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## Association of plasma and cortical beta-amyloid is modulated by APOE $\epsilon$ 4 status

Shanker Swaminathan<sup>a,b</sup>, Shannon L. Risacher<sup>a</sup>, Karmen K. Yoder<sup>a</sup>, John D. West<sup>a</sup>, Li Shen<sup>a,c</sup>, Sungeun Kim<sup>a,c</sup>, Mark Inlow<sup>a,d</sup>, Tatiana Foroud<sup>a,b,c</sup>, William J. Jagust<sup>e</sup>, Robert A. Koeppe<sup>f</sup>, Chester A. Mathis<sup>g</sup>, Leslie M. Shaw<sup>h</sup>, John Q. Trojanowski<sup>h</sup>, Holly Soares<sup>i</sup>, Paul S. Aisen<sup>j</sup>, Ronald C. Petersen<sup>k</sup>, Michael W. Weiner<sup>l</sup>, and Andrew J. Saykin<sup>a,b,c,\*</sup> for the Alzheimer's Disease Neuroimaging Initiative<sup>\*\*</sup>

<sup>a</sup>Center for Neuroimaging, Department of Radiology and Imaging Sciences, Indiana University School of Medicine, Indianapolis, IN 46202, USA

<sup>b</sup>Department of Medical and Molecular Genetics, Indiana University School of Medicine, Indianapolis, IN 46202, USA

<sup>c</sup>Center for Computational Biology and Bioinformatics, Indiana University School of Medicine, Indianapolis, IN 46202, USA

<sup>d</sup>Department of Mathematics, Rose-Hulman Institute of Technology, Terre Haute, IN 47803, USA

<sup>e</sup>Helen Wills Neuroscience Institute, University of California, Berkeley, Berkeley, CA 94720, USA

<sup>f</sup>Division of Nuclear Medicine, Department of Radiology, University of Michigan, Ann Arbor, MI 48109, USA

<sup>g</sup>Department of Radiology, University of Pittsburgh, Pittsburgh, PA 15261, USA

<sup>h</sup>Department of Pathology and Laboratory Medicine, University of Pennsylvania School of Medicine, Philadelphia, PA 19104, USA

<sup>i</sup>Bristol Myers Squibb Co, Wallingford, CT 06492, USA

<sup>j</sup>Department of Neurosciences, University of California at San Diego, San Diego, CA 92093, USA

<sup>k</sup>Department of Neurology, Mayo Clinic and Foundation, Rochester, MN 55905, USA

<sup>l</sup>Department of Veterans Affairs Medical Center, Center for Imaging of Neurodegenerative Diseases, San Francisco, CA 94121, USA

### Abstract

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\*Corresponding author: Andrew J. Saykin, PsyD, Center for Neuroimaging, Department of Radiology and Imaging Sciences, Indiana University School of Medicine, Indianapolis, IN 46202, USA, Tel.: 317-278-6947; Fax: 317-274-1067; asaykin@iupui.edu.

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The authors declare no conflicts of interest relevant to the present work.

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**Background**—*APOE*  $\epsilon 4$ 's role as a modulator of the relationship between soluble plasma beta-amyloid ( $A\beta$ ) and fibrillar brain  $A\beta$  measured by Pittsburgh Compound-B positron emission tomography ( $[^{11}C]PiB$  PET) has not been assessed.

**Methods**—Ninety-six Alzheimer's Disease Neuroimaging Initiative participants with  $[^{11}C]PiB$  scans and plasma  $A\beta_{1-40}$  and  $A\beta_{1-42}$  measurements at time of scan were included. Regional and voxel-wise analyses of  $[^{11}C]PiB$  data were used to determine the influence of *APOE*  $\epsilon 4$  on association of plasma  $A\beta_{1-40}$ ,  $A\beta_{1-42}$ , and  $A\beta_{1-40}/A\beta_{1-42}$  with  $[^{11}C]PiB$  uptake.

**Results**—In *APOE*  $\epsilon 4$ - but not  $\epsilon 4$ + participants, positive relationships between plasma  $A\beta_{1-40}/A\beta_{1-42}$  and  $[^{11}C]PiB$  uptake were observed. Modeling the interaction of *APOE* and plasma  $A\beta_{1-40}/A\beta_{1-42}$  improved the explained variance in  $[^{11}C]PiB$  binding compared to using *APOE* and plasma  $A\beta_{1-40}/A\beta_{1-42}$  as separate terms.

**Conclusions**—The results suggest that plasma  $A\beta$  is a potential Alzheimer's disease biomarker and highlight the importance of genetic variation in interpretation of plasma  $A\beta$  levels.

### Keywords

Alzheimer's disease (AD); mild cognitive impairment (MCI); Alzheimer's Disease Neuroimaging Initiative (ADNI); beta-amyloid ( $A\beta$ ); plasma beta-amyloid; positron emission tomography (PET); Pittsburgh Compound-B ( $[^{11}C]PiB$ ); Apolipoprotein E (*APOE*)

## 1. Introduction

Alzheimer's disease (AD) is the most common type of dementia, affecting an estimated 5.4 million Americans. At present, there are no treatments that can stop its progression. However, worldwide research efforts are being conducted to identify improved methods to prevent, diagnose, and treat this disease [1]. Objective measures of biological or pathogenic processes, termed biomarkers, can help in the evaluation of disease risk or prognosis. To date, no reliable biomarkers for AD in peripheral blood have been found [2].

AD is characterized by declining memory and cognition. Amnesic mild cognitive impairment (MCI) is a clinical condition thought to be a prodromal stage of AD, in which an individual has cognitive problems not normal for his/her age, but are not severe enough to interfere significantly with daily life activities. An estimated 14–18% of individuals aged 70 years and older have MCI, and approximately 10–15% of these individuals with MCI will progress to dementia, mostly AD, each year [3, 4].

