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Overlapping structural and functional brain changes in patients with long-term exposure to fibromyalgia

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Abstract

Objective—There is vast evidence for brain aberrations in patients with fibromyalgia (FM) and it is possible that central plasticity is critical for the transition from acute to chronic pain. However, the relationship between brain structure and function is poorly investigated.

Methods—The present study, including 26 FM patients and 13 age- and gender-matched healthy controls, investigated the differences between patients and controls regarding functional connectivity during intermittent pressure pain and measures of brain structure. Magnetic resonance imaging (MRI) was used to obtain high-resolution anatomical images and functional MRI scans for measures of pain-evoked brain activity.

Results—FM patients displayed a distinct overlap between decreased cortical thickness, brain volumes and measures of functional regional coherence in the rostral anterior cingulate cortex. The morphometric changes were more pronounced with longer exposure to FM pain. In addition,

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we found associations between structural and functional changes in the mesolimbic areas of the brain and comorbid depressive symptoms in FM patients.

Conclusion—The combined integration of structural and functional measures allowed for a unique characterization of the impact of FM pain on the brain. Our data may lead to the identification of early structural and functional brain alterations in response to pain, which could be used to develop markers to predict the development of FM and other pain disorders.

Keywords

Magnetic Resonance Imaging; fibromyalgia; morphology; functional connectivity; ReHo

Chronic pain is a common health problem with limited treatment options. As a result, patients often suffer from persistent pain for decades, with inadequate access to effective pain relief and high rates of comorbid depression (1). In spite of the high prevalence of chronic pain, the impact of long-term exposure of on the human brain is still poorly investigated.

Fibromyalgia (FM) is a condition of widespread musculoskeletal pain, soft tissue tenderness, fatigue and sleep disturbances (2). Studies suggest that the presence of long-term localized pain is the most prevalent precursor of developing widespread pain (3) and FM (4). Moreover, long-term follow-ups demonstrate that FM remains chronic, with low probability of full recovery (5). There is evidence for central nervous system aberrations in FM (6, 7) for example, augmented responses to experimental pain stimuli (8, 9), changes in resting-state functional connectivity (10, 11) and altered function of brain neurotransmitters (12–15). In addition, studies found that FM is associated with brain morphological changes, such as decreased gray matter in the insula, rostral anterior cingulate cortex (rACC) and medial prefrontal cortex, compared to age-matched healthy controls (16–20).

Neuroimaging has significantly contributed to our understanding of the brain mechanisms associated with FM (21). Nevertheless, the linkage between brain structure, brain function and clinical symptoms, which could potentially elucidate the pathology and development of the disorder, is still missing. The combination of several independent brain measures, in the same group of patients, may represent a critical step to elucidate the central mechanisms of FM and negative impact of long-term exposure to pain. To that end, we designed a study where we first investigated the difference between FM patients and healthy controls regarding measures of brain morphology and functional regional homogeneity. Then, we investigated how the duration of FM symptoms and comorbid depressive symptoms had affected the morphology and regional homogeneity within the patient group. We hypothesized that brain regions previously implicated in FM pathology would display both functional and morphometric changes compared to healthy controls. We also hypothesized that the altered brain structure and functional changes observed in FM patients would be associated with the duration of FM symptoms and presence of comorbid depressive symptoms.

Materials and Methods

Participants

A total of 92 female FM patients aged 25 to 55 years, mean age 44 (SD = 8.2) were enrolled. Of the 92 patients 9 were excluded from fMRI analyses due to image artifacts or en passant findings of intracranial anomalies, leaving 83 patients for analysis with matched healthy controls. A total of 13 healthy female controls were available; aged 24 to 48 years, mean age 34 (SD = 8.6). Due to the relatively large number of patients, each healthy control could be

age-matched with two FM patients (n=26, range 24–48 years, mean 38, SD = 6.8). All patients in this study were investigated as part of the baseline assessments of a pharmacological fMRI clinical trial including three sites: one in England, Sweden and Germany. The same brain imaging assessments were also performed in healthy controls at all three sites, consecutively recruited throughout the study. The study was approved by the local Ethical Committee at each of the three participating sites and all participants gave written informed consent. Parts of the present dataset were used in Jensen et al 2010, where all 92 available FM patients were analyzed (22) and Jensen et al 2009, where 11/26 FM patients and 13/13 controls from the present study were included (23). None of the previous publications included analyses of brain morphology or regional functional connectivity.

