



The Nonallergic Asthma of Obesity

A Matter of Distal Lung Compliance

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Abstract

Rationale: The pathogenesis of asthma in obesity is poorly understood, but may be related to breathing at low lung volumes.

Objectives: To determine if lung function in obese patients with asthma and control subjects would respond differently to weight loss.

Methods: Lung function was evaluated by conventional clinical tests and by impulse oscillometry in female late-onset, nonallergic patients with asthma and control subjects before, and 12 months after, bariatric surgery.

Measurements and Main Results: Patients with asthma ($n = 10$) had significantly lower FEV₁ (79.8 ± 10.6 vs. $95.5 \pm 7.0\%$) and FVC (82.4 ± 13.2 vs. $93.7 \pm 8.9\%$) compared with control subjects ($n = 13$). There were no significant differences in FRC or TLC at baseline. Twelve months after surgery, control subjects had significant increases in FEV₁ (95.5 ± 7.0 to 100.7 ± 5.9), FVC (93.6 ± 8.9 to $98.6 \pm 8.3\%$), FRC (45.4 ± 18.5 to $62.1 \pm 15.3\%$), and TLC (84.8 ± 15.0 to $103.1 \pm 15.3\%$), whereas patients with asthma had improvement only in FEV₁ (79.8 ± 10.6 to 87.2 ± 11.5). Control subjects and patients with asthma had a significantly different change in respiratory system resistance with weight loss: control subjects exhibited a uniform decrease in respiratory system resistance at all frequencies, whereas patients with asthma exhibited a decrease in frequency dependence of resistance. Fits of a mathematical model of

lung mechanics to these impedance spectra suggest that the lung periphery was more collapsed by obesity in patients with asthma compared with control subjects.

Conclusions: Weight loss decompresses the lung in both obese control subjects and patients with asthma, but the more pronounced effects of weight loss on lung elastance suggest that the distal lung is inherently more collapsible in people with asthma.

Keywords: bariatric surgery; forced oscillation technique; impedance; lung volume

At a Glance Commentary

Scientific Knowledge on the Subject: Obesity is a major risk factor for asthma. It has been thought that this may be related to airway reactivity induced by breathing at low lung volumes.

What This Study Adds to the Field: Differences in lung volume do not distinguish between obese patients with and without asthma. Changes with weight loss suggest that obese patients with asthma have more collapsible peripheral airways than obese patients without asthma, suggesting that asthma in obesity is related to an abnormality in the lung periphery.

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Obesity is an important risk factor for asthma (1–3), especially in women (1), and is associated with poor asthma control (4, 5) and resistance to standard controller therapies (6, 7). The mechanistic link between asthma and obesity remains unclear. A number of causative factors have been proposed, including systemic and/or airway inflammation, mechanical effects caused by chronic lung compression, and comorbidities of obesity (3). Asthma in obesity may arise for a variety of different reasons. Indeed, some obese patients with asthma have an early onset form of allergic disease that is complicated by the development of obesity, whereas others develop *de novo* asthma later in life as a consequence of obesity (8). These represent two distinct obese asthma phenotypes (9–11) that likely have distinctly different causes.

Here we focus on the late-onset nonallergic phenotype of asthma in obesity, because this form of disease seems to be a direct consequence of obesity. We have previously shown that these patients with asthma have minimal airway inflammation, which does not change with weight loss (11). This form of asthma has a potentially straightforward explanation: obese patients with asthma breathe at low lung volumes as a result of mass loading of their chest wall, leading to the kind of airways hyperresponsiveness that has been modeled in normal-weight volunteers via imposed reductions in lung volume (12). This explanation is supported by recent data showing that weight loss improves lung function and airway reactivity, particularly in those with late-onset low-IgE disease (9). However, only a subset of the obese population has asthma; most obese individuals have normal lung function (13) even though one would presume that all obese individuals are at risk for breathing at low lung volumes. The role of lung volume in the asthma of obesity thus remains an open question.

Prior studies suggest that obesity may cause abnormalities particularly in peripheral lung function (14–16). This is poorly measured by conventional lung function tests, which involve deep breaths and forced maneuvers that mask changes in the lung periphery, and so we used impulse oscillometry as an adjunctive measure of lung function before and after weight loss. Impulse oscillometry uses the dynamic relationship between an imposed flow signal and the resulting airway pressure signal to determine

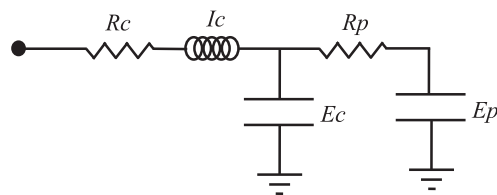


Figure 1. Electric circuit representation of lung mechanics in which the proximal airways (resistance [R_c]; gas inertance [I_c]) connect to a central elastic compartment representing the stiffness (E_c) of the conducting airways. The central compartment in turn connects to a distal compartment representing the elastance of the alveolar tissue (E_p) via a conduit representing the resistance (R_p) of the peripheral airways.

the mechanical impedance of the respiratory system over a range of frequencies from 5 to 35 Hz. Importantly, no large changes in lung volume are involved, so the measurements reflect lung function at volumes relevant to tidal breathing.