Accumulation of beta-amyloid ( $A\beta$ ) fragments into amyloid plaques in the brain is one of the defining pathologies of AD. Attempts to monitor the presence and/or progression of amyloid deposition have primarily focused on measurements of  $A\beta$  in the brain and cerebrospinal fluid (CSF). The level of CSF  $A\beta_{1-42}$  has been shown to be a sensitive biomarker for detection and diagnosis of AD [5–7]. Positron emission tomography (PET) imaging techniques with ligands such as Pittsburgh Compound-B ( $[^{11}C]PiB$ ) [8] and  $[^{18}F]$ florbetapir [9, 10], which bind fibrillar  $A\beta$  plaques with high affinity are being studied for their efficacy in predicting and diagnosing AD and have shown some promise [11–13].

Identifying a peripheral biomarker of central  $A\beta$  deposition may help in the diagnosis and treatment of the disease at earlier stages. Measuring soluble  $A\beta$  levels in plasma would provide an easy method to study  $A\beta$  species, as the procedure is minimally invasive and relatively inexpensive. The utility of plasma  $A\beta$  as a potential AD biomarker has been assessed in previous studies, but the results have been inconsistent [14–17]. Possible reasons for the inconsistent results could be the use of different enzyme-linked immunosorbent assays and platforms, and timing of sample collection in relation to the stage of disease

progression. Therefore, additional studies are needed to fully characterize the utility of plasma A $\beta$  measures as sensitive and effective biomarkers of AD.

Genetic factors, such as the *APOE* (apolipoprotein E) gene, may play a role in amyloid accumulation and the development of AD. The *APOE* gene is expressed as three variants:  $\epsilon 2$ ,  $\epsilon 3$ , and  $\epsilon 4$ . The *APOE*  $\epsilon 4$  allele is the strongest genetic risk factor of late-onset AD and confers a dose-dependent increase in AD risk of approximately four-fold in carriers compared to non-carriers [18–20]. The  $\epsilon 4$  allele is also associated with increased fibrillar A $\beta$  [21] and decreased soluble plasma A $\beta_{1-42}$  [22] in a dose-dependent manner. The *APOE* gene codes for the apoE protein, which is essential for maintaining blood brain barrier (BBB) integrity [23]. The apoE4 form of the apoE protein, coded for by the  $\epsilon 4$  allele, has been associated with reduced A $\beta$  clearance from the brain [24] and plasma [25] and with impaired tight junction integrity [26].

To our knowledge, only four studies have investigated the relationship of soluble plasma A $\beta$  and fibrillar brain A $\beta$  as measured by [ $^{11}\text{C}$ ]PiB [22, 27–29]. The first study [27] did not identify any relationships between plasma A $\beta_{1-40}$  and A $\beta_{1-42}$  levels and [ $^{11}\text{C}$ ]PiB binding. In the other studies, inverse correlations were observed between plasma A $\beta_{1-42}$  and [ $^{11}\text{C}$ ]PiB uptake [22, 28] and between A $\beta_{1-42}$ /A $\beta_{1-40}$  and brain amyloid [28, 29]. However, none of these studies examined the potential influence of genetic variation in AD-related genes (e.g., *APOE*  $\epsilon 4$ ) on relationships between peripheral and central markers of A $\beta$ . Furthermore, these studies only included regional measures of [ $^{11}\text{C}$ ]PiB uptake rather than voxel-based mapping across the whole brain, which may have limited the findings as extracting information from spatially large regions may dilute or obscure relevant results that are spatially constrained.

In the present report, we studied the associations among [ $^{11}\text{C}$ ]PiB brain uptake, soluble plasma A $\beta$  measurements, and *APOE*  $\epsilon 4$  genotype status in 96 participants from the Alzheimer's Disease Neuroimaging Initiative (ADNI) to determine whether the relationship of soluble plasma A $\beta$  measures and fibrillar brain amyloid was influenced by *APOE*  $\epsilon 4$  status. First, we used the average regional [ $^{11}\text{C}$ ]PiB uptake across four target brain regions known to have amyloid deposition in AD as a quantitative phenotype in regression analyses. We then conducted whole-brain, voxel-wise regression analyses to identify spatially-specific clusters in which *APOE*  $\epsilon 4$  genotype modulated the association of plasma and brain PET measurements of A $\beta$ .

## 2. Methods

### 2.1. Alzheimer's Disease Neuroimaging Initiative

Data used in the preparation of this report were obtained from the ADNI database (<http://adni.loni.ucla.edu>). The ADNI was initiated in 2003 as a \$60 million, 5-year public-private partnership by the National Institute on Aging, the National Institute of Biomedical Imaging and Bioengineering, the Food and Drug Administration, private pharmaceutical companies and nonprofit organizations. ADNI's primary goal is been to test whether serial magnetic resonance imaging (MRI), PET, other biological markers, genetics, and clinical and neuropsychological assessments can be combined to detect and measure the progression of MCI and early AD. Determining sensitive and specific markers of very early AD progression can aid researchers and clinicians in developing new treatments and monitoring their effectiveness, as well as lessen the time and cost of clinical trials.

Michael W. Weiner, MD, Veterans Affairs Medical Center and University of California-San Francisco, is the Principal Investigator of this initiative. ADNI is the result of the efforts of many co-investigators from a broad range of academic institutions and private corporations.

As part of the initial phase of ADNI, more than 800 participants, ages 55 to 90, were recruited from over 50 sites across the USA and Canada, including approximately 200 cognitively healthy older individuals (healthy control or HC) to be followed for three years, 400 people with MCI to be followed for three years and 200 people with early AD to be followed for two years. Further information about ADNI can be found in [30] and at <http://www.adni-info.org>.

The study was conducted after Institutional Review Board approval at each site. Written informed consent was obtained from all study participants or their authorized representatives.

