



Published in final edited form as:

Int J Radiat Oncol Biol Phys. 2015 June 1; 92(2): 423–429. doi:10.1016/j.ijrobp.2015.01.019.

Clinical validation of 4DCT-ventilation with pulmonary function test data

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Abstract

Purpose—A new form of functional imaging has been proposed in the form of 4DCT-ventilation. Because 4DCTs are acquired as part of routine care for lung cancer patients, calculating ventilation maps from 4DCTs provides spatial lung function information without added dosimetric or monetary cost to the patient. Before 4DCT-ventilation is implemented it needs to be clinically validated. Pulmonary function tests (PFTs) provide a clinically established way of evaluating lung function. The purpose of our work was to perform a clinical validation by comparing 4DCT-ventilation metrics with PFT data.

Methods and Materials—Ninety-eight lung cancer patients with pre-treatment 4DCT and PFT data were included in the study. PFT metrics used to diagnose obstructive lung disease were recorded: forced expiratory volume in 1 second (FEV1) and FEV1/forced vital capacity (FEV1/FVC). 4DCT data sets and spatial registration were used to compute 4DCT-ventilation images using a density-change based and a Jacobian-based model. The ventilation maps were reduced to single metrics intended to reflect the degree of ventilation obstruction. Specifically, we computed the coefficient of variation (CoV) (standard deviation/mean), ventilation V20 (volume of lung 20% ventilation), and correlated the ventilation metrics with PFT data. Regression analysis was

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Conflict of interest: This work was partially funded by:

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used to determine whether 4DCT-ventilation data could predict for normal versus abnormal lung function using PFT thresholds.

Results—Correlation coefficients comparing 4DCT-ventilation to PFT data ranged from 0.63–0.72 with the best agreement between FEV1 and CoV. 4DCT-ventilation metrics were able to significantly delineate between clinically normal versus abnormal PFT results.

Conclusions—Validation of 4DCT-ventilation with clinically relevant metrics is essential. We demonstrate good global agreement between PFTs and 4DCT-ventilation, indicating that 4DCT ventilation provides a reliable assessment of lung function. 4DCT-ventilation enables exciting opportunities to assess lung function and create functional avoidance radiotherapy plans. The current work presents supporting evidence for the integration of 4DCT-ventilation into clinical trials.

Introduction

A new and exciting form of lung functional imaging has been proposed that uses 4-dimensional computed tomography (4DCT) (1, 2) data to calculate ventilation maps (3–7). Because 4DCTs are acquired as part of routine clinical care for lung cancer patients, calculating ventilation maps from 4DCTs provides clinicians the ability to evaluate spatial lung function without the added dosimetric or monetary cost to the patient. 4DCT-ventilation also has attractive imaging characteristics including good spatial resolution (compared to nuclear medicine ventilation) and by definition 4DCT-ventilation provides both anatomical information (from the 4DCT) and functional information (from the 4DCT-ventilation) in one scan. Several authors have proposed potential clinical uses for 4DCT-ventilation (5, 8–14). Yamamoto et al and others (11, 14) proposed using 4DCT-ventilation for functional avoidance radiotherapy treatment planning. The hypothesis is that by avoiding the more functional portions of the lung (as defined by the 4DCT-ventilation), the rate of thoracic clinical toxicity could be reduced for lung cancer patients. _____ tested the ability of dose and dose-function to predict clinical radiation pneumonitis and found that 4DCT-ventilation can improve prediction of clinical toxicity. 4DCT-ventilation has been used to assess changes in lung function throughout (8) and after (13) radiotherapy. Outside of the scope of oncology, several authors have also shown the ability of 4DCT-ventilation to detect non-oncologic lung conditions such as emphysema and chronic obstructive pulmonary disease (COPD) (12, 15).

