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Doppler Echocardiography Inaccurately Estimates Right Ventricular Pressure in Children with Elevated Right Heart Pressure

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Abstract

Background—Doppler echocardiography (DE) is widely used as a surrogate for right heart catheterization (RHC), the gold standard, to assess and monitor elevated right heart pressure in children. However, its accuracy has not been prospectively validated in children. The objective of this study was to evaluate the accuracy of DE in predicting simultaneously measured RV pressure by RHC in pediatric patients, and to determine if the degree of RV hypertension affects the accuracy of DE in assessing right heart pressure.

Methods—Eighty children (age 0–17.9 years, median 5.5 years) with two-ventricle physiology and a wide range of right heart pressures underwent simultaneous DE and RHC. The pressure gradient between the right ventricle and right atrium was directly measured by RHC and simultaneously estimated by DE using tricuspid valve regurgitation. Patients were then grouped based on RHC measured right ventricular systolic pressure (RVSP): group 1 (n=43) with RVSP <1/2 systemic systolic blood pressure (SBP); group 2 (n=37) with RVSP = 1/2 SBP; group 3 (n=56) with RVSP <2/3 SBP; and group 4 (n=24) with RVSP = 2/3 SBP. Correlation and Bland-Altman analyses were performed on all groups. Accuracy was predefined as 95% limits of agreement within ±10mmHg.

Results—Despite a reasonable correlation between DE and RHC in all groups, there was poor agreement between techniques as RVSP/SBP increased. DE was inaccurate in 1/43 (2%) patients in group 1 versus 9/37 (24%) in group 2, and was inaccurate in 1/56 (2%) in group 3 versus 8/24 (33%) in group 4. Over- and underestimation occurred equally in all groups.

Conclusion—DE inaccurately estimates right ventricular pressure in children with elevated right heart pressure. It should not be relied upon as the sole method of assessing right heart hemodynamics in children with RV hypertension.

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Keywords

Right Ventricle; Doppler Echocardiography; Tricuspid Regurgitation; Children

Introduction

A wide variety of cardiopulmonary disease processes can lead to elevation of right heart pressure. In broad categories, elevation of right ventricular (RV) pressure can result from RV outflow tract obstruction, branch pulmonary artery obstruction, pulmonary vascular obstructive disease, pulmonary venous obstruction, or left ventricular inflow obstruction.¹ Right heart catheterization (RHC) remains the gold standard for evaluating right heart hemodynamics in these patients.^{2, 3} The risk of exposure to radiation and the invasive nature of RHC prompted investigators in the 1980s to introduce non-invasive methods of assessing right heart hemodynamics, specifically Doppler echocardiography (DE). These studies showed excellent correlation between DE estimated RV pressure using tricuspid valve regurgitation (TR) and direct RHC measured RV pressure.⁴⁻⁸ Due to its widespread availability and non-invasive nature, DE is now a widely used surrogate for RHC to determine and monitor right heart pressure in a wide variety of disease processes.⁹⁻¹⁶

Recently, the accuracy of DE in estimating right heart hemodynamics has come into question.^{17, 18} The initial studies comparing DE and RHC to assess right heart hemodynamics utilized correlation and regression analysis.⁴⁻⁷ This type of statistical analysis has its shortcomings as highlighted by Bland and Altman in their seminal paper in 1986. Bland and Altman argued that a high degree of correlation between two methods of measurement should not be interpreted as indicating accuracy and interchangeability of the two methods. Instead, they advocated using bias and precision statistics to compare different techniques of measuring the same physiologic variable.¹⁹ The Bland-Altman analysis is now the accepted statistical method of comparing two methods of measuring the same physiologic variable, superseding correlation and regression.²⁰ Recent studies in adults comparing DE and RHC using Bland-Altman analyses have suggested that DE is not as accurate as previously described for the assessment of right heart hemodynamics.^{17, 18, 21} A prospective, simultaneous study comparing DE and RHC using Bland-Altman analyses has not been performed in children.

In a prospective, simultaneous DE-RHC study in children, we sought to analyze the accuracy of DE in estimating right heart pressure. We further sought to determine if the degree of RV hypertension affects the accuracy of DE in assessing right heart pressure.

Methods

Patient Population

All children aged 0–17.9 years old who presented to the St. Louis Children's Hospital cardiac catheterization laboratory for a clinically indicated RHC between November 2011 and November 2012 were considered for enrollment. Inclusion criteria were two-ventricle physiology, adequate TR envelope on pre-catheterization echocardiogram, and sinus rhythm. Exclusion criteria were single ventricle physiology, presence of a subpulmonary morphologic left ventricle, and presence of a mechanical tricuspid valve. Informed, written parental consent was obtained for all subjects. Informed, written assent was obtained for all subjects >12 years of age. The study was approved by the Institutional Review Board for human studies at Washington University School of Medicine.

