

Neuroimaging the Epileptogenic Process

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Published online: 1 February 2014
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Abstract Epilepsy is one of the most common chronic neurological conditions worldwide. Anti-epileptic drugs (AEDs) can suppress seizures, but do not affect the underlying epileptic state, and many epilepsy patients are unable to attain seizure control with AEDs. To cure or prevent epilepsy, disease-modifying interventions that inhibit or reverse the disease process of epileptogenesis must be developed. A major limitation in the development and implementation of such an intervention is the current poor understanding, and the lack of reliable biomarkers, of the epileptogenic process. Neuroimaging represents a non-invasive medical and research tool with the ability to identify early pathophysiological changes involved in epileptogenesis, monitor disease progression, and assess the effectiveness of possible therapies. Here we will provide an overview of studies conducted in animal models and in patients with epilepsy that have utilized various neuroimaging modalities to investigate epileptogenesis.

Key Words Magnetic resonance imaging · Magnetic resonance spectroscopy · Diffusion weighted imaging · Positron emission tomography · Functional magnetic resonance imaging · Biomarkers · Epilepsy · Epileptogenesis

Introduction

Epilepsy is a common neurologic disease characterized by the occurrence of spontaneous recurrent seizures [1]. Epilepsy affects approximately 50 million people worldwide [2], and holds an annual economic cost of over \$12.5 billion in the USA alone [3]. Although some epilepsy patients may be responsive to pharmaceutical treatments, at least 30 % of patients are drug-resistant [4]. Furthermore, anti-epileptic drugs (AEDs) often have adverse side-effects and, even in drug-responsive cases, AEDs merely suppress seizures without stopping or interfering with the epileptogenic disease process that converts a healthy brain into an epileptic brain [4, 5]. Therefore, therapies capable of preventing or reversing epileptogenesis are needed to cure this disease. Unfortunately, a major limitation in the development and implementation of such interventions is the poor understanding, and consequent lack of reliable biomarkers, of the epileptogenic process [5, 6].

Neuroimaging provides non-invasive research and medical tools with the capacity to identify early biomarkers involved in epilepsy, longitudinally monitor disease progression, and assess the effectiveness of epileptogenic therapies [7]. This article will review the research conducted at both the basic experimental and clinical level that has utilized various neuroimaging modalities to study epileptogenesis *in vivo*. The first section ([‘Neuroimaging Biomarkers in Animal Studies of Epilepsy’](#)) will present and evaluate studies that have utilized neuroimaging within animal models of epilepsy to identify potential biomarkers of epileptogenesis that may be translatable to the clinical setting. The second section ([‘Neuroimaging Biomarkers in Clinical Studies’](#)) will review the literature using neuroimaging in the clinical epilepsy setting. Detailed technical descriptions of the neuroimaging techniques and animal models that will be discussed are beyond the scope of this review, and readers are directed to the references provided in the appropriate sections for further information.

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Neuroimaging Biomarkers in Animal Models of Epilepsy

It is challenging to study early epileptogenic processes in the clinical setting as epilepsy is diagnosed in patients after the onset of spontaneous recurrent seizures, which represents the culmination of epileptogenesis [7]. Animal models of epilepsy, both acquired and genetic, provide the opportunity to rigorously investigate experimental subjects known to be experiencing epileptogenic processes, and thereby hold the potential to increase our understanding and identify early biomarkers of this disease. Briefly, some of the most commonly used and well-validated animal models of epilepsy that will be discussed in this section include exposure to proconvulsant chemicals, such as pilocarpine or kainic acid, to induce status epilepticus (SE) and consequent spontaneous seizures modeling temporal lobe epilepsy (TLE) [8]; electrical stimulation, or kindling, of temporal brain regions (e.g., amygdala) to model TLE [8]; and the fluid percussion brain injury (FPI) model of traumatic brain injury (TBI) and post-traumatic epilepsy (PTE) [9–11]. This section will provide a summary of the epileptogenic-related changes and neuroimaging biomarkers that have been identified to date within these models.

Magnetic Resonance Imaging: Signal, Volumetrics, and Contrast Agents

Magnetic resonance imaging (MRI) is based on the magnetic excitation of hydrogen nuclei in body tissue, and the consequent recording of the electromagnetic signals that are returned from the body [12]. Given its widespread clinical availability, non-invasive nature, and relative low cost, MRI is an attractive technique in both basic and clinical research. Specific to the basic experimental setting, epilepsy animal

model studies have incorporated conventional MRI techniques for over 20 years [13], with T_1 , T_2 , and T_2 -weighted (T_2W) signal measures amongst the most commonly employed [14].

