



# Magnetoencephalographic alpha band connectivity reveals differential default mode network interactions during focused attention and open monitoring meditation

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According to several conceptualizations of meditation, the interplay between brain systems associated to self-related processing, attention and executive control is crucial for meditative states and related traits. We used magnetoencephalography (MEG) to investigate such interplay in a highly selected group of “virtuoso” meditators (Theravada Buddhist monks), with long-term training in the two main meditation styles: *focused attention* (FA) and *open monitoring* (OM) meditation. Specifically, we investigated the differences between FA meditation, OM meditation and resting state in the coupling between the posterior cingulate cortex, core node of the Default Mode Network (DMN) implicated in mind wandering and self-related processing, and the whole brain, with a recently developed phase coherence approach. Our findings showed a state dependent coupling of posterior cingulate cortex (PCC) to nodes of the DMN and of the executive control brain network in the alpha frequency band (8–12 Hz), related to different attentional and cognitive control processes in FA and OM meditation, consistently with the putative role of alpha band synchronization in the functional mechanisms for attention and consciousness. The coupling of PCC with left medial prefrontal cortex (lmpFC) and superior frontal gyrus characterized the contrast between the two meditation styles in a way that correlated with meditation expertise. These correlations may be related to a higher mindful observing ability and a reduced identification with ongoing mental activity in more expert meditators. Notably, different styles of meditation and different meditation expertise appeared to modulate the dynamic balance between fronto-parietal (FP) and DMN networks. Our results support the idea that the interplay between the DMN and the FP network in the alpha band is crucial for the transition from resting state to different meditative states.

**Keywords: meditation, mindfulness, magnetoencephalography, default mode network, resting state networks, brain rhythms**

## INTRODUCTION

Recently, the neural correlates of meditation states and traits have been increasingly studied in cognitive and affective neuroscience (Cahn and Polich, 2006; Lutz et al., 2008; Raffone and Srinivasan, 2010). Such growth of interest has been supported by several findings about the salutary effects of meditation on physical and mental health, as related in particular to mindfulness based programs (e.g., Chiesa and Serretti, 2010; Keng et al., 2011). Moreover, neuroimaging findings have clarified the role of brain structures and processes involved in meditation and mindfulness based training (e.g., Cahn and Polich, 2006; Chiesa and Serretti, 2010).

Several conceptualizations of meditation practice have underpinned a central role for attention and cognitive control skills

(Lutz et al., 2008; Malinowski, 2013a,b). These skills are crucial for the development and maintenance of mindfulness, the intentional and non-judgmental awareness of the fields of experience in the present moment, such as about perceptual, thought and feeling contents, that, in turn, leads to therapeutic outcomes and wellbeing effects (Kabat-Zinn, 1994; Wallace and Shapiro, 2006; Malinowski, 2013a). Meditation practices can be usefully classified into two main styles—*focused attention* (FA) and *open monitoring* (OM)—depending on how the attentional processes are directed (Cahn and Polich, 2006; Lutz et al., 2008). In the FA (“concentrative”) style, attention is focused on a given object in a sustained manner, and thus emphasizes sustained attention and attention regulatory skills. The second style, OM meditation, involves the monitoring of any content of ongoing

experience, and thus emphasizes mindfulness rather than FA and attentional control (Sumedho, 1994; Goldstein and Kornfield, 2001).

In this framework, the interplay between brain networks related to attention and control processes, and self-related processing appears fundamental for the understanding of meditation and mindfulness skills (Malinowski, 2013b). Indeed, mind-wandering and self-related processes occupy a large part of mental activity of human beings (Killingsworth and Gilbert, 2010): imagining future events, thinking about something different from what is currently being done, are mental states that frequently occur in everyday life (Killingsworth and Gilbert, 2010). It is not surprising, then, that mind-wandering parallels the brain's mode of operation that is associated with the recruitment of the so called Default Mode Network (DMN; Raichle et al., 2001). The DMN is one of the most robust among the Resting State Networks (RSNs), and entails the posterior cingulate cortex, the medial prefrontal cortex, the posterior lateral parietal/temporal cortices, and the parahippocampal gyrus (Raichle et al., 2001; Buckner et al., 2008; Watanabe et al., 2013). These areas have shown to be co-activated during passive mental states (e.g., task-unrelated cognition).

Another network that appears relevant for meditation and mindfulness skills is the Fronto-Parietal control network (FP). The FP network includes many regions identified as supporting cognitive control and decision-making, such as lateral prefrontal cortex, middle frontal gyrus, anterior insula/frontal operculum, anterior cingulate cortex, and anterior inferior parietal lobule (Vincent et al., 2008). The FP network also supports internally vs. externally focused goal-directed cognition by coupling with either the default or dorsal attention network (Christoff et al., 2009; Spreng et al., 2010; Spreng and Schacter, 2012). This functional interplay between the DMN and FP represents a model for goal-directed cognition that might significantly contribute to the understanding of the functional mechanisms underlying meditation.

Functional MRI (fMRI) studies have so far shown an enhancement of BOLD functional connectivity between the nodes of the DMN and executive control brain areas at rest and during meditation practice in selected meditator populations (Brewer et al., 2011). The recruitment of the DMN during meditation has been hypothesized to signal the involuntarily drift of attention away from the focus of meditation towards mind wandering (Hasenkamp et al., 2012; Tang et al., 2012). Nevertheless, more recent work has shown that activation of the DMN might serve for adaptive functions beyond rumination and mind wandering (Ottaviani et al., 2013). Moreover, evidence exists for a differential coupling of the DMN with other brain regions in different meditation styles (Xu et al., 2014), thus indicating a possibly more complex involvement of the DMN in meditation.

