

WJO 5<sup>th</sup> Anniversary Special Issues (5): Knee**Neuromuscular interactions around the knee in children, adults and elderly**

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**Abstract**

Although injury and neuromuscular activation patterns may be common for all individuals, there are certain factors which differentiate neuromuscular activity responses between children, adults and elderly. The purpose of this study is to review recent evidence on age differences in neural activation and muscle balances around the knee when performing single joint movements. Particularly, current evidence indicates that there are some interesting similarities in the neuromuscular mechanisms by which children or the elderly differ compared with adults. Both children and elderly display a lower absolute muscle strength capacity than adults which cannot fully be explained by differences in muscle mass. Quadriceps activation failure is a common symptom of

all knee injuries, irrespective of age but it is likely that its effect is more evident in children or adults. While one might expect that antagonist co-activation would differ between age categories, it appears that this is not the case. Although hamstring: quadriceps ratio levels are altered after knee injury, it is not clear whether this is an age specific response. Finally, evidence suggests that both children and the elderly display less stiffness of the quadriceps muscle-tendon unit than adults which affects their knee joint function.

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**Key words:** Knee stability; Knee joint; Stiffness; Electromyography; Strength imbalance; Aging, Co-activation; Age; Injuries

**Core tip:** Children and elderly display a lower absolute muscle strength capacity than young adults. This may be due to a higher quadriceps activation failure as well as a more compliant quadriceps muscle-tendon in children (probably due to maturation) and elderly (due to age effects on neuromuscular system) than adults which, in turn, leads to an altered strength capacity. In contrast, age differences in muscle co-activation are not age dependent. Current evidence precludes any conclusions on whether muscle strength balance ratios are age specific.

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**INTRODUCTION**

The well documented benefits of physical activity and

exercise for health include an increase in physical competency and psychosocial interaction as well as decreased health risks<sup>[1,2]</sup>. However, physical activity also carries a risk of injury<sup>[3,4]</sup>.

The knee joint is one of the most common injured joints<sup>[5]</sup>. Alteration of normal neuromuscular function around the knee is considered as a significant contributor to injuries. For this reason, restoration of neuromuscular function represents a fundamental aim of post-injury rehabilitation.

Although injury and neuromuscular activation patterns may be common for all individuals, there are certain factors which differentiate neuromuscular activity responses between children, adults and elderly. The effects of growth and maturation on neuromuscular function have not been thoroughly investigated but there is evidence that children display different neuromuscular profiles compared with adults. It is also known that aging has a significant impact on the force generation capacity of the muscular system which is accompanied by changes in neuromuscular activation patterns. The purpose of this study is to review current and recent evidence on neural activation and muscle strength balances around the knee in children, adults and aged individuals. The main research question was whether there are similarities in neuromuscular interaction during single joint tests across the life span.

There are numerous techniques to evaluate neuromuscular function depending on the scope of assessment and the applied methodology. Evaluation may help in the understanding of the causes of knee injury, and aid in the development of more effective training and rehabilitation programs<sup>[6,7]</sup>. After providing a brief introduction on knee injury epidemiology, age differences in four different areas of neuromuscular function will be examined. First, the ability of the central nervous system to provide the essentially stimuli for muscular activation are examined. This is translated into quantification of the extent the central nervous system is able to activate the entire motor pool. Second, muscle co-activation which is defined as the simultaneous activity of various muscles acting around the knee will be examined. This is achieved mainly by comparing electromyography (EMG) signals of the antagonistic muscle groups of the knee. Third, muscle strength imbalances around the knee will be examined, mainly refereeing to the hamstrings (H) to quadriceps (Q) moment ratio (H:Q ratio) during isometric or isokinetic tests. Forth, factors related to the properties of the muscle-tendon units of the knee joint and their role for knee joint function will be presented. This study will focus on experimental evidence from single joint movements rather than multi-joint activities.

## RESEARCH

A worldwide review of published work on neuromuscular interactions during single joint movements was conducted. Studies were selected for this review if they were written in English, they focused on neuro-muscular

or musculo-tendinous strategies during knee joint tests. The literature search was performed from date of inception until end of November 2013 on the following electronic databases: Scopus (1995-2013), Web of Science (1970-2013), PubMed (1948-2013), Proquest, CINAHL, EBSCO, Embase, and Cochrane. The use of key words “knee”, “age-related”, “neuromuscular”, “children” “knee flexors”, “knee extensors”, “activation level”, “neural adaptation”, “ageing”, “muscle strength”, “antagonist”, “coactivation”, “co-contraction”, “tendon stiffness” “injury mechanisms”. Studies excluded were non-English language papers, conference abstracts, research reports, personal correspondence. A total of 831 studies that met the inclusion criteria were assessed by two co-authors followed by blind assessment by a third co-author with respect to: (1) sample size; (2) reliability of measurement protocols; and (3) clear data presentation. Case studies or studies which did not report the reliability of their protocol or their data were not clearly presented were excluded from the analysis.

## KNEE INJURY EPIDEMIOLOGY: A SHORT OVERVIEW ON AGE DIFFERENCES

The current literature on knee injuries is extensive and it cannot be fully presented in this review. Nevertheless, it is worthwhile to provide a brief overview on potential similarities and differences in knee injury profiles across lifespan.

Knee injuries are frequently seen in the everyday clinical practice of orthopaedic surgeons and general practitioners. In the general population, the incidence is suggested to be 11 cases per 1000 person-years<sup>[8]</sup>. In a recent study, Gage *et al*<sup>[9]</sup> examined 6664324 knee injuries and they found that individuals aged 15 to 24 years displayed the highest injury rate while children younger than 5 years had the lowest rate which is confirmed by similar studies in this area<sup>[8,10,11]</sup>.

The most common injury is a knee sprain without clearly identifiable internal derangement, and the most common diagnoses are anterior cruciate ligament (ACL) tear (20.3%), medial meniscus tear (10.8%) and chondral lesion (10.6%)<sup>[10]</sup>. Other frequent diagnoses include acute patellar dislocation (22%) and collateral ligament tear (9%)<sup>[12]</sup>.

There are various factors which have been considered to increase the risk for knee joint injury. In general, a higher age increases the risk of disabling knee injuries<sup>[13]</sup>. However, it appears that risk factors act in combination with other factors rather than individually. For example, higher age, obesity, and poor physical conditioning are frequently suggested to be risk factors for musculoskeletal injuries as a whole<sup>[13-15]</sup>. In another example, a higher age combined with higher weight increase the risk for deeper chondral lesions<sup>[15]</sup> as well as knee injuries in general<sup>[12]</sup>. The number of chondral lesions increases with age<sup>[16]</sup>.

Systematic participation in sports and gender are ad-

ditional factors which are also related to a higher injury risk. It is not surprising that current literature focuses primarily on young athletes<sup>[3,10,17-19]</sup>. For example, knee injuries are reported to account for 60% of high school sports-related surgeries<sup>[17,20]</sup>. Patellar dislocations typically occur in young adults during sports<sup>[21]</sup>. Risk factors for acute patellar dislocations are suggested to be higher height and weight<sup>[12,22]</sup>. Participation in sports, quadriceps muscle weakness, and female sex are associated with ACL tears<sup>[23-26]</sup> while all these factors acting in combination with older age increase the risk for meniscal tears<sup>[5,27]</sup>. Further, female athletes have been reported to be four to six times more likely to sustain a major knee injury<sup>[17,20]</sup>.

