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# Daytime Sleepiness Is Associated with Decreased Default Mode Network Connectivity in Both Young and Cognitively Intact Elderly Subjects

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**Study Objectives:** Sleep deprivation and daytime somnolence impair numerous aspects of physical, cognitive, and memory performance. However, most studies examining the effect of somnolence on brain function focus on acute sleep restriction in young adults. We examine the relationship between chronic daytime somnolence and connectivity in six brain networks in both young and elderly subjects using stimulus-free resting-state functional magnetic resonance imaging.

Design: Cross-sectional.

Setting: Outpatient research at the Massachusetts General Hospital.

**Participants:** Young (n = 27) and elderly (n = 84) healthy, cognitively normal volunteers. **Interventions:** None.

**Measurements and Results:** Compared with young subjects, cognitively normal elderly adults report less daytime somnolence on the Epworth Sleepiness Scale (ESS) (P = 0.019) and display reduced default mode network (DMN) connectivity (P = 0.004). Across all subjects, increasing daytime sleepiness was associated with decreasing functional connectivity in the DMN (P = 0.003, partial r of ESS = -0.29). There was no difference in the slope of this relationship between young adults and elderly subjects. No other cortical networks were correlated with daytime sleepiness. Daytime sleepiness and DMN connectivity were not related to sex, brain structure, or body mass index.

**Conclusions:** These findings suggest that daytime sleepiness is associated with impaired connectivity of the DMN in a manner that is distinct from the effects of aging. This association is important to consider in any study using DMN connectivity as a biomarker. Additionally, these results may help identify those subjects at risk for future memory decline.

Keywords: Epworth Sleepiness Scale, functional connectivity, neuroimaging, magnetic resonance imaging, sleep

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# INTRODUCTION

Chronic sleep deprivation is a burgeoning public health concern, with as many as one-third of Americans showing signs of sleep deprivation—a number that is rising.<sup>1,2</sup> Chronic sleep deprivation and sleep restriction lead to significant neurological and psychiatric comorbidities that are known to be detrimental to cardiovascular health,<sup>3</sup> safety,<sup>4,5</sup> and guality of life.<sup>6,7</sup> Sleep deprivation has also been linked to declines in memory performance.<sup>8-12</sup> Although the relationship between nighttime sleep deprivation and daytime sleepiness is complex,<sup>13</sup> excessive daytime sleepiness increases risk of cognitive impairment and decline in elderly subjects at risk for dementia.<sup>14-17</sup> Additionally, young adults and cognitively normal elderly adults exhibit differential sensitivity to sleep deprivation. Younger adults show more cognitive impairment with sleep deprivation than do elderly adults,<sup>18</sup> although sleep deprivation in older adults also leads to poorer memory performance.<sup>19,20</sup> However, it remains unclear the specific effects of chronic sleepiness on the waking brain.

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Resting-state functional connectivity magnetic resonance imaging (fcMRI) identifies large-scale brain networks by identifying correlated intrinsic activity.<sup>21-23</sup> These networks overlap with known anatomical connections.<sup>24,25</sup> One of these networks, the default mode network (DMN), is strongly implicated in internal modes of cognition.<sup>26</sup> Although further work is necessary to separate the relative effects on episodic and working memory, the strength of correlated activity within the DMN appears closely tied to memory performance.<sup>27-29</sup> Decreased DMN connectivity is observed in amnestic mild cognitive impairment<sup>30,31</sup> and Alzheimer disease dementia.<sup>30,32</sup> Group-level fcMRI can be used to predict Alzheimer disease progression<sup>33</sup> and to differentiate subjects with mild cognitive impairment who are particularly likely to progress to dementia,<sup>34</sup> underscoring the potential clinical utility of DMN fcMRI.

DMN connectivity is significantly decreased in subjects who are deeply asleep<sup>35</sup> or lightly sedated,<sup>36,37</sup> as well as in subjects who are descending into sleep.<sup>38,39</sup> Additionally, sleep-deprived subjects also show significantly decreased DMN connectivity.<sup>40,41</sup> These results suggest that decreased DMN connectivity during the daytime may reflect a more "sleep-like" state in the brain. This may also indicate a neural mechanism by which disordered sleep can lead to decreased memory performance.