Signal Changes

T_2 signal changes on MRI have been consistently reported at various phases of the epileptogenic process in numerous animal models, with the common underlying pathological changes being edema, gliosis, and cell loss (see Table 1) [15–18]. In chemoconvulsant SE models, increased T_2 values and T_2W hyperintensity have been reported in several brain regions, including the cortex, hippocampus, thalamus, amygdala [19, 20], and piriform and entorhinal cortices [15], beginning as early as 2 h after SE [20]. These acute changes typically return to baseline within 48–72 h [15, 20], and have been reported to predict the development of epilepsy at 4 months after SE [15]. However, in contrast to these findings, other studies have reported a global decrease in T_2 values in the acute stages after SE [17], and evidence of T_2W hyperintensity for up to 9 weeks after SE [16]. Consistent with chemically-induced SE models, SE induced by electrical stimulation of the rat amygdala resulted in increased T_2 values in the amygdala beginning 2 days after SE [21], and increased T_2W signal intensity in the hippocampus 2 weeks after kindling had ceased [22]. Taken together, these findings suggest temporal complexities in T_2 signal changes occurring in post-SE TLE models, likely representing the evolving pathophysiological processes in epileptogenesis [16, 17] that must be clarified and considered when translating the use of T_2 -based biomarkers to the clinical setting.

Studies using animal models of PTE and febrile seizures (FS) have also reported T_2 signal changes possibly related to

Table 1 Neuroimaging biomarkers in animal models

Imaging modality	Animal model	Potential biomarker	Related pathophysiology
MRI— T_2 signal	Post-SE, FPI, kindling, FS	Acute T_2 signal increase and T_2W hyperintensity	Edema, gliosis, cell loss
MRI—volumetrics	Post-SE, FPI	Decreased volume of limbic structures (i.e., hippocampus)	Structural atrophy
MRI—contrast agents	Post-SE	Mn^{2+} - and Gd^{3+} -enhanced signal change	Mossy fibers and BBB breakdown
DWI	Post-SE, FPI, absence epilepsy, FS	Altered ADC, FA, and tractography	Edema, axonal injury, connectivity
MRS	Post-SE	Reductions in glutamate, glutamine, GABA, and NAA, and increased myo-inositol and glutathione	Neurotransmitters, neuronal death and dysfunction, glia activation
PET	Post-SE, FPI	Decreases in [18F]FDG—PET signal, increases in [18F]PBR111—PET signal	Hypometabolism, inflammation
fMRI	Post-SE, absence epilepsy	Changes in BOLD signal	Neuronal activity and metabolism

MRI = magnetic resonance imaging; DWI = diffusion-weighted MRI; MRS = magnetic resonance spectroscopy; PET = positron emission tomography; fMRI = functional MRI; SE = status epilepticus; FPI = fluid percussion brain injury; FS = febrile seizure; T_2W = T_2 -weighted; ADC = apparent diffusion coefficient; FA = Fractional anisotropy; GABA = gamma-aminobutyric acid; NAA = N-acetyl aspartate; BOLD = blood oxygen level-dependent; BBB = blood–brain barrier

epileptogenesis. In the FPI model of PTE, early increases in T_2 signal values were found to be associated with functional and histological outcomes at both acute and chronic time-points [23]. However, it should be noted that these initial T_2 changes were found to be poor predictors of subsequent decreases in seizure threshold [23]. In a hyperthermia-induced FS model, rats that experienced prolonged febrile seizures displayed increased T2W signal intensity at 1 and 8 days after FS [24], increased T_2 values at 1 month after FS [25], and had an increased likelihood of developing spontaneous seizures after FS [24, 25]. However, the increase in T_2 value itself was not found to be an accurate predictor of epileptogenesis [25]. Taken together, further research is required to determine the usefulness of T_2 -based biomarkers to predict the development of epileptogenesis that ultimately results in spontaneous recurrent seizures in the context of these models.

Volumetric and Morphological Analyses

In addition to signal changes, conventional T_1 and T_2 MRI also allow for volumetric and morphological analyses of brain structures involved in epileptogenesis. As shown in Fig. 1, volumetric and morphological changes in the hippocampus and other limbic structures have been reported in both SE

[26–29] and FPI models [11, 23, 30, 31]. However, these changes are typically preceded by abnormalities identified by other more sensitive neuroimaging methods [11, 23, 28–31]. As such, volumetric and morphological changes may not be ideal neuroimaging biomarkers to identify early pathophysiological processes involved in epileptogenesis, but may have more of a role to assess subsequent progressive neurodegenerative changes, in particular atrophy of key structures such as the hippocampus, that may follow an epileptogenic brain insult [11, 29, 30, 32].