Catheterization Data

All patients underwent simultaneous measurement of the peak RV to right atrium (RA) pressure gradient (ΔP) by RHC and by DE. All data collection was done with the patient in the supine position and under the usual sterile conditions of the catheterization laboratory. RV and RA pressure tracings were recorded using a standard fluid-filled, end-hole catheter in pullback fashion. RV and RA pressure tracings were recorded simultaneously to performance of DE. The RHC measured ΔP (ΔP_C) was calculated by subtracting the RA V-wave pressure from the peak RV systolic pressure (RVSP) at end-expiration. Cardiac output was calculated using the Fick method²² and indexed to body surface area. Simultaneous systemic blood pressure was obtained by arterial catheter in patients where arterial access was clinically indicated and by upper extremity non-invasive cuff measurement in those where arterial access was not clinically indicated. Interpretation of RHC data was done by a single, experienced interventional cardiologist (JJM) to exclude interobserver variability. The interventional cardiologist was blinded to the patients' diagnoses and DE data.

Echocardiography Data

Two-dimensional and color-DE was performed using commercially available ultrasound equipment (Vivid 9, GE Medical Systems, Milwaukee, Wisconsin). With the patient in the supine position, continuous-wave Doppler recordings of the maximal TR jet velocity (V) were obtained in standard apical or parasternal windows (whichever produced the highest velocity signal). The Doppler beam was kept in parallel alignment with the direction of the TR jet as visualized by color Doppler. The majority (80%) of echocardiographic studies were performed by a single cardiac sonographer. The remainder of the studies was performed by two additional cardiac sonographers. No saline or contrast injection was used to enhance weak signals. Patients were excluded from the study if there was no measurable TR by color Doppler at the time of data acquisition. DE estimated ΔP (ΔP_E) was calculated using the modified Bernoulli equation, $\Delta P_E = 4V^2$. An average of three consecutive cardiac cycles was used to account for respiratory variation. Interpretation of DE data was done by a single, experienced echocardiographer (GKS) to exclude interobserver variability. The echocardiographer was blinded to the patients' diagnoses and RHC data.

Assessment of TR envelope quality

To minimize the effect of TR spectral envelope quality on the accuracy of DE, the data was analyzed using only patients with optimal TR envelopes. A TR envelope was deemed "optimal" by the interpreting cardiologist (GKS) when the spectral Doppler envelope edge was clearly identifiable in at least the first 3/4 of systole. Optimal envelopes had a clear, rounded edge clearly demonstrating the peak of the TR velocity. The remainders were deemed "suboptimal" and were not included in data analysis. Examples of TR envelope quality are shown in Figure 1. An independent assessment of TR envelope quality was also done in 20 randomly selected patients by a separate, blinded observer (GKG) and interobserver reliability was assessed using Cohen's kappa method.

Stratification of patients based on RV pressure

Patients were categorized based on the ratio between RHC measured RVSP and simultaneously measured systemic systolic blood pressure (SBP). In patients with left heart obstruction, a simultaneous catheter measured left ventricular systolic pressure was used as the SBP. Two clinically relevant thresholds were used to define RV hypertension and subsequently categorize patients: (1) $RVSP \geq 1/2 SBP$ and (2) $RVSP \geq 2/3 SBP$.^{1, 23} Group 1 included patients with $RVSP < 1/2 SBP$ and group 2 included patients with $RVSP \geq 1/2 SBP$. Group 3 included patients with $RVSP < 2/3 SBP$ and group 4 included patients with $RVSP \geq 2/3 SBP$.

Statistical Analysis

Values for descriptive statistics are reported as mean \pm SD for normally distributed data and median (interquartile range) for non-normally distributed data. Correlation coefficients between RHC and DE-derived pressures were calculated using the Pearson correlation method and the relationship of the methods was assessed using linear regression. Agreement between methods was assessed using Bland-Altman analysis.¹⁹ Accuracy of DE measurements was predefined as 95% limits of agreement within ± 10 mmHg. Fisher's exact test was used to compare categorical data between groups. Receiver operating characteristic (ROC) analysis was used to assess the associations between high RVSP (the reference standard) and ΔP_E . The previously used clinically relevant thresholds were used to define RV hypertension: (1) RVSP $\geq 1/2$ SBP and (2) RVSP $\geq 2/3$ SBP. Binomial exact confidence intervals were calculated for the area under the curve (AUC). The Youden index was used to determine on the ROC curve the point maximizing the difference between the true positive ratio and the false positive ratio. Bootstrapped (1000 replications) confidence intervals were calculated for this point (criterion value). Based upon the criterion value, sensitivity, specificity, positive predictive value, negative predictive value, and their 95% confidence intervals were calculated. For the calculation of positive and negative predictive values, the ratio of cases in the positive and negative groups was used to represent disease prevalence. P-values <0.05 were considered statistically significant. Statistical analyses were performed with SPSS version 19 (SPSS Incorporated, Chicago, IL), JMP Statistical Software Release 10.0.0 (SAS Institute, Inc., Cary, NC), and MedCalc Statistics for Biomedical Research version 12.3.0.0 (MedCalc Software, Mariakerke, Belgium).

