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## Optical Trapping of Individual Human Immunodeficiency Viruses in Culture Fluid Reveals Heterogeneity with Single-Molecule Resolution

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### Abstract

Optical tweezers use the momentum of photons to trap and manipulate microscopic objects contact-free in three dimensions. Although this technique has been widely used in biology and nanotechnology to study molecular motors, biopolymers and nanostructures, its application in viruses has been very limited largely due to the small size of these nanoparticles. Using optical tweezers that can simultaneously resolve two-photon fluorescence at single-molecule level, here we show that individual HIV-1 can be optically trapped and manipulated, which allows multi-parameter analysis of single virions in culture fluid under native conditions. We show that individual HIV-1 differs in the numbers of envelope glycoproteins by more than one order of magnitude, which implies substantial heterogeneity of these virions in transmission and infection at single-particle level. Analogous to flow cytometry for cells, this fluid-based technique may allow ultrasensitive detection, multi-parameter analysis and sorting of viruses and other nanoparticles in biological fluid with single-molecule resolution.

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Optical tweezers (OTs) use the momentum of photons to trap and manipulate microscopic objects contact-free in three dimensions (3D)<sup>1–5</sup>. Although this technique has been widely used in biology and nanotechnology to study molecular motors, biopolymers<sup>3,6–15</sup>, and for trapping of metal nanoparticles<sup>16–18</sup> and various nanostructures<sup>4,19–22</sup>, there have been no demonstrations or studies on optical manipulation of a single animal virus<sup>23</sup>. Several challenges exist besides the issue of biosafety. First, the presence of a permanent or an induced dipole moment in the object is required for optical trapping<sup>3</sup>. Ashkin and Dziedzic first demonstrated optical trapping of tobacco mosaic virus (TMV) in 1987<sup>23</sup>. TMV is 300 nm long and 15 nm in diameter<sup>24</sup>. This long cylindrical structure displays a permanent

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### Additional information

Supplementary information accompanies this paper at [www.nature.com/naturenanotechnology](http://www.nature.com/naturenanotechnology).

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dipole moment<sup>25</sup> which may facilitate its trapping by OTs. While majority of animal viruses are spherical in shape<sup>26,27</sup>, their dipole moments may be intrinsically small as compared to other aspheric objects of similar volume<sup>23</sup>. Second, animal viruses are typically less than 300 nm in size<sup>26,27</sup>. The gradient force responsible for trapping of a Rayleigh scatterer scales with the cube of the particle dimension<sup>3</sup>. The lower viscous drag from the solvent on smaller particles also allows them to easily escape once being trapped. Hence the smaller the particle, the more difficult to trap and manipulate it using light. Third, the refractive indices of animal viruses have never been measured. Although the trapping force increases in general with the refractive index of the object<sup>28</sup>, how a single animal virus may interact with light rays and generate trapping forces on itself is unknown. All these aspects present challenges to manipulation of an animal virus using light. Can a single animal virus be trapped and manipulated using light? By using an ultrahigh resolution OTs instrument that we constructed recently<sup>29</sup>, here we show that individual HIV-1 can be trapped and manipulated in culture fluid ‘contact-free’ in 3D under native conditions. We developed this capability into a quantitative technique, ‘virometry’. This technique permits multi-parameter analysis of individual HIV-1 virions in culture fluid under native conditions with single-molecule resolution, and can be applied to other viruses and nanoparticles in solution for their detection and measurement of size, shape and protein compositions with unprecedented sensitivity.

### Optical Trapping of Single HIV-1 in Culture Fluid

To demonstrate the optical trapping of animal viruses in biological fluid, we have recently prepared the HIV-1 virions derived from the X4-tropic NL4-3 provirus clone<sup>30</sup>. These viruses were tagged internally with EGFP fused to Vpr<sup>31,32</sup>, an accessory protein of HIV that physically associates with the virion core<sup>33</sup> and thus serves as a fluorescent marker<sup>31</sup> for virion manipulation. The infectivity of this virus was 0.1% in TZM-bl cells<sup>30</sup>, a value that was comparable to wild-type viruses. Control experiments showed that EGFP-Vpr also distinguished virions from microvesicles (Supplementary Note 1). Without any fixation procedure, we diluted the live virus stock in the complete media and injected them into a microfluidic chamber (Fig. 1a). Upon trapping of a virion by the 830 nm infrared laser<sup>29</sup> focused at the center of the chamber, the virion was immediately ‘visible’ in the dark background due to simultaneous two-photon excitation of EGFP by the trapping laser<sup>29,34</sup> (Fig. 1b). Such events were not observed when complete media only, viruses without EGFP-Vpr labels, or culture supernatants transfected with EGFP-Vpr were used as controls, suggesting that the fluorescent particles resulted from virions tagged with EGFP. Under these conditions, a single fluorescent particle could be trapped in culture fluid and manipulated in various patterns by steering the laser beam without interference from other virions (Supplementary Video). Typical two-photon fluorescence (TPF) time courses from individually-trapped virions are shown in Fig. 1c, where the initial bursts of fluorescence well above background indicated the arrival of HIV-1 virions at the optical trap. The subsequent decay of TPF with time could all be fit by single exponentials with an average time constant of  $53.7 \pm 8.0$  s ( $N=19$ ), very close to the rate of photobleaching that we measured previously for EGFP either on a surface ( $50.8 \pm 4.2$  s)<sup>34</sup> or inside a cell ( $52.7 \pm 5.2$  s)<sup>35</sup>. This comparison confirmed the presence of EGFP in these particles.