Contrast Agents

The contrast in conventional MRI signal can be further enhanced by administration of exogenous contrast agents, such as manganese (Mn^{2+}) and gadolinium (Gd^{3+}) complexes. These agents have been used to study epileptogenesis in post-SE [16, 33–36] and FPI [32, 37] rodent models, and enable the assessment of various pathologies potentially involved in the epileptogenic process, such as blood–brain barrier breakdown [16, 37], mossy fiber sprouting [35], and reorganization of neural connections [31, 32]. For example, studies utilizing serial Mn^{2+} -enhanced imaging at 2 days and 6 weeks after SE found increased T_1 -weighted signal intensity

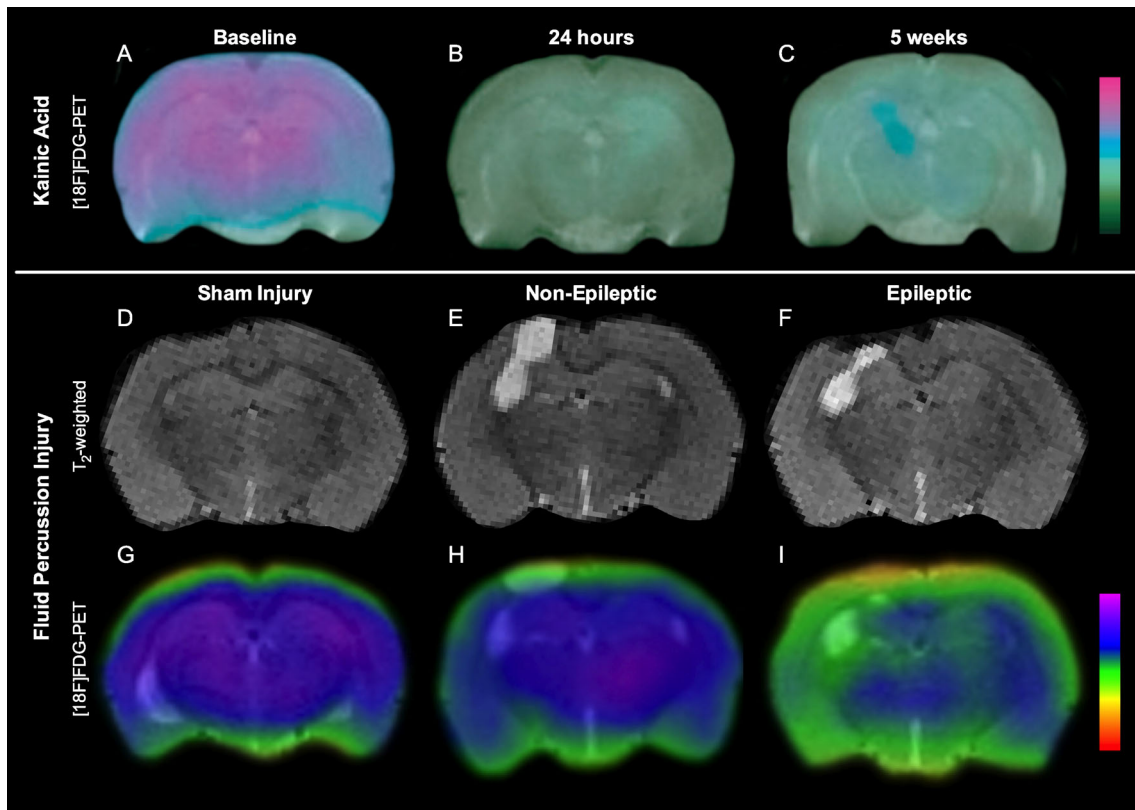


Fig. 1 Volumetric and [18F]FDG–positron emission tomography (PET) changes in kainic acid model of temporal lobe epilepsy and fluid percussion injury model of traumatic brain injury (TBI). There is persistent hypometabolism, and progressive degeneration after kainic acid-induced

status epilepticus (A–C; adapted from [29]). Although all rats suffer progressive neurodegeneration after fluid percussion injury (D–F), rats that develop post-traumatic epilepsy display persistent hypometabolism at 3 months after TBI (G–I; adapted from [11])

in the hippocampus that were related to spontaneous seizure outcome in the chronic epilepsy phase, suggesting that Mn^{2+} -enhanced imaging could provide a preclinical biomarker for the severity of epileptogenesis [34]. Unfortunately, a major limitation and confounder with the use of contrast agents, especially Mn^{2+} , is their high toxicity in mammals [14, 30]. However, these issues continue to be improved and, as such, contrast agents remain an effective tool in the study of epileptogenesis, particularly in the basic experimental setting.