## 2.2. Participants

Data from ninety-six participants in the ADNI cohort were evaluated. Participant selection was based on the availability of the following data: [ $^{11}\text{C}$ ]PiB PET scans, plasma measurements of  $\text{A}\beta_{1-40}$  and  $\text{A}\beta_{1-42}$  at time of PET scan, and *APOE*  $\epsilon 4$  genotype data. At the time of PET scan, 22 participants were in the AD group, 52 in the MCI group and 22 in the HC group. The participants included 89 non-Hispanic Caucasians, two non-Hispanic African Americans, two non-Hispanic Asians, two Hispanic Caucasians, and one Caucasian participant of unknown ethnicity. Additional demographic information about the included sample is presented in Table 1.

**2.2.1. [ $^{11}\text{C}$ ]PiB PET image data**—For all participants, PET data consisted of each participant's initial [ $^{11}\text{C}$ ]PiB scan in the ADNI longitudinal imaging protocol. Initial scans were acquired at either the participant's baseline visit, 12-month visit, or 24-month visit (Table 1). Methods for the acquisition and processing of [ $^{11}\text{C}$ ]PiB PET scans for the ADNI sample have been described elsewhere [31, 32]. The PET data used in the present study were what was available as of October 2010. The ADNI database includes normalized whole-brain [ $^{11}\text{C}$ ]PiB images, as well as normalized regional [ $^{11}\text{C}$ ]PiB average uptake values extracted from anatomically-defined regions of interest (ROIs). Both pre-existing ROI data and whole-brain [ $^{11}\text{C}$ ]PiB images were downloaded and analyzed in the present study. Regional [ $^{11}\text{C}$ ]PiB standardized uptake value ratios (SUVR) from four ROIs (anterior cingulate, frontal cortex, parietal cortex and precuneus) were averaged and used as a quantitative phenotype, which will be referred to as “average regional [ $^{11}\text{C}$ ]PiB uptake”. This metric has been previously used to classify participants as positive or negative for amyloid deposition [32].

The whole-brain [ $^{11}\text{C}$ ]PiB PET images evaluated in the present study were preprocessed (“PIB Coreg, Avg, Std Img and Vox Size, Uniform Resolution”), as has been previously described [32]. Briefly, the images were set to a standard orientation and voxel size, intensity normalized using a cerebellar grey matter (GM) ROI, and smoothed to a common resolution of 8 mm full-width at half maximum. These pre-processed scans were downloaded in Neuroimaging Informatics Technology Initiative (NIfTI) format from the ADNI scan repository (<http://adni.loni.ucla.edu>) and processed further using Statistical Parametric Mapping [33] version 5 (SPM5) (<http://www.fil.ion.ucl.ac.uk/spm/>) implemented via MATLAB v7.1.0 (MathWorks, Natick, MA, USA) [34]. Specifically, for all participants, 1.5 Tesla T1-weighted 3D magnetization prepared rapid acquisition gradient echo (MP-RAGE) MRI scans [35] acquired at the same time point as the [ $^{11}\text{C}$ ]PiB scans were also downloaded from the ADNI site (<http://adni.loni.ucla.edu>). The pre-processed [ $^{11}\text{C}$ ]PiB PET image of each participant was co-registered to their corresponding MRI scan. PET and MRI data were then spatially normalized to Montreal Neurological Institute (MNI) space using transformation parameters estimated from the SPM segmentation algorithm [36]. These spatially-normalized PET images were used for the whole-brain voxel-wise analysis.

**2.2.2. Plasma A $\beta$  data**—Plasma A $\beta_{1-40}$  and A $\beta_{1-42}$  levels for participants with [ $^{11}\text{C}$ ]PiB PET scans from the same time point that the PET data were acquired were obtained from the ADNI database. The methods for the collection, measurement and quality control (QC) of plasma samples have been previously described [22, 37].

**2.2.3. APOE  $\epsilon 4$  genotyping**—The *APOE*  $\epsilon 4$  status of all participants was determined by two single nucleotide polymorphisms (rs429358 and rs7412), as previously described [38]. Participants were classified as *APOE*  $\epsilon 4$ - (absence of the  $\epsilon 4$  allele), or *APOE*  $\epsilon 4$ + (presence of the  $\epsilon 4$  allele).

### 2.3. Statistical analyses

The influence of *APOE*  $\epsilon 4$  status on the association between plasma A $\beta$  and average regional [ $^{11}\text{C}$ ]PiB uptake was assessed in R version 2.10.0 [39] and SAS 9.3 (SAS Institute Inc., Cary, NC, USA) using the following regression models:

1. Average regional [ $^{11}\text{C}$ ]PiB uptake=Plasma A $\beta_{1-40}$ +*APOE*  $\epsilon 4$  status+(Plasma A $\beta_{1-40}$ \**APOE*  $\epsilon 4$  status)
2. Average regional [ $^{11}\text{C}$ ]PiB uptake=Plasma A $\beta_{1-42}$ +*APOE*  $\epsilon 4$  status+(Plasma A $\beta_{1-42}$ \**APOE*  $\epsilon 4$  status)
3. Average regional [ $^{11}\text{C}$ ]PiB uptake=Plasma A $\beta_{1-40}$ /A $\beta_{1-42}$ +*APOE*  $\epsilon 4$  status+(Plasma A $\beta_{1-40}$ /A $\beta_{1-42}$ \**APOE*  $\epsilon 4$  status)

Models with significant interactions between plasma A $\beta$  and *APOE*  $\epsilon 4$  status on average regional [ $^{11}\text{C}$ ]PiB uptake were identified. For these models, the variance in average regional [ $^{11}\text{C}$ ]PiB uptake explained by different terms in the model was determined using the following regression models:

