

Air-stable droplet interface bilayers on oil-infused surfaces

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Droplet interface bilayers are versatile model membranes useful for synthetic biology and biosensing; however, to date they have always been confined to fluid reservoirs. Here, we demonstrate that when two or more water droplets collide on an oil-infused substrate, they exhibit noncoalescence due to the formation of a thin oil film that gets squeezed between the droplets from the bottom up. We show that when phospholipids are included in the water droplets, a stable droplet interface bilayer forms between the noncoalescing water droplets. As with traditional oil-submerged droplet interface bilayers, we were able to characterize ion channel transport by incorporating peptides into each droplet. Our findings reveal that droplet interface bilayers can function in ambient environments, which could potentially enable biosensing of airborne matter.

nanofabrication | superhydrophobic | networks

Inspired by the pitcher plant (1), it was recently found that nano/microstructured hydrophobic substrates can be impregnated with lubricating fluids to create slippery surfaces for droplets (2–5). In contrast to dry, superomniphobic surfaces (6), lubricant-infused surfaces demonstrate stable liquid repellency at extreme pressures and temperatures (5, 7), are self-healing to mechanical damage (5), and their wettability and optical properties can be tuned (7, 8). A wide variety of applications are being explored for lubricant-infused surfaces, such as enhancing condensation heat transfer (9, 10), self-cleaning (11), fog harvesting (12), and omniphobic textiles (13), or minimizing ice nucleation (14, 15), ice adhesion (16, 17), and biofouling (18). Though previous studies have characterized the dynamics and possible wetting states of isolated droplets on lubricant-infused surfaces (5, 19–22), the interactive behavior of multiple droplets has not been reported.

For the more traditional scenario of water droplets completely submerged in a reservoir of immiscible fluid, the physics of droplet–droplet interactions are well known. Water droplets submerged in crude oil can exhibit stable noncoalescence; this is because the crude oil contains surface-active components, such as resins and asphaltenes, which congregate at the droplet interfaces (23). When amphiphilic phospholipids are introduced into an oil reservoir containing water droplets, droplet interface bilayers (DIBs) can form between adjacent water droplets (24, 25). Recently, DIBs have emerged as an ideal model membrane system due to attractive features such as durability (26, 27), tunable size and curvature (28–30), deformability (31), facile electrical characterization of ion channels (32–35), the option to introduce asymmetry into the system (36), and droplet interchangeability (26, 32). In the absence of any stabilizing agents, water droplets colliding in an immiscible fluid will exhibit coalescence when their interaction time exceeds the time required to drain the film of fluid trapped between the droplets (37, 38). Droplet collision is typically controlled by applying a constant force (i.e., gravity) (39, 40), constant approach velocity (41, 42), or constant flow rate (43, 44). For experimental studies in pure oil baths, the time required for colliding water droplets to exhibit film rupture and coalesce typically ranges from 10^{-3} to 10^2 s, depending on parameters such as oil viscosity, droplet size, and the flow field (40, 42–44).

Here, we show that water droplets in an ambient environment exhibit noncoalescence when colliding on an oil-infused surface, even in the absence of any surfactants. This phenomenon is due to the oil meniscus that surrounds each water droplet; when the oil menisci of neighboring droplets overlap, the menisci spontaneously merge together to minimize their surface energies and an oil film is squeezed upward to form a barrier between the colliding droplets. Though droplet coalescence will eventually occur due to film drainage, the time required for film rupture is several hours for moderate-viscosity [~ 100 centistokes (cSt)] oils and is 1–3 orders of magnitude longer compared with droplets submerged in an oil bath (40, 42–44). These findings should refine the understanding of using oil-infused substrates for processes involving droplet–droplet interactions, such as condensation (9, 10) and fog harvesting (12).

When incorporating amphiphilic phospholipids into the water droplets, we demonstrate that the thinning oil membrane between noncoalescing droplets gets replaced by a stable lipid bilayer, somewhat analogous to the formation of a black lipid membrane in an aperture painted with oil (45). To our knowledge, this is the first report of producing droplet interface bilayers in an ambient environment. We show that air-stable DIBs still allow for the robust electrical characterization of ion channels inserted in the lipid bilayer. Previously, it has been demonstrated that black lipid membranes or DIBs can be used for biosensing (46–50), light sensing (26), microscale biobatteries (26), electrical circuits (51, 52), and engineering tissue-like material (53). However, these suspended lipid bilayers have always been confined to fluid reservoirs (25, 45). We suggest that our air-stable DIBs will allow for an unprecedented degree of control regarding the fabrication, manipulation, transportation, and utilization of functional droplet networks.

