ORIGINAL ARTICLE

# Parameters influencing the outcome after total disc replacement at the lumbosacral junction. Part 2: distraction and posterior translation lead to clinical failure after a mean follow-up of 5 years

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#### Abstract

Purpose The aim of the second part of the study was to investigate the influence of parameters that lead to increased facet joint contact or capsule tensile forces (disc height, lordosis, and sagittal misalignment) on the clinical outcome after total disc replacement (TDR) at the lumbosacral junction.

Methods A total of 40 patients of a prospective cohort study who received TDR because of degenerative disc disease or osteochondrosis L5/S1 were invited to an additional follow-up for clinical (ODI and VAS for overall, back, and leg pain) and radiographic analysis (a change in disc height, lordosis, or sagittal vertebral misalignment compared with the preoperative state). Based on the final ODI, patients were retrospectively distributed into groups N (normal:  $\langle 25 \, \%\geq 25 \, \%$ ) for radiographic parameter comparison. A correlation analysis was performed between the clinical and radiological results.

Results A total of 34 patients were available at a mean follow-up of 59.5 months. Both groups ( $N = 24$ ;  $F = 10$ patients) presented a significant improvement in overall pain, back pain, and ODI over time. At the final follow-up, higher clinical scores correlated with a larger disc height, increased lordosis, and posterior translation of the superior

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vertebra, which was also reflected by significant differences in these parameters in the group comparison.

Conclusions Parameters associated with increased facet joint capsule tensile forces lead to an inferior clinical outcome at mid-term follow-up. When performing TDR, we therefore suggest avoiding iatrogenic posterior translation and overdistraction (and consecutive lordosis).

Keywords Total disc replacement · Lumbar spine · Facet joint degeneration · Clinical outcome · Misalignment - Degenerative disc disease

## Introduction

Motion-preserving technologies, such as lumbar total disc replacement (TDR), have been introduced as alternatives in the surgical treatment of low back pain resulting from degenerative disc disease (DDD) to avoid the negative side effects associated with vertebral fusion  $[1–10]$  $[1–10]$  $[1–10]$ . The clinical efficacy of TDR has been demonstrated in a variety of clinical class I and long-term studies [\[1](#page-7-0), [5,](#page-7-0) [8,](#page-7-0) [10–13](#page-8-0)]. Nevertheless, several factors that negatively affect the clinical outcome after TDR have recently been elucidated [\[14–17](#page-8-0)]. A preoperatively existent high-grade facet joint degeneration (FJD) can especially lead to inferior clinical results; therefore, FJD was suggested as a contraindication for this procedure  $[18]$  $[18]$ . However, facet joint forces may increase after TDR followed by a de novo development or the progression of preoperatively existing initial FJD in a relevant percentage of patients (20–36 %) with a resulting inferior clinical outcome [\[19–23](#page-8-0)]. In a prospective study, Siepe et al. [[23\]](#page-8-0) found that FJD appeared more frequently at the index level compared with the adjacent levels and significantly more frequently at the lumbosacral junction

compared with the levels above it. The latter may be caused by the unique facet joint configuration of L5/S1 or specific sagittal profile parameters [[24\]](#page-8-0) that theoretically result in higher facet joint shear stresses or contact forces [\[25](#page-8-0)]. Interestingly, patients with FJD progression after TDR present with inferior clinical results a few month postoperatively [\[23](#page-8-0)], which suggests that FJD itself may not be the only cause of pain or functional impairment. Several factors, such as malposition in the frontal plane, the grade of restoration of the disc height by segmental distraction, or the consecutive changes of the local sagittal curve with increased segmental lordosis, may affect facet joint forces after TDR [[20,](#page-8-0) [25,](#page-8-0) [26\]](#page-8-0). In our probabilistic finite element model (FEM) analysis [[27\]](#page-8-0), we demonstrated that a segmental misalignment in the sagittal plane after TDR with an anterior or posterior shift of the superior vertebra leads to a significant increase in facet joint contact or capsule tensile forces. Although alterations in facet joint kinematics appear to be the crucial factor for clinical success after TDR (especially at the lumbosacral junction), these parameters have not been clinically investigated for their contributions to persistent postoperative pain, the progression or development of FJD, or a resulting functional impairment.