Individuals 65 years and older sustained a higher proportion of injury due to stairs, ramps, landings, and floors (42.0%), compared to adults and children<sup>[9]</sup>. Furthermore, ageing is a well-defined risk factor for knee osteoarthritis, as the risk for osteoarthritis increases by 2 to 10 times in people between 30 and 60 years of age and even more for individuals above 60 years<sup>[28,29]</sup>. Knee arthritis is more common among men below the age of 50, while it is more frequent among women above this age<sup>[30]</sup>. Obesity and overweight are also known risk factors for knee osteoarthritis, due to mechanical overload of the knee joints<sup>[30,33]</sup>. Occupations requiring repetitive weight-lifting and squatting<sup>[34]</sup> as well as repetitive knee torsion<sup>[35]</sup> and knee bending have been associated with knee osteoarthritis.

To summarize, it appears that knee injury rates are higher in young adults than children and the elderly. Adults suffer mostly from ligamentous injuries chondral lesions and sprains, children display less serious injuries while arthritis represents a characteristic injury of older individuals. Knee injury risk factors, such as obesity, gender, body mass index and poor physical conditioning or systematic participation in sports contribute to injury, irrespective of age.

## COMMON NEUROMUSCULAR MECHANISMS AROUND THE KNEE

### Arthrogenic muscle inhibition

Knee injury or surgery or arthritis lead to weakness of the quadriceps muscle group<sup>[36-40]</sup>. One of the factors responsible for this atrophy is an on-going neural inhibition that prevents the quadriceps from being fully activated, a process known as arthrogenic muscle inhibition. This inhibition has been quantified using EMG or the interpolated twitch technique. In addition, activation failure can be induced by experimentally creating an effusion (*via* saline injection into the joint) which is typically seen after knee surgery<sup>[41]</sup>.

Even early after injury, quadriceps weakness can be substantial, despite little time for atrophy<sup>[36]</sup>. Quadriceps EMG signal reduction ranges from 50% to 70% in the first few hours after meniscectomy; it then increases up to 80% for the next 3 d and it remains at high levels up to 15 d<sup>[42]</sup>. The reduction in the quadriceps EMG is some-

what lower after total knee arthroplasty reaching 30% in the first 4 wk after surgery<sup>[43]</sup>. Following ACL surgery, activation failure continues for approximately 6 mo<sup>[44,45]</sup> but it is gradually reduced to 6% deficit 18 mo after<sup>[46]</sup>. Similarly, total knee arthroplasty is followed by significant quadriceps inhibition up to 6 mo<sup>[47]</sup> and 24% decline 33 mo<sup>[47]</sup> after surgery.

The magnitude of quadriceps failure depends on the severity of joint damage, especially in individuals with ACL problems. For example, Urbach *et al*<sup>[48]</sup> found a lower central activation deficit in 30 patients with isolated rupture of the ACL compared with that displayed by patients with ACL rupture and accompanying joint damage. ACL rupture leads to a 3%-8% decline in quadriceps activation<sup>[36,49]</sup> while ACL rupture with simultaneous damage in other joint structures leads to a higher decline<sup>[48,50]</sup>.

Central activation failure can also affect the uninjured side<sup>[36,49-51]</sup>. Becker *et al*<sup>[51]</sup> showed that patients who underwent partial meniscectomy displayed a 20% failure in the injured side and 17% failure in the contralateral side. Similar results were reported for individuals who experienced an ACL injury<sup>[49]</sup> which led the authors to conclude that the difference between ACL injured patients and controls is due to a reduction in muscle size and activation failure. Chmielewski *et al*<sup>[36]</sup> also reported a decline in central muscle activation of 21% in both limbs post ACL-surgery<sup>[36]</sup>. Would this indicate a generalized activation failure and not solely a preferential one? The implication for testing and rehabilitation after knee surgery is that using strength measurements of the uninvolved limb as targets for rehabilitation of the involved limb may set lower strength targets than needed. In fact, Urbach *et al*<sup>[48]</sup> reported that due to contralateral deficits in central activation, the mean underestimation of the isometric muscle-force deficit ranged from 22% to 48%. Therefore, the validity of tests for the assessment of muscle function when using the uninjured side as reference was questioned. Others, however, did not find a quadriceps inhibition of the contralateral limb<sup>[52]</sup> proposing that rehabilitation protocols after knee joint injury should focus on ipsilateral and not bilateral neuromuscular and mechanical alterations that occur as a result of joint damage.

There are several factors which may contribute to activation failure such as swelling<sup>[53]</sup>, pain<sup>[54]</sup>, inflammation<sup>[55]</sup> and damage to joint receptors<sup>[56]</sup>. For example, activation failure may be due to swelling<sup>[53]</sup> and an associated increase in intraarticular pressure<sup>[57]</sup>. Since intraarticular pressure is higher towards knee extension, inhibition will be greater near extension rather than flexion<sup>[58]</sup>. For these reasons, in the acute stages after injury or surgery, isometric quadriceps exercises should be performed in 30 to 50° of knee flexion, where intraarticular pressure is the lowest<sup>[40]</sup>.

The mechanisms responsible for arthrogenic inhibition vary and include both central and peripheral nervous system. In a recent review, Rice *et al*<sup>[40]</sup> identified three spinal pathways which may affect arthrogenic inhibition. First, inhibition of group I nonreciprocal interneurons

which receive inputs from tendon organs. Second, an enhanced flexion reflex that inhibits agonist activity and facilitates antagonist muscle activation<sup>[59]</sup>. Third, a deficit in the transmission of Ia input to the motoneuron pool, termed  $\gamma$ -loop dysfunction may be observed after ACL injury<sup>[60,61]</sup>. In addition, to the above spinal mechanisms, the role of corticomotor excitability as a contributor to activation failure was also examined. Interestingly, Heroux and Trenblay<sup>[62]</sup> reported a higher excitability of corticomotor projections targeting muscles in ACL deficient individuals. It has been proposed that this increase in corticospinal excitability may serve to counteract a-motoneuron inhibition by spinal reflex pathways<sup>[40]</sup>.

In summary, atrogenic muscle inhibition represents a common symptom seen after many knee injuries. In many instances, clinicians consider reduced quadriceps strength as a result of muscle atrophy. However, the presence of inhibition after injury indicates that interventions employing only muscle strengthening exercises are not entirely appropriate to enhance neuro-muscular function. The use of techniques to increase quadriceps activation, such as electrical stimulation, has the potential to increase the effectiveness of rehabilitation programs.

### Muscle co-activation

Neuromuscular function is not only related to the ability to recruit the entire motor unit pool of a certain muscle but also to the ability to achieve an optimal activation of all muscles acting around the knee. Muscle co-activation has been examined by comparing the surface electromyographic (EMG) signal of the involved muscles expressed as percentages of reference EMG values<sup>[63-67]</sup> or by using the EMG signals to calculate a co-contraction index<sup>[68]</sup>. Numerous studies have examined antagonist co-activation levels during various activities<sup>[69-72]</sup>. Antagonist co-activation of the hamstrings in most movements ranges from 5% to 10% and increases in more demanding activities such as chair up and down exercises<sup>[69]</sup>.