Results and Discussion

Noncoalescence of Water Droplets on Oil-Infused Surfaces. Droplet–droplet interactions were characterized on an oil-infused

Significance

By suspending a lipid bilayer in an aperture or between water droplets, single-molecule transport through membrane channels can be electrically detected. To date, all suspended bilayers have been confined to fluid reservoirs. This study demonstrates that droplet interface bilayers can be created in an ambient environment using noncoalescing water droplets on an oil-infused surface. Air-stable droplet interface bilayers are easy to manipulate and electrically characterize, and could potentially allow for the biosensing of airborne molecules.

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superhydrophobic surface. Listed in order of increasing viscosity, the five different oils used for experiments were hexadecane; Krytox 100; 50- and 350-cSt silicone oil (at 25 °C); and Fomblin 25/6 (*SI Appendix, Table S1*). These low surface-tension oils uniformly impregnate the surface roughness to prevent deposited water droplets from directly contacting the substrate: $\theta_{os(a)} \approx \theta_{os(w)} \approx 0^\circ$, where subscripts *a*, *o*, and *w* are the air, oil, and water phases, and *s* is the substrate (5, 21). The superhydrophobic surface was composed of silicon nanopillars, because it was previously found that nanotextured surfaces are best suited for locking in a film of oil that is long-lasting (54) and highly stable against external forces (55). When a water droplet was deposited onto an oil-infused surface, an oil meniscus rapidly formed around the droplet to balance its three-phase contact line: $\vec{\gamma}_{oa} + \vec{\gamma}_{wo} + \vec{\gamma}_{wa} = 0$. It should be noted that because $\gamma_{wo} + \gamma_{oa} < \gamma_{wa}$ for all oils used here (except hexadecane; *SI Appendix, Table S2*), a thin film of oil is cloaked about the water–air interface, and $\vec{\gamma}_{wa}$ is actually replaced by $\vec{\gamma}_{wo} + \vec{\gamma}_{oa}$ (21, 56). For brevity, the oil-cloaked droplet interface will henceforth be referred to simply as the water–air interface.

When two water droplets came into contact on an oil-infused surface, they exhibited either coalescence or noncoalescence depending on their initial point of contact (Fig. 1). Droplets colliding at the water–air interfaces experienced immediate coalescence, revealing that the thin cloak of oil surrounding the droplets is not sufficient to prevent coalescence (Fig. 1*A*). This scenario will not be considered any further, because the dynamics of conventional droplet coalescence have been reported elsewhere (57). When the initial contact occurred at the droplets' surrounding oil menisci, however, the droplets exhibited noncoalescence for minutes or even hours despite becoming firmly attached to each other (Fig. 1*B–D*).

The mechanism for noncoalescence is a thin film of oil that gets squeezed upward between the droplets as the menisci merge. Surface-tension measurements of the oil–water interfaces confirmed that all of the oils (except for Fomblin) did not contain any appreciable surface-active materials (*SI Appendix, Fig. S1*), indicating that noncoalescence occurs independently of any stabilizing agents. It has previously been shown that water condensing in an oil bath exhibits an ordered hexagonal structure due to delayed coalescence (58); however, without a supporting substrate, these condensate drops were primarily submerged beneath the oil surface, whereas the noncoalescing droplets observed here are suspended almost entirely above the oil interface.

By varying the amount of excess oil on the surface, the contact angle of a deposited droplet and the shape of its oil meniscus could be tuned to control the occurrence of coalescence vs. noncoalescence (*SI Appendix, Fig. S2*). In short, noncoalescence will occur if the oil menisci extend beyond the droplet profiles, which is the case if either of the following conditions are met:

$$\begin{aligned} \theta_w < 90^\circ, \\ \theta_w > 90^\circ \text{ and } R < L + L_o, \end{aligned} \quad [1]$$

where θ_w is the contact angle of the water droplet on the oil-infused surface (with respect to the horizontal), R is the droplet's radius of curvature, L is the droplet's contact radius with the oil meniscus, and L_o is the decay length of the oil meniscus (*SI Appendix, Fig. S3*). Over hundreds of trials, Eq. 1 was confirmed for a variety of droplet sizes (2.5–10 μL) and oil viscosities (~ 1 –1,000 mPa·s). The cutoff point is illustrated in Fig. 1, where droplets exhibited coalescence for an oil film spin-coated at 1,000 rpm for 45 s (Fig. 1*A*) and noncoalescence for a thicker