Screening

Before inclusion in the study, both FM patients and healthy controls were carefully screened for the inclusion and exclusion criteria. All FM patients were recruited from primary care and at the beginning of the screening visit an experienced pain physician confirmed the FM diagnosis, using the 1990 American College of Rheumatology criteria (24). The inclusion criteria required that FM patients had an average pain intensity of at least 40 out of 100 mm on a visual analogue scale (VAS) during the week prior to screening. Exclusion criteria included, for example, severe psychiatric disorder, suicide risk or history of substance, drug, or alcohol abuse. The data in the present study was collected as the baseline measure of a pharmacological Randomized Controlled Trial (RCT) and therefore patients' medications or other treatments were strictly limited. The inclusion criteria required discontinuation of all treatments that could influence the patients' pain perception, i.e., antidepressants and mood stabilisers, analgesics (tramadol, codeine, dextropropoxyphene), strong opioids including patches, anesthetic patches, anticonvulsants, centrally acting relaxants, joint injections, trigger/tender point injections, biofeedback and transcutaneous electrical nerve stimulation.

Pain stimulation

Experimental pain stimuli were applied to the thumbnail using a standardized method where a computer-controlled stimulator applies pressure via a 1 cm² hard rubber probe (25). The thumb is inserted into a cylindrical opening and the probe applies pressure to the nail bed. Pressure pain is commonly used in FM studies because pressure sensitivity is a diagnostic criterion for FM and elicits a deep pain sensation that is clinically valid in this group of patients.

Brain imaging

Brain images were collected using 1.5 Tesla scanners at each of the three study sites, respectively. In London, a General Electric HDx scanner was used, in Stockholm a General Electric Twinspeed Signa Horizon and in Cologne a PHILIPS scanner was used. Multiple T2*-weighted single-shot gradient echo EPI sequences were used to acquire blood oxygen level dependent (BOLD) contrast images. The following parameters were used: repetition time: 3000 ms (35 slices acquired), echo time: 40 ms, flip angle: 90 degrees, field of view: 24 × 24 cm, 64 × 64 matrix, 4 mm slice thickness with 0.4 mm gap and sequential image acquisition order. Visual distraction during scans was minimized by placing a blank screen in front of the patient's field of view from inside the scanner. In addition to the functional scans, high-resolution T1-weighted structural images were acquired in coronal orientation for analysis of brain morphology. Parameters were: Spoiled Gradient Recalled 3D sequence, repetition time: 24 ms, echo time: 6 ms, flip angle 35 degrees with a voxel size of 0.9 × 1.5 × 0.9 mm³.

The scanning procedure was standardized between sites, by using written manuscripts for all oral instructions and practical training for the investigators. All FM patients and healthy

controls were site-matched in order to make sure there was an equal number of patients and controls from every site. We also performed several statistical analyses to validate that the site-factor had no significant effect on brain data. Previous evidence (26) validate that the variance between individuals in neuroimaging studies is greater than the variance between scanners at different sites.

Procedure - Behavioral data

The day before fMRI scanning, each participant was calibrated for subjective pain ratings by receiving one ascending and one randomized series of pressure stimuli. Pressures (duration 2.5 seconds) were delivered at 30 seconds intervals. Participants were instructed to rate the intensity of the pain evoked by each stimulus by putting a mark on a 0–100 mm VAS ranging from “no pain” to “worst imaginable pain”. Each participant’s pain threshold (first VAS > 0 mm) and stimulation maximum (first rating > 60 mm VAS) was used to compute five different pressure intensities within the range of the threshold and maximum. In total, 15 stimuli, each lasting 2.5 seconds, were delivered in a randomized order and a polynomial regression was used to determine each individual’s pressure at VAS 50 mm, hereafter referred to as P50.

The Beck Depression Inventory (BDI) was used to quantitatively assess depressive symptoms. The BDI is a 21-item measure of the severity of depressive symptoms, and it has been extensively validated for use with both medical and mental health populations (27). A score of 0–9 indicates minimal depression, 10–18 indicates mild depression, 19–29 indicates moderate depression and 30–63 indicates severe depression.

Procedure - Functional imaging

Experimental pain during fMRI scanning was induced by means of painful pressures, individually calibrated to represent each participant’s 50 mm VAS (P50), as well as non-painful pressures, representing 0 mm VAS. Again, all stimulations were randomly distributed over the scanning time, preventing participants from anticipating the onset time and event type. The time interval between stimuli had a mean stimulus onset asynchronicity of 15 seconds (range 10–20 seconds). The study design included four different random sequences but the particular order was randomized for each participant. Each participant received at least two sequences. The total duration of two sequences was 16 minutes. Participants were instructed to focus on the pressures on the thumb and to not use any distraction or coping techniques.

