Research Article

An Electrically Tight *In Vitro* Blood–Brain Barrier Model Displays Net Brain-to-Blood Efflux of Substrates for the ABC Transporters, P-gp, Bcrp and Mrp-1

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Abstract. Efflux transporters of the ATP-binding cassette superfamily including breast cancer resistance protein (Bcrp/Abcg2), P-glycoprotein (P-gp/Abcb1) and multidrug resistance-associated proteins (Mrp's/ Abcc's) are expressed in the blood-brain barrier (BBB). The aim of this study was to investigate if a bovine endothelial/rat astrocyte in vitro BBB co-culture model displayed polarized transport of known efflux transporter substrates. The co-culture model displayed low mannitol permeabilities of $0.95 \pm 0.1 \cdot 10^{-6}$ cm s⁻¹ and high transendothelial electrical resistances of $1,177\pm101 \ \Omega \cdot cm^2$. Bidirectional transport studies with ³Hdigoxin, ³H-estrone-3-sulphate and ³H-etoposide revealed polarized transport favouring the brain-to-blood direction for all substrates. Steady state efflux ratios of 2.5 ± 0.2 for digoxin, 4.4 ± 0.5 for estrone-3-sulphate and 2.4 ± 0.1 for etoposide were observed. These were reduced to 1.1 ± 0.08 , 1.4 ± 0.2 and 1.5 ± 0.1 , by addition of verapamil (digoxin), Ko143 (estrone-3-sulphate) or zosuguidar+reversan (etoposide), respectively, Brain-toblood permeability of all substrates was investigated in the presence of the efflux transporter inhibitors verapamil, Ko143, zosuquidar, reversan and MK 571 alone or in combinations. Digoxin was mainly transported via P-gp, estrone-3-sulphate via Bcrp and Mrp's and etoposide via P-gp and Mrp's. The expression of P-gp, Bcrp and Mrp-1 was confirmed using immunocytochemistry. The findings indicate that P-gp, Bcrp and at least one isoform of Mrp are functionally expressed in our bovine/rat co-culture model and that the model is suitable for investigations of small molecule transport.

KEY WORDS: blood–brain barrier; breast cancer resistance protein; multidrug resistance-associated protein; p-glycoprotein; polarized small molecule transport.

INTRODUCTION

The blood-brain barrier (BBB) regulates the exchange of molecules between the blood and the brain interstitial fluid. The BBB is impermeable to the majority of drugs and drug candidates, which poses a challenge for the pharmaceutical industry [1]. The brain capillary endothelial cells express complex tight junction networks, which, together with metabolising enzymes and drug transporters, constitute the BBB [2]. A number of transporters of the ATP-binding cassette family, including P-glycoprotein (P-gp/*Abcb1*), breast cancer resistance protein (Bcrp/*Abcg2*) and multidrug resistance-associated proteins (Mrp's/*Abcc*'s), are localized at the luminal membrane of the endothelial cells [3–10], where they restrict access to the central nervous system for a large number of drug compounds [11–14].

Cell culture models can be useful tools to estimate the BBB permeability of new drug candidates *in vitro*, if they

display barrier properties comparable to those of the native barrier. Bovine blood-brain barrier in vitro models have been studied for more than three decades, and changed culture protocols have gradually improved the models [15]. In primary endothelial monocultures, P-gp activity has previously been demonstrated using uptake and efflux studies in the presence and absence of inhibitors [16-18]. However, these studies did not demonstrate vectorial transport, as the endothelial cells were cultured on culture plates. Other studies have demonstrated expression and function of P-gp in the bovine brain endothelial cells [19-21], but vectorial transport studies have shown efflux ratios below 2 [19–23], which is the generally accepted threshold for concluding active efflux transporter involvement [24]. However, with the exception of the Cecchelli et al. [21], these cell culture models displayed transendothelial electrical resistance (TEER) values in the range of 100–300 $\Omega \cdot \text{cm}^2$ [20, 22, 23], which are relatively low compared to the estimated in vivo barrier TEER of 1,000–2,000 $\Omega \cdot cm^2$ [25, 26].

The apparently low functional expression of P-gp observed in these studies could be due to insufficient differentiation of the endothelial cells into a BBB-like phenotype, or alternatively, an active efflux could have been masked by high paracellular fluxes in the low-resistance monolayers [27–29]. Indeed, one study in a tighter rat triple

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co-culture model with TEER ranging from 350–600 $\Omega \cdot \text{cm}^2$ and fluorescein permeability of 1.8–4·10⁻⁶ cm·s⁻¹ resulted in an efflux ratio around 2.5 [30].

Recently, our group published a new culture protocol based on the model published by Gaillard *et al.* [31] to improve the tightness of a bovine endothelium/rat astrocyte BBB model [32, 33]. The co-cultured endothelial cells displayed high TEER values, low mannitol fluxes, and polarized transport of the small molecules, L-glutamate and L-aspartate favouring the abluminal-to-luminal direction [34].

The aim of the present study was to investigate if our bovine endothelial/rat astrocyte *in vitro* BBB co-culture model displayed polarized transport of known efflux transporter substrates. We investigated the tightness of the model during transport experiments, as well as the expression and function of P-gp, Bcrp and Mrp-1 in the model using radiolabelled efflux transporter substrates and immunocytochemistry. Overall, our findings indicate that the endothelial cells of the *in vitro* model functionally express efflux transporters including Bcrp, P-gp and Mrp-1, which mediates a net efflux of transporter substrates from the abluminal to the luminal compartment.

