

The N-terminal Flanking Region of the A1 Domain Regulates the Force-dependent Binding of von Willebrand Factor to Platelet Glycoprotein Ib α *

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Background: Hemodynamic force-regulated VWF-GPIb α interaction mediates platelet adhesion during the early stage of hemostatic and thrombotic processes.

Results: The VWF-A1 N-terminal sequence impedes the VWF-GPIb α interaction at low forces but stabilizes it as force increases.

Conclusion: The interplay between force and A1 N-terminal sequence regulates the VWF-GPIb α interaction.

Significance: Force regulation is crucial to the balance of the platelet adhesive function in hemostasis and thrombosis.

Binding of platelet glycoprotein Ib α (GPIb α) to von Willebrand factor (VWF) initiates platelet adhesion to disrupted vascular surface under arterial blood flow. Flow exerts forces on the platelet that are transmitted to VWF-GPIb α bonds, which regulate their dissociation. Mutations in VWF and/or GPIb α may alter the mechanical regulation of platelet adhesion to cause hemostatic defects as found in patients with von Willebrand disease (VWD). Using a biomembrane force probe, we observed biphasic force-decelerated (catch) and force-accelerated (slip) dissociation of GPIb α from VWF. The VWF A1 domain that contains the N-terminal flanking sequence Gln¹²³⁸–Glu¹²⁶⁰ (1238-A1) formed triphasic slip-catch-slip bonds with GPIb α . By comparison, using a short form of A1 that deletes this sequence (1261-A1) abolished the catch bond, destabilizing its binding to GPIb α at high forces. Importantly, shear-dependent platelet rolling velocities on these VWF ligands in a flow chamber system mirrored the force-dependent single-bond lifetimes. Adding the Gln¹²³⁸–Glu¹²⁶⁰ peptide, which interacted with GPIb α and 1261-A1 but not 1238-A1, to whole blood decreased platelet attachment under shear stress. Soluble Gln¹²³⁸–Glu¹²⁶⁰ reduced the lifetimes of GPIb α bonds with VWF and 1238-A1 but rescued the catch bond of GPIb α with 1261-A1. A type 2B VWD 1238-A1 mutation eliminated the catch bond by prolonging lifetimes at low forces, a type 2M VWD 1238-A1 mutation shifted the respective slip-catch and catch-slip transition points to higher forces, whereas a platelet type VWD GPIb α mutation enhanced the bond lifetime in the entire force regime. These data reveal the structural determinants of VWF activation by hemodynamic force of the circulation.

During the early stage of hemostatic and thrombotic processes, platelets tether to and translocate or roll on von Willebrand factor (VWF)² immobilized on disrupted vascular surfaces. This adhesive interaction is primarily mediated by binding of the 45-kDa N-terminal domain of the α subunit of the platelet glycoprotein Ib-IX-V complex (GPIb α) to the A1 domain of VWF (1–3). Remarkably, the VWF-GPIb α interaction has to be delicately balanced because insufficient adhesion cannot stop bleeding to maintain hemostasis, whereas excessive adhesion may result in thrombosis (4). Because such binding occurs under arterial blood flow, the VWF-GPIb α interaction is regulated by hemodynamic force (5–7). Circulating platelets do not bind VWF unless putative conformational changes occur around its A1 domain that exposes the GPIb α binding site (VWF activation) as a result of high hemodynamic force (8). The present view of the force-dependent VWF activation includes two steps: 1) relief of an autoinhibitory mechanism involving interdomain associations within the A1A2A3 tri-domain (9, 10) and between A1 and D'D3 (11) and 2) up-regulation of A1 binding affinity to GPIb α (6, 12–14). However, the biophysical and structural basis of how the VWF-GPIb α interaction is regulated when its hemostatic adhesive function is most needed remains unclear, in part, because of discrepant data.

To elucidate the molecular mechanism regulating VWF-GPIb α interaction, we previously used atomic force microscopy (AFM) and a flow chamber to show that A1-GPIb α and VWF-GPIb α interactions behaved as catch-slip bonds such that increasing force initially prolonged and then shortened bond lifetime (6). However, another study using optical tweezers (OT) observed a different phenomenon at forces lower than those

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² The abbreviations used are: VWF, von Willebrand factor; AFM, atomic force microscopy; BFP, biomembrane force probe; Lp, polypeptide Gln¹²³⁸–Glu¹²⁶⁰; OT, optical tweezers; ptVWD, platelet-type VWD; Sp, scramble polypeptide; VWD, von Willebrand disease; GPIb α , Glycoprotein Ib α ; GOF, gain of function; RBC, red blood cell.

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examined by us, reporting an A1-GPIIb α bond that could flex between two slip-bond states at ~ 10 pN (15). Note that in previous studies, different groups used recombinant sequences with different lengths of the N and C termini outside of the disulfide loop (Cys¹²⁷²–Cys¹⁴⁵⁸) that comprises the structure of the A1 domain. These sequences can be categorized into two groups: most studies of flow effects on platelet adhesion used A1 constructs that start at ~ 1238 (1238-A1) or even beyond 1238 to the N terminus (N-longer A1) (6, 14, 16–22), whereas most structural and kinetic studies used A1 constructs that start at ~ 1261 (1261-A1) or even shorter than 1261 at N terminus (N-shorter A1) (15, 23–29). In addition, many lines of evidence suggest that the N-terminal flanking sequence Gln¹²³⁸–Glu¹²⁶⁰ included in the 1238-A1 but excluded in the 1261-A1 constructs may play an important role in the VWF activation and may be responsible for discrepant observations from different studies. It has been shown that a N-shorter A1 (1271–1467) spanning the structurally resolved residues can bind GPIIb α but does not support platelet adhesion as efficiently as the N-longer A1 containing the N-terminal flanking sequence at high shear rates (17). Furthermore, it has been shown that a 15-residue N-terminal sequence (1237–1251) can completely inhibit the binding of VWF to GPIIb α (30). Recently, another sequence (Gln¹²³⁸–Glu¹²⁶⁰) was suggested to be part of an autoinhibitory mechanism that stabilizes A1A2A3 interdomain associations (31). Still, how this short N-terminal flanking sequence regulates VWF-GPIIb α interaction under force remains unclear.

To gain mechanistic insights into the regulatory effects of VWF regions surrounding A1, especially its N-terminal flanking region, on the force-dependent VWF-GPIIb α interaction, we used a biomembrane force probe (BFP) to analyze single-bond dissociation of GPIIb α from VWF, 1238-A1, and 1261-A1 under forces lower than those previously studied in the absence and presence of the Gln¹²³⁸–Glu¹²⁶⁰ sequence in solution. We showed that GPIIb α formed catch-slip bonds with VWF and slip-catch-slip bonds with 1238-A1, which govern platelet rolling on these substrates, but slip-only bonds with 1261-A1. Soluble Gln¹²³⁸–Glu¹²⁶⁰ inhibited whole blood platelet attachment, suppressed the respective GPIIb α catch bonds with VWF and 1238-A1, but rescued that with 1261-A1. The 1238-A1 mutation R1450E that exhibits the gain of function (GOF) phenotype of the type 2B VWD prolonged bond lifetime at zero force, whereas the 1238-A1 mutation G1324S that exhibits the loss of function phenotype of the type 2M VWD shifted the respective slip-catch and catch-slip transition points to higher forces. The GPIIb α mutation G233V that exhibits the GOF phenotype of platelet type VWD (ptVWD) retained the slip-catch-slip bond feature but greatly prolonged bond lifetime in the entire force regime. These results pinpoint the structural determinants of the VWF-GPIIb α catch bond, explain the discrepancy between catch and flex bonds, and elucidate the regulating mechanisms for VWF activation by hemodynamic force of the circulation.

EXPERIMENTAL PROCEDURES

Proteins and Antibodies—The recombinant WT VWF 1238-A1 domain (residues 1238–1471) (16), as well as single-residue

mutants R1450E and G1324S, has been described (22). The N-terminally truncated A1 domain (1261-A1) was expressed in bacteria and purified as the 1238-A1 protein. Plasma VWF was from Calbiochem. The N-terminally biotinylated polypeptide Gln¹²³⁸–Glu¹²⁶⁰ (Lp, QEPGGLVVPPTDAPVSPPTLYVE) of the A1 N-terminal flanking region and the scramble polypeptide (Sp, QLPTGVLGEPSTAVPTVYEVTPP) were synthesized by Selleck Chemicals (Houston, TX). Glycocalicin (extracellular domain of GPIIb α) was cleaved and purified from outdated platelets as described previously (6). Anti-GPIIb α mAb (AK2) was from Abcam (Cambridge, MA). Anti-A1 blocking (5D2) and anti-GPIIb α capturing (WM23) mAbs were gifts from Dr. Michael Berndt (Curtin University, Bentley, Australia) and Dr. Renhao Li (Emory University, Atlanta, GA), respectively.

