

A new oral formulation for the release of sodium butyrate in the ileo-cecal region and colon

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Abstract

AIM: To develop a new formulation with hydroxy propyl methyl cellulose and Shellac coating for extended and selective delivery of butyrate in the ileo-caecal region and colon.

METHODS: One-gram sodium butyrate coated tablets containing 13C-butyrate were orally administered to 12 healthy subjects and 12 Crohn's disease patients and the rate of 13 C-butyrate absorption was evaluated by 13 CO₂ breath test analysis for eight hours. Tauroursodeoxycholic acid (500 mg) was co-administered as a biomarker of oro-ileal transit time to determine also the site of release and absorption of butyrate by the time of its serum maximum concentration.

RESULTS: The coated formulation delayed the ¹³C-butyrate release by 2-3 h with respect to the uncoated tablets. Sodium butyrate was delivered in the intestine of all subjects and a more variable transit time was found in Crohn's disease patients than in healthy subjects. The variability of the peak 13 CO₂ in the kinetic release of butyrate was explained by the inter-subject variability in transit time. However, the coating chosen ensured an efficient release of the active compound even in patients with a short transit time.

CONCLUSION: Simultaneous evaluation of breath ¹³CO₂ and tauroursodeoxycholic acid concentrationtime curves has shown that the new oral formulation consistently releases sodium butyrate in the ileo-cecal region and colon both in healthy subjects and Crohn's disease patients with variable intestinal transit time. This formulation may be of therapeutic value in inflammatory bowel disease patients due to the appropriate release of the active compound.

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Key words: Sodium butyrate; Inflammatory bowel diseases; Ulcerative colitis; Crohn's disease; Controlled release formulation; Pharmacokinetics; Stable isotope; Breath test

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INTRODUCTION

Butyric acid, a short chain fatty acid, is the main colonic bacterial product of non-starch polysaccharides^[1]. Impaired butyric acid metabolism (usually as butyrate species) has been implicated in the development of ulcerative colitis ${(\rm{UC})}^{[2]}$ but there are conflicting data regarding its role in the pathogenesis of $UC^{[3-11]}$. Large bowel mucosa biopsy specimens from quiescent UC patients have also shown reduced oxidation of butyrate but not of glucose and glutamine, the two other major fuel sources for colonic epithelium[3]. *In vitro* studies conducted in terminal ileal mucosa biopsy specimens from UC patients support this concept^[4]. A study on colonic sodium butyrate (NaB) metabolism using 14 C-butyrate rectal instillation and 14 CO₂breath test in patients affected by extensive UC showed a reduction in NaB oxidation, which returned to normal on remission^[10]. The authors concluded that while impaired NaB metabolism is unlikely to be a primary cause of UC, impairment of short chain fatty acid metabolism by coloncytes may be a pathogenic factor. Another study indicated that in quiescent UC patients, the rate of NaB metabolism is not impaired $[11]$.

It has recently been demonstrated that NaB exhibits anti-inflammatory properties as documented by a strong inhibition of interleukin (IL)-12 production by suppressing both IL-12p35 and IL-12p40 mRNA accumulation, and enhances IL-10 secretion in Staphylococcus aureus cellstimulated human monocytes $^{[12]}$. Investigation of the effects of NaB on some G1 phase-related proteins in a colon carcinoma cell line (HT29) has revealed another potential pharmacological property, since NaB is able to reduce cyclin D1 and p53 level in a dose-dependent

fashion and to suppress cell growth^[13]. Thus, the lack of NaB in diets poor in carbohydrates could lead to clinically relevant functional alterations. In vivo, the growth inhibitory effects of NaB on colon cancer cells appear to be somewhat less marked^[14,15].

Some clinical applications of NaB treatment have already been successfully evaluated. NaB enemas seem to provide an effective treatment for acute radiation proctitis, α ccelerating the healing process^[16,17]. Oral co-administration of NaB and mesalazine in patients with active UC seems to improve the efficacy of mesalazine monotherapy^[18,19].

