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Overuse Activity in the Presence of Scapular Dyskinesis Leads to Shoulder Tendon Damage in a Rat Model

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Abstract

Shoulder tendon injuries are common clinical conditions and are a significant source of pain and dysfunction. These conditions are more common in individuals who perform repetitive overhead activities and in individuals who have abnormal scapular kinematics, termed scapular dyskinesis (SD). However, the long term consequences associated with overuse activity in the presence of SD are unknown. Therefore, the objective of this study was to determine the effect of overuse in combination with SD on joint mechanics and properties of the rotator cuff and biceps tendons. A rat model of scapular dyskinesis was used. 90 adult male Sprague-Dawley rats (400–450 grams) were randomized into three groups: nerve transection (SD), sham nerve transection + overuse (OV), or nerve transection + overuse (SD + OV). Rats were sacrificed at 2, 4, and 8 weeks after surgery. Shoulder function and passive joint mechanics were evaluated over time and tendon properties (mechanical, histological, organizational, and compositional) were measured. Results demonstrated that overuse activity and SD are each independently detrimental to tendon properties (e.g., diminished mechanical properties, disorganized collagen). However, tendon damage caused by the addition of overuse may be worse, with more parameters altered, than damage caused by the addition of SD. This study helps define the mechanical mechanisms leading to tendon damage and provides a framework for distinguishing treatment strategies for active patients and those with abnormal scapular mechanics.

Keywords

scapular dyskinesis; animal model; rotator cuff; biceps; overuse injury

Introduction

Shoulder injuries including rotator cuff and biceps tendinitis are widespread and debilitating clinical conditions. These injuries are particularly common in individuals who perform repetitive overhead activities due to their occupation or sport.⁹ Previous studies have

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demonstrated that isolated overuse activity, and overuse activity combined with reduced subacromial space, results in the development of rotator cuff tendinopathy.²³ Overuse activity can lead to chronic tendon injuries characterized by disorganized collagen fibers, increased cellularity, altered cell shape (for example, more rounded), and decreased mechanical properties, indicative of degenerative tissue.²⁴ These changes may be a result of intrinsic or extrinsic mechanisms, such as excessive repetitive strain or mechanical compression of the rotator cuff under the acromial arch (defined as subacromial impingement), respectively.

Individuals who perform repetitive overuse activities (such as athletes and manual laborers) may also develop abnormal shoulder mechanics. Altered scapulothoracic joint kinematics, caused by muscular inhibition, altered neuromuscular control, or fatigue, is common.2, 12, 29, 30 These changes may contribute to joint injury, such as subacromial impingement. Abnormal scapulothoracic joint kinematics, referred to as scapular dyskinesis, may disrupt glenohumeral joint motion, which presents as increased joint translations due to laxity of the static restraints, and possibly predisposing the dynamic stabilizers, such as the rotator cuff and biceps, to injury. Several studies have demonstrated a strong association between scapular dyskinesis and shoulder injuries, such as shoulder impingement and rotator cuff disease;6, 8, 10, 25, 27 however, additional basic science studies are warranted in order to determine this association and identify cause and effect relationships. Identification of scapular dyskinesis as a risk factor for shoulder injury in an active population may help guide the development of prevention programs.

Using an animal model, we have previously demonstrated that scapular dyskinesis can contribute directly to the initiation and progression of rotator cuff and biceps tendon injuries.19 However, the long term consequences associated with overuse activity in the presence of scapular dyskinesis are unknown. The underlying mechanisms and specific relationship by which scapular dyskinesis affects the rotator cuff and biceps can only be elucidated in an animal model where time from injury and post-operative activity levels can be carefully controlled and evaluated over time.

Therefore, the objective of this study was to determine the effect of overuse in combination with scapular dyskinesis on joint mechanics and properties of the rotator cuff and biceps tendon in a rat model. We hypothesized that scapular dyskinesis in combination with repetitive overuse will alter joint function and diminish tendon properties when compared to scapular dyskinesis alone (H1) and when compared to overuse alone (H2).