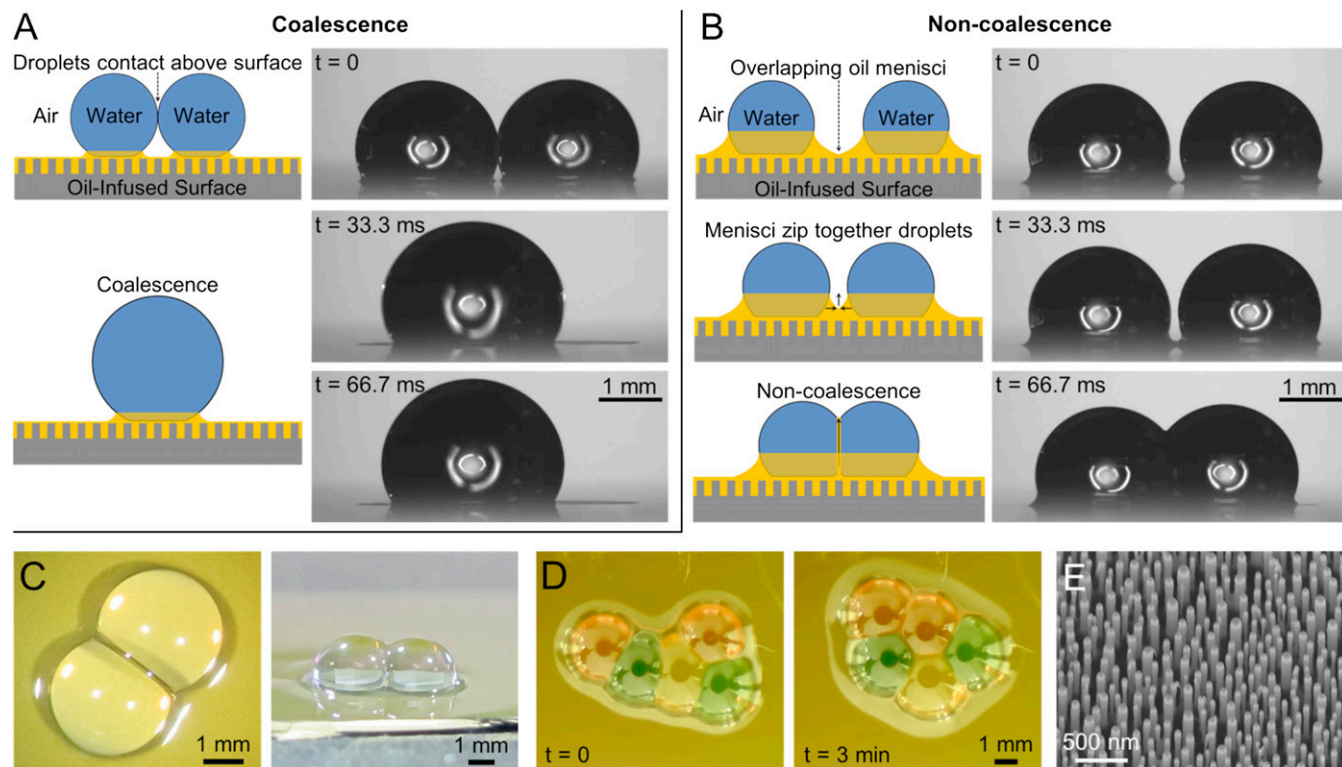


Fig. 1. Interactive behavior of water droplets on an oil-infused surface. (*A*) Droplets colliding at the liquid–air interfaces exhibited coalescence. (*B*) When the oil menisci of two droplets overlapped, an oil film formed between the droplets to enable noncoalescence. (*C*) Top-down and isometric photographs of noncoalescing droplets. (*D*) Multiple droplets could be connected into a network; due to the negligible hysteresis, these networks spontaneously rearranged over time to minimize their surface energy. (*E*) SEM of nanopillared substrate. The oils used were (*A* and *B*) Krytox 100 and (*C* and *D*) Fomblin 25/6; food coloring was used in *D*. See *SI Appendix, Movies S1–S3*.

film spin-coated at 500 rpm for 45 s (Fig. 1B). For the remainder of the experiments reported here, an excess oil thickness of $\sim 50 \pm 10 \mu\text{m}$ was deposited over the infused nanostructure; this was chosen because 50 μm of excess oil is thick enough to ensure that the criteria for noncoalescence will consistently be met ($\theta_w \approx 90^\circ$) but is also thin enough to elevate the majority of the water droplet(s) above the oil-air interface.

When the oil menisci of multiple droplets overlap, the droplets spontaneously pull together to minimize the surface energies of the oil menisci. The collision velocity of the droplets is proportional to the viscous-capillary velocity (57) of the oil,

$$v \propto \frac{\gamma_{oa}}{\mu_o}, \quad [2]$$

where v is the maximum cumulative velocity exhibited by the droplets before deceleration and γ_{oa} and μ_o are the surface tension and viscosity of the oil menisci pulling the droplets together (SI Appendix, Fig. S4). When Eq. 1 is satisfied, the water droplets exhibit noncoalescence upon collision due to the formation of an intermediate oil film. After collision, the immobilized droplets remain stuck together and exhibit a near-constant profile over time (the surface was cooled to the dew point to prevent droplet evaporation).