Statistical analyses - Behavioral data

The correlations between duration of FM symptoms, pain ratings and sensitivity to pressure-pain were performed by means of partial correlations, controlling for physical age and depression scores, using the statistical software SPSS, version 18.0.

Statistical analyses – Neuroimaging data

Cortical Thickness—The cortical surface reconstruction was performed using FreeSurfer version 5.1 (<http://surfer.nmr.mgh.harvard.edu>). FreeSurfer uses a series of computationally intensive steps on the T1-weighted structural volumes to estimate the gray/white interface (28–30). These steps include motion correction and averaging, computing Talairach transforms, intensity normalization, skull stripping, tessellation of the gray matter/white matter boundary, automated topology correction, automatic volume labeling and white matter segmentation. Any inaccuracies in the reconstruction of white and pial surfaces of individual subjects were manually corrected before calculating cortical thickness. The

cortical thickness measure was computed as the distance between the pial and white surfaces at each point across the cortical mantle.

Group analyses were performed by resampling each subject's data to the FreeSurfer average atlas, distributed as a part of FreeSurfer. Cortical thickness maps were smoothed using a Gaussian kernel with a full width half maximum of 10 mm. General Linear Model was calculated at each vertex on the surface covarying for physical age. To test for significant differences in cortical thickness between the two groups, the slope of the lines for the two groups, representing the rate of change of thickness over time, was assumed to be constant and the offset/ intercept representing cortical thickness was varied to get the best fit for each group. In order to determine the relationship between cortical thickness and clinical scores in patients, thickness was regressed on a vertex-by-vertex basis against scores of duration and depression while controlling for physical age. For this analysis an initial vertex wise threshold of $p < .001$ was used, uncorrected.

MRI Volumes—The automated procedure for labeling different brain structures, and getting their volumetric measures, is described in detail by Fischl et al (29). This procedure assigns a neuroanatomical label to each voxel in an MRI volume based on probabilistic information automatically estimated from a manually labeled training set, including both grey and white matter. This technique has been shown to be comparable in accuracy to manual labeling. The automatic segmentations were also visually inspected for accuracy. In the present paper, we report results of total brain volumes (supra-tentorial), volumes for cortical and sub-cortical gray matter, white matter, and the *a priori* regions of interest including rostral Anterior Cingulate Cortex (rACC), amygdala, lateral orbitofrontal cortex (IOFC).

Statistical analyses for volumetric measures extracted from FreeSurfer's automated segmentation, were performed using SPSS 18.0. Group differences between FM patients and controls in cortical gray matter, sub-cortical gray matter, cortical white matter, sub-cortical white matter and segmentation volumes of the *a priori* ROIs were analyzed using independent samples t-tests. To get an estimate of the relationship between neuroanatomical volumes from the *a priori* ROIs and the behavioral measures depression scores and pain duration, partial correlation analyses were performed. The correlation between ROI volumes and FM duration was controlled for 'age' and 'depression' and, conversely, the correlation between ROI volumes and depression was controlled for 'age' and 'duration'. For all comparisons, the resulting p-values were corrected using the Bonferroni method. Since there were six *a priori* ROIs (three bilateral structures), the resulting corrected threshold for all pairwise comparisons was $p < .008$.

Regional Homogeneity (ReHo) functional connectivity—All pre-processing and ReHo analyses were performed using DPARSFA (Data Processing Assistant for Resting State fMRI, Advanced) based on SPM8 (31–33). Pre-processing included the following steps: removal of the first 10 time points, slice timing correction using the middle slice as a reference, realignment (motion correction), normalization into MNI space using an EPI template, linear trend removal, and temporal filtering of results by 0.01–0.08 Hz. After this, the ReHo according to Kendall's coefficient concordance (KCC) (34) was calculated using a cluster consisting of 27 voxels. At a given voxel, ReHo was defined as the KCC of the time series of this voxel with those of its 26 nearest neighbors. The resulting map of ReHo values at each voxel was then divided by the global mean value within the whole-brain mask. This result was then smoothed with a kernel of 4 mm. Ultimately, a two-sample t-test and two separate regression analyses were performed, using the second-level analysis function in the Statistical Parametric Mapping 8 (SPM8) software (SPM8, Wellcome Trust Centre for Neuroimaging, London, UK) and Matlab 7.4 (Mathworks). In line with previous studies, a

threshold of voxel-wise $p < .005$ uncorrected with 20 contiguous voxels was used for predefined ROI's. For non-ROI brain regions, the threshold was set at voxel-wise $p < .001$ (uncorrected) and $p < .05$ FWE-corrected at cluster level.