4DCT-ventilation must be properly validated before being put into clinical practice. Studies have attempted to validate 4DCT-ventilation by comparing it against other ventilation imaging modalities such as nuclear medicine ventilation-perfusion (VQ) imaging (16–18), xenon-CT (6, 19), positron emission tomography (20), and magnetic resonance imaging (21). The studies generally found good agreement on a global level with worsening results locally. Although the validation studies have provided promising results, more work is needed to demonstrate that 4DCT-ventilation is able to reliably depict patient lung function information.

Pulmonary function tests (PFTs) are routinely used by pulmonologists and provide an established way of evaluating lung function (22). In oncology, surgeons use PFTs to assess

whether patients will be able to withstand lung surgery (23) and radiation oncologists can use PFTs to evaluate patients with poor lung function prior to radiation therapy (24). In this work we propose to use PFTs to further clinically validate 4DCT-ventilation in a large lung cancer patient dataset. The purpose of our work was to retrospectively compare 4DCT-ventilation with PFT data in 98 lung cancer patients.

Methods and Material

Patient population

Ninety-eight lung cancer patients from _____ were used for the study. Patients were chosen retrospectively and included if they had 4DCT simulation and PFTs acquired prior to radiation treatment and within 100 days of each other. Patients were excluded if they had any thoracic interventions (surgery, chemotherapy, or radiation) between the 4DCT and PFT acquisitions. Patient and clinical characteristics are shown in Table 1. Patients with disease stages I–IV were included in the study which provided a patient database with a wide array of PFT lung function results. Of the 98 patients, 28 (29%) had pre-existing COPD.

PFT data

PFTs use spirometry to measure air flow and are an established way of measuring lung function. Patients with poor PFT results have been shown to have clinically significant lung function deterioration and more respiratory complaints (25). Pulmonologists routinely use PFTs to diagnose lung disease such as asthma and COPD. Standard PFT metrics used to diagnose obstructive lung disease were recorded (22). For each patient we noted the Forced Expiratory Volume in 1 second (FEV1) and the ratio of the FEV1 and the Forced Vital Capacity (FEV1/FVC). PFT metrics were reported as percentage of predicted value which is based on healthy subjects with the same anthropomorphic characteristics (height, age, gender, and others) as the patient being tested (22). Generally, lower PFT metrics indicate worse lung function. In addition to evaluating the raw PFT data we separated the data into 2 groups (normal and abnormal lung function) and performed a binary analysis. Due to the uncertainties in spirometry testing pulmonologists often delineate normal versus abnormal lung function using a PFT threshold, rather than interpreting PFT data as a continuous variable. A PFT value of 70% (26) is a commonly used threshold to separate normal versus abnormal results. To mimic the pulmonologist's binary interpretation of PFT results, we used a 70% threshold of FEV1 and FEV/FVC to delineate normal versus abnormal lung function for the binary analysis.

4DCT-ventilation

The patient's pre-treatment simulation 4DCT scan was used to calculate 4DCT-ventilation images. The 4DCT scans were acquired either on a Brilliance Big Bore scanner (Phillips Healthcare, Andover, MA) using a bellows belt to track breathing motion or a Discovery PET/CT (GE Healthcare, Waukesha, WI) system with a Varian RPM to track breathing motion. The lungs were then segmented on the inhale and exhale phases of the breathing cycle (7). As part of the segmentation any voxel with a Hounsfield Unit (HU) greater than -250 was excluded. A deformable registration algorithm based on compressible flow that

was previously presented (27) was used to map lung voxel elements from inhale to exhale. The accuracy of the registration was shown to be 1.25 mm in the lung (27). 4DCT-ventilation was calculated using the HU-based model (3, 4, 8) and the Jacobian model (5, 6, 13). The HU (3, 4, 8) model uses the following equation to calculate ventilation

$$\frac{V_{in}-V_{ex}}{V_{ex}}=1000\frac{HU_{in}-HU_{ex}}{HU_{ex}(1000+HU_{in})}, \text{ Equation 1}$$