1. Variance in average regional [ $^{11}\text{C}$ ]PiB uptake explained by plasma A $\beta$  term alone:  
Average regional [ $^{11}\text{C}$ ]PiB uptake=Plasma A $\beta$
2. Variance in average regional [ $^{11}\text{C}$ ]PiB uptake explained by *APOE*  $\epsilon 4$  status term alone:  
Average regional [ $^{11}\text{C}$ ]PiB uptake=*APOE*  $\epsilon 4$  status
3. Variance in average regional [ $^{11}\text{C}$ ]PiB uptake explained by plasma A $\beta$  and *APOE*  $\epsilon 4$  status terms together:  
Average regional [ $^{11}\text{C}$ ]PiB uptake=Plasma A $\beta$ +*APOE*  $\epsilon 4$  status
4. Variance in average regional [ $^{11}\text{C}$ ]PiB uptake explained by plasma A $\beta$ , *APOE*  $\epsilon 4$  status, and (plasma A $\beta$ \**APOE*  $\epsilon 4$  status) terms together:  
Average regional [ $^{11}\text{C}$ ]PiB uptake=Plasma A $\beta$ +*APOE*  $\epsilon 4$  status+(Plasma A $\beta$ \**APOE*  $\epsilon 4$  status)

The influence of *APOE*  $\epsilon 4$  status on the association between plasma A $\beta$  and [ $^{11}\text{C}$ ]PiB uptake was further assessed in whole-brain voxel-wise analyses in SPM5 using the following regression models:

1. Voxel [ $^{11}\text{C}$ ]PiB uptake=Plasma A $\beta_{1-40}$ +*APOE*  $\epsilon 4$  status+(Plasma A $\beta_{1-40}$ \**APOE*  $\epsilon 4$  status)
2. Voxel [ $^{11}\text{C}$ ]PiB uptake=Plasma A $\beta_{1-42}$ +*APOE*  $\epsilon 4$  status+(Plasma A $\beta_{1-42}$ \**APOE*  $\epsilon 4$  status)

3. Voxel [ $^{11}\text{C}$ ]PiB uptake = Plasma  $\text{A}\beta_{1-40}/\text{A}\beta_{1-42} + \text{APOE } \epsilon 4 \text{ status} + (\text{Plasma } \text{A}\beta_{1-40}/\text{A}\beta_{1-42} * \text{APOE } \epsilon 4 \text{ status})$

In the voxel-wise analyses, an explicit GM mask was used to restrict analyses to GM regions. Significant interactions were determined using a voxel-level threshold of  $p < 0.005$  (uncorrected) and cluster-level threshold of  $k = 200$  contiguous voxels to achieve cluster-level uncorrected  $p < 0.05$ . Clusters identified in the left or right cerebellum were not considered as the [ $^{11}\text{C}$ ]PiB PET images had been intensity normalized using a cerebellar GM region of interest. Voxels at which significant relationships existed were displayed on a three-dimensional rendered brain. The MNI coordinates of voxels that were peak maxima and local maxima (voxels  $> 4$  mm apart) in each cluster were converted to Talairach coordinates, and queried in Talairach Client v2.4.2 [40, 41] software to determine the associated anatomic labels. Random field theory corrected  $p$  values ( $p_{\text{corr}}$ ) were used to identify significant clusters. Mean [ $^{11}\text{C}$ ]PiB uptake from each significant cluster was extracted for all participants and their distribution in  $\text{APOE } \epsilon 4-$  and  $\text{APOE } \epsilon 4+$  participants was further examined in R version 2.10.0 and SAS 9.3. We then further evaluated the relationship of mean [ $^{11}\text{C}$ ]PiB uptake from the biggest and most significant cluster and plasma  $\text{A}\beta$  levels. The variance in mean [ $^{11}\text{C}$ ]PiB uptake extracted from the significant cluster explained by different terms in the model was determined using the following regression models:

1. Variance in mean [ $^{11}\text{C}$ ]PiB uptake from the significant cluster explained by plasma  $\text{A}\beta$  term alone:

Mean [ $^{11}\text{C}$ ]PiB uptake from the significant cluster = Plasma  $\text{A}\beta$

2. Variance in mean [ $^{11}\text{C}$ ]PiB uptake from the significant cluster explained by  $\text{APOE } \epsilon 4$  status term alone:

Mean [ $^{11}\text{C}$ ]PiB uptake from the significant cluster =  $\text{APOE } \epsilon 4$  status

3. Variance in mean [ $^{11}\text{C}$ ]PiB uptake from the significant cluster explained by plasma  $\text{A}\beta$  and  $\text{APOE } \epsilon 4$  status terms together:

Mean [ $^{11}\text{C}$ ]PiB uptake from the significant cluster = Plasma  $\text{A}\beta + \text{APOE } \epsilon 4$  status

4. Variance in mean [ $^{11}\text{C}$ ]PiB uptake from the significant cluster explained by plasma  $\text{A}\beta$ ,  $\text{APOE } \epsilon 4$  status, and (plasma  $\text{A}\beta * \text{APOE } \epsilon 4$  status) terms together:

Mean [ $^{11}\text{C}$ ]PiB uptake from the significant cluster = Plasma  $\text{A}\beta + \text{APOE } \epsilon 4$  status + (Plasma  $\text{A}\beta * \text{APOE } \epsilon 4$  status)

### 3. Results

We first investigated the influence of  $\text{APOE } \epsilon 4$  status on the association between plasma  $\text{A}\beta$  and average regional [ $^{11}\text{C}$ ]PiB uptake. No significant interactions between plasma  $\text{A}\beta_{1-40}$  and  $\text{APOE } \epsilon 4$  status or between plasma  $\text{A}\beta_{1-42}$  and  $\text{APOE } \epsilon 4$  status were observed on average regional [ $^{11}\text{C}$ ]PiB uptake. However, a significant interaction between plasma  $\text{A}\beta_{1-40}/\text{A}\beta_{1-42}$  and  $\text{APOE } \epsilon 4$  status ( $p = 0.025$ ) on average regional [ $^{11}\text{C}$ ]PiB uptake was observed. Inclusion of age at time of scan and gender as covariates did not alter this finding.  $\text{APOE } \epsilon 4$  genotype status ( $\epsilon 4-$  or  $\epsilon 4+$ ) conferred different patterns of association between plasma  $\text{A}\beta_{1-40}/\text{A}\beta_{1-42}$  and average regional [ $^{11}\text{C}$ ]PiB uptake. Specifically, in the  $\text{APOE } \epsilon 4-$  participants, there was a positive relationship between plasma  $\text{A}\beta_{1-40}/\text{A}\beta_{1-42}$  and average regional [ $^{11}\text{C}$ ]PiB uptake (Slope = 0.162;  $p = 0.008$ ;  $r^2 = 0.141$ ) (Fig. 1A). However, this relationship did not exist in the  $\text{APOE } \epsilon 4+$  participants (Slope = -0.005;  $p = 0.901$ ;  $r^2 < 0.001$ ) (Fig. 1B). The  $\text{APOE } \epsilon 4$  status and plasma  $\text{A}\beta_{1-40}/\text{A}\beta_{1-42}$  terms explained 17% and 6% of variation in average regional [ $^{11}\text{C}$ ]PiB uptake, respectively. The two terms together explained 19% of variation in average regional [ $^{11}\text{C}$ ]PiB uptake. Inclusion of the (plasma

