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A comparison of spectral quality in magnetic resonance spectroscopy data acquired with and without a novel EPI-navigated PRESS sequence in school-aged children with fetal alcohol spectrum disorders

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Abstract

Single voxel spectroscopy (SVS) can generate useful information regarding metabolite concentrations provided that the MR signal can be averaged over several minutes during which the subject remains stationary. This requirement can be particularly challenging for children who cannot otherwise be scanned without sedation. To address this problem we developed an EPI volume navigated (vNav) SVS PRESS sequence, which applies real-time head pose (location and orientation), frequency, and first-order B0 shim adjustments. A water-independent preprocessing algorithm removes residual frequency and phase shifts resulting from within-TR movements. We compare results and performance of the standard and vNav PRESS sequences in a sample of 9- to 10-year-olds from a South African cohort of children with fetal alcohol spectrum disorders (FASD) and healthy controls. Magnetic resonance spectroscopy (MRS) data in the deep cerebellar nuclei were initially acquired with the standard PRESS sequence. The children were re-scanned 1 year later with the vNav PRESS sequence. Good quality data were acquired in 73% using the

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vNav PRESS sequence, compared to only 50% for the standard PRESS sequence. Additionally, tighter linewidths and smaller variances in the measured concentrations were observed. These findings confirm previous reports demonstrating the efficacy of our innovative vNav sequence with healthy volunteers and young children with HIV and expand its application to a school-aged population with FASD—disorders often associated with attention problems and hyperactivity. This study provides the most direct evidence to date regarding degree to which these new methods can improve data quality in research studies employing MRS.

Keywords

magnetic resonance spectroscopy; motion correction; B0 correction; EPI navigator; fetal alcohol spectrum disorders; South Africa

Introduction

Single voxel spectroscopy (SVS) can provide useful information regarding metabolite concentrations when the spectra are acquired within the intended anatomy with a constant frequency and optimal main magnetic field (B0). Acquiring these spectra is usually straightforward, provided subjects remain stationary during the scanning session and scan adjustments are appropriately performed. However, when movement occurs, it can go undetected and lead to acquisition of spectra from the wrong anatomical regions and spectral artifacts, such as frequency shifts and line shape distortions. Several minutes of signal averaging may be necessary, which is often not possible for restless or uncomfortable children, particularly those with developmental brain disorders, such as attention deficit hyperactivity disorder (ADHD) or fetal alcohol spectrum disorders (FASD), among whom attention problems and hyperactivity are common (e.g., Coles et al. 1997; J. Jacobson et al. 2011; Mattson et al. 2011). We have previously demonstrated the benefits of using an echo planar imaging (EPI) volume navigated (vNav) Point Resolved Spectroscopy (PRESS) sequence with normal adult volunteer subjects (Hess et al. 2011; 2012) and with a sample of young HIV-exposed children (Hess et al. in press). In this study we extend these findings by demonstrating the benefits of using an EPI vNav PRESS sequence in a sample of 9- to 10-year-old school-aged Cape Coloured (mixed ancestry) children who are participating in a prospective longitudinal study on FASD in Cape Town, South Africa (Jacobson et al. 2008).

The vNav is capable of measuring within each TR head pose (location and orientation), zero-order B0 offset (implemented as RF transmit/receive frequency), and spatially higher-order B0 offsets (implemented with shim gradients of which the linear terms are adjustable in real time). We present a comparison of the results obtained with the standard and vNav PRESS sequences. In this comparison the spectra were obtained in a cerebellar volume of interest (VOI).

Head pose tracking is important in SVS as there is no way of confirming whether all measurements were acquired from the same volume. In this respect, spectroscopy differs from imaging, where blurring and artifacts are apparent in the resulting image in the presence of motion. In SVS, which uses large voxels, such as $20 \times 20 \times 20 \text{ mm}^3$, voxel shifts on the order of 2 to 3 mm may seem inconsequential. However, if the movement is

enough to alter the gray/white matter ratio, mechanisms for partial volume correction will be rendered invalid. By using the vNav to perform head pose correction, one can ensure that the measurements are consistently acquired from the same anatomical region.

FASD is characterized by a broad range of irreversible neuropsychological deficits, including poorer IQ—Full Scale IQ in children with FAS (Streissguth et al. 1990; Mattson et al. 1997; Jacobson et al. 2008, 2011) and problems in the Freedom from Distractibility domain comprised of Arithmetic and Digit Span in more moderately exposed children (Jacobson et al., 2004). Eyeblink conditioning is also exceptionally sensitive to prenatal alcohol exposure (Jacobson et al. 2008, 2011). Eyeblink conditioning, which has also been linked to effects of alcohol exposure in animals, is a cerebellar-mediated nonverbal classical conditioning paradigm, in which the subject learns to associate a conditioned stimulus, typically a pure tone, with a brief air puff to the eye (unconditioned stimulus) that elicits a reflexive blink. In the 5-year follow-up of our Cape Town Longitudinal Cohort, none of the children with full fetal alcohol syndrome (FAS) met criteria for conditioning, compared to 75% of the healthy controls; only 33.3% of the children with partial FAS (PFAS) and 37.9% of the heavily exposed nonsyndromal children met criteria for conditioning (Jacobson et al., 2008). These findings were subsequently confirmed in a school-aged cohort (Jacobson et al., 2011). FAS, the most severe form of FASD, is characterized by distinctive craniofacial dysmorphism (short palpebral fissures, thin upper lip, flat or smooth philtrum), small head circumference, and growth retardation (Stratton et al. 1996). PFAS is diagnosed when there is a history of heavy maternal drinking during pregnancy, the presence of two or more of the principal alcohol-related facial anomalies, and small head circumference, growth retardation, or cognitive and/or behavioral dysfunction (Hoyme et al., 2005).