Results

Between group effects

Behavioral outcomes—A two sample t-test revealed a significant difference in pressure pain sensitivity (P50) between FM patients and healthy controls, $t(37)=-4.0$, $p < .001$, two-tailed; validating that patients needed significantly lower amounts of pressure than controls to experience comparable pain intensities (see Table 1).

Neuroimaging outcomes

Cortical thickness: A vertex-wise whole brain analysis of cortical thickness generated significance maps for groups of vertices with significant differences between FM patients and controls. This analysis revealed several regions of significantly lower cortical thickness in FM patients compared to controls: the left rACC, which was part of our a priori hypothesis, as well as others beyond the territory of the hypothesis: left superior frontal gyrus, right superior temporal gyrus, right and left middle temporal gyrus and right fusiform gyrus. Only one group of vertices displayed higher cortical thickness in FM patients compared to controls, located in the right superior parietal gyrus (see Table 2 and Figure 1).

MRI volumes: In an overall analysis of total brain volume (supratentorial), including both cortical and subcortical structures, patients displayed significantly lower total brain volume than controls, $t(37)=-3.6$, $p=0.001$. The automated segmentation of cerebral matter in FreeSurfer allowed for more specific comparisons of white and gray matter volumes. Analyses of gray matter volumes, both cortical and subcortical, revealed that patients had significantly lower volumes than controls in cortical gray matter $t(37)=-3.2$, $p=.003$, two-tailed, as well as subcortical gray matter $t(37)=-2.7$, $p=.010$, two-tailed. In addition to gray matter volumes, patients displayed significantly lower volume of cortical white matter compared to healthy controls $t(37)=-2.9$, $p=.006$, two-tailed indicating that the decreased brain volumes seen in FM were not only an effect of gray matter atrophy.

Comparisons of a priori ROI volumes (listed previously) between patients and controls revealed that patients had significantly lower volumes in the left rACC, $t(37)=-4.7$, $p=.00003$ and the left IOFC, $t(37)=-3.79$, $p=.0005$. The right IOFC and right amygdala approached significance but were not significant after Bonferroni correction: right IOFC, $t(37)=-2.49$, $p=.017$; and right amygdala, $t(37)=-2.75$, $p=.009$. The left amygdala and the right rACC were not significantly different between patients and controls.

ReHo functional connectivity: Analyses of functional regional homogeneity (ReHo) revealed significantly lower coherence in the rACC in FM patients, compared to controls. The cluster was partially located in the left cingulate cortex but also extended into the left medial prefrontal cortex. There were no regions that showed significantly higher regional coherence in patients than controls (see Table 2 and Figure 2).

Within group effects - FM Duration

Behavioral outcomes—Within the patient group ($n=26$), a partial correlation displayed no significant association between the duration of FM and ratings of clinical pain intensity (VAS), $r=.029$, $p=.892$; but a moderate correlation between FM duration and sensitivity to P50 pressure pain, $r=.405$, $p=.050$; see Table 1.

Neuroimaging outcomes

Cortical thickness: Regression analyses were used to investigate the effects of FM duration on cortical thickness in patients (n=26). Significance maps indicating regions with significant associations between cortical thickness and FM duration revealed specific regions on the cortical surface (see Table 3). The middle temporal gyrus displayed a significant negative association between FM duration and cortical thickness, as well as the rACC, which was included in our a priori hypothesis, indicating lower cortical thickness with longer FM duration (see Figure 3). Several groups of vertices, specifically in the left middle frontal cortex, bilateral parietal lobes and bilateral temporal lobes, displayed higher cortical thickness with longer duration of FM pain (see Table 3).

MRI volumes: A regression analysis revealed that the supratentorial brain volume, including both cortical and subcortical grey matter areas, was significantly decreased with longer FM duration, $r=-.435$, $p=.030$. In separate analyses of cortical and subcortical gray matter, there were significant decreases in gray matter volume with longer FM duration for subcortical gray matter, $r=-.403$, $p=.046$; but only a trend towards significance for the cortical gray matter, $r=-.384$, $p=.058$. A separate correlation between FM duration and white matter volumes displayed a significant decrease of white matter with longer FM duration, $r=-.403$, $p=.046$.