Thin Film Drainage Between Water Droplets. After a period that ranges from seconds to hours depending on the experimental conditions, the intermediate oil film collapses, causing the droplets to finally coalesce together. The drainage time required for film rupture depended primarily upon the viscosity of the oil, with $t_c \sim 10\text{--}1,000 \text{ s}$ for $\mu_o \sim 10 \text{ mPa}\cdot\text{s}$ and $t_c \sim 1,000\text{--}10,000 \text{ s}$ for $\mu_o \sim 100 \text{ mPa}\cdot\text{s}$ (Fig. 2). These lifetimes of noncoalescence are 1–3 orders of magnitude longer compared with submerged water droplets ($\sim 1 \text{ mm}$) colliding in an oil bath, where $t_c \sim 0.1\text{--}10 \text{ s}$ for $\mu_o \sim 10 \text{ mPa}\cdot\text{s}$ and $t_c \sim 10\text{--}100 \text{ s}$ for $\mu_o \sim 100 \text{ mPa}\cdot\text{s}$ (40, 42, 44). When an oil containing surfactants is used (Fomblin), the noncoalescing droplets were stable for at least 24 h in the absence of evaporation (SI Appendix, Fig. S5).

In addition to oil viscosity, the volume of the colliding water droplets also affected the lifetime of noncoalescence, particularly for the low-viscosity Krytox oil. The tested droplet volumes were 2.5, 5, and 10 μL . The 2.5- μL droplets consistently exhibited shorter droplet lifetimes compared with the 5- μL droplets; this is because droplets with a smaller radius of curvature exhibit a larger Laplace pressure. It would therefore be expected that the 10- μL droplets would last even longer than the 5- μL droplets; however, this was not always the case. The 10- μL droplets exhibited the widest range of noncoalescence lifetimes, with some coalescing almost immediately while others did indeed last longer than the 5- μL droplets. One possible explanation is that larger droplets collide at larger Weber numbers ($We = \rho_w v^2 R / \gamma_{wa}$), which could reduce the initial film thickness. For example, droplet collisions on Krytox oil exhibited $We \sim 0.001$ for 2.5- μL droplets compared with $We \sim 0.01$ for 10- μL droplets. The importance of inertial effects is attested by the observation that droplets colliding with externally imposed velocities exhibited higher rates of early film rupture compared with static droplets joined together solely by the oil menisci's surface tension.

The drainage and eventual collapse of the oil film is primarily due to the Laplace pressure and long-range intermolecular forces acting on the film (37),

$$\Delta P = \frac{2\gamma_{wa}}{R} + \frac{A_H}{6\pi H(r,t)^3}, \quad [3]$$

where ΔP is the pressure difference between the droplets and oil film, R is the radius of curvature of two same-sized drop-

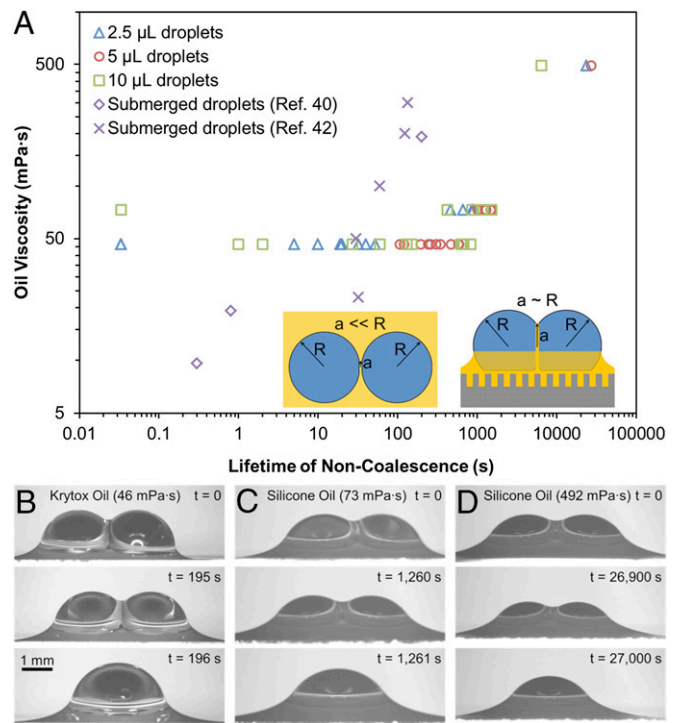


Fig. 2. (A) Time required to drain an oil film between water droplets on surfaces infused with Krytox or silicone oils. The substrate was held at 8 $^\circ\text{C}$ to prevent droplet evaporation. The drainage time was 1–3 orders of magnitude longer compared with droplets submerged in oil baths (whose data are shown here from refs. 40 and 42), most likely due to the larger film radius (Inset). (B–D) Side-view imaging of the lifetime of noncoalescing 5- μL droplets on surfaces infused with (B) Krytox, (C) 50 cSt silicone oil, and (D) 350 cSt silicone oil. See SI Appendix, Movies S4 and S5.