The most recent studies of the incidence of FAS and PFAS combined in the Cape Coloured population in the Northern and Western Cape Provinces of South Africa has been estimated to be 88–89 per 1000, which is among the highest in the world (May et al. 2007; May and Gossage 2011; Urban et al. 2008). This population, composed mainly of descendants of white European settlers, Malaysian slaves, Khoi-San aboriginals, and black Africans, has historically comprised the large majority of workers in the wine-producing region of the Western Cape. The high prevalence of FAS in this community is a consequence of very heavy maternal drinking during pregnancy (Croxford and Viljoen 1999), which is due to poor psychosocial circumstances and the traditional *dop* system, in which farm laborers were paid, in part, with wine. Although the *dop* system has been outlawed since the 1920s, heavy alcohol consumption persists in a high proportion (~30%) of women during pregnancy in this community (Jacobson et al. 2006; Jacobson et al. 2008) despite extensive efforts to intervene to reduce pregnancy drinking.

The high prevalence of heavy alcohol consumption during pregnancy in a single cohort is unusual and led to our conducting the first prospective study of FAS beginning in pregnancy (Carter et al. 2005; Jacobson et al. 2008; Molteno et al. in press). Within the context of this research program, we conducted the first functional MRI studies in South Africa (Cheng et al. in press; Diwadkar et al. 2013; Meintjes et al. 2010), which contributed to the establishment of the research-dedicated Cape Universities Brain Imaging Centre (CUBIC). Extensive pediatric neuroimaging research is currently being conducted by numerous

research groups at CUBIC, including development of innovative methodological techniques, such as the one examined here. In this study, magnetic resonance spectroscopy (MRS) was administered initially to a sample of 56 nonsedated children from our longitudinal FASD cohort with a standard PRESS sequence at age 9 years and again 1 year later with the novel vNav PRESS sequence, providing a unique opportunity to examine the degree to which the latter can improve spectral quality.

The aim of the present study was to compare the quality, accuracy, and measurement variance in the spectroscopy data acquired in these nonsedated school-aged children with FASD using the standard and vNav PRESS sequences.

Methods and Applications

Study Participants

The sample consisted of 59 Cape Coloured children (30 males, 29 females) born between 1999–2001 whose mothers were recruited during pregnancy to participate in a longitudinal study of FASD (Jacobson et al. 2008). Forty-three of these children were heavily exposed prenatally to alcohol; of the 16 healthy controls, 15 were born to women who abstained from drinking and 1 to a woman who drank minimally during pregnancy (i.e., 2 drinks on 3 occasions). The mothers who drank during pregnancy averaged 1.0 oz absolute alcohol or the equivalent of 2 standard drinks/day (Table 1). However, they concentrated their drinking to 1–2 days/week, thereby consuming an average of 7.1 standard drinks/occasion. In 2005 we organized an FASD diagnostic clinic in which each of the children were examined by two expert dysmorphologists: 9 (20.9%) of the heavily alcohol exposed children were diagnosed with FAS; 19 (44.2%) with PFAS; 15 (34.9%) were classified as nonsyndromal heavily exposed (HE) children. As expected, heavy drinkers smoked more than controls. Only three women reported using marijuana during pregnancy, one used cocaine, and none used methaqualone (“mandrax”). IQ was assessed on the Wechsler Intelligence Scale for Children-IV (WISC-IV; Wechsler, 2003) at 9 years (see detailed description in Jacobson et al., 2011 and Diwadkar et al., 2013). As we have previously reported (e.g., Jacobson et al., 2008, 2011), there was a dose-dependent effect of prenatal alcohol on the WISC IQ test. In 2009, when the children were 9.4 years of age ($SD=0.4$), data were acquired from 56 of the children in the deep cerebellar nuclei (Fig. 1) using a standard PRESS sequence. In 2010, when the children were 10.4 years ($SD=0.4$), MRS scan data were acquired from 52 children in the same region using the EPI volume navigated (vNav) PRESS sequence. Table 1 presents the breakdown per group for the populations scanned in 2009 and 2010.

Scan Protocol and Subject Preparation

Pre-scan preparation included practice in a mock scanner where each child was exposed to the noises and feeling of being in a tunnel, followed by a tour of the scanner. The child was then given the choice of whether to continue with scanning or not. It was made clear that s/he could terminate the scan at any time should s/he wish and that a research nurse/assistant would be present in the scan room at all times. During both scans, the child watched a video (e.g., *Finding Nemo*), using standard headphones. Heads were tightly packed in the head coil with foam pillows to minimise head motion. All scans were acquired according to protocols

that had been approved by both the Faculty of Health Sciences Human Research Ethics Committee at the University of Cape Town and the Institutional Review Board of Wayne State University. The mother or father provided written informed consent; all children provided oral assent.

