

Resting-State Glutamate and GABA Concentrations Predict Task-Induced Deactivation in the Default Mode Network

Yuzheng Hu,* Xi Chen,* Hong Gu,* and Yihong Yang

Neuroimaging Research Branch, National Institute on Drug Abuse, National Institutes of Health, Baltimore, Maryland 21224

Deactivation of the human brain's default mode network (DMN) is regarded as suppression of endogenous activity to support exogenous task-related processes. This phenomenon has important functional relevance and insufficient DMN deactivation has been implicated in several neuropsychiatric disorders. However, the neurochemical mechanism of the DMN's deactivation remains largely unknown. In the present study, we test the hypothesis that the major excitatory and inhibitory neurotransmitters, glutamate and GABA, respectively, are associated with DMN deactivation. We used magnetic resonance spectroscopy to measure neurotransmitter concentrations in the posterior cingulate cortex/precuneus (PCC/PCu), a key component of the DMN, and functional magnetic resonance imaging to evaluate DMN deactivation induced by an n-back working memory task. Our results demonstrate significant associations of glutamate and GABA with DMN deactivation. Specifically, high regional GABA concentration in the PCC/PCu area is associated with enhanced deactivation induced by the task in the same region, whereas high glutamate concentration is associated with reduced deactivation. Furthermore, the association between GABA and DMN deactivation increases with the cognitive loads. These neurochemical characteristics of DMN deactivation may provide novel insights toward better understanding of the DMN's functions under normal physiological conditions and dysfunctions in neuropsychiatric disorders.

Introduction

Neuroimaging studies have demonstrated that, compared with the resting state, activity in a set of brain regions including the posterior cingulate cortex/precuneus (PCC/PCu), medial prefrontal cortex (mPFC), and hippocampus consistently decrease (termed as deactivation) during a wide range of tasks requiring external orientation (Shulman et al., 1997). These distributed brain regions were defined as the default mode network (DMN) by Raichle et al. (2001). DMN deactivation is thought to be associated with suppression of spontaneous brain activities and reallocation of resources to ongoing, attention-demanding tasks (McKiernan et al., 2003); therefore, the more demanding the task, the stronger the deactivation of the DMN tends to be (Singh and Fawcett, 2008). Furthermore, several studies have found that DMN deactivation is correlated with behavioral performance. For example, stronger deactivation of PCC in a working memory (WM) task predicts better performance (Anticevic et al., 2010). In contrast to DMN function in healthy participants, failure of DMN deactivation has been observed in psychiatric disorders such as schizophrenia (Whitfield-Gabrieli et al., 2009), Alzheimer's dis-

ease (Greicius et al., 2004), and autism (Kennedy et al., 2006). These findings indicate the importance of DMN deactivation contributing to both normal cognitive functions and psychiatric disorders. However, the underlying neurochemical mechanism of DMN deactivation remains largely unknown.

DMN deactivation has been well depicted by blood oxygen level-dependent (BOLD) imaging (Ogawa et al., 1990). Although influenced by multiple physiological and biophysical factors (Ogawa et al., 1993), BOLD signal has been found to be coupled with neural activity (Logothetis et al., 2001). Particularly, negative BOLD response has been found to associate with decreased neural activity (Stefanovic et al., 2004; Shmuel et al., 2006). At the cellular level, neuronal activity is regulated by multiple neurochemical processes including cycling of glutamate and GABA, the major excitatory and inhibitory neurotransmitters in the CNS. The coordination between glutamatergic neurons and GABAergic interneurons is believed to have a direct impact on BOLD contrast (Logothetis et al., 2001; Buzsáki et al., 2007). Congruent with this idea, previous studies have shown a negative correlation between GABA concentration and BOLD signals (Northoff et al., 2007; Stagg et al., 2011). A positive correlation between glutamate concentration and BOLD signal change has also been reported (Enzi et al., 2012). In addition, associations among glutamate, GABA, and functional connectivity have been reported (Kapogiannis et al., 2013). However, the coordinative effects of glutamate and GABA on task-induced BOLD change have so far not been well demonstrated.

By combining BOLD and magnetic resonance spectroscopy (MRS) techniques, the relationship between neurotransmitters and brain activation/deactivation can be examined at a system level. Based upon the findings mentioned above, we hypothe-

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*Y.H., X.C., and H.G. contributed equally to this work.

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Correspondence should be addressed to Yihong Yang, PhD, Neuroimaging Research Branch, National Institute on Drug Abuse, National Institutes of Health, Baltimore, MD 21224. E-mail: yihongyang@mail.nih.gov.

