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## Amyloid- $\beta$ efflux from the CNS into the plasma

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### Abstract

**Objective**—The aim of this study was to measure the flux of amyloid- $\beta$  (A $\beta$ ) across the human cerebral capillary bed in order to determine if transport into the blood is a significant mechanism of clearance for A $\beta$  produced in the central nervous system (CNS).

**Methods**—Time-matched blood samples were simultaneously collected from a cerebral vein (including the sigmoid sinus, inferior petrosal sinus, and the internal jugular vein), femoral vein, and radial artery of patients undergoing Inferior Petrosal Sinus Sampling (IPSS). For each plasma sample, A $\beta$  concentration was assessed by three assays and the venous to arterial A $\beta$  concentration ratios were determined.

**Results**—A $\beta$  concentration was increased by ~7.5% in venous blood leaving the CNS capillary bed compared to arterial blood, indicating efflux from the CNS into the peripheral blood ( $p < 0.0001$ ). There was no difference in peripheral venous A $\beta$  concentration compared to arterial blood concentration.

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**Interpretation**—Our results are consistent with clearance of CNS-derived A $\beta$  into the venous blood supply with no increase from a peripheral capillary bed. Modeling these results suggests that direct transport of A $\beta$  across the blood-brain barrier accounts for ~25% of A $\beta$  clearance, and reabsorption of cerebrospinal fluid A $\beta$  accounts for ~25% of the total CNS A $\beta$  clearance in humans.

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## INTRODUCTION

Abnormal metabolism of the protein amyloid- $\beta$  (A $\beta$ ) is hypothesized to initiate a pathological cascade leading to Alzheimer's disease (AD). Amyloid plaques, one of the pathologic hallmarks of Alzheimer's disease, are composed primarily of aggregates of A $\beta$ , which is generated by the cleavage of amyloid precursor protein (APP) by beta-secretase and gamma-secretase.<sup>1</sup> A $\beta$  production occurs primarily by neurons in the central nervous system (CNS), but also in peripheral tissues. In autosomal dominant Alzheimer's disease, mutations causing overproduction of A $\beta_{42}$  raise soluble levels and induce aggregation and plaque formation leading to early onset of Alzheimer's disease.<sup>2, 3</sup> Additionally, individuals with Down's syndrome, who have three copies of APP and higher levels of A $\beta$ , all develop AD.<sup>4</sup> Taken together with recent data demonstrating altered clearance of CNS A $\beta_{42}$  in sporadic Alzheimer's disease<sup>5</sup>, the balance between production and clearance of A $\beta$  may contribute to amyloid pathology and the development of AD.

After generation in the brain, soluble A $\beta$  enters the extracellular fluid and can be cleared by a variety of mechanisms including phagocytosis by glia, proteolytic degradation, transport to the cerebrospinal fluid (CSF) with subsequent reabsorption into the venous blood, and direct transport across the blood-brain barrier (BBB) into the venous blood (Figure 1).<sup>6-8</sup> Concentrations of A $\beta$  in the CSF, which is in direct communication with the brain interstitial fluid (ISF), are useful AD biomarkers, with low A $\beta_{42}$  concentrations when amyloid plaque is present.<sup>9</sup> Although transport from the CNS into the venous blood is thought to be a significant mechanism for clearing CNS-derived A $\beta$ <sup>10</sup>, plasma A $\beta$  has not shown utility as an AD biomarker.<sup>11, 12</sup> While clearance of CNS A $\beta$  into the peripheral plasma has been demonstrated in animal models,<sup>13, 14</sup> the contribution of centrally produced A $\beta$  to peripheral blood A $\beta$  concentration in humans is unknown. Additionally, the relative importance of different clearance mechanisms remains unclear.<sup>15</sup>

Removal of A $\beta$  peptides from the brain using immunotherapies such as A $\beta$ -targeted monoclonal antibodies has emerged as a prominent therapeutic strategy.<sup>16, 17</sup> Additionally, mechanistic work on the bidirectional transport of A $\beta$  across the BBB via transporters such as RAGE and LRP has opened up the possibility of modulating A $\beta$  BBB transport as a therapeutic strategy.<sup>10, 18-20</sup> By elucidating the contribution of the various natural mechanisms of A $\beta$  efflux, this work will provide insight into the physiology of A $\beta$  clearance and facilitate the design of improved therapies directed at removing A $\beta$  from the brain.