Current evidence suggests that not everyone is affected in the same way by obesity-related reductions in lung volume; some otherwise normal individuals develop nonatopic asthma when they become obese, whereas others remain nonasthmatic. This leads to the hypothesis that these two groups of obese individuals respond differently when their lung volumes are normalized through major weight loss. Verification of this hypothesis would provide important insights into the mechanisms of obese asthma. Accordingly, in the present study we compared lung

function in two groups of obese female subjects, one with late-onset low-IgE asthma and the other without asthma, and then determined how lung function changed in both groups after major weight loss because of bariatric surgery. Some of these results have previously been published in abstract form (17), and data from these subjects pertaining to asthma control and inflammatory changes with weight loss have previously been published (9, 11).

Methods

Participants

Participants undergoing evaluation for bariatric surgery at the University of Vermont teaching hospital were invited to participate in this study. We studied female

Table 1. Baseline Demographics and Lung Function

	Control	Asthma	P Value
Number	13	10	
Age, yr	43.6 ± 7.1	47.8 ± 6.6	0.17
BMI, preoperative	43.1 ± 5.6	48.5 ± 10.0	0.12
BMI, postoperative	32.7 ± 4.0	38.6 ± 7.2	0.02
FEV ₁	95.5 ± 7.0	79.8 ± 10.6	<0.001
FVC	93.7 ± 8.9	82.4 ± 13.2	0.02
FEV ₁ /FVC	102.2 ± 4.8	97.6 ± 9.4	0.09
TLC	84.8 ± 15.0	87.7 ± 11.9	0.63
IC	123.6 ± 16.3	117.4 ± 19.7	0.42
SVC	90.4 ± 9.0	83.1 ± 12.5	0.13
FRC	45.4 ± 18.5	45.5 ± 10.0	0.79
ERV	29.9 ± 21.5	21.1 ± 15.4	0.29
RV	81.7 ± 30.3	98.5 ± 23.5	0.17
RV/TLC	94.6 ± 28.3	112.3 ± 22.6	0.13
DL _{CO}	93.0 ± 16.3	94.8 ± 14.0	0.78

Definition of abbreviations: BMI = body mass index; DL_{CO} = diffusing capacity of carbon monoxide; ERV = expiratory reserve volume; IC = inspiratory capacity; RV = residual volume; SVC = slow vital capacity.

Values are expressed as mean and standard deviation % predicted. *P* values are for unpaired *t* tests for normally distributed data, and the Kruskal-Wallis test for nonnormally distributed data. Lung function values are shown as % predicted using Hankinson and coworkers (34) for spirometry, Goldman and Becklake (35) for lung volumes, and Gaensler and Wright (36) for DL_{CO}.

subjects because of their greater propensity to develop asthma when obese (1), compared with males. The study was reviewed by the local institutional review board, and written informed consent was obtained from all participants. Participants were evaluated before, and 12 months after, bariatric surgery. Late-onset nonallergic participants with asthma ($n = 10$) were initially diagnosed with asthma at more than 12 years of age and had physiologic evidence of asthma. This evidence was either provocative concentration of methacholine causing a 20% drop in FEV₁ (PC₂₀) less than 16 mg/ml (18), or improvement in FEV₁, FVC, or both of greater than or equal to 12% and 200 ml with bronchodilator (19). All subjects also had IgE less than 100 IU/ml. Participants with no asthma ($n = 13$) had no diagnosis of asthma and did not respond in a clinically significant manner to either methacholine or bronchodilator (PC₂₀ >16 mg/ml methacholine, response to bronchodilator <12%, and/or 200 ml in FEV₁). Exclusion criteria included (1) smoking history more than 20 pack-years; (2) smoking within the prior 6 months; (3) FEV₁ less than 60% predicted; (4) treatment with systemic steroids during the prior 6 weeks; (5) active pulmonary disease other than asthma (those with obstructive sleep apnea were not excluded); and (6) significant other disease that, in the opinion of the investigators, would interfere with study participation.

Study Design

We performed a cross-sectional comparison of asthmatic versus nonasthmatic to establish baseline differences between these two groups. We then performed a prospective observational study comparing the responses to weight loss. In all subjects we measured standard spirometric parameters, lung volume by gas dilution, and diffusing capacity of carbon monoxide according to American Thoracic Society guidelines (19–21). We also measured respiratory system impedance between 5 and 35 Hz during tidal breathing using impulse oscillometry (Jaeger, Wurzburg, Germany) during normal tidal breathing (details in online supplement).

Patients with asthma performed a methacholine challenge test using the five-breath dosimeter method according to American Thoracic Society guidelines (18)

both before and 12 months after bariatric surgery.