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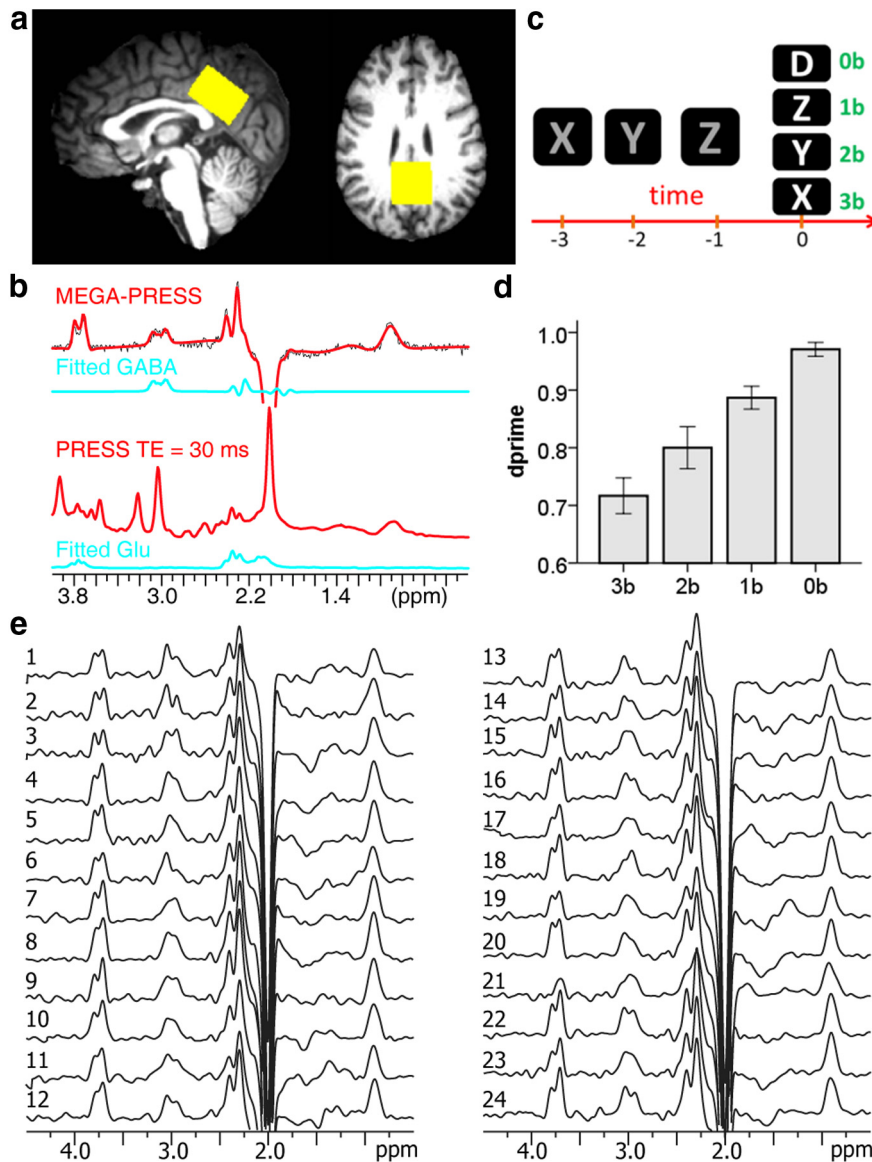


Figure 1. MRS and fMRI experiments. *a*, A VOI was placed at the PCC/PCu for ^1H spectroscopy. *b*, Regional GABA and glutamate concentrations were assessed using MRS techniques. *c*, An n-back working memory task was administered to probe the default mode network deactivation, with 0-back as the control condition (time scale is 2 s). *d*, Behavioral performance (dprime) during the working memory task demonstrated a significant memory load effect. *e*, Individual GABA spectra. A weighting function of Lorentzian–Gaussian transformation ($l_b = -3$ Hz, $g_b = 8$ Hz) was applied, and the displayed peak intensities were normalized to N-acetylaspartic acid.

sized that DMN deactivation is associated with both excitatory and inhibitory neurotransmitters and the associations are dependent on cognitive load. To test this hypothesis, the present study examined the relationship between DMN deactivation induced by a WM task with different loads and the endogenous concentrations of glutamate and GABA in the PCC/PCu region. Positive and negative correlations with BOLD signals were expected for glutamate and GABA, respectively, in a load-dependent fashion.

Materials and Methods

Subjects. Twenty-four healthy subjects (age: 34.4 ± 8.6 years; 10 females) participated in the study. Subjects had no histories of neurological or psychiatric disorders and had no current or past drug abuse. The use of drugs that affect neurotransmitter levels or cortical inhibition and excitation was exclusionary for participants in this study. Participants were questioned about prescription medication and illicit drug use and under-

went urine toxicology assessing the presence of prescription medications and drugs of abuse at their initial screening visit. They were also screened for drugs of abuse (urine toxicology) including benzodiazepines on the day of scanning. Before the experiment, all subjects provided written informed consent approved by the Institutional Review Board of the National Institute on Drug Abuse.