$A\beta_{1-40}/A\beta_{1-42} * APOE \epsilon 4$  status) interaction term in the model increased the explained variance in average regional [ $^{11}C$ ]PiB uptake to 24%.

To further examine the spatial extent of the potential influence of the *APOE*  $\epsilon 4$  status on the association of plasma  $A\beta$  and [ $^{11}C$ ]PiB uptake, we performed whole-brain voxel-wise regression analyses. *APOE* genotype did not significantly affect the positive or negative associations between plasma  $A\beta_{1-40}$  and [ $^{11}C$ ]PiB uptake and between plasma  $A\beta_{1-42}$  and [ $^{11}C$ ]PiB uptake in cerebral regions. However, *APOE* genotype significantly altered the negative correlation of plasma  $A\beta_{1-40}/A\beta_{1-42}$  and [ $^{11}C$ ]PiB uptake in a significant cluster in the left inferior frontal gyrus (MNI peak coordinates:  $x=-40, y=18, z=-6; k=6152$  voxels; cluster-level  $p_{corr} < 0.001$ ) (Fig. 2 and Table 2). Similar to the data from the average regional [ $^{11}C$ ]PiB uptake analysis, there was a positive relationship between plasma  $A\beta_{1-40}/A\beta_{1-42}$  and mean [ $^{11}C$ ]PiB uptake from the inferior frontal gyral cluster in the *APOE*  $\epsilon 4-$  participants (Slope=0.250;  $p=0.001$ ;  $r^2=0.213$ ) (Fig. 1C), but not in the *APOE*  $\epsilon 4+$  participants (Slope=-0.050;  $p=0.404$ ;  $r^2=0.015$ ) (Fig. 1D). Inclusion of age at time of scan and gender as covariates again did not alter this finding. The *APOE*  $\epsilon 4$  status and plasma  $A\beta_{1-40}/A\beta_{1-42}$  terms by themselves explained 13% and 4% of variation in mean [ $^{11}C$ ]PiB uptake from the significant cluster, respectively. The two terms together explained 14% of variation in mean [ $^{11}C$ ]PiB uptake from the significant cluster. Inclusion of the (plasma  $A\beta_{1-40}/A\beta_{1-42} * APOE \epsilon 4$  status) interaction term along with the two terms in the model increased the variance explained in mean [ $^{11}C$ ]PiB uptake from the significant cluster to 23%. No clusters were identified when considering the positive correlation of plasma  $A\beta_{1-40}/A\beta_{1-42}$  and [ $^{11}C$ ]PiB uptake.

#### 4. Discussion

The investigation of  $A\beta$  species in plasma offers advantages over conventional methods for measuring  $A\beta$  levels in the brain and CSF. Obtaining and analyzing plasma samples is relatively inexpensive, minimally invasive, and can easily be performed at multiple time points. Therefore, a plasma-based biomarker for early detection and diagnosis of AD would be ideal. In the ADNI cohort, a strong association has been observed between CSF  $A\beta_{1-42}$  and fibrillar brain  $A\beta$  (indexed with [ $^{11}C$ ]PiB) [31], while a weak but significant association has been observed between CSF  $A\beta_{1-42}$  and soluble plasma  $A\beta_{1-42}$  [37]. However, the association between soluble plasma  $A\beta$  and fibrillar brain  $A\beta$  is unclear.

In the present report, we investigated the relationship of soluble plasma  $A\beta$  ( $A\beta_{1-40}$ ,  $A\beta_{1-42}$  and  $A\beta_{1-40}/A\beta_{1-42}$ ), *APOE*  $\epsilon 4$  status, and fibrillar brain  $A\beta$  (indexed with [ $^{11}C$ ]PiB) in the ADNI cohort. In two types of analytic approaches, *APOE*  $\epsilon 4$  genotype status had a significant effect on the relationship between plasma  $A\beta_{1-40}/A\beta_{1-42}$  and [ $^{11}C$ ]PiB uptake. Specifically, a positive relationship between plasma  $A\beta_{1-40}/A\beta_{1-42}$  and [ $^{11}C$ ]PiB signal was observed in *APOE*  $\epsilon 4-$  participants, but not in *APOE*  $\epsilon 4+$  participants (Fig. 1). This finding may reflect a stronger relationship between plasma  $A\beta$  and accumulation of fibrillar amyloid in the brain in individuals at an earlier and/or less severe disease state (e.g. *APOE*  $\epsilon 4-$ ). A recent study suggested that plasma  $A\beta$  levels in cognitively stable individuals tend to increase slightly with age [15]. Cognitively normal individuals with higher plasma  $A\beta$  levels are thought to be at an increased risk of progression to AD. Plasma  $A\beta$  levels in individuals who go on to develop AD tend to be elevated in the pre-dementia stage, reach a peak, and then fall prior to developing clinical AD symptoms. Increasing brain amyloid deposits in the later stages of disease may perhaps reduce interstitial  $A\beta$  in the brain and CSF, confounding the relationship between plasma  $A\beta$  and brain amyloid.