Methods

Study Design

A rat model of scapular dyskinesis was used¹⁹, in this Institutional Animal Care and Use Committee (IACUC) approved study. Ninety male Sprague-Dawley rats (400–450 g) were randomized into 3 groups: nerve transection (SD, N=30), sham nerve transection + overuse activity (OV, N=30), or nerve transection + overuse activity (SD + OV, N=30). Methods for surgical transection of the accessory and long thoracic nerves were previously published.¹⁹ First, a 2 cm vertical incision was made 1 cm posterior to the ear. The cervical nerve, clavo-

trapezius, and acromiotrapezius muscles were identified. The clavo-trapezius and acromiotrapezius muscles were separated cranial to the cervical nerve to expose the spinal accessory nerve, located above the omotransversarius muscle. The spinal accessory nerve was transected 2 mm and 5 mm proximal to the acromio-trapezius and removed. The site was irrigated with sterile saline and the overlying skin was closed with staples. Next, the animal‧ s forelimb was abducted and internally rotated, and a 3 cm axillary incision was made in the caudal direction along the abdominal fascia, exposing the serratus anterior muscle. Next, the latissimus dorsi muscle was identified, an incision was made along the fascial interface, and a blunt dissection was performed between the latissimus dorsi muscle and serratus anterior to gain proximal exposure to the serratus anterior muscle and long thoracic nerve. The long thoracic nerve was transected 2 mm and 5 mm proximal to the serratus anterior and removed. The site was irrigated with sterile saline, the abdominal fasica was sutured closed with 4-0 Vicryl suture (Ethicon, Inc., Blue Ash, OH), and the overlying skin was then closed with staples. Overuse activity was modeled as stated in our previous publications.^{18, 24} Initially, rats in overuse groups underwent a 2-week treadmill training period to acclimate them to running at the desired speed and for the desired duration. All groups then underwent unilateral surgical transection (or sham transection) of the spinal accessory and long thoracic nerves, resulting in denervation of the trapezius and serratus anterior muscles, respectively. Pre- and post-operative analgesics (buprenorphine, 0.05 mg/kg) were administered up to 2 days following surgery. Animals returned to unrestricted cage activity for 5 days and were then subjected to overuse activity or continued unrestricted cage activity. Overuse activity consisted of treadmill running at 17 m/min on a 10° decline for 1 hour per day 5 days per week. Rats were sacrificed 2, 4, and 8 weeks following surgery and either frozen (for mechanical testing, $N=10$) or fixed in formalin (for histology and immunohistochemistry, $N=5$).

Quantitative Ambulatory Assessment

Forelimb ground reaction forces (medial/lateral, braking, propulsion, and vertical) were quantified using an instrumented walkway, consisting of two 6 degree-of-freedom load/ torque cells.²⁰ Rats were acclimated prior to formal recording of ambulatory data. Data was collected one day prior to surgery (baseline), and at days 5, 7, 14, 28, 42, and 56 days postsurgery. All parameters were normalized to animal body-weight.

Passive Joint Mechanics

Passive shoulder joint range of motion (ROM) and stiffness were quantified using a custom device.²¹ Briefly, the animal was placed under anesthesia and the forearm was secured into a rotating clamp at 90° of elbow flexion and 90° of glenohumeral forward flexion. The scapula was manually stabilized (to isolate glenohumeral motion) and the arm was rotated through the full range of internal and external rotation three times. Range of motion was calculated using the average of the three maximum values for both internal and external rotation. A bilinear fit was applied to calculate joint stiffness in the toe and linear regions for both internal and external rotation. Data was collected one day prior to surgery (baseline), and at days 14, 28, and 56 days post-surgery. All parameters were normalized to baseline values.

Tendon Sample Preparation

Tendon tissue samples were prepared at the time of mechanical testing. 19 Briefly, the animals were thawed and the scapula and humerus were dissected out with the biceps and supraspinatus tendons intact. The tendons were fine dissected under a stereomicroscope to remove surrounding excess tissue. Cross-sectional area of each tendon was measured using a custom laser device.

