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Association of Trochlear Dysplasia with degenerative Abnormalities in the Knee:

Data from the Osteoarthritis Initiative

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Abstract

Objective—To evaluate trochlear morphology as a potential risk factor for patellofemoral osteoarthritis, determined by morphological and quantitative measurements of cartilage degeneration using 3T magnetic resonance imaging (MRI) of the knee.

Materials and Methods—MR images of right knees of 304 randomly selected subjects, aged 45-60 years, from the Osteoarthritis Initiative (OAI) progression cohort were screened for trochlear dysplasia, defined by an abnormal trochlear depth. Out of 304 subjects, n=85 demonstrated a shallow trochlea (depth 3mm; 28%). In these, and also in a random sample of controls with normal trochlear depth (n=50), the facetal ratio and the sulcus angle were calculated and knee structural abnormalities were assessed by using a modified Whole-Organ-MR-Imaging Score (WORMS). Cartilage segmentation was performed and T_2 relaxation times and patellar cartilage volume were determined. ANOVA and multivariate regression models were used for statistical analysis of the association of MRI structural measures and trochlear morphology.

Results—Knees with a shallow trochlea showed higher patellofemoral degeneration (WORMS mean \pm standard deviation, 11.2 \pm 0.5 versus 5.7 \pm 0.6; Multivariate regression, P<0.001) and lower patellar cartilage volume than controls (900±664mm³ versus 1671±671mm³; P<0.001). Knees with an abnormal medial-to-lateral facetal ratio (<0.4) showed increased patellofemoral WORMS scores (12.3 ± 0.9 versus 8.3 ± 0.5 ; P<0.001). Knees with an abnormal sulcus angle (>170°) also

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showed increased WORMS scores (12.2 \pm 1.1 versus 8.6 \pm 0.6; P=0.003). T₂ values at the patella were significantly lower in the dysplasia group with a shallow trochlea. However, significance was lost after adjustment for cartilage volume (P=0.673).

Conclusion—Trochlear dysplasia, defined by a shallow trochlea, was associated with higher WORMS scores and lower cartilage volume, indicating more advanced osteoarthritis at the patellofemoral joint.

Keywords

Patellofemoral joint; Magnetic Resonance Imaging; Osteoarthritis; Cartilage

Introduction

Patellofemoral joint disorders represent a common cause of anterior knee pain [1, 2]. As the largest sesamoid bone of the body, the patella functions to magnify the moment arm of the patellar tendon; thereby increasing the effectiveness of extensor musculature [3]. Between 30 and 90 degrees of flexion, the patella is engaged with the trochlea. The morphology of the trochlea, in addition to several other static and dynamic stabilizers, helps to keep the patella stable during this engagement.

Trochlear dysplasia is a geometric abnormality in the shape and depth of the trochlear groove. It can be assessed with axial [4] and lateral knee radiographs [5], computed tomography or MRI of the knee. On MRI, Pfirrmann et al. proposed that a trochlear depth of 3 mm or less or a facet asymmetry defined by an abnormal medial-to-lateral facetal ratio of less than 0.4 have good sensitivity and specificity for trochlear dysplasia [6]. On plain radiographs, a sulcus angle >150° indicates trochlear dysplasia. However, two-dimensional imaging underestimates the angle and shows substantial differences of about 20° to more accurate MR measurements [7–10].

A dysplastic trochlea can lead to abnormal patellar tracking, chronic patellar dislocation and to an abnormal distribution of loading, which increase the risk for osteoarthritis (OA) [11, 12]. Most studies have used plain radiographs to evaluate trochlear dysplasia and OA. There is little information about trochlear dysplasia and its association with degenerative changes at the patellofemoral joint when evaluated with 3T MRI studies, which are particularly sensitive to detecting early degenerative biochemical intrasubstance changes. T₂ relaxation time measurements can be used as a biomarker to non-invasively detect and quantify intrasubstance degeneration, more specifically collagen disruption and water content changes.

The Osteoarthritis Initiative (OAI) was launched by the NIH and is a longitudinal, observational multi-center study that includes nearly 5000 participants. One of the primary goals of the study is to better understand the evolution of knee OA and associated factors (http://www.oai.ucsf.edu/) [13].

The purpose of the present study was to determine whether knees with an abnormal trochlear depth, an abnormal medial-to-lateral trochlear facetal ratio or an abnormal sulcus angle have a higher prevalence of MRI findings of OA, as measured by semi-quantitative morphological joint scores, cartilage volume and T_2 relaxation time.

