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## **Using advanced noninvasive imaging techniques to probe the links between regional coronary artery endothelial dysfunction and atherosclerosis**

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### **Abstract**

Cardiovascular disease remains the number one cause of death in the US annually. The development in recent years of imaging strategies that can identify coronary endothelial dysfunction noninvasively provide new information about the early presence and local spatial heterogeneity of endothelial function in patients with, and those at risk for, coronary artery disease. In this summary, we will briefly review the mechanisms relating endothelial function and atherosclerosis, contemporary imaging strategies now able to quantify coronary endothelial function noninvasively, and recent insights on human coronary endothelial function.

### **Introduction**

Coronary atherosclerotic disease is a spatially heterogeneous vascular disorder occurring at discrete locations with a chronic, staccato progression often punctuated by abrupt, unheralded plaque changes, erosion and rupture. Although systemic cardiovascular risk factor modification strategies, such as those directed at hyperlipidemia, hypertension, and tobacco abuse, reduce cardiovascular events and have been temporally associated with a 50% reduction in annual cardiovascular mortality rates over the last two decades, cardiovascular disease remains the number one cause of death in the US annually (Roger et al. 2011). Coronary endothelial dysfunction is both a consequence and cause of atherosclerosis and may be an important factor that contributes locally to coronary atherosclerosis and its progression. Historically coronary endothelial function could only be studied during invasive cardiac catheterization procedures, which sometimes precluded evaluation of healthy or low risk populations and often of serial studies in a given patient.

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The development in recent years of imaging strategies that can identify coronary endothelial dysfunction noninvasively provide new information about the early presence and local spatial heterogeneity of endothelial function in patients with, and those at risk for, coronary artery disease. Although prior reviews of endothelial function and atherosclerosis have been published, the literature on noninvasive coronary endothelial functional imaging approaches is relatively recent and the concept of heterogeneity of coronary endothelial function is rapidly evolving, with potential translational importance. Thus, we will briefly review here the mechanisms relating endothelial function and atherosclerosis, contemporary imaging strategies now able to quantify coronary endothelial function noninvasively, and recent insights on spatial heterogeneity of human coronary endothelial function.

### **The endothelium as a dynamic organ responding to signaling pathways critical in vascular physiology and pathology**

The vascular endothelium plays a central role in the maintenance of vascular health (Vita and Keaney 2002), and controls vasomotor tone, hemostatic balance, vascular permeability, innate and adaptive immunity and trafficking blood cells (Vita and Keaney 2002) while also inhibiting vascular smooth muscle cell proliferation and apoptosis (Herman and Moncada 2005). In addition to acting as a functional and structural barrier between blood and vessel wall preventing platelet and leukocyte adhesion and aggregation, the endothelium behaves as a receptor-effector structure sensing physical and chemical stimuli and/or releasing products to maintain homeostasis. The endothelium can be described as an endocrine organ, capable of producing a large variety of different molecules including vasodilators and vasoconstrictors, procoagulants (e.g., tissue factor, von Willebrand factor) and anticoagulants (e.g., thrombomodulin), inflammatory and anti-inflammatory, fibrinolytics (e.g., tissue plasminogen activator,) and antifibrinolytics, oxidizing and antioxidizing molecules (van Hinsbergh 2012). The endothelium also regulates vascular tone by releasing vasoconstrictors such as endothelin-1 (ET-1), and by converting angiotensin I to II. ET-1 and angiotensin II have roles not only in vasoconstriction, but also in the development of atherosclerosis, including stimulation of smooth muscle cell proliferation, vascular remodeling, and inflammatory cell adhesion (Figure 1), (Ferrario and Strawn 2006).