Tendon Mechanical Testing

Tendon mechanical testing was performed.18 Briefly, stain lines, for local optical strain measurements, were placed on the biceps and supraspinatus tendons, dividing the insertion and mid-substance regions. The scapula and humerus were embedded using polymethymethacrylate (PMMA) and secured in a custom testing fixture. The proximal end of each tendon was gripped with cyanoacrylate annealed sand paper and secured using custom grips. The specimens were immersed in PBS at 37°C during testing. Uniaxial tensile testing was performed with preconditioning (10 cycles from 0.1 N to 0.5 N), stress relaxation (4% strain for biceps and 5% strain for supraspinatus at a rate of 5 %/sec for 600 sec), and ramp to failure (0.3%/sec). Stress (force divided by cross-sectional area) and strain (determined from stain line displacements that were tracked using custom texture tracking software) were calculated and elastic modulus was determined using a linear regression of the linear region of the stress-strain curve. The viscoelastic parameter, percent relaxation, was calculated through analysis of the stress-relaxation curve and determination of the peak and equilibrium loads.

Tendon Histology

Histologic analysis was performed for the biceps and supraspinatus tendons.¹⁹ Briefly, tissues were harvested immediately following sacrifice and processed using standard paraffin procedures. Sagittal sections (7µm) were collected, stained with Hematoxylin–Eosin (H&E), and imaged at the insertion and mid-substance using traditional and polarized light microscopy at 200X and 100X magnifications, respectively. The mid-substance of the biceps was further subdivided into four regions: insertion site (INS), intra-articular space (INTRA), proximal groove (PROX), and distal groove (DIS). 15 Cell density (number of cells/mm²) and cell shape (aspect ratio; 0–1, with 1 being a circle) were quantified in the traditional light images using a bioquantification software system (Bioquant Osteo II; BIOQUANT Image Analysis Corp, Nashville, TN, USA). Polarized light images were analyzed using custom software to evaluate tendon organization.⁵ The angular deviation (AD) of the collagen orientation for each specimen, a measure of the collagen fiber alignment, was calculated in each tendon location.

Tendon Immunohistochemistry

Tissue specimens used for histology were also used to localize ECM proteins using previous immunohistochemical techniques.14, 19 Staining for collagens type II and III, the proteoglycan decorin, and the inflammatory marker, IL1-β was performed and the proteins were visualized using DAB (Table I). Staining results were independently graded by three

blinded investigators, using a scale of $0-3$ (0=undetectable, 1=low, 2= medium, 3=high) and the mode of these values was used as the final specimen score.

Statistical Analysis

For the ambulatory assessment, multiple imputations were conducted using the Markov chain Monte Carlo method for missing data points $(\sim 10\%)$. For both ambulatory assessment and passive joint mechanics, significance was assessed using a 2-way ANOVA with repeated measures on time with follow-up t-tests between groups according to our hypotheses (H1: SD vs. $SD + OV$ and H2: OV vs. $SD + OV$) at each time point. Tissue mechanics and histologic parameters between groups were assessed using a 1-way ANOVA with follow-up t-tests. Immunohistochemistry scores were evaluated using a Kruskal Wallis with follow-up Mann-Whitney tests. Bonferroni corrections were used for multiple comparisons and significance was set at $p<0.05/2=0.025$, trends at $p<0.1/2=0.05$.

Results

Ambulatory Data

Shoulder function was significantly altered in the $SD + OV$ group (Figure 1). Vertical force was significantly decreased in the $SD + OV$ group compared to OV at 5 days, 2 weeks, and 6 weeks, with a similar trend at 8 weeks (Figure 1A). However, vertical force for the SD and SD + OV groups were not different at any time point. Propulsion force was significantly increased in the $SD + OV$ group compared to OV at all time-points (Figure 1B). However, propulsion force for the SD and $SD + OV$ groups were not different at any time point. Braking force was significantly decreased in the $SD + OV$ group compared to OV at 5 days post-injury (Figure 1C). No other differences in braking force were observed between groups. Lastly, medial-lateral force was significantly more medial 1 week post-injury in the SD group compared to the $SD + OV$ group (Figure 1D). No significant differences in spatiotemporal parameters (step width, stride length, or speed) were observed between groups.

Passive Joint Mechanics

Passive joint mechanics were altered in the SD + OV group (Table II). External rotation range of motion was significantly decreased in the SD + OV group compared to the SD group at 2 and 8 weeks post-injury and compared to the OV group 2 weeks post-injury. No other significant differences in passive joint mechanics were observed between groups.