Materials and Methods

Subjects

From the Progression cohort of the OAI, 304 subjects aged 45 to 60 were randomly selected and measurements of trochlear dysplasia on MRIs of their right knee were performed. The progression cohort is characterized by the presence of symptomatic knee OA. A shallow trochlea was identified in 85 subjects. A control group of 50 right knees without shallow trochlea was randomly selected from the remaining subjects with normal trochlear depth. An abnormal medial-to-lateral facetal ratio was found in 30/ 135 subjects. An abnormal sulcus angle was found in 22/ 135 subjects. There was no significant difference regarding age, BMI, gender, Physical Activity Scale for the Elderly (PASE) [14], and knee-bending activities between the subjects with a shallow trochlea (n=85) versus controls (n=50; P>0.05 for all comparisons; Table 1). There was no significant difference between subjects with an abnormal facetal ratio (n=30) and controls (n=105; gender, P=0.686; BMI, P=0.327; age, P=0.973; knee-bending, P=0.462; PASE, P=0.641). Also, there was no significant difference between subjects with an abnormal sulcus angle (n=22) and controls (n=113; gender, P=0.772; BMI, P=0.113; age, P=0.486; knee-bending, P=0.364; PASE, P=0.199).

The study protocol, amendments and informed consent documentation were reviewed and approved by the local institutional review boards of the participating OAI sites. Datasets 0.C.1 and 0.E.1 used in the preparation of this article were obtained from the OAI public website (http://www.oai.ucsf.edu/). Exclusion criteria for the OAI were rheumatoid arthritis, bilateral severe knee joint space narrowing, contraindications or inability for MRI, and poor MR quality.

Bilateral knee radiographs

Bilateral standing posterior anterior (PA) "fixed flexion" plain radiographs of the knee were obtained in a plexiglass positioning frame (SynaFlexerTM; CCBR-Synarc, San Francisco, California) with 20–30° flexion and 10° internal rotation of bilateral feet. Kellgren-Lawrence (KL) scores were assessed in our institution (T.M.L., 22 years of experience).

MR imaging

MRI examinations were obtained with dedicated 3T MRI systems (Trio, Siemens, Erlangen, Germany). A standard knee coil was used. The following sequences of the right knee were analyzed in this study: (1) coronal 2D intermediate-weighted (IW) fast spin-echo (FSE) sequence (TE / TR = 29 / 3850 ms, field of view (FOV) = 14 cm, slice thickness = 3 mm, inplane spatial resolution = 0.365×0.456 mm², flip angle = 180, bandwidth = 352 Hz / pixel), (2) sagittal 3D dual-echo steady-state (DESS) sequence with water excitation (WE) and coronal and axial reformations (TE / TR = 4.7 / 16.3 ms, field of view (FOV) = 14 cm, slice thickness = 0.7 mm, in-plane spatial resolution = 0.365×0.456 mm², flip angle = 25, bandwidth = 185 Hz / pixel, (3) sagittal 2D IW fat-suppressed (fs) FSE sequence (TE / TR = 30 / 3200 ms, field of view (FOV) = 16 cm, slice thickness = 3 mm, in-plane spatial resolution = 0.357×0.511 mm², flip angle = 180, bandwidth = 248 Hz / pixel) and (4) a sagittal 2D multislice multischo (MSME) spin echo (SE) sequence (TR = 2700 ms, seven TEs = 10 ms, 20 ms, 30 ms, 40 ms, 50 ms, 60 ms, 70 ms, field of view (FOV) = 12 cm, slicethickness = 3 mm with 0.5mm gap, in-plane spatial resolution = 0.313×0.446 mm², bandwidth = 250 Hz / pixel), which was used to obtain quantitative T₂ relaxation time measurements (21).

Trochlear Morphology

Trochlear measurements were performed in rights knees using the axial reconstructed image from the 3D dual-echo in steady state (DESS) sequence with selective water excitation (WE)

in all right knees. At the axial slice 30 mm proximal to the knee joint line [6], the following trochlear measurements were obtained (Figure 1; upper row): (i) the maximal anteroposterior distance from the medial femoral condyle to the line paralleling the posterior aspects of both femoral condyles (distance a), (ii) the maximal anteroposterior distance from the lateral femoral condyle to the line paralleling the posterior aspects of both femoral condyle to the line paralleling the posterior distance from the lateral femoral condyle to the line paralleling the posterior aspects of both femoral condyles (distance b), (iii) the minimal anteroposterior distance from the deepest point in the trochlear groove to the line paralleling the posterior aspects of both femoral condyles (distance c), (iv) the length of the medial (distance d) and lateral (distance e) facets of the patella. The trochlear depth was calculated as [(a + b) / 2] - c. A trochlear depth of 30 mm or less was considered shallow. The facetal ratio was calculated as d / e. A facetal ratio of 0.4 or less was considered abnormal. The sulcus angle (α) was calculated as 180° – asin ((a - c)/e) – asin ((b - c)/d). A sulcus angle above 170° was considered as abnormal.