Platelets and Cells—Abiding protocols approved by the respective institutional review boards of the Georgia Institute of Technology and Baylor College of Medicine, 10 ml of blood were collected from healthy donors for isolation of platelets and red blood cells (RBCs) and for direct use in flow chamber experiments after mixed with Lp or Sp. RBCs were washed, biotinylated, and stored for experiments for several weeks as described previously (32). Platelet-rich plasma was prepared in a 1:10 citrate buffer (170 mM sodium citrate and 83 mM citric acid in distilled water). To prevent unwanted platelet activation, 2 μ M prostaglandin E₁ was added to the citrate buffer. Blood was centrifuged at 150 $\times g$ for 15 min at room temperature. Platelet-rich plasma was then centrifuged at 900 $\times g$ for 10 min. The platelet pellet was resuspended in the HEPES-Tyrode buffer (134 mM NaCl, 12 mM NaHCO₃, 2.9 mM KCl, 0.34 mM sodium phosphate monobasic, 5 mM HEPES, and 5 mM glucose, 1% BSA, pH 7.4) as the washed platelets. CHO α 9 cells transfected to express WT or G233V GPIIb α have been described previously (33).

Platelet and CHO α 9 Cell Lysates—Platelets (2×10^9) were pelleted and resuspended in a 5-ml lysis buffer (125 mM NaCl, 50 mM Tris, pH 8.0, 1% Triton X-100) at 4 $^{\circ}$ C for 30 min with stirring. To avoid the unwanted shedding of GPIIb α , the final medium included 5 mM EDTA, 2 mM phenylmethylsulfonyl fluoride, and 1 \times protease inhibitor (#78437; Pierce). After 16,000 $\times g$ centrifugation at 4 $^{\circ}$ C for 20 min, the platelet lysates in the supernatant were collected through a filter (50 K; Millipore, Billerica, MA). CHO α 9 cells transfected to express WT or G233V GPIIb α were lysed similarly.

Functionalization of Glass Beads—VWF, A1, glycocalicin, and capturing mAb WM23 were precoupled covalently with maleimide-PEG3500-*N*-hydroxysuccinimide (molecular mass, ~ 3500 Da; JenKem Technology, Plano, TX). Modified proteins were mixed with streptavidin-maleimide (Sigma-Aldrich), linked to 3- μ m (diameter) silanized beads (Fig. 1, *B* and *D*, *left* for VWF or A1 and *right* for glycocalicin or WM23) and washed, as described previously (32). To immobilize full-length GPIIb α on surfaces, beads precoupled with WM23 were incubated with platelet or CHO α 9 cell lysates in a rotor for 2 h at room temperature and washed (Fig. 1*B*, *right*). After resuspending in PBS with 1% human serum albumin, beads were ready for immediate use in BFP experiments. To coat Lp or Sp on beads, streptavidin-precoupled beads were prepared as above. Biotin-labeled Lp or Sp was coupled to streptavidin beads (Fig. 1*B*, *left*)

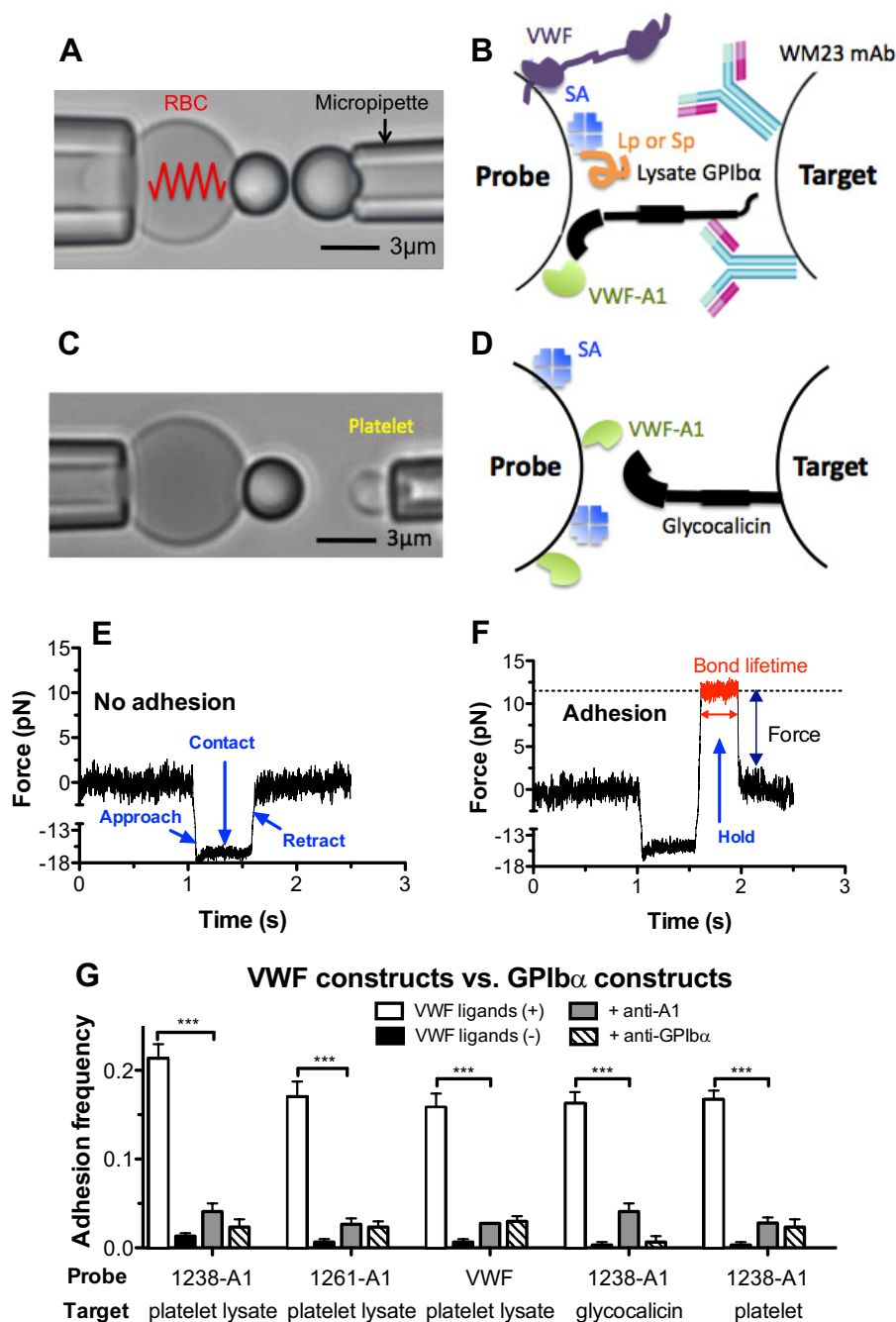


FIGURE 1. BFP force clamp assay. *A* and *C*, BFP photomicrograph. A micropipette-aspirated RBC with a bead (*left*, termed “probe”) attached to the apex formed a pico-force sensor, as depicted by a spring. It was aligned with another bead (*A*) or a platelet (*C*) (*right*, termed “target”) aspirated by an apposing micropipette. *B* and *D*, BFP functionalization with purified molecules. A1 or full-length VWF was covalently coupled to the probe (*left*). GPIIb α was captured from lysates of platelets or CHO α b9 cells by mAb WM23, which was covalently precoated on the target (*B*, *right*). Glycocalicin was covalently coupled to the target (*D*, *right*). Streptavidin was also covalently coupled to the probe for attachment to biotinylated RBC, as well as coupling the polypeptide Gln¹²³⁸–Glu¹²⁶⁰ (Lp) or scramble polypeptide (Sp). *E* and *F*, force versus time traces from two representative test cycles. A target was driven to approach a probe (<1.1 s, ~0 pN), contacted for 0.5 s (1.1–1.6 s, ~15 pN), retracted, and ended the cycle if no adhesion was detected (>1.6 s, ~0 pN) (*E*) or held at a preset force until dissociation if adhesion was detected (1.6–2 s, ~12 pN, indicated in red), after which the target was retracted to the starting position (>2 s, ~0 pN) (*F*). Lifetime was measured from the point when the clamped force (12 pN) was reached (1.26 s) to the point when the bond dissociated (2 s), signified by a force drop to zero. *G*, binding specificity. Adhesion frequencies between targets coated with platelet lysate GPIIb α , glycocalicin, or platelet GPIIb α and probes coated without (–, black columns) or with (+, white columns) 1238-A1 or VWF, in the absence or presence of 50 μ g/ml anti-A1 (5D2, gray columns) or anti-GPIIb α (AK2, hatched columns) blocking mAb. Each probe-target pair was tested repeatedly for 100 approach-contact-retract cycles to estimate an adhesion frequency. Five probe-target pairs were tested to obtain mean \pm S.E. ***, $p < 0.001$ as assessed by unpaired, two-tailed Student’s t test.

by a 2-h incubation at room temperature. After that, the same washing steps were used before BFP experiments.