All scans were acquired on a 3T Allegra (Siemens, Erlangen, Germany) MRI scanner with a birdcage transmit-receive head coil. The protocol consisted of (1) a three plane localiser, (2) a vNav set sequence (duration 1 s), which sets the navigator position, acquired only for the 2010 scans that used the vNav PRESS sequence, (3) T2 weighted acquisitions in three orientations to localise the cerebellar deep nuclei due to signal loss in this region arising from iron deposits (Dimitrova et al., 2006) (TR = 2 s, TE = 88 ms, Echo Train Length = 5, slice thickness = 3 mm, and resolution $0.9 \times 1.2 \times 3 \text{ mm}^3$), and (4) the SVS acquisition using either the standard PRESS acquisition (2009) or the vNav PRESS sequence (2010). PRESS scan parameters were voxel size $20 \times 12 \times 16 \text{ mm}^3$, 128 measurements, TE = 30 ms, TR = 2 s, and bandwidth = 1000 Hz. Vector sizes of 1024 and 512 were used for the standard and vNav PRESS sequences, respectively.

The vNav uses Prospective Acquisition CorrEction (PACE) (Thesen et al. 2000) to register each navigator to the navigator from the first TR (post preparation scans) in order to correct head pose. In addition, the sequence employs a dual-contrast 3D EPI sequence module to generate within each TR a B0 field map and calculate the absolute frequency and first order B0 gradient for the intended VOI. In this manner the absolute head position, frequency in the VOI, and first-order shim in the VOI are updated by the navigator each TR. Additionally, a frequency and first-order shim appropriate to the larger field of view of the navigator itself are calculated and applied to each TR.

The vNav protocol was as follows: resolution $5 \times 5 \times 5 \text{ mm}^3$, FOV $220 \times 200 \times 110 \text{ mm}^3$, matrix 44×40 , 22 partitions, TE₁ 8 ms, and TE₂ 12.8 ms, TR 21 ms, flip angle 2°, bandwidth 3906 Hz/px. The orientation was set by the operator and chosen to cover the intended VOI in addition to maximally covering the brain, as shown in Figure 1. The duration of the vNav sequence module was 966 ms and the online processing, including pose, frequency, and shim calculations, took 170 ms per navigator.

Offline phase- and frequency-corrected averaging

We developed a method to perform offline frequency- and phase-corrected averaging. This method, which is independent of the residual water in each FID, consists of three steps: i) residual water peak removal, ii) frequency detection by cross-correlation with a simulated spectrum, and iii) complex combination weighting determined by singular value decomposition (SVD). All processing is performed in the spectral domain and upsampled to a frequency resolution of 0.49 Hz. Prior to any processing, a copy of the spectrum acquired in each TR without any water editing is retained for the final averaging. Water peak removal is necessary before preprocessing as it improves the cross-correlation baseline and more importantly prevents fluctuations in the water saturation from biasing the SVD. A comprehensive model spectrum was simulated using jMRUI NMR Scope (Graverondemilly et al. 1993) for the same sequence described above and a linewidth of 2 Hz. The model spectra included choline, creatine (Cr), phosphocreatine, phosphocholine, GABA,

glutamate, glutamine, myo-inositol (INS), N-acetylaspartate (NAA), and N-acetylaspartylglutamate (NAAG). The range of -3.5 ppm to -1 ppm was cross-correlated with each spectrum to detect its frequency offset and thus re-align both the original (non water-edited) and water-edited spectra appropriately.

SVD is applied in the range -3.5 ppm to -1 ppm to the water-edited and frequency-adjusted spectra. The output of the SVD operation is the set of matrices \mathbf{U} , \mathbf{S} , and \mathbf{V} , where \mathbf{U} and \mathbf{V} describe the right and left singular vectors, entries on the diagonal of \mathbf{S} are the singular values, and \mathbf{USV}^T equals the input spectra. The first row of \mathbf{V} is a complex set of weights applied to each non-water edited spectrum (\mathbf{O}_s), which are summed and multiplied by the mean of the first row of \mathbf{V} . This process regenerates the left hand singular vectors using the original unedited spectra with appropriate scaling.

The preprocessing steps described above could only be applied to the scans that employed the vNav because scans acquired with the standard PRESS sequence did not record individual measurements prior to averaging.

Spectral Analysis

The first criterion in determining the success of a technique is how much of the data is usable. Our criteria for exclusion of data were linewidths greater than 0.08 ppm (9.9 Hz) or signal-to-noise ratio (S/N) less than 8 . We also added a visual check of the spectra to ensure they conformed to the spectral plot expected (i.e., no large unknown signals or other type of interference). The excluded data were eliminated from further processing.

The vNav records the motion and shim corrections applied in a log file. These logs were used to calculate the absolute position of the SVS voxel relative to the initial reference position throughout the scan, and thus determine the extent of subject movement during the scan.

All metabolite analyses were performed in LCModel (Provencher 2001), where a water reference spectrum was used for water and eddy current correction. The measures used from LCModel were the metabolite concentrations, their percent standard deviation (%SD), linewidth, and S/N.

Results

Only 28 of the 56 scans acquired in 2009 without the vNav provided spectra of suitable quality (50% success rate); whereas in 2010, with the vNav, 39 of the 41 (95%) completed scans provided spectra of suitable quality (Fig. 2), i.e., only two of the scans did not meet our quality criteria. Spectra for 11 subjects were not acquired at the second scan due to navigator-related failures listed in Table 2, giving a 73% success rate from the total of 52 scans. Using the standard PRESS acquisition, only 33.3% of the children with FAS provided good spectra, compared with 57.1% of the controls. Using the vNav PRESS, good spectra were obtained from 71.4% and 75.0% of the children with FAS and controls, respectively, with all failures resulting from technical difficulties with the vNav. The proportion of good spectra for the PFAS children increased from 50.0% to 83.3%; for the heavily exposed

nonsyndromal, from 60.0% to 66.7%. Thus, whereas the vNav PRESS was associated with improved spectral quality within all four groups, the benefit was greatest for the most severely affected FAS group.

