI, it can be for sure



Table 2Diagnostic accuracy of non invasive methods for identifying severe liver fibrosis (> F3)		
	AUROC	Ref.
Laboratory test (APRI score)	0.80	Lin et al ^[71]
	0.76	Friedrich-Rust et al ^[7]
	0.84	Leroy et al ^[72]
Transient elastography	0.87	Boursier <i>et al</i> ^[73]
	0.96	Ferraioli <i>et al</i> ^[74]
	0.90	Friedrich-Rust et al ^[7]
Acoustic radiation force	0.91	Friedrich-Rust et al ^[7]
impulse	0.90	Lupsor <i>et al</i> ^[16]
	0.99	Fierbinteanu-Braticevici et al ^[17]

AUROC: Area under the receiver operating characteristic curve; APRI: Aspartate aminotransferase platelet ratio index.

employed in the follow up of cirrhotic patients in order to avoid multiple biopsies comparing the result before and after treatment. Liver biopsy is not suitable for repeated evaluations because it is invasive and can cause major complications $(0.3\%-0.5\%)^{[37]}$. Moreover liver fibrosis is a sequential and continuous process, and the staging of liver fibrosis should be evaluated frequently (Table 2). In contrast to liver biopsy, ARFI imaging is not invasive and can be repeated many times in the same patient^[27].

FOCAL LIVER LESIONS

Solid focal liver lesions are common findings during abdominal examinations. The accurate characterization and differential diagnosis are important aims of all the imaging modalities available today^[38-43]. Only three papers describe the application of ARFI technology in the study of solid focal liver lesions, with different results^[44-46].

The first human images of hepatic malignancies acquired in vivo using the ARFI technique or any other elasticity imaging technique appeared in the work of Fahey et al^[44]. His group compared B-mode and ARFI images both qualitatively (assessing the lesion margins definition by B-mode ultrasonography and ARFI imaging) and quantitatively (comparing the images contrast for both the techniques). They came to the conclusion that lesions margins definition at ARFI imaging was superior to that seen at B-mode US imaging (qualitative analysis). They also calculated that ARFI imaging can provide improvements in defining the contrast of tissue masses demonstrating, in fact, that the mean contrast for suspected hepatocellular carcinoma (HCC) in B-mode imaging was 2.9 dB (range 1.5-4.2 dB) vs 7.5 dB (range 3.1-11.9 dB) in ARFI images, with all HCCs appearing less stiff (brighter) than regional cirrhotic non-tumorous liver parenchyma. Moreover, the mean contrast for hepatic metastases in B-mode images was 3.1 dB (range 1.2-5.2 dB) vs 9.3 dB (range 5.7-13.9 dB) in ARFI images. Metastatic lesions in fact are stiffer (darker) than regional non-cirrhotic, nonneoplastic liver parenchyma. Fahey et $al^{[44]}$ also stated that combined US/ARFI could find application in tumor screening, lesion characterization and early detection of disease. Since HCC screening is not considered costeffective in regions with low prevalence, due to the low sensitivity of both sonography and serum AFP sampling^[47], ARFI imaging can improve sensitivity and costefficiency given its low cost, its capability of improving tumor contrast in comparison to US alone. If ARFI imaging had been proven to be a feasible alternative to contrast-enhanced ultrasound for liver applications, it could hold potential advantages related to the cost and complexity of the imaging protocol used for HCC screening. The authors, however, did not take into account the mechanical response of benign abdominal masses to applied radiation forces, thus they couldn't evaluate the ability of ARFI in differentiating benign from malignant liver masses.

More recent works about ARFI imaging applied to solid focal liver lesions are the ones from Cho *et al*^[45] and from Gallotti *et al*^[46]. The first one evaluates ARFI values calculated on HCCs, metastases, cholangiocarcinomas and hemangiomas, the second one evaluated in addition adenomas and focal nodular hyperplasia (FNHs), but did not consider cholangiocarcinomas.

Benign lesions

In regard to hemangiomas, Gallotti *et al*^{46]} agree with Cho *et al*^{45]} about the great variability of this type of lesions (mean wave velocity value of the lesion 2.30 m/s; mean wave velocity value of the surrounding parenchyma 1.45 m/s), since its stiffness depends on the amount of fibrotic septa which divide the dilated vascular space.