Semi-quantitative, morphological image analyses

MR images of the right knee were reviewed on picture archiving communication system (PACS) workstations (Agfa, Ridgefield Park, NJ, USA). Two musculoskeletal radiologists (S.C.T., T.M.L.) separately scored knees using the UCSF modified whole-organ magnetic resonance imaging score (WORMS) [15–17]; if scores were not identical, consensus readings by both radiologists were performed. For the patellofemoral joint, the following joint structures were evaluated: (i) cartilage, (ii) bone marrow edema pattern, (iii) subchondral cysts and (iv) the patellar tendon. For the femorotibial joint compartment, (iv) collateral ligaments and (v) meniscus abnormalities were evaluated additionally to (i) to (iii). Cartilage was scored as follows: 0=normal; 1=increased signal; 2=partial-thickness defect <1 cm; 2.5=full-thickness defect <1 cm; 3=multiple areas of partial-thickness defects, or >1 cm but <75% of the region; 4= 75% of the region; 5=multiple areas of full- thickness loss or a >1 cm but <75% of the region; 6=75% of the region. Subchondral bone marrow edema pattern (BME) was graded as follows: 0=none; 1=<0.5 to 2.0 cm; 3=>2.0 cm. Subarticular cysts were graded as follows: 0=none; 1=<0.5cm; 2=0.5 to 2.0 cm; 3=>2.0cm. The patellar tendon and the collateral ligaments were graded as either normal or abnormal. Meniscus changes were graded in six regions (medial and lateral: anterior, body, posterior) by the following: 0=normal; 1=intra-substance abnormalities; 2=non-displaced tear; 3=complex tear; 4=maceration. For the entire medial and lateral meniscus, grading was defined by the following: 0 if all compartments were graded as 0, 1 if one or more compartments were graded as 1, 2 if one compartment was graded as 2, 3 if more than one compartment was graded as 2, 4 if one or more compartments were graded as 3, 5 if one compartment was graded as 4, 6 if more than one compartment was graded as 4. Maximum WORMS scores are summarized in Table 2.

T₂ relaxation time measurements and patellar cartilage volume measurements

Segmentation of the cartilage at the patella and trochlea, the medial and lateral femoral condyle and medial and lateral tibia plateau, was performed by one investigator (S.C.T.) and supervised by a musculoskeletal radiologist (T.M.L.) to generate T_2 maps from the sagittal 2D MSME SE sequences of the right knee. Images were transferred to a remote SUN/ SPARC workstation (Sun Microsystems, Mountain View, CA, USA) and analyzed with software developed at our institution using an Interactive Display Language (IDL; Research Systems, Boulder, CO, USA) environment. An IDL routine was used to simplify the manual drawing of splines delineating cartilage areas and to calculate the mean T_2 values from the regions of interest created in the T_2 maps. T_2 values were calculated as global values (mean of all compartments), and for each individual compartment. Using the same software, segmentation for patellar cartilage volume measurements was performed by one radiologist (P.M.J.) and supervised by a musculoskeletal radiologist (T.M.L.). Absolute cartilage

volume (mm³) was calculated for the patellar compartment from the regions of interest created in the maps.

Reproducibility measurements

Reproducibility for the semi-quantitative analyses of the WORMS score for each compartment from our group was reported previously [18]. Inter-observer agreement for T_2 measurements in our group was described previously with an inter-reader reproducibility error for mean T_2 of 1.57 % or 0.53 ms [19]. Mean intra-reader reproducibility for T_2 measurements was 1.66 % or 0.55 ms.

Statistical Analysis

All statistical analyses were performed with JMP software Version 9 (SAS Institute, Cary, NC). The level of significance for all calculations was defined as p < 0.05. For covariates, mean values are reported with ± standard deviation (SD). KL-scores were considered as ordinate variables. T-tests were used to detect differences between the groups. Multivariate regression analyses were performed to analyze the association of either trochlear abnormality (abnormal trochlear depth, abnormal facetal ratio and abnormal sulcus angle) with WORMS scores and T_2 relaxation time. Mean values are reported with \pm Standard Error of the Mean (SEM), if not otherwise stated. Cartilage volume was included in the multivariate regression model to account for possible associations between cartilage volume and T_2 relaxation time. As previously suspected [13, 20], T_2 values may reach a ceiling or even decrease with increasing cartilage loss. Such an association would affect T₂ values found with OA, which are typically higher than normal (not lower) due to increased water content and collagen fibrillation. Total WORMS scores and scores for cartilage and meniscus were approximately normally distributed and considered as linear values in this model. BME and subchondral cysts were analyzed as dichotomous variables (absence versus presence of abnormalities, defined as score >0) using a logistic regression, since these variables were not normally distributed. All regression models were adjusted for age, gender and OA risk factors, including previous injury or surgery at the knee, family history of joint replacement, presence of Herbeden's nodes and BMI.