The reference vNav volume and associated field map for one of the scans is shown in Figure 3. To quantify the extent to which the scans were affected by motion, we have plotted box-and-whisker plots of the maximum absolute vector translations and rotations of the child's head from the start of the scan, expressed firstly about the centre of the navigator volume, representing gross head translation and rotation, and secondly about the centre of the SVS voxel, translations only. (Fig. 4). Displacements were calculated using the motion estimates of the vNav that are recorded in a log file. None of the scans exhibited more than 3 mm maximum absolute voxel displacement.

Figure 5 compares the mean and standard deviation of the linewidth and S/N using the standard and navigated PRESS sequences. There is a clear improvement in both the mean linewidth ($p = 0.03$) and S/N ($p = 0.0001$) in the 2010 scans compared to the 2009 scans.

Over and above the quality measures of linewidth and S/N, we wanted to assess the consistency of the measured metabolite concentrations. To compare the variance and range of metabolite concentrations, we have plotted box-and-whisker plots in Figure 6 of the concentrations in the nonalcohol-exposed control children for the 2009 (standard PRESS) and 2010 (vNav PRESS) scans, respectively. Data points were excluded from this plot if % SD exceeded 30%. The following metabolites are shown: NAA, INS, Cr, NAAG, and guanidoacetate (GUA).

Discussion

This study provides new evidence for the efficacy of our EPI volume navigated single voxel spectroscopy PRESS sequence for school-aged children with developmental brain disorders, such as FASD and ADHD that may make it difficult for the participant to remain stationary over the several minutes required by the MRS scan. This new PRESS sequence applies real time head pose (location and orientation), frequency, and first-order B0 shim adjustments. The present study extends our previous findings in which our novel vNav PRESS sequence was used successfully with healthy volunteers (Hess et al. 2011; 2012) and with young children with HIV (Hess et al. in press) to a pediatric population with FASD. In a direct comparison of the quality of the data generated by the standard and vNav PRESS sequences, we found a 50% increase in the number of usable scans, as well as significant improvements in linewidth and S/N. As reported above, the improvement was greatest in the most severely impaired group—children with full FAS—who had provided the fewest usable scans (only 33%) using the standard PRESS acquisition. Thus, these data provide support for the suggestion that the SVS motion correction may be especially useful in studies of difficult or developmentally disabled populations of children, who may be prone to inattention or difficulty inhibiting movement.

While prospective frequency adjustment corrects the system frequency for TR-to-TR changes, pose changes within TR may still result in both residual frequency and phase

variations. These phase variations result from the velocity encoding effect of the PRESS (or STEAM) gradients. Detecting the frequency and phase shift of each measurement enables constructive averaging. Methods that use the residual water signal within the spectra (Ernst and Li 2009; Helms and Piringer 2001; Star-Lack et al. 2000) or a high signal metabolite peak to detect the frequency and phase for each measurement (Gabr et al. 2006; Waddell et al. 2007) have been proposed. In cases where complete water suppression is employed, the frequency and phase of the residual water may be misleading due to the relative shift in the suppression band that results in asymmetric water saturation. We present a post-processing technique that is independent of the residual water and uses the spectral range from -3.5 ppm to -1 ppm for both frequency and phase correction.

In the first scan, standard PRESS without the vNav, only 50% of the spectra were usable due to poor spectral quality. As no motion tracking was performed, we can only speculate as to the reason for these failures. We suspect that the main problem was poor B0 shimming in the cerebellar VOI. In the follow-up scan performed 1 year later with the vNav, no significant motion correction was applied (motion never exceeded 3mm), and yet 73% of subjects scanned yielded good data. In contrast to the standard PRESS acquisitions, the vNav PRESS sequence provided good spectral quality in all but two scans with the remaining failures occurring as a result of technical failures with the new sequence. These technical failures would not have been present in a standard PRESS sequence. These failures are discussed below and solutions are suggested to prevent them from happening in the future. Some portion of this improvement in spectral quality may be attributable to the increased maturity of the subjects (1 year), and their past experience in the scanner may have made them less restless. However, these factors do not seem sufficient to explain an improvement of this magnitude, particularly since, as we have reported in a subsequent study, more optimal linewidths were seen in a sample of 5-year-old children with HIV when they were scanned for the first time using vNav PRESS (Hess et al. in press). We, therefore, conclude that the combination of vNav shimming with offline frequency and phase correction are primarily responsible for generating the higher quality spectra. The scans within quality bounds saw a mean linewidth reduction of 1.2 Hz and an S/N improvement of 2.5 (from 9.6 to 12.1) when using the vNav and offline preprocessing. The effect of this improvement in spectral quality is apparent with the reduced range and variance of several metabolites, as shown in Figure 6.

We encountered three causes of failures for the vNav scans. The first and most prevalent ($n=5$) was observed in the EPI B0 field maps of the vNav, where an error in the phase unwrapping resulted in a 208 Hz (2π) phase offset at the cerebellar voxel of interest. This type of error is typical in B0 field maps of this kind where no absolute reference frequency is present. We have since introduced a simple algorithm to avoid this problem in the future. The algorithm uses the prior knowledge that in the first vNav image, before any shim manipulation, the SVS voxel has a frequency offset of 0 Hz, as adjusted by the scanner. It should be noted that this failure has not been observed in other ROI's that are within the cerebrum and is exaggerated by the proximity of the cerebellum.