Freely-diffusing particles in culture fluid may undergo concentration-dependent aggregation. How do we know that the trapped particle correspond to a single HIV-1 virion? Independent of EGFP fluorescence, we could also detect the trapping of the virus from changes in laser deflection at the objective's back focal plane (BFP) (Fig. 2a, blue). The occasional trapping of an apparent viral aggregate produced quantitatively different laser deflection signals<sup>29,36</sup> (Fig. 2a, red), suggesting that one could potentially use this signal to distinguish viral particles of different size. We analyzed the time courses of the laser deflection by conversion to power spectra in the frequency domain (Fig. 2b). For both the single particle (blue) and virion aggregate (red), the power spectra could be well described with Lorentzian up to 10 kHz (green curves, Supplementary Methods), consistent with the Brownian motion of a particle in a harmonic photonic field<sup>3</sup>. Furthermore, this fitting yielded very different parameters for the single particle and virion aggregate:  $D^{\text{volt}}$ , the diffusion coefficient (in the unit of  $\text{V}^2/\text{s}$ ) and  $f_c$ , the corner frequency (in Hz). To test the sensitivity of these parameters in differentiating particles of different size, we delivered diluted virions through a microfluidic channel into the complete media followed by trapping of the virion in the vicinity of the channel opening (Supplementary Fig. 1). This scheme allowed us to trap one, two and three particles sequentially using a single laser beam (Supplementary Fig. 1), and measure  $D^{\text{volt}}$  and  $f_c$  for the apparent single, double and triple particles, respectively. The distributions of these values are plotted in Fig. 2c and d. As shown, both  $D^{\text{volt}}$  and  $f_c$  conform to statistically different distributions for single versus double or triple particles (Supplementary Table 1), suggesting that the laser deflection is sensitive enough to distinguish a single particle from particle aggregates.

## Measurement of Single HIV-1 Virion Diameter

Single HIV-1 particles are heterogeneous in diameter<sup>37</sup>. To help distinguish individual viral particles of different diameters, we set out to use the sensitive laser deflection signal to directly measure the diameter for each trapped virion in the culture fluid (Methods). This method works by calibration of the laser deflection signal using a distance standard<sup>38</sup> and the  $D^{\text{volt}}$  can be converted to the diffusion coefficient of the particle in space ( $D$ , in the unit of  $\mu\text{m}^2/\text{s}$ )<sup>38</sup>. The diameter of the particle,  $\phi_{\text{BFP}}$ , can then be calculated using the Stokes-Einstein equation (Supplementary Methods). We first tested this method by trapping polystyrene beads of various sizes in water. These results were compared with the diameters of the beads determined from transmission electron microscopy (TEM) images ( $\phi_{\text{TEM}}$ , Supplementary Fig. 2). Over the range of bead sizes we tested, these two methods yielded good agreement, with  $\phi_{\text{BFP}}$  slightly larger than  $\phi_{\text{TEM}}$  by 5.5% on average, which reflected either the error in laser deflection measurement or hydration of particles in water. Fig. 3a shows the power spectrum of a trapped virion obtained from this calibration procedure in complete media, with voltage converted to distance as shown on the right axis, which yields a diameter of 165 nm for this particular virion. Fig. 3b shows the histogram of  $\phi_{\text{BFP}}$  determined for 137 single HIV-1 particles in complete media at a concentration of  $4.0 \times 10^7$  virion/ml, which displayed a population with a mean of 154 nm, and a median of 148 nm. The reduced chi-squared statistic from this analysis varied from 1.10 to 1.16 (Supplementary Fig. 3), indicating a good quality of power spectrum fitting. This virion size distribution was quantitatively similar to what was reported previously for authentic, mature HIV-1 virions

by cryoelectron microscopy (cEM)<sup>37</sup>. Our mean diameter was 6.2% larger than  $145 \pm 25$  nm for single HIV virions measured by cEM. This positive deviation was consistent with the trend seen for reference beads, suggesting that these particles indeed corresponded to single virions in complete media. This positive deviation can result from either hydration of the particles in culture media or potential shrinkage of the feature size under EM (Supplementary Note 2). From calibrated power spectra for single HIV-1 virions, we also obtained stiffness of the optical trap (Supplementary Methods), which is shown in Fig. 3c with a mean value of 3.2 fN/nm. This stiffness is about 30-fold lower than typically reported values for bigger particles<sup>3</sup> and explains the difficulty in trapping virions of this size. The variation in trap stiffness as compared to variations in particle diameter also suggests that HIV-1 virions deviate from true Rayleigh scatterers. To examine how well the measured particle diameter and trap stiffness can differentiate particles of different size, we conducted sequential trapping of one, two and three particles as illustrated in Supplementary Fig. 1, and measured  $\phi_{\text{BFP}}$  and trap stiffness for the apparent single, double and triple particles, respectively. The distributions of these values are plotted in Supplementary Fig. 4a and b. As shown, both  $\phi_{\text{BFP}}$  and trap stiffness conform to statistically different distributions for single versus double or triple particles (Supplementary Table 2), suggesting that these parameters are sensitive enough to distinguish a single particle from particle aggregates.

## Concentration-dependent Aggregation of HIV-1 Virions in the Complete Media

Freely-diffusing particles in the complete media may undergo concentration-dependent aggregation. To examine the aggregation status of HIV-1 virions under native conditions in the complete media, we conducted diameter measurement for single particles trapped at various concentrations in the microfluidic chamber. Fig. 4a shows the histogram of  $\phi_{\text{BFP}}$  determined for 128 apparent single particles at  $1.2 \times 10^8$  virions/ml in the complete media (grey bars), which displays two distinct populations as indicated by the double-Gaussian fit (dashed lines). The primary peak, with a mean of 156 nm and a standard deviation of 30 nm, accounts for 72% of the particles. This number is very close to the average diameter of 154 nm for single HIV virions measured at  $4.0 \times 10^7$  virions/ml, suggesting that these particles indeed correspond to single virions. The secondary peak in this histogram, with a mean of 305 nm and a standard deviation of 44 nm, is about twofold larger than the size of a typical HIV-1 virion. These particles were rarely observed when trapping at a concentration of  $4.0 \times 10^7$  virions/ml, suggesting that they resulted from a concentration-dependent aggregation. This conclusion is further supported by the same experiment done at even higher concentration of virion particles. Fig. 4b shows the histogram of  $\phi_{\text{BFP}}$  determined for 103 apparent single particles at  $4.0 \times 10^8$  virions/ml in the complete media. No clear peaks were present. Particle diameters ranged from 90 to 440 nm, with an average diameter of  $232 \pm 78$  nm (median 219 nm). This feature is reproducible from an independent repeat of the same experiment, suggesting a concentration-dependent aggregation of HIV-1 particles. Fig. 4c shows the distribution of EGFP TPF intensity from single HIV-1 virions upon their initial trapping. This distribution was broad and asymmetric, ranging from 1,000 to 40,000 a.u., with a major peak around 30,000. This variation of TPF intensity exclusively resulted from EGFP-Vpr molecules packaged into virions because control virions without EGFP showed