MATERIALS AND METHODS

Materials

The radioisotopes ³H-digoxin (specific activity 40.0 Ci·mmol⁻¹), ³H-estrone-3-sulphate (specific activity 54.4 Ci·mmol⁻¹) and ¹⁴C-D-mannitol (specific activity 58.5 mCi·mmol⁻¹) were purchased from Perkin Elmer (Hvidovre, Denmark). ³H-etoposide (specific activity 0.401 Ci·mmol⁻¹) was purchased from Moravek Biochemicals (Brea, California, USA). Primary antibodies, mouse α -MRP1 (ab24102), rabbit α -von Willebrand's factor (ab6994), rabbit α -GFAP (ab7260) and rat α -BCRP (ab24115) were from Abcam (Cambridge, United Kingdom), while rabbit α -ABCB1 (PAB11144) was from Abnova (Johngli, Taiwan). Propidium iodide, Alexa-488 conjugated phalloidin and secondary antibodies, goat antirabbit IgG and rabbit anti-rat IgG (both coupled to Alexa-488) were from Molecular Probes (Leiden, The Netherlands). All other chemicals and reagents were bought from Sigma-Aldrich (Rødovre, Denmark) unless otherwise stated.

Isolation and Culture of Primary Astrocytes

Astrocytes were isolated according to previously established protocols [35]. After 3 weeks of culture, the astrocytes were passaged, resuspended in DMSO–FBS (1:9) (approximately $2 \cdot 10^6$ cells per vial) and stored in liquid nitrogen. In the third week of culture, the medium was collected. The astrocyte conditioned medium (ACM) was used later during endothelial cell culture.

Isolation of Endothelial Cells and Establishment of Endothelial/Astrocyte Co-cultures

The isolation of bovine brain endothelial cells and the coculture with astrocytes are described in detail elsewhere [33]. Briefly, brain capillaries were isolated from freshly slaughtered calves below 12 months of age obtained from a slaughterhouse directly after slaughtering (Herlufmagle, Denmark). The grev matter was isolated and homogenized in Dulbecco's Modified Eagles Medium-AQ (DMEM) using a Dounce Tissue Grinder of 40 ml (Wheaton Science Products, Millville, USA). Capillaries were isolated by filtration through 160-µm mesh filters (Millipore, Copenhagen, Denmark) and digested for 1 h in DMEM supplemented with 10% foetal bovine serum, 10 ml·L⁻¹ non-essential amino acids (×100) and 100 $U \cdot ml^{-1}$ -100 $\mu g \cdot ml^{-1}$ penicillin-streptomycin solution (DMEM-Comp)+enzymes, DNAse I (170 U·ml⁻¹),collagenase type III (200 U ml⁻¹) and trypsin TRL (90 U ml⁻¹) (Worthington Biochemical Corporation, Lakewood, USA). The digested suspension was filtered through 200-µm mesh filters (Merrem and La Porte, Zaltbommel, The Netherlands), and the capillary pellet was resuspended in foetal bovine serumdimethylsulfoxide (9:1) and stored in liquid nitrogen.

Frozen bovine brain capillaries were thawed and cultured for 4 days (37°C, 10% CO₂) in DMEM-Comp-ACM (1:1) supplemented with 125 μ g·ml⁻¹ heparin in collagen type IV/fibronectin (1 μ g·cm⁻² of each) coated T75 flasks. The endothelial cells were passaged and seeded at a density of 90,000 cells cm⁻² on collagen/fibronectin-coated Transwell polycarbonate filter inserts (area=1.12 cm², pore radius= 0.4 µm, Corning Life Sciences, New York, USA). Astrocytes for direct contact co-culture were prepared 2 days prior to passage of the endothelial cells by turning the filter inserts upside-down and applying cell suspension to the bottom of the inserts (120,000 cells \cdot cm⁻²). The astrocytes were allowed to adhere for 15 min before the inserts were put back in the culture trays. The co-cultures were cultured for three days in DMEM-Comp supplemented with 125 µg ml⁻¹ heparin followed by 3 days of culture in DM+TES consisting of DMEM without NaHCO₃ (Gibco, Breda, The Netherlands), supplemented with 8-(4-CPT)-cyclic adenosine monophosphate (312.5 µM), dexamethasone (0.5 µM), RO-20-1724 (17.5 µM) and N-[tris(hydroxymethyl)methyl]-2aminoethanesulfonic acid (TES) (50 mM).

TEER Measurements and Transport Studies

TEER was measured after equilibration to room temperature prior to all experiments, using an Endohm-12 cup electrode chamber (World Precision Instruments, Sarasota, Florida) connected to a Millicell-ERS device (Millipore, Massachusetts, USA).

Transcellular transport studies were performed directly in the culture medium after 6 days of co-culture. $1 \ \mu \text{Ci} \cdot \text{ml}^{-1}$ of the ³H-labelled substrate (either digoxin, estrone-3-sulphate or etoposide) was added to either the luminal or abluminal solution together with $1 \ \mu \text{Ci} \cdot \text{ml}^{-1}$ ¹⁴C-D-mannitol. Culture trays were placed on a temperature-controlled shaking table at 37°C, 90 rounds per minute. Aliquots (50 μ l from the luminal or 100 μ l from the abluminal compartment) were removed from the receiver wells after 30, 60, 90, 120 and 150 min and from the donor wells after 150 min (to confirm mass balance). Samples were replaced with pre-heated (37°C) DM+TES. Samples were transferred to Ultima Gold scintillation fluid (Perkin-Elmer), and radioactivity was counted in a Tri-Carb 2,100 TR Liquid Scintillation Analyzer (Packard Instrument Company, Meriden, USA).