where V_{in} and V_{ex} are the inhale and exhale volumes and HU_{in} and HU_{ex} are the inhale and exhale Hounsfield units of the individual lung voxels. Applying Equation 1 on a voxel-by-voxel basis produces a 3D spatial map of ventilation function throughout the lung (Figure 1). Smoothing was applied to produce final ventilation voxel sizes of $9\times 9\times 3$ mm³. The HU model is derived from the idea that CT numbers are composed of a linear combination of water-like material and air-like material (3,4). The Jacobian-based ventilation was calculation by directly taking the Jacobian of the deformable registration results (5, 6, 13) and is based on the idea that local partial derivatives are related to the volume change of a given voxel. For each patient we manually reviewed the 4DCT scans for image artifacts and the deformation fields for anomalies and discontinuities. Review of the registration entailed overlaying the deformation vectors over the CT image and qualitatively evaluating whether the voxel movement was consistent with expected respiratory patterns and whether the magnitude and direction of any registration vectors significantly deviated from the patterns of the surrounding voxels. Six patients had to be excluded due to image artifacts (lung cut-off or volume averaging artifacts) and no patients had to be excluded due to their deformation fields.

In order to compare the 4DCT-ventilation to PFT metrics, the 4DCT-ventilation images had to be reduced to single descriptive metrics. We derived single metrics from the 4DCT-ventilation that were intended to reflect the degree of ventilation obstruction and heterogeneity of the ventilation image. We computed the coefficient of variation (CoV) defined as the ratio of the standard deviation and the mean (20), the percentage of lung with 20% ventilation or less (V20) (15, 18), and an observer based binary metric of whether a ventilation defect was present or not. Larger CoV and V20 values indicated a more heterogeneous ventilation image and consequently worsening lung function. The observation of defect presence was done using consensus between 2 observers. Each observer reviewed cases independently using the 4DCT-ventilation image overlaid with the CT. Cases where the observers independently disagreed were discussed to produce a consensus observation of defect presence or absence.

The 4DCT-ventilation derived metrics (CoV, V20) were compared to the PFT metrics (FEV1, FEV1/FVC) using correlation coefficients and linear regression analysis. Two separate binary end-point analyses were performed. First, PFT metrics were compared among the group of patients with and without noted ventilation defects using t-tests (significance set at 0.05). Finally, we used logistic regression analysis to determine whether normal versus abnormal lung function (as defined by a PFT threshold of 70%) could be

predicted using the 4DCT-ventilation and performed receiver operator characteristic (ROC) analysis to test model fit with area under the curve (AUC) metrics.

Results

A representative patient example is shown in Figure 1. The 4DCT-ventilation image, 4DCT-ventilation derived heterogeneity metrics, and the PFT data all indicate poor patient lung function. The 4DCT-ventilation image shows major ventilation defects in both lungs, the CoV indicates that the standard deviation of the image is nearly as large as the mean (indicating greater image heterogeneity), and the FEV1 is 36% of what is expected for that patient; all indications of poor lung function status.

The correlation of the 4DCT-ventilation derived metrics (CoV and V20) and the PFT metrics (FEV1, FEV1/FVC) were on the order of 0.7 for the HU method (Table 2). The lowest correlation occurred between the V20 and FEV1 (correlation=0.63, $p<0.01$) and the highest correlation occurred between the CoV and FEV1 (correlation=0.72, $p<0.01$). Correlation for the Jacobian-based ventilation metrics were on the order of 0.4 with the best correlation between FEV1/FVC and V20 (correlation=0.46, $p<0.01$). The scatter plot comparing the FEV1 as a function of the 4DCT-ventilation derived CoV shows that as the CoV decreases (lung function gets worse) the FEV1 congruently indicates worsening lung function (Figure 2).

The patients were grouped according to whether they had observed ventilation defects and the PFT values of the 2 groups were compared (Table 3). The group that had no observed ventilation defects had a mean FEV1 of 70.8 while the group that had ventilation defects had a significantly ($p=0.034$) worse FEV1 mean value of 60.3.

