

# Sustained Delivery of Commensal Bacteria from Pod-Intravaginal Rings

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**Topical administration of live commensal bacteria to the vaginal tract holds significant potential as a cost-effective strategy for the treatment of sexually transmitted infections and the delivery of mucosal vaccines. Probiotic-releasing intravaginal rings (IVRs) embody significant theoretical advantages over traditional daily-dosage forms, such as sustained and controlled delivery leading to improved adherence to therapy compared to that of frequent dosing. The conventional IVR designs, however, are not amenable to the delivery of live bacteria. We have developed a novel pod-IVR technology where polymer-coated tablets (“pods”) of *Lactobacillus gasseri* strain ATCC 33323, a commensal microorganism of human origin, are embedded in silicone IVRs. The release rate of bacterial cells is controlled by the diameter of a delivery channel that exposes a portion of the pod to external fluids. *In vitro* studies demonstrated that the prototype devices released between  $1.1 \times 10^7$  and  $14 \times 10^7$  cells per day for up to 21 days in a controlled sustained fashion with stable burst-free release kinetics. The daily release rates were correlated with the cross-sectional area of the delivery channel. Bacteria in the IVR pods remained viable throughout the *in vitro* studies and formed biofilms on the surfaces of the devices. This proof-of-principle study represents the first demonstration of a prolonged, sustained release of bacteria from an intravaginal device and warrants further investigation of this device as a nonchemotherapeutic agent for the restoration and maintenance of normal urogenital flora.**

The burden of sexually transmitted infections (STIs) among women, particularly in resource-poor regions, highlights the urgent need for female-controlled cost-effective approaches to prevention and treatment (1). Strategies involving the administration of commensal bacteria to the vaginal tract are emerging as a promising platform to achieve these important goals (2). Probiotics, “live microorganisms which when administered in adequate amounts confer a health benefit on the host” (3), have been shown to promote and restore healthy vaginal microbiota in clinical trials (2–4). Both oral and intravaginal probiotic regimens for the prevention and treatment of bacterial vaginosis (BV) (5–8) and urinary tract infections (UTIs) (9, 10) have demonstrated clinical efficacy. Because probiotic lactobacilli express a number of characteristics that are antagonistic to pathogens but complementary to host immunity, their use has been proposed to improve reproductive health and pregnancy outcomes (11).

Commensal and attenuated pathogenic bacteria also are being developed as vectors for mucosal vaccines against STIs (2). *Listeria monocytogenes* is a promising candidate vaccine vector against HIV because it induces a strong cell-mediated immune response and can be readily manipulated to express viral antigens. Proof-of-concept studies have been performed using recombinant *L. monocytogenes* strains that express HIV Gag in feline (12) and nonhuman primate (13) HIV models. Similarly, human vaginal isolates of *Lactobacillus jensenii* were genetically modified to secrete functional two-domain CD4 proteins, thereby inhibiting HIV-1 entry into target cells in a dose-dependent manner (14). A recombinant *L. jensenii* organism expressing the HIV-1 entry inhibitor cyanovirin-N demonstrated a 63% reduction in the transmission of a chimeric simian HIV strain (SHIVSF162P3) following repeated vaginal challenges in macaques (15). *L. monocytogenes* expressing the H-2K(b) glycoprotein B peptide from herpes simplex virus 1 (HSV-1) triggered a robust CD8 T cell response providing protective immunity against HSV infection (16). Intravaginally administered recombinant *Streptococcus gor-*

*donii* and *Salmonella enterica* engineered to express antigens of human papillomavirus type 16 were evaluated in mice (17, 18) and cynomolgus macaques (19) in an effort to develop effective topical vaccines for cervical cancer. Recently, attenuated bacterial pathogens have been investigated as delivery vectors for heterologous antigens that may simultaneously vaccinate against two pathogens (20).