lets, A_H is the Hamaker constant, and $H(r,t)$ is the thickness of the oil film. The droplets used here were smaller than the capillary length, $\kappa^{-1} = \sqrt{\gamma_{wa} / \rho g} \approx 3 \text{ mm}$ (4), so gravity is not expected to play a significant role. Because the intermolecular forces scale with H^{-3} , the oil film rapidly collapses as intermolecular forces become dominant at a critical thickness (37, 38),

$$H_c \sim \left(\frac{A_H R}{12\pi\gamma_{wa}} \right)^{1/3}, \quad [4]$$

which is approximately $H_c \approx 100 \text{ nm}$ for $A_H \sim 10^{-18} \text{ J}$ (56), $R \sim 1 \text{ mm}$, and $\gamma_{wa} = \gamma_{wo} + \gamma_{oa} \approx 65 \text{ N/m}$.

For an oil film of thickness $H(r,t)$ and constant radius a , it can be assumed that $H \ll a$. Therefore, the lubrication approximation can be invoked, where only the radial velocity of the draining oil film, u_r , is considered. Neglecting inertial terms and assuming axisymmetry and an immobile interface (i.e., no plug flow), the Navier–Stokes velocity profile for a given film thickness is given by

$$u_r = \frac{\Delta P}{2\mu_o a} \left(z^2 - \left(\frac{H}{2} \right)^2 \right), \quad [5]$$

where z is the perpendicular distance from the center line of the oil film. Though it is likely that the film interfaces exhibit some degree of curvature and/or deformation (38, 42), an analytical approximation of the drainage rate may be obtained by assuming

rigid, parallel interfaces, such that $H(r, t) \rightarrow H(t)$ (full derivation in *SI Appendix*):

$$\frac{dH}{dt} = -\frac{1}{3\mu_o a^2} \left(\frac{\gamma_{wa} H^3(t)}{R} + \frac{A_H}{12\pi} \right). \quad [6]$$

Eq. 6 reveals that, all other parameters being equal, the drainage rate is inversely proportional to a^2 , which is important because for conventional film drainage between two submerged same-sized water droplets of radius R , the point contact made between colliding droplets results in film drainage where $H \ll a \ll R$ (42); this is in sharp contrast to our large-area oil film that forms between two colliding droplets on an oil-infused surface, where $H \ll a \sim R$ (Fig. 2A, *Inset*). The large increase in the size of a is one possible explanation for the dramatically long lifetime of noncoalescence observed here compared with lifetimes reported for submerged droplets. Another possible reason is that droplets on an oil-infused surface require no external forces to collide together, whereas submerged droplets require gravity or an applied flow field which can accelerate the drainage rate.

By inserting electrodes into each of the noncoalescing droplets and applying a triangular waveform voltage, the average thickness of an oil film can be estimated:

$$H_{avg}(t) = \frac{\epsilon_r \epsilon_0 A}{C(t)}, \quad [7]$$

where ϵ_r is the relative permittivity of the oil (2.14 for hexadecane and 2.75 for silicone oils), $\epsilon_0 = 8.854 \times 10^{-12} \text{F/m}$ is the vacuum permittivity, $A \approx 3 \times 10^{-6} \text{m}^2$ is the approximate surface area of the oil film between $5\text{-}\mu\text{L}$ droplets ($R \approx 1 \text{mm}$), and $C(t)$ is the capacitance calculated from current measurements (*SI Appendix, Figs. S6 and S7*). The electrodes were inserted into two separate $5\text{-}\mu\text{L}$ water droplets, and then the droplets were joined together using a micromanipulator to measure $H_{avg}(t)$ for the complete lifetime of noncoalescence (Fig. 3). For the remainder of the experiments shown here, a nonconductive superhydrophobic surface composed of silica nanoparticles on a glass slide (*SI Appendix, Fig. S8*) was used to prevent current from passing into the substrate.