## SUBJECTS AND METHODS

### Participants

This study recruited patients undergoing venous cerebral blood sampling for medical reasons. All participants were being evaluated for autonomous pituitary microadenomas and were scheduled to undergo Inferior Petrosal Sinus Sampling (IPSS), a procedure requiring moderate sedation, fluoroscopically-guided placement of catheters into the jugular veins and inferior petrosal sinuses bilaterally, and timed sample collection for measurement of ACTH levels.<sup>21</sup> Fourteen participants were enrolled in this study. Three withdrew due to lack of radial artery access, eleven completed the protocol, and ten produced enough sample for analysis. Participants were over 18 years of age (27 – 53 years) and included 1 male and 10 females. Patients were confirmed by medical history review to have no cognitive impairment or diagnosis of dementia. The study was performed with written informed consent of the participants and the approval of the Washington University School of Medicine Institutional Review Board.

### Sample Collection

In order to measure the flux of A $\beta$  across the brain, we used time-matched arterial, peripheral venous, and central venous blood samples. The study protocol involved placement of an arterial line in the radial artery and sampling of blood from the sigmoid sinus and internal jugular bulb, in addition to sampling from routine IPSS locations (common femoral vein and inferior petrosal sinuses) under moderate sedation with IV Fentanyl and Versed (Figure 1). All samples were drawn from catheters. The total volume of blood collected during the study was 144 ml (54 ml for research and 90 ml for clinical) over 20 minutes. The amount of blood drawn for research at was 5 ml at the internal jugular bulb (IJ), 5 ml at the sigmoid sinus (SS), 2 ml  $\times$  3 at the left inferior petrosal sinus (IPSL), 2 ml  $\times$  3 at the right inferior petrosal sinus (IPSR), 5 ml  $\times$  2 and 2 ml  $\times$  3 at the peripheral vein (PV), and 5 ml  $\times$  2 and 2 ml  $\times$  3 at the radial artery. Four sets of samples were drawn before administration of corticotrophin-releasing hormone (CRH) and one set was drawn 10 minutes after administration. At each time point, an arterial, peripheral venous, and central venous sample were simultaneously collected in tubes containing 50  $\mu$ l 0.4 M EDTA and 50  $\mu$ l 1x protease inhibitor cocktail (Roche). Samples were placed immediately on ice, plasma was separated by centrifugation, 10  $\mu$ l <sup>15</sup>N-labeled A $\beta$  internal standard (rPeptide, consisting of 0.01 ng/ $\mu$ l A $\beta$ <sub>40</sub> and 0.001 ng/ $\mu$ l A $\beta$ <sub>42</sub> stored in 4:1 0.1% NH<sub>4</sub>OH:MeCN at –80 °C) was added to a 0.5 ml aliquot of plasma, and aliquots were frozen in polypropylene tubes and stored at –80 °C. Due to low sample volume, patient 7 was not analyzed by IP/MS and patient 1 was not analyzed by xMAP.

### ELISA

The ELISA protocol was run as previously described,<sup>22</sup> with the following modifications: 2.5  $\mu$ g/ml HJ5.1 antibody (anti-A $\beta$ <sub>13–28</sub>) was used to coat Costar 3690 plates and 0.1  $\mu$ g/ml biotinylated 6E10 (anti-A $\beta$ <sub>1–17</sub>, Covance) antibody was used for detection.

## xMAP

A $\beta$ <sub>40</sub> and A $\beta$ <sub>42</sub> isoforms were analyzed in plasma using the INNO-BIA plasma A $\beta$  Forms kit (Innogenetics) according to the manufacturer's instructions. Briefly, A $\beta$ <sub>40</sub> and A $\beta$ <sub>42</sub> were simultaneously identified and quantified using a dual laser flow cytometry based immunoassay. Capture antibodies 21F12 (anti-A $\beta$ <sub>42</sub>) and 2G3 (anti-A $\beta$ <sub>40</sub>) were covalently coupled to separate sets of microsphere beads embedded with different ratios of red dyes. The emission signature following excitation at 635 nm was used to identify the analyte as either A $\beta$ <sub>40</sub> or A $\beta$ <sub>42</sub>. Biotinylated 3D6 was used as the detector antibody. After incubation with phycoerythrine-labeled streptavidin, assays were analyzed using the Luminex 100 IS instrument (Luminex) and mean fluorescence intensity after excitation at 532 nm was used for quantification.