Results

Patient Characteristics

A total of 395 patients aged 0–17.9 years underwent medically indicated RHC during the study period. Forty patients were excluded due to single ventricle physiology, 2 patients were excluded with mechanical tricuspid valve and 2 patients were excluded due to subpulmonary morphologic left ventricle. Of the remaining 351 patients, 153 had measurable TR on pre-catheterization echocardiogram and were deemed eligible for enrollment. Ten patients declined to participate and 19 patients were unable to be consented in time to participate. A total of 124 patients with a wide variety of cardiopulmonary disease processes were consented for the study. DE images were unable to be acquired in 8 patients due to hemodynamic instability at the time of RHC and in 12 patients due to logistic difficulties. A total of 104 patients underwent simultaneous RHC and DE. Four patients had no detectable TR at the time of RHC. Twenty patients were deemed to have suboptimal TR envelopes and were excluded. A total of 80 patients had simultaneous RHC and DE data obtained and analyzed. The median age was 5.5 years (1.6–10.4 years). Patient demographic data are summarized in Table 1. The RHC measured RVSP ranged from 17 to 89mmHg and RA V-wave pressure ranged from 4 to 20mmHg. The DE measured maximal TR jet velocity ranged from 1.7 to 5m/s. The ΔP_C ranged from 6 to 81mmHg and the ΔP_E ranged from 11 to 100mmHg. Baseline hemodynamic data are summarized in Table 2.

Assessment of TR envelope quality

Twenty patients were deemed to have suboptimal TR envelopes (defined as less than 3/4 of systole filled) and were excluded from data analysis. Excellent interobserver reliability was seen in the determination of TR envelope quality ($\kappa=0.83$, $p<0.001$). Examples of TR envelope quality are shown in Figure 1.

Stratification of patients based on RV pressure

A total of 80 patients were categorized based on the RVSP/SBP ratio. Group 1 included 43 patients with RVSP <1/2 SBP, group 2 included 37 patients with RVSP = 1/2 SBP, group 3 included 56 patients with RVSP <2/3 SBP, and group 4 included 24 patients with RVSP = 2/3 SBP.

Accuracy of DE in estimating RV pressure

Correlation between ΔP_C and ΔP_E was reasonable in all groups (group 1: R=0.8; group 2: R=0.81, group 3: R=0.95; group 4: R=0.75, $p<0.001$) (Figure 2). Agreement between the two methods was good in group 1 (bias 3.07mmHg, 95% limits of agreement +9.66 to -3.52mmHg), but poor in group 2 (bias 1.49mmHg, 95% limits of agreement +22.43 to -19.45mmHg), and good in group 3 (bias 2.5mmHg, 95% limits of agreement +10.18 to -4.5mmHg) but poor in group 4 (bias 1.16mmHg, 95% limits of agreement +26.41 to -24.09mmHg) (Figure 3).

With accuracy predefined as 95% limits of agreement ± 10 mmHg, DE was inaccurate in 1/43 (2%) patients in group 1 versus 9/37 (24%) patients in group 2 and inaccurate in 1/56 (2%) patients in group 3 versus 8/24 (33%) patients in group 4. An example of the inaccuracy of DE is shown in Figure 4. Over and under-estimation occurred equally in all groups.

Clinical implications

To determine the clinical relevance of our findings, we calculated a DE derived RVSP/SBP ratio and compared our findings with the true RHC determined RVSP/SBP ratio using the same two clinical relevant cutoffs used previously. The DE derived RVSP ($RVSP_E$) was calculated using $\Delta P_E + RHC$ measured RA V-wave pressure. In the $RVSP_E = 1/2SBP$ group, $RVSP_E/SBP$ ratio misclassified 14/80 patients (18%). Eight were underclassified and 6 were overclassified. In the $RVSP_E = 2/3SBP$ group, the $RVSP_E/SBP$ ratio misclassified 16/80 patients (20%). Eight were underclassified and 8 were overclassified.

Sensitivity, specificity, and predictive value of DE

ROC analysis was used to assess the associations between high RVSP (the reference standard) and ΔP_E . Two clinically relevant thresholds were used to define RV hypertension: (1) $RVSP = 1/2SBP$ and (2) $RVSP = 2/3 SBP$. Using $RVSP = 1/2SBP$ as the threshold, there was an AUC of 0.93 (95% CI 0.85–0.97, $p<0.001$). A ΔP_E of >28mmHg was 82% sensitive and 89% specific in detecting an $RVSP = 1/2SBP$, with an 86% positive predictive value and 86% negative predictive value. Using $RVSP = 2/3SBP$ as the threshold, there was an AUC of 0.91 (95% CI 0.84–0.96, $p<0.001$). A ΔP_E of >35.5mmHg was 81% sensitive and 88% specific in detecting an $RVSP = 2/3 SBP$, with an 81% positive predictive value and 88% negative predictive value (Figure 5).