Transport studies were performed in both the luminal-toabluminal (L-A) and abluminal-to-luminal (A-L) direction. Transporter functionality was evaluated by co-application of the inhibitors, verapamil (50 µM), Ko 143 (0.5 µM) (Toronto Research Chemicals, Toronto, Canada), reversan (5 µM), MK 571 (50 μ M), zozuguidar (0.5 μ M) and combinations of these. Inhibitors were added to both compartments as ×100 stock solutions 15 min prior to the addition of radiolabelled substrates. Tight junction integrity was assessed by measuring TEER through transport experiments performed without the addition of radiolabelled substrates. TEER was measured at 37°C prior to the experiment as a reference point and subsequently at the time points of sample withdrawal (also at 37°C). An alternative protocol, where the culture medium was changed to Hank's balanced saline solution with calcium/ magnesium (HBSS) containing HEPES (10 mM), 0.05% bovine serum albumin (BSA) and the differentiation factors, 8-(4-CPT)-cyclic adenosine monophosphate (312.5 µM), dexamethasone (0.5 μ M) and RO-20-1724 (17.5 μ M), (same as in the DM+TES culture medium) prior to initiation of the transport experiment was evaluated. The culture medium was replaced with pre-heated HBSS, and the cells were left to equilibrate on the temperature-controlled shaking table for 15 min (37°C, no stirring). Then, the simulated transport experiment was performed as above.

Immunocytochemistry

Cultured cells and freshly isolated capillaries were fixed and permeabilized with 4% paraformaldehyde+0.2% Triton X-100 for 15 min at room temperature and subsequently blocked for 30 min at room temperature in phosphate buffered saline (PBS) supplemented with 2% BSA and 0.1% Tween 20. Samples were stored in PBS+2% BSA and 0.1% Tween 20 or incubated with antibodies against von Willebrand's factor (1:400), glial fibrillary acidic protein (1:500), Bcrp (1:20), P-gp (ABCB1) (1:100) or Mrp1 (1:20) overnight at 4°C. The cells/capillaries incubated with primary antibodies were subsequently incubated 30 min at room temperature with 5 µg ml⁻¹ goat anti-mouse IgG (Mrp1), 5 µg ml⁻¹ goat anti-rabbit IgG (von Willebrands factor, P-gp, glial fibrillary acidic protein) or 5 µg ml⁻¹ rabbit anti-rat IgG (Bcrp), while the cells stored in PBS were incubated 30 min at room temperature with Alexa-488 conjugated phalloidin (1:200). The cells/capillaries were counterstained with propidium iodide (1.5 µM) for 5 min and mounted on coverslips. Cells were imaged using a Zeiss LSM 510 laser confocal microscope (Carl Zeiss, Jena, Germany).

Data Analysis

Measured TEER values were standardized against the surface area of the filter inserts to achieve corrected TEER values as $\Omega \cdot \text{cm}^2$. Standardized TEER values measured during transport experiments were plotted against time.

The measured molar amounts in the receiver samples were corrected for the dilution from replacing the receiver samples using Eq. 1:

$$Mass_{total} = V_{s} \times \left(\sum_{n=1}^{\infty} C_{n-1}\right) + C_{n} \times V_{t}$$
(1)

 $V_{\rm s}$ is the volume of the receiver samples, $V_{\rm t}$ is the total volume of the receiver solution and C_n is the concentration of the isotope in the receiver sample, *n*. The corrected amount transported was plotted as total amount transported per cm² per unit of time. Fluxes (J) were calculated from the steady state slopes of the straight lines (accumulated substrate per cm² as a function of time). Apparent permeability values were calculated using Eq. 2.

$$P_{\rm app} = \frac{J_{\rm ss}}{C_{\rm donor}} \tag{2}$$

 $P_{\rm app}$ is the apparent permeability, $J_{\rm ss}$ is the observed steady-state flux and $C_{\rm donor}$ is the concentration in the donor compartment after spiking. Efflux ratios were calculated as the apparent permeability in the A–L direction divided by the apparent permeability in the L–A direction. Obtained efflux ratios were compared using one-sided analysis of variance (ANOVA) followed by Bonferroni's test (α =0.05).

All curve fitting and statistical analyses were performed in Graph Pad Prism version 6 (GraphPad Software, La Jolla, CA, USA).

Data are reported as means \pm standard error of the mean (SEM). *n* denotes the number of times an experiment was performed as a whole. *N* denotes the number of filter inserts used for each condition within each single experiment.

RESULTS

Bovine Endothelial Cells Co-cultured with Rat Astrocytes Displayed Endothelial Cell Morphology and Expression of von Willebrand's Factor

Bovine brain endothelial cells, co-cultured with rat astrocytes on opposite sides of permeable polycarbonate supports, were characterized using immunocytochemical stainings of filamentous actin and the cell-specific markers for endothelial cells and astrocytes, von Willebrand's factor and glial fibrillary acidic protein, respectively (Fig. 1).