BFP Experiments—Our home-built BFP has been described (34). A personal computer installed with custom-written

LabView™ programs were used for image analysis and piezoelectric translator control, which ran in repeated cycles to measure adhesion frequency as well as bond lifetime (force clamp assay at non-zero forces and thermal fluctuation assay at the zero

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force) (32, 34–36). In each cycle, the target was driven to approach and contact the probe with a 20-pN compressive force for a certain contact time (0.5 s for glyocalicin, 0.2 s for GPIIb/IIIa from platelet or CHO α 3 β 9 cell lysates and for platelet GPIIb/IIIa) that allowed for bond formation and then retracted for adhesion detection. During the retraction phase, an adhesion event was signified by tensile force (Fig. 1F), but no tensile force was detected in a no-adhesion event (Fig. 1E). For the adhesion frequency assay, adhesion and no-adhesion events were enumerated to calculate an adhesion frequency in 100 repeated cycles for each probe and target pair. Because the adhesion frequency P_a depends on the site densities of receptors (m_r) and ligands (m_l) on the contact area, to compare the binding affinity of Lp to different receptor candidates, the effective affinities per receptor density (Fig. 2D) were derived via formula $-\ln(1 - P_a)/m_r$ (37). In the force clamp assay, the target was held at a desired force to wait for bond dissociation and returned to the original position to complete the cycle. Lifetime was measured from the instant when the force reached the desired level to the instant of bond dissociation (Fig. 1F, red trace) (34, 35). In the thermal fluctuation assay, the target was held at zero force to allow contact with the probe via thermal fluctuation. Bond formation and dissociation were identified from the respective reduction and resumption of the probe thermal fluctuation. Lifetime was measured from the moment of bond formation to the moment of bond dissociation as described previously (32).

Flow Chamber Assays—Whole blood perfusion was performed as described previously (9, 38). Briefly, whole blood mixed with 0.5 mM of Lp or Sp was perfused through a parallel plate flow chamber (Glycotech, Gaithersburg, MD) at 1,500 s^{-1} shear rate over the chamber floor coated with collagen (100 μ g/ml) or VWF (100 μ g/ml) by physical absorption. After a 2-min perfusion, the surface was washed with PBS, and several frames of attached platelets were recorded. Tethered platelets were observed with a phase contrast objective (40 \times) and recorded by video microscopy.

Platelet rolling velocity was measured as described previously (6). Briefly, washed platelets were perfused at various wall shear stresses over 1238-A1 or 1261-A1 (100 μ g/ml) absorbed on the flow chamber floor. Mean rolling velocities were measured over a 0.1-s interval by video microscopy with frame by frame analysis by the Nikon NIS-Elements software. At each wall shear stress, \sim 20 velocities of rolling platelets were measured and averaged. The data are presented as means \pm S.E. The washed platelet tethering was snapshot with a phase contrast objective (20 \times) during the experiments.

Direct Binding Assay by ELISA—This assay was performed similarly to that described previously (10, 31). Microtiter wells were coated with lysate GPIIb/IIIa, A1, or A2. Biotin-labeled Lp or Sp (0.5 mM) were incubated with above putative receptor-coated wells for 1 h at 37 $^{\circ}$ C. After washing, the wells were incubated with 1:200 dilution of neutravidin-horseradish peroxidase conjugate (Pierce) 1 h at 37 $^{\circ}$ C. The wells were again washed, and the substrate (*o*-phenylenediamine; Sigma) was added. The reaction was stopped with 0.025 ml of 2 N H_2SO_4 , and the plates were read at 490-nm absorbance. Net binding was determined by subtracting absorbance values from wells added only BSA from the total binding values obtained in wells

added the corresponding polypeptides. VWF-A2 as the isotype control in this assay has been described previously (9).

Analysis of Lifetime Distributions with a Two-state Model—At each force bin, the survival frequency as a function of bond lifetime t_b was calculated as the fraction of events with lifetime $>t_b$. In our previous study (6), 1238-A1-GPIIb/IIIa bonds were assumed to dissociate from a single state so that the pooled bond lifetimes were analyzed by a single exponential distribution (Equation 1) after treating a small fraction ($<10\%$) of long lifetimes (>2 s) as outliers.

$$\text{Survival frequency} = \exp(-k_{\text{off}}t_b) \quad (\text{Eq. 1})$$

Taking the log linearizes the right-hand side of Equation 1, the semi-log survival frequency *versus* bond lifetime plot is predicted to appear linear. The negative slope of the line would be used as an estimate for off rate k_{off} . However, if long lifetime events were included, the $\ln(\text{survival frequency})$ *versus* t_b plots were no longer linear (see Fig. 8). To analyze such data, we extended the single-state model to a two-state model that assumes a slow dissociation state coexisting with a fast dissociation state (35). The survival frequency data for each force bin were fitted by Equation 2, which superimposes two exponential decays,

$$\text{Survival frequency} = \omega_1 \exp(-k_1 t_b) + \omega_2 \exp(-k_2 t_b) \quad (\text{Eq. 2})$$

where k_i and ω_i are the off rate and the associated fraction of the i th state ($i = 1, 2$), which satisfy the constraints $\omega_1 + \omega_2 = 1$ and $k_1 < k_2$, respectively.

RESULTS

We used a BFP to measure adhesion frequency and bond lifetime between VWF, A1 domains, and polypeptides coated on a glass bead (Fig. 1, B and D, left, Probe) attached to the apex of a micropipette-aspirated RBC (Fig. 1, A and C, left) and GPIIb/IIIa or glyocalicin immobilized on another glass bead (Fig. 1, B and D, right) or platelet aspirated by an apposing micropipette (Fig. 1, A and C, right, Target). For better molecular orientation with purified protein, GPIIb/IIIa was captured from platelet lysates by WM23, a mAb with the epitope in the macroglycopeptide region (Fig. 1B). After a controlled contact, the BFP detected the absence (Fig. 1E) or the presence (Fig. 1F) of adhesion from the force signal upon target retraction, calculated adhesion frequency from repeated tests (Fig. 1G), and measured bond lifetime under constant force (Fig. 1F).

The binding specificity was established as GPIIb/IIIa-bearing targets (lysate GPIIb/IIIa, glyocalicin, or platelet GPIIb/IIIa) adhered at significantly higher frequencies to probes coated with VWF ligands (1238-A1, 1261-A1, or VWF) than those not coated with VWF ligands or blocked by anti-A1 or anti-GPIIb/IIIa mAb (Fig. 1G). The severely shortened lifetimes of the rare adhesions in the presence of blocking antibodies suggest that the remaining adhesion events are mostly nonspecific (data not shown).

GPIIb/IIIa Dissociates from 1238-A1 as a Triphasic Slip-Catch-Slip Bond, 1261-A1 as a Monophasic Slip-only Bond, and Full-length VWF as a Biphasic Catch-Slip Bond—Using AFM in a previous study (6), we observed that 1238-A1-glyocalicin dis-