## Immunoprecipitation/Mass Spectrometry (IP/MS)

CNBr-activated Sepharose beads were conjugated to HJ5.1 antibody and pre-cleaned with formic acid. Plasma samples containing 450  $\mu$ l plasma with 9  $\mu$ l <sup>15</sup>N-labeled A $\beta$  internal standard (rPeptide, consisting of 0.01 ng/ $\mu$ l A $\beta$ <sub>40</sub> and 0.001 ng/ $\mu$ l A $\beta$ <sub>42</sub> stored in 4:1 0.1% ammonium hydroxide to acetonitrile at -80 °C) were treated with 2.5  $\mu$ l 1x complete protease inhibitor (Roche), 55  $\mu$ l 5 M urea, 2.5  $\mu$ l 5% Tween-20 in PBS, and 30  $\mu$ l 50% antibody bead slurry in PBS with 0.02% azide. Immunoprecipitation was carried out for 2 hours at 25 °C with end over end rotation. After washing the beads with 0.5 M urea and 25 mM ammonium bicarbonate, samples were eluted with neat formic acid, digested with Lys-C, and desalted using C08 TopTips (Glygen). Samples were dried using a Centriva Concentrator (Labconco), resuspended in 25  $\mu$ l of 10% acetonitrile, 0.1% formic acid in water, and transferred to autosampler vials. Using a 4  $\mu$ l injection volume, samples were run on a nanoACQUITY UPLC system coupled to a Xevo TQ-S mass spectrometer (Waters). Peptides were separated on a reverse-phase column (1.7  $\mu$ m BEH130 C18 100  $\mu$ m  $\times$  100 mm) operated at a flow rate of 500 nl/min with a gradient mixture of solvents and analyzed by targeted mass spectrometry on the mid-domain A $\beta$ <sub>17-28</sub> peptide (LVFFAEDVGSNK).<sup>23</sup> The ratio of endogenous A $\beta$  (<sup>14</sup>N) to <sup>15</sup>N uniformly-labeled internal standard A $\beta$  was calculated using MassLynx V4.1 software and quantified according to a standard curve.

## A $\beta$ Standards Preparation

Recombinant A $\beta$  (rPeptide) was purchased and stored at 0.6 mg/ml in formic acid at -80 °C. Stock A $\beta$  was diluted through a series of buffers before use and standards produced at final concentrations of 1250 pg/ml, 625 pg/ml, 313 pg/ml, 156 pg/ml, 78 pg/ml, and 0 pg/ml. In order to reproduce plasma matrix effects on samples, 50  $\mu$ l preparations of A $\beta$  standards for IP/MS were spiked into 400  $\mu$ l of A $\beta$  depleted plasma. Plasma depletion was performed by immunoprecipitation with HJ5.1 antibody beads and measured to be more than 95% depleted of A $\beta$  by ELISA.

## Statistical Analyses

Venous A $\beta$  concentrations were divided by time-matched arterial A $\beta$  concentrations to calculate the V/A ratio. Data was not normalized and all data points were included in the analysis. Data are presented as mean (95% CI). Venous to arterial A $\beta$  ratios from

experimental sampling locations were compared by unpaired two-tailed t-tests with alpha equal to 0.05. Assays were compared by one-way ANOVA and Bonferroni's multiple comparison test. All statistical analysis was performed using GraphPad Prism version 5.0 for Mac OS X (GraphPad Software).

## RESULTS

Plasma A $\beta$  concentrations were measured by 3 assays: IP/MS, ELISA, and xMAP. xMAP measured the A $\beta_{40}$  and A $\beta_{42}$  isoforms separately, while IP/MS and ELISA targeted a mid-domain peptide common to both isoforms and thus measured total A $\beta$ . Total A $\beta$  measurement by xMAP was taken as the sum of A $\beta_{40}$  and A $\beta_{42}$  isoforms, which compose the majority of A $\beta$ . By IP/MS, the average plasma [A $\beta$ ] was 365 pg/ml (352–377 95% CI). With ELISA, the average plasma [A $\beta$ ] was 173 pg/ml (157–189 95% CI). Using xMAP, the average plasma [A $\beta_{40}$ ] was 201 pg/ml (194–208 95% CI), [A $\beta_{42}$ ] was 41 pg/ml (40–43 95% CI), and total [A $\beta$ ] was 243 pg/ml (235–251 95% CI).

In order to normalize the different A $\beta$  concentrations among the assays, and to compare the arterial-venous concentration differences, the venous/arterial (V/A) ratio was utilized to calculate the change in A $\beta$  concentration across the brain capillary bed. A ratio greater than 1 corresponds to a net increase in [A $\beta$ ] after flow through the capillary bed (brain efflux), a ratio less than 1 corresponds to a net decrease in [A $\beta$ ] (brain influx), and a ratio equal to 1 indicates no net flux.