Discussion

In this study we evaluated the accuracy of DE in predicting simultaneously measured RV pressure by RHC in pediatric patients. Our study population had a wide variety of cardiopulmonary disease processes leading to a wide range of RV pressures. We have shown for the first time that the degree of RV hypertension affects the accuracy of DE in estimating right heart pressure.

Using predefined accuracy limits of 95% limits of agreement within bias ± 10 mmHg, DE was inaccurate in estimating RHC measured RVSP in 24% of children with $RVSP = 1/2$ systemic. DE became more frequently inaccurate with increasing RV pressure and was

inaccurate in 33% of children with $RVSP \geq 2/3$ systemic. Furthermore, the direction of inaccuracy was unpredictable, with both over- and underestimation occurring equally. From a clinical and diagnostic perspective, our DE derived RVSP misclassified patients approximately 20% of the time, depending on which RVSP/SBP ratio cutoff was used. Since our method of generating a DE derived RVSP was done by adding an actual RHC measured RA pressure to the DE measured RV-RA pressure gradient, our incidence of misclassification is likely underestimated. In actual clinical practice, a true RA pressure is unavailable and an estimated RA pressure is typically used. This would more than likely lead to increased error in the DE estimated RVSP and a higher incidence of misclassification. This was seen in the study by Fisher et al, where pulmonary hypertension severity was misclassified in almost 50% of patients when using an estimated RA pressure to generate a DE estimated pulmonary artery systolic pressure (PASP).¹⁸

The clinical implications of these findings are significant, as DE is widely used to screen for and manage many different causes of RV hypertension. RV hypertension has previously been defined as $RVSP > 1/2$ systemic levels and it is a common clinical practice to refer children for invasive cardiac catheterization once DE shows an estimated RV pressure of $> 1/2$ to $2/3$ systemic levels.¹ An American Heart Association class II indication exists for RHC with balloon angioplasty in children with pulmonary artery obstruction and $RVSP > 2/3$ systemic pressure.²³ Both American College of Cardiology/American Heart Association and American Society of Echocardiography guidelines for clinical use of echocardiography^{24, 25} recommend the use of serial echocardiography in pediatric patients to monitor hemodynamic adaptation to surgical or transcatheter repair or palliation in order to identify recurrence of abnormalities. Such longitudinal monitoring allows for proactive surgical, transcatheter, or medical intervention. Our study questions the accuracy and predictive value of DE as a solo monitoring tool in these situations.

Our results extend the findings of recent studies demonstrating the overall inaccuracy of DE in estimating right heart pressures in adult patients with pulmonary hypertension^{17, 18, 21} to a strictly pediatric population with a broad range of diagnoses. Importantly, the aforementioned studies did not stratify patients based on RV pressure, which we have done. Skinner et al simultaneously compared DE and RHC for assessment of right heart hemodynamics in 26 infants and found that in patients with RV systolic pressure > 60 mmHg, the accuracy of DE diminished.²⁶ Our study confirms this finding in a larger, more robust pediatric patient population. Furthermore, previous studies highlighting the inaccuracy of DE have measured PASP.^{17, 18} In order to report an estimated PASP by DE, RA pressure was estimated non-invasively in these studies. While echocardiographic methods of estimating RA pressure have previously been validated in adults²⁷, these methods have not been well studied in children and have more recently come into question.²⁸ Rich et al found that the estimation of RA pressure was an important source of error in the DE estimated PASP and may have contributed to the inaccuracy of DE that they reported.¹⁷ We avoided this important source of error by comparing the RV to RA pressure drop by both DE and RHC.

Several explanations exist as to why a discrepancy between DE and RHC measurements may be seen. First, using the Bernoulli equation to estimate pressure gradient between two chambers assumes a perfect, parallel alignment between the ultrasound beam and the maximal regurgitant jet.²⁹ Small deviations in angle ($< 20^\circ$) may produce mild errors ($< 10\%$) in velocity measurements, which may be acceptable in low velocity flows. However, when the Doppler is used to obtain pressure gradients, even a small error in velocity can produce significant discrepancy in the gradient due to the quadratic relationship between velocity and pressure gradient.³⁰ In our study, the TR jet was visualized by colorflow mapping in order to ensure that the angle between the Doppler beam and TR jet was $< 20^\circ$ for all patients. The