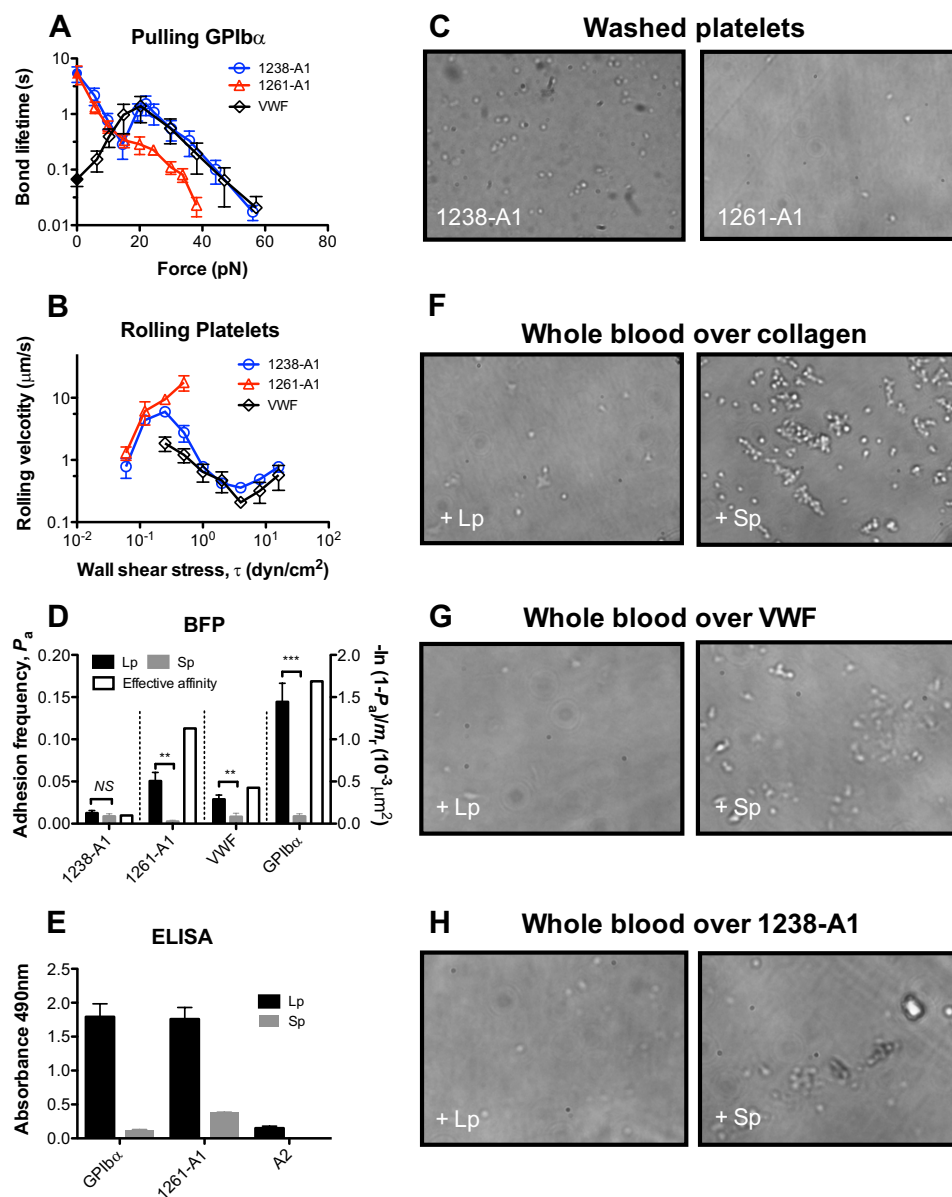


FIGURE 2. The role of Gln¹²³⁸-Glu¹²⁶⁰ on GPIIb α interactions with VWF and 1238-A1. *A*, force-dependent of lifetime of platelet lysate GPIIb α bonds with the VWF and two forms of A1. Lifetimes (mean \pm S.E. of >20 measurements per point) were measured by the thermal fluctuation assay (closed symbols) at zero force and by the force clamp assay at nonzero forces (open symbols). *B*, wall shear stress-dependent rolling velocity (mean \pm S.E. of ~ 20 platelets per point) on VWF and two forms of A1. *C*, platelets attach differently to 1238- and 1261-A1 coated surfaces. Washed platelets were perfused over a surface coated with 1238- or 1261-A1 at 8 dyn/cm² wall shear stress. Representative snapshots were shown. *D*, adhesion frequency P_a (left y axis, closed bars, mean \pm S.E. of >3 probe-target pairs each contacting 100 times per bar) between targets bearing 1238-A1, 1261-A1, VWF, or platelet lysate GPIIb α and probes bearing Gln¹²³⁸-Glu¹²⁶⁰ (Lp, black columns) or a control scramble polypeptide (Sp, gray columns). NS, not significant; **, $p < 0.01$; ***, $p < 0.001$, assessed by unpaired, two-tailed Student's *t* test. The right y axis variable (open bars) represents a metric of the propensity of Lp binding to its counter-molecule whose variable site density (m_r , measured separately by flow cytometry) has been accounted for via the formula $-\ln(1 - P_a)/m_r$ to allow for comparison of Lp binding to 1238-A1, 1261-A1, VWF, and GPIIb α (37). *E*, ELISA showing specific binding of polypeptide Lp in a purified system. Data (mean \pm S.E. of triplicates, two separate experiments) show binding of lysate GPIIb α , 1261-A1, and VWF-A2 (as a negative control) to immobilized polypeptide Lp (black columns) or Sp (gray columns) (0.5 μ M). *F-H*, effect of Gln¹²³⁸-Glu¹²⁶⁰ on platelet adhesion under shear. Whole blood mixed with 0.5 μ M Lp (left column) or Sp (right column) was perfused over a surface coated with collagen (*F*), VWF (*G*), or 1238-A1 (*H*) at 1,500 s⁻¹ wall shear rate. After a 2-min perfusion, the platelets were washed with PBS and observed microscopically. All photomicrographs are representatives of separate experiments using the same blood donor.

sociated as a biphasic catch-slip bond at forces of >15 pN. A recent study using OT reported that the 1261-A1-GPIIb α dissociation behaved as a "flex bond" at forces of <20 pN that switched between two slip-bonds with 20-fold different off rates (15). To investigate this apparent discrepancy, we measured single-bond lifetimes in the full force regime by BFP using both 1238- and 1261-A1 domains. The former includes the Gln¹²³⁸-Glu¹²⁶⁰ sequence, whereas the latter excludes it. We

observed a very similar catch-slip bond for 1238-A1 dissociation from GPIIb α (captured from platelet lysates by WM23) in the same force regime as that of the previous AFM study (6) (Fig. 2*A*, blue circle). At forces of <15 pN, however, an additional slip bond was observed, qualitatively similar to the slip bond observed in the OT study (15). In addition to force clamp experiments, we used a thermal fluctuation assay to directly measure the bond lifetime at zero force (32). The value of $5.4 \pm$

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1.6 s so measured matched the zero force extrapolation of the slip bond trend in the low force regime (Fig. 2A, blue circle). Thus, the force-dependent single 1238-A1-GPIb α bond lifetime exhibits a triphasic pattern transitioning from a slip bond at 0–16 pN to a catch bond at 16–25 pN, followed by another slip bond at >25 pN.

In sharp contrast, the 1261-A1-GPIb α interaction was a slip-only bond whose lifetime decreased monotonically with increasing force (Fig. 2A, red triangle). Below 15 pN, the lifetime *versus* force curves of the two A1s coincided. Between 16 and 25 pN, however, the lifetime curve for 1238-A1 increased, whereas that for 1261-A1 decreased. Beyond 25 pN, the lifetimes of GPIb α bonds with both A1 domains decreased with increasing force, but the bond lifetimes were significantly shorter for 1261-A1 than 1238-A1. In addition, without force-induced bond strengthening, few 1261-A1 bonds survived the target retraction to reach >40 pN forces for lifetime measurement (Fig. 2A). These results indicate that the Gln¹²³⁸-Glu¹²⁶⁰ sequence in *cis* plays a key role in stabilizing the A1-GPIb α interaction under force, because truncating this sequence eliminated the A1 catch bond with GPIb α .

To determine how well the GPIb α binding properties of the A1 domain represent those of VWF, we measured the force-dependent lifetime of single GPIb α bond with full-length VWF using BFP thermal fluctuation and force clamp assays. Gratifyingly, the lifetime *versus* force curve of the VWF-GPIb α bond (Fig. 2A, black diamond) was very similar to that of the 1238-A1-GPIb α bond (Fig. 2A, blue circle) at the catch-slip bond force regime. At lower forces (<16 pN), however, the GPIb α bond with VWF continued to behave as a catch bond, sharply contrasting to those with both A1s. At zero force, the GPIb α bond lifetime was ~80-fold lower with VWF than A1 (0.067 *versus* 5.4 s). These data suggest an autoinhibitory mechanism involving VWF domains surrounding A1 that reduced the bond stability with GPIb α . However, this inhibition can be relieved as VWF was progressively activated by increasing force such that the GPIb α bond with 1238-A1 achieved its full stability as that with VWF, giving rise to the VWF-GPIb α catch bond at forces <16 pN. These data also caution us not to overinterpret and generalize binding results obtained using A1 domains before confirmation with full-length VWF.

Platelet Rolling Velocities on 1238-A1, 1261-A1, and VWF Were Governed by Their Respective Slip-Catch-Slip, Slip-only, and Catch-Slip Bonds with GPIb α —Previously, we demonstrated an inverse relationship between rolling velocity and bond lifetime—the longer the bond lifetime, the slower the rolling velocity (6, 39)—that provided definitive evidence that flow-enhanced rolling is caused by catch bonds (40). To corroborate the single-bond lifetime results in Fig. 2A, we measured platelet rolling on surfaces coated with either of the two A1 domains or VWF over a range of wall shear stresses in a flow chamber. The velocities of washed platelets rolling on these substrates showed stress-dependent patterns mirroring the corresponding patterns of bond lifetimes: triphasic for 1238-A1, monophasic for 1261-A1, and biphasic for VWF (Fig. 2B). At shear stress >1 dyn/cm², 1261-A1 no longer supported platelet rolling, preventing measurements beyond that point. This is evident from the snapshots taken at 8 dyn/cm² that show 1238-A1 supported

platelet tethering and rolling at high shear, whereas 1261-A1 did not (Fig. 2C).