Nitric Oxide (NO), the predominant mediator of normal vascular function, is released by healthy endothelium and diffuses within the vessel wall, causing smooth muscle dilation in response to stimulation by endogenous factors such as bradykinin, acetylcholine, and catecholamines as well as ischemia, temperature change, and mechanical stimuli, including shear stress, as previously reviewed (Libby 2012). Because of the fundamental role of NO in mediating endothelial function, detection of impaired vasodilation in response to stressors that increase endothelium-derived NO is often used to measure abnormal endothelial function (Corretti et al. 2002). When the normal balance between vasodilators and vasoconstrictors cannot be maintained by the endothelium, the term "endothelial dysfunction" is often used and it refers to a maladapted endothelial phenotype characterized by reduced NO bioavailability, increased oxidative stress, elevated expression of proinflammatory and pro-thrombotic factors, and abnormal vasoreactivity to endothelialdependent stressors (Drexler 1997). A growing number of interventions known to reduce

cardiovascular risk improve endothelial function (Egashira et al. 1994) (Hornig et al. 1996) (Eguchi et al. 2012). In addition, endothelial dysfunction is an independent risk factor for cardiac death, myocardial infarction, and stroke (Bonetti et al. 2003). Thus, because established cardiovascular risk factors operate through the common pathway of impairment in endothelial function, endothelial function has been proposed as a "barometer" (Vita and Keaney 2002) for cardiovascular health that may be useful for guiding patient care and evaluating therapeutic strategies.

### **Endothelial function in peripheral arteries**

Endothelial function was first studied in the peripheral arteries because they are more accessible than the coronary arteries (Flammer et al. 2012). Briefly, invasive and noninvasive techniques have been used to assess peripheral endothelial function. Venoocclusive strain-gauge plethysmography has, for more than 100 years, been used to measure the forearm vein impedance following intra-arterial infusion of vasoactive drugs at doses designed to limit systemic effects (Joyner et al. 2001). Intra-arterial infusion of vasodilators causes either endothelium-dependent (ie acetylcholine, bradykinin and substance P) or independent (sodium nitroprusside) vasodilation. Acetylcholine acts primarily via eNOS stimulation through endothelial muscarinic membrane receptor activation, which generates nitric oxide by metabolizing L-arginine (Flavahan 1992). The response to endotheliumindependent vasodilatory agents, such as nitroglycerin or sodium nitroprusside, defines the vasodilatory properties of the blood vessels independent of the endothelium, and has been used as a control stimulus. The dose required to produce a local effect is much lower than the systemically effective dose. However, the need for arterial cannulation limits its use in large-scale studies. Ultrasound has been used to quantify the vasoactive shear stress related response following arterial occlusion with a blood pressure cuff that results in postocclusion flow mediated dilatation (FMD) (Celermajer et al. 1992, Corretti et al. 2002). Because ultrasound quantification of FMD is non-invasive and easily repeated, it has become the most widely used noninvasive method for assessing endothelial function. However the method of evaluating endothelial response by FMD is rather technically challenging, time consuming and associated with a significant learning curve (Corretti et al. 2002). Although brachial FMD has been considered one of the most promising cardiovascular risk markers (Bonetti et al. 2003), a recent large prospective cohort study failed to demonstrate a significant correlation between brachial FMD and the incidence of coronary heart disease (Yeboah et al. 2012). Fingertip peripheral arterial tonometry (PAT) techniques evaluate finger arterial pulse wave amplitude before and during reactive hyperemia and have been proposed as noninvasive method to assess microvascular function in individuals (Kuvin et al. 2003). Although both FMD and PAT responses reflect aspects of vasoreactivity, conflicting results regarding their correlation have been reported (Lee et al. 2012) and it is not clear that they always reliably predict cardiovascular events (Anderson et al. 1995, Yeboah et al. 2012).

### **Invasive measures of coronary endothelial function**

Seminal clinical studies of coronary endothelial dysfunction were performed invasively, measuring the vasomotor response of epicardial arteries with quantitative coronary

angiography and coronary blood flow by Doppler in response to graded concentrations of acetylcholine (Ludmer et al. 1986). These approaches have been considered the "gold standard" for the evaluation of coronary endothelial function for the last 25 years. Interestingly, when used in the coronary circulation, acetylcholine causes dilatation of the epicardial vessels if endothelial function is preserved but constriction with endothelial dysfunction. The vasoconstriction is likely related to unopposed muscarinic receptor stimulation (Ludmer et al. 1986) and is in contrast to other vascular beds, such as the brachial or femoral arteries, where endothelial dysfunction is manifested as a diminished dilator response rather than constriction (Panza et al. 1993). Isometric handgrip exercise, cold pressor, and mental stress are considered predominant endothelial-dependent stressors because they dilate normal coronary arteries and paradoxically constrict atherosclerotic arteries (Brown et al. 1984, Nabel et al. 1988) (Yeung et al. 1991).