Building on the relationship between sleep deprivation and impaired memory and the rich literature linking decreased DMN fcMRI to mnemonic dysfunction, here we examine

Table	1-Demogra	phic	information
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	n = 8	<b>y</b> emales)	<b>Young</b> n = 27 (12 females)			
Dependent Measure	Mean	SD	Range	Mean	SD	Range
Age	73.2	5.7	66-87	22.6	4.4	18-29
CDR	0.0	0.0	0-0			
MMSE	29.0	0.9	27-30			
AMNART	122.8	7.5	90-131			
Years of Education	17.0	2.7	10-21	14.4	2.2	12-19
ESS	5.9	3.7	0-16	7.8	3.0	4-14
DMN Connectivity	0.55	0.22	0.08-1.01	0.70	0.29	0.07-1.13

Elderly and young subjects statistically differ for Epworth Sleepiness Scale (ESS) (P = 0.019) and default mode network (DMN) connectivity (P = 0.004). AMNART, American National Adult Reading Test; CDR, Clinical Dementia Rating Scale; MMSE, Mini-Mental State Examination; SD, standard deviation.

whether self-reported daytime somnolence affects DMN fcMRI. To address the effect of daytime somnolence (rather than acute sleep deprivation) on functional connectivity and memory, we focused on self-report of daytime somnolence using the Epworth Sleepiness Scale (ESS). We examined both young and cognitively normal older adults to determine if DMN fcMRI is differentially related to daytime sleepiness in these different age groups.

# METHODS

#### Participants

Eighty-five clinically normal elderly subjects (age 66-87 y) and 27 young adults (age 18-29 y) participated in the study (Table 1). All subjects were native English speakers and had normal or corrected-to-normal vision; had no history of sleep, psychiatric, or neurological disorders; and had no history of head trauma. Elderly inclusion criteria included Mini-Mental State Examination (MMSE) scores of  $\geq 27$ , a Clinical Dementia Rating of 0, and scores within one standard deviation of age-adjusted norms for Logical Memory IIa. Subjects with a confirmed diagnosis of a sleep disorder and subjects using continuous positive airway pressure were excluded. The elderly adults are a subset of the longitudinal Harvard Aging Brain study participants. Informed consent was obtained in accordance with the guidelines and procedures governed by the institutional review board of the Massachusetts General Hospital (Boston, MA).

#### **Neuropsychological Measures**

All subjects completed the ESS <sup>42</sup> within 50 days of the MRI. The ESS assesses the likelihood of dozing (rated from 0-3) in eight different scenarios. The ESS has been shown to remain largely stable over time across several populations.<sup>43,44</sup> However, subjects with obstructive sleep apnea who started CPAP treatment showed a marked decrease in ESS.<sup>43</sup> The ESS has been found to be internally consistent in elderly men<sup>44</sup> and elderly women.<sup>45</sup> Using a cutoff score of 10, the ESS is 93.5% sensitive and 100% specific for diagnosis of excessive daytime sleepiness.<sup>46</sup> Elderly participants also completed the

Digit Symbol Substitution Test, the Rey Auditory Verbal Learning Test, digits span backward, the Free and Cued Selective Reminding Test, the Trail Making Test parts A and B, and the Letter Number Sequencing Test.

## **MRI Data Acquisition and Processing**

Subjects underwent an MRI on a Siemens Trio Tim 3.0 Tesla scanner (Siemens Medical Systems, Erlangen, Germany) equipped with a 12-channel phased-array head coil. Head motion was restrained with extendable foam-padded clamps and a memory-foam head coil insert. Resting-state data were acquired in two separate, sequentially acquired scans using gradient-echo echo-planar imaging sensitive to blood oxygenation level-dependent contrast.<sup>47,48</sup> Subjects were instructed to keep their eyes open, lie still, and remain awake. A fixation cross was projected