Early evidence indicated that hamstrings co-activation represents a reflex response to ACL loading which is also accompanied by quadriceps inhibition<sup>[64]</sup>. The presence of mechanoreceptor input provided by the cruciate ligaments have been confirmed in healthy individuals<sup>[73]</sup> but it is absent following surgical ACL reconstruction<sup>[74]</sup>. This was supported by several studies showing a higher hamstring EMG in ACL deficient patients during the impact phase of the side-step cutting manoeuvre<sup>[75]</sup>, walking<sup>[76,77]</sup> or landing<sup>[78]</sup> although such patterns have not always been confirmed<sup>[79,80]</sup>. In addition, some studies have reported an earlier onset of muscle activity during the late stance phase of walking after ACL injury<sup>[76,77,79]</sup>. The increased and earlier hamstring and gastrocnemius activation in ACL deficient individuals aims to maintain the knee joint stable by preventing anterior subluxation as the ground reaction forces increase upon heel contact<sup>[76-77]</sup>. In addition, increased level of antagonist co-activation increases joint active stiffness<sup>[69]</sup>. This is also related with proprioception deficits often observed in ACL deficient knees<sup>[81]</sup>.

More recent evidence indicates that non-contact ACL injuries are more likely when total hamstring pre-activation is much less than the corresponding quadriceps pre-activity during side cutting<sup>[82]</sup>. Furthermore, a higher hamstring coactivation near terminal knee extension was observed in ACL deficient individuals compared with uninjured individuals<sup>[83]</sup>. The observation that co-activation is found in both uninjured and injured individuals led Alkjaer *et al.*<sup>[83]</sup> to suggest that antagonist co-activation is not only a reflex response but it may be modulated by central motor programming. Some evidence seems to support this statement<sup>[84,85]</sup>, although, clearly more concrete evidence is necessary.

Using mathematically or EMG-driven models, research studies have estimated the antagonist moment in healthy subjects<sup>[86,87]</sup> and in ACL deficient subjects<sup>[83-84]</sup> as well as its effect on joint forces<sup>[73,86,88,89]</sup>. Isolated contraction of the quadriceps increases shear force between the tibia and the femur at the last 20° of knee extension which is partly counteracted by hamstring activation<sup>[86,88,89]</sup>. This results also in a wider pressure distribution along the articular surfaces of the joint and prevents early tissue damage and osteoarthritis<sup>[73]</sup> while it may reduce ACL strain at angles near full extension<sup>[90]</sup>. This notion is supported by modeling data by Yangawa *et al.*<sup>[91]</sup>, which confirms that coactivation of the hamstring muscles during isolated dynamic (isokinetic) knee extension effectively reduces anterior tibial translation. Further evidence seems to confirm these findings as a higher hamstring coactivation and moment near terminal knee extension was observed in ACL deficient individuals compared with uninjured individuals<sup>[83]</sup>. The elevated antagonist hamstring moment observed in the ACL deficient subjects may reflect a compensatory neuromuscular adaptation to counteract the increased laxity of the knee joint<sup>[83]</sup>. However, others have not found any difference in antagonist hamstring moment between ACL deficient, ACL reconstruction, and uninjured individuals<sup>[84]</sup>. Methodological issues in EMG - moment data treatment may account for these variations<sup>[83]</sup> which guarantees further research in this area.

### Strength imbalances

Since neuromuscular activation is altered in knee pathological conditions, then changes in force generation capacity of the surrounding musculature may be observed. These are also accompanied by alterations in size of the muscle as a result of injury or subsequent immobilization. Muscular imbalances around the knee refer mainly to the relationship between absolute muscle strength developed by antagonistic muscle groups. The H:Q peak moment ratio takes into consideration the function of two opposing (agonist-antagonist) muscle groups and it represents the most frequent parameter used to estimate muscle strength balance<sup>[6,7,92]</sup>.

The methods used to calculate the H:Q strength ratios vary. Early research studies have mainly examined the concentric H:Q ratios, frequently defined as “conventional” ratios<sup>[93,94]</sup>. A theoretical value of 0.6 of the ratio ob-

tained frequently under isometric or slow isokinetic concentric tests is often considered as “normal”<sup>[95]</sup>. However, conventional ratios have been gradually replaced by the “functional” ratios which involve the calculation of eccentric H: concentric Q ( $H_{ecc}:Q_{con}$ ) muscle strength ratio<sup>[6,7,92,93,96]</sup>.

There has been a long debate on the usefulness of antagonist to agonist strength ratios as an injury predictor or as a target for restoring normal knee muscle function<sup>[97]</sup>. A methodological approach is to measure H:Q ratio in athletes in the pre-season period and follow this for the forthcoming seasons. It has been found that athletes with a  $H_{con}:Q_{con}$  ratio closer to 1.0 may have a reduced risk of hamstrings strain<sup>[98]</sup>. Also, a  $H_{con}:Q_{con}$  ratio closer to 1.0 in athletes with ACL injury has been suggested to reduce the risk of an anteriolateral subluxation of the tibia<sup>[99]</sup>. Croisier *et al.*<sup>[100]</sup> identified a lower  $H_{ecc}:Q_{con}$  ratio in players with a previous hamstring injury during the pre-season assessment and applied a rehabilitation program to restore the ratio into normal values. They then followed the players for 12 mo. Their results showed that none of the players experienced a re-injury. Further, epidemiological evidence in 462 players followed for one season showed a total of 35 hamstring injuries, most of which were experienced by players with lower  $H_{con}:Q_{con}$  and  $H_{ecc}:Q_{con}$  ratios<sup>[101]</sup>. Recently, Kim *et al.*<sup>[95]</sup> found an association of lower than 0.6 of the  $H_{con}:Q_{con}$  ratio at 60°/s and non-contact leg injuries in National College American Association athletes. In an almost parallel study, Fousekis *et al.*<sup>[102]</sup> reported that professional soccer players with  $H_{ecc}$  strength asymmetries were at greater risk of hamstring strain while players with  $Q_{ecc}$  strength and flexibility asymmetries were at greater risk of quadriceps strain.

Other studies have examined the ability of H:Q ratio to identify individuals with knee joint problems from uninjured ones. Early studies have identified<sup>[79,92]</sup> a significantly lower isokinetic Q moment in patients with ACL deficiency compared to healthy subjects while  $H_{ecc}$  and  $H_{con}$  moment deficits were not as significant. This is in line with later studies<sup>[103,104]</sup> who reported a higher H:Q ratio in subjects with ACL reconstruction<sup>[103,104]</sup> compared with uninjured individuals. Similar findings have been reported when comparing individuals with knee osteoarthritis with controls<sup>[105,106]</sup> which may indicate that compensation strategies with regards to antagonist to agonist muscle balances are more generic than solely ACL problems.