Polypeptide Gln¹²³⁸-Glu¹²⁶⁰ Binds GPIb α and 1261-A1 and Inhibits Platelet Adhesion—It has been reported that the VWF-derived polypeptide Leu¹²³²-Asp¹²⁶¹ acts as a putative GPIb α binding site and can inhibit VWF binding to platelet (30). In addition, it was recently suggested that this A1 N-terminal sequence may bind A1 noncovalently (31). We therefore measured direct binding of BFP probes bearing a similar polypeptide Gln¹²³⁸-Glu¹²⁶⁰ (Lp) to BFP targets coated with GPIb α , VWF, 1238-A1, or 1261-A1. Specific binding of Lp to GPIb α , VWF, and 1261-A1, but not 1238-A1, was observed as the adhesion frequencies to the former three molecules (but not the last molecule) were abrogated when Lp was replaced by a control scramble polypeptide (Sp) (Fig. 2D, closed bars). To compare the propensities of Lp binding to these molecules, the specific adhesion frequencies (P_a , obtained by subtracting the adhesion frequency of Sp from that of Lp) were converted to effective binding affinities per unit receptor site density ($-\ln(1 - P_a)/m_r$) by normalizing the average number of adhesion bonds ($-\ln(1 - P_a)$) by the respective site densities of 1238-A1, 1261-A1, VWF, and GPIb α (m_r). Although we did not measure the site density of Lp, the same batch of Lp-bearing beads were used to analyze binding of all four receptors. Hence the respective effective affinities per unit receptor density should be equal to the effective two-dimensional affinities of Lp for 1238-A1, 1261-A1, VWF, and GPIb α multiplied by the same constant of Lp site density. The values for the latter three molecules were ~11-, 4.7-, and 17-fold higher than that for 1238-A1, respectively (Fig. 2D, open bars). Compared with 1261-A1 and GPIb α , the VWF binding to Lp was much weaker, possibly because this binding was mediated by the VWF structure outside 1238-A1. Additional population experiments by ELISA (Fig. 2E) confirmed the direct interactions of Lp to GPIb α and 1261-A1 by single-bond experiments. Thus, VWF has at least two binding sites for GPIb α : one resides within 1261-A1 and the other involves Gln¹²³⁸-Glu¹²⁶⁰. This sequence also binds noncovalently to 1261-A1 and other VWF domains in addition to forming a covalent peptide bond with 1261-A1 in the full-length VWF structure.

To investigate the functional role of Lp in platelet adhesion under shear, we perfused whole blood mixed with soluble Lp or Sp over a collagen-coated (Fig. 2F), VWF-coated (Fig. 2G), or 1238-A1-coated (Fig. 2H) surface in a flow chamber. These experiments mimic the hemostatic scenario at disrupted vascular sites where plasma VWF deposits on exposed subendothelium to capture circulating platelets (41). Many more attached platelets were observed when whole blood was mixed with Sp (Fig. 2, F–H, right panels) than with Lp (Fig. 2, F–H, left panels), confirming the role of Gln¹²³⁸-Glu¹²⁶⁰ to inhibit the binding between platelet and VWF (30).

Soluble Gln¹²³⁸-Glu¹²⁶⁰ Reduces GPIb α Bond Lifetimes with VWF and 1238-A1 but Rescues the Catch Bond with 1261-A1—Because Lp binds GPIb α much better than VWF (Fig. 2D), its inhibitory effect on platelet adhesion (Fig. 2, F–H) may be explained by its binding to GPIb α (Fig. 2, D and E), which may interfere, at least in part, with the VWF-GPIb α interaction that mediates platelet adhesion. To test this hypothesis, we used

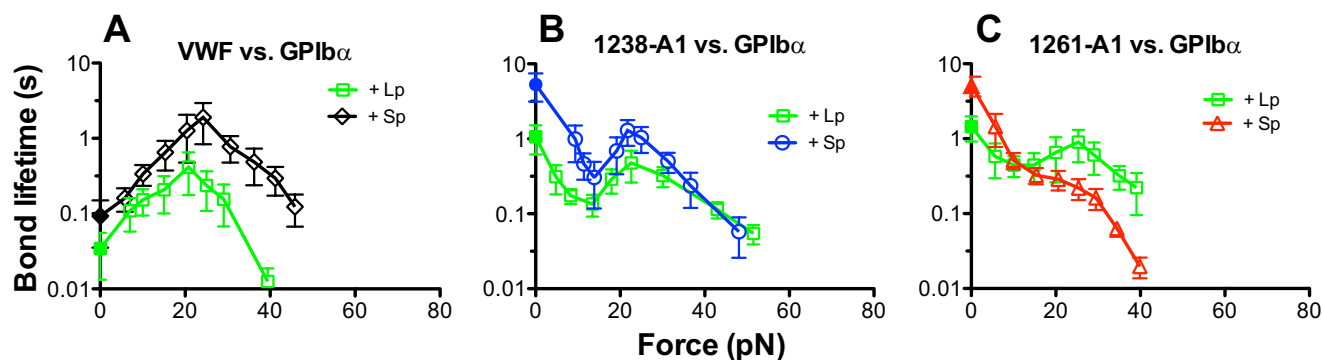


FIGURE 3. The effect of soluble Gln¹²³⁸–Glu¹²⁶⁰ on GPIIb/IIIa interactions with VWF (A), 1238-A1 (B), or 1261-A1 (C) in the presence of soluble Lp or Sp (10 μ g/ml or 4.2 μ M). Lifetimes (mean \pm S.E. of >20 measurements per point) were measured by the thermal fluctuation assay (closed symbols) at zero force and by the force clamp assay at nonzero forces (open symbols).

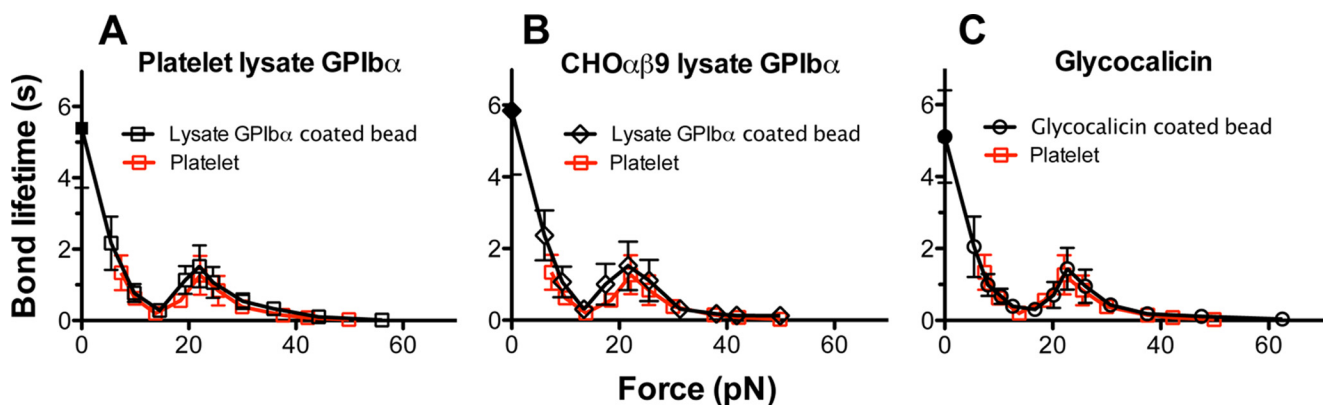


FIGURE 4. Force-dependent lifetimes of 1238-A1 bonds with different GPIIb/IIIa preparations. Plots of lifetime versus force of 1238-A1 bonds with GPIIb/IIIa from lysates of platelets (A, black squares) or CHO α 9 cells (B, black diamonds) captured on targets or with glycocalicin (C, black circles) coated on targets. The curve of 1238-A1 bonds with GPIIb/IIIa expressed on platelets (red squares) were used as the standard to compare the properties of purified proteins. The previous data of 1238-A1 interaction with platelet lysate GPIIb/IIIa from Fig. 2A were replotted for comparison in A. Lifetimes (mean \pm S.E. of >20 measurements per point) were measured by the thermal fluctuation assay (closed symbols) at zero force and by the force clamp assay at nonzero forces (open symbols).

BFP to directly measure the effect of Lp on force-dependent VWF–GPIIb/IIIa bond lifetime. Supporting our hypothesis, VWF–GPIIb/IIIa bond lifetime was shortened by the addition of soluble Lp (Fig. 3A), but not Sp (compare Figs. 2A and 3A), over the full force regime.

To further elucidate the mechanism for the A1 N-terminal flanking region to regulate platelet binding, we measured lifetimes of GPIIb/IIIa bonds with 1238-A1 and 1261-A1 in the presence of soluble Lp or Sp. As expected, the respective lifetime versus force curves of GPIIb/IIIa interactions with 1238-A1 and 1261-A1 were indistinguishable in the absence (Fig. 2A) and presence (Fig. 3, B and C) of Sp, for the control sequence should have no effect. In the presence of Lp, however, the lifetime curves of the 1238-A1 (Fig. 3B) downshifted but still retained their triphasic profile. More interestingly, the monophasic lifetime curve of 1261-A1 became triphasic, first decreasing, then increasing, and again decreasing with increasing force (Fig. 3C). In fact, in the presence of Lp, the 1261-A1 and 1238-A1 curves were close to each other but distinct from the VWF curve. Thus, soluble Gln¹²³⁸–Glu¹²⁶⁰ suppresses GPIIb/IIIa binding to VWF and 1238-A1 but rescues the GPIIb/IIIa catch bond with 1261-A1. The former suggests that Lp competes for GPIIb/IIIa binding with VWF and 1238-A1, whereas the latter suggests that a possible 1261-A1–Lp–GPIIb/IIIa sandwich bond may restore the catch bond behavior. These data show that the

Gln¹²³⁸–Glu¹²⁶⁰ sequence plays a similar role in *trans* as it does in *cis* in stabilizing the A1–GPIIb/IIIa bond against increasing force. The inability for the recent OT study (15) to observe GPIIb/IIIa catch bond may be explained by their use of 1261-A1 in the fusion construct.