The intravaginal administration of probiotics traditionally has been achieved using a variety of dosage forms, including tablets (21), capsules (7, 8), suppositories (9), and tampons (22). Collectively, these approaches have led to detectable, but not optimally sustainable, levels of the delivered bacteria. In women, these levels may not be sufficient to overcome existing biofilms refractory to the administered organism. The topical delivery of commensal bacteria using intravaginal rings (IVRs) holds significant potential for female-controlled STI prevention and treatment. The microorganisms can be administered in a controlled manner in sustained-release formulations, and adherence issues are significantly reduced compared to daily dosing. Intravaginal rings are being explored for the delivery of small-molecule antiviral agents (microbicides) to protect against sexually contracted HIV (23) and HSV acquisition (24), as well as for the treatment of recurrent genital herpes (25). However, microbicidal IVR technologies based on the established matrix and reservoir designs (23, 26), in which the antimicrobial agent is dispersed and diffuses through

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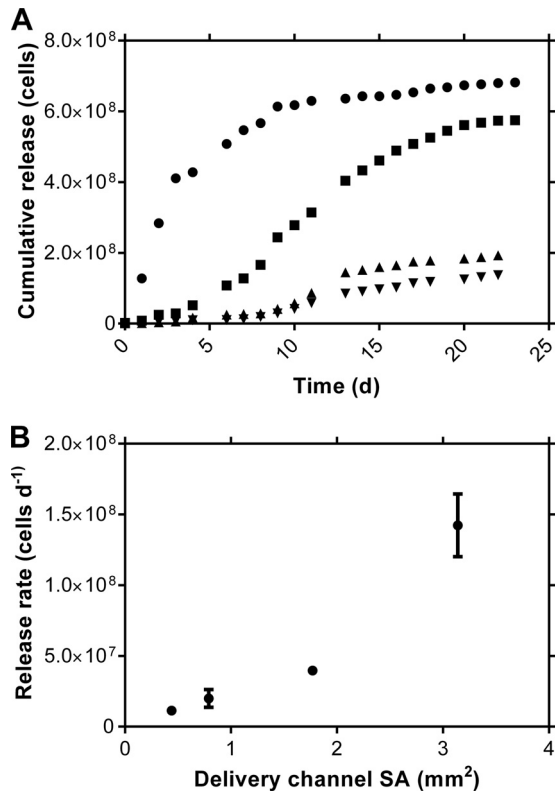
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**FIG 1** *In vitro* release kinetics of live *L. gasseri* from single-pod-IVR segments as a function of delivery channel size ( $n = 3$ ). (A) Median cumulative release versus time (●, 2.0-mm diameter; ■, 1.5-mm diameter; ▲, 1.0-mm diameter; ▼, 0.75-mm diameter). (B) Mean ( $\pm$  standard deviation) release rates as a function of delivery channel cross-sectional area (SA).

the ring elastomer, are not amenable to the delivery of live bacteria.

Consequently, we have developed a novel pod-IVR (27) formulated with the commensal organism *Lactobacillus gasseri* ATCC 33323, a neotype strain of human origin (28, 29). The sustained delivery of *L. gasseri* was obtained for up to 21 days *in vitro* with controlled-release kinetics. The bacteria remained viable in the IVRs throughout the study.

## MATERIALS AND METHODS

**Preparation of *L. gasseri* tablets.** *L. gasseri* (ATCC 33323) cultures were inoculated from frozen stock into de Man, Rogosa, and Sharpe (MRS) medium and incubated for 24 h at 37°C and 130 rpm. The cells were harvested via centrifugation for 30 min at  $3,000 \times g$  and 4°C. Pooled cell pellets (ca. 15 g) were dried by lyophilization, and the resulting powder was blended with sodium carboxymethyl cellulose (CMC) (25% [wt/wt]) by gentle tumbling for 24 h. The resulting mixtures were compacted into 3.0-mm (outer diameter) tablets in a manual pellet press (Parr Instrument Company).