Statistical Analyses

Data were summarized using descriptive statistics in terms of mean values and standard deviations. We used a Mann-Whitney test to compare differences between obese subjects with and without asthma. Paired *t* tests were used to compare changes in measures within subjects from baseline to 12 months after bariatric surgery. Mixed models repeated measures analysis of variance was used to compare

changes within the asthmatic and control groups over time. Given the exploratory nature of this study, we did not attempt to control for multiple comparisons. Statistical tests were performed with STATA 11.0 (College Station, TX).

Mathematical Modeling of Impedance

We fit the two-compartment model represented in Figure 1 to the measured impedance spectra. This model attempts to strike a balance between representing the likely most relevant physiologic features of the lung while remaining simple enough

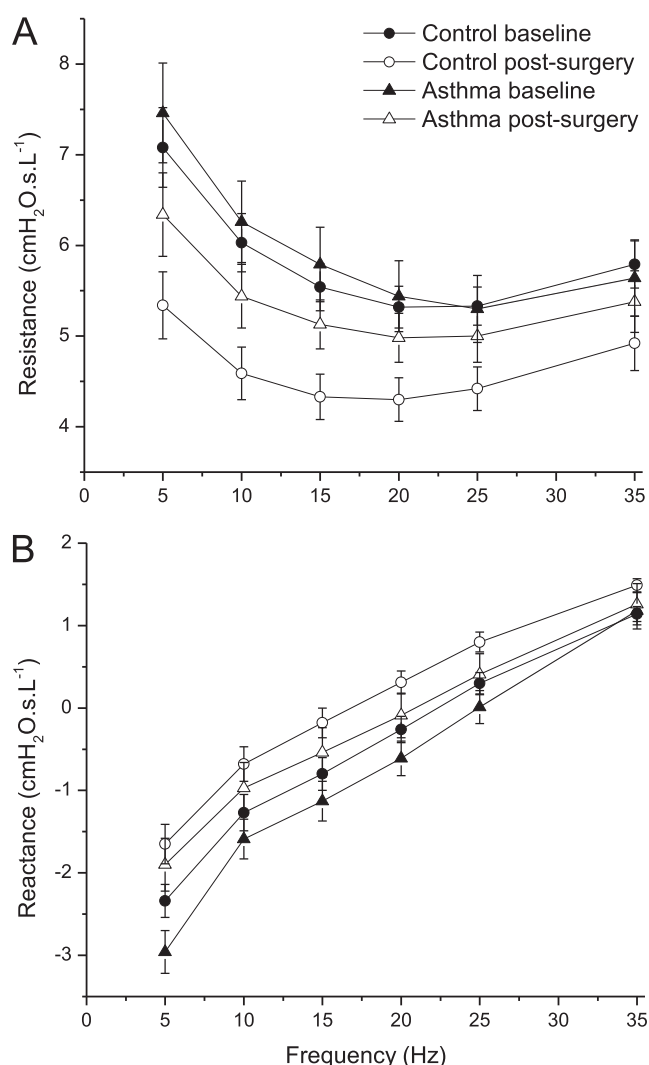


Figure 2. Respiratory system resistance (A) and reactance (B) measured (mean \pm SE) in control subjects and patients with asthma both at baseline and at 12 months after bariatric surgery. Mixed models repeated measures analysis of variance showed a significant group \times visit interaction for change in resistance in response to weight loss between patients with asthma and control subjects ($P = 0.03$ both unadjusted and adjusted for body mass index), but not for change in reactance ($P = 0.68$ unadjusted and $P = 0.48$ adjusted for body mass index).

to provide a unique fit to a given set of impedance data. Model simulation and fitting details are provided in the online supplement.

Results

Baseline Comparisons

At baseline, patients with asthma had significantly lower FEV₁ and FVC, and tended to have a higher residual volume/TLC, compared with control subjects. There was no difference in FRC or TLC between patients with asthma and control subjects (Table 1). Patients with asthma tended to be slightly heavier at baseline, although this did not reach statistical significance (Table 1).

There were no significant differences in baseline impedance between patients with asthma and control subjects, although both resistance and reactance tended to be more dependent on frequency in the patients with asthma (Figures 2A and 2B, respectively).

Effects of Weight Loss on Lung Function Tests

Twelve months after bariatric surgery, FEV₁, FVC, FRC, and TLC increased significantly in control subjects, suggesting reduced lung restriction (Table 2). FEV₁ and PC₂₀ also improved significantly in patients with asthma after surgery (Table 3), but there was no change in either FRC or TLC in this group, and TLC and residual volume tended to increase with weight loss more in control subjects than in patients with asthma (Table 4). Bronchodilator responsiveness measured by FEV₁ did not change with surgery in patients with asthma, although there was a trend toward less response in FVC (Table 3). This suggests unchanged airway tone, but perhaps less response in terms of airway closure, after weight loss and that the primary change with surgery was related to changes in airway closure and the lung periphery. There was no relationship between increase in FRC and improvement in PC₂₀ in subjects with asthma (Figure 3; $r = -0.4$; $P = 0.32$). There was no change in diffusing capacity with weight loss. Patients with asthma and control subjects still tended to be obese after weight loss, at which point the patients with asthma were significantly heavier than the control subjects (Table 1).