### **Noninvasive Detection of Coronary Endothelial Function**

Although catheter-based studies of coronary endothelial function have provided critical insights over many years into the mechanisms, importance, and clinical relevance of coronary endothelial function and its relationship to atherosclerosis, the invasive nature is not well suited to studies in healthy and low risk populations or to longitudinal studies in the same individual over time. Advances in newer imaging technologies such as magnetic resonance imaging, positron emission tomography, and computed tomography promise noninvasive means to assess coronary vasomotor responses that could greatly extend our understanding of the role of coronary endothelial dysfunction in both early and later stage atherosclerosis as well as the impact of conventional and evolving strategies on endothelial function and atherosclerosis.

### **Positron Emission Tomography (PET) and Multi-detector Computed Tomography (MDCT)**

The availability of PET scanners is growing and several positron-emitting tracers can be reliably used to quantify myocardial blood flow (MBF), including<sup>15</sup>O-labeled water, <sup>13</sup>Nammonia and 82Rubidium. Although the spatial resolution of PET is limited and does not permit direct visualization of the coronary arteries at this time, MBF can be quantified in absolute terms (ml/min/g) with PET and intervention-induced MBF changes used to infer coronary artery vasomotor responses (Yoshinaga et al. 2011). Cold pressor testing and mental stress are the most common interventions used to probe coronary endothelial function with PET and such studies have identified abnormal responses in subjects with CAD risk factors but angiographycally normal coronaries (Schindler et al. 2010) and in stenosed and in non-stenosed segments of CAD patients (Arrighi et al. 2000). Because MBF is affected by both epicardial coronary vasomotor tone and microvascular beds, it is not possible with PET to distinguish epicardial coronary responses from microvascular responses or to identify segmental arterial differences in coronary endothelial function. MDCT offers a much higher spatial resolution than PET and is currently the leading modality for noninvasively imaging coronary artery anatomy. Changes in coronary crosssectional area in response to vasoactive stressors can be quantified with MDCT and, in theory, could be related to the presence of local coronary calcium and/or to local

atherosclerosis determined by MDCT angiography. Unlike conventional cardiac catheterization with a Doppler flow probe, MDCT cannot currently quantify coronary blood flow, although it can be used to index relative MBF (Salerno and Beller 2009). Both PET and MDCT expose subjects to the risks of ionizing radiation which may be an important consideration in low risk populations and some research settings where imaging would be performed two times: in the absence and presence of an endothelial-dependent stressor.

### **Magnetic Resonance imaging (MRI)**

MRI is an appealing non-invasive imaging platform for quantifying coronary endothelial function because it is a tomographic technique offering high soft tissue contrast, excellent spatial resolution, the ability to quantify blood velocity and flow, as well as local atherosclerosis and vessel remodeling without exposing subjects to ionizing radiation. Specifically, coronary MRI has been validated as a noninvasive means to assess coronary cross-sectional area (Scheidegger et al. 1996) and flow velocity (Hundley et al. 1996). It has also been used to document endothelial-independent coronary artery vasomotor responses to nitroglycerin, which are altered in patients with calcified and severe coronary artery disease (Jin et al. 2012). Recently, our group developed an MRI approach to noninvasively quantify coronary endothelial function that exploits the increased signal available with high-field (3T) MRI systems and phased-array detector coils and combines that with isometric handgrip exercise, a well-tolerated endothelial-dependent stressor that is easily performed in a MRI scanner. "Bright blood" cine MR images are acquired orthogonal to the long-axis of coronary arteries during a single breathhold (15–20 sec) in order to obtain cross-sectional coronary artery dimensions (area and diameter) throughout the cardiac cycle with an approximate time resolution of 30–45ms (Figure 2) (Hays et al. 2010). Phase-contrast cine MR images are obtained in the same imaging plane and provide robust, validated measures of blood flow on a pixel-by-pixel basis. With measures of coronary cross-sectional area and blood velocity, local coronary blood flow can be calculated. In healthy subjects without CAD risk factors, isometric handgrip results in coronary vasodilation, an increase in coronary blood velocity, and coronary blood flow (Hays et al. 2010). In patients with documented CAD, the same stressor causes an identical hemodynamic response (i.e. increase in rate pressure product) but instead coronary vasoconstriction and reduced coronary blood flow. The response is rapid (within 30 seconds), resolves quickly (within 2 minutes), and is reproducible on repeat study (Hays et al. 2010). In patients with singlevessel critical CAD the vasomotor response in the severely diseased vessel (not at the site of stenosis but approximately 2 cm away) was more abnormal than that in a non-stenosed coronary artery (Figure 2B). To evaluate earlier stages of atherosclerosis, the MRI technique for evaluating local coronary endothelial function was combined with "black blood" MRI to quantify coronary wall thickness (CWT), an important index of arterial remodeling and early coronary atherosclerosis (Kim et al. 2007) (He et al. 2012). Using this combined approach, patients with non-critical CAD demonstrated abnormal coronary endothelial function (impaired coronary vasodilation and flow changes in response to isometric handgrip stress) and increased CWT and normalized wall index, a quantitative measure of vessel remodeling (Figure 3) (Hays et al. 2012). Importantly, in patients with mild coronary disease, CWT correlated inversely with the endothelial-dependent vasomotor response indicating that at