The volumes of the right and left rACC were negatively correlated to FM duration, suggesting decreased rACC volumes with longer FM duration; left rACC, $r=-.44$, $p=.034$; right rACC, $r=-.54$, $p=.007$. The left and right IOFC also displayed negative correlations with FM duration; left IOFC, $r=-.42$, $p=.040$; right IOFC $r=-.58$, $p=.001$. Amygdala volumes were not significantly correlated with FM duration; left amygdala, $r=-.42$, $p=.052$; right amygdala, $r=-.29$, $p=.17$. After Bonferroni correction for multiple comparisons, we conclude that the decreased volume observed in the right IOFC and right rACC were significantly correlated to FM duration (see Figure 3).

ReHo functional connectivity: The effect of FM duration on functional regional coherence was assessed by means of an fMRI regression analysis in FM patients (n=26), using FM duration as a covariate of interest. The regression of FM duration revealed no significant changes in functional regional coherence; negative or positive.

Within group effects – Depression

Behavioral outcomes—Within the patient group (n=26), a partial correlation displayed no significant association between BDI depression scores and FM duration, $r=.23$, $p=.26$; and no correlation between depression scores and ratings of clinical pain intensity, $r=.10$, $p=.60$.

Neuroimaging outcomes

Cortical thickness: The effect of BDI depression scores on cortical thickness was analyzed by means of regression analyses, creating a cortical thickness map revealing depression related thinning in FM patients. Several areas on the cortical surface displayed significant negative correlations between cortical thickness and depression scores. The significant regions were located primarily in the parietal and occipital cortex, indicating that cortical thinning in these regions were associated with higher BDI scores. Only one group of vertices, located in the left parietal lobe (supramarginal gyrus), displayed a positive correlation between depression and cortical thickness (see Table 3).

MRI volumes

Total brain volume: There were no significant correlations between BDI scores and the supratentorial grey matter brain volume, including both cortical and subcortical areas $r=-.02$, $p=.92$; cortical gray matter $r=-.19$; $p=.37$; subcortical gray matter $r=.05$, $p=.82$; or cortical white matter $r=.14$, $p=.50$.

ReHo functional connectivity—A regression analysis of functional regional coherence and BDI depression scores revealed significant changes in regional coherence in the ventral striatum/Nucleus Accumbens (NAc). With high levels of comorbid depressive symptoms, patients displayed relatively lower regional coherence in the NAc region of the striatum (MNI coordinates: $x=21$, $y=15$, $z=0$; cluster size: 57 voxels; peak T-value: 3.85; $p<.005$ cluster corrected). There were no significant results for the opposite depression contrast.

Discussion

In this study, we investigated structural and functional brain differences between FM patients and matched controls. Our results suggest that the rACC, a key region for modulation of pain, had significantly decreased cortical thickness, brain volume and regional functional connectivity in FM, as compared to healthy controls. The volumetric changes were more pronounced with longer exposure to FM pain. Also, there were structural and functional changes in the mesolimbic areas of the brain associated with comorbid depressive symptoms. The present study provides unique evidence for overlapping neuroanatomical and functional brain changes in patients with chronic pain.

Consistent with previous studies (35, 36) our study found that FM patients were significantly more sensitive to experimental pain than controls, reflecting a core symptom and diagnostic criterion in FM. In line with this behavioral difference, the analysis of regional functional connectivity in FM patients and controls revealed lower rACC coherence in FM patients, compared to controls. Impaired pain inhibitory responses in FM patients have previously been associated with lower activations of the rACC (23) and less functional connectivity between the rACC and other regions of the brain's pain modulatory system (37). The functional connectivity method used in this study, ReHo, is a model-free estimation of the synchrony of spontaneous fMRI signal oscillations within spatially neighboring voxels and has recently proven to be sensitive to disease-related alterations, as demonstrated in several different disorders (38–40). Other functional connectivity methods such as seed based methods (which focus on connectivity between a particular seed and other brain regions) (41) and independent component analysis (ICA, which focuses on identifying different components of brain networks) (42) are used to identify key networks of the brain. ReHo, on the other hand, measures the local synchrony of different brain regions, facilitating the identification of key brain regions, rather than networks. This unique character of ReHo is important when investigating the relationship between brain structure and functional. Since the rACC is a key region for descending inhibition of pain (43, 44), the lower rACC coherence in FM patients provides support for the hypothesis that the FM pathology may be associated with dysfunction of descending pain modulation (36, 45, 46).