A threshold value of 70% was used for the PFT data to delineate normal versus abnormal lung function and the average ventilation-based CoV and V20 values were compared between the 2 groups. All comparisons produced statistically significant differences in ventilation-derived metrics (for both HU and Jacobian methods) for the normal versus abnormal groups. As an example, the average CoV value for the poor lung function group (FEV/FVC < 70%) was 0.83, while the average for the normal lung function group (FEV1/FVC > 70%) was 0.53 with the difference being significant ($p<0.01$). Similarly the FEV1/FVC differences between the groups with and without ventilation defects approached statistically significant differences ($p=0.086$). The sigmoid model fit converged (Figure 3) with a statistically significant fit ($p<0.01$) indicating the ability of the CoV to delineate between normal versus abnormal lung function. Model fit between the ventilation and PFT metrics was assessed using ROC analysis. The AUC values assessing model fit ranged from 0.81–0.86 for the HU based ventilation metrics and were 0.64–0.72 for the Jacobian based metrics (Table 2).

Discussion

The patient example (Figure 1), correlation coefficients on the order of 0.7, AUC values on the order of 0.8, and scatter plot (Figure 2) all indicate good overall agreement between 4DCT-ventilation and PFT data. In general, HU-based ventilation metrics produced better

lung function. Most suggested uses of 4DCT-ventilation propose to use 4DCT-ventilation for inpatient comparisons but the work presented here suggests that certain 4DCT-ventilation metrics can be used to compare lung function among different patients.

Although PFTs present a single metric (rather than a 3D spatial map) and have their own shortcomings, they are currently an established gold standard of evaluating lung function. Clinical applications of 4DCT-ventilation such as radiotherapy functional avoidance and lung function assessment are based on the idea that 4DCT-ventilation provides clinically meaningful lung function information (5, 8, 9, 11, 12, 14) and this work along with others suggests that 4DCT-ventilation is able to provide an accurate assessment of lung function.

Because the data were collected retrospectively the PFTs and 4DCTs were generally collected at different time points. Patient breathing effort was also different between PFT and 4DCT data collection. PFT data collections are taken with the patient in forced breathing states while 4DCT data is generally taken under free breathing or abdominal compression conditions. In future prospective studies, correcting for patient breathing effort could improve correlation between the 2 methods of assessing lung function. There were uncertainties in both the PFT and 4DCT-ventilation data. PFTs are subject to uncertainties due to patient effort and co-operation, determination of reference values, and test interpretation. 4DCT-ventilation calculations are still subject to uncertainties due to the quality of the 4DCT (29) and the deformation algorithm (30), differences in the calculation metrics used (7), and reproducibility of the imaging (31, 32). An attempt was made to mitigate the uncertainties of the 4DCT-ventilation by reviewing all 4DCTs, deformations, and 4DCT-ventilation images. One of the challenges of the proposed work was to convert 3D ventilation images into single metrics. We chose 4DCT-ventilation metrics that we deemed clinically meaningful and metrics that were previously proposed (15, 18). However, the used metrics can have their shortcomings. For example, with certain thoracic conditions homogenous ventilation may not necessarily equate to normal patient lung function. Evaluating lung function can be complex and in some cases multiple evaluation tools (PFTs, imaging, clinical interpretation) may be needed for a full characterization. Another uncertainty lies in the observer reading of 4DCT-ventilation images. There are currently no established guidelines for the interpretation of 4DCT-ventilation and future work needs to be performed to establish quantitative and qualitative criteria for evaluation. In addition to V20, CoV, and defect presence, we analyzed the ipsilateral to contralateral ratio and minimum ventilation in each lung third which did not produce any meaningful correlations. Future development of 4DCT-ventilation metrics, including novel normalization strategies, is needed. We believe with continually improving 4DCT-ventilation techniques and refinement of 4DCT-ventilation derived metrics the accuracy in predicting lung function will only improve.