MRS data acquisition and processing. MRS and fMRI scans were performed on a Siemens 3T Trio scanner using a 12-channel coil. The MRS experiments preceded the fMRI task. A $2.4 \times 3.2 \times 3.6$ cm³ voxel of interest (VOI) was placed at the PCC/PCu (Fig. 1*a*) and a control region was placed at the primary visual cortex. The ^1H spectrum optimized for detecting GABA was acquired by a MEGA-PRESS sequence (Rothman et al., 1984; Mescher et al., 1998) with the following parameters: TE/TR = 68/5000 ms; number of average = 96 (scan time = 8 min). The editing pulses with a duration of 19.9 ms and a bandwidth of 45 Hz were applied alternatively at frequency of 1.9 or 7.5 ppm. There were two loops in the GABA sequence: the interleaving of edit on/off in the inner loop and the averaging in the outer loop. It has been reported in the literatures that PRESS with TE ~30 ms achieves reliable glutamate detections (Mullins et al., 2008; Hancu, 2009). Therefore, the glutamate concentration was obtained by a PRESS sequence (TE/TR = 30/3000 ms; number of average = 128; scan time = 6 min) from the same VOI. Field map shimming was performed before MRS scans to ensure the line-width of water <14 Hz. A VAPOR (VARIABLE pulse Power and Optimized Relaxation delays) module (Tkáč et al., 1999) was used in both sequences to achieve water suppression. Spectra of water were also acquired from the same VOI using the same MEGA-PRESS and PRESS sequences without the water suppression module, respectively. The number of average of the water spectra was 16. All MRS data were quantified using LCModel (version 6.3-0D; Provencher, 1993, 2001; Fig. 1*b*). The LCModel assumes that the experimental spectrum can be fitted in the frequency domain by the linear combination of a group of basis sets, each of which is the frequency spectrum of a certain metabolite/macromolecule (MM), together with a baseline to compensate MM signals that the MM basis sets do not account for. The reliability of the measurement was indicated by the Cramer–Rao lower

bounds (CRLB) and a commonly accepted CRLB criterion of 20% was chosen to reject low-quality spectra. Different basis sets from simulation were used for the MEGA-PRESS and PRESS quantifications. Both GABA and glutamate concentrations were referenced to the unsuppressed water concentration. The MRS signal of water is subject to different proton densities and T1 and T2 relaxation times in gray matter, white matter, and CSF. Therefore, the volume fractions of different tissue types were calculated by segmenting T1 images in SPM8. The water signal was then corrected by different tissue fractions and sensitivity factors in gray matter (0.92), white matter (0.81), and CSF (1.0) to account for the partial volume effect (Geramita et al., 2011). T1 and T2 values of GABA (T1 = 1310 ms, T2 = 88 ms) (Edden et al., 2012; Puts et al., 2013) and glutamate (T1 = 1270 ms, T2 = 181 ms) (Mlynárik et al., 2001; Ganji et al., 2012) were used for a global relaxation correction for absolute quantification in millimolar (mM).

Working memory task. Participants performed an n-back WM task (Owen et al., 2005) during a 14 min block design fMRI scan. The n-back

task presented a single letter for 500 ms, followed by an interstimulus interval of 1500 ms under four conditions: 0-back (0b), 1-back (1b), 2-back (2b), and 3-back (3b). In the 0b vigilance condition, participants were asked to respond with a button press to letter “D”; in the 1b condition, participants responded if the current letter was identical to the previous one; and in the 2b/3b conditions, participants responded if the current letter was identical to the second/third previous one (Fig. 1c). The task scan included three runs and each run had eight blocks during which each condition (0b, 1b, 2b, or 3b) was presented twice. There were 15 consecutive trials in each block (33% targets). The 0b block was placed at the beginning of each run and the order of 1b, 2b, and 3b blocks was counterbalanced. A 2 s visual instruction preceded each block to indicate the upcoming condition. The primary behavioral measurement of task performance at each task condition was *dprime*, estimated by the hit rate penalized by the false alarm rate (Haatveit et al., 2010). All subjects practiced a brief version of the *n*-back WM task outside the scanner before imaging.

fMRI data collection and preprocessing. A single-shot gradient-echo echo-planar imaging sequence was used to acquire BOLD images during the WM task scans. The imaging parameters were as follows: TR/TE = 2000/27 ms; FA = 78°; slice thickness = 4 mm without gap; 39 slices; FOV = 220 × 220 mm² with in-plane resolution of 3.44 × 3.44 mm². To facilitate spatial normalization, an anatomical scan was acquired using a T1-weighted 3D magnetization prepared rapid gradient echo sequence (256 × 192 × 208 matrix size; 1 × 1 × 1 mm³ spatial resolution; TI/TR/TE = 900/1900/3.51 ms; flip angle = 9°).

Preprocessing steps for fMRI data included slice-timing correction, head motion correction, spatial smoothing with a 6 mm Gaussian kernel, and quadratic detrending. General linear models were constructed to obtain the task-evoked activation maps during the 1b, 2b, and 3b WM task compared with the vigilant 0b condition; the six motion parameters were included as covariates. The task activation maps were then normalized to standard Talairach and Tournoux space with a resampling resolution of 3 × 3 × 3 mm³ using nonlinear registration (Geng et al., 2009) to facilitate group analysis.

Statistical analyses. WM load effects on behavior performance (*dprime*) were assessed by repeated-measures ANOVA. The relationship between glutamate and GABA concentrations in the PCC/PCu and relationships of the two neurotransmitters with gender and age were examined by bivariate correlation analyses.