onto a screen positioned at the head of the magnet bore and viewed with a mirror attached to the head coil. Forty-seven interleaved axial slices aligned parallel to the anterior-/posterior-commissure plane provided whole brain coverage with the following parameters: repetition time (TR) = 3,000 ms, echo time (TE) = 30 ms, flip angle =  $85^\circ$ , field-of-view (FOV) = 216  $\times$  216 mm, matrix = 72  $\times$  72, and 3  $\times$  3  $\times$  3 mm voxels. One hundred twenty-four volumes were acquired in each scan. T1-weighted structural images were acquired with a multiecho magnetization-prepared rapid gradient echo (MEMP-RAGE) sagittal-oriented sequence<sup>49</sup> with the following parameters: TR = 2,200 ms; inversion time (TI) = 1100 ms; TE = 1.54 ms, 3.36 ms, 5.18 ms, and 7ms; flip angle = 7°; FOV = 230  $\times$ 230 mm; matrix size =  $192 \times 192$ ; NEX = 1; and  $1.2 \times 1.2 \times$ 1.2 mm voxels. A root-mean-square image was produced from all four echoes and was used in the structural analyses.

# **Structural Preprocessing**

MEMP-RAGE data were processed with SPM8 (http:// www.fil.ion.ucl.ac.uk/spm/; version r4290) using the following supervised voxel-based morphometry (VBM) protocol: (1) T1-weighted images were manually translated and/or rotated to match the rotation and origin of the Montreal Neurological Institute (MNI) Template; (2) the translated/rotated T1-weighted images were segmented using the "New Segment" tool to produce rigidly aligned gray matter and white matter segments; (3) the rigidly aligned segments were normalized using a fast diffeomorphic image registration algorithm (DARTEL),<sup>50</sup> which included estimating the flow fields, warping the images to MNI space, and modulating the images; and (5) then the images were smoothed with a 6-mm full width at half maximum (FWHM) gaussian kernel.

#### **Structural Analysis**

To examine the effect of sleepiness on brain structure, we conducted a series of VBM analyses: (1) whole-brain regressions using the VBM-derived amounts of gray matter as the dependent variables, (2) small-volume correction in the ventromedial prefrontal cortex (vmPFC), and (3) small-volume correction in the DMN regions of interest (ROIs). These analyses were conducted using multiple regression models in SPM8 where the volume for each subject was entered as the dependent variable, with ESS as the independent variable, while controlling for age, sex, and total gray matter. Because age contributes significantly to changes in morphometry, young and elderly subjects were analyzed in separate models. Second, previous work has shown a specific effect of ESS on structure in the vmPFC using small-volume correction.<sup>51</sup> To assess this in our data, we performed a small-volume correction using 10-mm spheres centered on MNI coordinates [-12 26 -27] and [12 18 -23] as the small volume. Small-volume correction reduces the number of comparisons performed by performing an analysis on a restricted volume, thereby lowering the criterion for significance. Third, we performed a small-volume correction using our DMN ROIs as the small volume. The whole-brain and small-volume correction significance testing were corrected for multiple comparisons using false discovery rate correction using q < 0.05.<sup>52</sup>

Finally, we used the amount of gray matter within the functional connectivity ROIs as a covariate in our main analyses. This covariate was calculated by extracting the relative amount of gray matter in each ROI for each subject. These values were averaged to create an overall metric of ROI gray matter volume.

#### fcMRI Preprocessing

Resting-state functional data were preprocessed using SPM8 and MATLAB (v7.11; MathWorks, Natick, MA). The first four volumes of each run were discarded to allow for T1-equilibration effects. Each run was slice-time corrected, realigned to the first volume of the run with INRIAlign (http://www-sop.inria.fr/epidaure/software/INRIAlign/)53,54 using a rigid-body rotation, normalized to the MNI echoplanar imaging template, and smoothed with a 6-mm FWHM gaussian kernel. After preprocessing, a series of regressors from the resting-state data were entered into a multiple regression analysis. These were: (1) motion parameters as estimated by the six realignment parameters, (2) average signal from a deep white matter mask, (3) average signal from a ventricle mask, (4) average signal from the whole brain mask, and (5) the first derivative of each of these nuisance regressors. The residuals from this model were then linearly detrended and low-pass filtered with a second-order Butterworth filter with a frequency cutoff of 0.08 Hz.22,55 These runs were then concatenated for all analyses.