Conclusion

The current work attempted to validate 4DCT-ventilation by comparing 4DCT-ventilation derived metrics of lung function with PFT data. We found fairly good correlation coefficients on the order of 0.7 comparing 4DCT-ventilation to PFTs. 4DCT-ventilation metrics were able to delineate between normal versus abnormal lung function patients as

defined by PFT thresholds (AUC values on the order of 0.8). PFTs provide an established way of measuring lung function and our validation data suggest that 4DCT-ventilation can provide an accurate assessment of lung function. 4DCT-ventilation enables exciting opportunities to assess lung function and create functional avoidance radiotherapy plans for lung cancer patients. The current work presents important supporting evidence towards thoracic clinical trial assessment of 4DCT-ventilation.

Acknowledgments

National Institutes of Health through an NIH Director's New Innovator Award DP2OD007044 (EC, RC, TG)

National Institutes of Health Research Scientist Development Award K01-CA181292 (RC)

State of Colorado Advanced Industries Accelerator Grant (YV)

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Summary

An exciting form of lung functional imaging has been proposed that uses 4DCT data to calculate ventilation maps. The purpose of our work was to validate 4DCT-ventilation by comparing it to pulmonary function test data (PFT). We found good agreement between 4DCT-ventilation derived metrics of lung function and PFT data. Our results suggest that 4DCT-ventilation can provide an accurate assessment of lung function, supporting the design of 4DCT-ventilation clinical trials.

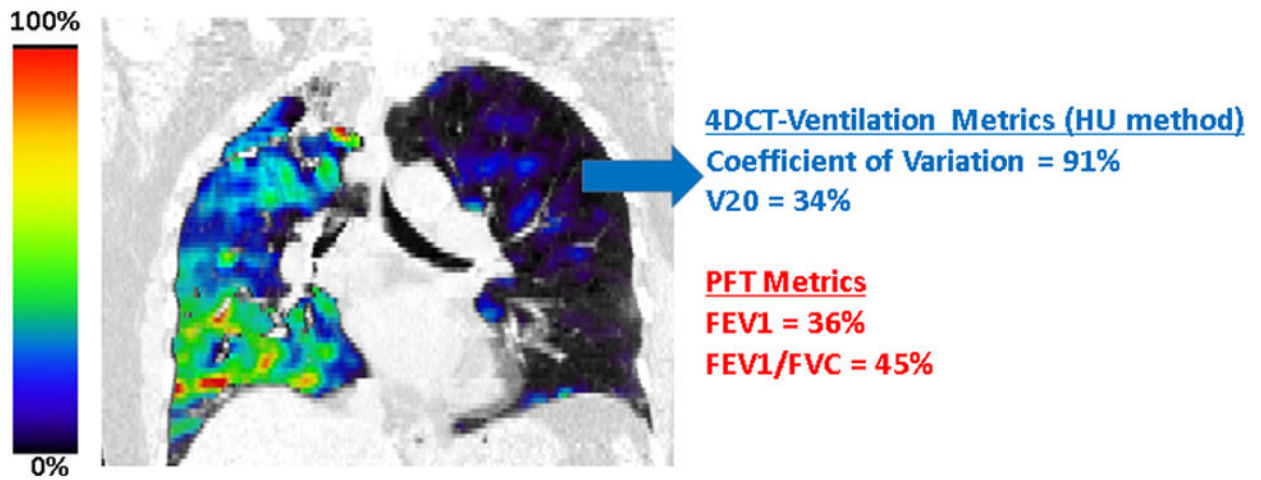


Figure 1.

A representative example of a patient with poor lung function. The ventilation defects in the 4DCT-ventilation image, 4DCT-ventilation derived metrics (using the HU method), and PFT data all indicate poor lung function for the presented patient.