The mean A $\beta$  concentrations for the different central venous sampling sites were not significantly different by one-way ANOVA for any of the assays used, so due to the limited sample size (n=11), all central venous sampling site V/A ratios (IJ, SS, IPSL, and IPSR) were grouped together and compared to peripheral V/A ratio measurements. The V/A ratios for A $\beta$  by IP/MS and ELISA were 1.087 (1.029 – 1.146 95% CI) and 1.111 (1.033 – 1.188 95% CI) respectively for blood from central veins, indicating efflux from the CNS into the plasma (Figure 2). The A $\beta_{40}$  V/A ratio for central venous samples by xMAP was 1.067 (1.018 to 1.115 95% CI), also indicating efflux from the CNS capillary bed. The A $\beta_{42}$  V/A ratio for central venous samples was 1.031 (0.9928 to 1.070 95% CI), which was not significant, but trended to efflux. In contrast, the A $\beta$  V/A ratio for blood that flowed through a peripheral capillary bed was not different from 1 by any assay (IP/MS 0.969 p=0.13, ELISA 1.045 p=0.25, xMAP $_{40}$  1.003 p=0.92, xMAP $_{42}$  0.9906 p=0.59), indicating no net efflux or influx of peripheral amyloid- $\beta$ .

Despite the differences in baseline A $\beta$  concentration, the V/A ratios were consistent between the IP/MS, ELISA, and xMAP assays with no significant difference in their means (p > 0.05) by Bonferroni's multiple comparison test. Thus, we combined all plasma total A $\beta$  concentration measures to increase the power of the study (Figure 3). The mean V/A ratio for central venous samples was 1.075 (1.046–1.104 95% CI), indicating that flow across the brain capillary bed results in an increase of venous plasma A $\beta$  concentration by 7.5% (4.6–10.4% 95% CI). In contrast, the mean V/A ratio for peripheral venous samples was 1.003 (0.9754–1.030 95% CI).

While the V/A ratio was consistent among the three assays used, the absolute changes in A $\beta$  concentration (V-A) varied with the average plasma A $\beta$  concentration measured by that assay. Assay-dependency of absolute measures of plasma A $\beta$  concentration is widely reported in the literature.<sup>24</sup> Therefore, we utilized the average concentrations by all three assays as estimates for modeling. In this study, the average plasma concentration of total A $\beta$  peptides as measured by IP/MS, ELISA, and xMAP was 264 pg/ml. The average V-A difference across the brain was 13.6 pg/ml. Other values used for modeling are listed in Table 1.

The plasma V-A difference across the brain multiplied by cerebral blood flow rate yields the rate of efflux of A $\beta$  peptides out of the brain.

$$V - A \text{ difference} \times Q_{\text{cerebral}} = 13.6 \text{ pg/ml} \times 715 \text{ ml/min} = 9.7 \text{ ng/min}$$

Based on this approximation, all processes that result in transfer of A $\beta$  peptides from the brain into the central veins sum to a rate of mass transfer of 9.7 ng/min.

### Total turnover of A $\beta$ peptides in the brain

Using stable isotope labeling kinetics (SILK), we recently reported a fractional turnover rate of 0.14 h<sup>-1</sup> for total irreversible loss of soluble A $\beta$  in the CNS of normal controls.<sup>2</sup> This rate multiplied by the pool size of A $\beta$  peptides in the brain yields the rate at which A $\beta$  peptides are removed from the brain.

The average total brain pools of A $\beta_{40}$  and A $\beta_{42}$  in aged normal controls have been measured using formic acid extraction to be 2 pmol/g wet tissue and 2 pmol/g wet tissue respectively.<sup>25</sup> Of these total pools, soluble forms accounted for 50% of A $\beta_{40}$  and 23% of A $\beta_{42}$ .<sup>25</sup> The total combined concentration of soluble A $\beta$  is thus calculated to be 6410 pg/g of wet tissue. This value is in the range of normal water-soluble brain A $\beta$  concentrations reported in the literature.<sup>26</sup> Using the sex-weighted average brain mass for our population of 10 females and 1 male (1211 g)<sup>27</sup> and assuming homogeneity:

$$[A\beta] \times \text{brain mass} = 6410 \text{ pg/g} \times 1211 \text{ g} = 7760 \text{ ng}$$

estimates the soluble A $\beta$  peptide pool size in the normal brain. The turnover rate of A $\beta$  peptides is then:

$$7760 \text{ ng} \times 0.14 \text{ h}^{-1} = 18.1 \text{ ng/min}$$

This is higher than the amount transferred to the cerebral venous blood (9.7 ng/min), suggesting that transport of A $\beta$  across the blood brain barrier and via CSF reabsorption into the venous blood may account for approximately 50% of the total clearance rate.