Therefore, we retrospectively analyzed the data of our patients treated with TDR at L5/S1 to identify sagittal geometry parameters (especially FEM-identified sagittal misalignment) responsible for clinical failure after TDR. We hypothesized that in patients who undergo TDR at the lumbosacral junction, an inferior clinical outcome is associated with a sagittal misalignment and/or an alteration of the local segmental curve or geometry.

#### Patients and methods

The present study is a retrospective analysis of patients included in a 1-year follow-up prospective cohort study that investigated the clinical and radiological outcomes after lumbar total disc replacement between 08/2005 and 12/2010.

The inclusion criteria for the original study were painful (as proven by provocative discography) single-level DDD Pfirrmann and Resnick  $[28]$  $[28]$  grade  $>III^\circ$  and/or Modic  $[29]$  $[29]$ grade  $\leq$  II° of segments L5/S1 or L4/5 (as found on MRI) after an unsuccessful period of conservative treatment for at least 6 months.

Patients were excluded from the study if they had degeneration of adjacent segments, as verified by MRI. Additionally, patients with FJD Fujiwara et al.  $[30] \geq \text{III}^{\circ}$  $[30] \geq \text{III}^{\circ}$  $[30] \geq \text{III}^{\circ}$ at any segment of the lumbar spine were excluded. A Fujiwara grade of  $II^{\circ}$  led to diagnostic facet joint infiltration, and patients were excluded from the original study in the case of a positive infiltration test result. Further exclusion criteria included additional degenerative findings; spinal deformities, spondylolisthesis Meyerding  $[31] > I^{\circ}$  $[31] > I^{\circ}$ , or destructive processes; previous operations on the lumbar spine with the exception of sequestrectomy; patients on long-term medication with corticoids or non-steroidal antiinflammatory drugs (NSAIDs) or those with psychological distress syndrome or a somatization disorder of grade  $>$  II<sup> $\circ$ </sup> according to Gerbershagen et al. [\[32](#page-8-0)]; patients with osteoporosis, kidney or liver diseases, malignant tumors, or a BMI  $>30$  kg/m<sup>2</sup>; an age of  $>65$  years; pregnancy; or chronic nicotine, alcohol, or drug abuse.

The original clinical outcome parameters were assessed using a visual analog scale (VAS; performed preoperatively and at 1 week and 12 months postoperatively) for overall pain and back and leg pain. The Oswestry Disability Questionnaire Version 2 was used to assess function (ODI; performed preoperatively and 12 months postoperatively). Radiographs of the lumbar spine were acquired preoperatively and 1 week and 12 months postoperatively in the upright standing position to identify implant-associated failures. Major and minor complications were also recorded.

The study was approved by the local research ethics committee. Informed written consent was obtained from each patient.

All surgeries were conducted by the same senior surgeon (M.P.) and were performed via a pararectal retroperitoneal approach. Prior to implant placement, the intervertebral disc was resected, and the cartilaginous endplate was removed. The implant (Maverick<sup>TM</sup> A-MAV<sup>TM</sup>, Medtronic, Memphis, USA) dimensions, angulations, and height were defined by fitting a test specimen/template according to the individual size and angle of the intervertebral space. The implant was press-fit anchored after distraction and resection of the posterior longitudinal ligament as described in the manual of the implant. Each patient was mobilized without an orthosis and given physiotherapy from the first postoperative day onward.

All patients with a TDR at L5/S1 included in the original study were invited to an additional radiological (plain upright standing lateral radiograph of the lumbar spine) and clinical examination (VAS for overall, back, and leg pain; ODI) for this study. All radiographic measurements and calculations were performed digitally employing functional X-ray analysis (ACES GmbH, Esslingen, Germany) of radiographs (DICOM images) of the lumbar spine acquired in the lateral upright standing position preoperatively and at the final follow-up. This included digital sharpening, noise reduction, scaling, and correction of possible errors by segmental rotation and out of plane mismatch. Intraindividual comparisons of the parameters are based on a validated overlay correlation algorithm without the necessity of manual landmark placement or contour alignment, or other manual alignment between the images. The anterior–posterior translation (in millimeters) of the superior vertebra in relation to the arch of lordosis at the posterior wall of the inferior vertebra (APT; anterior, positive values; posterior, negative values; Fig. 1), the percentage of the vertebral translation in relation to the length of the inferior endplate (M) according to Meyerding [\[31](#page-8-0)], segmental lordosis (SL), and the anterior (aDH), middle (mDH), and posterior disc height (pDH) of the surgically treated segment were the parameters measured. The mean disc height (meanDH) was calculated using aDH, mDH, and pDH. The difference in the SL, aDH, mDH, pDH, meanDH, APT, and M parameters between the preoperative and final follow-up states was calculated and used for new parameters referred to as "delta."