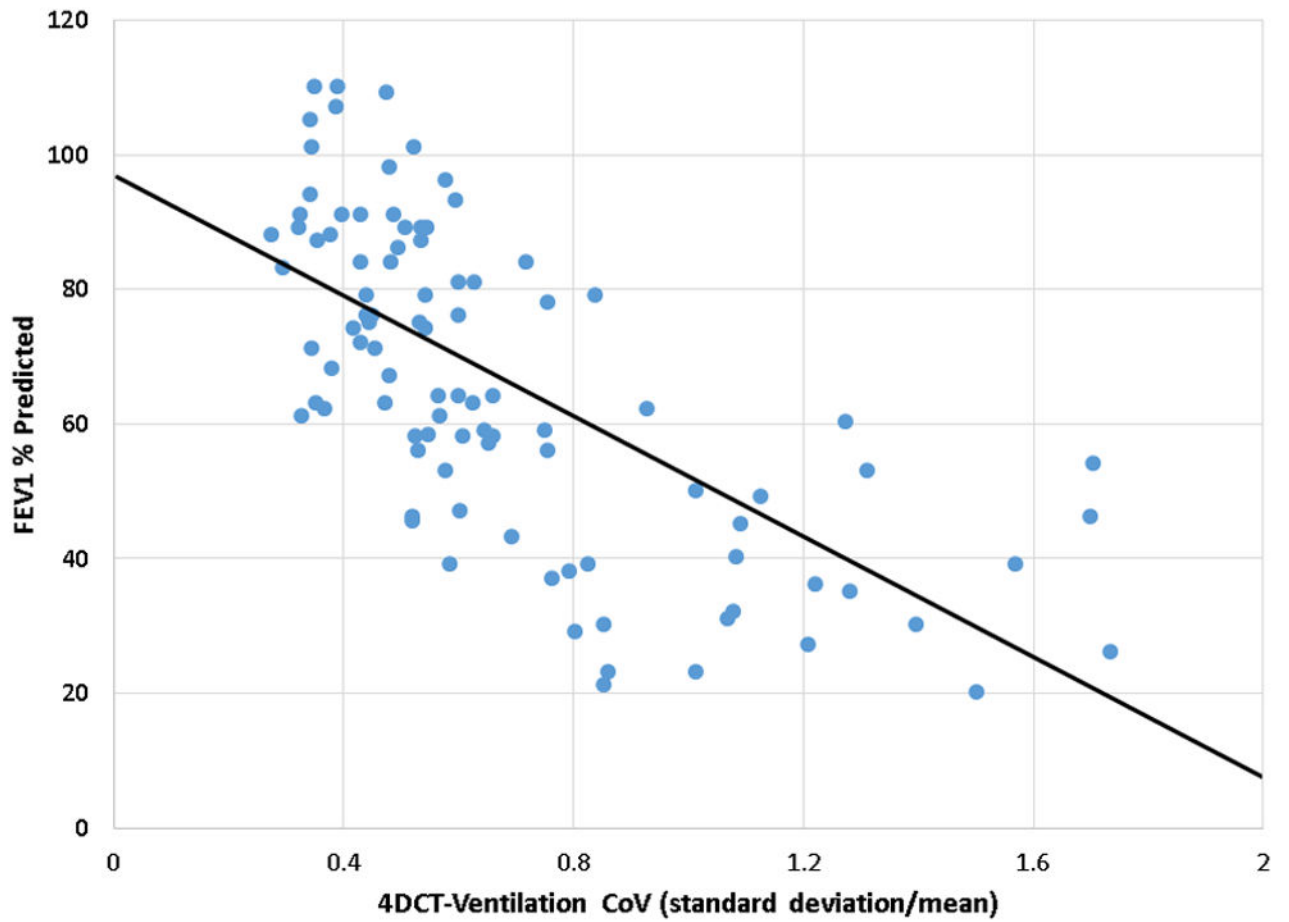


Figure 2.

Scatter plot showing the relationship between the FEV1 and the 4DCT-ventilation derived CoV (using the HU method). As the CoV increases (lung function gets worse) the FEV1 is congruently reduced.