A long tradition of studies has investigated the functional role of brain rhythms by electroencephalography (EEG) or magnetoencephalography (MEG), and, in particular, the functional correlate of the alpha rhythm has been long debated. Oscillations in the alpha band (8–12 Hz) have been classically interpreted as

the functional correlate of drowsiness, being of larger amplitude during e.g., eye closed (Berger, 1929), supporting the idea of alpha power as related to an “idling” state. Later evidence pointed out that an increase of alpha power is associated to deactivation of task-irrelevant brain areas, whereas a power decrease in alpha is associated to their activation (Pfurtscheller, 2003). This idea was advanced into an alpha-inhibition hypothesis, which suggests that alpha synchronization may reflect top-down control processes (Klimesch, 1996, 1999; Klimesch et al., 2007). Opposite evidence exists for task-related increase in alpha power for high level cognitive processes such as those elicited by mental calculation, mental imagery, or internally driven attention (e.g., Hari et al., 1997; Cooper et al., 2003; Kounios and Beeman, 2009). Along the same line, recent evidence from alpha phase-synchronization/phase-coherence, which is hypothesized to represent a mechanism for short and long range communication in the brain (Lachaux et al., 1999; Varela et al., 2001; Fries, 2005; Palva et al., 2005; Engel et al., 2013), suggests a direct role for alpha band synchronization in the functional mechanisms of attention and consciousness (Palva and Palva, 2007; Knyazev, 2013). In this framework, it is not surprising that several studies have shown a link between DMN structures and power and phase synchronization in the alpha frequency range with concurrent EEG-fMRI (Laufs et al., 2003a,b; Mantini et al., 2007; Jann et al., 2009; Michels et al., 2010; Sadaghiani et al., 2010, 2012; Knyazev et al., 2011) and MEG (de Pasquale and Marzetti, 2014).

Brain rhythms, as measured by EEG and MEG, have also been studied to the specific aim of disclosing the impact of meditation practices. These studies, revealed a high heterogeneity of the frequency specific signatures of brain changes induced by meditation both in the same or in different traditions (Cahn and Polich, 2006; Ivanovski and Malhi, 2007; Nolfe, 2011). In this framework, evidence exists for the Individual Alpha Frequency (IAF; Klimesch, 1999) to be lowered as a consequence of intensive meditation training in Saggar et al. (2012). Due to IAF lowering, in those subjects, part of the standard alpha band was indeed pertaining to an individualized beta band, in which the authors found training induced power modulations. This finding might implicitly suggest that the heterogeneity reported in the literature might also be a consequence of the same nomenclature used for frequency bands that might potentially not fully overlap across different studies.

Furthermore, it should be noted that the great majority of EEG/MEG studies have investigated frequency specific connectivity changes at the level of electrodes/sensors and their results cannot be directly related to specific brain areas or brain networks due to volume conduction confounds (Schoffelen and Gross, 2009).

The recent development of methods to study ongoing functional connectivity at brain level with MEG, opens the way for reconciling the view on intrinsic activity as expressed by specific spatial brain modes, i.e., RSNs, and alpha band role in attention and consciousness (Engel et al., 2013), offering a direct window into the high complexity of brain information processing (de Pasquale et al., 2012; Larson-Prior et al., 2013). On the basis of such development, here we studied MEG

functional connectivity at the level of brain sources to investigate DMN interactions in meditation. Specifically, we used a phase-coherence based approach that estimates the degree of linear coupling/synchronization between oscillatory signals of distant neuronal ensembles. We hypothesize that DMN internal coupling as well as its interactions with executive control (FP) network show frequency specific traits which differ in FA and OM meditation, with a crucial role played by the alpha rhythm. Moreover, coupling ranks might represent a marker of FA and OM meditation skills or expertise. Specifically, given that the posterior cingulate cortex (PCC) is the core node of the DMN (Buckner et al., 2008), in this work we assessed MEG functional connectivity by mapping phase-coherence with respect to the PCC node of the DMN across three experimental conditions: FA meditation, OM meditation and a rest condition. Our study involved a highly selected group of “virtuoso” meditators (Theravada Buddhist monks), with long-term training in both FA and OM meditation styles (see also Manna et al., 2010), emphasizing the cultivation of attention and awareness (monitoring) skills through all moments of their monastic life (Sumedho, 1994).

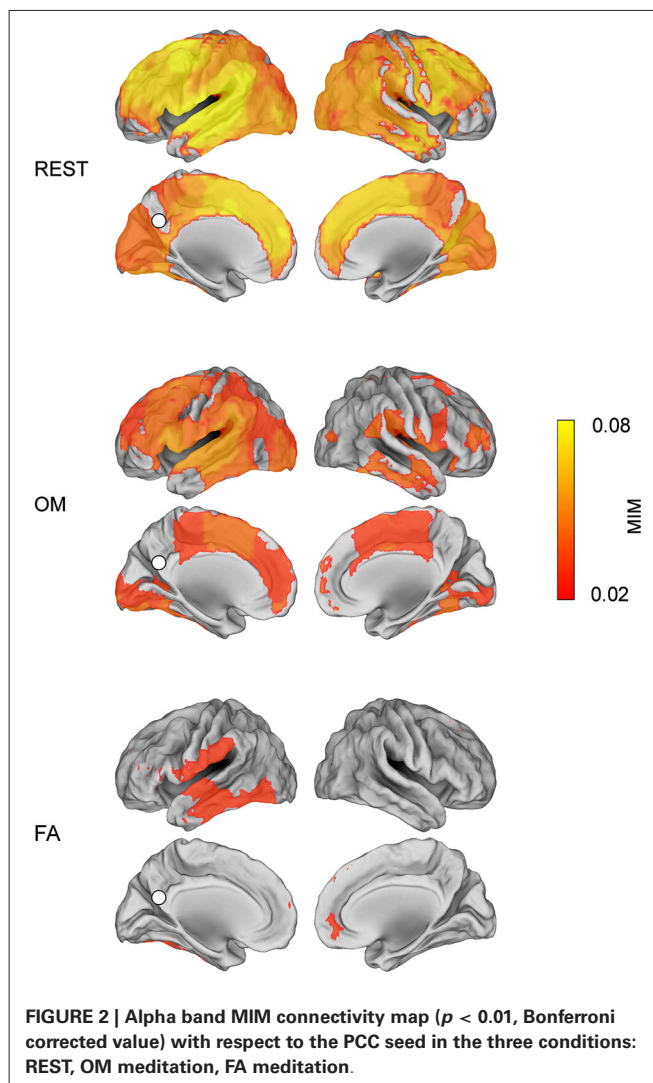
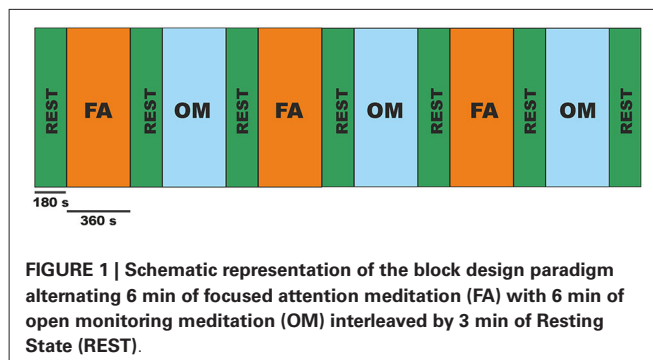
## MATERIALS AND METHODS