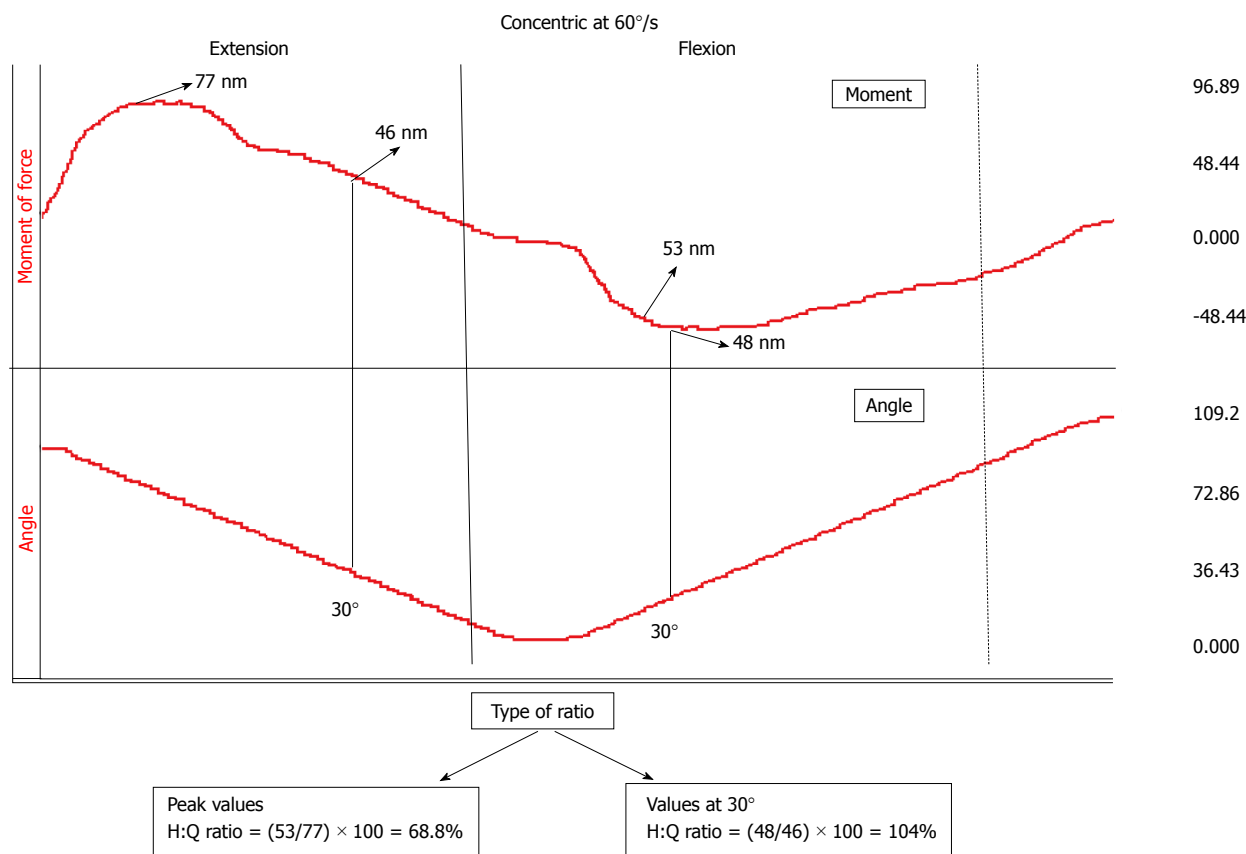
Knee related injuries may also be due to differences in strength between the two legs. Furthermore, strength levels of the unaffected limb frequently represent a reference value against which restoration of strength of the affected limb. Evidence on bilateral leg differences in soccer players is unclear as some studies have reported no differences<sup>[107]</sup> whereas others reported a 10% difference in both Q and H strength in favor of the non-dominant leg<sup>[108]</sup>. Others, however, have shown that bilateral leg differences exist only in the hamstrings but not in the quadriceps (players displayed weaker hamstrings in the

dominant leg than the non-dominant one)<sup>[109,110]</sup>. The existence of muscle specific bilateral differences in strength led researchers to explore whether H:Q ratios differ between limbs. Again, there is some evidence that the non-dominant or non-preferred limb shows somewhat higher ratios than the dominant one but still this evidence is not always statistically significant<sup>[108,111]</sup> or differs between tested speeds<sup>[110]</sup>. However, a lower  $H_{ecc}$  moment in the injured limb compared to the contralateral limb continues even after ACL reconstruction surgery<sup>[112]</sup>. It is not clear whether such deficits pre-existed or they were due to ACL injury or reconstruction.

Although functional ratios have been considered as better indicators of muscle balance, there is still not sufficient evidence supporting their use. A problem associated with the use of H:Q ratios is that they were assessed using peak force values during a maximum voluntary effort<sup>[113-115]</sup>. This raises two issues: (1) that injuries occur at a specific joint angle while the H:Q ratio is calculated using peak force values irrespective of joint angle. The value of calculating the H:Q ratio at a specific joint angle, the one which is closer to the injury mechanism of the specific knee structure would be higher<sup>[116]</sup> (Figure 1). Particularly, peak moment H/Q ratio ranges from 0.5 and 0.6<sup>[96,117]</sup> and increases near full knee extension exceeding values of 1.0<sup>[117,118]</sup>. This increase was attributed to a relative dominance of the H near full extension<sup>[118]</sup> in order to stabilize the knee joint when the strain on the ACL is the greatest<sup>[90]</sup>. The shift of  $H_{ecc}/Q_{con}$  ratio at angles of knee extension was also attributed to a limitation in knee extensor motor unit recruitment at joint angles of greatest ACL strain<sup>[118]</sup>. Nevertheless, whether H:Q ratio at a specific joint angle can discriminate knee injured individuals from uninjured ones or to predict injury is still unclear; (2) during explosive movements, such as soccer match play situations, the time available to stabilize the knee joint is frequently very short (< 50 milliseconds)<sup>[119]</sup>. However, during a standard isometric test the peak force occurs within 400-500 ms from onset of contraction. This suggests that in most explosive movements there is no time available for maximum force generation. Thus, the relevance of using  $H_{con}:Q_{con}$  and  $H_{ecc}:Q_{con}$  based on peak values has been questioned<sup>[120]</sup>. In one of the first studies, Aagaard *et al.*<sup>[115]</sup> proposed that rate of force development (RFD), defined as the rate of rise in force at the onset of contraction, may be a better index of neuromuscular activity around the knee. Based on these aspects, Zebis *et al.*<sup>[120]</sup> have recently assessed the H:Q ratio using the RFD values obtained during maximum isometric contraction in twenty three soccer players. They reported that two female players who sustained an ACL injury had a normal H:Q peak force ratio but a low RFD H:Q ratio.