For the first time in Gallotti *et al*⁴⁶ paper also FNHs and adenomas were studied. FNH resulted the stiffest lesions after metastases and cholangiocarcinomas, indipendently from their dimensions and from the presence or absence of central scar. In fact, even if present, the ROI has to be located out of the fibrotic central scar. The high stiffness (mean wave velocity value of the lesion 2.75 m/s; mean wave velocity value of the surrounding parenchyma 1.57 m/s^[46]) is explained with the well known high fibrotic content of this type of lesion. Thus, if the result will be confirmed by further studies, the cut-off of 2 m/s, suggested by Cho *et al*^[45] to distinguish benign from malignant lesions, can no longer be used.

On the other hand, adenomas showed wave velocity values similar to those observed in the surrounding liver $er^{[46]}$: this is a solid focal liver lesion, the softest analysed (mean wave velocity value of the lesion 1.25 m/s; mean wave velocity value of the surrounding parenchyma 1.40 m/s). The presence of cells similar to normal hepatocytes and few stroma explain the low mean wave velocity value calculated in adenomas compared to other focal liver lesions.

Malignant lesions

According to Fahey *et al*^[44], but inconsistent with results of Cho *et al*^[45] despite the similar diameter of the lesions, in Gallotti *et al*^[46] almost all the HCCs evaluated resulted in softer lesions compared to the surrounding cirrhotic liver (mean wave velocity value of the lesion 2.17 m/s;



mean wave velocity value of the surrounding parenchyma 2.99 m/s), and the main elastographic value was significantly lower than that of the surrounding parenchyma. This discrepancy might be explained by the difference in the severity of the cirrhosis of the background liver in each study population. In Cho *et al*⁴⁵ the degree of liver cirrhosis of patients with HCCs was likely to be less severe (15 out of 20 patients with HCCs had chronic liver disease of Child-Pugh classification A) compared with that seen in the other studies, assuming that the liver is stiffer with more severe liver cirrhosis.

There is concordance^[44-46] about the fact that all metastatic lesions (mean wave velocity value of the lesion 2.87 m/s; mean wave velocity value of the surrounding parenchyma 1.63 m/s^[46]) and, when considered, cholangiocarcinomas, are stiffer than the surrounding liver. This is probably due to the presence of fibrous content potentially found in many of these lesions. The presence of necrotic degeneration, mainly in the biggest masses, does not influence the results since the ROI for the stiffness calculation has to be accurately positioned out of the necrotic portion. Summarizing, based on the preliminary results of the study of solid focal liver lesions^[44-46], it can be also concluded that ARFI seems to be an useful in the following scenarios: (1) for differential diagnosis between adenomas and FNHs; (2) for the study of metastases; and (3) for the study of HCCs in cirrhotic liver. Future perspective could be the application of ARFI in liver lesion detection by using volumetric automated acquisition.

CONCLUSION

Virtual Touch Tissue Quantification is a new non invasive imaging based technique able to estimate liver stiffness diagnosing cirrhosis with a good accuracy. The first assessment of patients with a suspicion of liver disease can be therefore easily performed with both conventional ultrasonography and Virtual Touch Tissue Quantification for liver stiffness assessment in a single step.

In conclusion, several studies about ARFI application in diffuse liver pathology have been made, and most of them state that ARFI itself can be used in the study of the liver with similar accuracy than transient elastography in diagnosing significant fibrosis^[7,20,21] or cirrhosis^[12,16,19]. However, ARFI has got some advantages in respect to TE since it does not require separate equipment and consequently it is not necessary an additional examination in addition to conventional US, saving time and costs. Moreover, during TE examination, only A-mode imaging is displayed on the screen in order to select the area of scanning and, consequently, ligaments, vascular structures or even lesions, may inadvertently be included in the ROI, possibly affecting the final results.

Another interesting finding is that Virtual Touch Tissue Quantification measurements can be successfully carried out almost in every patient while TE is unsuccessful in 7% of cases (*e.g.*, in patients with narrow intercostal spaces and in those with morbid obesity), as reported also in literature^[22-26]. On the contrary, there are just few indications about ARFI and focal liver lesions, so further studies are needed in order to find ARFI the correct place in the everyday clinical practice.

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P-Reviewers Diamantis I, Faintuch J, Maruyama H S-Editor Huang XZ L-Editor A E-Editor Li JY







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