### PARTICIPANTS, PROCEDURES, AND ACQUISITION

An experienced meditator group of Theravada Buddhist monks was enrolled in this study. Specifically, the experienced meditator group consisted in eight Theravada Buddhist monks (all right handed males, mean age 37.9 years, range 25–53 years, SD 9.4 years), with, on average, over 15,750 h of meditation practice in Theravada Buddhist monasteries. The monks were recruited from the Santacittarama monastery, in Italy, where they follow a Thai Forest Tradition. In this tradition, monks experience regular intensive meditation retreats, with a balanced practice of *Samatha* (FA) and *Vipassana* (Open Monitoring, OM) meditation forms. These retreats also include a long winter retreat lasting for about 3 months. Outside the retreat periods, the monks typically practice 2 h per day balanced FA and OM meditation styles, with the monastery community. The experiment was conducted with the subject written informed consent according to the Declaration of Helsinki, as well as with the approval of the local responsible Ethical Committee. Only highly trained monk meditators were included in the study, with a minimal meditation expertise of about 2500 h, since an extensive training is necessary for reliably perform the two meditation styles. The same group underwent also fMRI scans which were analyzed in a previous study by our group (Manna et al., 2010).

The experimental paradigm consisted in a block design of 6 min FA meditation and 6 min OM meditation blocks, each preceded and followed by a 3 min non meditative resting state block (REST). Each sequence was repeated three times, see **Figure 1**. During all conditions, the subjects were sitting under the MEG scanner keeping their eyes closed and did not employ any discursive strategy, recitation, breath manipulation, or visualization technique.

The switch between conditions was instructed by the experimenter through an auditory word-signal consisting in the



condition name, i.e., “Rest”, “Samatha”, “Vipassana” delivered via an interphone prior to the beginning of each recording block during a pause to the MEG acquisition between the end of one block and the beginning of the subsequent one (corresponding to the black vertical lines in the scheme of **Figure 2**).

At the end of the experiment, all participants were subject to a retrospective assessment of their ability to perform the

task consisting in an in-house developed questionnaire. All participants reported they could correctly perform the three task conditions and experienced no differences in the difficulty in performing the two meditation styles. They also reported that the MEG scanner was perceived as a natural setting for mindfulness meditation thanks to the sitting position and the quiet environment.

MEG data were recorded by the 165-channel MEG system installed inside a magnetically shielded room at the Institute of Advanced Biomedical Technologies (ITAB), University of Chieti (Pizzella et al., 2001; Chella et al., 2012). This system includes 153 dc SQUID integrated magnetometers arranged on a helmet covering the whole head plus 12 reference channels. Electrocardiogram (ECG) and electro-oculogram (EOG) signals were also recorded for artifact rejection. All signals were band-pass filtered at 0.16–250 Hz and digitized at 1 kHz.

After each FA meditation, OM meditation and REST block, the position of the subject's head with respect to the sensors was determined by acquiring the signal generated by five coils placed on the subject's scalp before the starting of the MEG session. The coil positions, together with anatomical landmarks (left and right preauricular and nasion), were measured by means of a 3D digitizer (3Space Fastrak; Polhemus) allowing for the definition of a subject head based coordinate system and coregistration to magnetic resonance (MR) anatomical images. Magnetic resonance images were acquired using a sagittal magnetization prepared rapid acquisition gradient echo T1-weighted sequence (MP-RAGE; Siemens Vision scanner 1.5 T; TR = 9.7 s, echo time TE = 4 ms, alpha = 12°, inversion time = 1200 ms, voxel size =  $1 \times 1 \times 1 \text{ mm}^3$ ).

### MEG BRAIN SIGNAL RECONSTRUCTION

The recorded MEG data were pre-processed by using an independent components analysis based algorithm (Mantini et al., 2011). In brief, the algorithm projects the MEG data onto a set of maximally independent components and automatically classifies them, thus identifying artifactual components (e.g., cardiac artifact, eye movements) and components generated by brain signals. A similar classification procedure has also been employed in Sagar et al. (2012). Components classified of brain origin were thus projected at the brain level in order to identify the location and intensity of the corresponding neural source/sources. To this aim, the brain component topographies were input to a weighted Minimum-Norm Least Squares (wMNLs) linear inverse implemented in the Curry 6.0 (Neuroscan) analysis software (Fuchs et al., 1999). Brain currents were reconstructed on a Cartesian 3D grid with 4 mm step (i.e.,  $4 \times 4 \times 4 \text{ mm}^3$  voxel size) bounded by the subject brain volume as derived from segmentation of individual MR images. Once the component topographies had been projected onto the brain space, the activity at each voxel at each sample in time was obtained as a linear combination of the component time courses weighted by their related brain source map. Further details are given in Marzetti et al. (2013).