**Manufacture of silicone intravaginal rings.** Human-sized polydimethylsiloxane (PDMS; silicone) pod-IVRs were prepared in a multistep process that has been described in detail elsewhere (27). Tablets containing ca. 30 mg of lyophilized *L. gasseri* (ca.  $7 \times 10^{14}$  cells) were coated with 5% (wt/vol) poly(D,L-lactide) in dichloromethane-ethyl acetate (1:1 [vol/vol]) to produce pods that were dried at room temperature for 72 h. The pods were embedded in IVRs (10 per ring) with a single mechanically punched delivery channel for each pod. The delivery channels were 2.0, 1.5, 1.0, or 0.75 mm in diameter, depending on the target release rate. The

IVRs were cut into single-pod segments for *in vitro* evaluation. The viability of the bacteria encapsulated in the IVRs was compared to that of the lyophilized material by culturing and typically exceeded 90%. The viability of the IVR bacteria after 21 days of evaluation *in vitro* (see below) remained at 90% relative to that of the lyophilized cells stored at 4°C.

**Bacterial enumeration.** The concentrations of bacterial cells in 150- $\mu$ l aliquots of release medium collected at predetermined time points were measured as a function of the optical density at 600 nm ( $OD_{600}$ ) in a 96-well format using a SpectraMax Plus absorbance microplate reader (Molecular Devices, Inc.). The  $OD_{600}$  reading was converted to the number of viable bacterial cells per ml of medium ( $N$ ) according to the equation  $N = 2.35 \times 10^8 \times 2.38 \times OD_{600}$ .

The factor  $2.35 \times 10^8$  represents the number of viable cells  $ml^{-1}$  providing an extinction of 1 absorbance unit (AU)  $cm^{-1}$  at 600 nm. This value was determined experimentally and is well within the normal range for bacterial cells (30). The factor 2.38 corrects the optical path length to the 150- $\mu$ l volume in a 96-well plate.

***In vitro* studies.** *In vitro* release studies were carried out in triplicate using procedures presented elsewhere (27). Briefly, the IVR segments were placed in dissolution medium consisting of 1 ml sterile  $1 \times$  phosphate-buffered saline (PBS; pH 7.2) and were incubated at room temperature ( $25 \pm 2^\circ C$ ) with shaking. The medium was replaced every 24 h and the segments were thoroughly rinsed with  $1 \times$  PBS before placing into fresh sterile release buffer.

**Bacterial viability.** The viability of the *L. gasseri* cells in the release medium was measured every 6 days by culture. The aliquots (150  $\mu$ l) were inoculated into 100  $\mu$ l MRS medium and incubated for 24 h at 37°C and 130 rpm. The  $OD_{600}$  of the resulting culture was used as a surrogate measurement of growth.

**SEM.** IVR segments with 2.0-mm-diameter delivery channels were incubated in release medium for 16 days at 25°C and 100 rpm. The segments were rapidly frozen by immersion in liquid propane and were prepared for scanning electron microscopy (SEM) as described previously (31, 32). Dehydration of the frozen segments was carried out by freeze-substitution in ethanol at  $-80^\circ C$ , followed by warming to ambient temperature and critical point drying. During this process, much of the biological material became detached from the IVR surface. The dried ring segments were cut lengthwise, mounted on metal specimen stubs, coated with a 10-nm-thick platinum film, and imaged using an XL30-SFEG 6 SEM (FEI Company, Hillsboro, OR) operating at 5 kV.

**Statistical analysis.** The data were analyzed using GraphPad Prism version 6.02 (GraphPad Software, Inc.).

## RESULTS

***In vitro* kinetic studies demonstrated sustained controlled release profiles for up to 21 days.** *In vitro* cumulative and daily release profiles (Fig. 1 and Table 1) from the *L. gasseri* IVR formulation exhibited burst-free sustained release, as is typical for pod-IVRs that deliver small molecules (27, 33, 34). The daily release rates, calculated from the linear portion of the cumulative release profile, displayed the expected (27) dependence on the delivery channel cross-sectional area (Fig. 1B).