For each trial, the oil film collapsed and coalescence occurred at a critical film thickness of $H_{avg}(t_c) \sim 0.1\text{--}1 \mu\text{m}$, ~ 1 order of magnitude larger than $H_c \approx 100 \text{nm}$ predicted by Eq. 4. It is therefore likely that the oil film exhibits a slight curvature in its profile, such that H_c is only obtained at a localized area with larger thicknesses elsewhere. Nevertheless, the parallel disk drainage model given by Eq. 6 reasonably approximated the experimental drainage rates (Fig. 3). Values of a used to fit Eq. 6 with the data ranged from $a \approx 100 \mu\text{m}$ to $a \approx 850 \mu\text{m}$ (depending on oil viscosity and excess oil thickness; *SI Appendix, Table S3*), which further supports the hypothesis that $a \sim R$ for air-stable interdroplet films. Though the insertion of electrodes did reduce the lifetime of noncoalescence compared with free droplets (Fig. 2A), it was confirmed that the applied voltage did not have any appreciable effect on the capacitance measurements (*SI Appendix, Fig. S9*).

Air-Stable Droplet Interface Bilayers. Thus far, we have characterized the formation and drainage of a thin oil film between noncoalescing water droplets on an oil-infused surface. The functionality of these noncoalescing droplets would be greatly enhanced if the intermediate oil film could be replaced by a lipid bilayer, because a lipid membrane would provide a stable droplet–droplet interface of known thickness that can facilitate molecular transport between droplets. In this final section, we mixed 2.4 mM of diphytanoyl phosphocholine (DPhPC) phospholipids in the water phase before droplet deposition on the oil-infused surface. Colliding droplets still exhibit

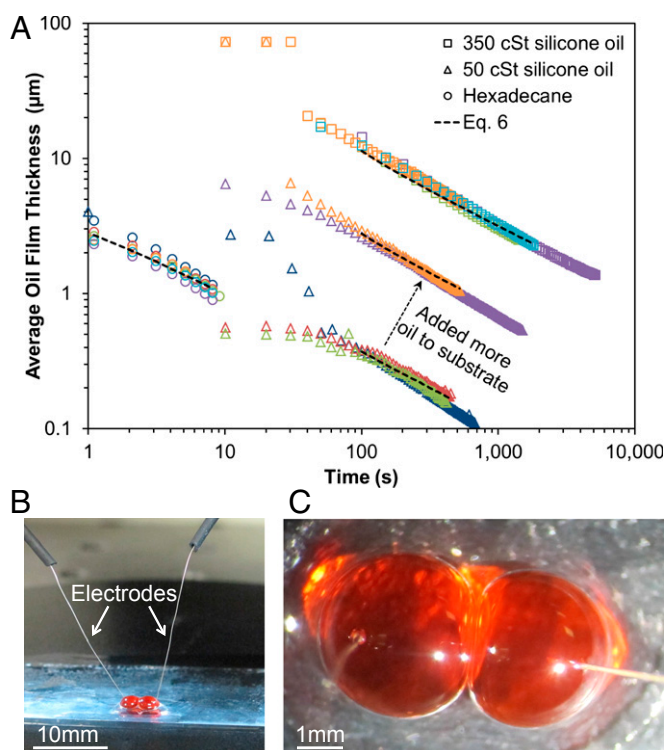


Fig. 3. (A) Electrical measurements of the average oil film thickness between noncoalescing water droplets for substrates infused with hexadecane (\circ) at room temperature (22°C), 50 cSt silicone oil (Δ) cooled to the dew point (17°C), or 350 cSt silicone oil (\square) cooled to the dew point (now 7°C due to change in humidity). Multiple trials for each oil are denoted by different colors, and the final data point for each trial indicates film collapse and coalescence. The drainage rates were in good agreement with the model (Eq. 6) as denoted by the dotted trend lines; see *SI Appendix, Table S3* for the values used in Eq. 6. The initial film thickness increased with viscosity and could also be increased by adding more excess oil to the substrate, as demonstrated here with 50 cSt silicone oil. (B and C) Side-view and top-down photographs of noncoalescing water droplets with inserted electrodes.

noncoalescence in the same manner as before, but now lipids assemble at the interfaces of the intermediate oil film. Instead of droplet coalescence occurring once the oil film drains and collapses, the droplet–droplet interface is stabilized by the formation of a lipid bilayer that is only 5–7 nm thick (analogous to the formation of a black lipid membrane). Hexadecane oil was chosen for these experiments due to its compatibility with phospholipids and because its low viscosity ensures that the initial oil film will rapidly drain and become replaced by a droplet interface bilayer.

Using the same electrical characterization technique described in the previous section, capacitance measurements reveal that the oil film is completely replaced by a lipid bilayer within 50 s (Fig. 4A). Due to the high freezing temperature of hexadecane (18°C), the surface could not be cooled down to the dew point, so over time the area of the bilayer steadily decreased to zero due to droplet evaporation. It is remarkable that the droplets never coalesced throughout the shrinkage of the droplet interface bilayer. In the future, a different choice of oil and/or humidity control could allow for the droplets to be held at the dew point; it should also be possible to use condensation in addition to evaporation to enable bilayers with reversibly tunable geometries.