### MEG FUNCTIONAL CONNECTIVITY

The estimated MEG brain signals were the starting point for the study of functional coupling of ongoing brain activity.

Here, to map MEG functional connectivity we used an extension of the imaginary part of coherence for detecting lagged coupling, namely the Multivariate Interaction Measure (MIM; Ewald et al., 2012; Marzetti et al., 2013), that maximizes the imaginary part of coherence between a given reference voxel (*seed*,  $s$ ) and any other voxel (*target*,  $j$ ). More specifically, the estimated MEG signal at each brain voxel is a vector quantity that can be represented through its components in a given reference system. Multivariate Interaction Measure is designed to maximize the imaginary part of coherence between vector quantities. The mathematical details on MIM derivation can be found in Ewald et al. (2012). For the reader convenience, we briefly review MIM definition in the following.

Given the vector Fourier transformed signals as a function of frequency  $f$  at the seed and target voxels:  $X_s(f)$  and  $X_j(f)$ , respectively, and introducing the compact notation  $X(f) = [X_s^T(f) \ X_j^T(f)]^T$ , the cross-spectrum between the two vectors  $X_s(f)$  and  $X_j(f)$ , can be written in the block form:

$$C(f) = \langle X(f)X(f)^* \rangle = \begin{pmatrix} C_{ss}^R(f) + JC_{ss}^I(f) & C_{sj}^R(f) + JC_{sj}^I(f) \\ C_{js}^R(f) + JC_{js}^I(f) & C_{jj}^R(f) + JC_{jj}^I(f) \end{pmatrix}$$

and MIM between  $s$  and  $j$  is thus defined as:

$$\text{MIM}_{sj} = \text{tr} \left( (C_{ss}^R)^{-1} C_{sj}^I (C_{jj}^R)^{-1} (C_{sj}^I)^T \right)$$

In the above notation,  $\text{tr}$  indicates matrix trace, the T subscript indicates matrix transpose, superscripts R and I denote the real and the imaginary parts, the  $^{-1}$  subscript indicates matrix inverse, the \* subscript indicates matrix conjugate transpose, and the capital J indicates the imaginary unit. A more detailed recapitulation of the method is also given in Marzetti et al. (2013).

In this work, cross-spectra were estimated with Fast Fourier analysis after signal linear de-trending and Hanning windowing and were averaged using time epochs of 1.0 s duration with 50% overlap leading to a frequency resolution of 1 Hz. The number of averaged epochs is approximately 700 for each block of the OM and FA meditations and approximately 350 for each rest block.

The method, being based on the maximization of imaginary coherence, largely overcomes the well-known limitation to the study of functional connectivity by EEG/MEG posed by signal mixing artifacts, i.e., any active source in the brain contributes, in a weighted manner, to the signals measured at all sensors through volume spread (see Figure 2A in Engel et al., 2013). This effect constitutes an especially severe confound for estimates of brain interactions (Nolte et al., 2004; Marzetti et al., 2007; Schoffelen and Gross, 2009; Sekihara et al., 2011) and needs to be taken into account by mapping MEG functional connectivity through robust measures.

Functional connectivity through MIM was here estimated with a seed based approach, i.e., between the signal at the *seed* voxel and the signals at all other target brain voxels (approximately 28,000), and, in order to investigate the role of the DMN in frequency specific coupling to other brain networks in the different conditions, the seed was chosen in the PCC, the core node of the DMN (Buckner et al., 2008).

Functional connectivity was estimated for frequencies corresponding to the delta to gamma brain rhythms, i.e., from 2 to 80 Hz. To improve frequency specificity, consecutive frequency bins were further averaged over frequency bands defined on the basis of IAF peak. The alpha band was thus defined for each subject as  $IAF \pm 2$  Hz; the definitions of the other frequency bands were individually adjusted accordingly. On average, these bands span the following frequency ranges: delta (2–3.5 Hz), theta (4–7 Hz), alpha (8–12 Hz), beta (13–30 Hz), gamma (30–80 Hz) in accordance with conventional practice.

To investigate significant functional connectivity to PCC, a non-parametric Wilcoxon signed-rank test was used to assess voxel-wise significance across subjects ( $p < 0.01$ , Bonferroni corrected). For each frequency band, the MIM distribution across subjects for each voxel was compared to the empirical distribution of MIM for independent sources (simulated as independent and identically distributed, i.i.d., Gaussian noise) using a Monte Carlo approach with 20,000 repetitions. This procedure allowed to identify significant connections to PCC for each condition after Bonferroni correction for multiple comparisons.

A paired two tail  $t$ -test was used to compare MIM values between conditions (e.g., OM meditation condition and REST) and to derive  $t$ -contrast maps between condition pairs after false discovery rate correction (Benjamini and Hockberg, 1995) for multiple comparisons ( $p < 0.01$ , FDR corrected), thus highlighting brain regions that are differently involved in a specific meditative state.

Specifically, to the aim of understanding whether different meditation styles involve differential coupling between PCC and other brain areas in different frequency bands, we evaluated coupling to PCC in terms of  $t$ -maps for all possible contrast pairs: i.e., OM-FA, OM-REST, FA-REST. All maps were normalized to a common Montreal Neurological Institute (MNI) atlas through an affine transformation implemented in SPM8 (Friston, 2003) for comparison across subjects and projected to the standard brain surface for visualization by using the Caret software<sup>1</sup> (Van Essen et al., 2001).