**IVR bacteria remained viable, even after 21 days.** The viability of the *L. gasseri* bacteria in the IVR formulations was maintained

**TABLE 1** Daily *Lactobacillus gasseri* release rates as a function of IVR configuration

No. of viable cells	Daily bacterial release rate <sup>a</sup> for IVR delivery channel diam (mm) of:			
	2.0	1.5	1.0	0.75
$10^7$ viable cells per day	$14 \pm 2.2$	$4.0 \pm 0.15$	$2.0 \pm 0.63$	$1.1 \pm 0.26$

<sup>a</sup> Mean  $\pm$  standard deviation ( $n = 3$ ).

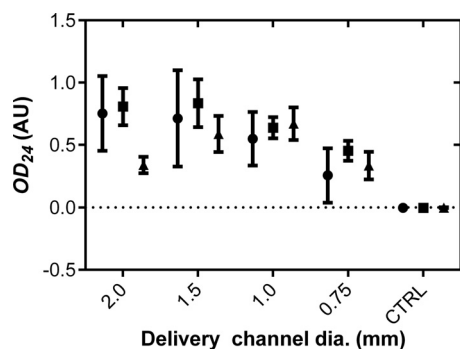


FIG 2 Viability of *L. gasseri* in IVR release medium at day 10 (●), day 12 (■), and day 21 (▲). The OD<sub>24</sub> readings correspond to the absorbance at 600 nm of MRS medium inoculated from the release buffer and incubated for 24 h at 37°C and 130 rpm. CTRL, negative control using MRS medium with no inoculation.

(90%, compared to lyophilized cells stored at 4°C), even after 21 days of incubation in release medium (Fig. 2). These results were confirmed by labeling (with the LIVE/DEAD BacLight bacterial viability kit; Life Technologies Corporation) the excised pod core and examining by fluorescence microscopy (data not shown). The concentration of viable cells in the release medium, measured in terms of the OD<sub>600</sub> (Fig. 2), was representative of the daily release rate at those time points (Fig. 1A).

***L. gasseri* biofilms form on the IVR surface.** Bacterial biofilms were clearly visible on *L. gasseri*-delivering IVR segments following prolonged incubation in PBS. These structures were delicate and readily detached from the IVR surface during handling. Two principal biofilm morphologies were observed by SEM examination of the cryopreserved specimens (Fig. 3): (i) open channels defined by bacteria embedded in extracellular polymeric substances (EPS) (Fig. 3A), sometimes linked by dense networks of nanofibers (Fig. 3B), and (ii) thick mats of aggregated bacteria (Fig. 3C). Bacterial mats also formed on the inner surface of the delivery channel (Fig. 3D to F).

## DISCUSSION

The pod-IVR design (27) contains a number of key unique features relevant to this study. The unmedicated structure that holds the bacterial pods can be made of any biocompatible elastomer (e.g., PDMS, ethylene-vinyl acetate copolymer, polyurethane, or latex), providing flexibility in material choice. In conventional IVRs, such as matrix and reservoir designs (23), including segmented (35, 36) and tubular (37, 38) configurations, the device elastomer forms an integral part of the delivery system controlling drug diffusion, an approach that is not amenable to the delivery of live bacterial agents.