In consistency with previous morphometric studies in FM (16–20) we found decreased measures of cortical thickness and brain volumes in FM patients, compared to controls. As expected, the cortical thickness of the rACC was decreased with longer FM duration. In line with our hypothesis, there was a negative association between FM duration and rACC volumes, suggesting that rACC volumes are decreased with increased duration of FM pain. A study from 2007, found lower mu-opioid receptor function in the rACC (12), possibly reflecting significant atrophy in this region. Our results indicate that the rACC may an important element in the development and/or pathophysiology of FM. In line with previous

morphometric reports of increased grey matter volumes in FM patients (20) we also found increased cortical thickness with increased FM duration in several temporal and frontal regions. It is possible that increased cortical thickness with longer FM duration reflects a compensatory mechanism, attempting to prevent the negative effects of a constant nociceptive input to the brain, however the anatomical specificity is not clear.

In a recent morphometric study (47) the authors found that the difference in gray matter volumes between FM and matched controls disappeared when controlling for comorbid affective measures, suggesting that brain atrophy might be more related to negative affect than pain. To address this concern, we used patients' ratings of depressive symptoms (BDI) to assess the specific impact of comorbid depression on brain function and structure in FM. A regression analysis of fMRI data revealed a significant association between high depressive scores and decreased functional coherence in the ventral striatum. The ventral striatum is part of the mesolimbic reward circuitry and low activations have previously been associated with core symptoms of depression, such as anhedonia and reduced motivation (48). There were no brain regions with significantly greater regional coherence with higher depression. The analysis of cortical thickness revealed significant decreases in cortical thickness in 9 regions with higher depression scores, including the parietal cortex, which has previously been implicated in depression (48). There was no spatial overlap between the functional decrease in mesolimbic activation and decreases in brain volumes. Furthermore, we did not find any significant depression-related changes in any of the regions that were defined as regions of interest (functional or structural). Taken together, our results indicate that depressive symptoms are associated with cerebral changes, independent from pain. The results are in line with our findings from an earlier neuroimaging study in which we found independent neural mechanisms for FM pathology and depression (22), even if depression and pain are inherently related in the clinical context.

Recent neuroimaging studies have investigated the causality between chronic pain and measures of decreased brain volumes (49, 50). Data suggest that long-term exposure to pain causes reductions in specific brain regions, and not vice versa. Here, we found that FM duration was significantly correlated to brain changes; nevertheless, the sequence of these changes needs to be fully investigated in longitudinal studies. Such studies could potentially explore whether structural and functional alterations are early indicators of the development of widespread chronic pain and may help to develop predictive tools for chronic pain.

Conclusion

The combination of functional and structural brain measures revealed that FM patients had overlapping decreases of cortical thickness, brain volumes and regional functional coherence in the rACC. The atrophy of the rACC, as measured by brain volumes, was associated with duration of FM pain. Given the crucial role of the rACC in descending pain modulation, our result implies that disrupted endogenous pain modulation is central in the development and pathophysiology of FM.

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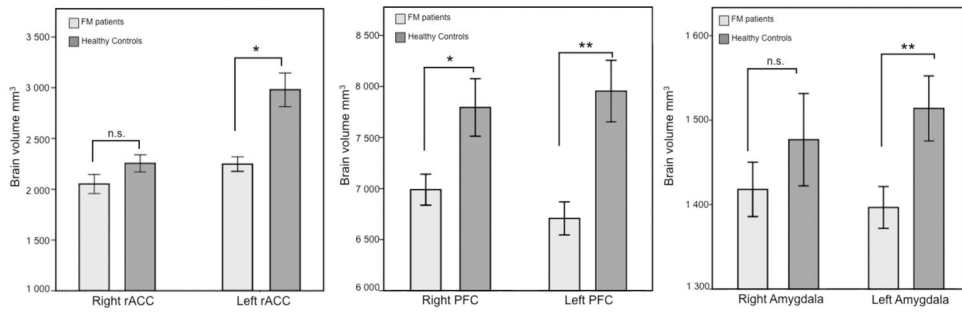


Figure 1. Cortical Thickness measures in FM patients and healthy controls

Measures of cortical thickness, using FreeSurfer, revealed lower cortical thickness measures in the left rACC (MNI $x=-6, y=36, z=11$) in FM patients, compared to age- and gender-matched healthy controls.