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the earliest stages of coronary atherosclerosis detected noninvasively there is local coronary endothelial dysfunction and it is related to the extent of early atherosclerosis (Figure 3I) (Hays et al. 2012). Taken together these findings demonstrate that endothelial dysfunction is heterogeneous in patients with CAD and suggests that a single measure of peripheral endothelial function is unlikely to represent the spectrum of endothelial function present in the coronary arteries of a CAD patient (Hays et al. 2010) (Hays et al. 2012). This is also consistent with the variable correlation between peripheral and coronary endothelial function noted in the literature (Anderson et al. 1995).

### **Heterogeneity of endothelial function**

As noted above the endothelium is not an inert layer of cells but a dynamic, responsive cellular lining that may display structural and functional heterogeneity to meet the diverse and varying demands of the local tissues (Aird 2007a, Aird 2007b). With the introduction of the electron microscope in the 1950s, the endothelium was described as a monolayer of cells with variable characteristics in different vascular beds (Tse and Stan 2010). The discovery of the variable morphology of endothelial cells led to the understanding that these cells differ from each other also in their function and response to certain stimuli. In fact, it is striking to note that vascular beds respond differently to pro-inflammatory stimuli. For example, TNF-alpha receptor expression differs among vascular territories (Al-Lamki et al. 2009) and intravenous injection of TNF-alpha in mice, induces E- and P-selectin expression in the heart, lung, kidney and liver but not in the spleen (Yao et al. 1999). At a genetic level, mapping of the endothelial cells in specific territories has identified the presence of "vascular zip-codes" referring to specific expression profiles for each vascular bed (Ruoslahti 2004). Interestingly, the plasticity of the endothelium is demonstrated by the ability to modify gene expression depending on the environment to which the endothelial cells are exposed. A recent study showed that the differences observed in vivo between endothelial cells harvested from porcine coronary artery when compared to the ones from an iliac artery were lost when those cells were cultured in vitro (Burridge and Friedman 2010), implying an active modification of the expression of certain genes depending on the environmental exposure. Differences in epigenetic regulatory mechanisms, affecting methylation status of gene promoters and posttranslational histone modifications such as acetylation, methylation, phosphorylation, may also partially explain endothelial subset preference of gene expression (Regan and Aird 2012). These epigenetic modifications are not a static characteristic of endothelial cells but can dynamically vary in time as has been recently shown for eNOS, whose histone markers were reset due to hypoxia, thus affecting gene expression (Fish et al. 2010).