## RESULTS

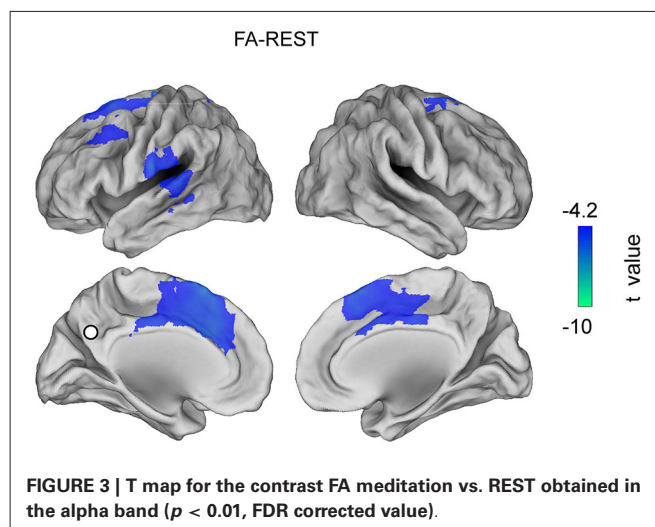
### STATE-DEPENDENT MEG FUNCTIONAL CONNECTIVITY

**Figure 2** shows condition specific alpha band MIM maps of functional connectivity to PCC after correction for multiple comparisons,  $p < 0.01$ , Bonferroni corrected. The PCC seed is indicated with a white dot. Moreover, the areas whose MIM value is equal or larger than the 75% of the maximum MIM value for each condition are listed in **Table 1**. Specifically, in OM meditation this procedure identified the PCC coupling to left lateral temporal cortex (lLTC), left superior frontal gyrus (lSFG), left middle superior frontal gyrus (lMSFG), left anterior cingulate cortex (lACC), left dorsolateral prefrontal cortex (ldlPFC), left angular gyrus (lAG) and right ventral inferior temporal gyrus (rvITG). In FA meditation, this procedure identified the PCC coupling to rvITG, right and left lateral temporal cortices (LTC) and left inferior occipital lobe (lIOG). During REST, the highest

**Table 1 | List of MNI coordinates for the areas most significantly connected to posterior cingulate cortex in the alpha band.**

	Hemisphere	x (mm)	y (mm)	z (mm)	ROI
OM	L	-61	-33	-6	LTC
	L	-17	30	61	SFG
	L	-43	20	49	MSFG
	L	-7	0	50	ACC
	L	-23	31	48	dIPFC
	L	-64	-42	38	AG
FA	R	56	-41	14	rvITG
	L	-26	-97	5	lIOG
	L	-61	-11	-6	LTC
REST	R	56	-41	-14	rvITG
	R	61	-22	-6	LTC
	L	-61	-33	-7	LTC
	L	-17	30	61	SFG
	L	-43	20	49	MSFG
	L	-7	0	50	ACC
	L	-64	-42	38	AG
	L	-4	46	12	mPFC
	R	4	0	47	ACC

The Region of Interest (ROI) represent areas whose MIM value is equal or larger than the 75% of the maximum MIM value for each condition. The ROI labelling is as follows: lateral temporal cortex (LTC), superior frontal gyrus (SFG), middle superior frontal (MSFG), ventral inferior parietal sulcus (vIPS), anterior cingulate cortex (ACC), dorsolateral prefrontal cortex (dlPFC), angular gyrus (AG), ventral inferior temporal gyrus (vITG), inferior occipital gyrus (IOG), left medial prefrontal cortex (lmpPFC).

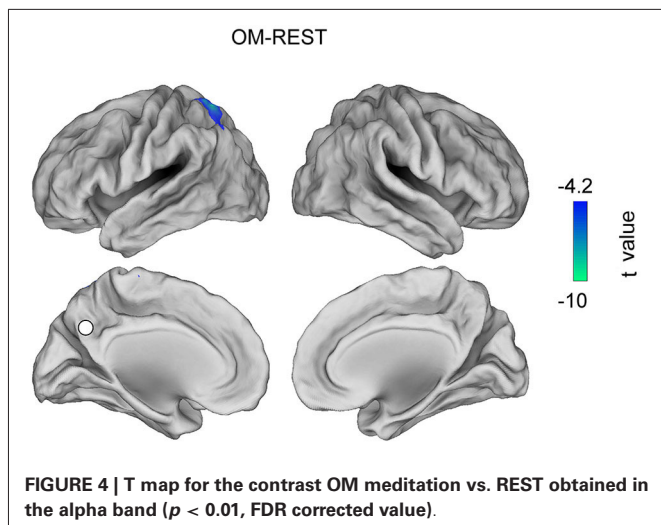


**FIGURE 3 | T map for the contrast FA meditation vs. REST obtained in the alpha band ( $p < 0.01$ , FDR corrected value).**

coupling was observed with respect to left medial prefrontal cortex (lmpPFC), lLTC, lSFG, lMSFG, lACC and lAG.