These considerations prompted us to develop a new oral formulation in which NaB is released in the terminal ileum and colon, the target of its potential pharmacological activity^[19].

The main problem in the development of controlled release formulation is to extrapolate *in vitro* release data to those achieved during *in vivo* studies. This is particularly crucial for drugs used in patients with gastrointestinal diseases in which the intestinal transit time shows a high variability.

The colonic target release of enteric coated butyrate requires an optimized coating able to prevent an early release (duodenum-jejunum-ileum) resulting in an absorption and metabolism of butyrate before reaching the colon. The coating is expected to release NaB from the ileo-caecal region as a result of a variation of intestinal pH but a delayed release delivery kinetic would result in a loss of a relatively high amount of butyrate in the stools.

Tuleu *et al*^{20]} have developed pellets for colonic delivery of NaB *via* oral route. When they are administered to rats a large amount is lost in the caecum for coating dissolution problems.

Optimization of the tablets is therefore crucial to determine in the healthy subjects and patients with Inflammatory bowel disease (IBD) the exact delivery site of butyrate in the intestine thus reducing false negative data in term of efficacy due to a poor delivery of the active compound in the target area.

Sodium butyrate tablets (1 g) coated with hydroxyl propyl methylcellulose (HPMC) and natural polymer Shellac have been developed and optimized by conventional *in vitro* studies. In the present study the optimal coating thickness was optimized *in vivo* by evaluating the release of the active ingredient by the kinetics of ${}^{13}CO_2$ excretion in the breath of healthy subjects and Crohn's disease patients after oral administration of ¹³C-labeled NaB included in the 1 g tablets. The rate of $^{13}CO₂$ production is the result of ¹³C-NaB intestinal absorption and metabolism that was evaluated by the rate of production of ${}^{13}CO_2$ in exhaled breath over 8 h. The ${}^{13}C/{}^{12}C$ isotope ratio was measured by isotope ratio mass spectrometry (IRMS). The intestinal transit time was evaluated by simultaneous coadministration of tauroursodeoxycholic acid (TUDCA).

TUDCA was selected as a biomarker of oro-ileal transit time since it is absorbed actively only in the ileum, the time of its peak serum level reflects the oro-ileal transit time. A sensitive and specific enzyme immunoassay was performed to evaluate serum TUDCA concentration at various time intervals after administration as previously described $[21]$.

To evaluate the kinetics of the release of NaB from

the tablets, we compared the time of maximum ${}^{13}CO_2$ excretion with that of peak serum TUDCA concentration within individual subjects in order to overcome the high variability in intestinal transit time.

MATERIALS AND METHODS

Oral NaB formulation

Plain and coated tablets containing hydroxyl propyl methylcellulose and shellac with a pH dependent extended release coating were used in the study. Both formulations contained 1 g of NaB and three batches of tablets containg 5% , 10% and 20% w/w of 13 C-NaB (CIL, Andover MA, USA) were prepared.

The difference between the two tablets was the internal pre-coating of HPMC and external coating of shellac, which is resistant to desgregation up to pH 7. All other excipients of the formulations were identical. The pre-coating of HPMC was made to avoid that basic characteristics of the active ingredient in the tablet nucleus would induce an early dissolution of shellac which is resistant to acid pH and soluble to basic pH. In order to optimize the release of NaB in the colon, different thickness films of shellac (50, 80 and 120 μm) were studied. Coated tablets (Sobutir) were supplied by Promefarm srl, Milan, Italy. The different formulations were then administered to the same subjects in order to verify simultaneously the kinetic of NaB release in relation to the oro-ileal transit time evaluated by the time of the serum TUDCA peak and select the formulation that would be admitted to the complete study.