Vasoreactivity varies among vascular beds in a given individual for several reasons including the intrinsic mechanical properties of the vascular bed, non-endothelial dependent factors and endothelial-dependent differences. In apo-E deficient mice, local endothelial function was associated with the local presence and extent of atherosclerosis (Crauwels et al. 2003) while in pigs, segmental coronary endothelial dysfunction was related to the presence of local markers of inflammation and oxidative stress (Pendyala et al. 2009). Spatially heterogeneous or segmental coronary endothelial function has been observed in patients with coronary artery disease (Suwaidi et al. 2000) and in patients following cardiac

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transplantation (Davis et al. 1996). With the use of spectral analysis of intravascular ultrasound (IVUS) radiofrequency data to characterize predominant plaque components, local coronary endothelial dysfunction in patients with early or minimal coronary atherosclerosis was closely associated with high-risk plaque characteristics such as the presence of a necrotic core (Lavi et al. 2009). More recently, local epicardial coronary endothelial dysfunction closely correlated with the presence and extent of a lipid core plaque detected by near-infrared spectroscopy (NIRS) and typically associated with high-risk lesions (Choi et al. 2013), The most recent non-invasive coronary MRI studies, mentioned earlier, built on this line of evidence for segmental coronary endothelial dysfunction and identified a greater degree of endothelial dysfunction in coronary arteries with more severe stenotic disease than in minimally diseased vessels in the same patients (Hays et al. 2010). All of these findings are consistent with a hypothesis that endothelial dysfunction is a heterogeneous process within the same patient that may predispose to segmental disease progression and events (Suwaidi et al. 2000). It should be noted that although both peripheral and coronary endothelial function have been considered predictors of future cardiovascular events (Schachinger et al. 2000), the two do not always closely correlate and vasoreactivity is not always uniform across vascular regions within the same individual (Silber et al. 2007). One study, using MRI compared brachial versus femoral vasoreactivity during postocclusion hyperemia and found that femoral but not brachial reactivity was impaired in patients with increased cardiovascular risk (Silber et al. 2007). Other data suggest that peripheral and coronary endothelial function measures may be weakly related (Anderson et al. 1995), possibly due to differences in vascular properties (Hirooka et al. 1994). The difference in local vascular properties between coronary and peripheral vessels is consistent with the clinical experience that acute coronary plaque rupture is common while brachial arterial plaque rupture rarely, if ever, occurs. Similarly, a recent study did not find any correlation between carotid intima media thickness (IMT) and coronary circulatory function using PET-measured MBF, again suggesting different features of early atherosclerosis in the peripheral and coronary circulations (Schindler et al. 2009). Taken together, there is an evolving body of evidence that endothelial function varies among vascular beds and varies segmentally within a vascular territory, in part related to local disease and suggests that measures of local endothelial function may offer a valuable window into the local vascular pathophysiology.

Many important questions remain unanswered and thus offer fertile areas for investigation in terms of the distribution and significance of endothelial function heterogeneity in atherosclerosis. Because noninvasive approaches offer the most readily applicable means to study vasoreactivity in larger populations and low-risk individuals, the type of endothelialdependent stressor becomes an important consideration. Intra-arterial acetylcholine cannot be readily administered in noninvasive settings and post-occlusion FMD, used extensively for peripheral endothelial function, cannot be directly applied to studies of coronary, pulmonary or renal vascular function. Thus it will be important to compare the responses and mechanisms of different currently used "less-invasive" endothelial-dependent stressors including isometric handgrip exercise, cold pressor testing, and mental stress.

### **Implications**

More important than the technical advances are the important biologic questions that can now be addressed with these new insights and tools. First, if endothelial function is indeed a barometer of local (or even segmental) vascular health, can noninvasive coronary endothelial function measures be used to predict local coronary atherosclerotic progression, plaque rupture and events? It is clear that anatomic indices of atherosclerosis alone are poor individual predictors of plaque progression and events (Stone et al. 2011) and it may be time to consider a new paradigm whereby endothelial cell physiology, rather than vessel anatomy alone, is used to gauge risk and likelihood of future events. Second, coronary endothelial function should be evaluated as a tool to assess the vascular impact of new and emerging treatment strategies and to guide drug development. New molecules and approaches designed to limit oxidative stress, local inflammation, apoptosis, or improve regenerative capacity could be evaluated repeatedly and noninvasively over time in the same subjects and same arterial segments with these approaches. Third, noninvasive assessment of coronary endothelial function should be investigated as a complementary tool in the development of individualized medicine.–In summary, coronary endothelial dysfunction is both a consequence and cause of atherosclerosis and the development in recent years of imaging strategies that can identify coronary endothelial dysfunction noninvasively may provide new information about the early presence and local spatial heterogeneity of endothelial function in patients with, and those at risk for, coronary artery disease.

