



REVIEW ARTICLE

A review of the effect of various ions on the properties and the clinical applications of novel bioactive glasses in medicine and dentistry



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Abstract Bioactive glass is a novel material that dissolves and forms a bond with bone when exposed to body fluids. Bioactive glasses are silicate-based, with calcium and phosphate in identical proportions to those of natural bone; therefore, they have high biocompatibility. Bioactive glasses have wide-ranging clinical applications, including the use as bone grafts, scaffolds, and coating materials for dental implants. This review will discuss the effects of ions on the various compositions of bioactive glasses, as well as the clinical applications of bioactive glasses in medicine and dentistry.

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1. Introduction

According to [Hench et al. \(1971\)](#), a material can be classified as bioactive if it evokes a specific biological response that results in bond formation between the material and a tissue (e.g., bone). Biomaterials were originally designed to be inert, and the discovery of bioactive glasses by Hench initiated an exciting new era in the field. In SiO_2 , CaO , Na_2O , and P_2O_5 systems, certain compositions were observed to resist removal and to form a strong bond with the bone after implantation ([Hench and Wilson, 1993](#)). These silicate-based bioactive glasses have a high degree of biocompatibility, with calcium and phosphorus in proportions identical to those of natural bone. Bioactive glasses have also been used to bind to tooth components ([Hench, 2006](#)).

The purpose of this review was to analyze the effect of ions in the properties of bioactive glasses and to summarize their major clinical applications in the field of medicine and dentistry reported in the literature. In preparing this review, all English-language articles published between 1971 (the first report of bioactive glass) and 2013 were accessed electronically using automated searches. The PubMed database and Google search engine were searched with keywords, including: bioactive glass, bioactive glass ions, clinical applications of bioactive glasses, and bioactive glasses in medicine and dentistry. We reviewed the abstracts of over 100 articles and short-listed 50 articles and scientific proceedings on the basis of their relevance to the review topic. Articles reporting similar findings were excluded. The final articles were printed and studied in detail.

2. Effects of ions on the composition of bioactive glasses

The first bioactive glass, BioglassTM, was discovered by Hench. The original formulation, commonly called 45S5, contained 45 wt.% SiO_2 , 24.5 wt.% Na_2O and CaO , and 6 wt.% P_2O_5 ([Kobayashi et al., 2010](#)). Most current research focuses on changing the structure of 45S5 by adding or removing ions to make the material more compatible for different clinical applications.

2.1. Effect of fluoride

The addition of fluoride can provide numerous advantages to bioactive glasses and ceramics ([Hench et al., 1988](#)). Fluoride prevents dental decay by inhibiting the demineralization of enamel and dentin, enhancing remineralization, and inhibiting bacterial enzymes ([Thuy et al., 2008](#)). Fluoride also forms fluorapatite (FAP) instead of carbonated hydroxyapatite, which is more acid-resistant. Thus, adding fluoride to bioactive glass can improve oral health ([Brauer et al., 2009](#)).

2.2. Effect of phosphate

Phosphate can be present in bioactive glasses as orthophosphate ([Elgayar et al., 2005](#)). When the bioactive glass is exposed to body fluids, a layer of hydroxycarbonate apatite is formed ([Wallace et al., 1999](#)). Hydroxycarbonate apatite layer significantly increases the biocompatibility of these bioactive glasses ([Olmo et al., 2003](#)). The resulting bioactive glass can be used to treat dentin hypersensitivity (DH) by occluding dentinal tubules ([Litkowski et al., 1997](#)). However, FAP is superior to hydroxycarbonate apatite in terms of acid resistance ([Lynch et al., 2012](#)). Increasing the P_2O_5 and cation contents in fluoride-containing glasses aids in maintaining the network connectivity and favors the formation of FAP, rather than fluorite, with apatite also being formed at low pH. These conditions (increasing P_2O_5 and cation content in fluoride containing glasses) are more favorable for clinical applications of dentistry and orthopedics ([Brauer et al., 2010](#)).