no detectable TPF under these conditions. This substantial variation of the initial TPF amplitudes suggests that one cannot simply use TPF intensity to confirm a single virus. Rather, size or trap stiffness measurement is required. Moreover, virion diameter is a better parameter than  $D^{\text{voltage}}$  in resolving subpopulations within a virus pool (Supplementary Fig. 5).

## Optical Trapping Virometry

We have recently developed single-molecule TPF imaging capability using our optical trap setup<sup>34,35</sup>. This imaging uses the optical trapping laser for direct and simultaneous TPF excitation of fluorophores such as fluorescent proteins at the laser focus whose fluorescence is detectable at single-molecule level. Because the optical paths for BFP interferometry operate independently from single-molecule TPF detection, we can thus trap a single HIV-1 in culture fluid and *simultaneously* monitor viral proteins via TPF by using appropriate fluorophore labels. Because our TPF detection has single-molecule sensitivity, this technique should offer many possibilities for quantitation and potential sorting of virions in culture fluid with exquisite sensitivity. To test this idea, we produced series of HIV-1 virions that were tagged with EGFP-Vpr but might carry different number of envelope glycoproteins as we varied the envelope plasmid input (pEnv, 0–4  $\mu\text{g}$ ) during virion production<sup>30</sup>. The infectivity of these virions increased with increasing pEnv (Supplementary Fig. 6) and reached a plateau at 1  $\mu\text{g}$  pEnv in the presence of 20  $\mu\text{g}/\text{ml}$  DEAE-dextran (Fig. 5a). To monitor the envelope content of individual virions, we prepared fluorescent-labeled monoclonal antibody b12<sup>39</sup> (Alexa594-b12) that specifically recognizes HIV-1 envelope glycoproteins gp120<sup>40,41</sup>. We chose Alexa-594 for labeling, which can be excited by the 830 nm trapping laser efficiently and yet has a minimal spectral overlap with EGFP emission (Supplementary Fig. 7). This strategy allowed us to measure EGFP-Vpr and gp120 for the same single virion almost simultaneously, both with single-molecule sensitivity<sup>34</sup> (Supplementary Fig. 8). Microvesicles that carried gp120 or antibody aggregates were also excluded from HIV-1 virions by using this two-color strategy. We incubated the EGFP-tagged viruses with Alexa594-b12 at an antibody concentration (15  $\mu\text{g}/\text{ml}$ ) that was sufficient to neutralize >95% HIV infectivity (Supplementary Fig. 9) to ensure the saturation binding of all functional gp120. Control experiments showed that gp120 shedding was negligible at this concentration of b12 (Supplementary Fig. 10). We thus expect the level of Alexa594-b12 fluorescence associated with individual virions to correlate with gp120 content on virion surface. We measured HIV virions prepared with 0, 0.01, 0.1, 0.2, 2 and 4  $\mu\text{g}$  pEnv by trapping them in complete media. A typical result is shown in Fig. 5b using 2  $\mu\text{g}$  pEnv as an example, where the intensity of Alexa-594 TPF for each particle was plotted as a function of particle diameter in red circles (N=231). For 2  $\mu\text{g}$  pEnv, 55% of the particles had diameters that were consistent with single virions and were highlighted in green. The intensity of Alexa-594 TPF associated with these particles displayed a broad distribution, varying from zero to 40,000 a.u.. Control experiments using virions without envelope glycoproteins (pEnv=0) showed no Alexa-594 fluorescence in >95% cases (Fig. 5b blue diamonds), confirming that the different levels of Alexa-594 TPF resulted from specific gp120 binding by Alexa594-b12. Fig. 5c shows a compendium of Alexa-594 TPF histograms from single virions prepared with varied pEnv. Throughout, all the distributions were broad even when the infectivity for the corresponding batch of HIV-1

was at plateau. The single-molecule sensitivity of current setup allowed us to roughly estimate the number of envelope trimers in single virions based on the average TPF intensity of a single Alexa-594 molecule, which yielded 0–18 envelope trimers per virion if assuming each Alexa594-b12 bound two gp120 molecules or 0–9 envelope trimers per virion if each Alexa594-b12 bound only one gp120 (Supplementary Note 3). Indeed, as shown in Fig. 5d, we could clearly distinguish particles that carried gp120 (red curve) from those that didn't due to single-molecule sensitivity (black curve). 12% of the single particles from 2  $\mu\text{g}$  pEnv did not show any Alexa-594 fluorescence (Fig. 5c), indicating that no gp120 was present on the virion surface. This fraction increased to 26% as we lowered pEnv to 0.01  $\mu\text{g}$  (Fig. 5c). Because envelope glycoproteins are required for virion infectivity (Fig. 5a), these data suggest that defective HIV-1 virions can be produced during virion budding, the fraction of which increases when envelope glycoproteins are supplied under limiting conditions (Supplementary Table 3). Furthermore, there were particles that had gp120 but clearly showed only two or three steps of Alexa-594 photobleaching (Fig. 5e and f). The fraction of these virions was 5% for 2  $\mu\text{g}$  pEnv and increased to 33% for virions prepared with 0.01  $\mu\text{g}$  pEnv. These data indicate that at most a single envelope trimer is present on these virions. The number of envelope trimers per virion was estimated previously using various methods<sup>42,43</sup>. However, as low as a single trimer on virion surface has not been reliably reported. Our technique allows us to clearly detect the presence of a single trimer on HIV-1 virion surface in culture fluid without ambiguity.