### Gender differences

Male and female relative H:Q ratio profiles differ significantly during and following puberty<sup>[121]</sup>. Isokinetic dynamometer measurements show that male athletes demonstrate significantly greater hamstrings peak torques with



**Figure 1** An example of different methods to calculate the hamstrings:quadriceps ratio. The raw data from moment of force (upper line) and angular position (lower line) as recorded from an isokinetic concentric knee extension-flexion trial. Using peak moment values results to a different ratio value compared with that obtained using values at a knee flexion angle of 30°. H: Hamstrings; Q: Quadriceps.

increasing maturity, while peak hamstrings torque remains stable with increasing maturational stage in female athletes<sup>[121]</sup>. Thus, it appears that lower hamstrings strength and H:Q ratios of female athletes relative to males may be related to the development of neuromuscular imbalances associated with the onset on maturation. These neuromuscular imbalances may increase injury risk in pubertal and post pubertal female athletes<sup>[121,122]</sup>. In a thorough review, Hewett *et al*<sup>[123]</sup> analysed 23 research studies and reported that isokinetic H:Q ratios do not differ between genders at slow velocities. As angular velocity increases, males display higher H:Q ratio than females. The authors commented that this difference may be related to females' decreased ability to dynamically control the knee joint during sports activities. However, more recent studies have reported an increase in both conventional and functional ratios in female athletes with increasing angular velocity<sup>[124,125]</sup>, which is not in line with the above conclusion. This might be due to differences in the characteristics of the samples examined, as both these studies referred to trained female athletes whilst data examined by Hewett *et al*<sup>[123]</sup> included mainly sedentary or untrained individuals.

Gender differences in knee injury occurrence are also related to more global neuromuscular differences that lead to injury than solely H:Q ratios. Muscle co-activation can decrease the dynamic valgus motion of the knee, which potentially places the knee at increased risk

of injury<sup>[123,126]</sup>. Individuals with chronic ACL deficiency showed lower internal/external rotation strength ratios than controls and acute ACL deficient subjects, indicating a compensatory mechanism developed by the patients to unload the ACL<sup>[103]</sup>. In contrast, ACL reconstruction patients showed fewer deficiencies compared with controls<sup>[103]</sup>.

Gender differences in hamstring and quadriceps muscle co-activation have also been examined. Palmieri *et al*<sup>[127]</sup> reported that females displayed lower co-activation than males and that medial co-activation had a linear relationship with external knee abduction moment in females only. A higher knee abduction moment is considered as a risk factor for ACL injury<sup>[128]</sup>. Therefore, it appears that females display a greater risk for ACL injury than males. Similar results were reported by Rozzi *et al*<sup>[129]</sup> upon landing from a jump. There is no single explanation on why females display deficits only on lateral muscles and not on the medial part. There are suggestions that lateral muscles may co-activate more than the medial ones to resist internal rotation moments which may increase ACL loading<sup>[130]</sup>. However, more evidence is necessary.

## NEUROMUSCULAR INTERACTIONS AROUND THE KNEE IN CHILDREN

Muscle strength increases during maturation, in terms

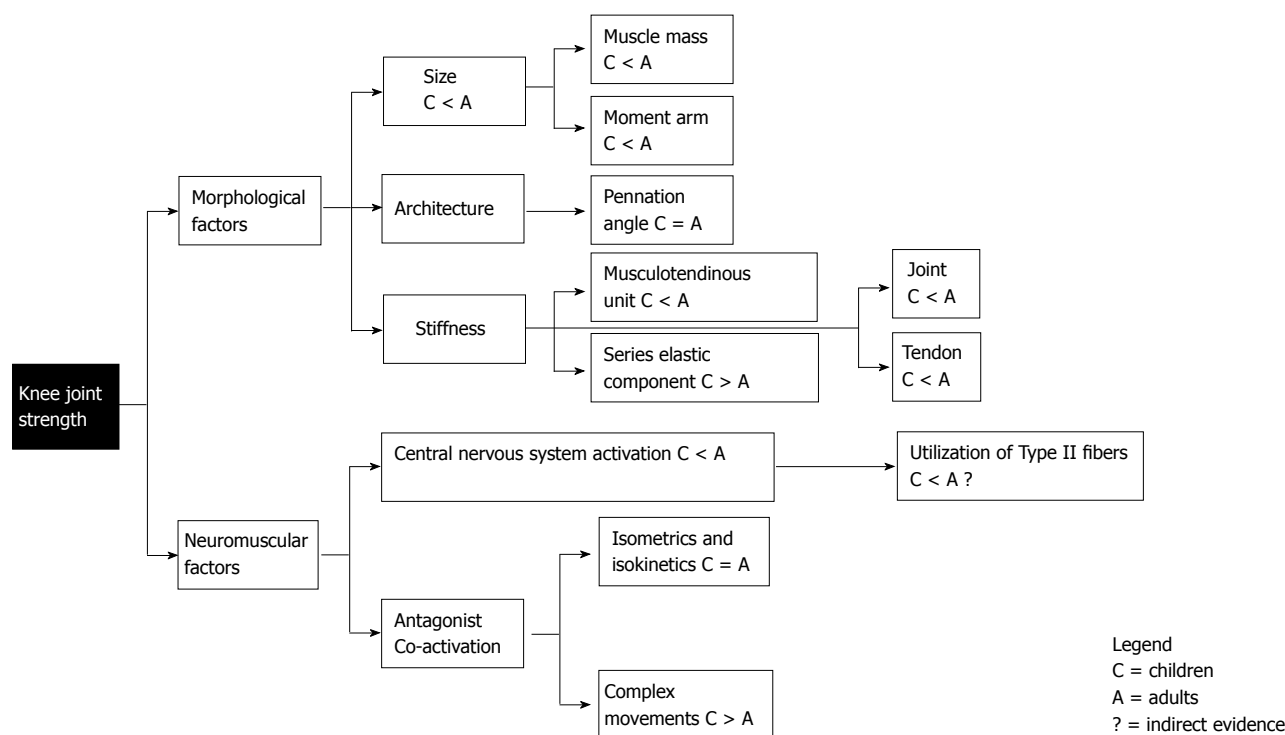


Figure 2 Schematic summary of comparison between children (C) and adults (A) regarding factors influencing knee joint strength.

of joint moment. This development is primarily a consequence of hormonal changes which result in muscle mass augmentation (hypertrophy)<sup>[131]</sup>, and in limb size increase (moment arm)<sup>[152]</sup>. However, differences in strength between children and adults cannot be fully explained by these parameters<sup>[133]</sup>. This designates the possible contribution of neuromuscular factors that could play a role in force deficit observed in children compared to adults. There are two main issues to mention regarding the neuromuscular aspect: Firstly, the level of central activation, *i.e.*, to what extent the central nervous system is able to activate the entire motor pool, and secondly, the level of antagonist co-activation, which reduces the net amount of moment produced around the joint. Hence, strength gain observed during developmental ages could be partly attributed to neural adaptations. In addition to this, differences between children and adults in muscle tendon unit (MTU) architecture and stiffness might also play a role on the force development around the knee joint (Figure 2).

Earlier studies have shown that the isokinetic strength normalized to cross sectional area (CSA) and thigh length is lower in 6-9 years old children compared to young adults<sup>[131]</sup>. The fact that this difference was more profound when the angular velocity was increasing reveals that muscle and limb size could not be the only factor affecting force production. This could be explained by findings supporting that children might have lower proportion of type-II muscle fibers<sup>[134]</sup>, which have fast contractile properties. However, several studies revealed no significant differences in muscle-fiber composition between children and adults<sup>[135,136]</sup>.