Diffusion-weighted MRI

Diffusion-weighted MRI (DWI) and related methods, such as diffusion tensor and tractography analyses, are based on the quantification using magnetic resonance of the diffusivity of water molecules in the brain, which is more directionally limited (anisotropic) in white matter tracts relative to gray matter [36–38]. Common measures generated from DWI include apparent diffusion coefficient (ADC)—the magnitude of overall water diffusion in a given direction; mean diffusivity—the mean diffusivity across a number of directions; and fractional anisotropy (FA)—a value between 0 (isotropic) and 1 (anisotropic) that describes the anisotropy of diffusion [36]. In unhealthy white matter, damaged axonal membranes become less constricting to molecules and are thus less anisotropic [36, 37]. Tractography is another DWI-based post-processing method that allows for the assessment of structural connectivity, and holds promise in the study of epileptogenesis [38]. Notably, changes in DWI-based measures are also commonly associated with edema [37].

In post-SE rat models of TLE an acute *increase* in ADC, beginning as early as 3 mins post-SE [39], has been reported [17, 40]. However, this is a dynamic and structurally-dependent response, with reports of acute *decreases* in ADC post-SE [17, 39–42], a return to baseline by 1 week, and *increased* ADC at chronic time-points [39]. ADC increases may be related to vasogenic edema or increased metabolic activity [17, 39, 43, 44], whereas the acute ADC decreases are associated with cytotoxic edema and neuronal loss [39, 43, 44]. Structural dependent changes in FA have also been identified at chronic epileptic stages after SE [45, 46]. Although chronic FA changes that occur after the manifestation of spontaneous seizures hold little value as an early biomarker for epileptogenesis, FA may be an effective biomarker if validated at earlier stages.

Changes in DWI outcomes have also been reported in the FPI [23, 31, 37] rat model of PTE at various stages in the epileptogenic process. Of particular importance, acute and chronic hippocampal ADC changes in the FPI model were associated with electroencephalography (EEG) parameters (i.e., total number of interictal epileptiform spikes and epileptiform discharges), mossy fibre sprouting, and seizure susceptibility after a chemoconvulsant challenge [23, 37]. It should

also be noted that reductions in FA and associated tractography have been reported in animal models of genetic generalized epilepsy with absence seizures (i.e., WAG/Rij rats) [47], and decreased ADC and increased FA have been reported in rats after FS [48]. Taken together, DWI-based approaches are sensitive and promising in identifying potential epileptogenic-related changes throughout the disease process. However, future research is still required to assess whether these DWI changes are reliable biomarkers that predict epileptic outcomes [14].

Magnetic Resonance Spectroscopy

Magnetic resonance spectroscopy (MRS) is a neuroimaging technique capable of identifying levels of brain metabolites, such as N-acetyl aspartate (NAA), choline, creatine (Cr), lactate, myo-inositol, and glutathione; levels of neurotransmitters, such as glutamate, glutamine, and gamma-aminobutyric acid (GABA); and other physiological changes, such as intracerebral pH, all of which may have relevance to epileptogenesis [49, 50]. In post-SE animal models of TLE, MRS has identified acute reductions in glutamate, glutamine, and GABA [51, 52], as well as acute and chronic reductions in NAA [50, 53–57], a marker of neuronal loss or dysfunction [49]. Furthermore, progressive increases in myo-inositol and glutathione have also been detected in acute stages after SE, and are maintained in epileptic rats [50]. Studies using the FPI model have also used MRS to identify acute abnormalities after injury [58, 59], though whether these changes are associated with PTE has yet to be determined. Abnormalities in NAA and Cr have also been reported after FS in rats and may be related to the later development of spontaneous seizures [48]. Overall, these findings demonstrate that MRS is capable of identifying biomarkers associated with numerous pathophysiological changes occurring throughout the epileptogenic process, and support its use in future investigations.

Positron Emission Tomography

Positron emission tomography (PET) uses radiotracers to visualize and quantify functional processes in the brain. A variety of radiotracers are available, including those capable of identifying pathophysiological processes recently implicated in epileptogenesis, such as metabolism, neuroinflammation, and hyperphosphorylated tau [60–64]. For example, *in vivo* [18F]PBR111–PET has found significant inflammation after SE in the hippocampus and amygdala during epileptogenesis [60]. To date, the most common radiotracer employed in animal epilepsy studies, as in human epilepsy practice and research, is the glucose analogue [18F]FDG–PET, a biomarker for glucose uptake and brain metabolism. As shown in Fig. 1, in chemoconvulsant post-SE rat models, [18F]FDG–PET signal has been consistently found to