Table 2. Change in Pulmonary Function with Surgery in Control Subjects

	Baseline	12 mo after Surgery	P Value
FEV ₁	95.5 ± 7.0	100.7 ± 5.9	<0.01
FVC	93.7 ± 8.9	98.6 ± 8.3	<0.01
FEV ₁ /FVC	102.2 ± 4.8	102.5 ± 6.3	0.84
TLC	84.8 ± 15.0	103.1 ± 15.3	0.01
IC	123.6 ± 16.3	122.0 ± 25.1	0.78
SVC	90.4 ± 9.0	95.3 ± 10.6	0.14
FRC	45.4 ± 18.5	62.1 ± 15.3	0.04
ERV	29.9 ± 21.5	49.8 ± 29.4	<0.01
RV	81.7 ± 30.3	113.7 ± 38.4	0.07
RV/TLC	94.6 ± 28.3	108.1 ± 25.0	0.27
DL _{CO}	93.0 ± 16.3	91.5 ± 14.1	0.74

Definition of abbreviations: DL_{CO} = diffusing capacity of carbon monoxide; ERV = expiratory reserve volume; IC = inspiratory capacity; RV = residual volume; SVC = slow vital capacity. Values are expressed as % predicted mean and standard deviation. *P* values are for paired *t* test. For all lung volume parameters and DL_{CO}, *n* = 12 at baseline and *n* = 9 after surgery.

Effects of Weight Loss on Respiratory System Impedance

Weight loss had a significantly different effect on respiratory system impedance in the group with asthma compared with the control group.

Control subjects had a parallel shift and significant decrease in resistance at all frequencies after weight loss (Figure 2A; $P < 0.05$, comparing control subjects before and after). By contrast, patients with asthma exhibited a decreased dependence of resistance on frequency such that resistance was elevated at 5 Hz compared with control subjects but remained essentially the same by 35 Hz. When the

impedance spectra were normalized to FRC, there was a significant group–visit interaction ($P = 0.03$ after transformation to achieve normality of distribution, which did not change when body mass index [BMI] was included in the model) for resistance, indicating that there was a significantly different response to weight loss in patients with asthma compared with control subjects. Change in resistance was significantly related to change in BMI in control subjects only (see Figure E1 in the online supplement).

Reactance became less negative in control subjects at all frequencies with weight loss (Figure 2B; $P < 0.05$ comparing

Table 3. Change in Pulmonary Function with Surgery in Subjects with Asthma

	Baseline	12 Months after Surgery	P Value
FEV ₁	79.8 ± 10.6	87.2 ± 11.5	0.03
FVC	82.4 ± 13.2	87.5 ± 14.1	0.21
FEV ₁ BD Δ*	6.56 ± 3.94	6.55 ± 4.74	0.95
FVC BD Δ*	6.33 ± 4.56	3.22 ± 6.04	0.12
FEV ₁ /FVC	97.6 ± 9.4	100.1 ± 6.5	0.50
TLC	87.7 ± 11.9	88.8 ± 21.2	0.87
IC	117.4 ± 19.7	103.3 ± 35.0	0.27
SVC	83.1 ± 12.5	85.6 ± 13.0	0.44
FRC	45.5 ± 10.0	46.7 ± 25.9	0.89
RV	98.5 ± 23.5	85.5 ± 52.8	0.47
ERV	21.1 ± 15.4	34.6 ± 25.8	0.20
RV/TLC	112.3 ± 22.6	90.2 ± 37.2	0.12
DL _{CO}	94.8 ± 14.0	91.9 ± 11.5	0.56
PC ₂₀ (mg/ml methacholine)	4.7 ± 4.0	9.9 ± 6.4	<0.001

Definition of abbreviations: BD = bronchodilator; DL_{CO} = diffusing capacity of carbon monoxide; ERV = expiratory reserve volume; IC = inspiratory capacity; PC₂₀ = provocative concentration of methacholine causing a 20% drop in FEV₁; RV = residual volume; SVC = slow vital capacity. Values are expressed as mean and standard deviation % predicted, except where indicated.

For all lung volume parameters and DL_{CO}, *n* = 10 at baseline and *n* = 8 after surgery.

*Values are % improvement with bronchodilator and standard deviation *P* values are for paired *t* test.