The molecular mechanism by which the *APOE*  $\epsilon 4$  allele leads to increased risk for AD is unclear. The *APOE* gene codes for the apoE protein, which is essential for maintaining BBB

integrity [23]. Furthermore, the various apoE protein isoforms are thought to differentially clear A $\beta$  from the brain into the plasma across the BBB. In a recent study, the authors found that mice expressing the human apoE4 protein had greater A $\beta$  concentrations in the interstitial fluid of the brain and hippocampus and showed reduced A $\beta$  clearance from the interstitial fluid of the brain when compared to mice expressing the human apoE2 or apoE3 proteins [24]. However, the authors did not find differences in A $\beta$  synthesis or amyloidogenic processing between mice expressing the different apoE protein isoforms. In another study conducted in *APOE*  $\epsilon$ 2,  $\epsilon$ 3, and  $\epsilon$ 4 knock-in and *APOE* knock-out (KO) mice injected with lipidated recombinant apoE2, E3, and E4 proteins, the authors found a difference in peripheral A $\beta$  clearance from the plasma by *APOE* genotype [25]. The results suggested that *APOE*  $\epsilon$ 4 gene expression results in a protein (apoE4) with lowered efficiency of peripheral A $\beta$  clearance from the plasma. Tight junction integrity in the BBB is also regulated by the apoE protein in an isoform-dependent manner, with impaired tight junction integrity and increased BBB permeability observed in mice with the apoE4 isoform compared to mice with expression of the apoE3 isoform [26]. Thus, reduced A $\beta$  clearance by apoE4 protein may lead to an impaired BBB, in turn, affecting A $\beta$  levels in the brain and plasma and the relationship between these compartments.

Binding of the apoE protein to A $\beta$  may also influence A $\beta$  clearance from the brain into the plasma. The apoE protein binds strongly to A $\beta$ , but the binding characteristics of the apoE4 isoform are different than those of the apoE3 isoform [42, 43]. Oxidized apoE4 binds more rapidly to synthetic A $\beta$  than oxidized apoE3. Binding by oxidized apoE4 was also more sensitive to pH changes than oxidized apoE3. In addition, the *APOE*  $\epsilon$ 4 allele is associated with increased vascular and plaque amyloid deposits [44]. *APOE*  $\epsilon$ 4 homozygotes have higher amyloid deposits in the vasculature and tissue compared to *APOE*  $\epsilon$ 3 homozygotes. *APOE*  $\epsilon$ 3/ $\epsilon$ 4 heterozygotes have intermediate amyloid deposits. In a recent study, free apoE protein was shown to facilitate a greater removal of A $\beta$  from the brain into the periphery across the BBB compared with apoE protein bound to A $\beta$  [45]. Furthermore, apoE isoform-specific differences were observed in A $\beta$  transport. Specifically, A $\beta$  bound to the apoE4 isoform had increased blood to brain transport when compared to A $\beta$  bound to the apoE3 isoform. Similar to a previous study, the authors found that the apoE4 isoform had decreased A $\beta$  clearance across the BBB in comparison to the apoE3 isoform. More recently, the authors in a different study observed that retinoid X receptor stimulation increased A $\beta$  clearance across the BBB, an effect which was believed to be partially mediated by the apoE protein [46].

The apoE protein has been shown to be present in greater amounts in the AD brain relative to those of healthy elders. Furthermore, apoE undergoes significantly more cleavage in the AD brain than in HC, especially in *APOE*  $\epsilon$ 4 carriers [47]. The N-terminal domain of the apoE protein contains the major receptor binding region and the C-terminal domain contains the lipid binding region. The C-terminal domain of both the apoE3 and apoE4 isoforms has been shown to interact closely with A $\beta$  [47]. Isolated C-terminal-truncated apoE4 protein fragments have been shown to be associated with A $\beta$  plaques [47]. Finally, inefficient clearance of A $\beta$  peptides produces neuronal and behavioral deficits in mice [48]. Thus, differential clearance of A $\beta$  by apoE protein isoform, which is coded for by different *APOE* genotypes, may be a potential explanation for the *APOE* genotype effects observed in the present study. Further investigation of mechanistic explanations is warranted.

It is important to discuss the limitations of the present study. First, the sample size in the present study was relatively modest, as only 96 participants in the ADNI cohort had both [<sup>11</sup>C]PiB PET scans and concomitant plasma measurements of A $\beta$ <sub>1-40</sub> and A $\beta$ <sub>1-42</sub>. Our results suggest a complex relationship between plasma A $\beta$ , brain A $\beta$ , and *APOE* genotype, warranting further investigation in independent and larger samples. Second, a majority of



the participants (n=52) in the present study had a diagnosis of MCI. Therefore, it is possible that the observed association may have been driven primarily by these participants. Due to the relatively small number of participants in the three diagnostic groups, we were unable to perform analyses within each diagnostic group to determine if there was an effect of diagnosis. Finally, genetic factors other than *APOE* may also play a role in modulating the association of plasma and brain A $\beta$ . Investigation of the impact of other known and novel AD-associated genetic variants on the relationship between plasma and brain A $\beta$  represents a possible future direction of this work.

## 5. Conclusions

In summary, we detected an association between soluble plasma A $\beta$  and fibrillar brain A $\beta$  that was modulated by *APOE*  $\epsilon$ 4 status. Replication and additional study in independent samples is needed to clarify the nature of this interaction, as well as to understand the underlying biological mechanisms. The present report suggests that plasma A $\beta$  levels have great potential as an AD biomarker and underscores the importance of genetic variation in the interpretation of plasma A $\beta$  levels.