Subjects studied

The study was carried out in 12 healthy subjects (6 males and 6 females, median age 42 years, range 18-60 years) and 12 Crohn's disease patients (9 females and 4 males, median age 40 years, range 18-65 years) with a relatively mild activity index ranging from 320 \geq C.D.A.I. \geq 220^[22]. To avoid any difference in the transit time, we studied only patients with the same level of activity index. In addition, the patients studied had no pure ileal or ileocolonic involvement and they did not receive steroid or immunosuppressive treatment. All patients during the study presented diarrhoea. Before this final controlled study volunteers received the different formulations under development and between the different studies a washout period of one week was used. Thirty minutes before the study, 2 mL of blood was collected for the baseline values, as were two separate samples of breath in a 10 mL capped glass tube. After administration of the 1 g^{13} C-NaB tablet and of 500 mg TUDCA as gelatine capsules (Tudcabil®, Pharmacia Upjohn, Milan, Italy), the subjects received a standard liquid test meal of 375 Kcal, containing 17 g of fat, 10.4 g of protein and 10 g of carbohydrates. Breath and blood samples were collected at 30 min intervals over an 8-h period (unless otherwise specified). The oroileal transit time was defined as the time interval between administration of TUDCA and the peak serum TUDCA (C_{max}) time^[21]. The time of the maximum ¹³CO₂ breath excretion was used to represent the time of release and absorption of sodium butyrate. The study approved by

Figure 1 Excretion of breath ¹³CO₂ after oral administration of uncoated (**A**) and shellac-coated (**B**) 1 g NaB tablets containing 10% w/w of ¹³C-NaB in 12 healthy subjects. The experiment of each formulation was repeated three times in the same subject for different weeks.

the Ethical Committee of University of Bologna was conducted according to the institutional guidelines.

Analytical methods

 13 CO₂ breath test: 13 CO₂ in each of the duplicate breath samples was analyzed by continuous flow isotope ratio mass spectrometry (IRMS; ANCA, PDZ Europa Ltd, Cheshire U.K.). The results were expressed as δ^{13} C that was calculated from:

$$
\delta^{13}C = \left(\frac{^{13}C/^{12}C \text{ (sample)}}{^{13}C/^{12}C \text{ (std)}} - 1\right) \times 1000
$$

where ${}^{13}C/{}^{12}C$ (std) is the Pee Dee Belemnite (PDB) reference standard $^{13}C/^{12}C$ ratio, the final value was expressed as a milli percentage ($\delta^{^{13}\rm{C}\%}$).

Serum TUDCA enzyme immunoassay

Serum TUDCA levels were determined by a specific chemiluminescent enzyme immunoassay previously developed and optimized in our laboratory^[21]. The method is a solid-phase competitive format with a TUDCAspecific polyclonal antibody immobilized on 96 wells black polystyrene microtiter plates. A horseradish peroxidase (HRP)-UDCA conjugate was synthesized, purified, properly characterized, and used as enzymatic tracer.

For the TUDCA assay 100 μL of the sample (serum diluted $1/50$, v/v with assay buffer: 0.05 mol/L phosphate/EDTA buffer, pH 7.4, containing 1 g/L bovine serum albumin) or of six standard TUDCA solutions with a concentration ranging from 0.01 to 1000 nmol/L was incubated in the 96-well microtiter plates coated with the antibody for 1 h at 37℃ with 100 μL of the properly diluted HRP-UDCA tracer. After washed with assay buffer, 100 μL of the chemiluminescent substrate (H_2O_2) luminol/enhancer SuperSignal ELISA Pico, Pierce, Ⅱ, USA) was added and the light signal was measured using a PMT based luminometer microtiter reader (Luminoskan Ascent, Thermo Electron Corporation MA, USA) .

TUDCA concentrations were determined by a plot of chemiluminescent (CL) signal *vs* the log of concentration and the best data fit was obtained by linear regression of the six point standards. Serum TUDCA was expressed as nmol/L of serum.

RESULTS

Optimization of NaB oral formulation

The 13 C-NaB dose to include in the 1 g NaB tablet was standardized by quantifying the amount of label to produce a breath $CO₂$ enrichment of the 13 C-isotope that could be accurately evaluated with respect to the baseline value representing its natural abundance.