Tendon Mechanics

Mechanical parameters were significantly altered in the $SD + OV$ group (Figures 2, 3, and 4). Tendon percent relaxation was significantly increased in the SD + OV group compared to SD for both the supraspinatus (at 4 and 8 weeks post-injury) and the biceps (at 8 weeks post-injury) (Figure 2). Additionally, supraspinatus tendon insertion modulus was significantly decreased in the $SD + OV$ group compared to SD at 8 weeks post-injury (Figure 3A). However, no differences were observed at the biceps tendon insertion at either time-point (Figure 3B). Supraspinatus and biceps tendon mid-substance modulus were significantly decreased in the $SD + OV$ group compared to the SD group and compared to the OV group at 8 weeks post-injury (Figure 4).

Tendon Histology

Tendon histology was significantly altered in the SD + OV group (S-Table I and Table II). Cell shape at the biceps distal groove was significantly less rounded in the $SD + OV$ group compared to both the SD and OV groups at 4 weeks post-injury (S-Figure 1). Additionally, cell shape at the supraspinatus mid-substance was significantly more rounded in the SD + OV group compared to the SD group at 8 weeks post-injury (S-Figure 2). No other differences in cell shape were observed. Cell density was significantly increased at the supraspinatus insertion in the $SD + OV$ group compared to the OV group at 8 weeks postinjury (S-Figure 3). No other differences in cell density were observed. Tissue organization was also significantly altered in the $SD + OV$ group (Figure 5). Angular deviation was significantly increased (indicative of greater collagen disorganization) at the supraspinatus and biceps insertion at 8 weeks in the $SD + OV$ group compared to the SD group (Figures 5A and 5B). Additionally, angular deviation was significantly increased at the supraspinatus mid-substance at both 4 and 8 weeks and at the biceps proximal groove at 4 weeks in the SD + OV group compared to SD (Figures 5C and 5D).

Tendon Immunohistochemistry

Tendon protein composition was also significantly altered in the $SD + OV$ group (Table III) and Table IV). Collagen II was significantly increased at the proximal groove of the biceps tendon at 4 weeks in the $SD + OV$ group compared to the SD group (Table III). Collagen III was significantly decreased at the biceps insertion at 2 weeks and supraspinatus insertion and mid-substance at 4 weeks in the $SD + OV$ group compared to the SD group. Additionally, collagen III was decreased at the proximal groove of the biceps tendon at 8 weeks in the SD + OV group compared to the OV group, with a similar trend compared to the SD group. Decorin was significantly decreased at the supraspinatus mid-substance at 8 weeks in the $SD + OV$ group compared to the SD group (Table IV). However, decorin was significantly increased at the biceps tendon insertion, with a trend at the intra-articular space, at 4 weeks in the $SD + OV$ group compared to the SD group. No differences in IL1- β were observed.

Discussion

Overhead athletes and manual laborers commonly develop scapular dyskinesis and continue performing overuse activity, potentially placing their shoulders at increased risk of injury. However, the long term consequences of continuing overuse activity in the presence of abnormal scapulothoracic joint kinematics have not been fully elucidated. Using a variety of measurements, results from this study demonstrate that overuse activity in the presence of scapular dyskinesis is detrimental to shoulder properties and that overuse activity alone has a greater effect (more parameters altered) on shoulder properties than scapular dyskinesis alone (Table V). These results suggest that overuse activity in the presence of scapular dyskinesis likely contributes to shoulder injury.

Results of this study demonstrated that overuse activity does not alter joint function (opposite H1) while scapular dyskinesis significantly alters shoulder function (consistent with H2). No differences were observed with the addition of overuse (SD vs. $SD + OV$)

while vertical and braking force decreased and propulsion force increased with scapular dyskinesis (OV vs. $SD + OV$). The altered loading profile placed on the shoulder joint in the presence of scapular dyskinesis may relate to functional deficits and associated pain and could have a significant effect on tendon properties. The changes due to scapular dyskinesis are similar to those previously described.¹⁹ Alternatively, overuse activity did not diminish joint function. Therefore, we can conclude that the mechanical mechanism by which overuse activity alters tendon properties and by which scapular dyskinesis alters tendon properties are distinct.