Finally, we incorporated transmembrane peptides into the droplets to alter the ionic conductance of the interface as a way to verify that the lipid-stabilized interface between droplets is a bilayer membrane. Specifically, alamethicin peptides from the

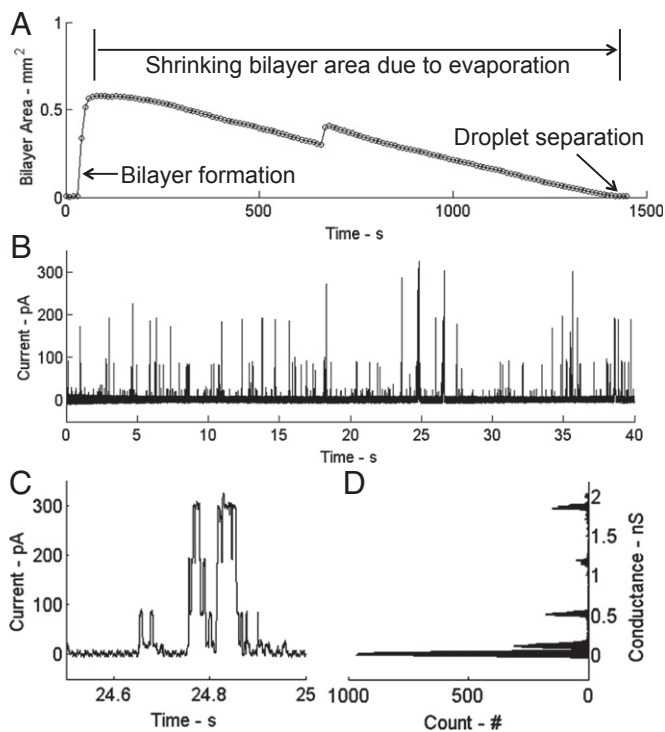


Fig. 4. (A) Bilayer area vs. time for an air-stable droplet interface bilayer. The area is determined from a capacitance measurement of the interface (*SI Appendix*). The maximum area (0.58 mm^2) corresponds to the maximum expansion of the thinned interface between droplets soon after initial bilayer formation, and the area reduces to zero over the next 23 min due to evaporation of the electrode-pinned droplets that causes them to pull apart as they shrink. The slight kink at $t \approx 700 \text{ s}$ was caused by one droplet suddenly shifting its position on the slippery surface. (B) Measurement of single-channel currents produced by alamethicin peptides at a voltage of $+160 \text{ mV}$. (C) A detailed view of one gating event shows the characteristic, multilevel current response seen for alamethicin oligomers. (D) A corresponding histogram of the conductance levels.

fungus *Trichoderma viride* were incorporated into the droplets at 10 nM to encourage the formation of voltage-dependent ion channels through the bilayer. Fig. 4B shows measured current for a holding potential of $+160 \text{ mV}$, where the transient increases correspond to the insertion and assembly of channel-forming alamethicin oligomers that span the thickness of the membrane. An example of the discrete changes in current that occur during these rapid pore-forming events is shown in more detail in Fig. 4C. A histogram of the channel conductance (i.e., current/voltage) during these gating transitions confirms the measured current levels to be those corresponding to the first four conductance levels (110 pS , 520 pS , 1.20 nS , and 1.85 nS) for alamethicin (59, 60). These results verify that the droplet–droplet interface is a bilayer membrane whose properties can be controlled and characterized using transmembrane biomolecules.

To our knowledge, this is the first report of fabricating a suspended lipid bilayer in an ambient environment. Black lipid membranes have always been confined to aqueous baths (45), and droplet interface bilayers have always been constructed in oil reservoirs (25) or in oil-in-water emulsions (61). Recent reports have obtained air-stable supported lipid membranes formed on a solid substrate (62, 63); however, the fluidity of such membranes is highly dependent on humidity, and transmembrane studies cannot be achieved with solid supported bilayers. Our air-stable droplet interface bilayers mitigate both of these limitations: the adjacent droplets maintain bilayer fluidity and suspend the bilayer to allow for molecular transport. The use of an oil-infused surface in place of an oil reservoir will enable

the robust fabrication and modulation of functional droplet networks via techniques such as micropositioning, condensation, evaporation, vibration (64), or magnetic fields (65); such techniques are typically more practical in an ambient environment.