Results

Study cohort

Out of 304 individuals from the OAI progression cohort, 85 had a shallow trochlear groove (trochlear depth 3 mm) in the right knee with a mean trochlear depth of 2.0 ± 1.0 mm (mean \pm standard deviation (SD)). In the control knees, the mean trochlear depth was 4.4 ± 1.0 mm. Twenty-six of 85 knees with a shallow trochlea and 4 of 50 control knees had a medial-to-lateral trochlear facetal ratio of less than 0.4. The 30 knees with a low trochlea facetal ratio had an average ratio of 0.35 ± 0.04 , while the subjects with a normal trochlea facetal ratio (n=105) had a mean ratio of 0.57 \pm 0.11. The mean length \pm SD of the medial and lateral facet in the entire cohort were 11.4 ± 3.0 mm and 22.1 ± 2.5 mm, respectively. In the subcohort with an abnormal facetal ratio means of 7.9 ± 1.0 mm and 22.8 ± 2.6 mm were detected; in the subcohort with a normal facetal ratio means of 12.4 ± 2.5 mm and 21.9 ± 2.4 mm were found. The mean sulcus angle in the entire cohort was $162 \pm 10^{\circ}$. Twenty-two of the knees with a shallow trochlea and no control knees had an abnormal sulcus angle of $>170^{\circ}$. The 22 knees with a high sulcus angle had an average angle of $177 \pm 8^{\circ}$, while the subjects with a normal sulcus angle (n=113) had an average angle of $159 \pm 8^{\circ}$. A significant difference in sulcus angle was found between the group with a shallow trochlea and the control group (167 $\pm 8^{\circ}$ versus 152 $\pm 6^{\circ}$; P<0.001).

Morphological patellofemoral abnormalities

The total WORMS score of the patellofemoral joint was 5.7 \pm 0.6 (mean \pm SEM) in the control group (Figure 2). In individuals with a shallow trochlea it was significantly higher (11.2 \pm 0.5; P<0.001). The patellofemoral WORMS score was also significantly **higher in individuals with low trochlear facetal ratio or abnormal sulcus angle than in the corresponding control cohort (facetal ratio, 12.3 \pm 0.9 versus 8.3 \pm 0.5; P<0.001; sulcus angle, 12.2 \pm 1.1 versus 8.6 \pm 0.6; P=0.003; Figure 2).

Considering the individual parameters of the patellofemoral WORMS score, subjects with trochlear dysplasia showed significantly more cartilage defects at the patellar cartilage as well as at the trochlear cartilage (P<0.001). Significantly higher scores for bone marrow edema pattern and subchondral cysts were found in individuals with a shallow trochlea in the trochlear and patellar compartments and in individuals with an abnormal sulcus angle in the patellar compartment (P<0.05). Subjects with a low trochlear facetal ratio had significantly more bone marrow abnormalities (Table 3).

Morphological femorotibial abnormalities

Only trochlear depth was associated with an increased WORMS score at the medial tibiofemoral compartment (5.0 ±0.8 for subjects with a deep trochlea versus 7.4 ±0.7 for subjects with a shallow trochlea; P=0.003; Table 3). Subjects with large sulcus angles had significantly higher WORMS scores at the lateral tibiofemoral compartment compared to controls (8.2 ±1.3 versus 5.4 ±0.7; P=0.026). Neither trochlear depth (medial meniscus, P=0.400; lateral meniscus, P=0.110) nor trochlear facetal ratio (P=0.073; P=0.532) was significantly associated with meniscus abnormalities. The mean WORMS score for the medial meniscus was 2.2 ±0.2 for the cohort with abnormal trochlear depth and 1.9 ±0.3 for controls (P=0.400). Subjects with an abnormal sulcus angle had more severe lateral meniscus lesions than corresponding controls (2.9 ±0.4 versus 1.8 ±0.2; P=0.012). For the medial femorotibial compartment, subjects with a shallow trochlea had significantly increased maximum cartilage scores (4.0 ±0.3 versus 2.6 ±0.4; P=0.010).

T₂ relaxation time measurements

Global T₂ relaxation time of the entire knee was not significantly associated with trochlear depth, trochlear facetal ratio or sulcus angle (P=0.442, P=0.903 and 0.541; Table 4). For individuals with abnormal trochlear depth, the mean global T₂ value was 44.4 \pm 0.3 ms, while the control group had a mean global value of 44.9 \pm 0.4 ms. When femoropatellar compartments were analyzed separately, individuals with a shallow trochlea had significantly lower T₂ values than controls at the patellar compartment (40.9 \pm 0.5 ms versus 42.7 \pm 0.6 ms; P=0.037). Patellar T₂ values did not show a significant difference in individuals with abnormal trochlear facetal ratio compared to controls (40.8 \pm 0.9 ms versus 41.8 \pm 0.4 ms; P=0.310) or in individuals with an abnormal sulcus angle compared to controls (41.5 \pm 1.0 ms versus 41.7 \pm 0.5 ms; P=0.464).