Passive joint mechanics were significantly altered with the addition of overuse (SD vs. $SD +$ OV). The addition of overuse activity in the $SD + OV$ group resulted in decreased external rotation range of motion compared to SD alone (at two time points) and compared to OV alone (at one time point). Passive motion is often used as a clinical measure of shoulder range of motion and stiffness. Several factors can contribute to shoulder stiffness including tightening of the capsuloligamentous structures and/or surrounding musculature, arthritis, adhesion formation, and inflammation. In this study, we observed decreased external rotation range of motion, indicative of tightening of the anterior structures. The changes observed in this study could be related to increased reliance on the surrounding muscles (such as the subscapularis, pectoralis major, teres major, or the latissimus dorsi) in response to eccentric overuse activity and leading to subsequent tightening.^{16, 31} Alternatively, the addition of scapular dyskinesis in the presence of overuse $(OV \, vs. SD + OV)$ had less of an effect on passive joint mechanics, except at 2 weeks post-injury. The initial insult of scapular dyskinesis may have had a significant effect on the secondary joint stabilizers, such as the joint capsule and surrounding musculature, leading to decreased range of motion. However, as both groups continued repetitive overuse activity, these changes were no longer apparent, suggesting that the effect of overuse may mask any underlying deficits due to scapular dyskinesis.

Consistent with our first hypothesis, overuse activity in the presence of scapular dyskinesis led to compromised tendon properties when compared to scapular dyskinesis alone (SD vs. SD + OV). Tendon percent relaxation was increased for both the supraspinatus and biceps tendons with the addition of overuse, consistent with previous findings for injured tendon.³ Additionally, supraspinatus insertion and mid-substance modulus and biceps mid-substance modulus were significantly diminished. Results for tendon organization support the mechanical changes observed. The supraspinatus and biceps insertion and mid-substance regions were more disorganized with the addition of overuse activity. In healthy tendon, collagen fibers typically align with the axis of loading. Alterations in loading (e.g. shear or compressive) could lead to a more random orientation of collagen fibers and diminish the mechanical integrity of the tendon as observed in this study (decreased viscoelastic and elastic properties). Additionally, the changes in collagen alignment may be related to microtrauma caused by mechanical compression and shear of the tendons due to repetitive excursion of the tendons under the acromion during overuse activity. Histologic changes in the tendon also supported the mechanical changes observed. A more rounded cell shape was observed in the supraspinatus mid-substance, consistent with a tendinopathic condition and likely indicative of altered cellular function (e.g., maintenance, repair, and remodeling of tendon matrix). Alternatively, cell shape was less rounded in the biceps tendon distal

groove, which may indicate increased eccentric stretching and tensile loading in this region, which does not pass under the acromial arch, with overuse.

In order to further elucidate the mechanical changes observed with overuse, protein expression was evaluated. Overuse activity resulted in increased collagen II in the biceps tendon, decreased collagen III in both the supraspinatus and biceps tendons, and decreased and increased decorin in the supraspinatus and biceps. The increased presence of collagen II in tendon may be related to changes in the mechanical loading environment observed by the tendon (such as increased compressive or shear loading), leading to abnormal collagen metabolism and resulting in the subsequent mechanical changes in the tendon at later time points. The reduction in collagen III with overuse is surprising, as the presence of collagen III in tendon has been associated with tendon microtrauma and decreased mechanical strength.^{1, 4} However, in the supraspinatus and biceps, these findings were only observed early (at 4 weeks and 2 weeks, respectively) and were not present later (at 8 weeks). This alteration in collagen III is indicative of abnormal collagen metabolism. The ratio of collagen I to collagen III deposition is important in tendon and the initial decrease in collagen III may be a compensatory strategy to maintain proper coordination and synthesis of the collagen matrix. The increased decorin observed in the biceps tendon at 4 weeks may be related to the tendon's initial response to changes in the mechanical loading environment and is consistent with the increased proteoglycan content observed with tendinopathy.⁷ Additionally, some in vitro studies have suggested that decorin inhibits collagen fibrillogenesis^{17, 28}, which is important for proper tendon function and force transmission. Therefore, the increase in decorin which occurred at 4 weeks post-injury may alter collagen fibrillogenesis, which could explain the mechanical deficits at 8 weeks. The decreased decorin observed in the supraspinatus tendon at 8 weeks is consistent with mechanical changes (increased percent relaxation and decreased modulus) observed at the same time point and with previous studies that have demonstrated downregulation of decorin following tendon injury. $1, 26$