Conclusion

Using oil-infused superhydrophobic surfaces, we have demonstrated that colliding water droplets exhibit noncoalescence due to the spontaneous formation of a microscopic oil film between the droplets. In the absence of surfactants the Laplace pressure and intermolecular forces eventually cause the intermediate film to collapse, but the lifetime of noncoalescence is 1–3 orders of magnitude longer compared with droplets colliding in a submerged fluid bath. When phospholipids are mixed into the noncoalescing water droplets, an air-stable droplet interface bilayer forms that was used to detect single-channel gating events. To our knowledge, this is the first time that suspended lipid bilayers have been produced and characterized in an ambient environment instead of in a fluid reservoir. We envision that our air-stable suspended bilayers will enable the robust construction and manipulation of functional droplet networks and potentially allow for the stochastic biosensing of airborne molecules.

Materials and Methods

Superhydrophobic Silicon Nanopillars. The silicon nanopillars were fabricated using a lithography-free technique adapted from a previous report (66). First, 100 nm of silicon dioxide (SiO_2) was thermally grown onto a (100) Si substrate and 5 nm of platinum was then deposited onto the SiO_2 using an electron beam evaporator. The sample was heated in a rapid thermal processor furnace (Easy Tube 3000; First Nano) at full power for 8 s in H_2 and Ar ambient to dewet the platinum film into an etch mask. The maximum temperature of the chamber at full power was $\sim 850 \text{ }^\circ\text{C}$. The SiO_2 was etched using $2 \text{ standard cubic centimeters per minute (sccm)}$ O_2 and 45 sccm C_4F_8 for 55 s at $15 \text{ }^\circ\text{C}$, 7 mTorr , and 200 W rf (Oxford Plasmalab 100). The Si was subsequently etched using 5 sccm Ar , 25 sccm SF_6 , and $58 \text{ sccm C}_4\text{F}_8$ for 6 min at $20 \text{ }^\circ\text{C}$, 10 mTorr , and 30 W rf . Scanning electron microscopy revealed an etch depth of $500 \pm 100 \text{ nm}$ and pillar diameters ranging from 10 to 100 nm (Fig. 1E). The nanostructure was rendered superhydrophobic by immersion in a solution of 0.1% (vol/vol) of (tridecafluoro-1,1,2,2-tetrahydrooctyl)triethoxysilane (Gelest Inc.) in hexane for 12 h . Droplets exhibited contact angles of $\theta_A = 168 \pm 3^\circ$ and $\theta_R = 166 \pm 3^\circ$ (66).

Superhydrophobic Glass. SiO_2 powder (*SI Appendix, Fig. S8A*) was annealed at $70 \text{ }^\circ\text{C}$ for 24 h . The mean size of the particle agglomerates was $610 \pm 140 \text{ nm}$ (*SI Appendix, Fig. S8B*). The powder was suspended in a solution of hexane and (tridecafluoro-1,1,2,2-tetrahydrooctyl)trichlorosilane (Gelest Inc.). The concentrations of the SiO_2 particles and silane in the hexane are 6 and $0.6 \text{ wt}\%$, respectively. After stirring the suspension for 8 h at room temperature, the powder was washed with hexane to remove nonreacted silane groups and then dried at $60 \text{ }^\circ\text{C}$ for 24 h . The resulting functionalized particles (*SI Appendix, Fig. S8C*) were suspended in a solution of polyurethane resin and acetone in a weight ratio $W_{\text{particle}} : W_{\text{resin}} : W_{\text{acetone}} = 1 : 1 : 20$. Superhydrophobic substrates with water contact angle $\sim 170^\circ$ were obtained by spin coating the suspension with a Speedline Technologies G3-8 at $1,000 \text{ rpm}$ for 30 s on glass slides (*SI Appendix, Fig. S8D*).

Electrical Measurements. Electrical measurements of oil- and bilayer-stabilized interfaces were performed by measuring the current induced by a triangle waveform voltage applied to two wire-type silver–silver chloride electrodes ($125 \mu\text{m}$) inserted into the droplets. The triangle voltage waveform was the output of a function generator (Agilent 33210A), and the resulting current was recorded using an Axopatch 200B patch-clamp amplifier and Digidata 1440A data acquisition device (Molecular Devices). Measurements of current were sampled at 20 kHz , and all electrical measurements are performed on glass substrates.

Droplets Solutions for Bilayer Tests. Hexadecane [99% (vol/vol); Sigma] was used as the infusing oil on the glass substrates for bilayer formation between droplets. Liposome solutions consisted of 2.4 mM DPhPC (Avanti Polar Lipids) suspended as 100-nM liposomes in a 200-mM NaCl (Sigma), 10-mM Mops (Sigma) buffer. Alamethicin peptides (A.G. Scientific) were stored in ethanol at 10 mg/mL , and then diluted to 10 nM (19.64 ng/mL) in liposome solution.

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