decrease during the acute post-SE period [29, 57, 65, 66], with some studies reporting a return to baseline at the subacute stage followed by decreased metabolism again in the chronic epileptic stage [29, 57]. Importantly, it has been reported that hypometabolism precedes, and is unrelated to, the atrophy of limbic structures, suggesting that the hypometabolism is not simply an effect of atrophy and may indicate cellular changes important in epileptogenesis [29]. A significant relationship has been reported between the degree of hypometabolism on [18F]FDG-PET in the entorhinal cortex early following lithium pilocarpine-induced SE in the rat and the chance of later developing spontaneous recurrent seizures, suggesting that this may be a biomarker of early epileptogenesis following a brain insult [66]. As seen in Fig. 1, [18F]FDG-PET following FPI in rats has also identified acute and persistent hypometabolism that preceded significant structural atrophy [11, 30], and may predict the later onset of PTE [11]. While further research is clearly required, and other limitations must be considered [62], these findings, together with the ability to assess other relevant pathophysiological processes *in vivo*, make PET a valuable experimental tool in the investigation of epileptogenesis.

Functional MRI

As with PET, functional MRI (fMRI) allows for the assessment of functional brain activity. However, fMRI is less expensive, less invasive, and provides superior temporal and spatial resolution relative to other functional neuroimaging techniques. For example, fMRI has temporal and spatial resolutions in the order of hundreds of milliseconds and one millimeter [12, 67, 68], whereas PET has temporal and spatial resolutions in the order of minutes and millimeters [62, 68]. Considering these factors, fMRI is now the most commonly used functional imaging method [12, 67]. Ogawa et al. [69] discovered the basic principle of fMRI, that MRI signal is sensitive to changes in blood oxygenation levels, over 20 years ago. As neuronal activity leads to increased blood flow and changes in blood oxygenation levels, or the blood oxygenation level-dependent (BOLD) signal, fMRI allows for the investigation of the location and networks of brain function [12, 67]. As epilepsy is known to involve abnormalities in neural activity and circuitry, fMRI represents a promising tool in the study of epileptogenesis [67].

Animal models of epilepsy are advantageous for fMRI studies as they allow for control over the type and timing of seizure, elimination of movement artifacts, and the use of more invasive techniques to complement fMRI analysis [67]. Studies using chemoconvulsant SE models have reported robust BOLD changes associated with seizure activity [67, 70–72]. Similarly, fMRI studies in animal models of genetic generalized epilepsy with absence epilepsy also report BOLD signal abnormalities associated with spontaneous spike-wake

discharges [67, 73–75]. Though there have been some inconsistencies regarding these findings (i.e., BOLD increase vs decrease) [76], and other potential confounds and limitations (e.g., animals are often under general anesthetic) to consider [67], these studies clearly demonstrate the ability and usefulness of fMRI in identifying functional abnormalities in epileptogenesis.

Neuroimaging Biomarkers in Clinical Studies

Many different neuroimaging modalities are utilized in the evaluation of patients with epilepsy. It is more challenging, though, to track the epileptogenic process in the clinical setting as the majority of our data come from patients with chronic epilepsy and the changes seen on imaging may reflect, to varying degrees, the genetics, the pathogenic process, aging, secondary damage, or even drug effects [77].

Ideally, a biomarker for epileptogenesis would help diagnose and predict epilepsy in the preclinical or early symptomatic stage, it would be specific to the epileptic process, it would monitor disease progression, and demonstrate reversal of epileptogenesis following therapeutic interventions [78, 79].

In order to help elucidate the role of imaging in the development of the epileptogenic process in humans, we will focus in this portion of the review on data from longitudinal clinical studies that may infer causality or help document disease progression. Clinical settings where neuroimaging has been used to study epileptogenesis include FS, PTE, early-onset epilepsy in children, and studies assessing long-term disease prognosis in chronic epilepsy.

MRI

Signal Changes

There has long been observed an association between FS and development of TLE later in life. In children, immediately after complex FS or prolonged status, increased T₂/DWI signal has been reported in the hippocampus [80, 81], ipsilateral thalamus, and anterior cingulate gyrus [82]. These acute changes are reversible [83] and thought to be secondary to cytotoxic or vasogenic edema. Concurrent EEG background abnormalities and focal spikes have also been reported [82]. Increased T₂ signal and hippocampal volume changes, in this setting, are the most predictive indicators of subsequent development of mesial temporal sclerosis (MTS) [7, 81, 84].

In the FEBSTAT study, a longitudinal study to try and elucidate the pathogenic link between FS and late development of epilepsy, 11.5 % of children presenting with prolonged (>30 min) febrile status had increased or equivocal T₂ signal in the hippocampus and more widespread in the

temporal lobe, compared with none among children with simple febrile seizures [85]. T2W hippocampal signal abnormality was associated with focal EEG slowing or attenuation suggestive of acute hippocampal injury [86].