The second failure of the vNav PRESS sequence ($n=4$) was also specific to the cerebellum. It arises due to the presence of significant ghosting and distortions in the vNav volumes that

render the B0 field maps unusable to calculate a vNav-specific B0 shim. All four scans that failed in this manner had at least one second order shim term set greater than $1650 \mu\text{T}/\text{m}^2$, which approaches the shim gradient limit. We believe that these large second-order shim gradients gave rise to EPI ghosts and distortions. From experience, increasing the volume over which the scanner adjusts these second order terms could provide more stable and less extreme values. In the future the B0 shimming algorithm used to calculate the higher order B0 shims should be reasonably constrained, or improved high order shim gradient amplifiers and waveform generators should be used for real time adjustment of these gradients.

The third failure of the vNav PRESS sequence ($n=2$) was the result of substantial water over-suppression, resulting in a water saturated spectrum. Over-suppression was identified because the residual water had a π phase shift from the water sample spectrum of the same voxel. The navigator estimated a shim magnitude of $350 \mu\text{T}/\text{m}$; this is an offset from that set by the scanner. It is possible that the subject was in a different position or moving during the scanner's shim and water suppression optimisation process, leading to a substantially different optimal shim to that at the start of the SVS scan.

The navigator tracks a subject's movement and maintains a subject-specific coordinate system during the scan, defined by the reference TR. None of the children moved enough to cause a voxel shift greater than 3 mm during the scan. They did, however, exhibit small movements as shown in Figure 4. These were generally within a single TR, similar to what might be expected from swallowing or coughing.

The offline correction software presented here has been found to be simple and robust, requiring no user interaction. The advantage of cross-correlating a spectral range with a simulated spectrum is that it combines the contributions from several metabolites to find the frequency, thus making it robust to noise and variations in the residual water. The choice of SVD to calculate weights for weighted averaging enables the effective minimisation of spectra that do not fit the spectral trend, such as those perturbed by rapid movement. Further, as the SVD operation is performed on complex data, the weights generated are inherently complex, enabling phase-coherent averaging.

Conclusions

We have demonstrated marked improvement in the successful acquisition of MRS data in school-age children when acquisitions using the standard PRESS sequence are compared with those acquired using vNav PRESS. The vNav PRESS sequence, which improved spectral quality for all the children, enabled us to acquire usable data even from the most severely affected children with FAS. The vNav provides a consistent within scan VOI location while maintaining an optimal B0. We have demonstrated improved spectral quality when using the vNav in conjunction with offline preprocessing software as well as a reduced range and variance of metabolite concentrations. These benefits come at no extra time investment to the end user and no technical or additional equipment costs when scanning in standard brain regions.

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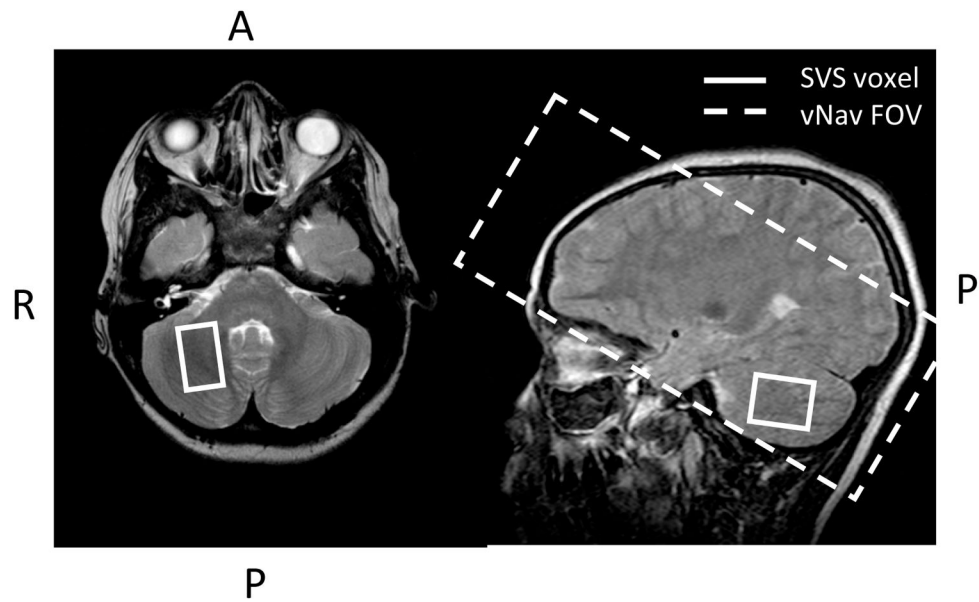


Fig. 1.
A) SVS volume of interest in the cerebellar deep nuclei, shown overlaid on the corresponding localising T2 turbo spin echo images B) Navigator FOV placement for scans with VOI in the cerebellum, it is angulated to ensure coverage of the cerebellum without increasing navigator duration

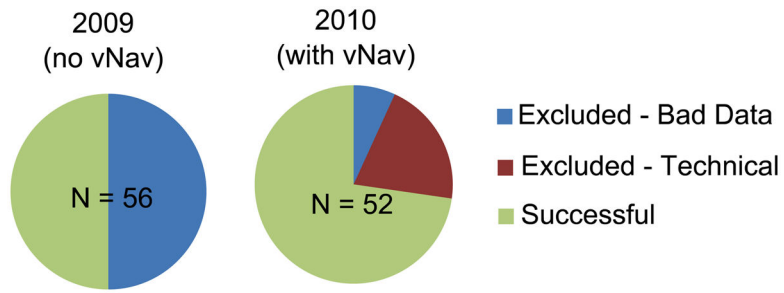


Fig. 2.
Pie charts showing the proportion of data excluded from each of the data sets due to either bad quality spectra or technical failures of the navigator