The pod-IVR platform was specifically designed for the sustained delivery of multiple agents, each with independently and precisely controlled delivery rates (27). We have demonstrated in pig-tailed macaques that the drug release rate can be modulated over a wide range (34). A key feature of the pod-IVR design is its versatility in the agents it can deliver, with drug substances spanning the range from hydrophobic and hydrophilic small molecules (24, 25, 33, 34, 39) to high-molecular-weight highly water-soluble biomolecules (M. Gunawardana, M. M. Baum, A. M. Malone, T. J. Smith, and J. A. Moss, submitted for publication). Moss et al. reported (39) the design and 28-day pharmacokinetic

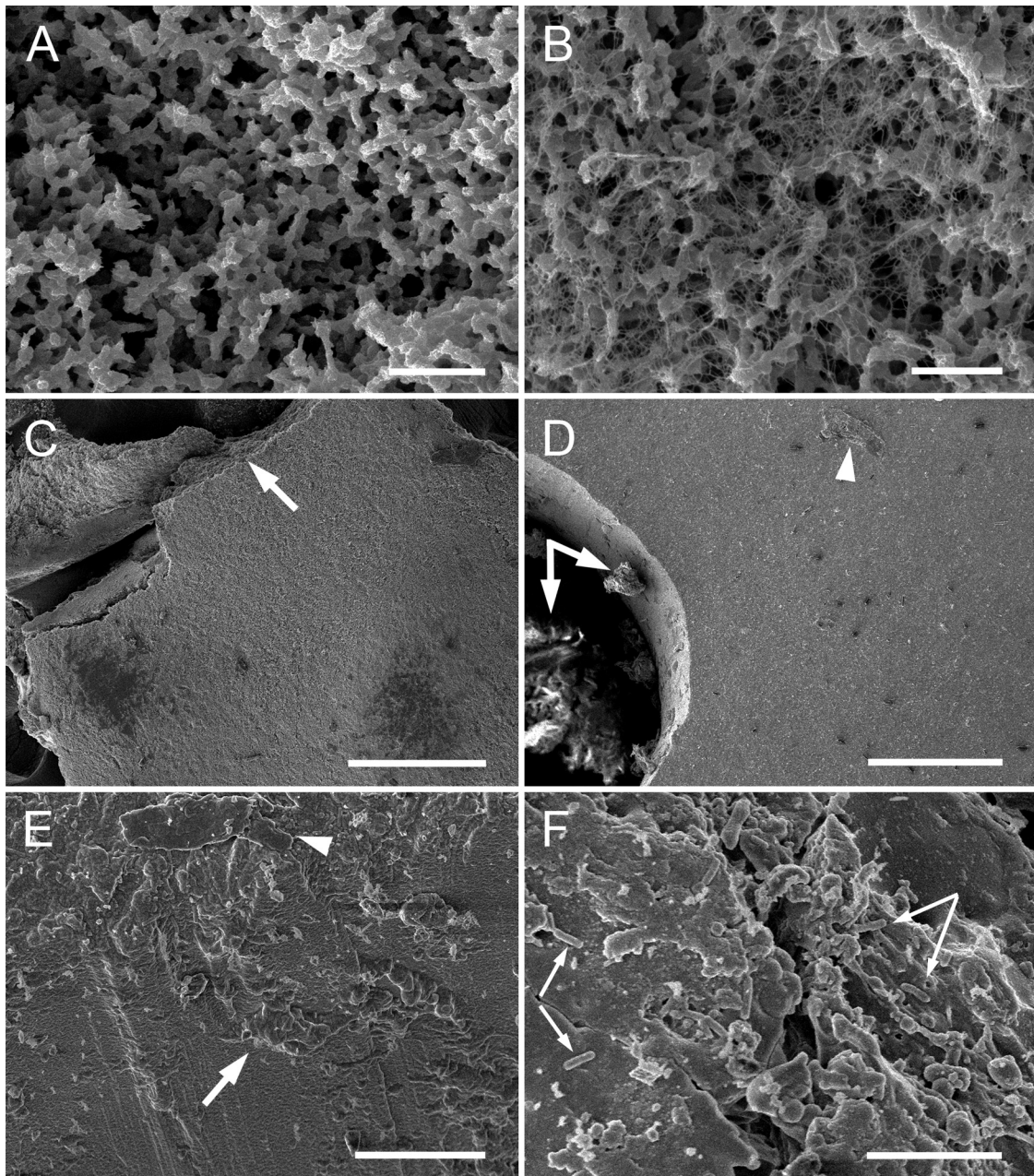
evaluation in sheep of a five-drug pod-IVR as a proof-of-concept advanced multipurpose prevention technology (MPT) that combines three antiretroviral drugs from different mechanistic classes with a proven estrogen-progestogen contraceptive for HIV and unintended-pregnancy prevention. No other IVR design has demonstrated the ability to deliver more than two agents. Pod-IVRs delivering antiviral agents have shown preliminary safety in pig-tailed macaques and women (25, 40), including culture-independent characterization of the vaginal microbiota (41). Based on the extensive *in vivo* track record of the pod-IVR design in rabbits (24), sheep (24, 33, 39), macaques (34, 40), and women (25, 41), no significant challenges are anticipated in translating the current IVR delivering commensal bacteria to *in vivo* studies.