Lastly, the ability to use a single 830 nm laser to excite both EGFP and Alexa-594 simultaneously offers a unique advantage to our technique. Because EGFP and Alexa-594 have minimal emission spectrum overlap (Supplementary Fig. 7), we can resolve both fluorescence for a single HIV-1 particle and thus examine the potential correlation between the two kinds of proteins within a single particle. To this end, we plotted Alexa-594 TPF as a function of EGFP-Vpr TPF for each single HIV-1 virions in Fig. 6a–e for the five batches of viruses that we have prepared with different pEnv inputs. As shown, there was little correlation between Alexa-594 and EGFP-Vpr in their TPF intensities at single-particle level. This conclusion is true regardless of the input quantity of pEnv. The correlation coefficients between Alexa-594 TPF and EGFP-Vpr TPF are 0.1668, 0.2002, 0.1035, 0.3054, 0.1087 for 0.01, 0.1, 0.2, 2 and 4  $\mu\text{g}$  pEnv (Fig. 6f), respectively, suggesting that Vpr and envelope glycoprotein incorporation into individual HIV-1 virions are two independent processes during HIV-1 virion budding.

## Optical Trapping of a Single Animal Virus

Optical trapping technique has been widely used in biology and nanotechnology to study molecular motors, biopolymers, and various nanostructures. However, there have been no demonstrations or studies on optical manipulation of any animal virus, largely due to the small size of these particles. Here we show that it is feasible to optically manipulate a single HIV-1 virion in culture fluid. Our technique combines the sensitive BFP interferometry<sup>36,44</sup> and simultaneous TPF at single-molecule level in a single experimental setup, which allows multi-parameter analysis of single HIV-1 virion in culture fluid with single-molecule resolution (Supplementary Note 4). Analogous to flow cytometry for cells, this technique

may well be applied to a broad spectrum of animal viruses<sup>26</sup> for ultrasensitive detection, multi-parameter analysis of particle heterogeneity, and potential sorting in biological fluid.

## Heterogeneity of HIV-1 Virions

Much is known about the heterogeneity of RNA viruses at nucleic acids level thanks to the advances in DNA sequencing technology. However little is known about the heterogeneity of RNA viruses in their protein compositions due to the lack of sensitive techniques to measure viral protein contents at single-molecule level per virion basis. Virometry directly reveals the heterogeneity of HIV-1 in their protein compositions with single-molecule sensitivity. For gp120, we found that its copy number varied over one order of magnitude despite the fact that all these virions were derived from a single clone. This property is a feature of single HIV-1 virions, as demonstrated by our analysis using different cutoff values for single virion diameters (Supplementary Fig. 11). The consequence of this variation might be a broad spectrum of infectivity for individual HIV-1 virions as shown in Fig. 5a and hypothesized in literature<sup>45</sup>. Indeed, recent studies have shown that the transmitted ‘founder’ virus that established infection in AIDS patients corresponded to virions that had higher envelope glycoprotein content<sup>46</sup>. Future experiments are necessary to determine if the heterogeneity observed in the spike number of NL4-3 virions is also relevant to R5-tropic viruses, which are generally believed to establish primary infections<sup>47</sup>. The substantial heterogeneity of envelope content in virions from both low and high pEnv inputs indicates a stochastic component in envelope glycoprotein incorporation during virion budding<sup>48–50</sup>. It will be of future interest to dissect the mechanisms behind this apparent heterogeneity in viral envelope content, whether it results from a passive incorporation process or an active recruitment mechanism through protein-protein interactions<sup>48,49,51</sup>.

## Methods

### Production of HIV-1 virions

Various HIV-1 virions were generated and assayed as described recently<sup>30</sup>. Briefly, 293T cells were transfected with 1.0 µg pNL4-3R<sup>-</sup>E<sup>-</sup> plasmid, various amounts of pEnv (NL4-3 envelope expression plasmid, the same as pcDNA3.1REC in Kim et al.) and pEGFP-Vpr using Mirus LT-1 transfection reagents in 2-ml culture volume in a 35-mm dish. 0.1 µg pEnv and 0.3 µg pEGFP-Vpr plasmids were used as default unless otherwise noted. Media was changed six hours post transfection and virions were harvested at 24 hours post transfection<sup>30</sup>. Infectious virion concentrations were measured using TZM-bl indicator cell line and the physical concentrations of the virion particles were determined using p24 ELISA assay as described<sup>30</sup>. The infectivity of the virions was calculated by taking the ratio between infectious virion concentration and physical particle concentration. More than 90% of the infectious units were retained in the complete media over the time frame of the experiments (Supplementary Fig. 12).

### OTs and TPF experiments

A home-made OTs instrument using tapered amplifier diode laser at 830 nm (SYS-420-830-1000, Sacher LaserTechnik LLC, Germany) was used for optical trapping