### Mass transfer by CSF reabsorption

Although CSF was not collected in this study, literature values can be used to estimate the typical contribution of CSF reabsorption to our measured efflux values. At steady state, the rate at which A $\beta$  peptides in the ISF become A $\beta$  peptides in the CSF is balanced by the rate at which A $\beta$  peptides in the CSF are reabsorbed into the venous circulation. The CSF reabsorption rate multiplied by the CSF concentration of A $\beta$  peptides yields the rate of transfer of A $\beta$  peptides from the brain into the blood assuming no accumulation or significant degradation of A $\beta$  in the CSF.<sup>28</sup> Using the same IP/MS technique described in this study, the average CSF total A $\beta$  concentration from twelve normal controls (ages 29 – 72) by IP/MS was measured to be 12.4 ng/ml.<sup>2</sup>

$$[A\beta]_{\text{CSF}} \times \text{CSF reabsorption rate} = 12.4 \text{ ng/ml} \times 0.4 \text{ ml/min} = 5 \text{ ng/min}$$

This indicates that mechanisms of efflux into the venous blood other than CSF reabsorption such as direct transport across the BBB result in a transfer of  $9.7 - 5 = 4.7$  ng/min of A $\beta$  peptides from the brain into the blood. Thus direct transport across the BBB represents ~25% of total CNS A $\beta$  clearance, while CSF reabsorption accounts for ~25% of CNS A $\beta$  clearance.

### Plasma turnover rate

While the rate of human plasma A $\beta$  turnover has not been reported, we utilized our efflux measurement to estimate a minimum plasma A $\beta$  turnover rate at steady state. The plasma pool size can be estimated as the total blood volume times the average measured plasma A $\beta$  concentration.

$$\text{Plasma pool size A}\beta \text{ peptides} = \text{plasma volume} \times \text{plasma concentration of A}\beta \text{ peptides} = 870 \text{ ng}$$

Using this estimate for the plasma pool size of A $\beta$  peptides, the minimum value for the fractional turnover rate of plasma A $\beta$  may then also be estimated.

$$\text{Minimum plasma A}\beta \text{ fractional turnover rate} = \text{Plasma A}\beta \text{ appearance rate} / \text{pool size} = 9.7 \text{ ng/min} / 870 \text{ ng} = 0.67 \text{ h}^{-1}$$

## DISCUSSION

In order to quantify *in vivo* brain transport of A $\beta$  across the BBB in humans, we measured A $\beta$  concentrations in time-matched arterial and venous samples, then calculated the V/A ratio, which indicates the net transport across a capillary bed. To our knowledge, no studies have previously addressed this in humans and these results are likely to be helpful for modeling amyloidosis, risk and causes of AD, and diagnostic and therapeutic approaches for AD.

A major strength of this study is the direct sampling from human cerebral veins and a time-matched artery for direct comparison in paired assay measurements. For arterial measurements, we assumed the A $\beta$  concentration to be uniform in arterial blood due to

mixing and used the radial artery as a surrogate for the blood entering the cerebral capillary bed. Within the heart, deceleration of blood during diastole destabilizes fluid flow inducing intracardiac vortices and transient turbulence.<sup>29</sup> The turbulence serves to mix the blood leaving the heart, resulting in homogeneous arterial blood.<sup>30</sup> Thus, arterial homogeneity is a common assumption in arteriovenous difference studies.<sup>31</sup> As this was a cerebral venous study, we did not have access to both radial and carotid arterial blood to verify this assumption.

Central venous measurements were made using catheterization of veins directly draining the brain. Thus, the V/A ratios calculated from cerebral sampling sites inform how the brain vascular bed changes the blood concentration of A $\beta$ , while V/A ratios calculated from a peripheral venous sampling site serve as a control. While all blood samples were obtained from catheters, we do not anticipate that this sampling method affected the measured A $\beta$  concentrations compared to venous puncture sampling.<sup>32</sup> Additionally, we do not believe that central venous catheterization significantly altered the A $\beta$  measurements by disrupting the BBB as the blood was collected upstream from the tip of the catheter.

While the novel sampling method utilized in this study afforded more accurate measures of CNS to plasma A $\beta$  flux, this data has several potential limitations. Eleven patients undergoing IPSS procedures were recruited for this study in order to access cerebral venous blood for the investigation of brain A $\beta$  clearance mechanisms in young non-AD people. The sample collection procedure limited the ability to recruit patients and obtain samples. The participants were being evaluated for pituitary microadenomas and received CRH during sample collection. The effect of a pituitary microadenoma on brain A $\beta$  flux is unknown. While acute and chronic overexpression of CRH have been shown to increase levels of soluble A $\beta$  and accelerate amyloid pathology in transgenic mouse models of AD,<sup>35, 36</sup> we do not anticipate that the administration of CRH used in this experiment would alter normal brain A $\beta$  flux over the time course of our sample collections (10 minutes). Further, samples collected before and after CRH administration showed no significant change in A $\beta$  levels ( $p=0.81$ ).