TR jet is a three dimensional phenomenon and using two dimensional echocardiography to visualize the TR jet assumes that the maximal TR jet is able to be captured in the two dimensional imaging plane.³⁰ It is possible that the actual maximal TR jet is outside the imaging plane when imaging in only two dimensions. This limitation could account for the inaccuracy of using 2D echocardiography to estimate right heart pressures. Furthermore, the modified Bernoulli equation assumes negligible viscous and inertial forces, as well as complete transformation of potential energy (pressure in the RV) to kinetic energy (the TR jet). Giardini et al demonstrated in an in vitro flow model of atrioventricular valve regurgitation that conditions commonly seen in clinical practice can lead to incomplete transformation of potential energy to kinetic energy. They showed that an eccentric TR jet may interact with the RA wall (Coanda effect) causing viscous losses. As well, increasing hematocrit, frequently encountered in patients with cyanotic congenital heart disease, can lead to viscous losses. Such viscous losses are unaccounted for in the modified Bernoulli equation, and can lead to underestimation of RV pressure. Finally, they suggested that in children, the absolute RA size is small and inertial forces unaccounted for by the modified Bernoulli equation can cause pressure recovery in the receiving chamber, leading to overestimation of RV pressure by DE.³¹ All of these factors can lead to both over and underestimation, as was seen in our study population.

The most plausible explanation for diminished accuracy of DE with increasing RV pressures is inherent to the Bernoulli formula itself. While performing DE, each increment of error in velocity measurement is squared and multiplied by four when applying the Bernoulli equation. Thus, it stands to reason that as the TR jet velocity increases, the calculated ΔP_E can differ from the ΔP_C by a larger increment. Skinner et al suggested it might be better to express TR in terms of velocity (m/s) rather than pressure drop (mmHg) to minimize this source of error.²⁶ However, pressure drop expressed in mmHg remains the accepted parameter in clinical practice today. The lack of agreement between DE and RHC seen in our study is likely a result of a combination of the inherent limitations of the simplified Bernoulli equation as well as limitations in study design, which are addressed below. Despite its limitations, echocardiography remains the most widely available and least invasive method for assessing right heart hemodynamics and function in children with RV hypertension. Our study highlights the importance of combining TR estimated RV pressure with other echocardiographic parameters of RV pressure evaluation when making clinical decisions regarding diagnosis and management of patients with RV hypertension. Such parameters may include RA enlargement, RV dilation/hypertrophy, interventricular septal configuration/motion, main pulmonary artery dilation, and pulmonary artery acceleration time.^{1, 32, 33} In the absence of other supporting evidence of RV pressure overload, the TR jet alone should be used with caution.

Limitations

Our study population was heterogeneous and subgroups of patients based on diagnoses and level of right heart obstruction were small. This precluded adequate subgroup analyses to test whether the level of right heart obstruction affects accuracy of DE. Jarcut et al recently showed that at similar levels RV pressure overload, patients with pulmonary valve stenosis had less RV dilation and better RV performance compared to those with pulmonary arterial hypertension.³⁴ This suggests that perhaps the nature of right heart obstruction affects right heart hemodynamics and function, which could affect the accuracy of DE in predicting RV pressures. Our study was also performed at one point in time, and therefore does not address accuracy of serial DE measures over time or test-retest variability.

Limitations of Study Design

Acquisition of DE data was limited by technical difficulties encountered during simultaneous DE and RHC. All DE data was obtained with patients in the supine position. Inability to change patient position may have affected acoustic window quality, particularly in apical views in older patients. Additionally, parasternal windows were difficult to obtain in some patients due to the position of sterile drapes, which impeded optimal probe position. These limitations may have led to inability to capture the highest velocity TR jet, contributing to out of plane error. DE was performed by three different cardiac sonographers, which raises the possibility of inter-observer variability in image acquisition. However, 80% of the studies were done by a single cardiac sonographer, minimizing the impact of this source of error. Finally, for the calculation of positive and negative predictive values, the ratio of cases in the positive and negative groups of our study population was used to represent disease prevalence. This does not represent true RV hypertension disease prevalence, as our study population consists of only children referred for RHC. Therefore, the prevalence of RV hypertension in our study population is almost certainly higher than in the general population. The true PPV of DE for detecting RV hypertension in the general population is likely lower and the true NPV likely higher than what we report.

Conclusions

This study is the first to show that DE estimates of RV pressure in children are not completely accurate, specifically in children with elevated right heart pressure. Significantly, both over and underestimation occur. DE may not be interchangeable with RHC in determining right heart pressure in children with RV hypertension. DE should not be relied upon as the sole method of diagnosing and managing children with elevated right heart pressure. Continued development of reliable, non-invasive techniques to assess right heart hemodynamics in children is warranted.

