

## Original Article

# Pulsed magnetic field promotes proliferation and neurotrophic genes expression in Schwann cells *in vitro*

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**Abstract:** As one of the most classic supportive cells, Schwann cells (SCs) have been considered as potential candidates for nerve regeneration. However, SCs cultured *in vitro* are found with attenuated biological activities, which limits their application. Pulsed magnetic field (PMF) has been demonstrated to be safe and efficient to regulate several cells activities. However, it is still unclear the effect of PMF on proliferation and expression of neurotrophic factors in SCs. Therefore, the present study was designed to examine such possible effects. The tolerance of SCs to PMF was examined by flow cytometry and scanning electron microscopy (SEM). The proliferation of cells was detected by an EdU labeling assay and a Prestoblu assay. The expression and secretion of neurotrophic factors in SCs was assayed by RT-PCR and ELISA. We found that 2.0 mT was the optimal intensity that caused relatively little apoptosis with profound proliferation in SCs. The gene expression and protein level of brain-derived neurotrophic factor (BDNF), glial cell derived neurotrophic factor (GDNF), vascular endothelial growth factor (VEGF) were up-regulated following PMF stimulation, additionally, the gene expression and protein level of neurotrophin-3 (NT-3) was not enhanced by PMF. Our results suggested that PMF could improve SC proliferation and biological function, which might shed a light on the potential utilization of PMF in nerve regeneration via SC activation.

**Keywords:** Schwann cells, pulsed magnetic field, cell proliferation, neurotrophic factor

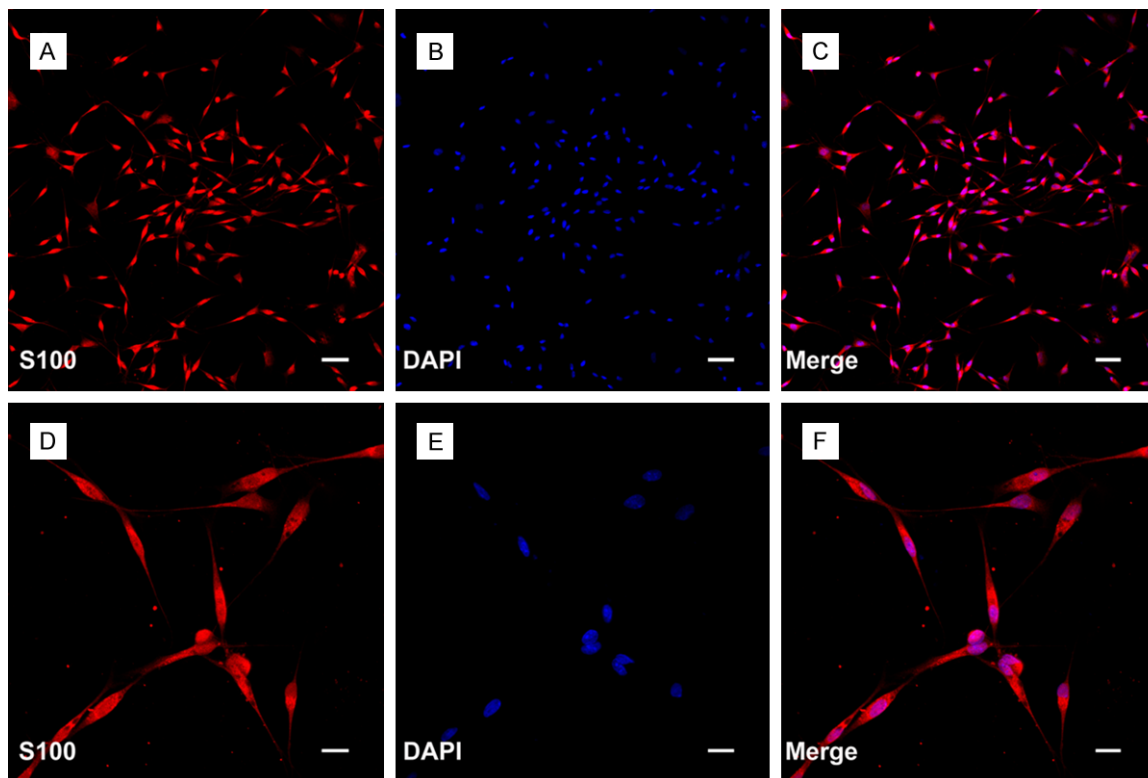
## Introduction

Nerve injury and regeneration are clinically and experimentally concerned in regenerative medicine. Generally, functional recovery is poor after nerve injuries, which results in the loss of motor, sensory and autonomic functions in both peripheral nervous system (PNS) and central nervous system (CNS) [1]. Nowadays, numerous biologic and cellular strategies have been reported as reparative approaches for anatomical restitution and locomotor recovery after nerve injury, amongst which Schwann cells (SCs) are attractive for its unique neurotrophic and neuroprotective effects [2].