Based on the ODI at the final follow-up, patients were retrospectively assigned to two groups (F—functionally impaired, ODI > 25 %; N—normal function ODI < 25 %). The cutoff of ODI 25 % was based on the mean function of the "normal" population (ODI 10  $\%$ ), the relevant clinical difference of ODI 15 %, and the acceptance of this cutoff between the patients with functional impairment and the "normal population"  $[33]$  $[33]$ . The radiological measurement parameters and clinical scores of the groups were compared, and a correlation analysis between the clinical scores and the radiologic measurement parameters was performed.

At the final follow-up, a facet infiltration test (5 ml at both sides; 0.5 % Carbostesin<sup>TM</sup>; AstraZeneca, Germany) was performed to identify the facet joints as main pain



Fig. 1 Schematic illustration of an anterior–posterior vertebral translation (APT) after TDR corrected by distraction and the arch of lordosis. (This figure is an idealized visualization of the measurement parameters and does not meet the accuracy or validity of the digital picture analysis algorithm or error correction routines). In both cases (upper and lower row), TDR resulted in distraction that was visible via the decrease in the flexion of the arch from the left to the right column. Both patients presented with a preoperative (pseudo) retrolisthesis because of a larger inferior endplate of L5 compared with the superior endplate of S1. The *blue dot* indicates the crossing of the radius between the center of lordosis and the posterior superior

edge of S1 and the arch of lordosis. The red dot (crossing of the arch of lordosis and the transposed radius from S1 to the inferior endplate line of L5) serves as a marker for the measurement of the APT (distance between the posterior inferior edge of the L5 (yellow dot) and the red dot). The upper row shows a patient with iatrogenic posterior translation (and increase of lordosis from  $11^{\circ}$  to  $14^{\circ}$ ) at the b postoperative compared to the a preoperative state. This is indicated by an increase in the distance between the yellow and red dot, whereas in the lower row, an anterior translation and a slight decrease of lordosis from  $12^{\circ}$  to  $11^{\circ}$  is the result of TDR (c preoperative, d postoperative)

generators. This test was performed for all patients in group F. In accordance with the literature [\[34](#page-8-0), [35](#page-8-0)], the infiltration test was judged to be positive in the case of a VAS drop of at least 50 % or  $>$ 3 cm 1 h after injection.

The data from this study were analyzed using the PASW 18.0 statistics software (SPSS Inc. Chicago, USA) and Prism 5.0 (GraphPad Software Inc., San Diego, USA). Inter-group comparisons of postoperative ODI and VAS were conducted with a two-sided two-way analysis of variance for repeated measures (RM-ANOVA), and an intra-group comparison was performed with a two-sided, one-way RM-ANOVA. Post hoc tests with Bonferroni's correction were performed for all ANOVAs. The normality of the distribution was checked using the D'Agostino and Pearson omnibus normality test prior to applying parametrical testing. The correlation analysis between the parameters was based on Pearson's correlation coefficient, and the difference in the radiologic parameters between the groups was determined using a two-sided  $t$  test. The significance level for all the statistical tests was set at  $p<0.05$ .

#### Results

Of the 40 patients included in the original study who were treated with a TDR at L5/S1, 34 (85 %) were available for the additional final evaluation at a mean of 59.5 (24–87) months after surgery. Four patients could not be contacted due to moving to an unknown address, and two patients were not willing to undergo a further clinical or radiological follow-up examination without specifying reasons. Of the 34 patients available for evaluation, 16 were female and 18 male. The mean age at surgery was 43.8 (minimum 29, maximum 60) years.

Two minor early postoperative complications were recorded during the primary study: one urinary tract infection that was treated with antibiotics and a persistent postoperative wound secretion that healed without specific treatment.

Ten patients were retrospectively assigned to group F because their final ODI was over 25 % (minimum 32 %, maximum 56 %), whereas all other (24; ODI minimum 0 %, maximum 14 %) patients were assigned to group N. The distributions of ODI and VAS scales over time and between groups are demonstrated in Fig. [2](#page-4-0)a–d.