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### **Figure 1.**

Cross-sectional depiction of a coronary artery progressing from normal endothelial function to endothelial dysfunction and plaque formation (left to right). In the healthy state the endothelium is responsible for regulating vascular tone with balanced production of vasodilators and vasoconstrictors. In endothelial dysfunction this balance is disrupted in favor of the vasoconstrictors. An inflammatory and/or pro-thrombotic state promotes the formation of the plaque, plaque erosion and rupture.

 $cGMP = cyclic guano sine monophosphate; cAMP = cyclic adenosine monophosphate; NO =$ nitric oxide; NOS = nitric oxide synthase;  $COX = cyclooxygenase$ ; BH4 = tetrahydrobiopterin; L-arg = L-arginine; L-cit = L-citrulline; EDHF= endothelium derived hyperpolarizing factor;  $IL =$  interleukin;  $TNF =$  tumor necrosis factor;  $ONOO =$ peroxinitrite; PAI1= plasminogen activator inhibitor 1; tPA = tissue plasminogen activator; ROS = reactive oxygen species; SMC = Smooth muscle cells





#### **Figure 2.**

Noninvasive detection of coronary endothelial dysfunction and regional differences in coronary endothelial function. (Upper Panel) "White blood" scout MRI of the right coronary artery (RCA) in long axis with white line representing orientation of subsequent crosssectional images shown in middle panel. (Middle Panel) Flow velocity-encoded MRI phase images showing a cross section of the RCA (A) that was selected for analysis for coronary flow velocity measurements in a healthy volunteer. The signal intensity is proportional to flow velocity, with a black signal indicating high velocity down through the imaging plane. In the magnified view of the RCA at baseline  $(B)$  and during isometric handgrip stress  $(C)$ , the decrease in luminal coronary signal intensity (increased blackness) illustrates an increase in through-plane coronary flow velocity. The cross section of the RCA in a coronary artery disease patient at rest (D) and during handgrip stress (E) indicates no increase in throughplane coronary flow velocity during stress. (Bottom Panel) Summary data showing relative change in coronary artery area, peak diastolic coronary flow velocity and blood flow during isometric handgrip stress for healthy subjects ( $n = 20$  [open bars]) and patients with singlevessel coronary artery disease (CAD)  $(n = 10)$ . Brackets show comparisons between arteries with mild CAD (hatched bars) versus severe CAD (solid bars) *within the same patients*. \*p < 0.005, †p < 0.001 versus healthy subjects. Reproduced with permission from Hays et al (Hays et al. 2010)

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#### **Figure 3.**

Noninvasive assessment of early coronary atherosclerosis, coronary endothelial function, and their relationship with MRI. (Upper Panel) Typical anatomic and functional coronary images using MRI at rest and with isometric handgrip stress. In a healthy subject (A), a scout scan obtained along the right coronary artery (RCA) in a healthy adult subject is shown together with the location for cross-sectional imaging (red line). B, A view perpendicular to the RCA in a healthy adult subject is shown, illustrating a black blood vessel wall cross-section. C, A white blood view for endothelial function in a healthy subject is shown at rest (C) and during stress (D). In a patient with CAD (E–H), a scout scan obtained parallel to the RCA is shown (E) together with the location for cross-sectional imaging (red line). F, RCA black blood vessel wall cross-sectional image in the same patient with CAD. G, A view perpendicular to the RCA in the patient with CAD is shown at rest (G) and during stress (H). (Lower Panel). Relationship between early atherosclerosis and endothelial function is shown in the summary data (I). MRI measures of coronary wall thickness (mm) versus percent coronary cross-sectional area changes with isometric handgrip stress in healthy subjects and patients with coronary artery disease (combined) while individual data points are shown for healthy subjects (blue diamonds) and patients with coronary artery disease (red diamonds). Reproduced with permission from Hays et al (Hays et al. 2012)