This raises the question whether children and adults possess similar proportion of muscle fibers types, but the former are not capable of fully recruit the fast ones. It has been shown that especially in large muscle groups, such as the quadriceps, children are incapable to fully recruit their motor units<sup>[137]</sup>. More recent studies using the twitch interpolation technique with magnetic or electric stimulation demonstrated that children activate their motor units in lesser extent than adults during knee extension<sup>[138]</sup>, and this is particularly evident in girls when compared to women<sup>[139]</sup>. This finding observed in children could at least partially account for their force deficit compared to adults. Furthermore, assuming that the size principle is valid for children too (*i.e.*, the higher the level of activation, the larger in size -and thus faster-motor units are recruited), it would be expected that children utilize in lesser extent type-II (fast) motor units compared to adults. This assumption is supported by experimental findings for the knee extensors, revealing that children have lower rate of torque development under isometric<sup>[140]</sup> and dynamic conditions<sup>[141]</sup>.

Despite the simplicity of using the anatomical CSA for the estimation of muscle size of children and adults, the most appropriate measure is the physiological CSA, which accounts for the pennation angle and is calculated as the ratio of muscle volume to fascicle length<sup>[138]</sup>. However, no difference between 8-10 years old children and adults is observed in the pennation angle of all quadriceps heads<sup>[138]</sup>. To our knowledge, no respective data exist in the current literature, regarding the pennation angle for the hamstring muscles in children and adults. This piece of information could have important implications, since

the pennation angle influences the shortening velocity of a muscle (and the force capacity of a muscle), and might affect the torque H:Q ratio at different contraction velocities.

Decreased torque H:Q ratio is an indicator for potential increased probability of lower extremity injury<sup>[142]</sup>. More particularly, it has been shown that collegiate athletes with isokinetic at 180 deg/s peak torque H:Q ratio less than 0.75 have higher incidence of injury<sup>[143]</sup>. According to cross-sectional studies, the isokinetic torque H:Q ratio at 60 deg/s remains unchanged from the age of 7 to 18 years, although the CSA H:Q ratio increases gradually after the age of 10 years<sup>[144]</sup>. On the other hand, post-pubescent athletes demonstrate a close correlation between the hamstrings and quadriceps CSA and the flexion and extension torque, respectively<sup>[145]</sup>. Furthermore, during puberty strength improvement of the knee flexors is diverged from the extensors, particularly for the females<sup>[121]</sup>. Although in males the hamstrings and quadriceps isokinetic peak torque increases proportionally during growth<sup>[107,121]</sup>, in females the peak torque of hamstrings does not follow the improvement achieved in quadriceps<sup>[121]</sup>. This deficit in knee flexion torque observed in females results in a decreased torque H:Q ratio. Further gender specific imbalances are observed on the level of knee anterior/posterior and medial/lateral muscle activation<sup>[146]</sup> during dynamic multijoint tasks. Females activate their quadriceps more compared to males<sup>[147-150]</sup> and this could contribute to the decreased H:Q ratio in torque output. Furthermore, decreased medial to lateral quadriceps<sup>[151]</sup> and hamstrings<sup>[129]</sup> activation ratio observed in females, could increase valgus, and varus laxity. These observations regarding the imbalances in activation level and torque output of the thigh muscles could increase the risk for ACL injury because hamstrings function synergistically with the ACL, especially at knee joint angles less than 45 degrees<sup>[64]</sup>.

A factor that could modify the torque H:Q ratio is the level of antagonist co-activation. However, no significant differences between children and adults have been observed<sup>[152,153]</sup>. Furthermore, in isometric contractions, the antagonist co-activation is even lower and still not significant between age groups<sup>[139,154]</sup>. On the other hand, co-activation is higher in children compared to adults when performing tasks involving multiple joints such as gait<sup>[155]</sup> and jumps<sup>[156,157]</sup>. This implies that movement coordination and learning factors might be an issue during developmental ages<sup>[135]</sup>, considering that the process of maturation of the corticospinal tract in terms of conduction velocity is not complete until the age of 11 years<sup>[158]</sup> and that the pyramidal system attains full functionality during puberty<sup>[159]</sup>.

Regarding the passive component of stiffness, Lebedowska and Fisk<sup>[160]</sup> have shown that passive knee stiffness increases with stature, within an age range between 6 and 18 years. Furthermore, Kubo *et al.*<sup>[161]</sup> measuring the tendon elongation of the vastus lateralis during isometric knee extension, concluded that the tendon of younger

boys was more compliant than older boys and young men. In line with the idea that the MTU is more compliant in children, Asai *et al.*<sup>[162]</sup> demonstrate that children had longer electromechanical delay compared to adults. This could also contribute to their reduced capacity to produce high rate of force development<sup>[140-141]</sup>. In contrast, series elastic component, quantified with quick-released movements in the knee extensors, revealed decreased stiffness with age<sup>[163]</sup>. The above differentiations in MTU stiffness between children and adults might influence the force/length relationship of the muscles acting around the knee joint. Stiffer MTU favors more direct force translation from the muscle to the bone<sup>[164]</sup>, whereas the opposite situation requires greater shortening velocity of the contractile apparatus, in which children are inferior<sup>[140,141]</sup>. The concept of differences in MTU stiffness that are reflected to changes in the joint torque/angle relationship has been supported<sup>[165]</sup> but also questioned<sup>[139]</sup> in previous studies, and therefore requires further investigation. More particularly, Marginson *et al.*<sup>[165]</sup> demonstrated that children demonstrate their maximal knee extension torque at more flexed joint angle (longer muscle) than adults, whereas O'Brien *et al.*<sup>[139]</sup> showed no difference in the optimal joint angle between children and adults.

It is apparent that the function of the knee depends on multiple factors, which are influenced during the developmental ages. Despite this complexity, O'Brien *et al.*<sup>[138]</sup> concluded that children's and adults' specific tension (the ratio between muscle strength and size) of the quadriceps is the same, taking into account differences in physiological cross sectional area, moment arm, level of activation, and co-activation. This implies that the muscle tissue is qualitatively very similar in children and adults. It is concluded that regardless of structural differences in muscle size, moment arm-joint angle relationship, central voluntary activation, H:Q ratio, and muscle-tendon stiffness, children's neuromuscular system is highly adaptive, although further systematic research with longitudinal studies are required to improve our understanding on the effects of growth and development in the force and power output of children.

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## NEUROMUSCULAR INTERACTIONS AROUND THE KNEE IN THE ELDERLY

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The aging process is associated with a significant decline in muscle strength (dynapenia) and strength development that might be caused by alterations of skeletal muscle properties as well as by neural modulations<sup>[166,167]</sup>. Regarding the knee joint, the reported age-related decrease in the measured isometric muscle force/moment of the knee extensors ranges from 19% to 38% when comparing groups of similar physical activity level<sup>[166,168-173]</sup> (Table 1). Even greater differences (50% or more) have been reported for people in their ninth decade and beyond<sup>[166]</sup>. When comparing the specific tension of the knee extensors between young and old women, a reduction of 17% during isometric contraction has been reported<sup>[174]</sup> (Table 1).