Patella cartilage volume measurements

Given the unexpected low T_2 values at the patella, the association of shallow trochlea and lower T_2 values was investigated by including patellar cartilage volume in the multivariate models because there are hints that T_2 values do not increase further or even decrease with advanced cartilage loss and OA. Increasing patellar T_2 values correlated significantly with increasing cartilage volume (Figure 3; R=0.44; P<0.001). Including cartilage volume (mm³) in the regression model, it showed a significant relationship with patellar T_2 values (P=0.003) and the influence of trochlear depth was eliminated (P=0.673). Low trochlear depth was further associated with a small cartilage volume at the patella (P<0.001; shallow trochlea, $900 \pm 72 \text{ mm}^3$, control, $1671 \pm 95 \text{ mm}^3$). Individuals with an abnormal facetal ratio also had smaller cartilage volume than individuals with normal facetal ratios, but the difference was not significant ($1237 \pm 73 \text{ mm}^3$ versus $1004 \pm 137 \text{ mm}^3$; P=0.263). An abnormal sulcus angle was significantly associated with smaller patellar cartilage volume ($795 \pm 158 \text{ mm}^3$ versus $1259 \pm 94 \text{ mm}^3$; P<0.001).

Discussion

This cross-sectional study study examined the association of trochlear dysplasia, assessed by 3.0T MRI and defined as (i) a trochlear depth of 3 mm or less, (ii) a medial-to-lateral facet ratio of 0.4 or less and (iii) a sulcus angle of $>170^{\circ}$ with the presence and severity of MRI findings of knee OA. Patellofemoral WORMS scores were significantly higher in the group with a shallow trochlea and patellar cartilage volume was significantly lower in the group with a shallow trochlea, suggesting a strong association of trochlear dysplasia with more severe patellofemoral joint degeneration.

A dysplastic joint component can potentially lead to early degeneration and damage of the joint. At the knee, a dysplastic trochlea has been shown to contribute to patellar maltracking and recurrent dislocations [21]. Minor dislocations can cause instability and chronic stress on the cartilage, which may lead to early OA. This was previously shown by Dejour et al on knee radiographs and computed tomography. On a lateral knee radiograph, the "crossing sign" was described, a geometrical abnormality at the cranial portion of the trochlea that prevents proper engagement of the patella during the early phases of knee flexion [22]. However, two-dimensional imaging may lead to misinterpretation of the patellar morphology [7]. Therefore, 3.0T MRI was used in our study for a more detailed analysis of cartilage, tendon and bone marrow and found similar results; individuals with lower trochlear depth showed significantly increased patellofemoral degeneration. Pfirrmann et al previously demonstrated a correlation of a trochlear depth of 3 mm or a medial-to-lateral facetal ratio of 0.4, measured in MR images, with trochlear dysplasia, diagnosed in lateral knee radiographs [6]. Further, the parameter "sulcus angle" was determined due to its clinical relevance regarding the diagnosis of trochlear dysplasia and postoperative follow-up measurements [9, 23, 24]. A sulcus angle of >150° on plain radiographs was reported to indicate trochlear dysplasia [9]. However, radiographs underestimate this angle as compared to MR measurements [8]. The sulcus can be measured either from the subchondral bone or from the articular cartilage; both have been shown to be highly accurate [10]. Van Huyssteen et al described a mean bony sulcus angle of 168° as measured in MRI, while the mean cartilage sulcus angle was 187° [25]. Using the osseous surface as a reference, Toms et al reported that the sulcus angle was larger in patients with severe cartilage defects (mean $= 173^{\circ}$) than in patients with normal cartilage (mean $= 151^{\circ}$) in a young patient cohort (<40 years) [10]. Salzmann et al. found a mean sulcus angle of 164° in patients with type B dysplasia (144° in plain radiographs) and 168° in patients with type C dysplasia (146° in plain radiographs) [8]. Based on these findings, 170° was selected as a threshold for an abnormal bony sulcus angle in our MRI analyses, which was present in 22/135 subjects.

The ability to detect morphological trochlear abnormalities on an MRI study can potentially influence the management choices of the referring clinician. Individuals who underwent a Henri Dejour trochleoplasty for a dysplastic trochlea reported an improvement in symptoms [26].

Total patellofemoral WORMS score was increased in individuals with trochlear dysplasia. Once cartilage loss occurs, changes in MRI morphology are frequently seen [16]. WORMS values for cartilage lesions, bone marrow edema pattern, cysts and ligament abnormalities, were increased in the trochlear dysplasia group in this study.