SCs are the myelinating glia of the PNS which are capable of directing axonal migration and outgrowth [3]. Accumulating studies have shown that SCs play a central role in axonal regeneration and elicit remyelination by producing various of trophic factors, as well as the

expression of cell adhesion molecules known to influence neurite growth [4, 5]. Therefore, the application of SCs has been regarded as a potential source of cell therapy for nerve regeneration. However, SCs cultured *in vitro* are found with attenuated biological activities, which significantly limits the application of SCs in the repair of nerve injuries. Thus, it is interesting to explore new ways to activate SCs to improve their viability and biological properties in cellular treatment for nerve regeneration.

Pulsed electromagnetic field (PMF) has been demonstrated to be safe and efficient to enhance nerve regeneration *in vivo* [6-9]. In addition, Studies have been reported that PMF is closely linked with ionic mobilization, protein synthesis and growth factors secretion in various cell types [10, 11]. Thus far, a few studies have focused on the effect of PMF on SCs. It has been noted that SCs is impacted by magnetic field in orientation control [12]. However, it



**Figure 1.** Isolated SCs from sciatic nerve of the Sprague Dawley rats. A and D: The expression of S100 was showed by immunofluorescent staining. B and E: Nuclei of SCs were visualized with DAPI (4'-6-diamidino-2-phenylindole) staining. C and F: Merged file showed that approximately more than 97% cells were positive staining. Scale bars: A-C: 100  $\mu\text{m}$ , D-F: 50  $\mu\text{m}$ .

still remains unclear with regard to the influence of PMF on SC biological activities. Accordingly, the aim of this study was to address the underlying role of PMF in SCs and to further facilitate the application of PMF in SCs for nerve regeneration.

## Methods and materials

### *SC culture and identification*

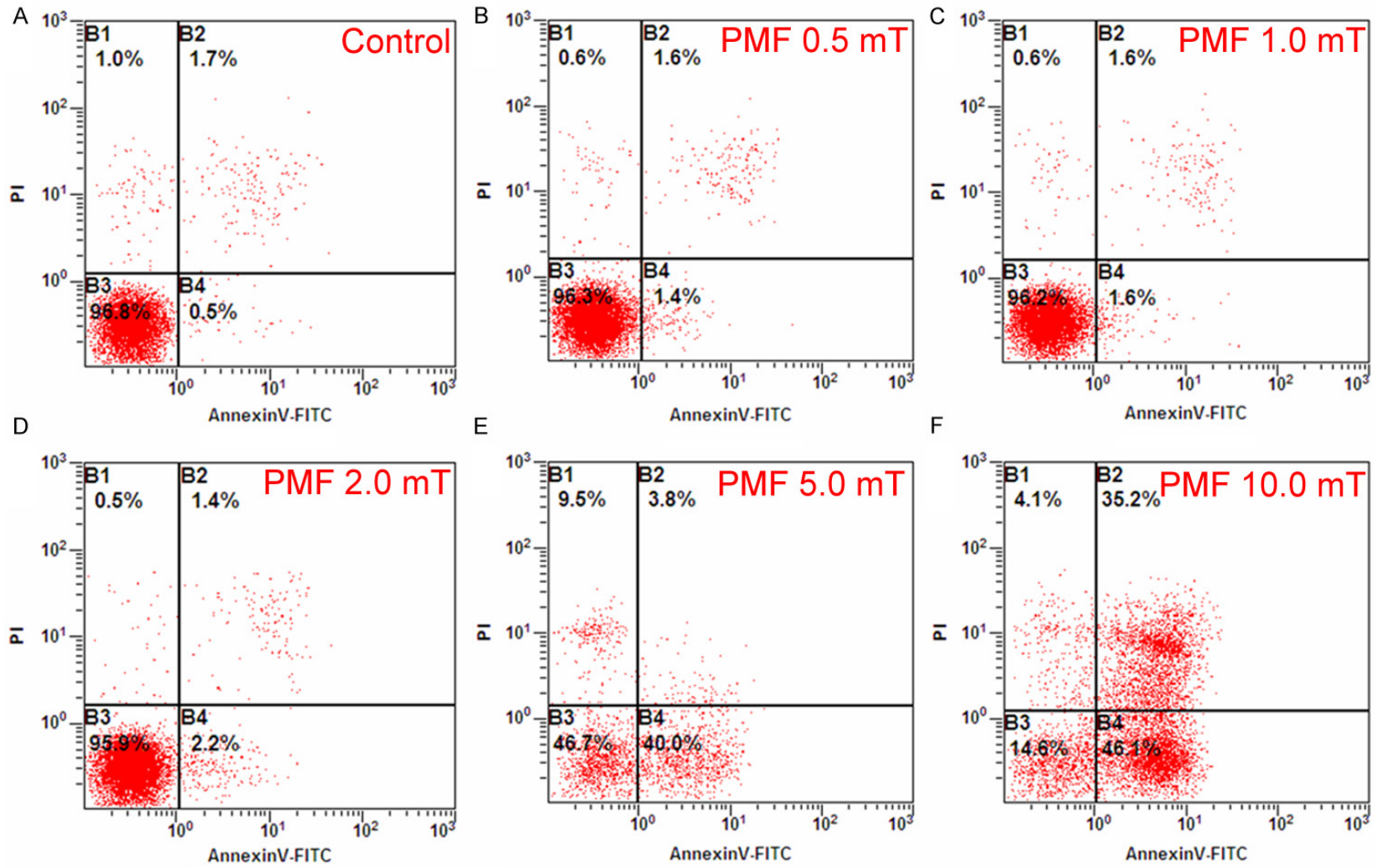
SCs were prepared and purified following a protocol described previously. All the experimental procedures were performed by the Guide for the Care and Use of Laboratory Animals. In brief, SCs were isolated from the sciatic nerves of newborn Sprague Dawley rats and further selected from fibroblasts. The purity of the SCs was determined by immunofluorescent staining with S-100. The final preparations consisted of a high purity (> 97%) of SCs (**Figure 1**). SCs were maintained in Dulbecco's modified Eagle's medium nutrient mixture F-12 (DMEM/F12; Gibco, USA) containing 10% fetal calf serum