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Abbreviations

DE	Doppler echocardiography
RHC	right heart catheterization
RVSP	catheterization measured right ventricular systolic pressure
SBP	systemic systolic blood pressure
RA	right atrium
RV	right ventricle
ΔP_c	catheterization measured right ventricle to right atrium pressure gradient
ΔP_E	echocardiography estimated right ventricle to right atrium pressure gradient
TR	tricuspid regurgitation
ROC	receiver operating curve
PASP	pulmonary artery systolic pressure

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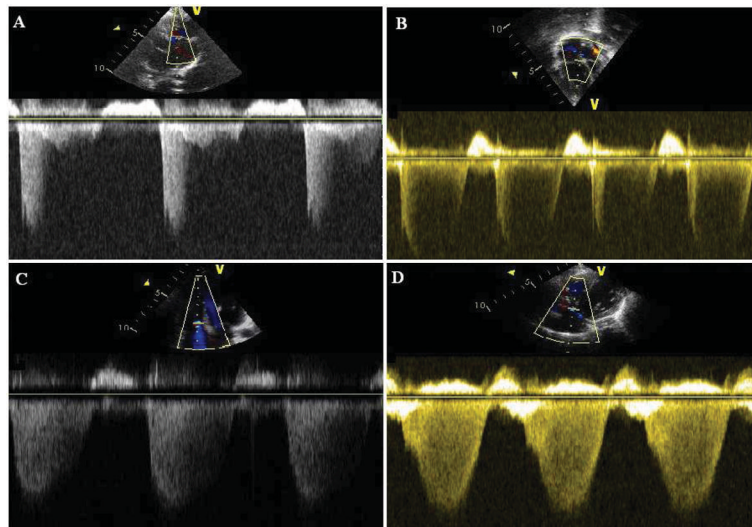


Figure 1. Tricuspid valve regurgitation envelope quality

TR envelope was deemed “optimal” if the spectral envelope was filled in at least the initial 3/4 of systole with a sharp, rounded edge clearly demonstrating the peak of the TR velocity. (A) 1/2 filled (patient excluded). (B) 2/3 filled (patient excluded). (C) 3/4 filled (patient included). (D) Full (patient included).

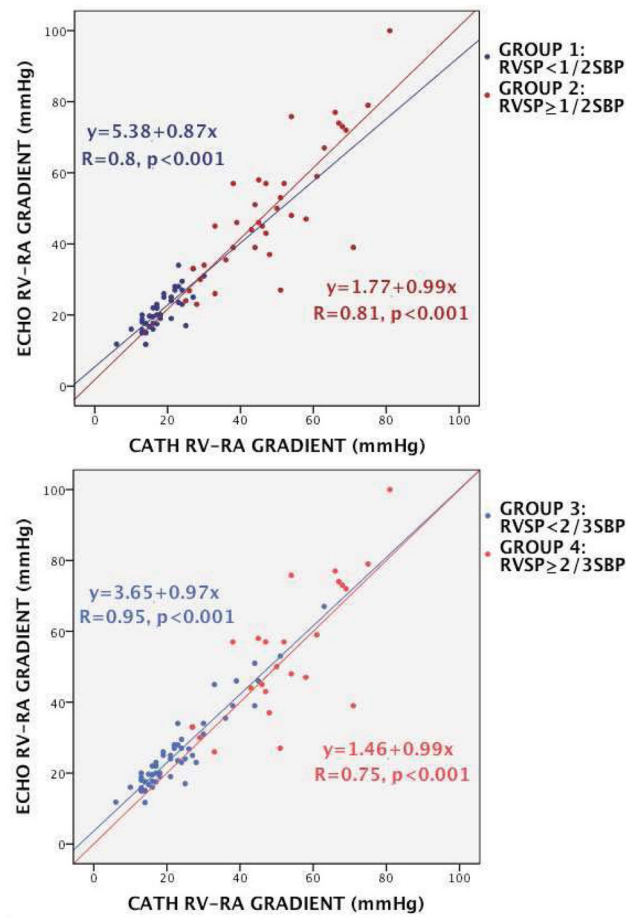


Figure 2. Correlation between DE and RHC derived RV-RA gradient

Regression plots showing similar correlation between ΔP_E and ΔP_C in all groups. The upper plot shows correlation between group 1 and 2 and the bottom plot shows correlation between group 3 and 4.