and simultaneous TPF measurement of HIV-1 virions<sup>29</sup>. Briefly, the trapping laser was focused to a diffraction limited spot using a 60× water immersion microscope objective (Nikon) with a numerical aperture of 1.2. We diluted the live virus stock in complete media to a concentration of  $0.4\sim 4.0 \times 10^8$  virions/ml and injected them into a microfluidic chamber for optical trapping. Brownian motion of the trapped virions was recorded using BFP interferometry<sup>44</sup> at 62.5 kHz for 10 s<sup>36</sup>. To measure virion diameter in culture fluid, a closed-loop nanopositioning stage (3D200, Mad City Labs) was used to oscillate the microfluidic chamber, the amplitude of which was measured directly using video microscopy (Supplementary Fig. 13). For trapping of virions, control experiments showed that oscillation did not induce any change in thermal background. An electron-multiplying charge-coupled device (EMCCD) camera (Evolve, Photometrics) was used for all fluorescence detection. To collect TPF with single-molecule sensitivity, a motorized filter wheel was installed in front of the EMCCD camera, in which the TPF from EGFP was monitored using an emission filter (HQ525/50m, Chroma) and the TPF of Alexa-594 was monitored using an emission filter (ET645/75, Chroma). In addition, a short pass filter (E700sp-2p, Chroma) was installed in front of the EMCCD camera to block the 830 nm trapping laser. A laser power of 130.8 mW at the focus was used throughout for optical trapping and simultaneous TPF excitation. The laser power was monitored using a position-sensitive detector and kept within 1% variation throughout all the experiments. The fluorescence averaged over the initial 2 s exposure time was recorded as the initial fluorescence of the virion. For the two-color experiments, the viruses bound with Alexa594-b12 were injected into the microfluidic chamber. Upon trapping of individual particles in culture media, the TPF emission from Alexa-594 was measured first and then filter was switched to EGFP channel to measure EGFP TPF. The residue leakage of EGFP channel fluorescence into Alexa-594 channel was experimentally measured and quantified by linear regression (Supplementary Fig. 7) and this information was used to correct for Alexa-594 TPF throughout. All the TPF was collected as described using Nis-Element (Nikon), with an EM gain of 200 and exposure time of 400 ms, except the TPF time courses in Fig. 1, where an exposure time of 1 s without EM gain was used. All the trapping and TPF experiments were conducted at a constant temperature of  $20.0 \pm 0.2$  °C in complete media, which consisted of DMEM supplemented with 10% Fetal Bovine Serum (HyClone). The step-finding algorithm that we developed recently<sup>52</sup> was used to identify steps from all single-molecule traces. All the correlation analysis was done using custom-written MATLAB scripts and the correlation coefficients were calculated using MATLAB built-in functions. Throughout this work, all errors are standard deviations unless otherwise noted.

## Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

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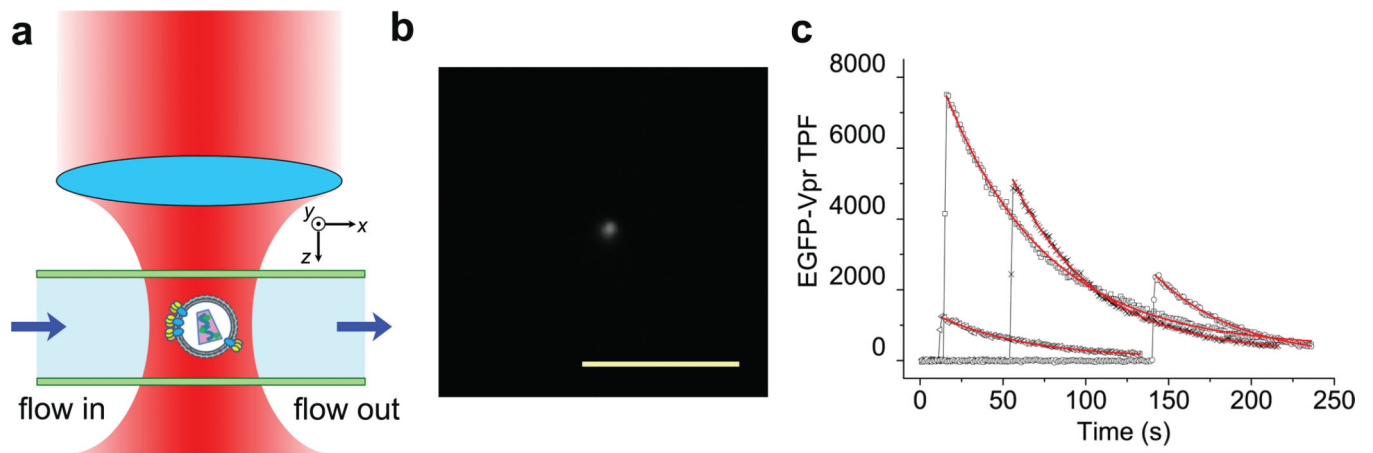
(NIAID), National Institutes of Health (NIH): pNL4-3 from Dr. Malcolm Martin; pNL4-3.Luc.R-E- from Dr. Nathaniel Landau; pEGFP-Vpr from Warner C. Greene; TZM-bl cells from Dr. John C. Kappes, Dr. Xiaoyun Wu and Tranzyme Inc; b12 antibody from Dr. Dennis Burton and Carlos Barbas.