Human-sized pod-IVRs can accommodate 10 polymer-coated bacterial tablets, containing up to 200 mg of material each, totaling 2 g per IVR. Each pod can theoretically deliver a different agent at an independently controlled release rate determined by the polymer membrane encapsulating the tablet and by the number and cross-sectional diameter of the delivery channels in the ring, as shown in Fig. 1B. We have demonstrated the simultaneous delivery of multiple agents at controlled rates from pod-IVRs *in vivo* (24, 39). The sustained delivery of multiple probiotics, such as the combination of *Lactobacillus rhamnosus* GR-1 and *Lactobacillus fermentum* RC-14 pioneered by Reid and colleagues (42), and probiotic bacteria in tandem with complementary drugs, such as estriol (43–45), a metabolic product of estradiol, and vitamin B complex (46), is possible using the pod-IVR platform.

Unlike oral probiotic dosage regimens (42), the intravaginal probiotic dose required to impact the vaginal microbiota has not been determined clinically; thus, the target probiotic delivery rates for sustained release intravaginal products have not been established. Table 2 summarizes the intravaginal probiotic doses used in a range of clinical studies. Orally administered formulations were not included due to the uncertainty of the vaginal dose received. Based on these data, a 28-day pod-IVR needs to deliver between  $0.6 \times 10^4$  and  $20 \times 10^8$  viable organisms per day, a range that is well within the capabilities of the pod-IVR platform discussed here (as supported by Fig. 1). A 10-fold increase in the release rate can be achieved simply by using 10 pods per IVR, and it can be increased further by using multiple delivery channels for each pod (27). Increasing the pod size from 30 mg, as described here, to 200 mg would provide sufficient bacterial loading to last 28 days.

The two *L. gasseri* biofilm architectures observed here showed morphological similarities with the phenotypes that were developed *in vivo* on pod-IVRs delivering antiviral agents in pig-tailed macaques (40) and women (25). In both cases, *Lactobacillus* spp. were well represented in the vaginal microbiota of the hosts (40, 41). The complete genome of *L. gasseri* ATCC 33323 has been sequenced (29), and interestingly, was found to encode 14 putative mucus-binding proteins, the highest number among the lactobacilli sequenced to date. In addition, the sequence data were suggestive of a putative exopolysaccharide gene cassette contributing to the features of the cell surface structure (29). These molecular findings are in agreement with our experimental observations regarding IVR surface colonization and biofilm formation by *L. gasseri* ATCC 33323. The open architecture (Fig. 3A), designated phenotype II (40), contained interwoven networks of uniform fibers (Fig. 3B) reminiscent of structures observed in monospecies *Pseudomonas* laboratory cultures (32). These so-called