In TBI, the presence of cortical or subcortical T₂ hyperintense lesions 1 year after the initial insult is associated with an increased risk of PTE [87]. Furthermore, on T₁-weighted magnetization transfer images, abnormalities extending beyond the T₂ changes or presence of gliosis surrounding hemosiderin deposits (especially when the gliosis wall is incomplete or shows a dynamic evolution in subsequent scans) are associated with higher risk for epilepsy [88, 89]. Furthermore, hippocampal T₂ increased signal and atrophy have been shown to be strong indicators of seizure recurrence following AED withdrawal in seizure-free patients [90].

The above findings of mainly T₂ signal abnormalities seen on structural MRI are suggestive of a potentially epileptogenic effect of both acute and chronic neural injury, but the causal link is still under investigation. In the case of FS, the long-term outcomes of the FEBSTAT study will hopefully shed more light into the significance of acute signal changes and their link to epileptogenesis.

Volumetric and Morphological Analysis

Some of the morphometric findings seen on MRI raise the possibility of a direct contribution to epileptogenesis. In the FEBSTAT study, developmental abnormalities of the hippocampus (hippocampal malrotation being the most common) were seen in the group of children with prolonged FS, suggestive of a possible predisposition to the initial epileptogenic insult [85]. Seizure-generating hypothalamic hamartomas appear to always have a connection to one or both mammillary bodies [91].

Cortical dysgenesis and development of subsequent epilepsy is well known, but prognosis after surgical removal of the visible structural abnormality varies. Lack of gray or white matter volume distribution abnormalities outside the primary lesion in the preoperative volumetric MRI is associated with better prognosis following lesionectomy [92]. Presence on MRI of thickened gyri and focal *versus* hemispheric involvement with severe hypometabolism on [18F]FDG-PET is a better predictor of specific epileptogenic cells than interictal or ictal EEG, and therefore may be used as a biomarker of epileptogenic tissue [93].

Gray matter volume reduction also correlates with epilepsy duration and has been reported for the hippocampus, entorhinal cortex [94], and thalamus [7]. It is more widespread in refractory TLE [90] and more severe in patients with MTS [7]. In TLE, MR volumetry has demonstrated bilateral white [95] and gray matter changes, and a history of FS is associated with smaller thalamic volumes ipsilateral to the seizure focus [82].

In familial mesial TLE, progression of hippocampal atrophy is seen in patients with frequent seizures and poor outcome [96].

Neocortical atrophy can be quantified by measuring cortical thickness across the entire cortical mantle to track continuous changes [97]. Cross-sectional analysis in refractory TLE showed progressive atrophy in the ipsilateral orbitofrontal, mesiotemporal, postcentral, and contralateral prefrontal areas. Longitudinal analysis over 2.5 years showed ipsilateral temporopolar and central, as well as contralateral orbitofrontal, insular, and angular region, cortical atrophy. Atrophy in somatomotor and parahippocampal regions in medial temporal lobe epilepsy (MTLE) has also been reported [94]. In patients with idiopathic generalised epilepsy (IGE), a 3.2 % decrease in global mean cortical thickness and focal cortical thinning in frontal, precentral, central, and lateral temporal regions has been described. Increased seizure frequency showed faster cortical thinning [97]. Contrary to the above findings, larger septal nuclei are reported in patients with TLE without MTS compared with extratemporal epilepsy, and controls raise a possible prophylactic effect against epileptogenesis of these structures [98].

Taken together, the above findings show that morphological change may be a direct marker of intrinsic epileptogenesis, but—as in animal models—MRI volumetric analysis plays more of a role in describing disease progression. Higher extracellular glutamate concentration (a highly excitotoxic molecule) has been associated with decreased ipsilateral epileptogenic hippocampal volume and history of increased frequency of seizures [99], but a causal link to epileptogenesis has not yet been demonstrated. Unfortunately, most longitudinal MRI epilepsy studies have had a small number of patients or limited follow-up. Therefore, long-term longitudinal documentation of these changes may help characterize the epileptogenic process per se in the future [94].

DWI

White matter is an integral part of the epileptic network and assessment of its integrity, as discussed in the animal studies, may offer further insight in understanding the epileptogenic process. DWI changes are thought to be an effect of ongoing neuronal damage representing downstream axonal degeneration. Correlation between duration of epilepsy and DWI abnormalities has been shown in some white matter tracts, especially in TLE without MTS [95]. In children with TLE there are reports of decreased FA in the hippocampi ipsilateral and contralateral to the seizure focus [7], in the uncinate fasciculus, arcuate fasciculus, internal longitudinal fasciculus, and cortical spinal tract, as well as increased mean diffusivity, but normal FA in the temporal lobe white matter and cingulate gyrus [95]. In patients with TLE there is reduced FA in the external capsule and corpus callosum [95]. When unilateral MTS is present, DWI shows more extensive, bilateral

decrease in white matter integrity [77] and bilateral fornix abnormalities [100].