The endothelial cells were large, flat and irregular, with a cobblestone-like morphology as previously observed [33]. The cells were organized in a monolayer, and the filamentous actin was concentrated at the cell borders (Fig. 1a). Von Willebrand's factor was expressed in vesicles throughout the endothelial cells (Fig. 1b). There was no staining of glial fibrillary acidic protein in the endothelial cells, indicating that no astrocytes were present (Fig. 1c). Astrocytes displayed a non-organized layer with irregularly shaped cells (Fig. 1d). No staining of von Willebrand's factor expression was observed (Fig. 1e), whereas glial fibrillary acidic protein was expressed in all astrocytes, although growing cells on top of the astrocyte layer appeared to have the highest expression (Fig. 1f).

The Co-culture Model Displayed High Paracellular Tightness, Which Decreased Gradually During Transport Experiments

The paracellular tightness of the co-culture model was estimated using TEER measurements. On day 6 of coculture, the TEER (at room temperature) reached an overall

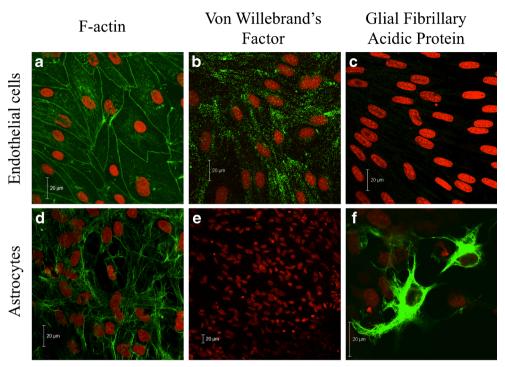


Fig. 1. Immunocytochemical characterization of *in vitro* blood-brain barrier models at day 6 of co-culture. *Upper row* Endothelial cells were stained with Alexa-488 phalloidin to visualize filamentous actin (**a**), with an antibody against von Willebrand's factor (**b**) or an antibody against glial fibrillary acidic protein (**c**) (*green*). Cell nuclei were counterstained with propidium iodide (*red*). *Lower row* Astrocytes stained with Alexa-488 phalloidin (**d**), an antibody against von Willebrand's factor (**e**) or an antibody against glial fibrillary acidic protein (**f**) (*green*). *Bars*=20 μ m

average of $1,177\pm101 \ \Omega \cdot \text{cm}^2$ (n=31, N=4-18). The TEER of individual batches varied from $327\pm30 \ \Omega \cdot \text{cm}^2$ (N=12) to $2,555\pm399 \ \Omega \cdot \text{cm}^2$ (N=18).

The change in tightness of the monolayers as a function of experimental time was examined in experiments where cocultures were placed on a shaking table at 37° C and stirred at 90 rounds per minute. The TEER was measured (at 37° C) at regular intervals, corresponding to the sampling times in a typical transport experiment (Fig. 2).

The resistance of co-cultures, incubated in culture medium, remained stable for the first 60 min after the onset of stirring, followed by a gradual decline from $1,081\pm31$ to $593\pm68 \ \Omega \cdot \text{cm}^2$ during the remaining 90 min (n=4). Change of medium from the DM+TES (containing 50 mM TES) to HBSS with 10 mM HEPES, 0.5% BSA and the same differentiation factors as in DM+TES (e.g. RO, cAMP and dexamethasone) caused an immediate drop in resistance to approximately 50% of the initial value followed by a decline during the first 60 min of stirring to approximately 10–20% of the starting level determined in culture media. All subsequent experiments were therefore performed using a protocol where the substrates were added directly to the culture medium.

The transendothelial flux of mannitol was estimated in all transport experiments in the study. The average steadystate mannitol permeability was $0.95 \pm 0.1 \cdot 10^{-6}$ cm·s⁻¹ (*n*=30, *N*=4–12). Steady-state flux of mannitol was maintained throughout the experiments (data not shown), indicating that the decrease in electrical resistance observed did not increase mannitol transport. The relationship between the apparent mannitol permeability and the TEER measured prior to the experiment showed a relationship much similar to an exponential decay function (Fig. 3).

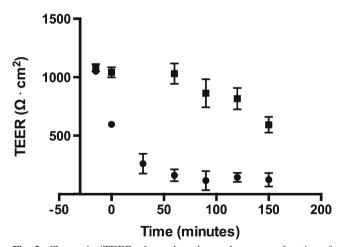


Fig. 2. Change in (TEER of co-cultured monolayers as a function of experimental time. TEER was measured at 37°C to avoid cooling of the cells prior to each measurement. The co-cultures were either incubated with their culture medium (*solid square*) or in HBSS with 10 mM HEPES and 0.5% BSA (*solid circle*). The first data point in both series corresponds to initial TEER-measurement in the culture media at 37°C. The medium was replaced with HBSS in one treatment group after the initial TEER measurement and both groups were incubated 15 min before the onset of stirring. The stirring was started at time zero. Data are averages±SEM (n=3-4, N=2-3)

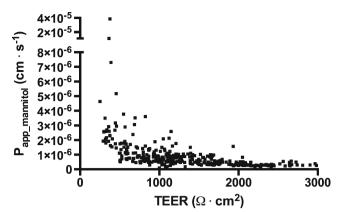


Fig. 3. Mannitol permeability as a function of TEER. Apparent mannitol permeabilities obtained from ¹⁴C–D-mannitol (20 μ M) flux experiments across single filter inserts plotted as a function of the transendothelial electrical resistance measured across the corresponding filter inserts at room temperature prior to the experiment