In all patients of group  $N$ , the ODI, VAS<sub>overall</sub>, VAS<sub>back</sub>, and VAS<sub>leg</sub> parameters significantly improved over followup (each ANOVA  $p_{time} < 0.001$ ; all parameters' post hoc tests preoperative vs. all others  $p \lt 0.001$ . In group F, significant clinical improvements were observed for ODI (ANOVA  $p_{time} = 0.002$ , post hoc tests preop vs. 12 months  $p \lt 0.01$  and vs. final follow-up  $p \lt 0.05$ ),

VAS<sub>overall</sub>, and VAS<sub>back</sub> (each ANOVA  $p_{time} < 0.001$ , post hoc tests for preoperative vs. 12 months and final followup  $p < 0.001$ ), but not for VAS<sub>leg</sub> (ANOVA  $p_{time} = 0.437$ ) (Fig. [2a](#page-4-0)–d). A comparison between groups N and F showed better ODI scores (ANOVA  $p_{\text{group}} < 0.001$ ,  $p_{\text{group } \times \text{ time}} < 0.001$ ), VAS<sub>overall</sub> (ANOVA  $p_{\text{group}} < 0.001$ ,  $p_{\text{group} \times \text{time}} = 0.002$ , and VAS<sub>back</sub> (ANOVA  $p_{\text{group}} < 0.001$ ,  $p_{\text{group}} \times \text{time} < 0.001$ , but not VAS<sub>leg</sub> (ANOVA  $p_{\text{group}} = 0.181$ ,  $p_{\text{group}} \times \text{time} = 0.155$ ) for group N. Post hoc comparisons are shown in Fig. [2a](#page-4-0)–d.

At the final follow-up, significant differences in the radiologic measurement parameters for (the change in) disc height, segmental translation, and lordosis were found between the groups (Table [1\)](#page-4-0). The results of the correlation analysis between ODI/VAS scores and the radiographic measurement parameters at the final follow-up are reported in Table [2;](#page-5-0) Figs. [3,](#page-5-0) [4,](#page-5-0) [5.](#page-6-0) A significant Pearson's correlation was found between the final ODI and preoperative aDH  $(r = -0.346, p = 0.045)$ ; the final VAS<sub>overall</sub> and preoperative mDH ( $r = 0.481$ ,  $p = 0.004$ ) and pDH ( $r = 0.524$ ,  $p = 0.001$ ); and the final VAS<sub>back</sub> and preoperative pDH  $(r = 0.506, p = 0.002).$ 

Facet infiltration at the index segment was evaluated in eight group  $F$  patients. Two patients did not agree to an additional injection. The infiltration test was positive in five of these eight patients  $(62.5 \%)$ .

#### Discussion

In the second part of our study, we detected that (over)distraction with increased segmental lordosis and posterior translation of the superior vertebra led to clinical failure at the lumbosacral junction after TDR. To our knowledge, we are the first to observe that the iatrogenic changes that cause increased facet joint capsule tensile and shear forces are more likely to precipitate an inferior clinical outcome than those that create increased contact forces.

Similar to the results of Siepe et al. [[22,](#page-8-0) [23\]](#page-8-0), the patients with clinical failure reported pain during the early postoperative stage without apparent FJD at this time. The early and final clinical scores correlated with each other. Based on the results of the present study, these (early) negative results can be attributed to relatively small intraoperative changes of the segmental geometry, such as posterior translation or (over)distraction followed by increased lordosis. Our probabilistic FEM study identified that sagittal misalignment can cause both, increased facet joint capsule tensile forces in the case of iatrogenic posterior translation and increased compressive forces when iatrogenically shifting the superior vertebra anteriorly [\[27](#page-8-0)]. Although both situations would theoretically explain the

<span id="page-4-0"></span>



**Table 1** Preoperative and final follow-up radiological measurement parameters (mean  $\pm$  SD)

preop.



12 months

1 week

final

 $*$  p values from two-sided t test between groups F and N

development of FJD in patients with TDR [[19–23\]](#page-8-0), we have proven that especially a posterior translation of the superior vertebra leads to clinical failure. As discussed, posterior translation leads to higher capsule tensile or shear forces. However, the combination of both overdistraction and an increase in segmental lordosis would theoretically aggravate the resulting facet joint capsule, but not the compressive joint forces.