In frontal cortical dysplasia (FCD) among patients with and without epilepsy, DWI abnormalities extend beyond the visible FCD abnormalities in both groups, but when white matter tracts projecting to and from the FCD were evaluated, those with seizures had more severe changes [101].

Following a single event of SE there was progressive atrophy of the left hippocampus with abnormal mean diffusivity over a period of 6 months thought to be secondary to delayed programmed cell death [100].

In a group of 5 children with epilepsy and large cavum septum pellucidum, use of DWI identified that the fornix body was consistently split into 2 bundles; the authors postulated a possible link to epileptogenesis, given the close association of the fornix to the limbic system [102].

DWI studies may prove a useful method for recording secondary cerebral damage, and more studies are needed to document the reproducibility of results and their potential prognostic utility in chronic epilepsy.

PET

[18F]FDG–PET

Metabolic dysfunction of neurons and glia is common in epilepsy and often specific enough to identify the seizure onset zone. As a measure of total glucose consumption [18F]FDG–PET is commonly used to identify hypometabolic areas [103].

In a series of patients with Sturge–Weber syndrome, transient interictal hypermetabolism on [18F]FDG–PET was documented in the posterior or frontal lobes within a short time before or after the onset of the first clinical seizures thought to be secondary to chronic ischemia inducing cortical damage and excitotoxicity. These changes were then followed by progressive loss of metabolism as epilepsy established itself [104].

A longitudinal study of 170 patients looking into long-term prognosis after hemispherectomy reported that hypometabolic abnormalities on [18F]FDG–PET may be a more reliable marker of potential independent epileptogenesis in the contralateral hemisphere than the structural abnormalities seen on brain MRI [105].

a-[11C]Methyl-L-tryptophan

a-[11C]Methyl-L-tryptophan tracer has been successful in children with tuberous sclerosis in differentiating epileptic from non-epileptic tubers. This particular radiotracer is interesting, as preliminary data suggest that its predilection to epileptogenic tissue may be due to increased focal activity of inflammatory pathways. Another radiotracer that has been

found in activated microglia is [11C]-(R)-PK11195. Given the fact that neuroinflammation plays a potential role in epileptogenesis, these tracers might be useful in tracking response to immunotherapy that is already available [106].

5-HT1A

Decreased 5-HT1A receptor binding correlated with the degree of epileptogenesis in regions involved in seizure onset and where discharges propagated. Reduced free fraction-corrected volume of distribution and significantly greater asymmetry was described in the fusiform gyrus, hippocampus, and parahippocampus ipsilateral to epileptic foci [7].

¹¹C-flumazenil

Complex mechanisms of epileptogenesis are characterized by metabolic and neurotransmitter/receptor disturbances. Functional impairment of inhibitory neurotransmission is probably a major factor. ¹¹C-flumazenil is a PET tracer that serves as a useful *in vivo* marker of central inhibitory GABA A-type benzodiazepine receptor. ¹¹C-flumazenil decreases are largely congruent with seizure onset zone and more severely depressed in the epileptogenic lesion than in adjacent cortex. Reductions have been described with various etiologies of seizures, in resected hippocampi, in spiking cortex, and in perilesional epileptogenic cortex with a highly variable pattern [107].

Single Photon Emission Computed Tomography

Single photon emission computed tomography (SPECT) studies use tracers sensitive to cerebral blood flow. One such tracer of central GABA-A benzodiazepine receptor binding is ¹²³I iomazenil. Studies in mesial TLE showed decreased binding that correlated with decreased neuronal density in the hippocampus and dentate gyrus. Similar changes were present in neocortical dysplasia, even in the absence of structural MRI lesions or SPECT studies evaluating cerebral blood flow [108, 109]. Among patients who had severe TBI, hypoperfusion in the temporal lobes 1 year after trauma, as measured with ^{99m}Tc hexamethyl-propyleneamine-oxime, correlated highly with the development of PTE [110]. However, despite this finding, no studies to date have suggested a role for SPECT as a biomarker for epilepsy.

MRS

MRS as a marker of epileptogenesis has primarily focused on measurements of the NAA/Cr ratio, reduction of which has been linked to neuronal mitochondrial injury and neuronal dysfunction.