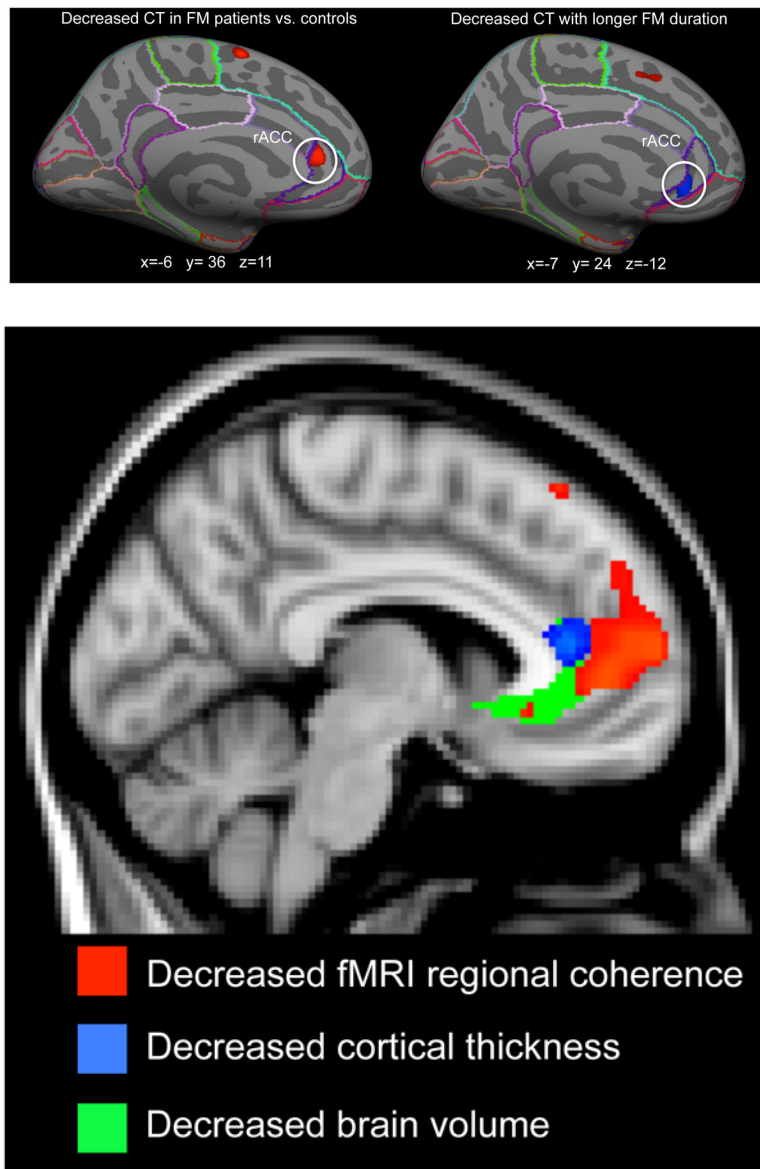


Figure 2. Overlap of three different brain measures comparing FM patients and controls
 Spatial overlap between the results from volumetric, cortical thickness and regional functional connectivity analyses (ReHo). For all three analyses methods, the rostral ACC displayed decreased measures in FM patients, compared to controls, with regard to brain volume, cortical thickness and functional connectivity.

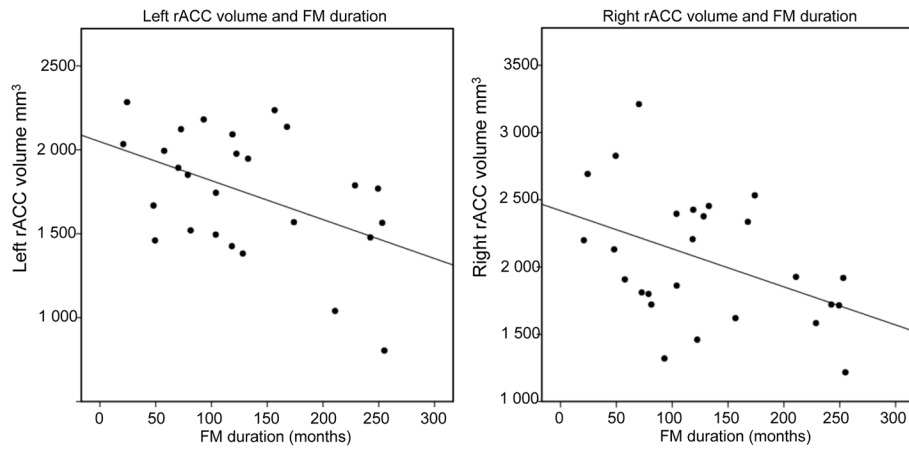


Figure 3. Duration of FM pain and brain volumes

The duration of FM pain was negatively correlated to brain volumes in the right OFC and right rACC, controlling for physical age and depression ($r=-.58$, $p=0.001$, two-tailed) and ($r=-.54$, $p=.007$, two-tailed).