Whole brain voxelwise fMRI activation/deactivation patterns at the group level were evaluated by ANOVA. Specifically, contrast maps of 1b, 2b, and 3b versus 0b estimated from the first level analysis were modeled as three levels of the WM load. A threshold for significance was set to $p < 0.01$ corrected for whole brain multiple comparisons based on Monte Carlo simulations, which corresponds to uncorrected $p < 0.001$ and a minimum cluster size of 594 mm³. To examine brain deactivation in more detail, a region of interest (ROI) was defined in the PCC/PCu based on the main effect of WM task revealed from the whole brain voxelwise ANOVA analysis. A post hoc test on BOLD signal changes across different WM loads was performed. In addition, to explore the functional relevance of the PCC/PCu deactivation, correlation between the BOLD signal change in the PCC/PCu and the task performance (*dprime*) was examined.

To assess how neurotransmitters exert influence on brain response to the WM task at different cognitive loads, a hierarchical regression procedure was performed to regress the PCC/PCu deactivation (BOLD signal change relative to 0b) on age, fraction of gray matter (GM), and glutamate and GABA concentrations, under conditions of 1b, 2b, and 3b separately. Age was included in the model because of its significant influence on the DMN deactivation (Grady et al., 2006; Spreng and Schacter, 2012). GM fraction was included because of its potential influence on the relationship between neurotransmitters and BOLD signal change. At the first step of regression (model 1), the PCC/PCu deactivation was predicted by a constant term, GM and age. At the second step (model 2), the PCC/PCu GABA and glutamate concentrations were added in. For a negative control purpose, the same regression procedures were performed by replacing GABA and glutamate concentrations from the PCC/PCu with that from the visual primary cortex. Glutamine or Glx (the

combination of glutamate and glutamine) was used to replace glutamate in the model 2 to construct two contrast models, which could be used to determine the unique excitatory profile of glutamate.

A previous study (Kapogiannis et al., 2013) suggested that glutamate and GABA measured from posterior medial cortex predict the resting state functional connectivity within the entire DMN. It would therefore be interesting to determine whether glutamate and GABA measured from the PCC/PCu region associate with the entire DMN deactivation. For this purpose, we did a complementary analysis. The DMN was defined as deactivated regions in the working memory task, mainly including mPFC, PCC/PCu, and bilateral parahippocampus. The same regression models used to examine the relationship between PCC/PCu deactivation and neurotransmitters were performed to examine the relationship between the entire DMN deactivation and neurotransmitters.

Results

Behavior

WM load was found to modulate task performance as measured by *dprime* (Fig. 1d; $F_{(3,69)} = 30.78$, $p = 0.0005$). Post hoc *t* tests using Bonferroni correction for multiple comparisons determined that *dprime* was significantly different between each pair of the two conditions ($p < 0.04$).

Glutamate and GABA levels in the PCC/PCu

Individual GABA spectra are shown in Figure 1e. The full-width at half-maximum of the MEGA-PRESS and the 30 ms PRESS metabolite spectra measured by LCModel were 5.3 ± 1.5 and 5.2 ± 1.2 Hz, respectively. The fitting quality, which was quantified as the ratio of the maximum in the spectrum minus baseline to twice of the root mean square of the fitting residuals, of the MEGA-PRESS spectra was 45 ± 8 and that of 30 ms PRESS was 51 ± 5 . The average CRLB of GABA was 9% (SD 1%, range 7–11%), that of glutamate was 5% (SD 1%, range 4–6%). No subject was excluded by the criterion of CRLB. Glutamate and GABA concentrations in the PCC/PCu were 7.46 ± 0.56 and 1.82 ± 0.20 mM, respectively. Age was negatively correlated with glutamate ($r = -0.43$, $p = 0.04$), but not GABA ($p = 0.18$). No gender effect was found on glutamate or GABA concentration ($p > 0.65$). No correlation was found between glutamate and GABA concentrations ($p = 0.84$). In the MRS VOI, the fractional tissue composition was $56 \pm 5\%$ for gray matter, $33 \pm 4\%$ for white matter, and $11 \pm 3\%$ for CSF.

Brain activation/deactivation during the WM task

Significant main effect of the WM task was shown in a number of brain regions. To illustrate activation and deactivation induced by the task, brain activities at the contrast of 3b-0b within these areas are displayed in Figure 2a. The task-induced positive activation regions included bilateral superior and inferior parietal lobules, middle and inferior frontal gyri, anterior insula, anterior cingulate cortex extending to supplementary motor area, thalamus, and precuneus. The task-induced deactivation regions were well overlapped with the DMN, including the PCC/PCu, mPFC, hippocampus, parahippocampal gyrus, superior temporal gyrus, and transverse temporal gyrus.