2.3. Effect of strontium

Strontium is a bone-seeking agent like calcium that is naturally found in the liver, physiological fluids, muscles, and bones ([Patrick et al., 1997](#)). Strontium can favorably impact bone cells. Strontium ranelate and strontium chloride have been used in the treatment of osteoporosis ([Dahl et al., 2001](#)). Strontium can be substituted for calcium in bioactive glass, resulting in better bone bonding and osteoblast stimulation, with anabolic and anti-catabolic properties ([Fredholm et al., 2012](#)). Strontium-substituted BioglassTM promotes osteoblast proliferation and decreases osteoclast activity in cell culture ([Gentleman et al., 2010](#)). Strontium in a silica-based dentifrice was observed to be clinically effective in treating DH ([Addy et al., 1987](#)).

2.4. Effect of zinc

Zinc can improve the ability of glass to bond with bone ([Aina et al., 2007](#)). Zinc is a fundamental ion that controls cell growth, differentiation, and development, but the biomechanical mechanisms involved in these processes are not entirely understood ([Brandao et al., 1995](#)). Zinc is essential for DNA replication and stimulates protein synthesis ([Tang et al., 2001](#)). Zinc deficiency slows skeletal growth and causes alterations in bone calcification ([Holloway et al., 1996](#)). Zinc can activate bone formation and inhibit bone resorption ([Yamaguchi and Yamaguchi, 1986](#)). Dentifrices with 2% zinc citrate have been used in the treatment of poor gingival health, as they have antiinflammatory and antimicrobial properties ([Williams et al., 1998](#)).

3. Clinical applications of bioactive glasses in medicine and dentistry

Bioactive glasses have a wide range of clinical applications in both medicine and dentistry (Melek et al., 2013). The first reported clinical application of bioactive glass was the treatment of conductive hearing loss for the reconstruction of the bony ossicular chain of the middle ear (Greenspan, 1999). Bioactive silicate glass has also been used for implant coatings, as a bone graft (Towler et al., 2002), in dentifrices (Tai et al., 2006), and as air-abrasive particles to remove carious enamel and dentin (Farooq et al., 2012). Goudouri et al. (2011) indicated that bioactive glass could be used as a dental material to improve the bonding of the restorative material to dentin.

3.1. Application as a bone graft

Bone grafts can impact osteogenesis, osteoconduction, and osteoinduction (Linde et al., 2008). Bioglass™ has been used clinically as a synthetic bone graft material for over 10 years under two different product names: Novabone™ for orthopedics (Ahmed, 2006) and Perioglass™ for maxillofacial surgery (Fetner et al., 1994). Bioglass™ was approved by the US Food and Drug Administration (FDA) in 2005 for osteostimulation (Hench, 1998). It functions as an osteoconductive scaffold and has an osteostimulatory effect (Boccaccini et al., 2010), which traditional calcium phosphate and calcium sulfate osteoconductive bioceramics do not have (Gerhardt and Boccaccini, 2010) (Table 1).

3.2. Application as a coating material for dental implants

Although hydroxyapatite can be sprayed on the surface of dental implants as a bioactive coating material, its use has unavoidable drawbacks (Eberhardt et al., 1992). Implant coatings require good adherence to the metal substrate.

Titanium implant surfaces are routinely coated with hydroxyapatite to produce this rough surface and improve osseointegration, but their adherence to the metal is not ideal (Whitehead et al., 1993). Consequently, researchers have studied components to improve physical compatibility with titanium (Pazo et al., 1998). Bioglass™ may be used as an alternate osteoprotective, abrasive surface material for implants (Koller et al., 2007). However, more research is needed for bioactive glasses to be used clinically as a coating material for dental implants.

3.3. Application as a disinfectant

Bioactive glasses can serve as topical endodontic disinfectants with no effects on dentin stability (Doyon et al., 2005). Bioactive glass can raise the pH of an aqueous environment to produce its antimicrobial effects (Allan et al., 2001). Bioglass™ can also mineralize, which may be advantageous in endodontics, but further research is required to support this idea. When implanted in areas of periodontal defects, Bioglass™ can inhibit bacterial colonization at the surgical site (Allan et al., 2002) by increasing the pH and calcium levels (Allan et al., 2001). Calcium hydroxide can be used as an intracanal dressing to form a hard apical barrier in young, traumatized teeth, but its alkaline nature can weaken the dentin structure by dissolving the acidic bonding agents in the organic dentin matrix (Andreasen et al., 2002). Calcium hydroxide has a better antimicrobial effect than bioactive glass (Zehnder et al., 2006).