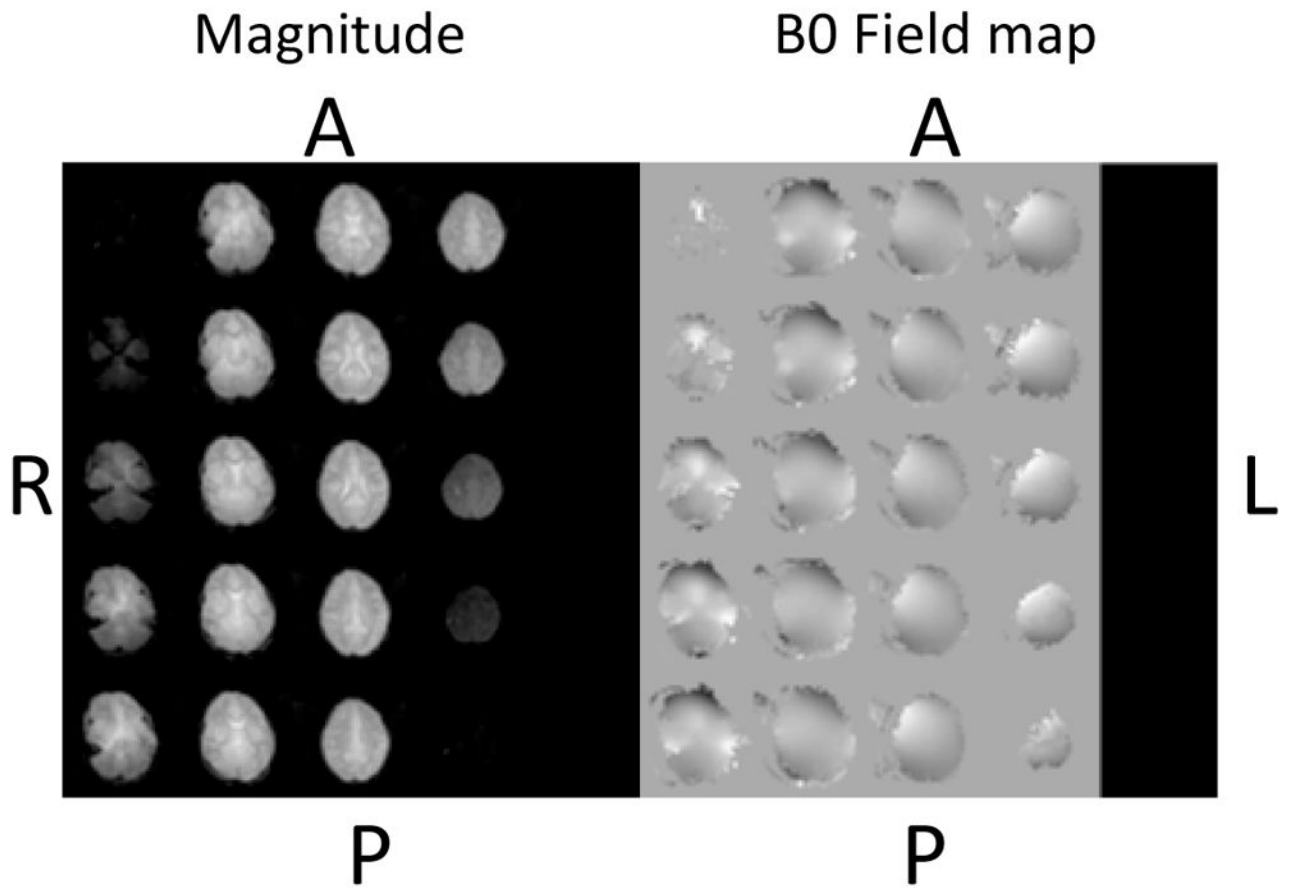


Fig. 3. Navigator: magnitude image of first echo (used for PACE motion estimation) (left) and unwrapped field map (right)