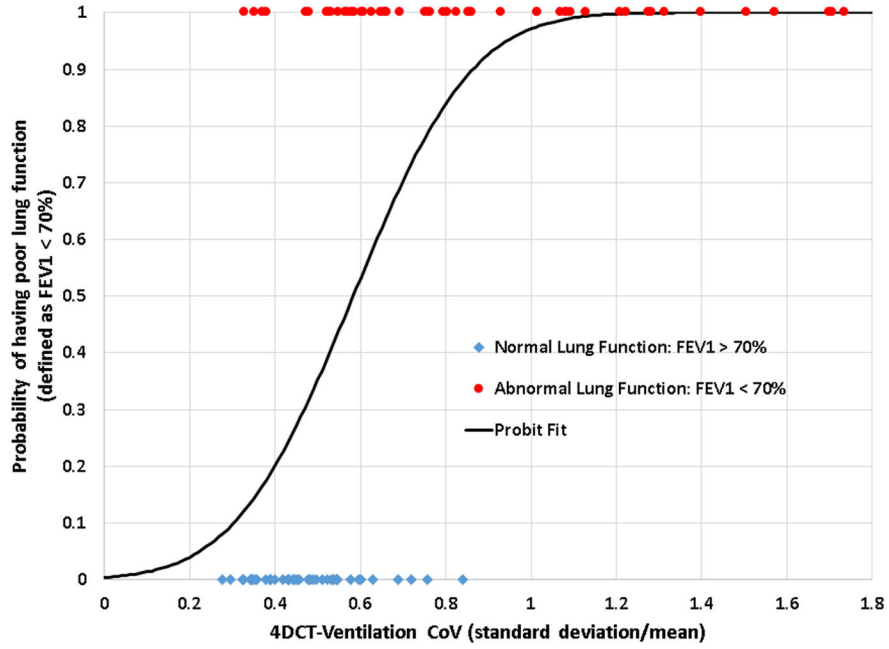


Figure 3. A PFT threshold of 70% was used to delineate between normal versus abnormal lung function. The graph shows raw data points and a sigmoidal curve fit to the binary results (normal/abnormal) as a function of the ventilation-derived coefficient of variation. The significant model fit of the curve indicates the ability of 4DCT-ventilation (using the HU method) to delineate between normal versus abnormal lung function.

Table 1

Patient and clinical characteristics for the patient population used for the study.

Parameter	Median (Range) or Number (%)
Age	68 (43–87)
Sex	
F	54 (55%)
M	44 (45%)
COPD	
yes	28 (29%)
no	70 (71%)
Tumor location	
Right	54 (55%)
Left	42 (43%)
Both	2 (2%)
Tumor Stage	
I	32 (33%)
II	4 (4%)
III	60 (61%)
IV	2 (2%)

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Correlation coefficients and area under the curve from the ROC analysis comparing PFT metrics and 4DCT-ventilation derived metrics.

Table 2

		4DCT-Ventilation HU Metrics			4DCT-Ventilation-Jacobian Metrics						
		CoV		V20		CoV		V20			
		CC	AUC	CC	AUC	CC	AUC	CC	AUC		
PFT Metrics		FEV1 % of reference		0.72	0.86	0.72	0.82	0.40	0.72	0.40	0.67
		FEV1/FVC		0.67	0.83	0.67	0.81	0.38	0.64	0.46	0.67

Abbreviations: PFT: Pulmonary function test, FEV1 = Forced expiratory volume in 1 second, FVC = Forced vital capacity, CoV = Coefficient of variation defined as the ratio of the standard deviation and the mean, V20 = volume of lung with 20% ventilation or less, CC=correlation coefficient, AUC = area under the curve.

Table 3

A comparison of mean PFT values for patients with and without noted ventilation defects.

	Ventilation defect present (mean \pm standard deviation)	No ventilation defect present (mean \pm standard deviation)	ttest p value
FEV1	60.3 \pm 22.8	70.8 \pm 25.1	0.034
FEV1/FVC	61.0 \pm 15.3	66.5 \pm 15.6	0.086

Abbreviations: PFT: Pulmonary function test, FEV1 – Forced expiratory volume in 1 second, FVC = Forced vital capacity.

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