**FIG 3** SEM images of *L. gasseri* biofilms that formed on IVR fragments *in vitro* following 16 days of incubation at 25°C at 100 rpm in PBS. (A and B) Biofilm morphologies displaying typical ultrastructural features of phenotype II (40), including regular open structures and nanowires. (D to F) Biofilms in the IVR drug delivery channel have a different morphology, resembling a dense bacterial mat, similar to phenotype I (40). (A) Bacteria, embedded in EPS, assemble into open architectures, including connective channels. Bar, 2  $\mu\text{m}$ . (B) Portions of the biofilm structures contain dense nanofiber networks attached to the branching bacterial aggregates. Bar, 2  $\mu\text{m}$ . (C) Biofilm fragment at low magnification consists of a thick mat of aggregated bacteria that readily detach from the IVR surface. The broken edge (arrow) represents the fragmentation line that developed during sample processing. Bar, 200  $\mu\text{m}$ . (D) The IVR delivery channel, at low magnification, contains a mass of material attached to the inner surface (arrows). Traces of material on the IVR surface also were present (arrowhead). Bar, 10  $\mu\text{m}$ . (E) The inner surface of the IVR delivery channel is covered with attached biological material. Bar, 20  $\mu\text{m}$ . (F) The attached biofilm contains bacteria (arrows). Bar, 10  $\mu\text{m}$ .

nanowires have been observed to be a consistent feature of bacterial biofilms (32, 47, 48). In our *in vivo* studies, the bacterial biofilms developed on epithelial cell monolayers covering the IVR surface (25, 40). Here, the biofilms easily became detached from the IVR surface during handling, possibly explaining why an epithelial cell monolayer was required to support *in vivo* surface ad-

hesion of the bacterial EPS. We observed no evidence that the biofilms affected the *in vitro* release rate of *L. gasseri*.

**Conclusion.** The delivery of *L. gasseri* from pod-IVRs in an *in vitro* model exhibited a controlled release of viable cells over 21 days. This proof-of-principle study demonstrates that the modular pod-IVR platform holds promise for the sustained release of

TABLE 2 Summary<sup>a</sup> of clinical trials involving intravaginal administration of probiotic formulations

Reference no.	Reason for treatment	Probiotic(s)	Dose(s)	Form	Regimen
49	BV	<i>Lactobacillus acidophilus</i>	5 × 10 <sup>8</sup> to 20 × 10 <sup>8</sup> CFU/ml	5 ml fermented milk product	2 × daily, 7 days
50	BV	<i>L. acidophilus</i>	1 × 10 <sup>8</sup> to 10 × 10 <sup>8</sup> CFU/ml	Capsule	2 × daily, 6 days
51	BV	<i>L. acidophilus</i>	>10 <sup>8</sup> CFU/ml	10–15 ml yogurt	2 × daily, 7 days; repeat after 1 wk
44	BV	<i>L. acidophilus</i>	≥10 <sup>7</sup> CFU	Tablet	1–2 × daily, 6 days
45	Vaginitis	Estriol	30 μg	Tablet	1 × daily, 6 days
		<i>L. acidophilus</i>	≥10 <sup>7</sup> CFU		
		Lactose	600 mg		
9	UTI	<i>Lactobacillus crispatus</i> GAI 98322	10 <sup>8</sup> CFU	Suppository	Every 2 days, 1 yr
7	BV	<i>Lactobacillus rhamnosus</i>	≥4 × 10 <sup>4</sup>	Capsule	1 × wk, 6 mos
8	BV	<i>L. rhamnosus</i>	6.8 × 10 <sup>8</sup> CFU	Capsule	1 × daily, 7 days on, 7 days off, 7 days on
		<i>L. acidophilus</i>	0.4 × 10 <sup>8</sup> CFU		
		<i>Streptococcus thermophilus</i>	0.8 × 10 <sup>8</sup> CFU		

<sup>a</sup> See reference 5.

beneficial bacteria to the vaginal tract and warrants further investigation as a nonchemotherapeutic agent for the restoration and maintenance of normal urogenital flora. Future *in vivo* evaluations of the devices will be critical to advance them through the development pipeline.

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