The relationship between mannitol permeability and electrical tightness of the cultures indicated that the largest differences in mannitol permeabilities were observed when TEER values were below 500 $\Omega \cdot \text{cm}^2$. Increases in TEER above this level only caused small reductions in permeability values (in the ranges between $0.3-1\cdot10^{-6} \text{ cm}\cdot\text{s}^{-1}$). This could explain why we observed a decrease in the transendothelial electrical resistance during the last part of the experimental time course (Fig. 2), but not a corresponding increase in mannitol fluxes. However, the variations in mannitol permeabilities were apparently reduced with increasing TEER levels resulting in very low variations when the TEER was above 2,000 $\Omega \cdot \text{cm}^2$.

The Efflux Transporter Substrates Digoxin, Estrone-3-Sulphate and Etoposide All Displayed Polarized Transport in the Brain-to-Blood Direction

Efflux transporter activity was examined in bidirectional flux studies. Luminal-to-abluminal (L - A) and abluminal-to-luminal (A - L) transendothelial fluxes of ³H-digoxin (P-gp substrate), ³H-estrone-3-sulphate (Bcrp and Mrp substrate) and ³H-etoposide (P-gp and Mrp substrate) were measured on day 6 of culture (Fig. 4) [36–39].

Transported amount of substrate as a function of time displayed a linear relationship from 30 to 150 min, indicating that the fluxes were in steady-state throughout the transport experiments.

Digoxin displayed steady state permeability values of $2.0\pm0.2\cdot10^{-6}$ cm·s⁻¹ (L–A) and $4.5\pm0.3\cdot10^{-6}$ cm·s⁻¹ (A–L), which were changed to $3.5\pm0.2\cdot10^{-6}$ cm·s⁻¹ (L–A) and $3.2\pm0.1\cdot10^{-6}$ cm·s⁻¹ (A–L) by co-application of verapamil (Fig. 4a). Estrone-3-sulphate displayed permeability values of $0.62\pm0.1\cdot10^{-6}$ cm·s⁻¹ (L–A) and $2.2\pm0.1\cdot10^{-6}$ cm·s⁻¹ (A–L), which were changed to $0.99\pm0.06\cdot10^{-6}$ cm·s⁻¹ (L–A) and $1.1\pm0.1\cdot10^{-6}$ cm·s⁻¹ (A–L) by co-application of Ko 143 (Fig. 4b). Etoposide displayed steady-state permeability values of $0.66\pm0.06\cdot10^{-6}$ cm·s⁻¹ (L–A) and $1.5\pm0.2\cdot10^{-6}$ cm·s⁻¹ (A–L), which were changed to $0.91\pm0.07\cdot10^{-6}$ cm·s⁻¹ (L–A) and $1.2\pm0.1\cdot10^{-6}$ cm·s⁻¹ (A–L) by co-application of zosuquidar and reversan (Fig. 4c). The corresponding efflux ratios are given in Fig. 5.

Digoxin had an efflux ratio of 2.5 ± 0.2 (*n*=11) indicating a net efflux via P-gp from the abluminal to the luminal compartment. Co-administration of 50 µM verapamil caused a significant reduction in the efflux ratio to 1.1 ± 0.08 (n=4) (P=0.0144). Estrone-3-sulphate displayed an efflux ratio of 4.4 ± 0.5 (n=7), indicative of a Bcrp-mediated efflux. The efflux was reduced to 1.4 ± 0.2 (n=3) by co-administration of 0.5 µM Ko 143 (P<0.0001). Etoposide displayed an efflux ratio of 2.4 \pm 0.1 (n=4), which was reduced to 1.5 \pm 0.1 (n=3) by co-administration of zosuguidar and reversan (P=0.018). For comparison, the efflux ratio of mannitol was 1.2 ± 0.1 (n=25). This was significantly lower than the values observed for digoxin (P < 0.0001), estrone-3-sulphate (P < 0.0001) and etoposide (P=0.048), whereas it was not significantly different from the efflux ratios in the presence of inhibitors (P=0.70 for digoxin+verapamil, P=0.73 for estrone-3-sulphate+Ko 143, P=0.43 for etoposide+zosuguidar+reversan). The transport studies thus indicated a net "brain-to-blood" (A-L) efflux of all substrates, which was inhibited by co-application of the respective inhibitors.

"Brain-to-blood" transport (A–L) of the three substrates was further examined in the presence of verapamil, Ko 143, zosuquidar, reversan, MK 571 and combinations of those, in order to better discriminate the involvement of the different efflux transporters in the transport process (Fig. 6).