In one study among patients with IGE, thalamic MRS imaging measuring NAA/Cr showed progressive thalamic neuronal dysfunction without volume decrease supporting the notion of abnormal thalamo-cortical circuitry as a substrate of seizure generation. There is significant reduction in thalamic NAA/Cr compared with normal controls that correlates with disease duration, but not the age of onset [111].

An intimate relation between interictal epileptiform discharges and reduction of the NAA/Cr ratio in the contralateral side has been described in MTLE patients, and it may be a possible marker of epileptogenesis of the contralateral side [112]; it has been associated with worse outcomes following epilepsy surgery [113]. Along the same lines, MRS in patients with TLE who failed to respond to the first AED trial had significantly lower NAA/Cr ratios compared with responders, possibly reflecting the different nature of the underlying epileptogenesis [90]. In one case of TLE with unilateral MTS there was normalization of the NAA/Cr ratio in the contralateral temporal lobe following successful temporal lobe resection [7], raising the possibility of a biomarker that could potentially track reversal of epileptogenesis.

Comparison of NAA/Cr data of 12 different limbic foci between resting controls and MTLE patients showed that although both groups shared a metabolic network between the thalami and hippocampi, in patients there was an additional metabolic covariance seen between the ipsilateral insula and basal ganglia. The authors postulated it may represent downstream metabolic injury linked to seizure spread, and it remains to be proven if this network plays a role in the late recurrence of seizures after epilepsy surgery [114].

fMRI

BOLD signal changes have helped identify epileptogenic networks that not only correlate with seizure foci, but which are also seen at sites distant from EEG foci [77]. Among MTLE patients, compared with resting controls, there is decreased basal functional connectivity seen in the epileptogenic medial temporal lobe [115–117]. Decreased functional connectivity has been described in left mesial TLE across a network that includes thalamic, brainstem, frontal, and parietal regions, as well as focally in the dorsal medial prefrontal cortex, mesial temporal lobe, and inferior temporal cortex compared with controls [7]. However, no conclusive studies have shown a direct correlation between the bold signal and seizure progression.

Taken together, PET, SPECT, MRS, and fMRI studies that detect cerebral function are proving to be more sensitive in identifying an “epileptic network” and offer a more dynamic look into the epileptogenic process, with some evidence also alluding to reversibility of findings following therapeutic interventions.

Future Directions and Conclusions

There is currently no therapy proven to prevent or reverse epileptogenesis in patients. To develop and implement such an intervention, the underlying disease mechanisms, and related biomarkers, must first be identified and validated. Therapies can then be discovered, implemented, and rigorously investigated in preclinical studies that make use of the epileptogenic biomarkers to monitor disease progression. If a biomarker is modified by therapeutic intervention, and this correlates with reversal of the epileptogenic process, these therapies and biomarkers may then be valuable as surrogate endpoints in well-designed clinical trials. As highlighted in this review, neuroimaging represents a non-invasive and clinically applicable technique that can contribute to each of these needs. Methods such as MRI, PET, MRS, fMRI, and DWI are capable of assessing, or have already been associated with, a number of pathophysiological changes occurring in epileptogenesis. Future preclinical and clinical studies that continue to identify and validate neuroimaging biomarkers, improve imaging methods, use multimodal imaging, and combine imaging with other validated techniques (e.g., EEG), will make further strides towards our better understanding of the epileptogenic process. There is also growing evidence from animal models that epilepsy is a preventable disorder (see [118] for a review), with the identification of promising anti-epileptogenic treatments, including rapamycin and sodium selenate [118, 119]. However, to maximize the translatability of these findings to human patients it is important that future preclinical anti-epileptogenic studies utilize valid and clinically applicable biomarkers, such as neuroimaging, in their assessment of these therapies [e.g., 120]. To date, the few human clinical trials investigating potential anti-epileptogenesis treatments have failed to demonstrate significant efficacy (see [121] and [122] for reviews). However, these failures have occurred in trials using therapies that lacked preclinical evidence of anti-epileptogenic effects and/or had major methodological shortcomings [121, 122]. In light of these failures, future anti-epileptogenic clinical trials should select a patient population with a high epilepsy risk or early in the disease process, include large sample sizes, employ a longitudinal study design with long observation periods, implement a treatment with strong preclinical evidence of anti-epileptogenic effects, and incorporate biomarkers, such as neuroimaging, that are reproducible, reliable, safe, and widely available [121, 122]. Neuroimaging provides promising epileptogenic biomarkers that are likely to play an integral role in our quest to develop interventions that are effective at preventing or reversing epilepsy.

Acknowledgments The authors declare there is no real or perceived conflict of interest. Full conflict of interest disclosures are available in the electronic supplementary material for this article.

Required Author Forms Disclosure forms provided by the authors are available with the online version of this article.

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