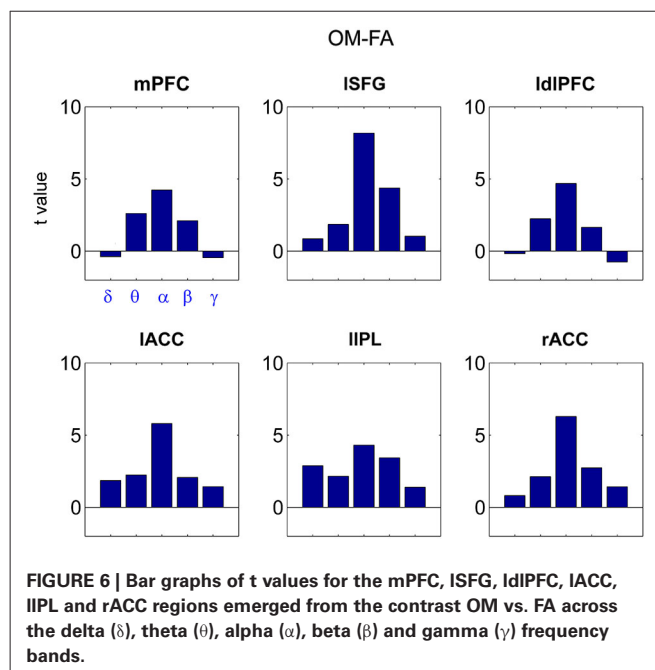
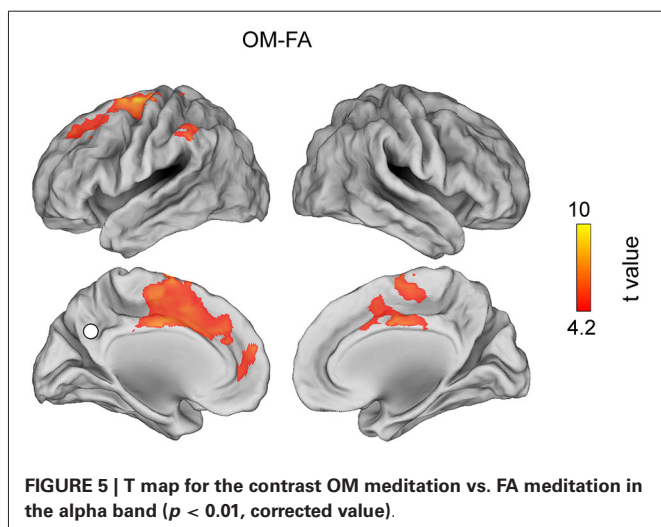
**Figures 3, 4, 5** show the topographies of significant  $t$ -maps ( $p < 0.01$ , FDR corrected) in alpha for all the contrast pairs, namely the FA meditation vs. REST contrast is shown in **Figure 3**; the OM meditation vs. REST contrast is shown in **Figure 4** and the OM vs. FA meditation results are reported in **Figure 5**.

<sup>1</sup><http://www.nitrc.org/projects/caret/>



**Table 2 | List of ROIs significantly differently connected to posterior cingulate cortex in the alpha band in the contrast between conditions.**

	Hemisphere	x (mm)	y (mm)	z (mm)	ROI	Connectivity to PCC
FA-REST	L	-17	30	61	<i>SFG</i>	REST > FA
	L	-43	18	43	<i>MSFG</i>	REST > FA
	L	-61	-33	-6	<i>LTC</i>	REST > FA
	L	-7	0	50	<i>ACC</i>	REST > FA
	R	21	8	69	<i>SFG</i>	REST > FA
	R	10	0	51	<i>ACC</i>	REST > FA
OM-REST	L	-22	-58	67	<i>IPS</i>	REST > OM
OM-FA	L	-4	46	12	<i>mPFC</i>	OM > FA
	L	-28	-4	69	<i>SFG</i>	OM > FA
	L	-23	31	48	<i>dlPFC</i>	OM > FA
	L	-1	-2	44	<i>ACC</i>	OM > FA
	L	-58	-37	42	<i>IPL</i>	OM > FA
	R	2	0	46	<i>ACC</i>	OM > FA



### FOCUSED ATTENTION MEDITATION VS. RESTING STATE

The alpha band connectivity in the contrast between FA meditation and REST (Figure 3) results in the PCC being more coupled to ISFG, left superior middle frontal gyrus (ISMFG), ILTC, left and right ACC during REST than during FA meditation. See Table 2.

### OPEN MONITORING MEDITATION VS. RESTING STATE

The contrast between OM meditation and REST results in only the left intraparietal sulcus being significantly less connected to PCC during OM meditation than during REST.

### OPEN MONITORING VS. FOCUSED ATTENTION MEDITATION

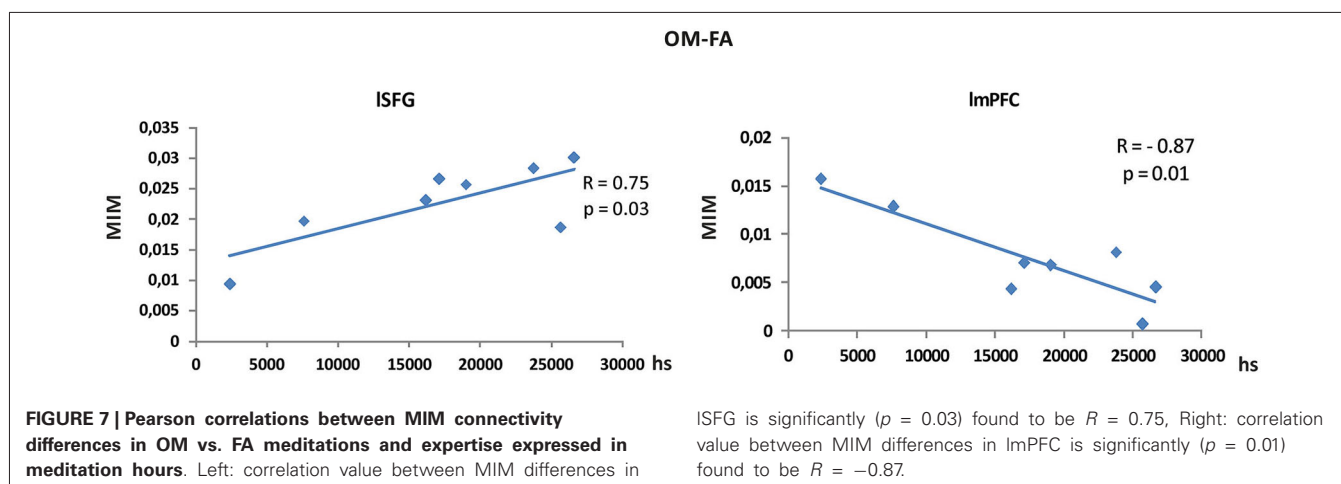
The contrast between OM meditation and FA meditation (Figure 5) highlights the stronger alpha band coupling during OM meditation of PCC with the following regions: *lmPFC*, *ISFG*, *ISMFG*, *dlPFC* and *IACC*, left inferior parietal lobule (*IPL*). See Table 2.