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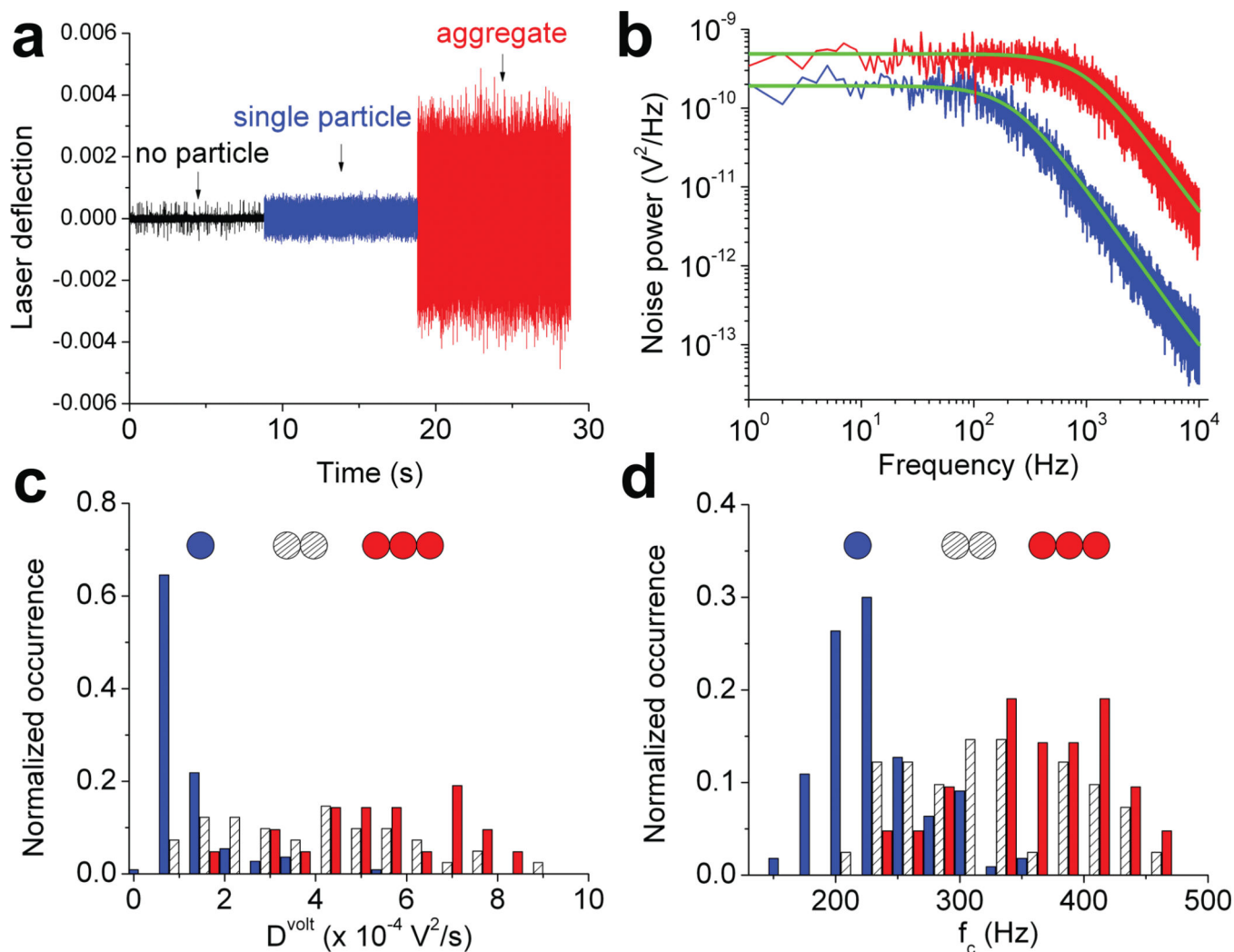
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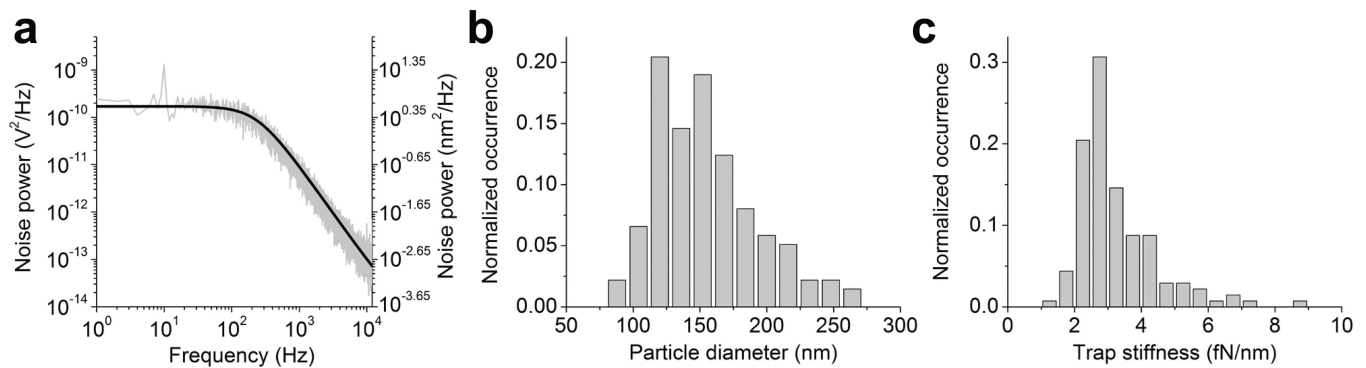


**Figure 1.**

Optical trapping of HIV virions in culture fluid. (a) HIV-1 virions were delivered into a microfluidic chamber and trapped by the IR laser focused at the center of the chamber. The  $xyz$  dimensions are shown as indicated, with  $y$  perpendicular to the figure plane. (b) TPF image of a trapped HIV virion. The scale bar is  $10\ \mu\text{m}$ . (c) Representative TPF time courses from individually-trapped HIV virions. All traces were fit with single exponential decay (red), with time constants for each trace as follows: 60.7 (square), 49.5 (cross), 51.5 (circle) and 54.1 s (triangle). Time zero started with the onset of TPF collection.