12 months

final

1 week

preop.

Clinical parameters	Radiological/clinical parameters	
	Positive correlations (Pearson's $r$ )	Negative correlations (Pearson's $r$ )
VAS <sub>overall</sub>	Disc height: mDH $(0.471)$ <sup>*</sup> ; pDH $(0.419)$ ; meanDH $(0.427)$	Translation: delta APT (-0.468)*; delta M $(-0.449)*$
	Postop VAS <sub>overall</sub> $(0.629)^*$ ; 12 months VAS <sub>overall</sub> $(0.440)^*$	
VAS <sub>back</sub>	Lordosis: delta $SL(0.415)$	
	Disc height: aDH $(0.428)$ ; mDH $(0.602)$ *; pDH $(0.557)$ *; meanDH $(0.564)$ *; delta aDH $(0.448)$ *; delta mDH $(0.415)$ ; delta pDH $(0.414)$ ; delta meanDH $(0.444)$ *	
	Postop VAS <sub>back</sub> (0.494) <sup>*</sup> ; 12 months VAS <sub>back</sub> (0.454) <sup>*</sup>	
VAS <sub>leg</sub>	Postop VAS <sub>leg</sub> $(0.662)^{*}$ ; 12 months VAS <sub>leg</sub> $(0.884)^{*}$	
<b>ODI</b>	Lordosis: SL $(0.439)^*$ ; delta SL $(0.538)^*$	Translation: delta APT (-0.436); delta M $(-0.546)*$
	Disc height: aDH $(0.495)^*$ ; mDH $(0.434)$ ; pDH $(0.386)$ ; meanDH $(0.459)$ <sup>*</sup> ; delta aDH $(0.531)$ <sup>*</sup> ; delta mDH $(0.421)$ ; delta pDH $(0.360)$ ; delta meanDH $(0.463)$ <sup>*</sup> ; 12 months ODI $(0.722)$	

<span id="page-5-0"></span>Table 2 Correlation results between clinical and radiological parameters at final follow-up

All demonstrated pairings of clinical and radiological or clinical parameters represent significant correlations ( $p < 0.05$ )

SL segmental lordosis, pDH posterior disc height, mDH middle disc height, aDH anterior disc height, meanDH mean disc height, M vertebral translation according to Meyerding, APT lordosis-corrected anterior posterior vertebral trsanslation, delta represents the difference between the final follow-up and the preoperative state, Postop postoperative

\* Indicates significance at  $p < 0.01$ 





Fig. 3 The scatter-dot diagrams illustrate the exponential relationship between the TDR-caused distraction amounts (change of the intervertebral disc height from preoperative to postoperative state = delta mDH) and the clinical scores **a** ODI and **b**  $VAS<sub>back</sub>$ .

In both scores, approximately 80 % of the clinical cases with an inferior outcome presented with a distraction of more than 6 mm (indicated by the gray area)

Fig. 4 The scatter-dot diagrams illustrate the exponential relationship between the lordosing effect of TDR from the preoperative to postoperative state (delta SL) and the clinical scores a ODI and **b** VAS<sub>back</sub>. In both scores, approximately 80 % of the clinical cases with an inferior outcome presented with a lordosis increase of more than  $5^\circ$  (indicated by the gray area)



<span id="page-6-0"></span>



This finding is of special importance because these parameters are mutually dependent on each other regarding how they affect the facet joints. This mutual dependence has been previously demonstrated in cadaver studies: segmental iatrogenic distraction leads to increased lordosis followed by a reduced overlapping area of articulation and an increase in the space within the facet joints, similar to a subluxation  $[36, 37]$  $[36, 37]$  $[36, 37]$  $[36, 37]$ . Rauschning  $[38]$  $[38]$  reported that subluxation of a joint leads to degeneration, which may explain the mechanism of FJD after TDR. All three parameters that correlated with an inferior clinical outcome in the present study lead to such a chronic subluxation. However, an iatrogenic anterolisthesis could likely neutralize the negative effect of segmental distraction on the tensile capsule forces. The number of our patients with anterior misalignment of the L5 vertebra  $>2$  mm was small  $(N = 4)$ , and these patients presented with good to excellent clinical results at the early and mid-term postoperative follow-ups. These patients have potentially tolerated higher contact forces because the facet joints are geared to such loads. Studies with a longer follow-up should determine whether higher contact forces also result in FJD and inferior clinical outcomes.