In order to overcome assay-related variability, three different assays were used to measure A $\beta$  levels. Both assays measuring total A $\beta$  demonstrated significant efflux from the CNS into the plasma. The fact that A $\beta_{40}$  as measured by xMAP demonstrated clear efflux, while A $\beta_{42}$  did not, may be due to the inherent difficulty in measuring A $\beta_{42}$  levels in plasma, which were 5 fold lower than A $\beta_{40}$ . Another possibility is that A $\beta_{42}$  is less efficiently effluxed out of the CNS. The combined data obtained in this study was consistent with a 7.5% increase in plasma total A $\beta$  concentration caused by net efflux of CNS-derived A $\beta$  into the venous blood. In contrast, the V/A ratio of A $\beta$  measured in the peripheral femoral vein was not significantly different from 1, indicating that there is no net efflux or influx of A $\beta$  across the leg capillary bed. Although the intensive nature of the procedure limited the number of participants, multiple measures and replication by three independent assays provides evidence that there is net A $\beta$  efflux from the brain to the plasma in humans.

Efflux measurements were not consistent between individuals or within individuals over time indicating that the movement of A $\beta$  between the CNS and the periphery may be a



dynamic process. Given the temporal variation in CSF A $\beta$  levels<sup>37</sup> and the large rapid changes in cerebral blood flow that can occur over seconds in response to neural activity,<sup>28, 38</sup> it is not surprising that A $\beta$  efflux from the CNS to the plasma may also be highly variable. Additionally, recent evidence has demonstrated that sleep and anesthesia drive large convective increases in ISF-CSF exchange that facilitate brain metabolite clearance, thus illustrating the dependence of at least one mechanism of CNS efflux on the sleep-wake status of the patient.<sup>39</sup> Given that the patients in this study were conscious during sample collection, the CNS to plasma efflux measured might underestimate the rates of efflux during sleep.

Prior studies have found inconsistent relationships between plasma A $\beta$  levels and AD.<sup>40</sup> Additionally, there is no correlation between A $\beta$  concentrations in matched CSF and plasma samples from patients with Alzheimer's disease<sup>41</sup> or APP transgenic mice.<sup>42</sup> Based on our data, A $\beta$  cleared from the CNS raises plasma concentrations by only 7.5% and this increase can only be observed when measured in central veins before significant dilution and peripheral clearance occurs. Although soluble A $\beta$  is approximately 50 times more concentrated in the brain and CSF than the plasma, the small CSF volume and large plasma volume results in only a small peripheral concentration increase.<sup>43</sup> Thus, despite brain efflux of A $\beta$  into the plasma, plasma A $\beta$  concentrations may not accurately reflect CNS AD pathology due to the effects of dilution and variation in blood A $\beta$  clearance rates.

Brain derived A $\beta$  is cleared from the CNS by several mechanisms including direct transport across the blood-brain-barrier (BBB), movement into the CSF and eventual reabsorption into the venous circulation, and phagocytic and enzymatic degradation within the CNS (Figure 1).<sup>6</sup> Of these four mechanisms for brain A $\beta$  clearance, both transport across the BBB and reabsorption into the venous circulation via CSF would cause an increase in the A $\beta$  concentration of blood leaving the brain compared to blood entering the brain. Additionally, previous work has demonstrated that both of these A $\beta$  transport processes are disrupted in transgenic mouse models of AD.<sup>44</sup>

Because little is known about human A $\beta$  brain to blood transport, we used our data to generate estimates of the relative importance of several clearance mechanisms. Our estimates of total brain amyloid- $\beta$  clearance rates suggest that transport of A $\beta$  to the blood by CSF and direct BBB transport may account for 50% of the total clearance of CNS amyloid- $\beta$ . Of the A $\beta$  cleared from the CNS into the venous blood, we estimate that half is transported directly across the BBB. However, this calculation is dependent on several assumptions regarding CSF reabsorption. CSF A $\beta$  levels measured via lumbar catheter rather than at the point of reabsorption were used for modeling. The existence of a rostrocaudal gradient of A $\beta$  in the CSF is debated. Tarnaris et al. compared A $\beta_{42}$  levels in cisternal and lumbar CSF and found a small rostrocaudal gradient.<sup>45</sup> In contrast, work by the Blennow group utilizing serial sampling measurements of 10 ml CSF did not demonstrate a spinal gradient for A $\beta_{42}$ .<sup>46, 47</sup> Based on these studies, if a gradient does exist from the site of reabsorption to the lumbar sampling site, the effect will likely be small and result in slight underestimation of the CSF clearance by our theoretical calculations. Additionally, this calculation assumes that all of the CSF is reabsorbed into the cerebral venous blood and recent studies suggest that alternative routes via the optic and olfactory nerves, cribiform