#### fcMRI First-level Analysis

Three *a priori* ROIs representing major nodal regions within the DMN were chosen for examination using a method described previously.<sup>56</sup> Each ROI represents an 8-mm sphere centered on a peak voxel in an established node of the default-mode network: the posterior cingulate cortex (PCC) MNI [0, -53, 26], medial prefrontal cortex (mPFC) MNI [0, 52, -6], and inferior parietal lobule (IPL) MNI [-48, -62, 36; 46, -62, 32]. The IPL spheres were combined into a single ROI. Time series data were extracted from every voxel within each ROI, and an arithmetic mean across time was calculated. Pairwise correlations between individual nodes of the DMN were calculated. Next, these pairwise nodal functional connectivity values were normalized using Fisher *r*-to-*z* transformation.<sup>57</sup>

We also computed a summary measure of DMN connectivity by averaging the z-values. Identical methods were used to determine the network health for five other prominent brain networks using previously published spherical ROIs: the dorsal attention, ventral attention, frontal-parietal control, visual, and motor networks<sup>58</sup> (see Table S1 for ROI locations). All connectivity data were analyzed using R (version 2.15.0, http://www.cran.r-project.org).

#### fcMRI Second-level Analysis: Main Model

Our main model analyzes overall DMN connectivity as the dependent variable. The amount of gray matter within the ROIs is entered as a covariate to control for the potentially confounding effects of age and cortical atrophy on connectivity. Because we include young and elderly subjects in the same model, age group is entered as a covariate. Age and the variable of interest, ESS, are included as parametric covariates, and allowed to interact with age group to control for the potential differing relationships between age and ESS on connectivity within young and elderly subjects.

#### fcMRI Second-Level Analysis: Selection of Covariates

First, we confirmed the normality of the ESS scores using the Shapiro-Wilk test (W = 0.984, P = 0.215). Next, we examined ESS scores and functional network connectivity for sex effects. None were found, so sex was not included as a covariate in any subsequent models. We then examined the data for any relationship with body mass index (BMI) to assess the potential contribution of undiagnosed sleep apnea. BMI was not significantly correlated with ESS or DMN connectivity. Because BMI was unrelated to ESS, we excluded it from the model. We investigated the effects of lag time between ESS and MRI acquisition because subjects did not have their MRI and ESS data acquisitions on the same day. Lag was not significantly correlated with ESS or DMN connectivity, nor did it significantly alter our subsequent analyses. Thus, we excluded it from the model. Because ESS scores have been shown to be stable over a period of 5 mo, this result was not surprising.<sup>43</sup> Next, we examined our DMN connectivity and sleepiness data for age group effects. Both of these models allowed age to interact with age group to control for any within-group effects of age. The DMN connectivity model also controlled for gray matter volume to eliminate the possibility of morphometry significantly contributing to the results. Age group was the only significant predictor in both models. Although both DMN connectivity and sleepiness were significantly different between young and elderly subjects (Table 1), neither the (age group)\*age nor the (age group)\*ESS interactions were significant in our main model, indicating a similar relationship between ESS and DMN connectivity in both young and elderly. However, we include these variables in our model because they do not significantly alter the relationship between ESS and DMN connectivity.

#### **Neuropsychological Models**

Finally, to examine the effects of daytime somnolence and DMN connectivity on cognitive function in our elderly sample, we examined the relationship between these measures and neuropsychological measures of cognitive performance. These



Figure 1—Residualized default mode network connectivity plotted against residualized Epworth Sleepiness Scale score (P = 0.003, partial r = -0.29).

 Table 2—Results of full analysis of covariance model with default mode

 network connectivity as dependent, and Epworth Sleepiness Scale as

 variable of interest

Predictor	F(1,105)	Р		
ESS	8.983	0.003		
Age Group	8.263	0.005		
Age	0.844	NS		
Age Group*ESS	1.211	NS		
Age Group*Age	0.129	NS		
Gray Matter	0.462	NS		
ESS, Epworth Sleepiness Scale.				

analyses were conducted using a standard general linear model controlling for age.