**Table 1** Information provided by cited articles about age-related reduction in muscle force

Ref.	Age-related reduction in muscle force/torque	Age of participants, yr	Testing condition	Physical activity level
Baroni <i>et al</i> <sup>[171]</sup>	30%-36%	y: 30 ± 6	Isometric KE	No systematic training
Laudani <i>et al</i> <sup>[173]</sup>	40%-53%	o: 69 ± 5 yr	Concentric KE (60-360°/s)	No systematic training
	36.9%	y: 28 ± 2	Isometric KE	Sedentary adults
		o: 70 ± 3		
Karamanidis <i>et al</i> <sup>[169]</sup>	21%	y: 21-32	Isometric KE	Endurance runners
	18.9%	o: 60-69	Isometric KE	Not active
Mademli <i>et al</i> <sup>[170]</sup>	28%	y: 30 ± 7	Isometric KE	Physically active
		o: 65 ± 3		
Savelberg <i>et al</i> <sup>[172]</sup>	33%	y: 23 ± 2	Isometric KE	Active runners
	43%	o: 65 ± 3	Isometric KF	Active runners
Macaluso <i>et al</i> <sup>[174]</sup>	17%	y: 23 ± 6	Isometric KE	Active
	30%	o: 70 ± 2	Isometric KF	Active
Frontera <i>et al</i> <sup>[195]</sup>	15.5%-22%	12-yr longitudinal study, initial mean	Isokinetic KF (60 and 240°/s)	Healthy
	17%-23%	age 65 ± 2	Isokinetic KE (60 and 240°/s)	Healthy

KE: Knee extension; KF: Knee flexion; Y: Young; O: Old.

The age-related decline in muscle strength is gender specific, with men losing almost twice as much strength as women<sup>[175]</sup>. Nevertheless, in absolute values, older women demonstrate significantly lower strength than men<sup>[176,177]</sup>, which can be explained predominantly by their higher fat mass<sup>[176]</sup>. Indeed, when investigating the decline in muscle quality of the knee flexors and extensors, *i.e.*, peak torque per unit of muscle mass, it was found that the rate of the decline was the same for both genders<sup>[178]</sup>. The higher proportion of body fat in women may put them at significant biomechanical disadvantage for greater disability in old age<sup>[176]</sup>. It seems that due to their gender-related lower average strength, old women may be at greater risk than old men of becoming impaired in certain motor tasks<sup>[177]</sup>.

Furthermore, when measuring knee extensor moments at different knee angle positions, the percentage loss of muscle strength was different at the different positions<sup>[168,179]</sup>. Karamanidis *et al*<sup>[168]</sup> found that the aging process revealed a clear reduction in maximal knee extension moment at intermediate knee joint angles (140° and 110°), but there was virtually no age effect at more extended (160° and 170°) or flexed (80°) knee joint positions. The authors proposed among other, two potential explanations for this phenomenon: (1) The discrepancy in the age-related reduction in muscle strength within the quadriceps muscles, with greater decline in Vastii (monoarticular) than in rectus femoris (biarticular) muscle<sup>[172]</sup>. It has been reported that, while the moment-knee-joint angle relationship of the Vastii muscles described by a parabolic curve having its vertex (maximum value) between 100° and 120°, the rectus femoris demonstrates a rather flat joint-moment-length curve<sup>[172]</sup>. Thus, it is possible that the relative contribution of the rectus femoris to the total knee extension moment is higher at more extended or flexed knee joint positions<sup>[172]</sup>, where no age-related effect on quadriceps muscle strength was found; and (2) The modulation of the EMG activity. In their study, Karamanidis *et al*<sup>[168]</sup> found that older adults have

an increased quadriceps femoris EMG activity at more extended (160° and 170°) as well as at more flexed (80°) knee joint angles in comparison to younger adults. This was not the case at intermediate knee joint angles (110° and 140°).

Knee flexors have been reported to demonstrate similar decline as knee extensors due to the aging process<sup>[166]</sup>. Nevertheless, Ogawa *et al*<sup>[180]</sup> found no significant change in muscle volumes and average CSA for the hamstring muscles between young and old adults, whereas quadriceps muscle volume and average CSA were 20% and 16% lower, respectively. This resulted to greater age-related decline in the specific tension for the knee flexors compared to knee extensors (Table 1)<sup>[174,180]</sup>. In contrast to the knee extensors, for the knee flexors the strength reduction is mainly caused by deterioration of the biarticular muscles, and not of the monoarticular muscles<sup>[172]</sup>. Furthermore, for the knee flexors, the age-related reduction of joint moment is almost invariant to joint angle<sup>[172]</sup>, something that does not hold for the knee extensors, as already mentioned above.

Age-related muscle weakness is associated with the well described decline of skeletal muscle mass. Yet, more recent studies have shown that this relationship is less robust than once believed<sup>[167]</sup>. Goodpaster *et al*<sup>[175]</sup>, when measuring knee extensor strength by isokinetic dynamometry, found that although the loss of muscle mass is associated with the decline in strength of older adults, this strength decline is much more rapid than the concomitant loss of muscle mass. Moreover, they reported that maintaining or gaining muscle mass does not prevent aging-associated reduction in muscle strength. Furthermore, there are age-related alterations in torque production capability that are not explained by a reduction in muscle mass, including reduced specific tension and slower rate of isometric torque production (expressed relative to peak torque)<sup>[167]</sup>. The altered neuromuscular activation is another critical component of the weakness observed in senescence<sup>[167]</sup>.

Nevertheless, the studies focusing on the underlying neuromuscular mechanisms of age-related reduction in knee extensors force generation capacity are limited. Moreover, the reported results are partially conflicting, especially the ones concerning alterations in neural drive to the quadriceps muscle. While some studies find greater activation deficit in the elderly, compared to young adults<sup>[181,182]</sup>, other studies do not find any significant differences between young and old in the ability to activate the knee extensor muscles to a high degree (93%-96%)<sup>[183-186]</sup>. Harridge *et al.*<sup>[187]</sup> found that very old adults (85-97 years) demonstrated significant impairment in central activation, with mean knee extensor voluntary activation level of only 81% (range: 69%-93%)<sup>[187]</sup>. This outcome suggests that deficits in the neural drive essentially contribute to the weakness of the knee extensor muscles observed in very old age<sup>[188]</sup>. On the contrary, Miller *et al.*<sup>[189]</sup> found that the ability to activate the quadriceps muscle was generally very high, and there was no significant difference between older (96%) and younger (98%) subjects. The study was conducted on 20 moderately active older subjects (mean age 75 years) and 12 younger (mean age 25 years). The above described inconsistency in reported findings may be primarily related to methodological limitations and differences in the techniques used to estimate muscles voluntary activation<sup>[181]</sup>, as well as to different physical condition of participants<sup>[188]</sup>. Mau-Moeller *et al.*<sup>[181]</sup> estimated the neural drive to the knee extensor muscles during maximal isometric contractions by means of both interpolated twitch technique and the root mean square of the EMG signal normalized to maximal M wave<sup>[181]</sup>. Both techniques led to the same outcome, *i.e.*, there was an age-related decline in the neural drive to the muscle which resulted in muscle weakness. Regarding the knee flexor muscles, to our knowledge there is no study investigating their voluntary activation.