plate, nasal submucosa, and cervical lymphatics are significant routes of CSF reabsorption.<sup>48</sup> CSF reabsorption can also occur in the spinal cord, particularly if superior sagittal sinus compliance is decreased.<sup>28</sup> CSF reabsorbed by this route would not contribute to the elevation in A $\beta$  measured in cerebral venous blood. Thus this modeling estimate provides the minimum contribution expected from direct transport across the BBB, which may represent up to 50% of total clearance of CNS A $\beta$ .

These measurements provide the first direct evidence of CNS to plasma A $\beta$  clearance in humans and are important for understanding the physiologic processes regulating A $\beta$  metabolism. Further understanding of brain clearance mechanisms of A $\beta$  will provide insights into Alzheimer's disease and potentially aid in diagnostic and therapeutic development.

## Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

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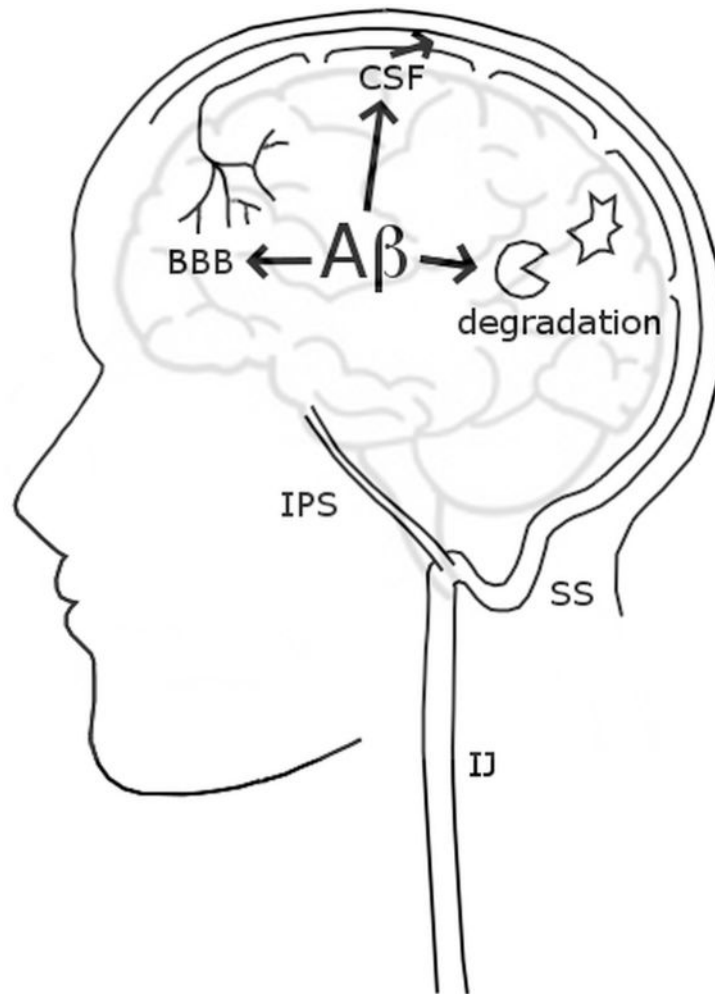
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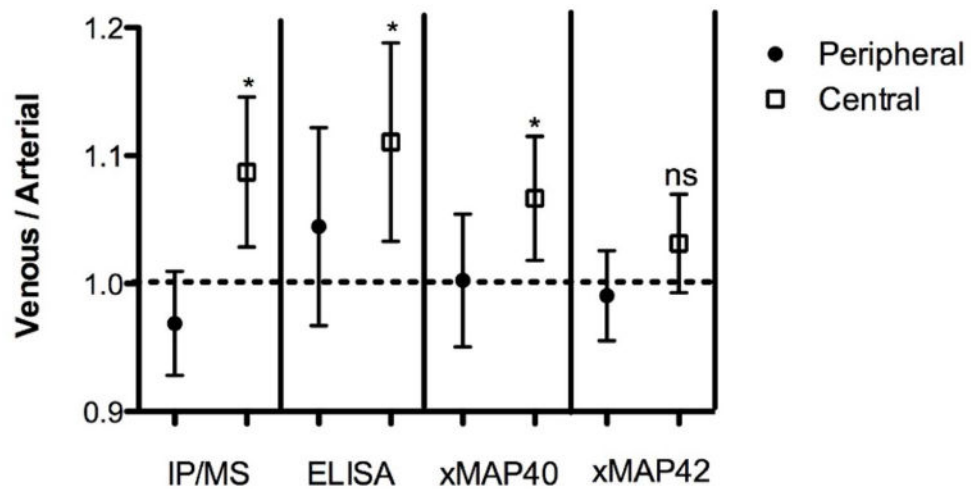
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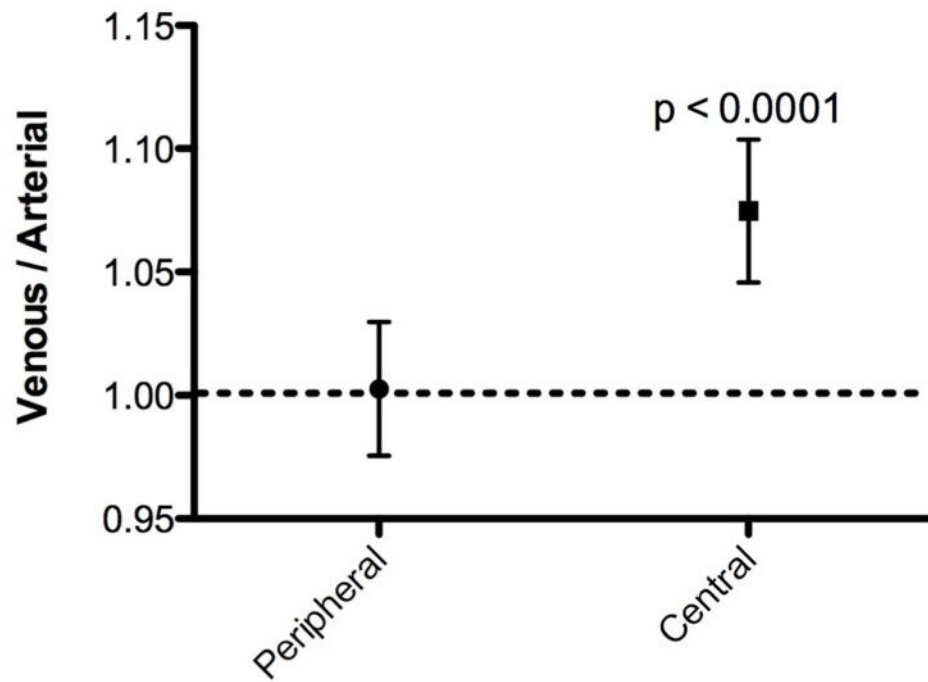