Table 4. Difference in Changes over Time in Lung Function between Control Subjects and Patients with Asthma in Response to Bariatric Surgery

	Control Subjects Mean Difference (95% CI)	Patients with Asthma Mean Difference (95% CI)	P Value*	Adjusted P Value†
FEV ₁	5.2 (0.9 to 9.4)	7.4 (2.5 to 12.2)	0.49	0.29
FVC	4.9 (−0.1 to 9.9)	5.1 (−0.6 to 10.8)	0.96	0.83
FEV ₁ /FVC	0.3 (−4.3 to 4.8)	2.5 (−2.7 to 7.7)	0.50	0.51
TLC	17.1 (4.6 to 29.7)	1.5 (−11.4 to 14.3)	0.08	0.16
IC	−2.7 (−20.6 to 15.2)	−13.2 (−31.6 to 5.1)	0.4	0.64
SVC	3.1 (−2.9 to 9.1)	3.0 (−3.0 to 9.0)	0.98	0.95
FRC	15.8 (0.3 to 31.3)	1.2 (−14.8 to 17.2)	0.18	0.19
ERV	19.2 (3.2 to 35.2)	12.6 (−3.7 to 29.0)	0.55	0.37
RV	30.8 (−1.5 to 63.1)	−12.8 (−46.2 to 20.6)	0.06	0.07
RV/TLC	12.2 (−12.4 to 36.9)	−22.0 (−47.5 to 3.4)	0.06	0.06
DL _{CO}	−0.2 (−8.6 to 8.2)	−2.9 (−12.2 to 6.4)	0.65	0.64

Definition of abbreviations: CI = confidence interval; DL_{CO} = diffusing capacity of carbon monoxide; ERV = expiratory reserve volume; IC = inspiratory capacity; RV = residual volume; SVC = slow vital capacity.

Values are % predicted mean difference and 95% CI.

*P values shown are for group × visit interaction results from mixed model repeated measures analyses of variance.

†Adjusted P value with body mass index as a covariate in the mixed model repeated measures analysis of variance.

control subjects before and after weight loss). Reactance became less negative in patients with asthma at 5 Hz with weight loss (Figure 2A; $P < 0.01$), with similar tendencies at the other frequencies. Overall, patients with asthma and control subjects responded similarly to weight loss: there was no significant group–visit interaction ($P = 0.68$) for change in reactance with weight loss (log transformation not needed).

Modeling Changes in Respiratory System Impedance

The impedance spectra obtained by fitting the model in Figure 1 to the mean data in Figure 2 are shown in Figure 4. The best-fit model parameter values are shown in Figure 5 along with their estimated standard deviations. The best-fit parameters vary considerably between the groups largely as a result of the vertical shifts in reactance between the groups, which translate into substantial differences in the two elastance parameters in the model. For example, weight loss caused peripheral elastance (E_p in Figure 5) to decrease in subjects with and without asthma. We interpret these changes as reflecting relief from lung compression. That is, a more compressed lung has less parenchymal tissue in communication with the airway opening and thus appears to be stiffer compared with a less compressed lung. A similar picture pertains to central elastance (E_c in Figure 5), and to a lesser extent to peripheral airway resistance (R_p in

Figure 5). The only significant finding in any of these fitted model parameters, however, was the 17% decrease in central airway resistance (R_c in Figure 5) that occurred after weight loss in the control subjects, compared with virtually no change in the patients with asthma. However, if one assumes flow in the central airway to be laminar (22), a 17% decrease in resistance corresponds to a decrease in central airway radius of only 4.5%.

The lack of significant differences in model parameters between the various

groups means that these parameters are quite sensitive to variations in the impedance data. This applies particularly to E_p , which controls the fraction of the imposed flow impulses that are shunted into the central airways. Changes in this fraction can be accommodated by relatively modest variations in E_c . This means that variations in the value of E_p are readily compensated for by changes in E_c , resulting in relatively little effect on how well the model fits the impedance data. We therefore calculated the total elastance of the model,

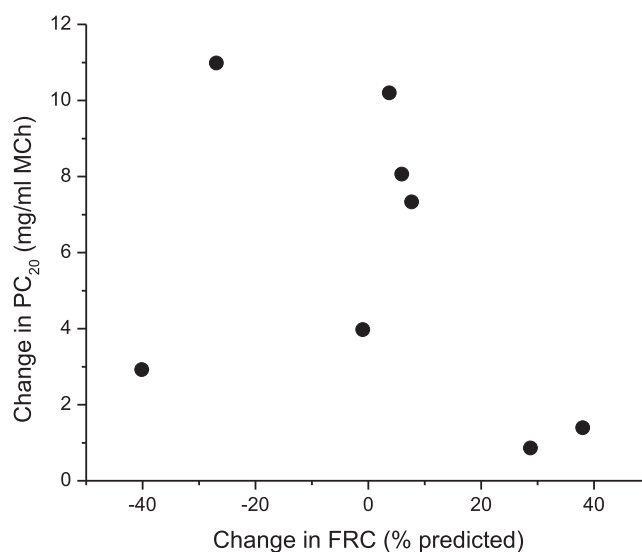


Figure 3. Change in airway reactivity to methacholine (MCh) versus change in FRC with weight loss in subjects with asthma. PC₂₀ = provocative concentration of methacholine causing a 20% drop in FEV₁.

