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Visualizing cancer and immune cell function with metabolic positron emission tomography

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Abstract

Cancer cells and immune cells modulate their metabolism according to specific needs during cancer progression and immune responses. The ability to measure cellular metabolic function in vivo would enable the evaluation of tumors and their response to therapy and also the effectiveness of cellular immune responses to cancer. Positron emission tomography (PET) is a highly sensitive clinical imaging modality that enables whole-body, quantitative measurements of tissue biochemical function. Here, we review work using PET probes for specific metabolic pathways to measure cell function in cancer and immunity. We focus on the use of probes for glycolysis and nucleoside salvage and then discuss the development of new metabolic probes that visualize distinct parameters of cell function during disease.

Cancer and the immune system: the need for functional imaging tools

Cancer results from aberrant cellular genetic activity that occurs in specific tissue microenvironments. Interactions between transformed cells and innate and adaptive immune cells play a critical role in determining tumor progression. Malignant transformation can trigger cellular immune responses that are capable of killing cancer cells early, before the emergence of detectable lesions [1']. Cancer, as it appears clinically however, occurs in a state of immune dysfunction. Helper T cells (CD4⁺), cytotoxic T cells (CD8⁺), macrophages, and natural killer cells (NK cells) are often found in tumors [1•]. While the presence of cytotoxic T cells or NK cell infiltrates often indicates a good prognosis [2], tumors can grow in the presence of immune cells. It is now known that tumors deploy an arsenal of weapons against immune cells to suppress their function and evade killing [3,4]. Moreover, specific types of immune activity, particularly chronic inflammation arising from innate immune cell infiltration, aid tumor growth and invasion [5].

Identification of key mechanisms underlying immune dysfunction in cancer has led to several therapeutic strategies that arm the immune system against tumor-induced immunosuppression. Vaccination with dendritic cells pulsed with proteins from a patient's

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tumor can mobilize endogenous T cells to attack that tumor [6]. Vaccination approaches have been coupled with the blockade of T cell inhibitory signals (e.g. by treating with monoclonal antibodies against CTLA-4) in order to augment T cell number and function in tumors [7]. Another promising immune modulatory strategy is adoptive cell transfer (ACT) therapy using tumor-reactive T cells primed *in vitro* to kill tumor cells [8,9]. Combining ACT therapy with dendritic cell vaccination and blockade of T cell inhibitory signals offers the potential for treating a variety of cancers that are typically difficult to manage with conventional therapies.

The central role of the immune system in cancer progression and anticancer therapies encourages the development of technologies that can measure parameters pertaining to both tumor cells and immune cells for diagnosing disease and monitoring treatment. Whole-body imaging modalities such as magnetic resonance imaging (MRI), computerized tomography (CT), single photon emission computerized tomography (SPECT), and positron emission tomography (PET) can detect pathological lesions throughout the body [10]. PET is particularly applicable to the task of measuring cell function because it provides clinically relevant measurements of tissue biochemistry [11]. This brief review will highlight the work that has led to the development of PET into a technology to measure distinct functional parameters of cancer and immune cells in vivo and evaluate the efficacy of cancer immunotherapy.

PET imaging of cell function

PET is a noninvasive imaging modality used in preclinical and clinical settings to measure site-specific accumulation of probes labeled with positron emitting radioisotopes at subnanomolar concentrations in the body. The biodistribution of a particular probe is a function of unique biochemical interactions between the probe and tissues. Numerous PET probes have been developed that measure reporter gene activity, cell surface receptor expression, and metabolism (reviewed in [12,13]). The following sections will focus on PET probes that measure the activity of metabolic pathways that are critical to cancer and immune cell function (Figure 1).

[¹⁸F]FDG-PET in cancer imaging

In the 1930s, the German biochemist Otto Warburg first observed that cancer cells metabolize glucose nonoxidatively through glycolysis, even in the presence of oxygen [14]. Over 70 years after its discovery, the significance of the Warburg effect for cancer development and progression is still under intense investigation. Since the ATP yield of glycolysis is many folds lower than that of oxidative phosphorylation, tumor cells take up massive amounts of glucose to generate the same amount of energy that normal tissues can produce by oxidative phosphorylation of far fewer glucose molecules [15]. High intracellular concentrations of metabolic byproducts of glucose breakdown provide the building blocks for biosynthetic pathways necessary for cell growth and proliferation [16,17]. Also, upregulation of glycolysis may enable cancer cells to survive hypoxic tumor environments while their metabolic byproducts such as lactate and protons are thought to inhibit the growth of normal cells and the function of immune cells (reviewed in [15,18]).

Gain of function of oncogenes and/or loss of function of tumor suppressor genes play key roles in regulating the cellular biochemical machinery required to sustain high rates of glycolysis [19,20••]. Elevated glycolysis in cancer cells, relative to neighboring normal tissues, provides the rationale for metabolic PET imaging using [18F]-2-fluorodeoxyglucose $([18F]FDG)$. $[18F]FDG$ is a radiolabeled glucose analog that is taken into cells through glucose transporters (GLUTs) and phosphorylated by hexokinase (HK), thus trapping it within the cell [21]. GLUTs and HK are downstream targets of several transcriptional

pathways activated during cellular transformation. As a result, $[18F]FDG$ accumulates at high levels in greater than 90% of tumors. [¹⁸F]FDG accumulation in cancer cells provides a quantitative, visual readout of oncogenic activity on a whole-body level.