To elaborate on brain deactivation to the WM task, an ROI in the PCC/PCu was selected based on the main effect of the WM task at the significance level of $p < 0.01$ (corrected for multiple comparisons), resulting in a volume of 12528 mm³ (Fig. 2a, arrows). A post hoc analysis revealed that the PCC/PCu deactivation was stronger under condition 2b and 3b than under condition 1b, but did not differ between condition 2b and 3b (Fig. 2b). The PCC/PCu deactivation was significantly correlated

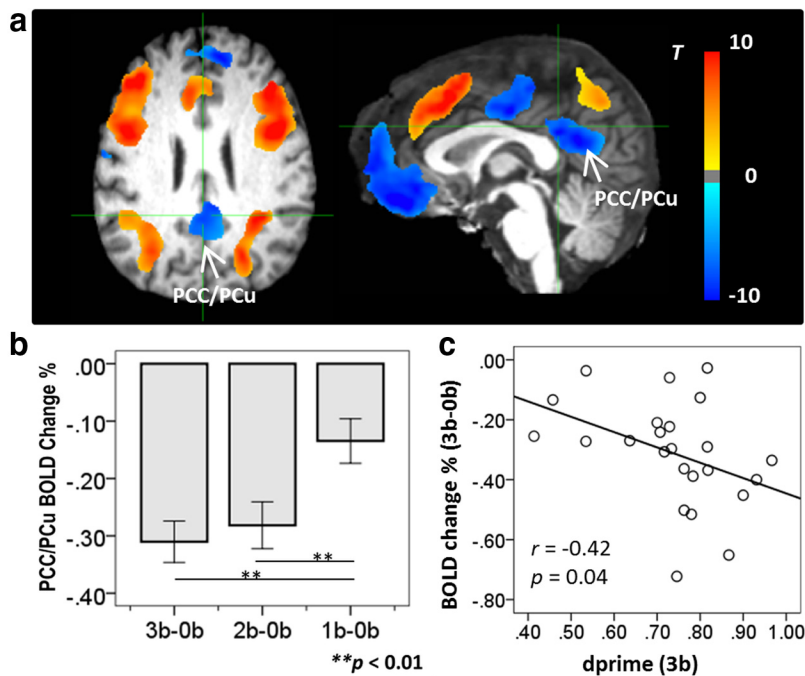


Figure 2. Brain activity during the working memory task. *a*, Brain areas showing main effect of the working memory task revealed by voxelwise ANOVA (corrected $p < 0.01$). To illustrate task-induced activation and deactivation, brain activities within these areas at the 3-back level are shown. *b*, Cognitive load modulated deactivation in the PCC/PCu region. *c*, The PCC/PCu deactivation was significantly correlated with 3-back working memory task performance.

with WM task performance as measured by dprime at condition 3b ($r = -0.42$, $p = 0.04$; Fig. 2*c*), but not at conditions 1b and 2b.

Glutamate and GABA levels modulate brain deactivation

Hierarchical regression showed that the PCC/PCu deactivation at low level of WM load could be predicted well by age (model 1). The prediction power, however, decreased when WM load increased. In contrast, after adding glutamate and GABA to the model (model 2), PCC/PCu deactivation could be predicted significantly at all levels of WM load (Fig. 3, Table 1). In addition, as revealed by coefficients of the regression models (Table 2), age demonstrated stable positive correlation with PCC/PCu deactivation at all cognitive loads when controlling for glutamate and GABA ($p < 0.002$). The contribution of GABA increased considerably at higher cognitive load conditions. Furthermore, a follow-up analysis showed that GABA concentration correlated with the change in PCC/PCu deactivation from lower (1b) to high (3b) cognitive load conditions ($r = -0.39$, one-tailed $p = 0.03$). Glutamate (5.44 ± 0.72 mM) and GABA (1.98 ± 0.22 mM) concentrations in the control region did not show associations with the PCC/PCu deactivation at any level of cognitive load in model 2 (coefficients significance, $p > 0.45$). In the PCC/PCu VOI, Glx significantly correlated with both glutamate ($r = 0.696$, $p = 0.0002$) and glutamine ($r = 0.595$, $p = 0.002$), but there was no correlation between glutamate and glutamine ($r = -0.16$, $p = 0.45$). When glutamine was used to replace glutamate in model 2, its regression coefficients were not significant (1b: $t = -1.084$, $p = 0.29$; 2b: $t = -1.18$, $p = 0.25$; 3b: $t = -0.26$, $p = 0.80$). When Glx was used to replace glutamate in model 2, its regression coefficients were not significant at 1b and 2b (1b: $t = 1.56$, $p = 0.13$; 2b: $t = 1.55$, $p = 0.14$) but was significant at 3b ($t = 2.62$, $p = 0.017$).

Regressions on the entire DMN BOLD signal change demonstrated that the models including glutamate and GABA signifi-

cantly explained more variations in the entire DMN BOLD signal change at all cognitive levels (1b: $p = 0.046$; 2b: $p = 0.04$; 3b: $p = 0.014$) compared with the models only including age and GM as predictors. The entire DMN deactivations were positively associated with glutamate (1b: $t = 2.48$, $p = 0.023$; 2b: $t = 2.10$, $p = 0.049$; 3b: $t = 2.06$, $p = 0.054$) and negatively with GABA (1b: $t = -1.66$, $p = 0.113$; 2b: $t = -2.27$, $p = 0.035$; 3b: $t = -3.00$, $p = 0.008$). All of the DMN BOLD signal changes were also positively associated with age at all cognitive levels ($p < 0.001$). Therefore, their association patterns were consistent with those in the PCC/PCu regression models (Fig. 3), with relatively smaller contributions of neurotransmitters but larger contribution of age.