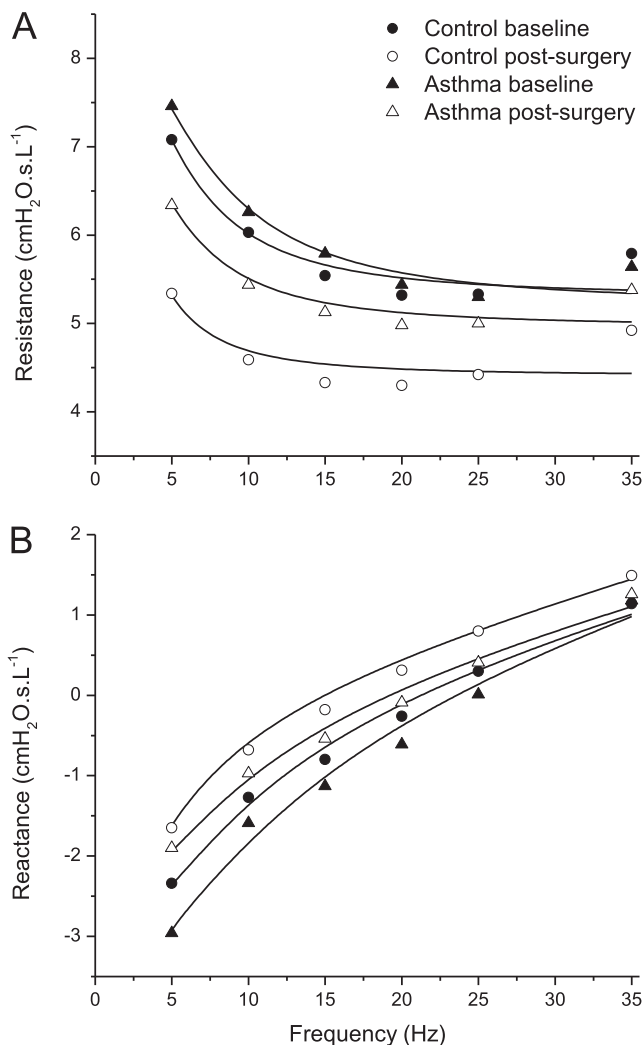


Figure 4. Respiratory system resistance (A) and reactance (B) obtained by fitting the model illustrated in Figure 3 (solid lines) to the means of the experimental measurements (symbols). The best-fit model parameter values are shown in Figure 5.

Etot, as a reflection of the combined effects of E_p and E_c (see online supplement for details of this calculation). In contrast to the individual model parameters, Etot was significantly reduced by weight loss in both control subjects and patients with asthma, and was significantly greater in patients with asthma compared with control subjects before weight loss (Figure 5).

Discussion

The obese patients with asthma and obese control subjects in our study exhibited similar abnormalities in baseline lung function (Table 1), but differing responses to weight loss (Tables 2–4). These differences manifested most clearly as

contrasting changes in respiratory impedance measured during normal breathing (Figure 2). In particular, obese control subjects experienced a parallel shift in both resistance and reactance with weight loss (Figure 2B). In contrast, obese patients with asthma had a significantly different change in resistance (Figure 2A) with weight loss compared with obese control subjects. Our modeling results (Figures 4 and 5) suggest that weight loss led to greater reductions in lung elastance in the patients with asthma, and that the patients with asthma started with greater elastance before weight loss. Etot, which can be taken as a measure of overall lung derecruitment, was significantly elevated in the asthmatic postsurgery group, and was significantly reduced by

weight loss in both groups (Figure 5). Taken together, these modeling results suggest that late-onset obese asthma is characterized by a lung periphery that is abnormally prone to collapse.

We anticipated finding that improvements in airway reactivity in patients with asthma would be related to increasing lung volume, and we initially hypothesized that these effects would be different compared with nonpatients with asthma. Interestingly, although we did find different effects of weight loss on lung volume, it was only in the nonpatients with asthma that FRC and TLC increased significantly with weight loss (Table 2). We also found no relationship between change in methacholine sensitivity and change in lung volume in our subjects (Figure 3), which is curious given that methacholine sensitivity and responsiveness have previously been shown to have a strong inverse dependence on FRC (12, 23). These findings seem to contradict our hypothesis that lung compression is behind the nonallergic form of obese asthma.

However, conventional lung function requires that subjects take a deep breath, which may mask phenomena of interest that arise when subtle changes in lung volume are at play. Accordingly, we also measured respiratory system impedance in our subjects using a method that avoided taking deep breaths. The impedance measurements showed significant differences in the responses to weight loss between patients with asthma and control subjects, but are somewhat difficult to interpret on their own. One possible explanation is differences in bronchodilator tone in patients with asthma with weight loss, but because change in FEV₁ with bronchodilator did not change with weight loss, this is unlikely. Therefore, to help us understand the physiologic significance of these differences in impedance, we invoked a mathematical model of the respiratory system (Figure 1). This model mimics the main frequency-dependent features of both resistance and reactance, particularly in terms of the negative frequency dependence of resistance (Figure 4A) and the vertical shifts in reactance between the various groups (Figure 4B), allowing us to hypothesize that variations in peripheral lung collapsibility are what distinguishes the patients with asthma from the control subjects. Taken together, the effects of surgery on the model parameters shown in Figure 5 lead us to