Global T₂ values, which are commonly used in the evaluation of early intrasubstance cartilage degeneration [27], were similar between the two groups. For patellar cartilage however, T₂ values of individuals with low trochlear depth demonstrated significantly lower T_2 values. These findings were unexpected, surprising and contradictory, since higher T_2 values usually correlate with presence of OA [28]. On the contrary, the lower T₂ values may be explained by greater cartilage loss in subjects with low trochlear depth, since significantly more cartilage abnormalities were detected in the trochlear dysplasia group. At least half of the individuals with low trochlear depth presented with full thickness cartilage loss at the patella (WORMS 5 or 6). Prior studies have shown that although T_2 relaxation time is correlated to histological degeneration of cartilage and a good marker for early OA, it may not be suitable for analysis of advanced degenerative joint disease [29]. David-Vaudey et al noticed early stage OA was associated with increased T₂, followed by slightly lower T₂ values for more severe lesions. They explained these findings by the fact that changes in collagen fibril anisotropy, associated with an increased T₂, precede changes in collagen content and a loss of water content, associated with slightly declining T_2 [30]. Further, during OA progression, the region most heavily affected by cartilage loss is the superficial cartilage layer, which also happens to account for the highest T_2 values [31]. With the additional risk factor of trochlear dysplasia, T₂ values may not increase further with worsened cartilage degeneration, which is consistent with Crema et al [13]. The additional cartilage loss, especially the superficial layer, which usually incooperates high T₂ values, may be responsible for the unexpected results. Therefore, cartilage volume at the patella was investigated and a significant association of lower cartilage volume with an abnormal trochlea depth was detected. Including cartilage volume in the multivariate regression model eliminated the significant influence of trochlea abnormalities on patella T₂ values but instead a low cartilage volume was associated with lower T₂ values. The additional cartilage loss likely accounts for the decrease in T₂ values and is highlighting the careful interpretation of T₂ relaxation time measurements in the context of morphological cartilage loss in subjects with advanced OA.

There are several limitations to this study. First, this study was cross-sectional and a longitudinal study is needed to better characterize the relationship between trochlear dysplasia and OA. In a cross-sectional study, effect cause has to be considered as an alternative possibility. Patellofemoral OA could potentially lead to secondary trochlear remodeling, resulting in abnormal trochlear depth, abnormal facetal ratio and abnormal sulcus angle. Individuals were recruited from the OAI progression cohort and all subjects already had OA, many of them already had severe OA changes at the patellofemoral joint, which made the interpretation of T₂ relaxation time measurements challenging. Further research is needed to determine if irregular trochlear morphology is also found in normal participants or participants with early OA. Moreover, only the shallow trochlea (n=85) and control participants (n=50) were included in analyses for an abnormal facetal ratios or sulcus angles.

In summary, our study demonstrated that trochlear dysplasia, defined by a shallow trochlea, a low medial-to-lateral trochlear facetal ratio or an abnormal sulcus angle, was associated with MRI findings indicating patellofemoral OA, including higher WORMS scores and smaller patella cartilage volume. In conclusion, these findings demonstrate that detecting and especially monitoring morphological trochlear properties on 3.0T MRI may be clinically relevant to identify early OA patients and may be important for risk evaluation, treatment decisions and further follow-up of subjects at risk for patellofemoral OA.

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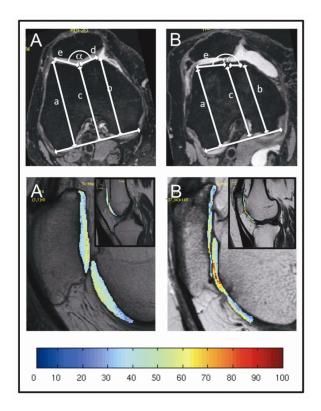


Figure 1.

Upper row: Measurements in the axial 3D DESS sequence with selective water excitation, 30 mm proximal of the joint line in a normal (A) and abnormal (B) patellofemoral joint with trochlear dysplasia. Lower row: Corresponding T_2 color maps of the patellofemoral joint overlaid with the first-echo images of MSME sequences of the same subjects. Blue color indicates low cartilage T_2 , while red color indicates high cartilage T_2 . Severe loss of the superficial cartilage and only a thin remaining profound cartilage layer results in low T_2 values.

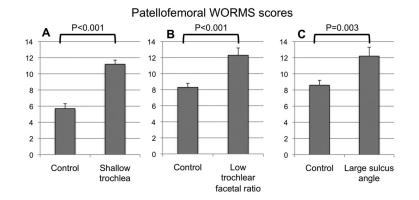


Figure 2.

Total WORMS score of the patellofemoral joint in subjects with trochlear dysplasia versus control. Subjects presenting A: a shallow trochlea of 3mm, B: a small facetal ratio of 0.4 and C: a large sulcus angle of $>170^{\circ}$ presented more patellofemoral abnormalities than control subjects.