 $[{}^{18}F]FDG-PET$ has been used for the last three decades to diagnose and stage an array of cancers, including gastrointestinal stromal tumors (GIST), lymphoma, melanoma, sarcoma, lung, and breast cancer [22–32]. Some tumor types, such as prostate carcinoma, are often indolent with low levels of glycolytic activity, making them difficult to detect with [¹⁸F]FDG-PET. Alternative probes for the detection of prostate cancer are needed.

Recently $[18F]FDG-PET$ has become a powerful technique to monitor the efficacy of anticancer therapies. One of the most notable examples of this application is visualizing the effect of targeted small molecule therapy on GIST. Imatinib inhibits c-kit, a receptor tyrosine kinase that contains activating mutations in more than 85% of cases of GIST [22]. GISTs are typically highly glycolytic tumors, and treatment with Imatinib leads to a dramatic reduction in tumor $[18F]FDG$ accumulation in responding patients. It is important to note that the functional perturbation determined by diminished $[{}^{18}F]FDG$ accumulation often occurs before tumor shrinkage is observed with anatomical imaging modalities such as CT and MRI [22]. In nonresponding patients (e.g. individuals harboring Imatinib resistance mutations), $[18F]FDG$ accumulation in the tumor does not diminish with drug treatment. [¹⁸F]FDG has been used to monitor and predict the effects of several other anticancer therapies, providing early readouts of treatment efficacy and helping guide decisions that eliminate unnecessary or ineffective treatment [33].

[¹⁸F]FDG-PET to visualize immune function

Phenotypically diverse cell types of the innate and adaptive immune systems rely heavily on glycolytic metabolism. Innate immune cells such as macrophages and granulocytes are critically dependent on HIF-1 -mediated induction of glycolytic genes to infiltrate inflamed tissue [34]. Adaptive immune cells upregulate the expression of GLUTs and HK in response to mitogenic signals [35]. This has enabled the use of $[{}^{18}F]FDG-PET$ in several immunemediated disorders. In preclinical settings, [18F]FDG-PET was shown to detect specific sites of immune activity in animal models of rheumatoid arthritis [36], experimental autoimmune encephalitis [37], colitis [38], and graft-versus-host disease [39[°]]. PET imaging in these instances can also measure the effects of systemic immunosuppressive therapy. In the clinic, [¹⁸F]FDG-PET has been used to evaluate inflammation in rheumatoid arthritis [40], GHVD [39^{*}], atherosclerosis [41], and infectious diseases [42].

The central role of glycolysis in cancer and immune cell function can lead to false positives when using $[18F]FDG-PET$ for cancer diagnostics [43,44]. Two areas that are particularly problematic are firstly, differentiating viable tumor cells from colocalized immune cells and secondly, distinguishing lymph node metastasis from immune activation in reactive lymph nodes [45]. These limitations have led to the design of metabolic PET probes that provide readouts of cellular metabolic function distinct from glycolysis, to potentially allow discrimination of tumor from immune activity.

Imaging cell proliferation with [¹⁸F]FLT

Fluorothymidine (FLT) is an analog of thymidine that accumulates in cells via the thymidine salvage pathway. Similar to endogenous thymidine, FLT is taken up by nucleoside transporters expressed on the cell surface and is phosphorylated by the S-phase specific enzyme thymidine kinase 1 (TK1), trapping the probe within the cell [46,47]. $[18F]FLT$ accumulates in highly proliferative tissues and largely correlates with positive staining for the proliferation antigen Ki67 [48]. $[$ ¹⁸F]FLT-PET has been evaluated as a probe for cell

proliferation in diagnostic studies of several types of cancer and compared with $\lceil {^{18}\text{F}|\text{F} \text{D} \text{G}}\rceil$ for the ability to specifically label tumors [49,50]. In some preclinical studies, measuring cell proliferation with [18F]FLT offers better tumor-specificity than measuring glycolytic activity with $[18F]FDG$. This is believed to be due to lower accumulation of FLT compared to FDG in tumor-infiltrating immune cells [51]. Nonetheless, $[{}^{18}$ F|FLT has limitations in cancer imaging. High levels of probe accumulation in actively proliferating marrow cavities limit the detection of lesions to areas away from central skeletal structures. Given the importance of thymidine and bromodeoxyuridine (BrDU) incorporation techniques in basic immunological studies, and the accumulation of $[18F]FLT$ in bone marrow, it is surprising that $[18F]FLT-PET$ has not been used more extensively to visualize immune responses in *vivo.* $[{}^{18}$ F]FLT-PET has shown promise in diagnosing extramedullary sites of leukemia, especially in areas such as the brain that have high levels of physiologic FDG accumulation [52]. $[18F]ELT-PET$ may allow the detection of therapies designed to enhance immune cell proliferation during cancer immunotherapy.