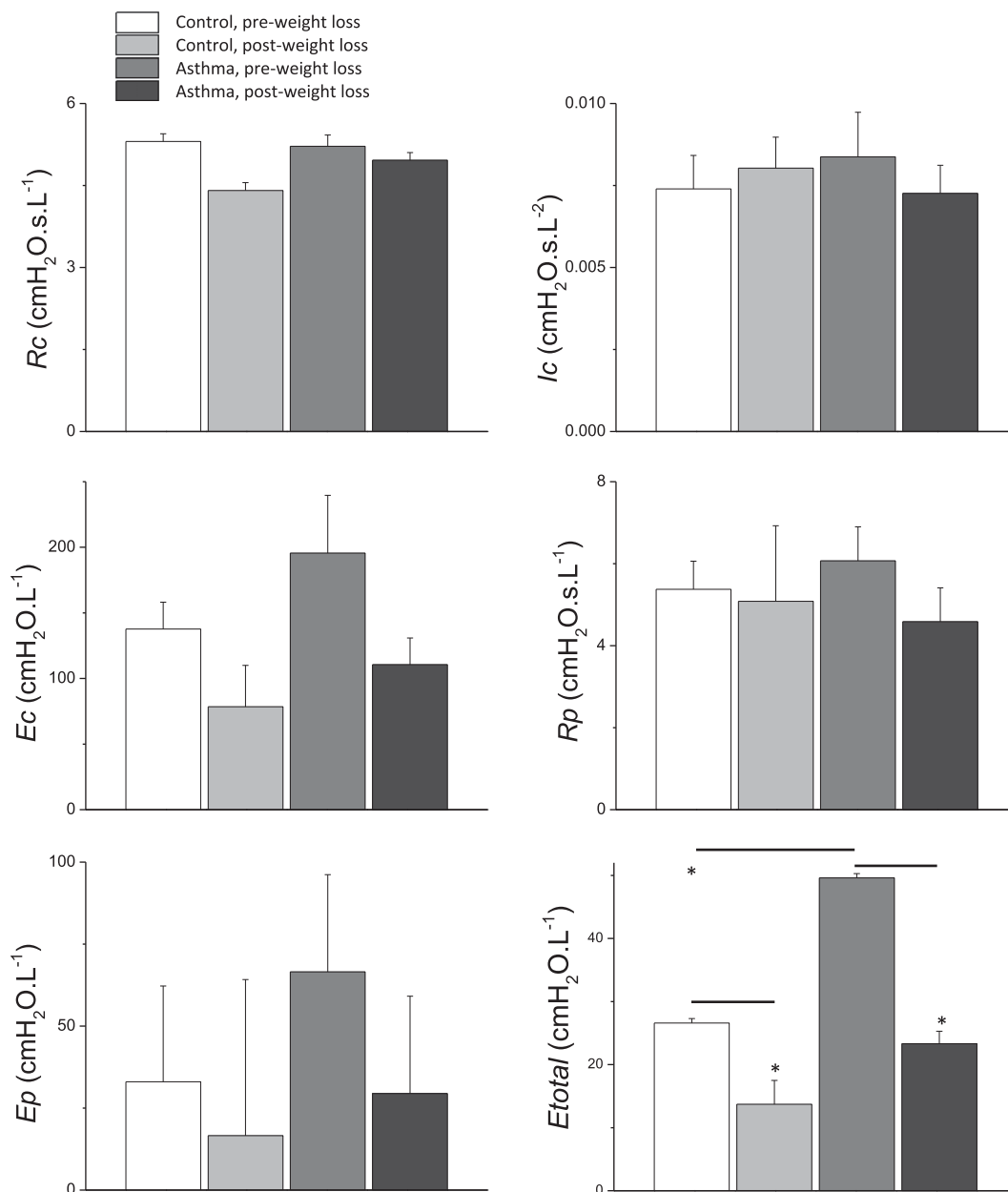


Figure 5. Parameter values determined by fitting the model shown in Figure 1 to the impedance data shown in Figure 2. The model parameter values were obtained by fitting the model to the mean impedance data, whereas the standard deviations shown by the error bars were obtained using a Monte Carlo approach described in the online supplement. The only significant difference among the individual model parameters is R_c in the control group after weight loss, which is different than the other three groups. E_{total} , however, was significantly reduced by weight loss in both the control subjects and the patients with asthma, and was significantly greater in the patients with asthma compared with the control subjects before weight loss ($*P < 0.05$). E_c = central elastance; E_p = peripheral elastance; E_{total} = total elastance; I_c = gas inertance; R_c = central resistance; R_p = peripheral resistance.

hypothesize that the peripheral airways and parenchyma of the asthmatic lungs were more compliant than those of the control lungs, making them more easily collapsed by lung compression. Such differences in collapsibility could have been caused by differences in the intrinsic stiffness of the airway wall. It is possible, therefore, that there exists within the normal population

a range of airway wall stiffness for which lung function is normal when lung volumes are normal, but that the compliant end of this distribution becomes asthmatic when lung volumes are reduced through the effects of obesity.