Table 1**Subjects' characteristics**

The mean value and Standard Deviation (SD) is given for each variable. 'The pressure at VAS 50' represents the pressure required to evoke pain that corresponds to a rating of 50 on a 0–100 mm visual analogue scale. The duration of FM symptoms is based on patients' subjective report. 'Weekly pain intensity' refers to patients' rating of the average clinical pain intensity over the last week, on a 0–100 mm visual analogue scale. The 'BDI score' refers to self-rated depressive symptoms where 0–9 indicates minimal depression, 10–18 indicates mild depression, 19–29 indicates moderate depression and 30–63 indicates severe depression. For the variables 'Age' and 'Pressure at VAS 50', the t-score and p-value from an independent samples t-test is also listed.

Variable	FM patients (n=26)	Controls (n=13)	t-score	p-value
Age (years)	38 (7)	34 (9)	1.8	0.08
Pressure at VAS 50 (kPa)	341 (133)	572 (186)	4.14	0.001*
Duration of FM symptoms (years)	11(6)	Na		
Weekly pain intensity (VAS mm)	72 (14)	Na		
BDI score	21 (11)	Na		

* significant

Table 2
Cortical thickness and functional differences between FM patients and healthy controls

FreeSurfer analyses of cortical thickness and ReHo analyses of functional regional coherence. The anatomical locations of each cluster is given in Montreal Neurological Institute (MNI) coordinates (x, y, z). Regions in italics denote our *a priori* regions of interest.

Cortical Thickness Controls > FM	Laterality	Number of vertices	X	Y	Z	Max p-value
<i>rACC</i>	L	136	-6	36	11	0.00041
Superior frontal	L	85	-7	-3	62	0.00046
Middle temporal	L	48	-56	-14	-20	0.00095
Superior temporal	R	250	55	-22	4	0.00024
Middle temporal	R	106	63	-16	-16	0.00037
Fusiform	R	60	37	-25	-22	0.00082

Cortical Thickness FM > Controls	Laterality	Number of vertices	X	Y	Z	Max p-value
Superior parietal	R	181	26	-61	44	0.00021

ReHo Controls > FM	Laterality	Cluster size (voxels)	X	Y	Z	p-value cluster
<i>rACC</i> / MPFC	L	756	-4	49	-11	0.05

Table 3

Cortical thickness related to FM duration and depression.

Cortical thickness measures for the duration of FM pain, using age and depression as covariates of no interest. Comorbid depression was measured by Beck's Depression Inventory (BDI). Negative results indicate decreased cortical thickness with longer FM duration or higher depression scores. Conversely, positive results indicate increased cortical thickness with longer FM duration or high depression. The anatomical locations of each cluster is given in Montreal Neurological Institute (MNI) coordinates (x, y, z). Regions in italics denote our *a priori* regions of interest.

Cortical Thickness FM Duration - Negative results	Laterality	Number of vertices	X	Y	Z	Max p-value
Middle temporal	R	99	63	-27	-16	0.0003
rACC	R	82	5	31	-7	0.00097
Cortical Thickness FM Duration - Positive results	Laterality	Number of vertices	X	Y	Z	Max p-value
Supramarginal	L	118	-50	-52	45	0.00011
Rostral middle frontal	L	118	-30	43	18	0.00015
Inferior temporal	L	122	-51	-63	-5	0.00040
Superior frontal	L	40	-20	8	61	0.00073
Pars opercularis	L	82	-33	22	12	0.00074
Inferior temporal	R	120	46	-34	-20	0.000082
Precentral	R	25	52	-4	8	0.00037
Caudal middle frontal	R	41	39	19	38	0.00062
Cortical Thickness Depression - Negative results	Laterality	Number of vertices	X	Y	Z	Max p-value
Pericalcarine	R	896	18	-72	5	0.0000036
Fusiform	R	161	38	-62	-18	0.00010
Fusiform	R	20	34	-46	-14	0.0007
Lateral occipital	R	55	24	-86	17	0.00056
Paracentral	R	64	17	-26	39	0.00062
Inferior parietal	L	133	-39	-70	44	0.000059
Caudal middle frontal	L	66	-25	-2	45	0.00018
Precuneus	L	60	-18	-77	30	0.00059
Fusiform	L	14	-37	-29	-25	0.00084

Cortical Thickness Depression – Positive results	Laterality	Number of vertices	X	Y	Z	Max p-value
Supramarginal	L	265	-54	-51	27	0.00032