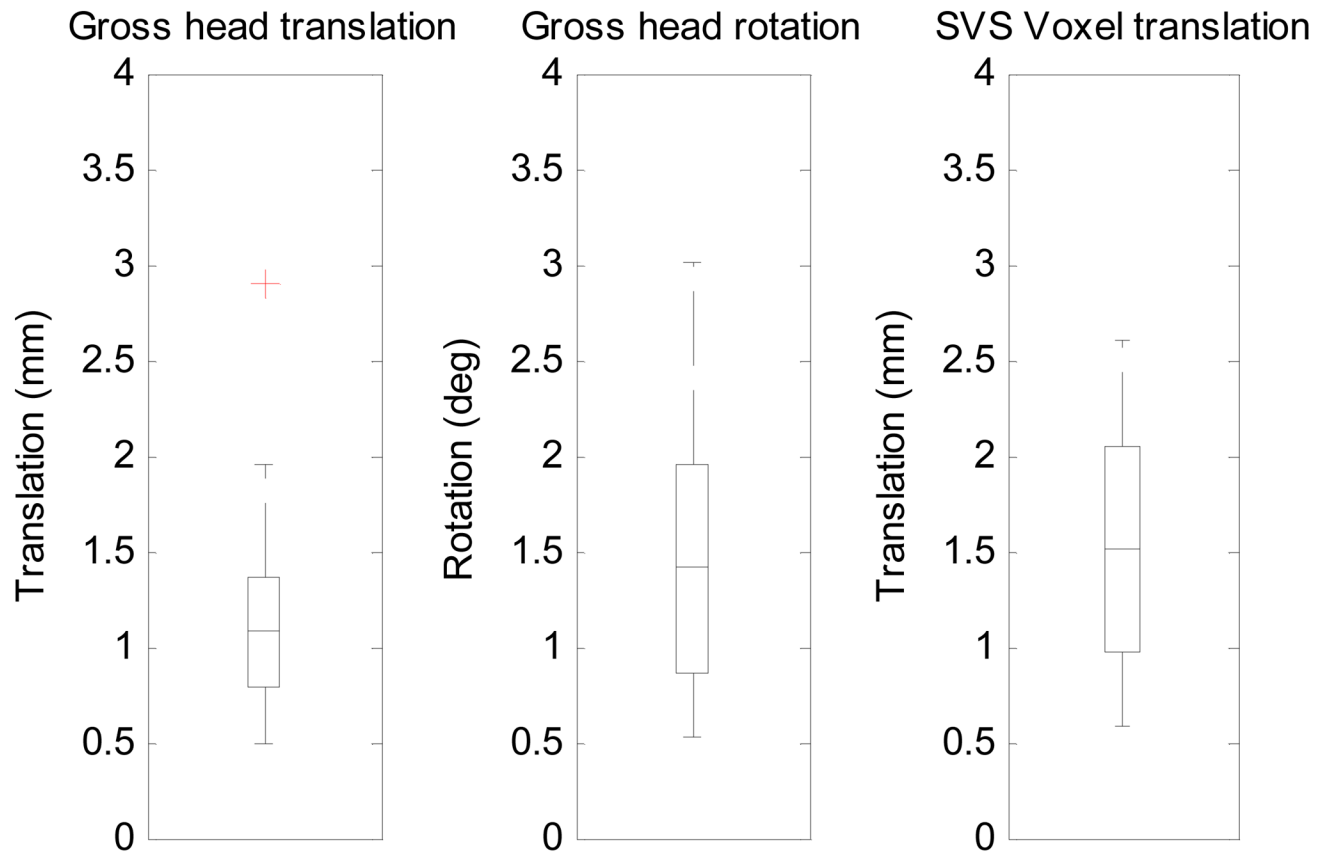


Fig. 4. Box-and-whisker plots showing of the maximum absolute vector translations and rotations of the child's head from the start of the scan, expressed firstly about the centre of the navigator volume, representing gross head rotation and translation, and secondly about the centre of the SVS voxel, translations only.

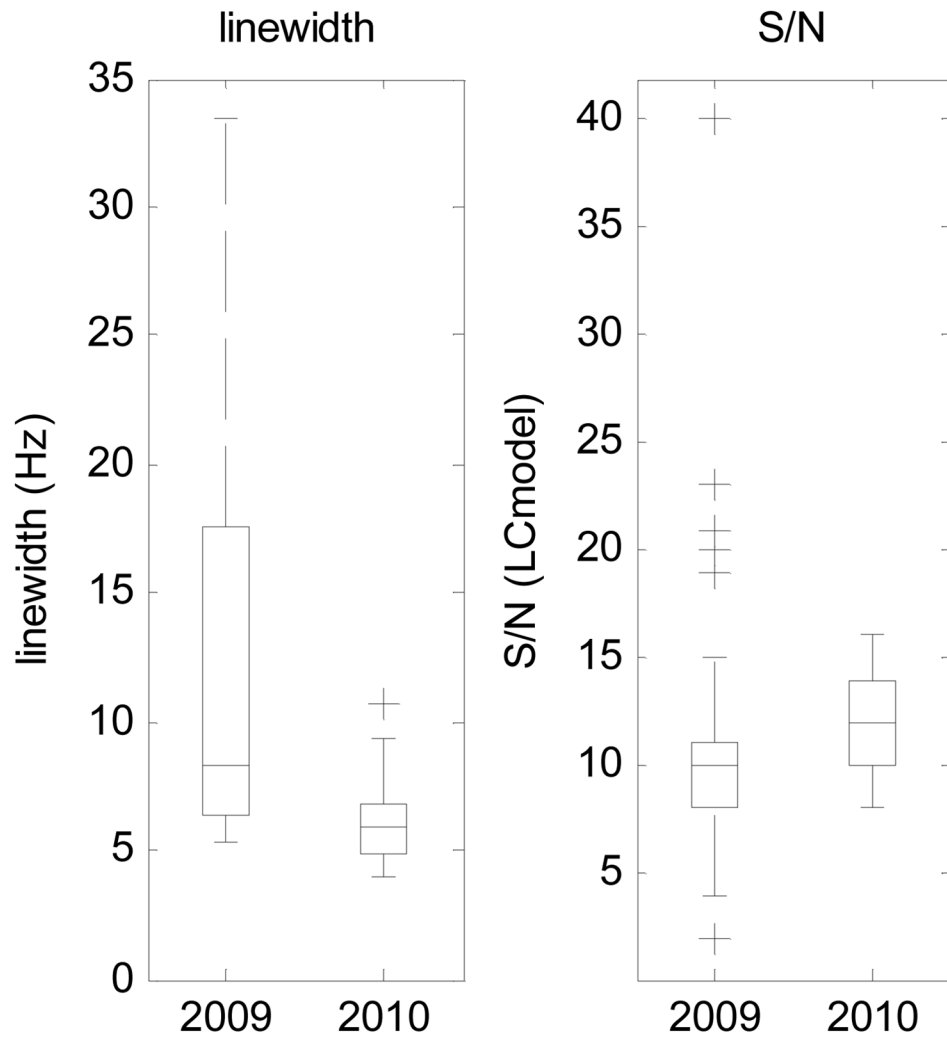


Fig. 5. Box-and-whisker plots of linewidth and signal-to-noise ratio (S/N), as measured by LCModel, for all scans without the vNAV (2009) and all scans with the vNAV (2010)