The previous explanation ascribes the pathogenesis of nonallergic obese asthma purely to the effects of reduced lung volume,

but other possibilities include (1) increased collapsibility of the airways caused by mechanical decoupling from the parenchyma, as can occur either as a result of peribronchial or alveolar fat accumulation (24) or during sleep (25); (2) abnormalities of surfactant function (26) leading to increased alveolar instability and collapse; and (3) the production by adipose

tissue of mediators that may have both direct and indirect effects on the airways (27). These various explanations for nonallergic asthma cannot be distinguished using the data of the present study, but represent an important question that needs to be resolved.

Of course, none of the computational findings shown in Figures 4 and 5 prove that the mechanisms embodied in the model in Figure 1 are actually responsible for the experimental data, because we can never be sure that there is no other model with the same descriptive capability. Probably most at issue in this regard is the role of regional ventilation heterogeneity, such as would be modeled by two or more peripheral compartments acting in parallel, and which has been shown to accompany imposed reductions in lung volume (23). Parallel heterogeneity also increases the negative frequency dependence of resistance, but these effects occurred in our impedance data over the frequency range 5–35 Hz (Figure 2), which means that at least one of the compartments involved must have had a time-constant in the range $1/5-1/35 = 0.029-0.200$ seconds. Such short time-constants are unlikely to arise from peripheral compartments experiencing compressive increases in airway resistance, which would be likely to increase time-constants above the normal value of about 0.2 seconds. Indeed, we have previously found time-constants of several seconds for the asthmatic lung periphery (28). A more likely source for a short time-constant is a high-elastance low-resistance compartment representing central airway stiffness, as in the model in Figure 1. Thus, although we certainly do not claim that parallel ventilation heterogeneity did not exist in our subjects, we believe that the observed frequency dependence of resistance above 5 Hz in these subjects was most likely caused by the effects of the imposed flow impulses being shunted into

the central airways. We must also acknowledge that the model in Figure 1 does not account for every feature of the experimental data. For example, it does not reproduce the increases in resistance above 20 Hz (Figure 2), which probably reflect the effects of tissue inertance that give rise to a resonant peak in resistance around 80 Hz (29), which the model is not able to mimic.

The onset of airway hyperresponsiveness at low lung volumes has been investigated extensively in nonobese subjects (12, 23, 30, 31), and is often explained as being caused by an impaired ability to stretch the airway wall (32). However, although obese individuals do breathe at reduced FRC, they typically have increased tidal volumes and minute ventilations compared with lean individuals (33), and so their airway smooth muscle may actually undergo more deformation during tidal breathing than control subjects. These considerations further support the notion that there is something mechanically different about the lungs of those subjects destined to become asthmatic with obesity, compared with those who remain nonasthmatic. Our hypothesis about increased collapsibility of the asthmatic lungs also potentially explains the curious finding that FRC and TLC did not change after surgery in the patients with asthma (Table 3), whereas they both increased in control subjects (Table 2). That is, more than usually collapsible airways in the patients with asthma might have resulted in persistent derecruitment of peripheral airways even when the compressive influence of excessive adipose tissue was relieved.

Finally, we must be aware of certain limitations of our study that could have impacted the results, quite apart from any assumptions made in the modeling of impedance discussed previously. We did not measure the anatomic site of weight loss, which might have differed between patients with asthma and control subjects. We

measured lung volumes by gas dilution (because not all subjects could fit into the body plethysmograph), so we would not have measured any gas trapped behind closed airways that would otherwise have added to our estimates of total lung volume. Also, the group with asthma remained significantly heavier than the control subjects after surgery (Table 1). It is thus possible that the patients with asthma did not lose enough weight to yield a significant improvement in lung volumes. It is also possible that some of the differences in E_{total} shown in Figure 5 could reflect intergroup differences in BMI. Nevertheless, both groups lost a large amount of weight and the patients with asthma were lighter after surgery than the control subjects were at baseline. Also, the patients with asthma improved significantly in terms of airways responsiveness after surgery, so we are confident that the differences in their behaviors relative to the control subjects do indeed signify the presence of some specific pathophysiologic mechanism related to obesity.

In summary, in the small sample of obese subjects we studied we found that late-onset nonallergic asthma is not purely a consequence of breathing at low lung volumes. However, arguments based on changes in respiratory system impedance with weight loss, and what may happen to lung volumes in the presence of recalcitrant lung derecruitment, lead us to the novel hypothesis that obese patients with asthma are distinguished from obese control subjects by having excessive collapsibility of the lung periphery, perhaps as a consequence of reduced distal airway wall stiffness. Therapies aimed at recruiting the lung, and keeping it recruited, may thus have a place in the management of obese late-onset nonallergic patients with asthma. ■

Author disclosures are available with the text of this article at www.atsjournals.org.

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