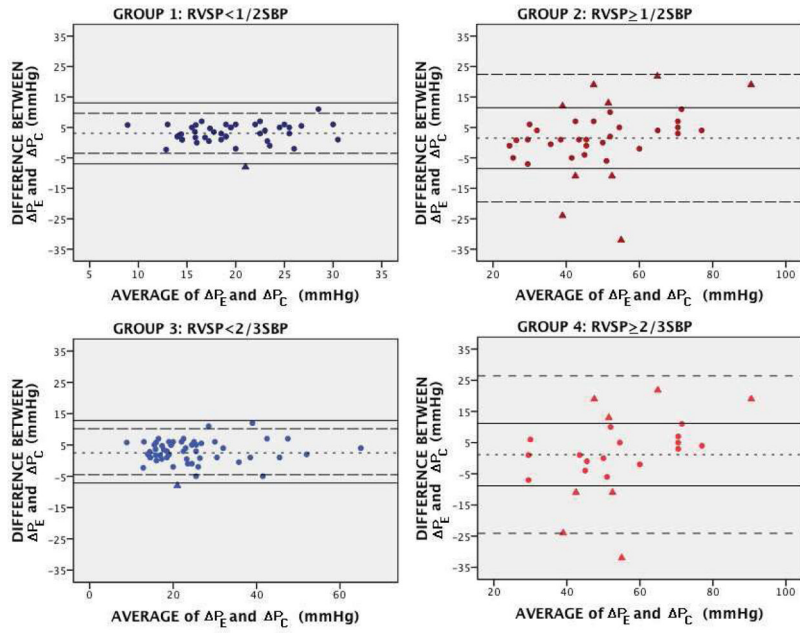


Figure 3. Bland-Altman analysis showing lack of agreement in groups with high RV pressure
Bland-Altman plots showing mean bias (dotted line), 95% limits of agreement (dashed lines), and predefined accuracy limits of bias ± 10 mmHg (solid lines). In groups with elevated RV pressure (2 and 4), the 95% limits of agreement are wide and many patients fall outside the predefined accuracy limits (triangles represent inaccurate measurements). Both over- and underestimation are seen equally.

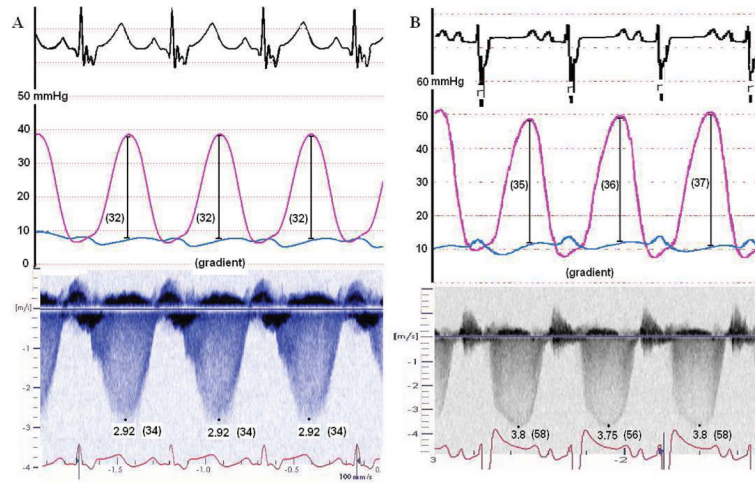


Figure 4. Inaccuracy occurs despite optimal TR envelope quality

DE can be both accurate and inaccurate in patients with full TR envelopes. This is shown in these simultaneous DE and RHC pressure recordings. (A) Patient with accurate DE predicted RV-RA gradient and full TR envelope and (B) patient with inaccurate DE predicted RV-RA gradient and full TR envelope.

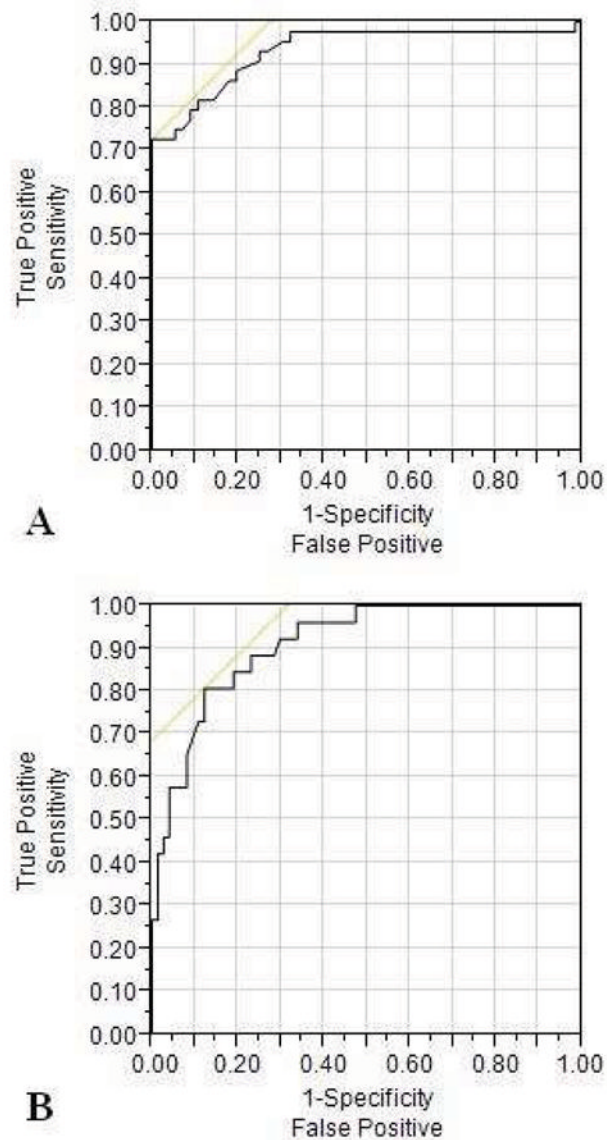


Figure 5. Receiver Operating Characteristic (ROC) curves

Receiver operative curves (ROC) showing the ability of ΔP_E to predict RV hypertension using two thresholds: (A) $RVSP \leq 1/2 SBP$, AUC 0.93 (95% CI 0.85–0.97, $p < 0.001$) and (B) $RVSP \leq 2/3 SBP$, AUC 0.91 (95% CI 0.84–0.96, $p < 0.001$). The yellow line is drawn at a 45 degree angle tangent to the ROC curve. This marks the point (criterion value) at which false negatives and false positives have similar costs.