Effects of Different Forms of WT GPIIb/IIIa—In addition to studying different force regimes and using different A1 domains, another possible cause of the discrepancies between our previous AFM data (6) and the OT data from another study (15) may be the use of different forms of GPIIb/IIIa. To test this possibility, we compared lysate GPIIb/IIIa from platelets or CHO α 9 cells captured by WM23 mAb on target beads (Fig. 1B) and glycocalicin covalently linked to target beads (Fig. 1D) with native GPIIb/IIIa expressed on platelets (Fig. 1C). The lifetime curves of 1238-A1 bonds with GPIIb/IIIa captured from lysates of platelets (Fig. 4A, black square) or CHO α 9 cells (33) (Fig. 4B, black diamond) or with glycocalicin (Fig. 4C, black circle) are indistinguishable from 1238-A1–platelet curve, displaying the same triphasic force dependence (Fig. 4, red square). These data indicate that the 1238-A1–GPIIb/IIIa bond dissociation characteristic is determined by the extracellular domain of GPIIb/IIIa and not affected by the different post-translational modifications of GPIIb/IIIa in platelets and CHO α 9 cells or how GPIIb/IIIa is immobilized on surfaces.

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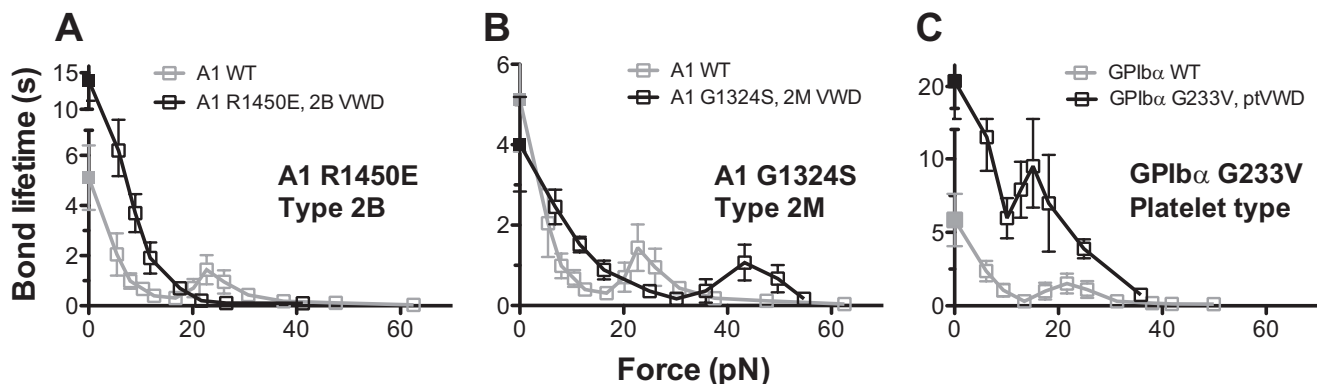


FIGURE 5. **Force-dependent lifetimes of 1238-A1-GPIIb α bonds with VWD mutations.** *A* and *B*, plots of lifetime versus force of glycofascin bonds with type 2B VWD mutant 1238-A1R1450E (*A*) and type 2M VWD mutant 1238-A1G1324S (*B*) (black squares). The previous data of 1238-A1-glycofascin interaction from Fig. 4C were replotted for comparison (gray squares). *C*, plots of lifetime versus force of 1238-A1 bonds with WT (gray squares) or G233V (black squares) GPIIb α from CHO α 99 cell lysates. Lifetimes (mean \pm S.E. of >20 measurements per point) were measured by the thermal fluctuation assay (closed symbols) at zero force and by the force clamp assay at nonzero forces (open symbols).

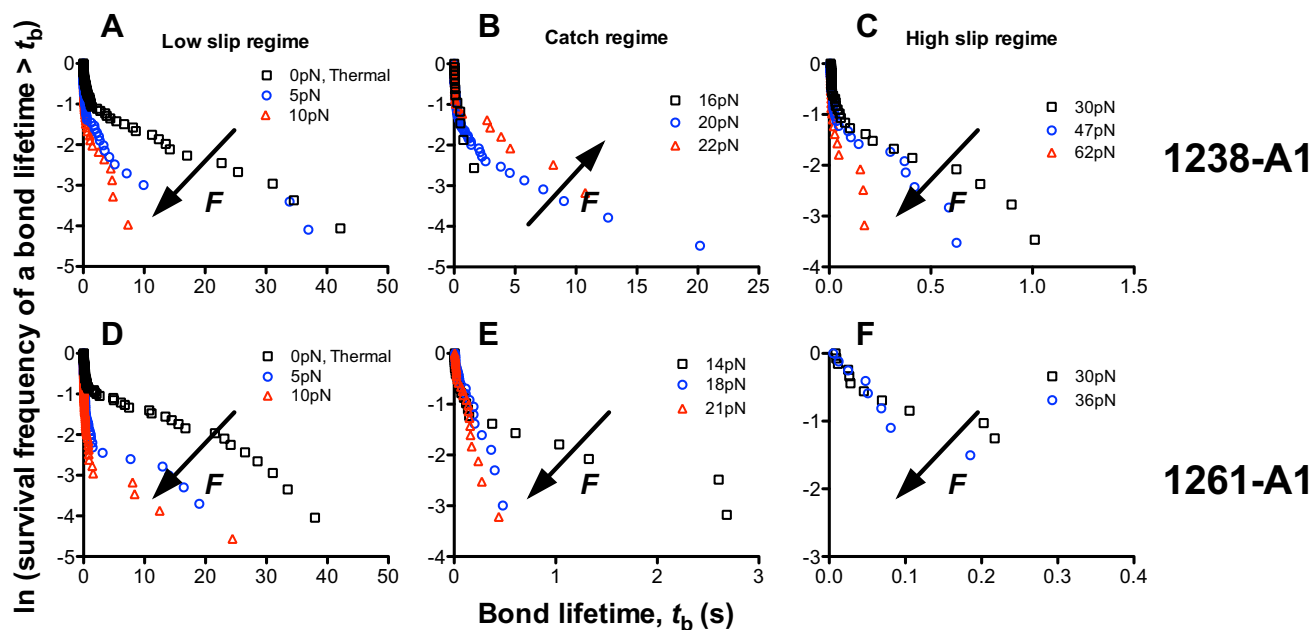


FIGURE 6. **Bond lifetime distributions.** Survival frequencies, calculated as the fraction of measurements (including both short and long lifetime events) with a bond lifetime $>t_b$, were plotted versus t_b for each force bin in each of three regimes: low (*A* and *D*), intermediate (*B* and *E*), and high (*C* and *F*) forces, for GPIIb α bonds with 1238-A1 (*A*–*C*) and 1261-A1 (*D*–*F*). These forces corresponded to the low slip bond, the catch bond, and the high slip bond regime for 1238-A1 interactions, but 1261-A1 interactions only showed slip bonds in the entire force regime. The arrows indicate the directions of force increase.

Effects of VWD Mutants—The putative conformational change resulting in VWF activation may be induced or affected by VWF or GPIIb α mutations naturally occurring in patients with VWD. Our previous AFM study demonstrated that a type 2B VWD mutation, 1238-A1R1450E, eliminated the catch bond found in the 1238-A1–glycofascin interaction by prolonging the lifetimes at low forces, resulting in an up and left shifts of the lifetime versus force curve relative to the WT curve (6). In contrast, a type 2M VWD mutant 1238-A1G1324S shortened lifetimes at low forces and right-shifted the biphasic catch-slip bond curve toward higher forces (12). The present BFP study extended the lifetime versus force curves for these mutants to lower forces. We found that glycofascin interaction with 1238-A1R1450E displayed a monophasic slip-only bond (Fig. 5*A*, black), but that with 1238-A1G1324S showed a right-shifted triphasic slip-catch-slip bond (Fig. 5*B*, black), qualita-

tively similar to that with the WT 1238-A1 (Fig. 5, gray). These data confirm the previous AFM results at forces >20 pN and add a new slip-bond regime at low forces for 1238-A1G1324S. The extended results also included lifetimes at zero force measured via the thermal fluctuation assay, which are 13.9 ± 2.7 and 4 ± 1.1 s for R1450E (Fig. 5*A*, black closed square) and G1324S (Fig. 5*B*, black closed square), respectively. The former value is much longer, whereas the latter value is slightly shorter than the zero force lifetime of 5.1 ± 1.2 s for the WT 1238-A1 (Fig. 5, gray closed square), explaining the GOF phenotype for 1238-A1R1450E and the loss of function phenotype for 1238-A1G1324S. We also studied a ptVWD mutant GPIIb α (G233V) captured from lysates of G233V CHO α 99 cells. Consistent with its GOF phenotype in other assays (42–44), the lifetime versus force curve of 1238-A1 bonds with GPIIb α G233V (Fig. 5*C*, black) was significantly