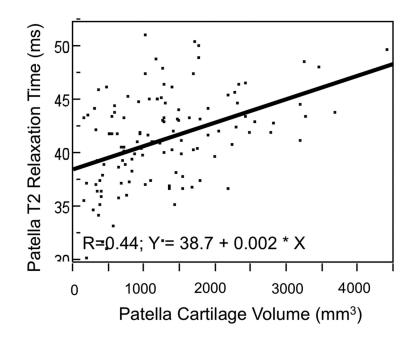


Figure 3.

Scatter plot with bivariate linear fit, visualizing the correlation of patellar cartilage T_2 values with patellar cartilage volume. Smaller cartilage volumes were associated with lower T_2 relaxation times.

Table 1

Epidemiological data of study cohorts. The control cohort was randomly selected.

	Individuals with shallow trochlea	Control	P-Value
Number of subjects (n)	85	50	
Age (years)	64.0 (SD: ±9.2)	64.2 (SD: ±9.8)	0.875
Gender (female, %)	81 %	80%	0.869
body mass index (kg/m2)	28.3 (SD: ±4.1)	28.2 (SD: ±4.6)	0.862
PASE (absolute score)	140.6 (SD: ±70.7)	141.8 (SD ±71.7)	0.929
Knee bending actividies (% positive)	72.9 %	77.4 %	0.510
Kellgren-Lawrence grade (0:1:2:3:4)	2:3:45:35:0	6:8:26:10:0	< 0.001

Table 2

Calculation of total WORMS score for the patellofemoral joint and the medial and lateral femorotibial joint.

	Patellofemo	oral total WORMS	Femorotibial total WO	RMS
		Max. score		Max. score
Cartilage	Patella	6	Femoral Compartment	6
	Trochlea	6	Tibial Compartment	6
BME	Patella	3	Femoral Compartment	3
	Trochlea	3	Tibial Compartment	3
Cysts	Patella	3	Femoral Compartment	3
	Trochlea	3	Tibial Compartment	3
Tendon	Patella	1	Collateral tendon	1
Meniscus			Total Meniscus score	6
Total score		25		31

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Summary of mean WORMS sores regarding individual parameters and total score for the patellofemoral joint and the femorotibial joint, depending on trochlea depth, medial-to-lateral trochlea facetal ratio and sulcus angle.

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A:		Trochlear depth	th		Facetal ratio			Sulcus angle		
Compartment	Parameter	Shallow n=85	Normal n=50	Difference (Lower 95% CI; Upper 95% CI)	Abnormal n=30	Normal n=105	Difference (Lower 95% CI; Upper 95% CI)	Abnormal n=22	Normal n=113	Difference (Lower 95% CI; Upper 95% CI)
Patellofemoral	Total WORMS	11.2×0.5	5.7 imes 0.6	5.5 (3.9; 7.0)*	12.3×0.9	8.3×0.5	3.9 (1.9; 6.0)*	12.2×1.1	8.6 imes 0.6	3.7 (1.3; 6.1)*
Patella	Cartilage	4.5×0.2	3.1×0.2	$1.4\ (0.9; 1.9)^{*}$	4.9×0.3	3.7×0.2	$1.2\ (0.5;\ 1.8)^{*}$	4.8×0.3	3.8×0.2	$1.1 (0.4; 1.8)^{*}$
Trochlea	Cartilage	3.5×0.2	1.6×0.3	1.9 (1.2; 2.5)*	4.0×0.2	2.5×0.2	$1.5\ (0.7;\ 2.3)^{*}$	3.7×0.5	2.6×0.2	$1.1\ (0.1;\ 2.0)^{*}$
	Total WORMS	7.4×0.7	5.0 imes 0.9	2.5 (0.4; 4.5)*	6.1 imes 1.1	6.6 imes 0.6	0.4 (-2.0; 2.9)	8.0 imes 1.3	6.2 imes 0.7	1.7 (-1.1; 4.5)
Medial femorotibial	Meniscus	2.2×0.2	1.9×0.3	0.4 (-0.4; 1.1)	1.5 imes 0.4	2.3×0.2	0.8 (-0.1; 1.7)	1.9 imes 0.5	2.2×0.3	0.4 (-0.7; 1.4)
	Cartilage (Sum)) 4.0×0.3	2.6 imes 0.4	$1.4\ (0.4; 2.5)^{*}$	3.7×0.6	3.4×0.3	0.3 (-1.0; 1.5)	4.3×0.7	3.3×0.4	0.9 (-0.5; 2.4)
	Total WORMS	6.4×0.6	4.8×0.8	1.7 (-0.4; 3.7)	6.3×1.1	5.7 imes 0.6	0.6 (-1.8; 3.1)	8.2 ×1.3	5.4 imes 0.7	3.0 (0.4; 5.7)*
Lateral femorotibial	Meniscus	2.2×0.2	1.6×0.3	$0.6 \ (-0.1; 1.3)$	2.2×0.4	1.9×0.2	0.3 (-0.6; 1.2)	2.9 ×0.4	1.8×0.2	$1.2\ (0.3;\ 2.2)^{*}$
	Cartilage (Sum)) 3.7 ×0.4	2.9 imes 0.5	0.8 (-0.4; 2.0)	3.6×0.6	3.3×0.3	0.3 (-1.1; 1.7)	4.5×0.7	3.2×0.4	1.5 (-0.1; 3.0)
B:		Trochlear depth			Facetal ratio			Sulcus angle		
Compartment	Parameter	Shallow n=85 I	Normal n=50	Odds ratio (Lower 95% CI; Upper 95% CI)	Abnormal n=30	Normal n=105	Odds ratio (Lower 95% CI Upper 95% CI)	Abnormal n=22	Normal n=113	Odds ratio (Lower 95% CI; Upper 95% CI)
Patella	BME	65/85 2	20/50	5.2 (1.4; 11.8)*	24/30	61/105	3.0 (1.2; 8.8) [*]	19/22	66/113	5.7 (1.7; 26.4)*
	Cyst	17/85 (0/50	– (6.5; -) *	4/30	13/105	1.0 (0.2; 3.3)	6/22	11/113	4.1 (1.2; 13.9)*
Trochlea	BME	46/85	11/50	7)*	20/30	37/105	3.7 (1.6; 9.1)*	14/22	43/113	2.5 (1.0; 6.9)
	Cyst	19/85 (0/50	- (7.1; -)*	8/30	11/105	2.9 (1.0; 8.3) [*]	6/22	13/113	2.5 (0.8; 7.8)
Medial femorotibial	Medial BME	27/85	9/50 2	ŝ	11/30	25/105	2.1 (0.8; 5.2)	10/22	26/113	3.2 (1.1; 9.4)*
	Medial Cyst	5/85	- 1/50	- (0.4; -)	0/30	6/105	0.0 (0; 5.8)	3/22	3/113	17.4 (2.1; 187.8)*
Lateral femorotibial	Lateral BME	12/85	6/50	1.2 (0.4; 3.8)	4/30	14/105	1.1 (0.3; 3.4)	5/22	13/113	2.9 (0.8; 10.1)
	Lateral Cyst	4/85	2/50	1.3 (0.2;9.8)	2/30	4/105	0.0 (0; 3.5)	1/22	5/113	1.9 (0.1; 15.2)