3.4. Application in bone regeneration

Bioactive glass can promote bone regeneration, with osteostimulatory effects *in vitro* (Hench, 2013). Similarly, in primate models, bioactive glass filled bony defects by stimulating osteoproduction (Wilson et al., 1987). Felipe et al. (2009) reported that bioactive glass particles were able to treat periodontal

Table 1 Comparison of HA/TCP and bioactive glasses as bone graft substitutes (Valimaki and Aro, 2006).

	HA and HA/TCP	Bioactive glasses
Chemical composition	One or two chemical components (Hydroxyapatite, tricalcium phosphate, or both)	Several components at least four components Original; four-component system of SiO ₂ , Na ₂ O, CaO and P ₂ O ₅ Hench et al. (1971) (4). Modified system; Na ₂ O–K ₂ O–MgO–CaO–B ₂ O ₃ –P ₂ O ₅ –SiO ₂ Brink et al. (1997) (6)
Physical forms	Porous blocks or granules	Granules or sintered porous blocks, fibers and Woven structures
Basic mechanism	Serves as osteoconductive surface	Forms chemical bonding with ongrowing new Bone.
Molecular mechanism of action <i>in vivo</i>	Not defined	Osteopromotive Induce high local bone turnover
Regulation of bioactivity	Based only on HA/TCP ratio	Can be regulated by modifying the chemical composition
Resorption rate	TCP is resorbed fast (months) HA is slowly/very slowly resorbed	Resorption can be highly regulated [from weeks to years] by modifying the chemical composition
Mechanism of resorption	Involves chemical dissolution and Osteoclastic resorption	Chemical dissolution
Antimicrobial properties	Not reported	Inhibition of bacterial growth <i>in vitro</i> , dependent on the chemical composition

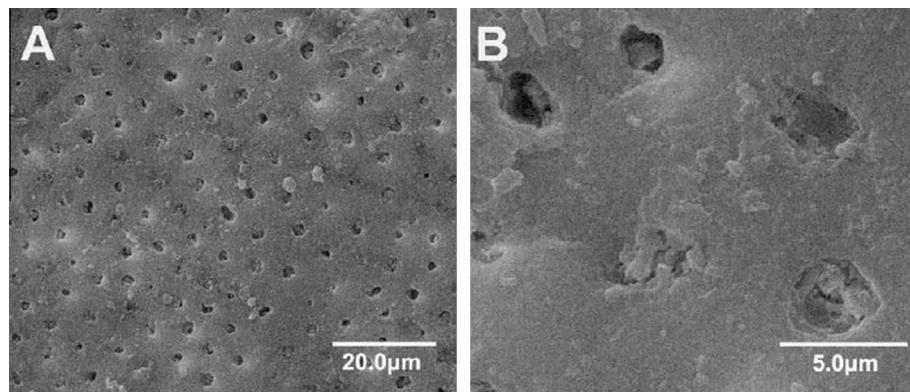


Figure 1 SEM-micrographs showing dentine surface brushed with Novamin™ (with 45S5) toothpaste for 2 min demonstrating tubule occlusion (Wang et al., 2010). (A) Bioactive glass particles on the dentine surfaces (at 1500 \times). (B) Bioactive glass particles embedded inside the dentinal tubules (at 7500 \times).

defects and triggered the development of mineralized bone in dogs.

3.5. Application in treating DH

The similarity between bone and dentin provides a rationale for testing bioactive glass in treating DH (Lynch et al., 2012). Bioglass™ 45S5, for example, can be used for remineralizing dentifrices for DH treatment (Farooq et al., 2013) (Fig. 1). However, there is no commercially available material for treating DH via permanent blockade of the dentinal tubules. Therefore, further research is needed to identify materials that form intimate bonds with the tooth structure and permanently block the tubules. Permanent bonding would reduce the incidence of dentinal tubule reopening resulting from oral fluid exposure.

4. Conclusion

Bioactive glasses have many applications in dentistry and medicine. Altering the composition of the bioactive glass by adding different ions changes its suitability for specific clinical applications. Considering the existing applications, there is a strong rationale for additional use in medicine and dentistry, and further research is needed to explore further applications.

Conflict of interest

The authors declare no conflict of interest.

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