**Figure 1.**

A diagram of the central venous system including sampling sites for central A $\beta$  measurements. CNS A $\beta$  is removed by a variety of mechanisms including direct transport across the BBB into the venous blood, transport to the CSF with subsequent reabsorption into the venous blood, and degradation by phagocytes and enzymes. IPS= Inferior Petrosal Sinus, SS= Sigmoid Sinus, IJ= Internal Jugular



**Figure 2.** Ratios of venous to arterial plasma A $\beta$  concentrations by 3 assays: IP/MS, ELISA, and xMAP. Central indicates veins draining the brain capillary bed and includes measurements from the internal jugular vein (IJ), sigmoid sinus (SS), left inferior petrosal sinus (IPSL), and right inferior petrosal sinus (IPSR). Peripheral represents measurements from the peripheral femoral vein (PV). \* $p < 0.01$ , ns = not significant. Error bars denote 95% confidence intervals.



**Figure 3.** Combined assay results. Central includes measurements from the internal jugular (IJ), sigmoid sinus (SS), left inferior petrosal sinus (IPSL), and right inferior petrosal sinus (IPSR). Peripheral represents measurements from the femoral vein (PV). Error bars denote 95% confidence intervals.



**Table 1**

## Values Used for Modeling

Quantity	Estimate
CSF concentration of A $\beta$ peptides ( $[A\beta]_{CSF}$ )	12.4 ng/ml <sup>2</sup>
CSF reabsorption rate	0.4 ml/min <sup>28</sup>
Cerebral blood flow rate ( $Q_{cerebral}$ )	715 ml/min <sup>28</sup>
Adult plasma volume	3.3 L <sup>49</sup>
Plasma concentration of A $\beta$ peptides	264 pg/ml
V-A difference across the brain	13.6 pg/ml