Consistent with our second hypothesis, scapular dyskinesis did further diminish tendon properties (OV vs. SD + OV). Supraspinatus and biceps mid-substance modulus were both diminished with the addition of scapular dyskinesis. However, the tendon changes due to scapular dyskinesis were not as prominent (only one mechanical parameter) as changes due to overuse (several mechanical parameters). Additionally, no differences in organization were observed with the addition of scapular dyskinesis. However, a few changes in histologic parameters (cell shape and cell density) were observed, with less rounded cell shape in the biceps distal groove and increased cell density at the supraspinatus insertion. Changes in protein were also observed with the addition of scapular dyskinesis. Decreased Collagen III was observed in the biceps tendon (OV vs. $SD + OV$), as similarly observed due to overuse. However, consistent with our mechanical and histological findings, immunohistochemical changes due to the addition of scapular dyskinesis were not as prominent as changes due to overuse alone. These findings indicate that overuse activity alone may have a greater effect on tendon properties than scapular dyskinesis alone. Future studies will implement additional biologic assays to quantify mRNA and protein expression in order to further characterize the biologic mechanisms involved in this tendon injury.

Results from this study demonstrate that overuse activity and abnormal scapular mechanics can each independently lead to tendon mechanical damage. However, the effect of overuse activity seems to be more substantial, with more parameters altered, then the effect of abnormal scapular mechanics. It is clear that the loading profile in each of these scenarios is different, as evidenced by differences in kinetic variables, which may explain why the effect on tendon properties is different. Scapular dyskinesis significantly altered joint mechanics while overuse activity did not. However, overuse activity resulted in significantly more structural and biological adaptations (such as decreased range of motion, diminished tendon properties, and altered matrix synthesis) than scapular dyskinesis alone. Overuse activity in the presence of scapular dyskinesis may be a more significant injury due to the extreme physiological demands placed on the joint. Clinically, asymmetric scapular motion is often present in healthy subjects (absent of symptoms), $11, 13$ suggesting that while scapular dyskinesis may be a risk factor, not everyone will develop significant shoulder injuries. Taken together, results from this study suggest that the risk for shoulder injury in patients with scapular dyskinesis may be higher in an active population.

This study has several limitations. First, we acknowledge that the use of an animal model does not exactly replicate the human condition. However, the rat shoulder has been wellestablished as an appropriate model for rotator cuff disease and the rat rotator cuff model has been cited over 200 times.²² Additionally, this model has been shown to reproducibly develop tendinopathy following repetitive overuse activity.²⁴ Second, acute transection of the spinal accessory and long thoracic nerves to induce scapular dyskinesis does not exactly mimic the clinical scenario. However, this model successfully and consistently creates scapular dyskinesis. The cause and effect relationships addressed in this clinical scenario can only be studied in an animal model where time from injury and activity level can be controlled and tissues rigorously evaluated. Despite these limitations, results clearly and consistently demonstrate that overuse activity and scapular dyskinesis are detrimental to shoulder tendon properties.

Identification of overuse activity as a risk factor for shoulder injury in individuals with scapular dyskinesis will help inform and guide clinicians in developing prevention and treatment programs. Specifically, activity levels of athletes and laborers could be monitored in order to prevent permanent shoulder injury. Additionally, early detection and intervention programs can be developed, such as preventative neuromuscular training and scapular movement screens, which could assist in prevention of further detrimental changes due to scapular dyskinesis.

Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

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Figure 1.

(A) The SD + OV group had decreased vertical force compared to OV at most time-points (except 1 and 4 weeks following injury). (B) The SD + OV group had increased propulsion force compared to OV at all time-points. (C) The $SD + OV$ group had decreased braking force compared to OV 5 days following injury. (D) No difference in medial/lateral force was observed. Data is shown as mean \pm standard deviation (p<0.025 (OV vs. SD + OV**), $p<0.05$ (OV vs. $SD + OV^{++}$, SD vs. $SD + OV^{+})$).

Figure 2.

(A) The supraspinatus tendon demonstrated increased percent relaxation at 4 and 8 weeks post-injury in the SD + OV group compared to SD. (B) The biceps tendon demonstrated increased percent relaxation at 8 weeks post-injury in the SD + OV group compared to SD. Data is shown as mean and standard deviation (p<0.025 (SD vs. $SD + OV^*)$).