During the course of three separate weeks, three 1-g NaB tablets containing 5%, 10% and 20% w/w of 13 C-NaB respectively, were administered to six healthy subjects. The excretion rate of ${}^{13}CO_2$ in breath was measured and the maximum value was calculated. The dose of 100 mg of the label was chosen giving a $\delta^{13}C\%$ of 15.3 that was much higher than the baseline value of -28%. This wide cut off could allow the accurate evaluation of not only the maximum excretion of ${}^{13}CO_2$ but also small variations during the 8-h study period and eventually low ${}^{13}CO_2$ excretion resulting in patients with impaired metabolism of NaB. The coating thickness was optimized according to the kinetics of the ${}^{13}CO_2$ excretion accounting for the release and absorption of butyrate from the tablet. The results obtained with 50, 80 and 120 μm thickness coating suggested that the coating size of 80 μm was the most adequate to prevent a too early release and absorption of NaB as occurred with the 50 μm thickness and to ensure complete release of the active ingredient in a time comparable with the oro-ileal transit time.

The NaB tablet containing 10% w/w of 13 C-NaB and 80 μm-thick coating was used to evaluate the final performance of the formulation. The intra-subject variability was evaluated by administering either coated or uncoated NaB formulations three times to the same subject in separate experiments and monitoring the excretion of ${}^{13}CO_2$ at 15 min time intervals (Figure 1). In the uncoated tablet, the intra-subject variability was very low and the curves were almost super impossible.

Figure 2 Profiles of the mean ¹³CO₂ breath excretion (A) and serum TUDCA concentrations (a) plotted against time. Data were collected after administration of the Shellaccoated tablet containing 10% w/w of ¹³C-butyrate and two gelatine capsules containing 250 mg each of TUDCA. Data are expressed as mean ± SD in 12 healthy subjects (A) and 12 Crohn's disease patients (**B**).

Figure 3 Tmax obtained in control subjects (**A**) and Crohn's disease patients (**B**) using serum TUDCA and 13CO2 breath tests.

The maximum excretion was achieved 45 min after administration of the dose and the absorption started just in the first 15 min. A slightly higher variability was observed when the coated formulation was administered as a result of an intra-subject variability in gastric emptying and overall gastrointestinal transit. The mean peak ${}^{13}CO_2$ excretion time of the coated tablets was 180 min (range 150-225 min), showing the extended release of NaB caused by the shellac coating.

Serum TUDCA chemiluminescent enzyme immunoassay

Chemiluminescent enzyme immunoassay fulfilling all the standard requirements of accuracy and precision was used. The intra and inter studies showed that the coefficient of variation was always below 9%. The limit of quantification of 10 nmol/L allowed direct analysis of TUDCA in a 20-fold diluted serum sample.

The mean serum TUDCA profiles together with the kinetics of ${}^{13}CO_2$ excretion obtained in the healthy subjects and Crohn's disease patients are shown in Figure 2. The serum TUDCA profile was characterized by two peaks. The first peak was reached 180-200 min after TUDCA administration and represented the oro-ileal transit time, the second peak was observed after 300-400 min as a result of the enterohepatic circulation of the absorbed TUDCA.

In the healthy subjects peak of serum TUDCA concentration was achieved at a median of 4 h (range 3-5 h) after NaB administration. The mean peak ${}^{13}CO_2$ excretion time occurred slightly earlier at 3.5 h and the range of variability was similar to that of TUDCA. A similar behavior was observed in Crohn's disease patients with a higher variability due to variation in the intestinal transit time.

Top panel and bottom panel are shown in Figure 3. The Tmax was obtained in control subjects and Crohn's disease patients using the serum TUDCA and ${}^{13}CO_2$ breath tests. No subject and Crohn's disease patient had an earlier release of ${}^{13}CO₂$ after administration of the coated tablets with respect to the Tmax of TUDCA. Similarly no subject and patient missed to give a peak of ${}^{13}CO_2$ excretion or reported the loss of intact tablets in stools.

The ileal release was defined (a priori) as the ${}^{13}CO₂$ peak occurring within 30 min from the time of TUDCA peak whereas colonic release was considered as the ${}^{13}CO_2$ peak occurring after this interval.