#### RESULTS

### Default-Mode Network Connectivity Is Different between Young and Elderly Subjects

As expected, and consistent with previous work,<sup>29,59-61</sup> the young group had significantly greater mean DMN connectivity than the elderly group while controlling for age and gray matter volume (P = 0.004; Table 1).

# Epworth Sleepiness Scale Scores Are Different between Young and Elderly Subjects

Our young subject group had significantly higher ESS scores than our elderly group while controlling for age (P = 0.019; Table 1). This finding is consistent with previous work that indicates that elderly adults have a reduced propensity for daytime sleep.<sup>62-64</sup>

# Increased ESS Scores Are Associated with Decreased DMN Connectivity

Grouping together older and younger subjects, but including age group as a factor, we observed that increasing ESS was significantly related to decreasing DMN functional connectivity (F(1,105) = 8.983, P = 0.003 partial r of ESS = -0.29; Figure 1, Table 2). Only ESS and age group were significantly related to DMN connectivity. Importantly, the age group by ESS interaction was not significant, indicating a similar relationship between ESS and DMN connectivity in both young and elderly subjects. These relationships were preserved when examining the pairwise ROI correlations individually (Table 3) as well as in a multivariate analysis of variance using all pairwise ROI correlations as dependent variables.

To determine whether decreased fcMRI is specific to the DMN or representative of widespread changes in functional connectivity in subjects with high ESS scores, we performed functional connectivity analyses in five other well-established brain networks: the dorsal attention, ventral attention, frontal-parietal control, visual, and motor networks.<sup>58</sup> ESS scores were not significantly correlated with functional connectivity in any of these other networks (Table 4), suggesting that daytime somnolence-related decreases in network connectivity are specific to the DMN. Additionally, the lack of association between daytime somnolence and functional connectivity in the primary sensory networks suggests that the changes in connectivity within the DMN are not attributable to differences in the global signal properties of the brain (i.e., does not represent a systematic alteration in measurement bias), but instead reflect specific changes within the DMN.

# Neither ESS Scores nor DMN Connectivity Are Associated with Differences in Brain Structure

Previous work has indicated that increasing daytime somnolence may have an effect on brain structure in young subjects.<sup>51</sup> To test this possibility in our sample, we analyzed the relationship between ESS scores and VBM-derived gray matter at the whole-brain level. This model assessed every voxel in the brain as a dependent variable, covarying for age and ESS score. Because age contributes significantly to changes in morphometry, young and elderly subjects were analyzed in separate models. However, no voxels survived false discovery rate correction (q < 0.05) at the whole-brain level for either positive or negative correlations with ESS in either group. We used smallvolume correction to perform a directed volumetric analysis of the ventromedial prefrontal cortex (which had previously been noted to covary with ESS)<sup>51</sup> but we found no significant relationships in this region. Finally, because our functional connectivity analysis focuses on DMN regions, we also performed a small-volume correction focusing on these regions. Again, no voxels survived false discovery rate correction.

To determine if DMN connectivity has an independent relationship from ESS on brain structure, we repeated the aforementioned structural analysis, substituting our DMN connectivity metric for the ESS measure. Once again, no voxels survived false discovery rate correction, indicating no relationship between network connectivity and brain structure in our sample. These results combined suggest that changes in daytime somnolence and functional connectivity are not linked to alterations in brain structure.

## Increased ESS Scores Are Not Associated with Cognitive Deficits

Although the neuropsychological testing within the elderly cohort spanned several cognitive domains, we found no relationship between any of the cognitive tests (Digit Symbol Substitution, Rey Auditory Verbal Learning Test, digits span backwards, Free and Cued Selective Reminding, Trail Making Part B minus Part A, and letter number span) and ESS. Additionally, within this sample, there was no relationship between the DMN connectivity metric and any of the neuropsychological test scores. None of the pairwise ROI measures were related to the neuropsychological test scores.

#### DISCUSSION

Daytime somnolence, as measured by the ESS, is associated with a reduction in DMN functional connectivity. This effect is found in both young and elderly subjects and the slope of the relationship is the same between these age groups. The relationship is not accounted for by changes in brain structure (as measured by VBM) and is specific to the DMN. An association between somnolence and connectivity is not seen in five other well-established functional networks.