With regard to the FEM and clinical results, it is important to intraoperatively avoid a misalignment of the implant in the sagittal plane. A posterior translation (especially at L5/S1) could result from different resistances of the two vertebrae against the anterior–posterior forces during preparation. The sacrum is stable and fixed in the pelvis, and therefore a posterior shift of the L5 vertebra during the cutting of the keel or the insertion of the implant could occur. Lee et al. [\[39](#page-8-0)] observed a malpositioning of the superior and inferior parts of the prosthesis in relation to the vertebral endplates caused by an angular mismatch between the prosthesis, the keel-cutting device, and the (distracted) lordosis of the segment during TDR (especially at L5/S1). Malpositioning could be another reason for anterior–posterior vertebral misalignment when employing a more constrained device similar to the one employed in the present study. Based on our results, the precise placement of the superior and inferior parts of the prosthesis is crucial for clinical success. A large misalignment could be detected radiographically and corrected by separate preparation of the superior or inferior component of the prosthesis during the operation. Nevertheless, although this could be clinically relevant, an intraoperative visualization of a 2- or 3-mm anterior–posterior misalignment appears to be at the margin of the measurement precision of fluoroscopy.

Distraction is usually necessary because the restoration of disc height after TDR is an important factor for a good clinical outcome [\[26](#page-8-0), [40\]](#page-8-0). However, it is difficult for the surgeon to determine the ideal degree of correction of a degenerated disc, because the optimum amount is unknown

<span id="page-7-0"></span>and varies individually. No diagnostic tools can currently use preoperative radiologic images to estimate the needed physiologic disc height. Additionally, anatomic structures, such as muscles, ligaments and joint capsules, adapt to the degenerated status of the segment, but are not changed by TDR. TDR implants require a minimum intervertebral space. Therefore, the amount of distraction is larger in cases with a higher-grade DDD. The influence of preoperative disc height on the clinical outcome is controversial [\[41](#page-8-0), [42\]](#page-8-0). However, the correlation between inferior postoperative clinical scores and a small preoperative disc height further strengthens the hypothesis that the postoperative adaptation of the soft tissue to distraction presents problems for motion preservation. Patients with highly degenerated segments and small disc heights could potentially experience larger benefits from fusion. In clinical practice, we therefore recommend avoiding segmental overdistraction because it could lead to the early clinical failure of TDR. Due to the correlation between these factors, an increased lordosis may be a good intraoperative indicator of excessive distraction.

Admittedly, our study is not without limitations. Due to the small number of patients, the results (especially the non-significant results) should be interpreted with caution. However, the radiologic factors that we found to be associated with inferior outcomes after TDR are supported by the calculations of our probabilistic FEM study and are consistent with several clinical observational studies [[20,](#page-8-0) [25](#page-8-0)–[27\]](#page-8-0). Additionally, significant results were obtained despite the use of relatively rigid statistical methods. Because shear stresses in the facet joints could not be measured and only 62.5 % of the infiltration tests were positive, there is no direct proof of these forces being responsible for the inferior clinical results. Another limitation of our study was that we only used one implant type: a (semi)constrained ball–socket model. Further studies are needed to determine whether our findings can be transferred to different or unconstrained implants. An idealized spine model was employed in the probabilistic FEM study. This model did not take into consideration the segmental degeneration or adaptation due to this process, the morphology of the facet joints, or the influence of the varying soft tissue properties of the spinal motion segment. Therefore, the FEM results can only partially explain the outcome observed in the clinical aspect of the study.

In conclusion, our results indicate that overdistraction and sagittal misalignment—especially a posterior translation of the superior vertebra—are associated with clinical failure after TDR. We suggest using smaller implant sizes. We believe that the size of the implant should be geared more to the preoperative disc height than to an estimated physiological value. However, further studies with larger patient cohorts are necessary to determine optimal values.

Additionally, the introduction of an iatrogenic posterior translation has to be carefully avoided. Instrument development should focus on increasing the precision of implant positioning because issues relating to the intraoperative detection of small misalignments have not been solved thus far.

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Conflict of interest None.

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