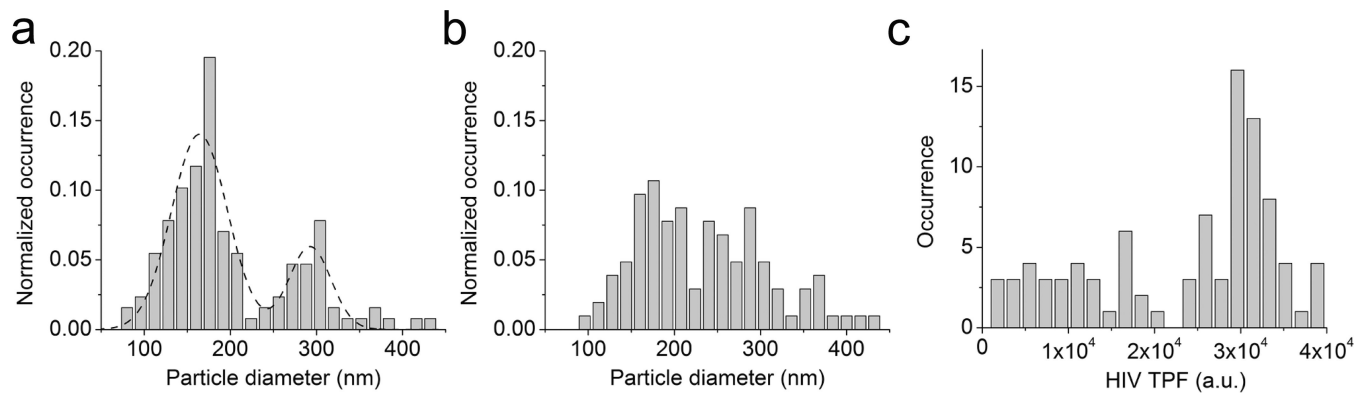


**Figure 2.** BFP interferometry to distinguish single HIV-1 particle from aggregates in complete media. (a) The laser deflection signal measured in real time using BFP interferometry. (b) Power spectra calculated from the data shown in (a) and fit to aliased Lorentzian with  $D^{\text{volt}}=8.53 \times 10^{-5} V^2/s$ ,  $f_c=223$  Hz (blue) and  $D^{\text{volt}}=0.0046 V^2/s$ ,  $f_c=982$  Hz (red). Histograms for  $D^{\text{volt}}$  (c) and  $f_c$  (d) derived from Lorentzian fitting parameters for apparent one (blue,  $N=110$ ), two (hashed,  $N=41$ ) and three (red,  $N=21$ ) particles trapped, with cartoons representing one, two and three particles above each histogram.



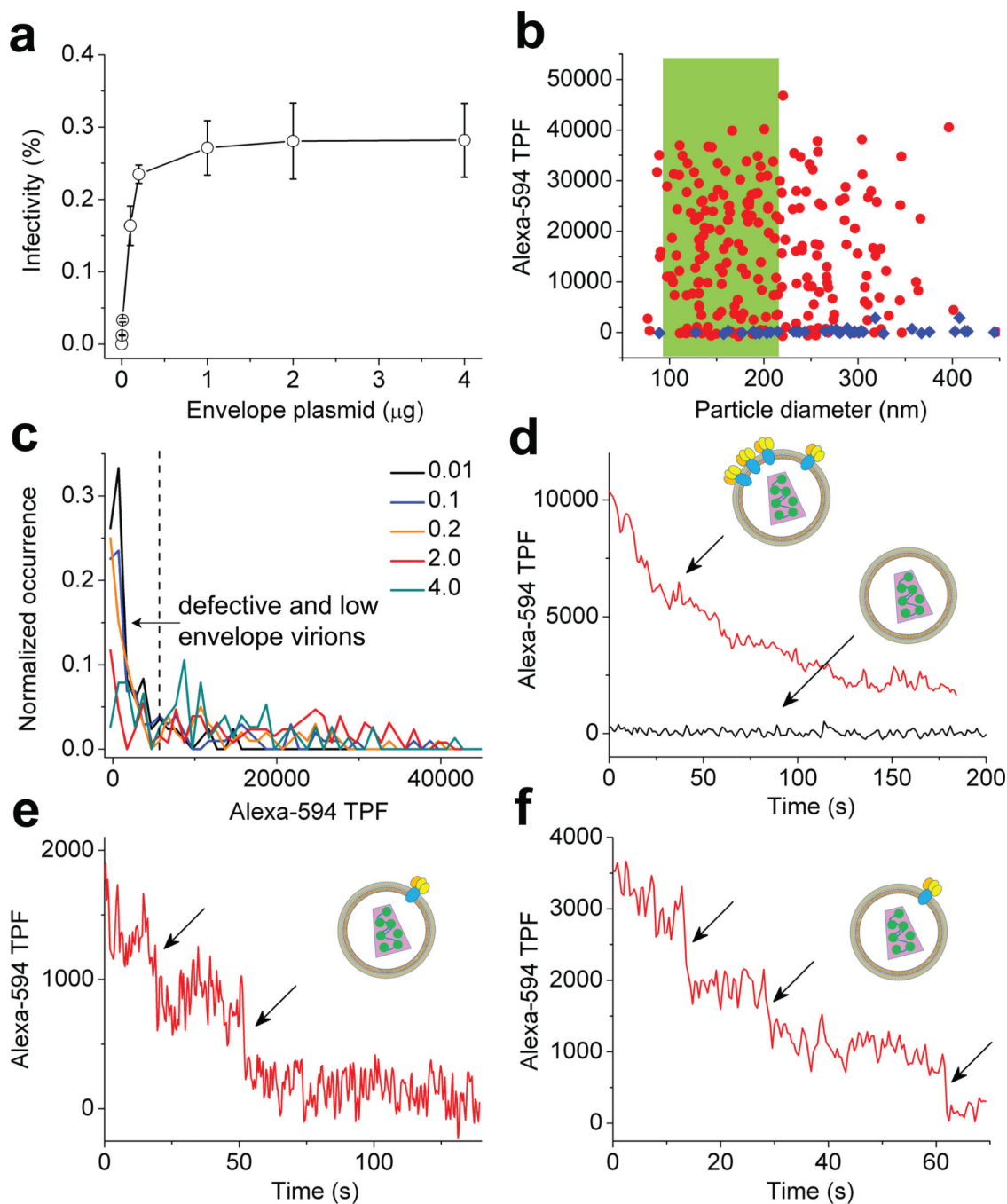
**Figure 3.**

Measurement of diameter for single HIV-1. (a) The power spectrum of a trapped virion when the chamber was oscillated at 10 Hz with amplitude of 176 nm along y-axis of the sample plane (Methods). The black curve is fitting of the thermal noise background to aliased Lorentzian with  $D^{\text{volt}}=9.37 \times 10^{-5} \text{ V}^2/\text{s}$  and  $f_c=233 \text{ Hz}$ . (b) Size histogram for single fluorescent particles from chamber oscillation along y-axis ( $N=137$ ). Concentration of the HIV-1 inside the chamber is  $4.0 \times 10^7$  virions/ml. (c) Distribution of the optical trap stiffness for each virion trapped ( $N=137$ ).