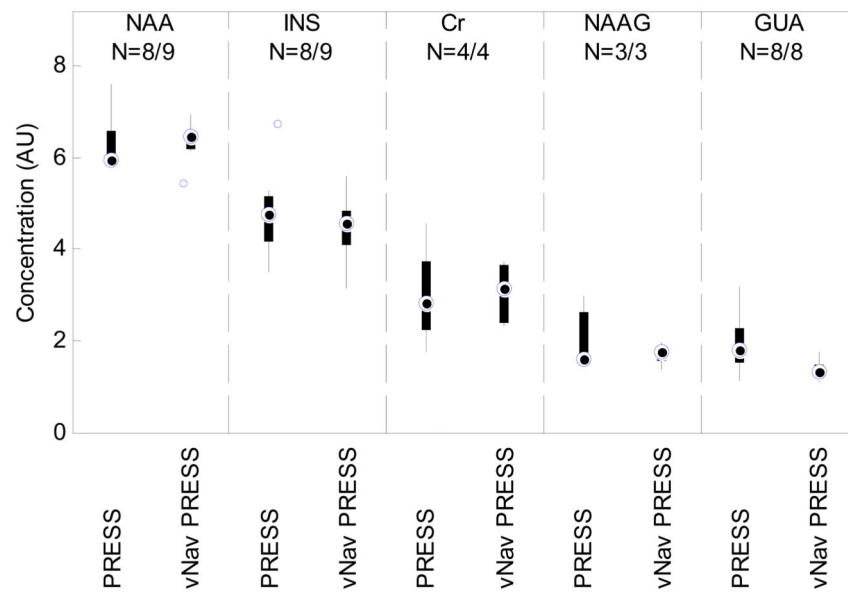


Fig. 6. Box-and-whisker plots comparing the variance and range of metabolite concentrations in control children using the PRESS (2009) and vNav PRESS (2010) sequences. Data points were excluded if their %SD exceeded 30% with the resultant number of data points given by N.

Maternal and child background characteristics and prenatal exposure to alcohol, smoking, and marijuana by FASD diagnostic groups ($N = 59$)

Table 1

	FAS ($N = 9$)	PFAS ($N = 19$)	Heavy exposed ($N = 15$)	Controls ($N = 16$)	F or χ^2
Maternal characteristics					
Education (years)	8.1 (1.7)	6.6 (2.3)	8.6 (2.9)	10.6 (1.6)	8.98***
Marital status (% married)	22.2	15.8	33.3	56.3	7.00 [†]
Child characteristics					
Gender (% male)	33.3	57.9	53.3	50.0	1.54
Age at scan 1 (years)	9.3 (0.3)	9.4 (0.3)	9.6 (0.6)	9.4 (0.4)	1.61
Age at scan 2 (years)	10.0 (0.5)	10.5 (0.4)	10.5 (0.3)	10.3 (0.3)	2.93*
WISC-IV IQ ^a	64.4 (8.6)	64.1 (10.2)	73.1 (8.0)	76.4 (9.1)	6.96***
Prenatal exposure					
Cigarettes/day	7.7 (5.7)	7.7 (6.0)	8.1 (7.1)	2.2 (5.3)	3.39*
Alcohol ^b					
Absolute alcohol/day	1.8 (2.2)	1.0 (0.7)	0.5 (0.5)	0.001 (0.003)	7.55***
Absolute alcohol/occasion	4.8 (1.8)	3.6 (1.9)	2.7 (1.6)	0.1 (0.3)	23.60***
Frequency (days/week)	2.1 (1.8)	1.9 (1.1)	1.0 (0.9)	0.01 (0.02)	12.65***

Values are mean (SD) or %. 56 children were scanned in 2009 (9 FAS, 18 PFAS, 15 heavy exposed, 14 controls), and 55 in 2010 (7 FAS, 18 PFAS, 15 heavy exposed, 12 controls)

^aBased on Wechsler Intelligence Scale for Children, 4th Edition.

^b1 oz absolute alcohol = the equivalent of about 2 standard drinks.

[†] $p < .10$

* $p < .05$

** $p < .01$

*** $p < .001$

Table 2

Technical failures of the vNAV by group for the 52 children scanned using the vNav PRESS acquisition in 2010.

Number of scans affected	Description	Total Exposed (FAS, $N = 37$)	Total Controls ($N = 15$)
5	Phase unwrapping algorithm generated a 2π phase offset, resulting in a frequency shift of 208 Hz. This rendered water suppression ineffective.	3	2
4	Ghosting in the first vNav EPI volume rendered the vNav unusable. This resulted from large shim terms set by the scanner for the voxel.	3	1
2	Water substantially over-suppressed (50% in these cases) as a result of a suboptimal pre-scan shim adjustment and resulting inappropriate water suppression adjustment.	2	0