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Figure 3.

(A) Supraspinatus insertion modulus was decreased at 8 weeks post-injury in the SD + OV group compared to SD. (B) No differences in biceps tendon insertion modulus was observed. Data is shown as mean and standard deviation ($p<0.025$ (SD vs. SD + OV*)).

Figure 4.

(A) Supraspinatus mid-substance modulus was decreased at 8 weeks post-injury in the SD + OV group compared to SD and compared to OV. (B) Biceps mid-substance modulus was decreased at 8 weeks post-injury in the SD + OV group compared to SD and compared to OV. Data is shown as mean and standard deviation ($p<0.025$ (SD vs. SD + OV*, OV vs. SD $+$ OV**)).

Figure 5.

(A) Supraspinatus insertion angular deviation was increased at 8 weeks post-injury in the SD + OV group compared to SD. (B) Biceps insertion angular deviation was increased at 8 weeks post-injury in the SD + OV group compared to SD. (C) Supraspinatus mid-substance angular deviation was increased at 4 and 8 weeks post-injury in the $SD + OV$ group compared to SD. (D) Biceps proximal groove (PROX) angular deviation was increased at 4

weeks in the SD + OV group compared to SD. Data is shown as mean and standard deviation (p<0.025 (SD vs. $SD + OV^*)$).

Table I

Primary an tibodies used for immunohistochemical staining Primary an tibodies used for immunohistochemical staining

Passive Joint Mechanics Passive Joint Mechanics

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Results for passive joint mechanics demonstrated decreased external range of motion (ROM) in the SD + OV group compared to the SD group at 2 and 8 weeks and compared to the OV group at 2 weeks. Results for passive joint mechanics demonstrated decreased external range of motion (ROM) in the SD + OV group compared to the SD group at 2 and 8 weeks and compared to the OV group at 2 weeks.
Data is shown as normalized Data is shown as normalized by baseline values (change from baseline) and as mean ± standard deviation (p<0.025 (SD vs. SD + OV*, OV vs. SD + OV**)).

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Table III

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At 4 weeks, collagen II staining was increased at the biceps proximal groove (PROX) in the SD + OV group compared to SD. Collagen III staining was decreased at the supraspinatus insertion (INS) and mid-substance (MID) in At 4 weeks, collagen II staining was increased at the biceps proximal groove (PROX) in the SD + OV group compared to SD. Collagen III staining was decreased at the supraspinatus insertion (INS) and mid-substance (MID) in the SD + OV group compared to SD. At 8 weeks, collagen III staining was decreased at the biceps proximal groove in the SD + OV group compared to OV, with a similar trend compared to SD. Data is shown as median and interquartile range (p<0.025, (SD vs. SD + OV*), (OV vs. SD + OV^{**)}, p<0.05 (SD vs. SD-+OV⁺)). compared to SD. Data is shown as median and interquartile range (p<0.025, (SD vs. SD + OV*), (OV vs. SD + OV^{**}), p<0.05 (SD vs. SD+OV⁺).

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Table IV

Tendon Immunohistochemistry (Decorin and $IL1-\beta$) Tendon Immunohistochemistry (Decorin and IL1-β)

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At 4 weeks, decorin staining was increased at the biceps insertion, with a similar trend at the intra-articular space (INTRA), in the SD + OV group compared to SD. At 8 weeks, decorin staining was decreased at the suprasp decreased at the supraspinatus mid-substance in the SD + OV group compared to SD. No differences in IL1-β were observed. Data is shown as median and interquartile range (p<0.025, (SD vs. SD + OV*), At 4 weeks, decorin staining was increased at the biceps insertion, with a similar trend at the intra-articular space (INTRA), in the SD + OV group compared to SD. At 8 weeks, decorin staining was (OV vs. SD + OV**), p<0.05 (SD vs. SD+OV⁺)). (OV vs. $SD + OV^{**}$), p<0.05 (SD vs. $SD + OV^{+}$)).

Table V

Results Summary

Comparison of all parameters between groups (SD=scapular dyskinesis, NS=no significance, S=supraspinatus, B=biceps)