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A: Adjusted I means × SEM and differences are presented for numeric outcomes.

B: The ratio n (abnormal scores)/ n (total) is presented for dichotomous variables (ratios are not adjusted; P-values, odds ratios and confidence intervals are adjusted J.

* P<0.05 ¹All regression models were adjusted for age, gender and OA risk factors, including previous injury or surgery at the knee, family history of joint replacement, presence of Herbeden's nodes and BMI.

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Table 4

Mean cartilage T_2 relaxation time values (ms) for subjects with trochlear dysplasia.

T2	Trochle	Trochlear depth			Facetal ratio	ratio			Sulcus angle			
Compartment	Shallow n=85	Shallow n=85 Normal n=50 P	4	Difference (lower 95% CI; upper 95% CI)	Abnormal n=30 Normal n=105	Normal n=105	Ч	Difference (lower 95% CI; upper 95% CI)	Abnormal n=22 Normal n=113	Normal n=113	Ч	Difference (lower 95% CI; upper 95% CI)
Global	44.4×0.3	44.9×0.4	0.442	0.442 0.5 (-0.6; 1.4)	44.7 ×0.6	44.6×0.3	0.903	0.1 (-1.1; 1.4)	44.5×0.7	44.6×0.3	0.541	0.4 (-1.0; 1.8)
Patella	40.9 imes 0.5	42.6 imes 0.6	0.037^{*}	0.037^{*} 1.7 (0.2; 3.1)	40.8×0.9	41.8×0.4	0.306	1.1 (-0.8; 2.9)	41.5×1.0	41.7×0.5	0.464	0.8 (-1.3; 2.8)
Trochlea	45.7×0.5	45.7 imes 0.6	0.973	0.1 (-1.3; 1.5)	45.9×0.4	44.9×0.8	0.251	1.0 (-0.7; 2.7)	46.2×1.0	45.6×0.5	0.873	0.2 (-1.8; 2.1)
Medial femorotibial	45.7 imes 0.6	46.0 imes 0.6	0.667	0.2 (-0.9; 1.4)	46.2 imes 0.8	45.8 imes 0.5	0.430	0.4 (-0.9; 1.8)	45.6×0.8	45.9×0.4	0.489	0.6 (-1.0; 2.2)
Lateral femorotibial	44.4×0.6	44.4×0.7	0.901	44.4×0.7 0.901 0.0 (-1.2; 1.3)	44.8×0.8	44.3×0.6	0.280	0.7 (-0.8; 2.1)	44.1×0.8	44.4×0.4	0.604	0.5 (-1.3; 2.2)