Discussion

Task load modulation and functional relevance of the DMN

Consistent with previous studies (Esposito et al., 2006; Tomasi et al., 2006), we found significant modulation of cognitive load on deactivation in the PCC/PCu in present study. The deactivation of the DMN was interpreted as the suppression of ongoing brain activities related to internal thoughts (Raichle et al., 2001; Raichle and Snyder, 2007) when reallocating attentional resources from internal processes to goal-directed external stimuli (McKiernan et al., 2003). Behaviorally, task difficulty increased with the memory load, as reflected by reduced performance outcome at higher loads (Fig. 1*d*). Meanwhile, higher cognitive loads exerted stronger suppression of DMN (Fig. 2*b*). The DMN deactivation was found to be correlated with behavioral performance (Fig. 2*c,d*), suggesting a functional relevance to the DMN deactivation. The modulation of DMN deactivation by cognitive load may reflect the flexibility of dynamic neural resource configuration according to task demands.

Gender and age effects

We did not find an effect of gender on neurotransmitter concentrations in the present study, but previous reports on gender difference in GABA concentration were inconsistent (O'Gorman et al., 2011; Aufhaus et al., 2013). Because of this discrepancy, one may suspect that gender could confound the relationships between neurotransmitters and brain deactivation. To address this issue, we conducted another hierarchical regression adding gender as an independent variable. Our results indicated that gender did not contribute to the PCC/PCu deactivation significantly in any of the models ($p > 0.26$). Including gender also did not alter the relationships between neurotransmitters and PCC/PCu deactivation.

In the present study we found that age was negatively correlated with DMN activity, which is consistent with previous studies (Lustig et al., 2003; Grady et al., 2006; Sambataro et al., 2010; Spreng and Schacter, 2012). An interesting observation in the present study is that the bivariate correlation between age and the DMN deactivation only holds at low cognitive load (1b), not at high load (2b and 3b). However, their relationship becomes sta-

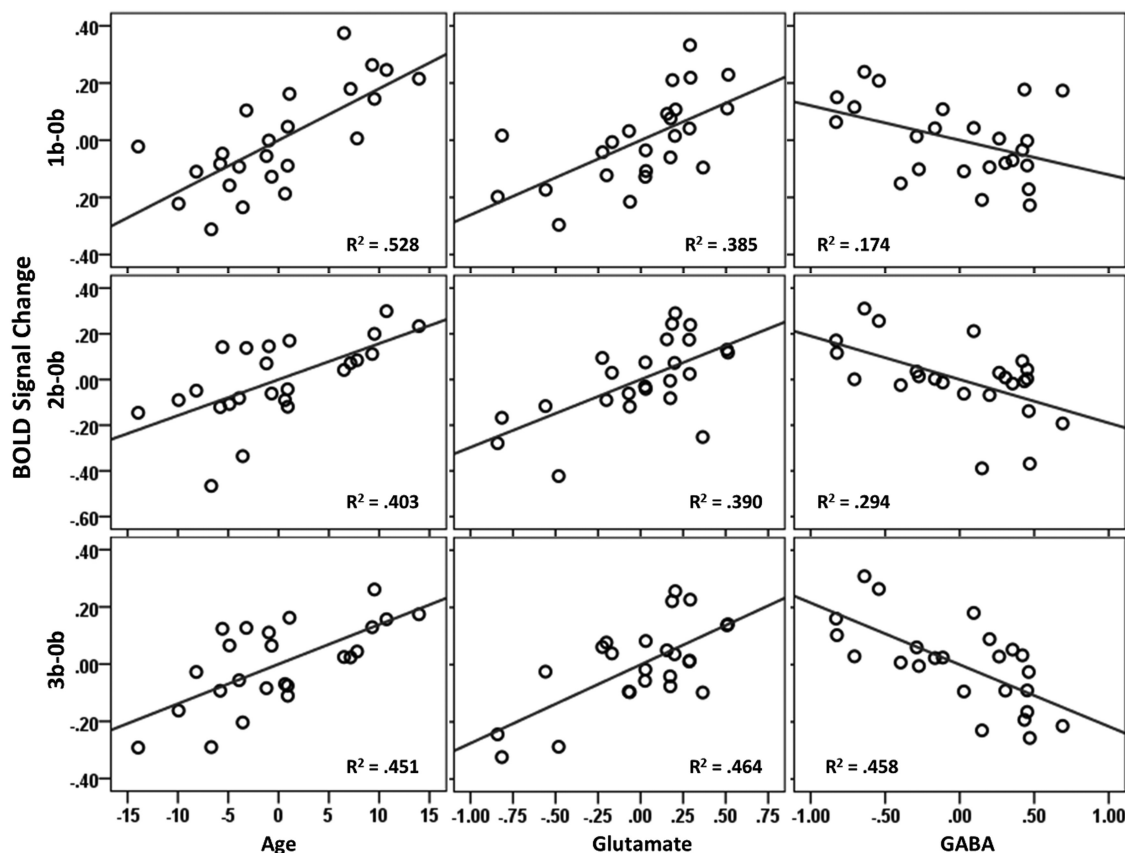


Figure 3. Partial regression plots. PCC/PCu deactivation can be predicted by age and regional glutamate and GABA concentrations assessed by MRS at resting state.