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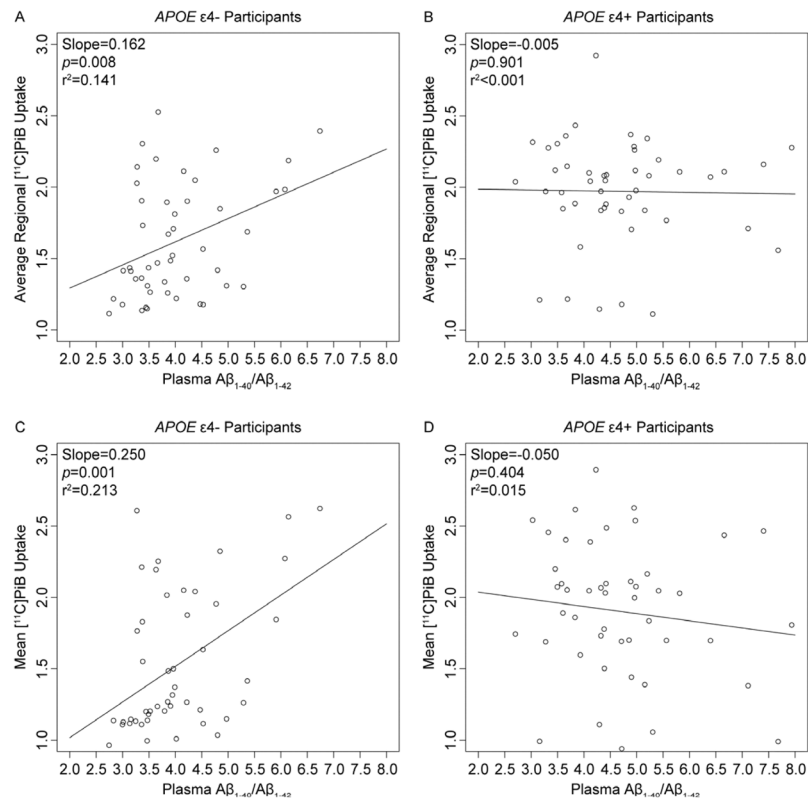
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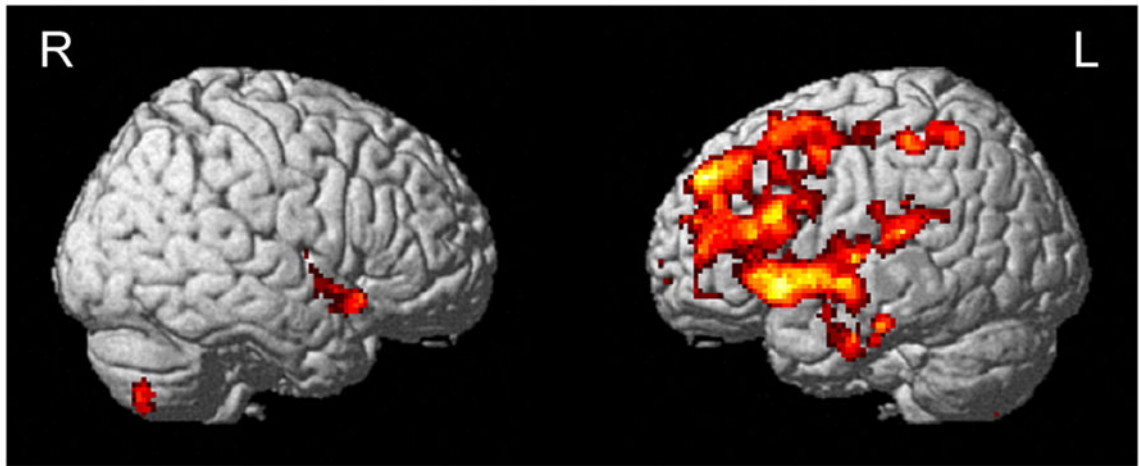
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**Fig. 1.** Scatter plots of plasma Aβ<sub>1-40</sub>/Aβ<sub>1-42</sub> versus average regional [<sup>11</sup>C]PiB uptake from the (Average regional [<sup>11</sup>C]PiB uptake=Plasma Aβ<sub>1-40</sub>/Aβ<sub>1-42</sub>+APOE ε4 status+(Plasma Aβ<sub>1-40</sub>/Aβ<sub>1-42</sub>\*APOE ε4 status)) model (A and B), and plasma Aβ<sub>1-40</sub>/Aβ<sub>1-42</sub> versus mean [<sup>11</sup>C]PiB uptake from the cluster identified in the (Voxel [<sup>11</sup>C]PiB uptake=Plasma Aβ<sub>1-40</sub>/Aβ<sub>1-42</sub>+APOE ε4 status+(Plasma Aβ<sub>1-40</sub>/Aβ<sub>1-42</sub>\*APOE ε4 status)) model (C and D).



**Fig. 2.** Brain regions identified in the (Voxel  $[^{11}\text{C}]\text{PiB}$  uptake = Plasma  $\text{A}\beta_{1-40}/\text{A}\beta_{1-42} + \text{APOE } \epsilon 4$  status + (Plasma  $\text{A}\beta_{1-40}/\text{A}\beta_{1-42} * \text{APOE } \epsilon 4$  status)) model (voxel-level threshold of  $p < 0.005$  (uncorrected), cluster size 200 voxels). The red-to-yellow scale indicates increasing statistical significance of association.

**Table 1**

## Sample characteristics

|   | AD (n=22)    | MCI (n=52)   | HC (n=22)    | <i>p</i> value* |
|---|--------------|--------------|--------------|-----------------|
| Initial [ <sup>11</sup> C]PiB scans at baseline/12-month/24-month visit | 3/13/6       | 11/36/5      | 0/20/2       | 0.034           |
| Age at time of scan (years, Mean±SD)                                    | 74.06±9.09   | 75.35±7.93   | 77.14±6.17   | 0.428           |
| Sex (Male/Female)   | 15/7         | 35/17        | 14/8         | 0.940           |
| Education (years, Mean±SD)  | 15.73±3.04   | 16.31±2.65   | 15.50±3.32   | 0.492           |
| Handedness (Right/Left)   | 20/2         | 48/4         | 17/5         | 0.165           |
| <i>APOE</i> ε4 status (ε4-/ε4+)   | 8/14         | 24/28        | 16/6         | 0.039           |
| Average regional [ <sup>11</sup> C]PiB uptake <sup>a</sup> (Mean±SD)    | 2.01±0.31    | 1.81±0.44    | 1.56±0.34    | 0.001           |
| Plasma Aβ <sub>1-40</sub> (pg/mL, Mean±SD)                              | 160.99±47.89 | 171.56±48.60 | 168.75±36.57 | 0.666           |
| Plasma Aβ <sub>1-42</sub> (pg/mL, Mean±SD)                              | 36.05±9.19   | 40.81±12.48  | 41.93±9.06   | 0.160           |
| Plasma Aβ <sub>1-40</sub> /Aβ <sub>1-42</sub> (Mean±SD)                 | 4.53±1.20    | 4.38±1.19    | 4.11±0.81    | 0.440           |

Abbreviations: AD, Alzheimer's disease; MCI, mild cognitive impairment; HC, healthy control.