Another neuromuscular mechanism of age-related reduction in knee extensors force generation capacity, regards the age-related changes in antagonistic muscle coactivation. The mechanical opposition to the agonist action can contribute to the reduced exerted moment at the knee joint. Studies investigating the effect of aging on the coactivation during knee extension are limited and their findings lack of consensus. Laudani *et al.*<sup>[173]</sup> found that old (mean, 70 years) and young (mean, 28 years) adults with similar physical activity level do not demonstrate significant difference in the coactivation during maximum isometric contractions ( $26.2\% \pm 22.8\%$  *vs*  $29.6\% \pm 20.5\%$ ). The increased standard deviation in their measured values indicates high intra-group variability, assigning to coactivation a rather person-dependent instead of age-related nature. Regarding dynamic contractions, no association was found between normalized antagonist activation and velocity, indicating that changes in coactivation cannot be responsible for age-related deficit in force production<sup>[190]</sup>. On the contrary, Tracy *et al.*<sup>[191]</sup> found that old subjects (mean, 71.5 years) exhibited dur-

ing submaximal isometric and anisometric contractions, greater coactivation of antagonist muscle compared to young ones (mean, 22 years). Similar findings have been reported for measurements over women during isometric knee extension contraction<sup>[174]</sup>. Furthermore, there is a highly determinant effect of coactivation on the capacity to produce isometric force on a short period of time<sup>[192]</sup>. However, significantly higher antagonistic coactivation was only found during contraction of the knee extensors and not during knee flexion<sup>[174]</sup>. During knee flexion, the co-contraction of knee extensors was found to be significantly lower for both old and young adults<sup>[173]</sup>.

The transfer of force between the muscular and skeletal systems may be affected by age-related changes in muscle architecture, as well as in the length and compliance of tendons<sup>[167]</sup>. An age-related reduction in vastus lateralis tendon and aponeurosis stiffness has been reported<sup>[168-170]</sup> (Figure 3). Thus, the greater compliance of the aged tendon and aponeurosis can influence the force-length and force-velocity relationship of the muscle (contractile element) and consequently its force generating potential<sup>[193]</sup>. The result is a more deteriorate function of the knee extensor muscles in the older population.

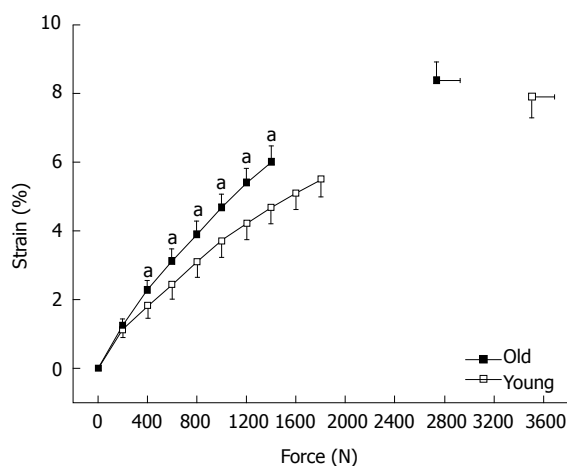
The above mentioned age-related alterations in neuromuscular interactions around the knee joint lead to differences in the way old adults perform activities of daily living. For example, when older adults descend and ascend stairs and ramps, they demonstrate an altered control strategy compare to young adults, causing a redistribution of the mechanical load at the tibiofemoral joint<sup>[194]</sup>. This has effects on the initiation and progression of knee osteoarthritis in the elderly, which in turn makes movement even more difficult<sup>[194]</sup>.

## CONCLUSION

In this review, we attempted to provide a global view of the neuromuscular mechanisms associated with knee joint injuries across lifespan. It is certain that neuromuscular strategies and mechanisms differ between children, adults and the elderly. However, there are some interesting similarities in the mechanisms by which children or elderly differ compared with adults.

Both children and elderly display a lower absolute muscle strength capacity than adults. This deficit may be due to a lower muscle mass (especially of the quadriceps) displayed by children and elderly, obviously for different reasons. The effects of a lower muscle mass are more evident in older individuals. However, when variations in muscle mass are taken into consideration, there are still differences between different age categories.

Quadriceps activation failure is a common symptom of all knee injuries, irrespective of age. However, for those individuals who have a lower quadriceps strength capacity, it is reasonable to suggest that functional impairment will also be higher. If we assume that knee injury conditions (swelling or pain and inflammation) are constant amongst different age groups, an initial differ-



**Figure 3** Strain-force curves of the vastus lateralis tendon and aponeurosis. The strain values at every 200 N and at maximum calculated tendon force during maximal voluntary isometric knee flexion contraction are displayed. The curves end at 1400 N for the old adults and at 1800 for the young ones, these values correspond to the maximum common force achieved by all subjects in either group, old and young adults. Y: Young ( $n = 12$ ); O: Old adults ( $n = 14$ ); Means and SEM; Age effect: ( $^aP < 0.05$ ) vs young.

ence in the ability to recruit the entire motor unit pool of the muscle would also contribute to a higher impairment after injury. Our review indicates that this is the case for both children (probably due to maturation) and elderly (due to age effects on neuromuscular system).

Another factor which might have affected the impaired ability to produce maximum muscle strength is a higher antagonist co-activation. Although co-activation levels may contribute to a high joint stability and stiffness, it appears that co-activation levels do not differ between children and adults or between elderly and adults, at least during isolated (static or dynamic) joint strength testing conditions. This indicates that it is the reduced muscle mass and central activation of the agonist muscles rather than higher co-activation by the antagonists that contributes to age related differences in absolute strength. It follows, that this particular neuromuscular mechanism, central or peripheral, is not age specific.

While extensive research has examined the strength balance around the knee through the H:Q ratio, there is a marked difference in the amount of research performed in adults compared to that performed in children and the elderly. Nevertheless, it appears that H:Q ratio levels are altered after knee injury mainly as a result of a lower quadriceps muscle strength. Current evidence does not indicate whether H:Q ratio differs between different age groups. Sparse data indicate that hamstring muscle strength tends to be relatively less affected by age compared with quadriceps muscle strength, but this is only a speculation.

It appears that stiffness of the muscle-tendon units around the knee differs between age groups. Interestingly, there is a common pattern regarding age variations in muscle-tendon stiffness: both children and the elderly display less stiffness of the quadriceps MTU than adults.

While in children this may be due to sexual maturation and in elderly due to deterioration of tissue, it could be suggested that the main characteristic is similar: both children and elderly show a more compliant muscle-tendon unit. It seems that tendons adaptations follow muscle's force capacity. Muscle force determines the strain of tendon cells, *i.e.*, the higher the force applied to tendon the higher its deformation. There is evidence that strain of tendon cells is an important regulator for the homeostasis of connective tissues. The resulted more compliant tendon in children and elderly affects both the force-length and force-velocity relationship of their muscles and, in turn, leads to an altered strength capacity.

Finally, an interesting question is whether age-related differences in neuromuscular strategies around the knee depend on gender. There have been no studies that specifically addressed such a question. Nevertheless, current evidence indicates that females display a higher injury rate than males. Such variation is observed from an early age where, there is evidence that muscle strength and co-activation profiles may place girls to a greater injury risk than boys. Similar results are also reported for older individuals, where additional factors, such as body mass, also contribute to gender variations.

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