**Figure 4.**

Aggregation of HIV-1 observed at high virion concentrations. (a) Size histogram for single fluorescent particles from chamber oscillation along y-axis and its double-Gaussian fit (dashed line) (N=128). Concentration of the HIV-1 inside the chamber is  $1.2 \times 10^8$  virions/ml. (b) Size histogram for single fluorescent particles from chamber oscillation along y-axis (N=103). Concentration of the HIV-1 inside the chamber is  $4.0 \times 10^8$  virions/ml. (c) Distribution of EGFP-Vpr TPF intensity from trapped virions that are confirmed to be single based on diameter measurement in (a) (N=92).



**Figure 5.** Optical trapping virometry. (a) Infectivity of HIV-1 virions as a function of pEnv in the presence of 20  $\mu\text{g/ml}$  DEAE-dextran. The error bars are standard deviations from three independent replicates. (b) Alexa-594 TPF as a function of particle diameter. Red circles are for HIV-1 from 2  $\mu\text{g}$  pEnv (N=231) while blue diamonds are for virions without envelope (N=42). (c) TPF intensity histograms for Alexa-594 from single HIV-1 particles, with black, blue, orange, red and olive curves for virions from 0.01 (N=84), 0.1 (N=102), 0.2 (N=100), 2.0 (N=128) and 4.0  $\mu\text{g}$  pEnv (N=76), respectively. (d)–(f) representative Alexa-594 TPF



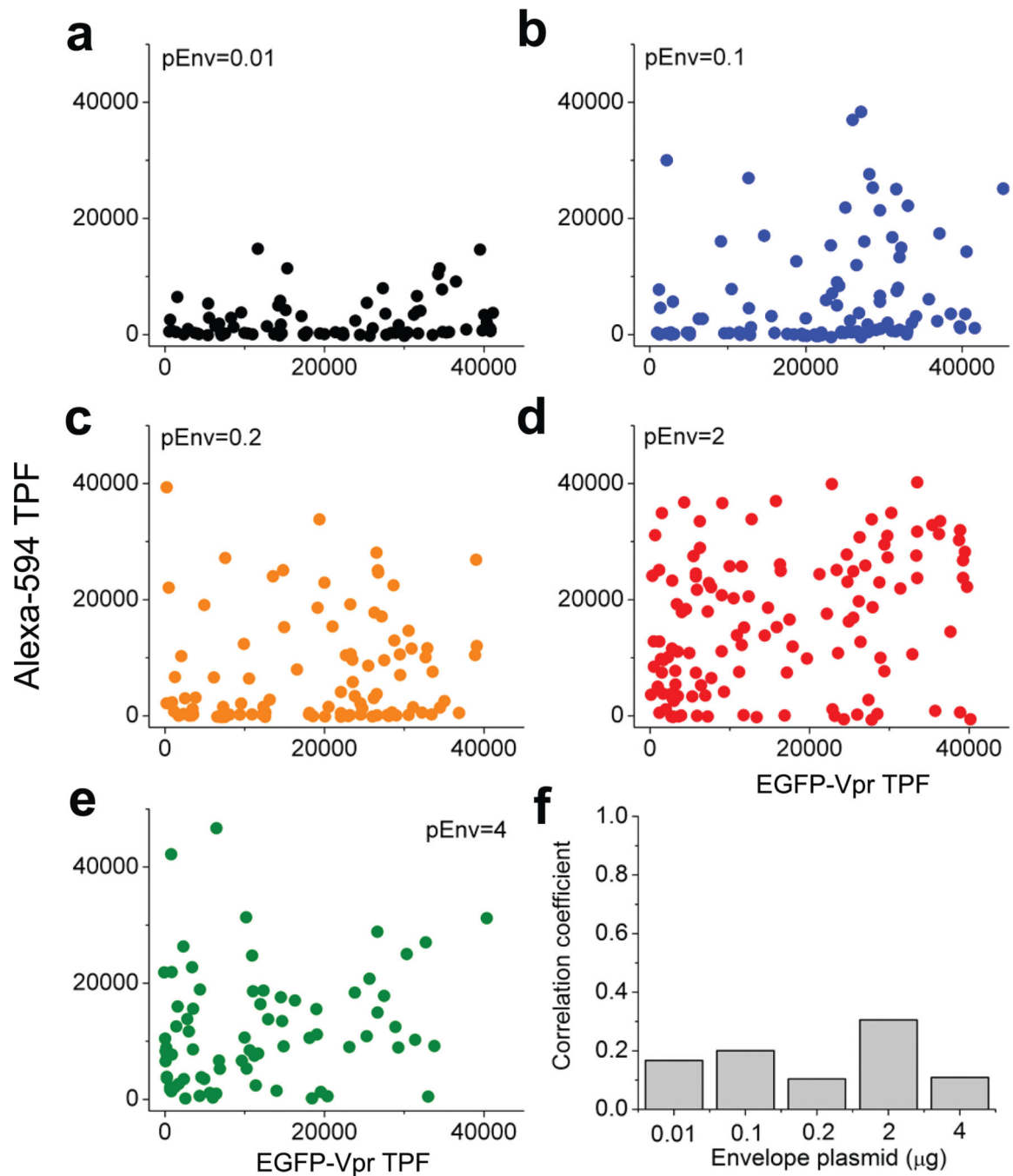
time courses from single virions bound with Alexa594-b12, where individual photobleaching steps in (e) and (f) are indicated with arrows. Insets, cartoons of HIV-1 virions with varied numbers of envelope glycoproteins.

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**Figure 6.**

Two-color correlation analysis for EGFP-Vpr and envelope glycoproteins in single HIV-1 virions. (a)–(e) Alexa-594 TPF was plotted as a function of EGFP-Vpr TPF for virions prepared with 0.01, 0.1, 0.2, 2 and 4  $\mu$ g pEnv, respectively as indicated (the same color code as Figure 5c). (f) The correlation coefficients calculated for each panel from a to e as a function of the pEnv inputs during virion production.