Table 1. Models to regress PCC/PCu BOLD signal on age, GM, glutamate, and GABA

Model	R ²	Adjusted R ²	ΔR ²	ΔF	p
1b					
1	0.297	0.230	0.297	4.428	0.025
2	0.585	0.498	0.289	6.611	0.007
2b					
1	0.132	0.049	0.132	1.593	0.227
2	0.530	0.431	0.398	8.055	0.003
3b					
1	0.095	0.009	0.095	1.107	0.349
2	0.617	0.536	0.521	12.922	0.0003

Model 1 predictors: (constant), age, GM; model 2 predictors: (constant), age, GM, glutamate, GABA; dependent variable: PCC/PCu BOLD signal change.

ble when controlling for glutamate and GABA concentrations. A plausible explanation is that glutamate and GABA may change with age and these changes may in turn result in changes in DMN activity. Conversely, the presence of the significant coefficients for age and neurotransmitters indicates their independent contributions to the variance of the task-induced deactivation. Ideally, age-related cognitive changes should be studied in an age range in which profound changes in cognition are expected. Whether the observed relationships in this study would hold in an aged population and how they link to age-related cognitive changes are interesting topics that warrant further investigation.

GABA/glutamate levels and neural activity

Our results are consistent with previous studies examining the effects of glutamate or GABA separately on BOLD signal change. The negative correlation between GABA concentration and DMN deactivation agrees with its profile as the major postsynap-

Table 2. Coefficients in regression models

Model	Beta (SE)	Beta'	t	p
1b				
1				
Age	0.013 (0.004)	0.574	2.844	0.010
GM	0.344 (0.857)	0.081	0.402	0.692
2				
Age	0.018 (0.004)	0.815	4.612	0.0002
GM	−0.918 (0.775)	−0.216	−1.185	0.251
Glutamate	0.261 (0.076)	0.640	3.446	0.003
GABA	−0.121 (0.060)	−0.321	−2.003	0.060
2b				
1				
Age	0.009 (0.005)	0.382	1.704	0.103
GM	0.237 (1.004)	0.053	0.236	0.816
2				
Age	0.016 (0.004)	0.674	3.583	0.002
GM	−1.262 (0.870)	−0.282	−1.451	0.163
Glutamate	0.297 (0.085)	0.690	3.489	0.002
GABA	−0.190 (0.068)	−0.480	−2.812	0.011
3b				
1				
Age	0.007 (0.005)	0.337	1.473	0.156
GM	0.735 (0.905)	0.186	0.812	0.426
2				
Age	0.014 (0.004)	0.670	3.947	0.001
GM	−0.702 (0.694)	−0.178	−1.012	0.324
Glutamate	0.275 (0.068)	0.724	4.053	0.0007
GABA	−0.216 (0.054)	−0.617	−4.004	0.0008

Dependent variable: PCC/PCu deactivation during WM task; model 1 predictors: (constant), age, GM; model 2 predictors: (constant), age, GM, glutamate, GABA.

Beta (SE), unstandardized coefficient (SE); and beta', standardized coefficient.

tic inhibitory neurotransmitter. The relationship between GABA and BOLD signal is highly accordant across different studies (Northoff et al., 2007; Muthukumaraswamy et al., 2009; Sumner et al., 2010). In addition to its association with the magnitude of BOLD signal, the GABA concentration was found to correlate with the latency and width of the stimulus-evoked HRF curve (Muthukumaraswamy et al., 2012), as well as electroencephalogram measures (Muthukumaraswamy et al., 2009; Rowland et al., 2013). In contrast to the suppression effect of GABA, the glutamate concentration has been found to be positively correlated with BOLD signal change. For example, when only controlling for age, regional glutamate concentration in perigenual anterior cingulate cortex (a part of DMN) was found to be positively correlated with task-induced deactivation (Enzi et al., 2012) and task-induced activation in supragenual anterior cingulate cortex (Duncan et al., 2011). Similarly, resting-state glutamate concentration in the dorsal anterior cingulate cortex (dACC) could predict the strength of the BOLD response to a task requiring cognitive control, not just in the dACC but also in other distinct brain regions including the retrosplenial cortex and inferior parietal lobule (both are considered as parts of DMN; Falkenberg et al., 2012). These results showed convincing evidence for the direct relevance between neurotransmitters and BOLD contrast. In the present study, we revealed significant coordinative effects of glutamate and GABA on task-induced BOLD signal change in PCC/PCu. We further demonstrated significant associations between PCC/PCu neurotransmitters and the entire DMN deactivation, suggesting that regional neurotransmitter profile in the hub of a network may significantly affect the activity of the whole network, possibly through functional connectivity (Kapogiannis et al., 2013).