All inhibitors, except Ko 143 and MK 571, significantly inhibited A-L transport of digoxin (P between 0.0019 and

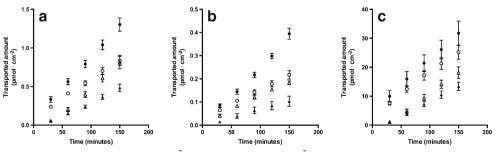


Fig. 4. Transendothelial transport of ³H-digoxin (0.03 μ M) (**a**), ³H-estrone-3-sulphate (**b**) (0.02 μ M) and ³H-etoposide (**c**) (2.64 μ M) across the co-culture model as a function of time, in the luminal-to-abluminal (*solid triangle*) and abluminal-to-luminal direction (*solid circle*) without or with inhibitors (luminal-to-abluminal, *open triangle*; abluminal-to-luminal, *open circle*), verapamil (50 μ M) (**a**), Ko 143 (0.5 μ M) (**b**) or zosuquidar+reversan (0.5 and 5 μ M, respectively) (**c**). Data are means±SEM (*n*=3–9, *N*=2–3)

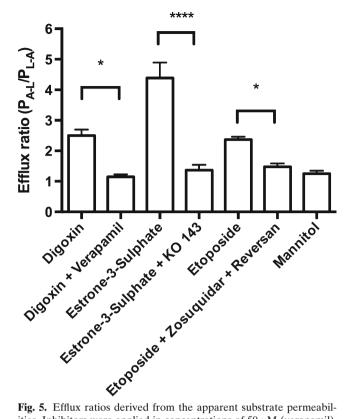


Fig. 5. Efflux ratios derived from the apparent substrate permeabilities. Inhibitors were applied in concentrations of 50 μ M (verapamil), 5 μ M (reversan) or 0.5 μ M (Ko 143 and zosuquidar). Data are means ±SEM (*n*=3–25, *N*=2–3).**P*<0.05, *****P*<0.0001

0.009) (Fig. 6a), with no differences between degrees of observed inhibition. This indicated that digoxin was mainly transported *via* P-gp. Estrone-3-sulphate transport was inhibited by all inhibitors (P<0.0001 except for zosuquidar, p=0.0031) (Fig. 6b). This indicated that P-gp, Bcrp and Mrp's were all involved in the transport process, however, to a different degree. Zosuquidar alone had a significantly lower inhibitory effect than all other conditions, indicating that P-gp played a minor role in the transport. The highest degrees of inhibition were observed when Bcrp and Mrp inhibitors were combined, *e.g.* verapamil+Ko 143 or reversan+Ko 143. Ko

143 alone inhibited to a similar degree as MK 571 and reversan alone, indicating similar contributions of Bcrp and Mrp's to the overall A–L transport of estrone-3-sulphate. Zosuquidar, reversan, MK 571 and reversan+zosuquidar all inhibited A–L transport of etoposide (P ranging from 0.0002– 0.0045), whereas the other conditions had no significant effects. This indicated that etoposide was mainly transported *via* P-gp and Mrp's, although it was surprising that verapamil did not inhibit the transport (P=0.19).

Taken together, the transport data demonstrate functionally active efflux transporters in the BBB model, with presence of P-gp, Bcrp and at least one isoform of Mrp.

Freshly Isolated Capillaries and Endothelial Cells in Co-culture Expressed P-gp, Bcrp and Mrp-1

The expression of P-gp, Bcrp and Mrp-1 was investigated in freshly isolated bovine brain capillaries and in endothelial cells from co-cultures using immunocytochemistry (Fig. 7).

All three transporters were expressed in brain capillaries (Fig. 7 a–c) as well as in endothelial cells, co-cultured for 6 days (Fig. 7d–i), as judged by immunocytochemical staining. Staining with an antibody against P-gp showed a diffuse expression throughout the cells (Fig. 7d). A similar expression pattern was observed for Mrp-1 (Fig. 7f), whereas Bcrp showed a partial up-concentration at the cell–cell contacts (Fig. 7e). The endothelial cells were further examined from the x,z dimension to determine if the transporters were localized in the luminal membrane (Fig. 7g–i). Low x,z resolution in combination with very thin endothelial cells makes it difficult to determine the exact localization. However, in comparison to the cell nuclei, P-gp expression was seemingly higher at the luminal membrane, whereas Bcrp and Mrp-1 seemed more diffuse.

DISCUSSION

Functional activity of efflux transporters is an important characteristic for *in vitro* BBB models. A recently published retrospective analysis of 32 Pfizer CNS drug candidates led to the conclusion that P-gp/Bcrp affinity was one of the most important factors determining the failure of the candidates [1]. In this study, we evaluated the electrical tightness and

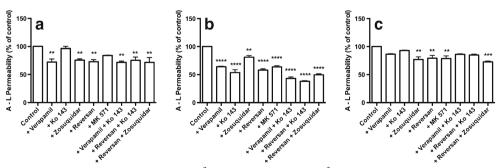


Fig. 6. Abluminal-to-luminal transport of ³H-digoxin (0.03 μ M) (**a**), ³H-estrone-3-sulphate (**b**) (0.02 μ M) and ³H-etoposide (**c**) (2.64 μ M) across the co-culture model in the presence of different inhibitors. Inhibitors were applied in concentrations of 50 μ M (verapamil and MK 571), 5 μ M (reversan) or 0.5 μ M (Ko 143 and zosuquidar). Data are standardized against the substrate permeability without inhibitors performed within the same experiment and shown as means±SEM (*n*=3–4, *N*=2–3). ***P*<0.01, ****P*<0.001