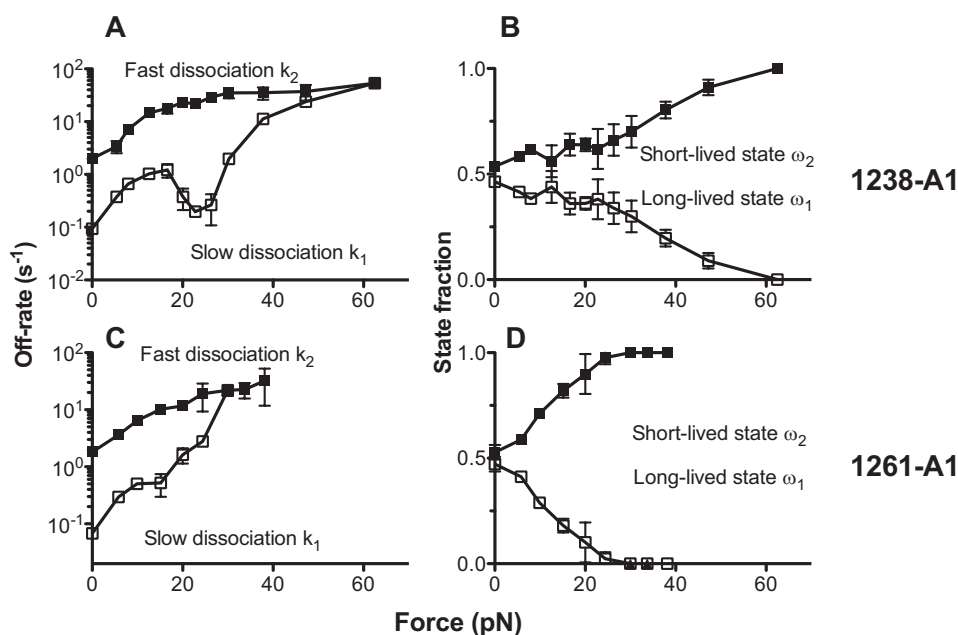


FIGURE 7. **Analysis of two-state kinetics.** A two-state model was fit to the bond lifetime distribution at each force bin of GPIIb α dissociation from 1238-A1 (A and B) or 1261-A1 (C and D) to evaluate model parameters at that force, which are plotted *versus* force. The kinetic parameters are: the slow (k_1) and fast (k_2) off rates of dissociation from the two states of different stabilities (A and C) and the fractions (ω_1 and ω_2 , $\omega_1 + \omega_2 = 1$) of bonds associated with the corresponding short-lived (high off rate) and long-lived (low off rate) states (B and D). The error bars represent \pm 95% confident interval of the best fit value.

upshifted relative to that with WT GPIIb α (Fig. 5C, *gray*). The zero force lifetime measured by the thermal fluctuation assay was 20.5 ± 7.4 s, \sim 4-fold longer than the WT value of 5.8 ± 1.8 s ($p < 0.01$ by Student's t test).

Characterization of A1-GPIIb α Dissociation by a Two-state Model—In addition to the force-dependent average of lifetimes, their distributions also demonstrated that 1238-A1-GPIIb α interaction dissociated as a slip-catch-slip bond (Fig. 6, A–C), but 1261-A1-GPIIb α interaction dissociated as a slip-only bond (Fig. 6, D–F). For the first order irreversible dissociation of a single monomeric bond from a single state along a single pathway in a single step, lifetime at each force bin should follow a single-exponential distribution, appearing linearly in the semi-log survival frequency *versus* lifetime plot, with the negative slope equal to the off rate. However, the semi-log lifetime distributions at many force bins (Fig. 6) appear as two line segments connected at \sim 2 s, invalidating the assumption underlying the simple kinetics model that predicts a single exponential decay (Equation 1). We found that such double exponentially distributed lifetimes are similar to those of the bonds between $\alpha_5\beta_1$ integrin and fibronectin (45, 46) but distinct from those of the bonds between P- or L-selectin and P-selectin glycoprotein ligand 1 or other ligands, whose lifetimes are distributed as single exponentials (47, 48).

Assuming that two subpopulations of A1-GPIIb α bonds coexist and dissociate at a slow (k_1) and a fast (k_2) off rate, respectively, we analyzed the lifetime distributions using a two-state model (Equation 2) to obtain the best fit force-dependent off rates and their associated fractions of these subpopulations of bonds of GPIIb α with 1238-A1 (Fig. 7, A and B) and with 1261-A1 (Fig. 7, C and D). For GPIIb α dissociation from both A1s, the off rate of the long-lived bond (k_1) was 1 order of magnitude smaller than that of the short-lived bond (k_2) at zero

force (Fig. 7, A and C), which is consistent with the results obtained by the recent OT study at low forces (15). Because the fractions of the long-lived (ω_1) and short-lived (ω_2) bonds were similar (Fig. 7, B and D), the long-lived bonds dominated the average lifetime. Although the relative fractions were stable around the catch bond force regime, overall, force gradually increased the fraction of short-lived bonds at the expense of the long-lived bonds. The fast off rate k_2 increased monotonically as the force increased. By comparison, the slow off rate k_1 first increased, then decreased, and again increased with force, accounting for the triphasic slip-catch-slip bond behavior. Surprisingly, the two states merged into one at force above 60 pN for 1238-A1 (Fig. 7A), but at much lower force \sim 30 pN for 1261-A1 (Fig. 7C). This analysis confirms that losing the Gln¹²³⁸–Glu¹²⁶⁰ sequence makes forced dissociation of GPIIb α from 1261-A1 much faster than 1238-A1.

Comparison with Previous Measurements by Different Methods—We replotted the present BFP lifetime *versus* force curves in Fig. 8A to compare with previous data obtained by AFM using 1238-A1 (6) and OT using 1261-A1 (15). At low forces, the OT measurements determined two states that dissociated at distinct rates (Fig. 8A, *blue circle* and *blue triangle*): one state at low forces and the other engaging at \sim 10 pN with a 20-fold longer lifetime and a greater force resistance. The authors termed this behavior “flex bond” (15). For a direct comparison, we overlaid the 1261-A1 lifetime distributions measured by the BFP (Fig. 8B, *black symbols*) on those measured by the OT at \sim 10 pN (Fig. 8B, *blue symbols*). The BFP measurement at \sim 10 pN also showed two states, although only the long-lived state was consistent with the OT data. However, we observed two states at forces between 0 and 60 pN for 1238-A1 (Fig. 7B) and between 0 and 30 pN for 1261-A1 (Fig. 7D) instead of just a single state below 9.55 pN that flexed to another state above

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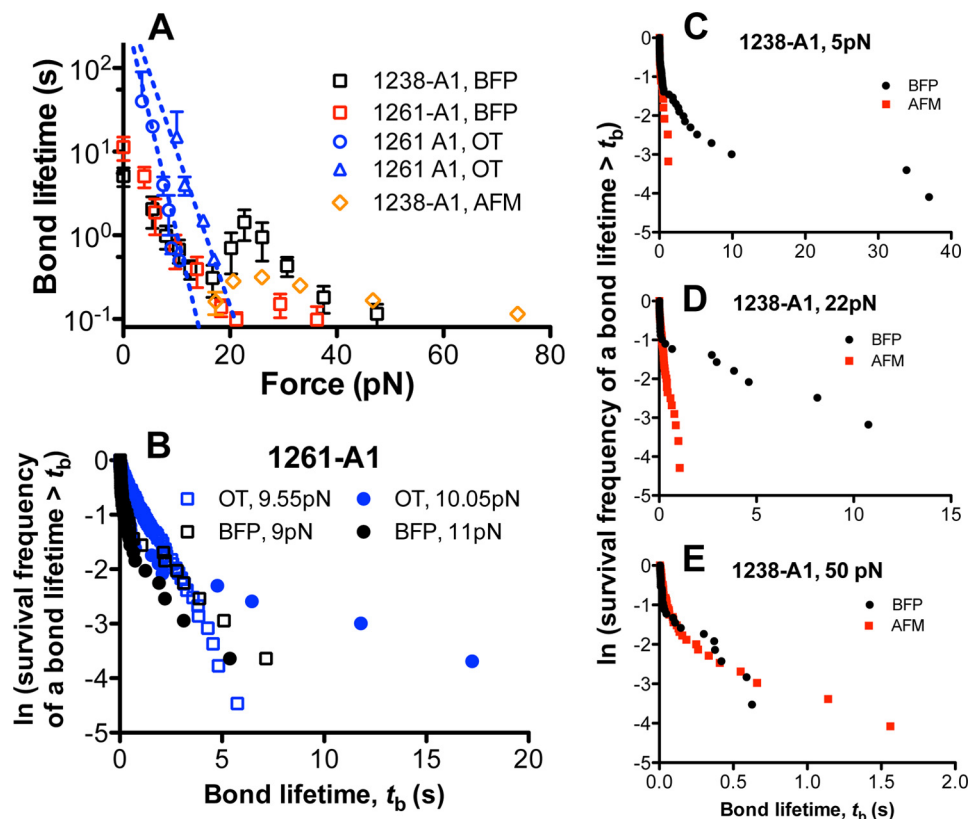


FIGURE 8. Comparison with previous results. A, plots of lifetime versus force of GPIIb/IIIa bonds with 1238-A1 (black square) or 1261-A1 (red square) measured by BFP in this study (mean \pm S.E. of >20 measurements per point), with 1238-A1 measured by AFM in our previous study (6) (orange diamond), and with 1261-A1 measured by OT in a previous study (15) (blue circle and triangle). B, comparison of 1261-A1 lifetime distributions measured by BFP in this study (black symbols) and by OT in the previous study (15) (blue symbols) at two very close force bins (squares and circles). C–E, lifetime distributions measured by BFP in this study (black) and those measured by AFM in our previous study (red) were compared at three representative forces: 5 pN for the low force regime where the low slip bond was observed in this study but not in our previous study (C), 22 pN for the intermediate force regime where the catch bond was observed in both of our studies (D), and 50 pN for high force regime where the high slip bond was observed (E) in both of our studies.