Previous work has indicated reduced DMN connectivity in subjects who are descending into sleep,<sup>38</sup> are deeply asleep,<sup>35</sup> are lightly sedated,<sup>36,37</sup> have acute sleep deprivation,<sup>40,41</sup> or who have slept poorly for a single night.<sup>65</sup> Our results extend these findings: chronic daytime somnolence is similarly associated with reduced DMN connectivity. These results suggest that sleepiness, or a sleep-like state, correlate with decreased DMN connectivity,

and that this disconnection occurs in both acute and chronic somnolence. This decrease in DMN connectivity may reflect a "local sleep" phenomenon whereby parts of the brain enter a sleep state during consciousness.<sup>66</sup>

Consistent with prior studies,<sup>29,59-</sup> <sup>61,67</sup> we found that older subjects have lower DMN connectivity than younger subjects, regardless of ESS score. This replicates the finding that some decreases in DMN connectivity are related to aging in the absence of pathological cognitive decline.<sup>60,68</sup> However, despite the fact that older individuals showed lower DMN fcMRI at baseline, the relationship between somnolence and DMN fcMRI was similar in both young and elderly cohorts. Thus, it is likely that the relationship between ESS and DMN fcMRI is distinct from the effect of normal aging. The observation that increasing ESS scores correlate with decreasing DMN fcMRI in young subjects suggests that this mechanism is unlikely to be neurodegenerative, a conclusion bolstered by the lack of a relationship between ESS and brain structure in older individuals. Additionally, we found that our elderly sample reported less daytime somnolence than our young sample, consistent with previous work,<sup>62-64</sup> again suggesting that the relationship between somnolence and DMN connectivity. However, data relating somnolence to DMN connectivity in nonselected aged populations are needed to confirm this hypothesis.

Sleep loss and fragmented sleep lead to decreases in many aspects of neurocognitive performance,<sup>8,11,20,69,70</sup> and chronic mild sleep deprivation is associated with adverse effects on reaction times, memory, cognition, and general health.<sup>8,10,11,71-73</sup> However, our elderly sample was selected on the basis of their intact cognitive test scores. This truncated the range on the cognitive measures, thereby decreasing the likelihood of significant cross-sectional associations with sleepiness. Furthermore, the ESS is a short self-reported questionnaire, and may therefore be relatively insensitive to incremental differences between subjects with similar levels of sleepiness. Finally, recent work indicates that daytime sleepiness is related to longitudinal change in neuropsychological scores as opposed to being directly related to baseline measures.<sup>14-17</sup>

 Table 3—Relationship between default-mode network pairwise correlations as dependent and Epworth

 Sleepiness Scale as variable of interest

	PCC - I	mPFC	PCC ·	IPL	mPFC	- IPL
Predictor	F(1,105)	Р	F(1,105)	Р	F(1,105)	Р
ESS	8.633	0.004	8.312	0.004	10.223	0.002
Age Group	16.288	0.0001	8.269	0.005	6.333	0.013
Age	1.737	NS	0.844	NS	1.401	NS
Age Group*ESS	1.591	NS	1.211	NS	0.241	NS
Age Group*Age	2.181	NS	0.129	NS	0.019	NS
Gray Matter	1.704	NS	0.932	NS	0.198	NS

ESS, Epworth Sleepiness Scale; IPL, inferior parietal lobule; mPFC, medial prefrontal cortex; PCC, posterior cingulate cortex.

Table 4—Relationship between Epworth Sleepiness Scale and network connectivity for six major cortical networks.

	Default	Mode	Dorsal A	ttention	Ven Atter	tral ntion	Con	trol	Vis	ual	Mot	or
Predictor	F(1,105)	Р	F(1,105)	Р	F(1,105)	Р	F(1,105)	Р	F(1,105)	Р	F(1,105)	Р
ESS	8.983	0.003	0.812	NS	0.362	NS	0.568	NS	0.182	NS	0.151	NS
Age Group	8.263	0.005	7.384	0.008	14.882	0.0002	13.966	0.0003	24.026	> 0.0001	4.149	0.04
Age	0.844	NS	2.132	NS	0.284	NS	0.088	NS	0.932	NS	0.796	NS
Age Group*ESS	1.211	NS	0.907	NS	1.196	NS	0.612	NS	1.696	NS	0.164	NS
Age Group*Age	0.129	NS	0.501	NS	1.748	NS	1.579	NS	0.472	NS	0.038	NS
Gray Matter	0.462	NS	0.699	NS	1.005	NS	1.226	NS	0.028	NS	0.601	NS

ESS, Epworth Sleepiness Scale.