The temporal correspondence between the maximum ${}^{13}CO_2$ excretion times, with the TUDCA time at the Cmax representing the biomarker oro-ileal transit time even if occurring at different times, usually slightly earlier suggested that the active ingredient was still delivered in the colon in high concentration and therefore we expected that it would exert its activity in IBD patients.

In all the studied subjects, NaB was efficiently released by the coated tablet, suggesting that the formulation developed could be used in these subjects to prevent an early absorption and deliver a large amount of NaB in the colon just starting from the terminal ileum as shown by the kinetic profile of ¹³CO₂ and serum TUDCA.

DISCUSSION

The present study was designed to evaluate a new NaB formulation able to deliver the active ingredients of 1 g tablets coated with shellac into the colon by oral administration. The coating delayed the release of the active ingredients by two-three hours with respect to the uncoated formulation, thus a large amount of NaB could reach the colon, as demonstrated by the temporal similarity between the profiles of ${}^{13}CO_2$ breath test and serum TUDCA concentration. In fact, TUDCA is absorbed by an active carrier-mediated mechanism only in the ileum^[23, 24], and previous studies comparing the TUDCA serum levels after its oral administration with other markers of intestinal transit-time such as sulfasalazine showed that this method provides a valid and practical means of assessment of the oro-ileal transit-time $[21]$. Comparison of the peak times of ¹³CO₂ excretion and serum TUDCA concentration could confirm the efficacy of shellac coating in delivering NaB to the colon independently of intestinal transit-time variability. The dissolution of Shellac coating at pH 7 and its thickness driving the kinetics of the dissolution process has been well optimized and a large amount of NaB which starts to be delivered after two hours reaches the intact ileo-cecal region as shown by the kinetics of TUDCA intestinal absorption.

It was recently reported that topical butyrate improves the efficacy of 5-ASA in refractory distal ulcerative colitis[17], due to the presence of NaB in the colon administered topically *in situ*. Vernia et al^[16] demonstrated in a pilot study that oral butyrate may improve the efficacy of oral mesalazine in active ulcerative colitis but a large scale investigation to confirm the present findings is still required. In this case the NaB was administered as tablets coated with a pH-dependent soluble polymer. More recently it has been reported that chronic feeding (tablets, 4 g a day for 8 wk) of this enteric coated NaB formulation (tablets, 4 g a day for 8 wk) (tablets, 4 g a day for 8 wk) can effectively induce clinical improvement/remission in mild Crohn's disease^[25].

An adequate enteric coating is needed for therapy of ileo-colonic disorders since when uncoated uncoated oral formulation of NaB is administered in an uncoated oral formulation, the compound is promptly dissolved and rapidly metabolized before reaching the colon as shown by the time of the maximum ${}^{13}CO_2$ excretion occurring within 30-45 min after the 13 C butyrate oral administration. A specific enteric coated formulation has been therefore designed to deliver the drug in that portion of the intestine keeping into account the high variability of the intestinal transit time observed in IBD patients.

The amount of ${}^{13}CO₂$ excreted in breath was similar among the Crohn's disease patients, showing that the rate and efficiency of NaB metabolism are similar in the healthy subjects. The patients were characterized by a mild active disease accounting for the efficient metabolism of butyrate and the oral formulation was expected to deliver NaB into the colon in a similar extent as to enema administration.

Furthermore the new coated ¹³C-NaB oral formulation containing 13C-labeled butyrate can also be used to evaluate the rate of colocyte-metabolized NaB by performing ${}^{12}CO₂$ breath test before and after chronic administration of NaB. The impairment of NaB utilization by colonocytes that has been observed in previous studies^[2-4] can then readily be evaluated by measuring the reduction in cumulative ${}^{13}CO_2$ excretion in the 8-h period following oral administration of colon-targeted NaB tablets. A similar approach could also be used to evaluate the effectiveness of therapies for IBD patients with mesalazine (either alone or in combination with NaB) and new formulations designed to improve NaB absorption and metabolism. The reported NaB formulation can effectively improve oral administration of NaB ensuring the release of the active compound in the lower intestine portion which is the target for its pharmacological activity.

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