10.05 pN (15). The effect of force measured by the BFP was gradual; 1-pN force change ~ 10 pN did not drastically change the two-state characteristics of the A1-GPIIb/IIIa bond (Fig. 8B, black symbols).

The second and third phases of the triphasic bond lifetime versus force curve in the present BFP study are qualitatively similar to the biphasic lifetime curve observed in our previous AFM study in the same force range and with the same 1238-A1 construct but have quantitatively longer lifetimes (6). This is due to an improvement—a counter-drifting system—to the BFP used in the present study, which enabled us to measure longer bond lifetimes. By comparison, bond lifetimes of >2 s were excluded as possible outliers in our previous AFM experiments (6), for they might be affected by instrument drift and/or resulted from multiple bonds. This can be seen by overlaying the lifetime distributions of the present BFP study with those of the previous AFM study measured at three representative force bins. Because of the 2-s cutoff in the lifetime measurement, the AFM data only match the short-lived state portion of the BFP data in the first slip regime (5 pN; Fig. 8C) and the catch regime (22 pN; Fig. 8D) but miss the long-lived state of the BFP data, explaining the shorter average lifetimes of the AFM data than the BFP data (Fig. 8A). By comparison, the AFM and BFP data match well in the second slip bond regime (55 pN; Fig. 8E) where the short-lived state dominates over the long-lived state

(Fig. 7B), thus preventing the 2-s cutoff used in the AFM study from biasing the data.

DISCUSSION

The present study investigated the structural determinants of force-induced activation of VWF binding to GPIIb/IIIa. We found that the 1238-A1-GPIIb/IIIa could fully account for VWF-GPIIb/IIIa at forces >20 pN, which behaved as a catch-slip bond, in agreement with our previous results (6). As force decreased, the VWF-GPIIb/IIIa continued to behave as a catch bond even when force became zero, whereas the 1238-A1-GPIIb/IIIa turned into a slip bond with ~ 80 -fold longer lifetime at zero force (Fig. 2A). Similar triphasic force-dependent kinetics has been observed by us in the dissociations of sLe^x-bearing microspheres and carbohydrate ligand-expressing cells from E-selectin (49). The 1238-A1-GPIIb/IIIa slip bond at low force suggests that VWF structural elements surrounding the 1238-A1 impede its binding to GPIIb/IIIa, which may be relieved by force. In sharp contrast, the 1261-A1-GPIIb/IIIa bond behaved as a slip-only bond in the entire force range and hence did not capture the dissociation characteristics of the VWF-GPIIb/IIIa bond despite the resemblance with the 1238-A1-GPIIb/IIIa bond at force <15 pN (Fig. 2A).

The distinct GPIIb/IIIa dissociation (Fig. 2A) from and platelet rolling (Fig. 2, B and C) on 1238-A1 and 1261-A1 highlight the

regulatory role of the A1 N-terminal flanking region. The addition of Lp to whole blood suppressed platelet attachment to immobilized collagen (Fig. 2F), VWF (Fig. 2G), and 1238-A1 (Fig. 2H) under flow, which may be explained, at least in part, by the competitive binding of this polypeptide to GPIb α (Fig. 2, D and E). This may reduce the VWF-GPIb α complex interface, thereby shortening bond lifetime (Fig. 3A). Interestingly, soluble Lp weakens the catch bond for 1238-A1 by downshifting the lifetime curve (Fig. 3B), whereas it rescues the catch bond for 1261-A1 by prolonging the lifetime of its bond with GPIb α at intermediate forces (Fig. 3C). The former can be explained by an inhibitory role of Lp, which was shown previously (30) and confirmed in this study (Fig. 2). Note that the zero force lifetimes for both 1238- and 1261-A1s were reduced by soluble Lp (Fig. 3, B and C), suggesting that Lp exerts its inhibitory effect at the low force regime and increasing force relieves the inhibitory effect. The data also suggest a similar function of the Gln¹²³⁸-Glu¹²⁶⁰ sequence in stabilizing the A1-GPIb α interaction at forces >16 pN regardless of whether it exists in *cis* (Fig. 2A, 1238-A1) or in *trans* (Fig. 3B, 1261-A1 + Lp) to A1. This may be explained by the interaction of Lp with 1261-A1 and GPIb α (Fig. 2, D and E), which may provide an additional cross-link by sandwiching Lp between 1261-A1 and GPIb α to strengthen their binding interface.

We extended our previous results on two 1238-A1 mutations by showing that the type 2B VWD mutant R1450E eliminated the catch bond by prolonging bond lifetime at low forces (Fig. 5A) and type 2M VWD mutant G1324S right-shifted the bond lifetime *versus* force curve (Fig. 5B). In addition, we analyzed 1238-A1 dissociation from the ptVWD mutant GPIb α G233V for the first time and found that this mutation significantly prolonged single-bond lifetime at all forces tested (Fig. 5C). Importantly, thermal fluctuation experiments showed that the bond lifetime at zero force for 1238-A1R1450E was \sim 2-fold longer than WT ($p < 0.05$), that for 1238-A1G1324S was 26% shorter than WT ($p < 0.05$), and that for GPIb α G233V was \sim 4-fold longer than WT ($p < 0.01$) (Fig. 5). These results are consistent with their respective GOF and loss of function phenotypes found in other assays, explaining the spontaneous binding of VWF to platelet for type 2B VWD (50, 51) and ptVWD (42–44), as well as the ineffective binding of VWF to platelet for type 2M VWD (22, 52) observed *in vitro*.

To reconcile the discrepant results between our previous AFM study (6) and a recent OT study (15), we investigated several differences between the two studies. We showed that 1238-A1 dissociated from glycolalgin (used in our previous work (6)) indistinguishably from platelet GPIb α or GPIb α from lysates of platelets or CHO $\alpha\beta$ 9 cells (Fig. 4). The present BFP data qualitatively agreed with our previous AFM data at forces >20 pN and the OT data at forces <20 pN (Fig. 8), indicating that the different force ranges used by the two studies may contribute to the discrepancies, whereas the different measurement techniques used were not the cause of the discrepancies. However, the different A1 constructs have been identified as the main cause of the discrepancies because the present BFP measurements qualitatively reproduced the same force-dependent lifetimes of GPIb α bonds with 1238-A1 as the previous AFM measurements (6) and with 1261-A1 as the recent OT

measurements (15) in their respective force ranges. We note that considerable variations in their ability to support platelet attachment between the N-longer and N-shorter A1s have long been reported. It has been shown that an N-longer A1 interacted with platelets at 50–6,000 s⁻¹ shear rates indistinguishably from full-length VWF, whereas an N-shorter A1 exhibited progressive loss of activity with increasing shear above 1,500 s⁻¹ and became essentially inactive at 6,000 s⁻¹. Our data reaffirm the importance of the VWF-GPIb α catch bond by its direct observation with full-length VWF and by elucidation of its different force-dependent dissociation characteristics from the two A1 domains. More significantly, both the present and our previous studies showed that the VWF-GPIb α catch bond governed flow-enhanced platelet rolling on VWF (Fig. 2B). Although we also observed a slip bond at forces of <20 pN resembling a flex bond (Fig. 8B) as reported by the OT study (15), this behavior differs from that of full-length VWF. Thus, our work has elucidated the regulation of VWF activation and catch bond formation with GPIb α by the A1 N-terminal flanking region.

Recently, a protein thermodynamic study showed that the *cis*-binding of Lp to A1 stabilizes the overall 1238-A1 structure (53). However, their flow chamber data showed that platelets roll slower on 1261-A1 than 1238-A1 under a range of shear stresses and suggested that 1261-A1 would also adapt a catch bond as 1238-A1 does. A possible explanation for this discrepancy is that two binding states exist for 1261-A1. Clarification of this issue is one of the goals of future studies.

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