Design of new metabolic PET probes to visualize the immune system

To further metabolic PET imaging technology, we have designed probes for metabolic pathways distinct from glycolysis and thymidine salvage. We focused on metabolic pathways that could enable the distinction of the immune cells from tumors. Previous studies have shown that hematolymphoid tissues are particularly enriched for deoxycytidine salvage and that the activation of the immune system augments the activity of this pathway [53,54]. Analogous to thymidine salvage, deoxycytidine salvage mediates the uptake of deoxycytidine, and related nucleosides, through specific transporters expressed on the cell surface. Intracellularly, deoxycytidine is phosphorylated and trapped by deoxycytidine kinase (DCK), a rate-limiting enzyme in deoxycytidine salvage [55].

Using a differential screening assay, we identified 1-(2-deoxy-2-fluoro-arabinofuranosyl) cytosine (FAC), a deoxycytidine analog that accumulates in cells based on DCK activity [56 $^{\bullet}$]. ¹⁸F-labeled FAC can be used as a PET probe to visualize DCK activity *in vivo*. Preclinical imaging in mice showed that $[18F]FAC$ accumulates in primary and secondary lymphoid organs, including the thymus, bone marrow, spleen, and lymph nodes as well as in the gastrointestinal tract. $[{}^{18}F]FAC-PET$ signal in peripheral lymph nodes and spleens of mice increased with immune activation due to viral infection and lymphoproliferative disorders. Importantly, in an antitumor immune response model, $[{}^{18}$ F]FAC showed intense signal in lymphoid organs but little accumulation in the tumor compared to $[{}^{18}F]FDG$ [56^{*}]. A comparison of FAC and FDG showed that these probes had different specificities for immune cell subtypes during an antitumor immune response. While deoxycytidine salvage was most prevalent in adaptive immune cells in active cell cycle, glycolysis was highest in innate immune cells (Nair-Gill et al., unpublished data). This finding demonstrates that imaging probes for distinct metabolic pathways can provide complementary functional information about the immune system *in vivo*, encouraging the use of multiple imaging probes in clinical situations to gather comprehensive information about immune function.

 $[$ ¹⁸F]FAC also has a potential role in stratifying tumors based on the expression of DCK. Nucleoside analog prodrugs such as gemcitabine, cytosine arabinoside (cytarabine), and 5 aza-2 -deoxycytidine (decitabine) are DCK substrates and this enzyme is critically required for their activation [55,57]. Loss of DCK activity in tumor cells is a common cause of resistance to these prodrugs. Thus, a noninvasive imaging method to detect functional DCK in tumors could guide the treatment of patients with nucleoside analog therapy. We have demonstrated that $[18F]FAC$ preferentially accumulates in DCK-positive cells. Cells lacking DCK expression are unable to phosphorylate and trap $[18F]FAC$ and show no probe accumulation. Using a preclinical cancer treatment model, we found that [18F]FAC-PET

was able to predict responses to gemcitabine [58^{*}]. DCK-positive tumors accumulated [¹⁸F]FAC during a pretreatment scan and responded to gemcitabine treatment, while tumors that were deficient for DCK were not detected with [¹⁸F]FAC-PET and continued to grow despite gemcitabine treatment. Importantly, $[18F]FDG$ imaging could not distinguish the gemcitabine sensitive and resistant tumors, demonstrating that functional imaging of distinct metabolic pathways can predict the effect of specific anticancer therapies [58••].

Concluding remarks

Measuring cellular metabolism can provide insight into the function of cancer and the immune system during disease. Whole-body imaging with metabolic PET can isolate sites of disease and monitor how therapeutic intervention affects cell function. We have summarized work on the development and application of PET probes with defined specificities for different metabolic pathways. Further understanding of the biological role of these pathways during cancer progression and immune responses should guide the use of metabolic imaging for diagnostics and the evaluation of specific therapies. Identification and characterization of metabolic pathways other than glycolysis and nucleoside salvage will provide opportunities to design new PET imaging probes. The development of new PET probes is essential: the ability to make several distinct measurements in the same subject will further the understanding of cancer and immunity on a personalized basis.

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Figure 1.

(a) Schematic showing the metabolic pathways measured by FDG, FLT, and FAC. HK = hexokinase; TK1 = thymidine kinase-1; DCK = deoxycytidine kinase. **(b)** Preclinical FDG-PET scan of a mouse after injection with the MoMSV oncoretrovirus. At the period of peak immune response, high FDG uptake is seen in the tumor, lymph nodes, and spleen. Reproduced from Radu et al. [56••]. **(c)** FLT-PET scan of a LN229 xenograft implanted in a scid/ scid mouse. **(d)** Preclinical FAC-PET scan of a mouse after injection with the MoMSV oncoretrovirus. At day 15, the peak of the immune response, increased FAC uptake is seen in the lymph nodes (LN) and spleen (SP) compared to tumor (TU). Reproduced from Radu et al. [56••].