### FREQUENCY SPECIFICITY

Notably, the coupling of PCC to the nodes of Default Mode and Fronto Parietal networks as listed in Table 2 was a specific signature of the alpha band as it was not observed in the other frequency bands included in the analysis. Figure 6 shows the t values, represented as bar graphs, for the OM vs. FA contrast. T values were extracted for the ROI coordinates listed in Table 2 for OM-FA for the delta ( $\delta$ ), theta ( $\theta$ ), alpha ( $\alpha$ ), beta ( $\beta$ ) and gamma ( $\gamma$ ) frequency bands. This is a representative situation showing the frequency specificity of the observed coupling.

### CORRELATION WITH MEDITATION EXPERTISE

To evaluate to what extent the alpha band differences between conditions reported in Figures 3, 4, 5 might be explained by



differences in meditation expertise within the monk group, we correlated the difference between MIM values in the two conditions with meditation expertise measured as overall meditation hours, for all brain areas listed in **Table 2**. Significant Pearson correlation was found in the contrast between OM and FA meditation for the ISFG and ImPFC nodes. The difference was calculated using values extracted from the voxel closest (according to Euclidean distance) to the MNI coordinate listed in **Table 2**. Nevertheless, consistent results were observed in the node surroundings within a sphere of about 1 cm diameter. Specifically, a positive correlation ( $R = 0.75$ ,  $p = 0.03$ ) was found for the difference of MIM values between OM and FA meditations in ISFG and a negative correlation ( $R = -0.87$ ,  $p = 0.01$ ) was found in ImPFC. See **Figure 7**. All the other brain regions and condition contrasts did not show a significant correlation with meditation expertise.

## DISCUSSION

This study aimed at investigating the effects of FA and OM meditation on MEG functional connectivity to the PCC, a crucial DMN node (Raichle et al., 2001; Buckner et al., 2008), in skilled long-term FA/OM meditators. Overall, the results indicate that the different conditions modulate the coupling between PCC and nodes of the DMN and of the FP (executive) network (Vincent et al., 2008) in the alpha band. The temporal richness of the MEG signal allowed us to quantify functional connectivity by frequency specific patterns able to capture stationary properties of network interactions in the brain. This goal was here achieved in a way robust to possible self-coupling confounds deriving by MEG poor spatial resolution and signal mixing artifacts.

Our phase coherence based approach was able to reveal stable functional connectivity patterns with respect to PCC across the meditation conditions and during the resting state. As shown in **Figure 2**, an overall reduced connectivity was observed during the two meditation conditions in comparison to the resting state, consistently with the EEG findings reported in Lehmann et al. (2012) and Berkovich-Ohana et al. (2013). This reduced connectivity was here expressed both in terms of lower average MIM values and of more localized connectivity topographies in meditation.

Moreover, high topographical similarity was shared between the resting state and the OM meditation condition, compared to all other condition pairs.

When FA meditation was compared to the resting state, see **Figure 3**, a lower engagement of left and right superior frontal gyrus, lMSFG and lateral temporal cortex and of left and right anterior cingulate cortex was observed. Indeed, in line with an earlier fMRI study (Manna et al., 2010), functional deactivations during FA meditation as compared to the resting state involve executive (FP) areas, which have been found to activate with the DMN during mind wandering in another study (Christoff et al., 2009).

When OM meditation was compared to the resting state, see **Figure 4**, the left intraparietal sulcus was more connected to PCC during REST than during OM meditation. The left intraparietal sulcus may thus be more involved in executive and monitoring functions in OM meditation (Szameitat et al., 2002; Lutz et al., 2008), rather than being as coupled to the DMN (PCC) as in the resting state.

More interestingly, when OM meditation was directly compared to FA meditation, see **Figure 5**, regions in the left hemisphere belonging to the DMN (i.e., ImPFC) and the FP network (i.e., IACC, ldlPFC and left inferior parietal lobe) were more functionally connected to PCC. Also ISFG, an area which has been involved in both self-referential processing, linked to the DMN (e.g., Goldberg et al., 2006), and executive functions and monitoring (e.g., du Boisgueheneuc et al., 2006), were more functionally connected to PCC during OM meditation in comparison to FA meditation. The higher coupling within the DMN can be related to the higher occurrence of thoughts and mental images during OM meditation than during FA meditation (Lutz et al., 2008; Raffone and Srinivasan, 2009). Similarly, the coupling with the ISFG can be related to an increased meta-awareness or monitoring of ongoing thoughts and mental images generated with involvement of the DMN, in OM as compared to FA meditation (Lutz et al., 2008; Raffone and Srinivasan, 2009). Indeed, the increased monitoring (mindfulness) during OM meditation would lead to a meta-awareness that enables the maintenance of the meditative state even in presence of spontaneous mentation. This mindful

observing ability is plausibly more developed in meditators with a higher level of expertise (Figure 7; Lutz et al., 2008), in line with our results here for (positive) correlation between functional connectivity to PCC and meditation expertise, showing that coupling is differentially regulated by meditation expertise in ISFG. Finally, a negative correlation between functional coupling of *l*mpFC to PCC and meditation expertise was found, as related to the OM vs. FA meditation contrast, which appears consistent with an expected reduced identification (self-reference) of more expert meditators with ongoing mental activity in any of the two forms of meditation (Lutz et al., 2008). This evidence may also be related to an attenuated medial prefrontal cortex activation with emotional thought contents (Northoff et al., 2004), likely to arise with OM meditation as compared to FA meditation, with meditation expertise. By contrast, meditators with a lower expertise exhibited a higher modulation of the coupling between PCC and *l*mpFC within the DMN in shifting between FA (with lower coupling) and OM (with higher coupling) meditation styles.