\* For categorical variables, Pearson chi-square was used to compute the *p* value. For continuous variables, one-way analysis of variance was used to compute the *p* value.

<sup>a</sup> Average regional [<sup>11</sup>C]PiB uptake is the average of [<sup>11</sup>C]PiB uptake values from four brain regions: anterior cingulate, frontal cortex, parietal cortex and precuneus, normalized to cerebellum.

Table 2

Brain regions identified in the (Voxel [ $^{11}\text{C}$ ]PiB uptake = Plasma  $A\beta_{1-40}/A\beta_{1-42}$  + APOE  $\epsilon 4$  status + (Plasma  $A\beta_{1-40}/A\beta_{1-42}$  \* APOE  $\epsilon 4$  status) model (voxel-level threshold of  $p < 0.005$  (uncorrected), cluster size 200 voxels)

| Region                         | Broadmann Area |     |     | Peak value coordinates (mm) |         |                | Voxel-level |              |            | Cluster-level |  |  |
|--------------------------------|----------------|-----|-----|-----------------------------|---------|----------------|-------------|--------------|------------|---------------|--|--|
|                                |                | x   | y   | z                           | T value | $P_{FWE-corr}$ | k           | $P_{uncorr}$ | $P_{corr}$ |               |  |  |
| Left inferior frontal gyrus    | BA47           | -40 | 18  | -6                          | 3.92    | 0.713          | 6152        | <0.001       | <0.001     |               |  |  |
| Left superior temporal gyrus   | BA22           | -46 | 6   | -4                          | 3.85    | 0.774          |             |              |            |               |  |  |
| Left middle frontal gyrus      | BA6            | -30 | 12  | 60                          | 3.81    | 0.816          |             |              |            |               |  |  |
| Left superior frontal gyrus    | BA8            | -28 | 20  | 56                          | 3.76    | 0.855          |             |              |            |               |  |  |
| Left precentral gyrus          | BA4            | -34 | -20 | 52                          | 3.68    | 0.910          |             |              |            |               |  |  |
| Left insula                    | BA13           | -42 | -8  | -8                          | 3.58    | 0.955          |             |              |            |               |  |  |
| Left middle frontal gyrus      | BA8            | -24 | 24  | 50                          | 3.43    | 0.990          |             |              |            |               |  |  |
| Left middle frontal gyrus      | BA10           | -36 | 42  | 14                          | 3.40    | 0.993          |             |              |            |               |  |  |
| Left middle temporal gyrus     | BA21           | -58 | -10 | -8                          | 3.35    | 0.996          |             |              |            |               |  |  |
| Left superior frontal gyrus    | BA9            | -18 | 48  | 34                          | 3.29    | 0.998          |             |              |            |               |  |  |
| Left inferior frontal gyrus    | BA45           | -50 | 20  | 20                          | 3.24    | 0.999          |             |              |            |               |  |  |
| Left anterior cingulate        | BA32           | 0   | 44  | 12                          | 3.23    | 0.999          |             |              |            |               |  |  |
| Left superior frontal gyrus    | BA10           | -26 | 42  | 30                          | 3.19    | 1.000          |             |              |            |               |  |  |
| Left medial frontal gyrus      | BA10           | -2  | 58  | -4                          | 3.17    | 1.000          |             |              |            |               |  |  |
| Left inferior parietal lobule  | BA40           | -54 | -22 | 26                          | 3.16    | 1.000          |             |              |            |               |  |  |
| Left transverse temporal gyrus | BA41           | -48 | -26 | 10                          | 3.16    | 1.000          |             |              |            |               |  |  |
| Left postcentral gyrus         | BA40           | -48 | -34 | 54                          | 3.73    | 0.878          | 273         | 0.023        | 0.448      |               |  |  |
| Left inferior parietal lobule  | BA40           | -36 | -52 | 56                          | 3.54    | 0.968          |             |              |            |               |  |  |
| Left inferior temporal gyrus   | BA20           | -64 | -8  | -26                         | 3.32    | 0.998          | 231         | 0.035        | 0.586      |               |  |  |
| Left fusiform gyrus            | BA20           | -62 | -4  | -28                         | 3.20    | 1.000          |             |              |            |               |  |  |
| Left middle temporal gyrus     | BA21           | -54 | 0   | -18                         | 2.84    | 1.000          |             |              |            |               |  |  |
| Right inferior frontal gyrus   | BA47           | 42  | 14  | -14                         | 3.32    | 0.998          | 262         | 0.026        | 0.482      |               |  |  |
| Right superior temporal gyrus  | BA22           | 46  | 0   | -4                          | 3.16    | 1.000          |             |              |            |               |  |  |
| Right sub-gyral                | BA13           | 44  | 2   | -8                          | 3.08    | 1.000          |             |              |            |               |  |  |
| Right insula                   | BA13           | 42  | -6  | 4                           | 2.92    | 1.000          |             |              |            |               |  |  |



Abbreviations:  $p_{\text{FWE-corr}}$ . Voxel-level  $p$  value after family-wise error correction;  $k$ , number of voxels in cluster;  $p_{\text{uncorr}}$ . Cluster-level uncorrected  $p$  value;  $p_{\text{corr}}$ . Cluster-level  $p$  value after random field theory correction.