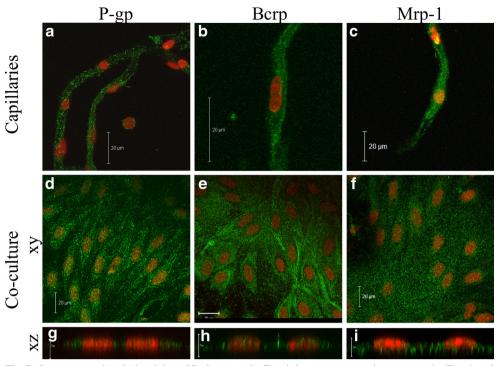


Fig. 7. Immunocytochemical staining of P-glycoprotein (P-gp), breast cancer resistance protein (Bcrp) and multidrug resistance-associated protein-1 (Mrp-1) in bovine brain endothelial cells: Freshly isolated bovine brain capillaries (**a**–**c**) and endothelial cells after 6 days of co-culture (**d**–**i**) were incubated with antibodies against P-glycoprotein (**a**, **d**, **g**), breast cancer resistance protein (**b**, **e**, **h**) or multidrug resistance-associated protein-1 (**c**, **f**, **i**) followed by incubation with species-specific secondary antibodies labelled with Alexa-488 (*green*). All samples were incubated with propidium iodide to visualize cell nuclei (*red*). *Bars*=20 µm (**a**–**f**) or 5 µm (**g**–**i**)

functional expression of P-gp, Bcrp, and Mrp's through determining efflux ratios of three known efflux transporter substrates, digoxin, estrone-3-sulphate and etoposide.

Efflux Transporter Activity in Bovine Blood-Brain Barrier Models

The apparent permeabilities for the three substrates were significantly higher in the A–L than in the L–A direction, which demonstrates that the model has functional efflux transporters and that it is suitable for examination of polarized BBB transport of small molecules. The efflux ratios were all above 2, a value, which has been established as a threshold value for demonstrating the presence of active efflux transporters [24]. The applied substrates and inhibitors were chosen to target P-gp, Bcrp and Mrp's. The ABC transporters have overlapping substrate and inhibitor profiles [40, 41], which makes it difficult to determine the exact contribution of an individual transporter to the efflux of a given substrate in our *in vitro* model. An overview of different studies applying the substrates and inhibitors is given below (Table I).

Digoxin has been widely used as a probe for determining P-gp activity [38]. Brain uptake of digoxin was approximately 35 times larger in P-gp knockout mice as compared to wildtype control mice, which indicated that P-gp is responsible for the low distribution of digoxin to the brain *in vivo* [57]. Digoxin is not a substrate for Bcrp [58], but other studies have indicated that the poor BBB permeability of digoxin is not explained by P-gp alone [11, 38]. Verapamil has been used as a P-gp inhibitor in concentrations from 5 to 150 μ M [23, 59-61], but it has also been shown to inhibit Mrp activity in concentrations of 5-10 µM [45, 62] as well as Bcrp activity, although not in the concentration range applied here [63, 64]. In our study, 50 µM verapamil lowered the efflux ratio of digoxin to 1.1, whereas the Bcrp inhibitor, Ko 143, had no effect on the digoxin transport indicating that the verapamil inhibition of A-L digoxin transport we observed was due to inhibition of P-gp or Mrp's. However, the general Mrpinhibitor MK571 did not inhibit the efflux of digoxin [39, 53, 65]. Zosuquidar, a more specific P-gp inhibitor [37, 51, 65] and reversan, a specific Mrp-1 and P-gp inhibitor [56] and combinations of those both inhibited digoxin transport to the same degree as verapamil. This indicated that the A-L efflux of digoxin was primarily mediated by P-gp in the bovine endothelial cell/rat astrocyte co-culture model.

Estrone-3-sulphate is a substrate for Bcrp [37, 43] and undergoes efflux across the BBB after intra-cerebral injection in rats [36]. Estrone-3-sulphate may be a substrate for other efflux transporters than Bcrp, although zosuquidar (LY335979) did not affect estrone-3-sulphate efflux in Caco-2 cells [37]. The Bcrp inhibitor, Ko 143, was applied to investigate Bcrp involvement in the observed estrone-3-sulphate efflux. Co-administration of 0.5 μ M Ko 143 inhibited the estrone-3-sulphate efflux. However, estrone-3sulphate transport was also affected by co-application of zosuquidar, verapamil, reversan and MK 571. The effect of the most specific P-gp inhibitor, zosuquidar, was low indicating little

Compound		Concentration used in this study (μM)	Reported $K_{\rm m}$, IC ₅₀ or K_i (μ M)	References
	Substrate of			
Digoxin	P-gp	0.03	P-gp: 170 $(K_{\rm m})$	[42]
Estrone-3-sulphate	Bcrp (Mrp-1)	0.02	Bcrp: 17 (K_m)	[43]
Etoposide	Mrp-1 (P-gp)	2.64	Mrp-1: 255 (K _m)	[44]
	Inhibitor of			
Verapamil	P-gp (Mrp-1, Bcrp)	50	P-gp: 10 (IC ₅₀) Mrp-1: 3-5 (IC ₅₀)	[45-49]
Zosuquidar	P-gp	0.5	P-gp: 0.024–0.07 (IC ₅₀)	[50, 51]
Ko 143	Bcrp	0.5	Bcrp: 0.01 (IC ₅₀)	[52]
MK571	Mrp-1/4	50	Mrp-1/4: 5/10 (IC ₅₀)	[53-55]
Reversan	Mrp-1(P-gp)	5	-	[56]

Table I. Overview of Applied Substrates and Inhibitors and Their Affinities for P-gp, Bcrp and Mrp's

P-gp involvement in the efflux. Verapamil, reversan and MK 571 inhibited the transport to a similar degree as Ko 143, whereas combinations of Bcrp and Mrp-1 inhibition (e.g. verapamil+Ko 143 and reversan+Ko 143) caused the highest degrees of inhibition. This indicated that both Mrp's and Bcrp are involved in the efflux of estrone-3-sulphate the *in vitro* model. Mrp-1 has previously been shown to transport estrone-3-sulphate, at least in the presence of glutathione [66], and Mrp-1, Mrp-4 and Mrp-5 have been shown at the mRNA transcript level in bovine primary endothelial cell cultures, as well as in the isolated bovine brain capillaries [9].