Coupled with literature tying DMN fcMRI with mnemonic function,<sup>74-76</sup> the current results raise the intriguing possibility that changes in DMN connectivity attributable to somnolence may be a mechanism by which excessive daytime somnolence (whether acute or chronic) leads to declines in memory function. Future studies aimed at assessing the relationship of nighttime sleep quality (as measured by actigraphy or polysomnography) to daytime sleep and DMN fcMRI will help to clarify the interdependent relationship between sleep structure and quality, propensity for daytime sleep, and DMN connectivity.

Additionally, this study was conducted without the benefit of simultaneous electroencephalographic recording. Consequently, we cannot guarantee that our subjects did fall asleep during the resting state scans. However, it is unlikely that this potential confound is present in our paradigm because (1) the ESS is not correlated with sleep latency in an elderly population,<sup>13</sup> (2) our fMRI scanning is performed during the mornings, early in the MRI session, and with eyes open, and (3) is divided into two shorter-duration (6-12 min) scans with interruptions that require subject response between scans. Finally, we performed detailed analyses of head movement to determine if subjects with high sleepiness scores moved more during the scans (suggesting hypnic myoclonia) or moved less (suggesting sleep atonia) but found no association with ESS scores (see supplemental materials for details). It is important to note that this confound potentially affects any study examining resting-state connectivity.

Finally, given the development of DMN fcMRI as a noninvasive biomarker in mild cognitive impairment and Alzheimer disease,<sup>77,78</sup> the current results suggest that ESS or other measures of somnolence or sleep quality may be useful additions to functional connectivity imaging studies in neurodegenerative disease. First, it appears that the effects of daytime sleepiness on DMN connectivity are dissociable from the effects of aging on DMN connectivity. Second, recent reports suggest that disruptions of sleep throughout the life span correlate with poorer cognition later in life,79 excessive daytime sleepiness increases an elderly individual's risk of cognitive decline,14-17 and sleep quality may be associated with beta-amyloid accumulation.<sup>80</sup> Further, it will be important to assess the possibility that sleepiness may mediate the changes in DMN connectivity that are observable during the conversion from cognitive normality to mild cognitive impairment and Alzheimer disease. Finally, consideration of the effects of excessive daytime somnolence on DMN fcMRI may help to explain the variability seen in neurodegenerative studies of DMN fcMRI, and to potentially identify subjects at risk for cognitive decline.

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#### DISCLOSURE STATEMENT

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## SUPPLEMENTAL METHODS

Although simultaneous electroencephalographic data were not available on individual subjects, we conducted an analysis on movement during our resting state acquisition to assess the relative likelihood that the patients with excessive daytime sleepiness (Epworth Sleepiness Scale  $\geq 10$ ) were sleeping, as opposed to sleepy, in the scanner.

To investigate decreased muscle tone due to stage 1 nonrapid eye movement sleep (NREM), we calculated the euclidian distance that the subject moved between each frame. Importantly, these distances are calculated frame-to-frame (i.e., euclidian distance from the frame before) as opposed to average deviation from the mean image. This allows us to avoid overemphasizing the effects of drift, or of a single large movement.

To investigate hypnic myoclonia due to subjects entering and exiting stage 1 NREM sleep, we calculated the number of frames where movement from the frame before exceeded 0.75 mm or 1.5 degrees, or both.<sup>1</sup>

Because the relationship between movement and sleepiness was unlikely to be linear, we divided our subjects into three groups: not sleepy (ESS  $\leq$  3, n = 23), middle (4  $\leq$  ESS  $\geq$  9, n = 68), and excessive daytime sleepiness (ESS  $\geq$  10, n = 21). This design allows us to focus on mean differences, which allows us to examine differences without presupposing the relationships between these means. However, we also examined linear models of both mean movement and count of largeamplitude movements, as well as a linear model containing both measures of movement and their continuous interaction. We conducted models controlling for age because elderly subjects have been shown to move more than younger subjects,<sup>1</sup> but this predictor was not significant in our group. We also conducted the analyses without age in the model to prevent the possible age/movement collinearity from suppressing any sleep/movement relationships. These models were nearly identical to models including age.