As shown in earlier neuroimaging studies, the ISFG is involved in self-related processing and awareness (Goldberg et al., 2006), which can be related to the notion of “narrative self” (Gazzaniga, 1995). In this respect, based on neuroimaging results, theorists have suggested that the brain systems for the reflective self are likely to involve lateral prefrontal areas, and not just midline DMN areas (Northoff et al., 2006; Tagini and Raffone, 2010). Our present study further suggests that the neural mechanisms for the “narrative self” may involve the crucial coupling between PCC and ISFG in the alpha band, which can be modulated by meditation, with differential effects of FA and OM styles. Since the ISFG has also been related to executive and monitoring functions (e.g., in working memory) (du Boisgueheneuc et al., 2006), the differential coupling between PCC and ISFG in the alpha band found in our study may be linked to a differential recruitment of neuronal populations in the ISFG for self-referential thought vs. executive and cognitive monitoring. Indeed, neuronal responses in lateral prefrontal cortex are highly adaptive, depending on the task setting and individual differences (Duncan, 2001). Interestingly, as suggested by our results, different styles of meditation and meditation expertise appeared to modulate such coupling and possibly the dynamic balance between the recruitment of FP and DMN networks.

Notably, all of the observed effects were specific to the alpha band (Figure 6). Besides the idling hypothesis, the role of alpha band phase coupling in meditation might be closely related to the role of alpha band synchronization as a functional mechanism of attention and consciousness (Palva and Palva, 2007; Knyazev, 2013). Indeed, an inhibitory role has been associated to the alpha rhythm to the aim of filtering out irrelevant sensory inputs (Klimesch et al., 2007; Bonnefond and Jensen, 2013) in a broad range of information processing tasks including selective spatial attention (Rihs et al., 2007; Foxe and Snyder, 2011; Van Ede et al., 2011) and working memory (Sauseng et al., 2009; Hagens et al., 2010; Spitzer and Blankenburg, 2011; Bonnefond and Jensen, 2012). Evidence indeed suggests that FA and OM meditation styles entail unique sets of attention and consciousness, and are not merely degrees of a state of relaxation

(Dunn et al., 1999). More specifically, our findings highlighted a possible role of such rhythm in maintaining the stability of DMN internal phase coupling and subserving its modulation with the FP network, according to the specific meditation state. Indeed, the presently observed findings are consistent with a top-down alpha modulation hypothesis as a mechanism involved in stress-therapy meditation (Kerr et al., 2011), and with the idea that cooperation between the DMN and the FP network helps sustain monitoring of thoughts against compulsory self-reference (identification) (Farb et al., 2007) and interference (Smallwood et al., 2012). Taken together, our results support the idea that an interplay between the DMN and the FP network is crucial for the transition from resting state to different meditative states.

It has to be noted that it is not trivial that nodes classically ascribed by fMRI as belonging to the DMN and the FP should emerge as coupled to PCC also in MEG connectivity studies. Indeed, MEG provides a window into the high complexity of brain information processing at the temporal scales relevant for behavior which translate into frequency resolved coupling. For this reason, different systems comprised by some of the network nodes classically identified by fMRI might be represented by MEG phase coherence at different frequency scales, possibly speaking for a functional dissociation of network subsystems in the frequency domain.

A possible limitation of this study is the relatively small number of subjects included in the analysis. Our emphasis was indeed on the high (“virtuoso”) skills in both FA and OM meditation of the Theravada Buddhist monks involved in our study, appearing as a rare and selected sample in literature. Moreover, we did not include a comparison with a group of novice practitioners. In this respect, however, a recent fMRI study (Manna et al., 2010) with the same participants performing FA and OM meditation, found the most relevant differences in the contrasts between FA meditation, OM meditation and resting state conditions within the monk group, in line with our present focus. Indeed, for novice meditators it might be difficult to control for and to differentiate between the meditative states which is the primary focus of this study. As a general remark, it is indeed difficult to objectively validate what the participants are doing in a task which involves inherently subjective and covert states, such as FA and OM meditations. We believe that our involvement of meditators (Theravada Buddhist monks) who are expert in both FA and OM meditation has minimized the chances of inaccurate performance of the two meditation tasks, and this was also evident from the retrospective reports. Finally, it would be worth in the future to include in the protocol a controlled manipulation of attention by introducing a task (e.g., a sustained response inhibition task as in Zanenko et al., 2013). This would allow to e.g., compare task based functional connectivity before and after the meditation blocks and to correlate connectivity results with task performance.

## CONCLUSIONS

To summarize, the present study allowed to characterize the coupling of the major DMN node, the PCC, with the rest of the brain, and highlighted, in a data driven manner, its



coupling to nodes of DMN and FP network specific to the alpha band. Our findings showed that the alpha band is selectively involved in the different couplings of PCC in the two meditation styles and during rest, and that a stable coupling within DMN and between DMN and FP network characterized the contrast between the two meditation styles, which was correlated to meditation expertise.

More generally, MEG functional connectivity was able to reveal important features of meditative states in the brain which were modulated by expertise. Indeed, MEG can provide a unique neuroimaging tool to study meditation and mindfulness processes thanks to its ability to recover brain functional coupling in a frequency resolved manner, thus reconciling the long tradition of the EEG based approach with an fMRI network based approach to meditation. Not secondary to this aim, the MEG scanner appeared as a more convenient setting for performing research on meditation thanks to the sitting position that the subject can maintain during the measurement, as well as to the absence of any disturbing external noise inside the shielded room in which the MEG system is set.

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