The system-level coordinative effects of glutamate and GABA concentrations on the DMN deactivation may involve complex cellular processes. It might be reasonable to assume that high regional GABA concentrations could facilitate inhibition of local neural activities through GABAergic interneurons, resulting in stronger brain deactivation. Similarly, high regional glutamate concentrations could promote excitation of local glutamatergic neurons. In the resting state, glutamatergic and GABAergic activities in the DMN may reach equilibrium to facilitate endogenous processes. When turning from the resting to a task state, the DMN suppression might be achieved by enhancing GABAergic activities to regulate glutamatergic activities. Therefore, individuals with a higher GABA/glutamate ratio tend to suppress ongoing neural activities more efficiently. Furthermore, because the inhibition of glutamatergic neurons might also decrease the probability of excitation of their downstream neurons, the inhibitory associations with GABA would be enhanced in these individuals.

Implications of abnormal DMN deactivation and neurotransmitters in mental disease

The associations between neurotransmitters and the DMN deactivation found in the present study may have important implications for neuropsychiatric disease. The DMN is suggested to be a fundamental brain network underlying normal and abnormal brain functions (Buckner et al., 2008; Anticevic et al., 2012). In contrast to the DMN deactivation patterns seen in healthy subjects, insufficient DMN deactivation has been observed in several psychiatric disorders. These studies suggest that the DMN abnormalities observed in fMRI studies may be closely associated with neuropsychiatric disorders. Meanwhile, abnormal neurotransmitter function has been reported in disease populations, espe-

cially in schizophrenia (Marsman et al., 2013). Our results indicate that coordination of glutamate and GABA is associated with task-induced DMN deactivation. Abnormal DMN deactivation in neuropsychiatric disorders may be associated with an imbalance of glutamate and GABA neurotransmitters. Further assessment of the relationships among clinical observations, activity, and neurotransmitter function of the DMN in such patient populations may provide useful insights into these diseases.

Limitations

We observed associations of local glutamate and GABA concentrations at resting state with task-induced BOLD signal change in the same region. However, as a distributed system, activity of one brain region is influenced by many other regions. Specifically, release of neurotransmitters could depend on remote afferent projections, which cannot be determined in the present study. Consideration of both remote afferent projections and local neurotransmitters would produce better models to predict BOLD signal change.

Technically, measurements of GABA and glutamate are challenging. The MM coediting is an important issue for the GABA detection using editing sequences, and the degree of MM signal contamination varies with sequences and parameters (Henry et al., 2001; Terpstra et al., 2002; Near et al., 2011). Nevertheless, previous studies (Hofmann et al., 2001; Mader et al., 2002) suggested that the MM concentrations in cortical regions of healthy adults are very stable with respect to age and gender. Therefore, individual differences in the contaminated GABA levels may reflect primarily the differences in the GABA itself (Donahue et al., 2010). In addition, the degree to which glutamate and glutamine can be separated at 3T is arguable. In the present study, the CRLBs of glutamate and glutamine fitting from LCMoel were $5 \pm 1\%$ and $14 \pm 2\%$, respectively, suggesting that both are quantifiable. Another limitation of glutamate measurement with ^1H -MRS is its inability to distinguish signals between metabolic and neurotransmitter pools. However, the relationship between neuronal glucose oxidation and glutamate/glutamine cycling is suggested to be linear (de Graaf et al., 2004), which supports the assumption that the total glutamate level measured by ^1H -MRS could be a reasonable metric of glutamate involve in glutamatergic neurotransmission.

In the present study, fMRI and MRS data were collected separately. It would be interesting to assess the association between neurotransmitter levels and brain activity at the same functional states. In addition, the influence of the menstrual cycle on the cerebral GABA and glutamate levels could be region specific (Epperson et al., 2002; Batra et al., 2008; Harada et al., 2011). However, as far as we know, there have been no reports about GABA or glutamate level changes in PCC/PCu across the menstrual cycle. This is a factor that we did not control for in the present study.

Summary

In conclusion, the present study demonstrates significant association between neurotransmitters and the DMN deactivation probed by a WM task. The major excitatory neurotransmitter, glutamate, prevents BOLD signal from deactivation, whereas GABA, the major inhibitory neurotransmitter, exerts the opposite effects. These neurochemical characteristics of DMN deactivation may provide novel insights into the function of DMN in healthy individuals and its dysfunction in brain disorders.

Notes

Supplemental material for this article is available at <http://irp.drugabuse.gov/PDFs/supp/supHu08282013.pdf>. This supplemental material docu-

ment includes: (1) individual GABA spectra, (2) an estimation of GABA-macromolecule contamination and glutamate-glutamine separation, and (3) relationships between the entire DMN deactivation and neurotransmitters. This material has not been peer reviewed.

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