Etoposide is a known substrate for both P-gp and Mrp-1 [3, 39]. Etoposide displayed active efflux across the BBB model. Zosuquidar, reversan and MK 571 all inhibited the A-L transport of etoposide to some extent, indicating involvement of both Mrp's and P-gp in the efflux of etoposide. Correspondingly, the efflux was fully inhibited by a combination of zosuquidar and reversan. Ko 143 did not inhibit A-L transport confirming that it was a specific Bcrp inhibiter. Verapamil, a combination of Ko 143 and reversan and a combination of Ko 143 and verapamil did not inhibit etoposide A-L transport. This was somewhat surprising, as the applied concentration of verapamil should inhibit P-gp and Mrp's to the same extent as zosuquidar and MK 571/ reversan. However, both Mrp-1 and P-gp have multiple binding sites, which could explain distinct effects of the different compounds [39, 67].

The substrate/inhibitor studies indicated expression of both P-gp, Bcrp and at least one isoform of Mrp in the model. Immunocytochemical stainings further confirmed the presence of P-gp, Bcrp and Mrp-1 in the endothelial cells as well as in freshly isolated capillaries. P-gp and Bcrp expression have previously been shown in BBB models [6, 19, 20, 30], whereas Mrp expression is more controversial. Mrp-1 has been shown on the mRNA level in bovine brain capillaries [9] and in bovine and porcine brain endothelial cells [9, 68] and on the protein level in rat brain endothelial cells [30], but also Mrp-4 and -5 mRNA have been shown in bovine and porcine endothelial cells [9, 10, 68]. However, only Mrp-4 was found in a recent human proteomics study on brain capillaries [7]. It is not safe to conclude from these data alone, if our BBB model expresses Mrp-1 or some of the other isoforms. The specificity of the Mrp-1 antibody has not been confirmed against the other isoforms, and the inhibition observed with reversan in the functional studies was generally of the same degree as for zosuquidar. Estrone-3-sulphate transport was inhibited by reversan to a significantly higher degree than by zosuquidar, indicating Mrp-1 expression. However, further studies would have to be performed to clearly distinguish between the Mrp isoforms involved.

Polarized Transport of Efflux Transporter Substrates May Be Difficult to Detect in *In Vitro* Models with Low Paracellular Tightness

A range of bovine-based BBB models have been published through the last 30 years, for review see [15]. The general TEER levels in these models have ranged from approximately 100–800 $\Omega \cdot cm^2$, which is reasonably tight compared to other models. However, we previously demonstrated that TEER across a bovine endothelial/rat astrocyte co-culture BBB model was raised approximately two-fold by culture in highly buffered differentiation medium reaching values above 1,600 $\Omega \cdot cm^2$ [32]. Low TEER in cell culture models may cause lack of polarized transport because of a large paracellular flux contributing to the overall transport of the substrate [28]. A recent study by Hakkarainen et al. demonstrated P-gp expression in primary bovine endothelial cells with western blotting and immunofluorescence, as well as P-gp function as evaluated by the calcein-AM assay, but did not observe a net transendothelial P-gp-mediated efflux. The authors also reported low TEER values and high sucrose permeabilities, indicating that the paracellular flux component may have masked the transcellular efflux [20]. We found high TEER values in this study, although they decreased gradually during the transport experiments. This may have been caused by the continuous mechanical stress from stirring and repeated sampling during the experiments, but stirring is important to minimize effects of unstirred water layers within the receiver and donor chambers [28]. However, the fluxes of mannitol remained stable through the experiments in spite of this breakdown, but the partial breakdown may be the reason for our apparent TEER cut-off value of 500 $\Omega \cdot cm^2$, which is higher than previously reported [69]. A method to decrease the apparent decline in paracellular tightness could be to run the experiments directly in the incubator, as shown by Lemmen et al. who performed 20-h transport experiments across pig endothelial cells in the incubator with real-time TEER monitoring demonstrating polarized transport of Hoechst dye

and stable TEER values throughout the experiment [70, 71]. This method may not be applicable for short-term transport studies with shaking and frequent sampling, where a gradual decline in TEER can be anticipated. For studies like these, our high-resistance model has demonstrated its usefulness.

Conclusion

The findings in this study indicate that P-gp, Bcrp and at least one isoform of Mrp are expressed and functionally active in the bovine endothelial/rat astrocyte *in vitro* blood– brain barrier co-culture model. Moreover, the model forms high-resistance barriers with low paracellular fluxes of a small hydrophilic compound. The model is therefore a promising tool for investigating BBB permeability and affinity for BBB efflux transporters for small molecular compounds.

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Efflux Transporter Activity in a Tight BBB Model

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