Table 1

Patient Demographics

	All Patients N=80	Group 1 N=43	Group 2 N=37	Group 3 N=56	Group 4 N=24
Age, years	5.5 (1.57–10.37)	6.8 (3.3–13.6)	4.9 (0.9–9.2)	6.2 (2.5–12.3)	3 (0.7–8.1)
Male, n (%)	48	51	43	46	50
Caucasian, n (%)	75	79	70	75	75
Weight, kg	16.8 (9–32.3)	21 (14.5–45.8)	12.7 (7.2–23.6)	20.2 (12.7–42.8)	10.8 (6.9–23.2)
BSA, m ²	0.7 (0.42–1.12)	0.85 (0.6–1.46)	0.53 (0.36–0.93)	0.81 (0.53–1.3)	0.47 (0.34–0.92)
Hemoglobin (g/dL)	11.2 ± 1.6	11.3 ± 1.3	11.1 ± 1.9	11.3 ± 1.3	11.1 ± 2.2
Diagnoses, n					
OHT	22	19	3	22	0
ASD	6	5	1	6	0
RVOTO/PS	19	3	16	7	12
branch PS	10	2	8	5	5
PAH	5	1	4	1	4
PVS	3	1	2	1	2
LHO	6	4	2	6	0
other	9	8	1	8	1
Reason for RHC, n					
diagnostic	5	1	4	1	4
RV biopsy	22	19	3	22	0
ASD device balloon/stent	6	5	1	6	0
	47	18	29	27	20

Values expressed as mean ± SD or median (interquartile range); ASD – atrial septal defect; BSA – body surface area; LHO – left heart obstruction; PAH – pulmonary arterial hypertension; PS – pulmonary stenosis; PVS – pulmonary vein stenosis; RVOTO – RV outflow tract obstruction; OHT – orthotopic heart transplant; other – 2 complete atrioventricular canal, 2 dilated cardiomyopathy, 2 Kawasaki disease, 2 patent ductus arteriosus, 1 Scimitar syndrome

Table 2

Baseline Hemodynamic Data

	All Patients	Group 1	Group 2	Group 3	Group 4
SBP	80.2 ± 11.9	84.5 ± 12.1	75.1 ± 9.7	83.6 ± 11.7	72.1 ± 8.2
DBP	49.8 ± 10	53.4 ± 12.1	45.5 ± 8	52.4 ± 9.8	43.7 ± 7.7
MAP	61.9 ± 10.4	64.5 ± 10.2	58.8 ± 8.7	64.2 ± 10.7	56.3 ± 7.2
CI, L/min/m ²	3.8 ± 1.1	4.1 ± 1.2	3.4 ± 0.9	4 ± 1.2	3.3 ± 0.8
HR, bpm	105 ± 25	102 ± 23	109 (90–125)	103 (83–115)	111 ± 29
RVSP	35 (27–55)	28 ± 5.83	57 (46–70)	30 (25–38)	66 (54–77)
RVEDP	9.9 ± 3.1	8.9 ± 3.3	11 ± 2.4	9.3 ± 3	10.5 (10–12)
Mean RA pressure	8.9 ± 3.2	8.3 ± 3.3	9 (7–11)	8.4 ± 3.1	9.5 (8–11)
RA A-wave	10.3 ± 3.3	9.5 ± 3.6	11 (9–12)	9.5 (7–11)	11 (10–13)
RA V-wave	10.5 ± 3.4	9.9 ± 3.5	10 (9–13)	10 (8–12)	11 (9–14)
RVSP/SBP	0.45 (0.34–0.7)	0.34 ± 0.08	0.7 (0.6–1)	0.36 (0.3–0.49)	0.9 (0.7–1)
ΔP _C	25 (17–46)	17 (14–22)	47 (37–60)	20 (15–27)	51.5 (45–67)
ΔP _E	27 (20–45)	20 (17–25)	46 (36–59)	23 (18–29)	53.5 (40–73)

Values expressed as mean ± SD or median (interquartile range); all pressures expressed in mmHg; bpm – beats per minute, CI – cardiac index, DBP – diastolic blood pressure, HR – heart rate, MAP – mean arterial pressure, RA – right atrium, RVEDP – RV end diastolic pressure, SBP – systolic blood pressure