#### SUPPLEMENTAL RESULTS

We present a series of analyses that indicate on the group level that we are recording sleepiness as opposed to sleep.

First, the resting-state data were collected using an eyes-open paradigm. Eyes-open resting state exhibits stronger correlations within the default mode network (DMN) than does eyes-closed resting state,<sup>1</sup> possibly due to fewer lapses into stage 1 NREM sleep or due to a heightened state of vigilance. Additionally, the resting-state data were acquired in two sequential runs. Instructions were given before each run, and each required a response with a button press before each run was initiated. This, too, limits the opportunity for sleep.

Second, previous work has indicated that ESS ratings are not related to quantification of sleep latency in a population of elderly community-dwelling adults.<sup>2</sup> That is, ESS scores are not related to how quickly elderly subjects actually fall asleep. Thus, patients with higher ESS scores may not necessarily be biased to fall asleep in the scanner more quickly.

Third, we analyzed subject movement during our restingstate scans. We hypothesize that subjects who may have fallen



Figure S1—Movement by sleepiness group. (A) Mean movement as euclidian distance moved from one repetition time (TR) to the next plotted by sleepiness group. None of the differences between group means are significant. (B) Number of volumes where TR-to-TR movement exceeded 0.75 mm or rotation exceeded 1.5 degrees. Again, none of the differences between group means are significant.

Table S1—Other	network seed locations	
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Network		Seeds	
Dorsal attention	[-22 -8 54]	[-34 -38 44]	[-51 -64 -2]
Ventral attention	[-54 -36 27]	[-5 15 32]	[-31 -24 39]
Control	[-40 50 7]	[-43 -50 46]	[-5 22 47]
Visual	[-13 -100 -8]	[-32 -89 -1]	[-23 -91 -15]
Motor	[-41 -20 62]	[-6 -26 76]	[-55 -4 26]

These seeds were isolated in Yeo et al. 2011.<sup>4</sup> In order to keep the comparison between DMN and these other networks comparable in terms of number of seeds, we selected only the top three seeds for each network as measured by their confidence ratings from a confirmation data set. Each seed was reflected across the hemispheric boundary by multiplying the x-coordinate by -1.<sup>5</sup> Each seed was averaged across hemispheres (similar to the inferior parietal lobule in the DMN), and the Fisher-Z transformed correlations between each seed were averaged to create a network-level metric.

asleep during the scan will fit into one of the following groups: (1) lower average movement due to decreased muscle tone, or (2) above-average large amplitude sharp movements due to hypnic myoclonia.<sup>3</sup>

None of the groups significantly differ for mean movement (Figure S1). The mean movement for the high ESS group is arithmetically, but not statistically, greater than the low group, indicating that it is unlikely that subjects in the high group have sleep-related muscle atonia in comparison with the low group. There is also no linear effect of ESS on mean movement (r = -0.064, P = 0.854). However, it is possible that mean

movement may be contaminated by hypnic jerks. Therefore, we repeated the aforementioned analyses using a count of repetition times exceeding threshold. Again, we see no significant differences (Figure S1B). Again, running counter to the hypotheses of high ESS subjects falling asleep in the scanner, the low sleepiness group contains the highest absolute values of large movements, as well as an arithmetically higher mean. There is also no linear relationship (r = 0.071, P = 0.696). Finally, no predictors were significant in a model including cutoff volumes, mean movement, and the continuous interaction of these two predictors, controlling for age (model  $r^2 = 0.008$ , P = 0.586). Combined, these results suggest that sleepier subjects are not exhibiting movement tendencies of subjects who are falling asleep. Although these data alone are insufficient to absolutely claim that the subjects are awake, they strongly implicate wakefulness during the scanning session.

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