(FCS; Gibco), antibiotics, bovine pituitary extract (Biomedical Technologies, USA) and forskolin (Sigma-Aldrich) at 37°C under humidified 5% CO<sub>2</sub>. SC cultures were passaged no more than five times before conducting experiments.

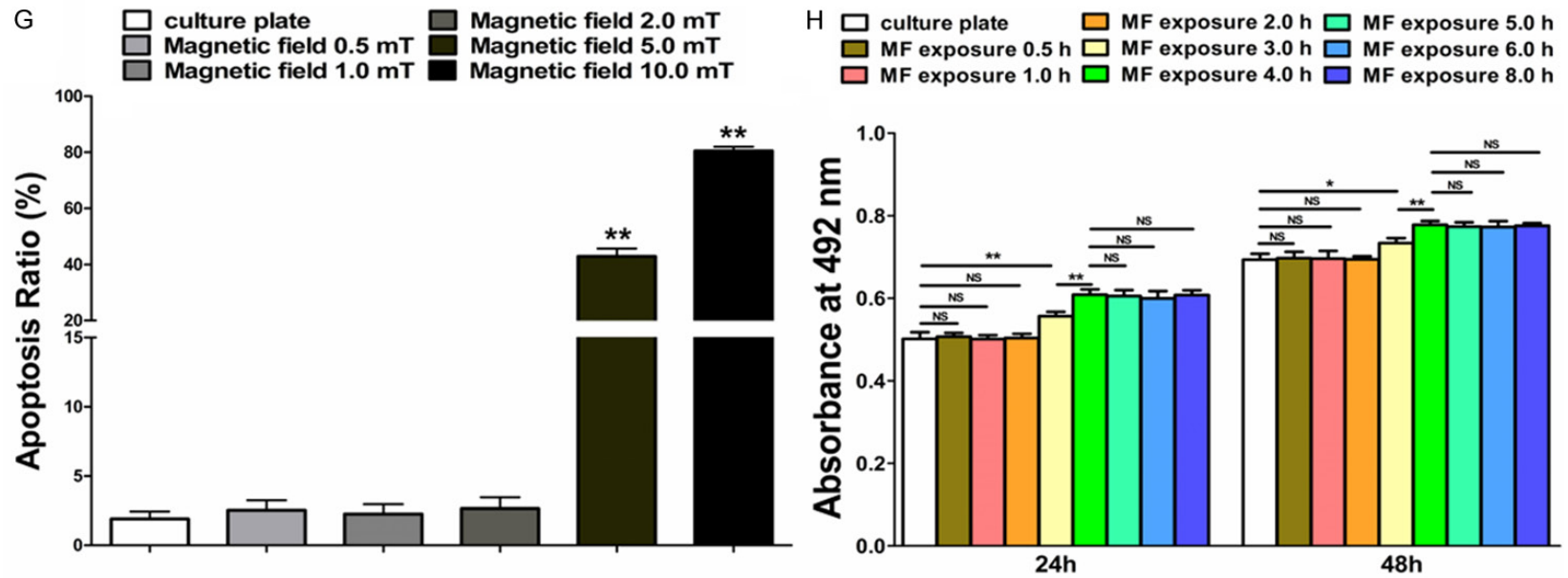
### *Magnetic field exposure system*

The magnetic stimulation system involved a solenoid and a magnetic field (PMF) generator to produce magnetic field with an adjustable magnetic induction of 0-20 mT and a frequency of 0-100 Hz. A PMF generator (GHY-III, China Patent, Xi'an, China) connected with the solenoid to produce an open-circuit output waveform PMF. The measurement accuracy of the electromagnetic field output was confirmed with a gaussmeter (Model 455 DSP Gaussmeter, Lake Shore Cryotronics, US). The PMF parameter was set to a frequency of 50 Hz as it was described in the previous experiments. Cells cultured in culture plates without solenoid was used as the culture plate group. In the no

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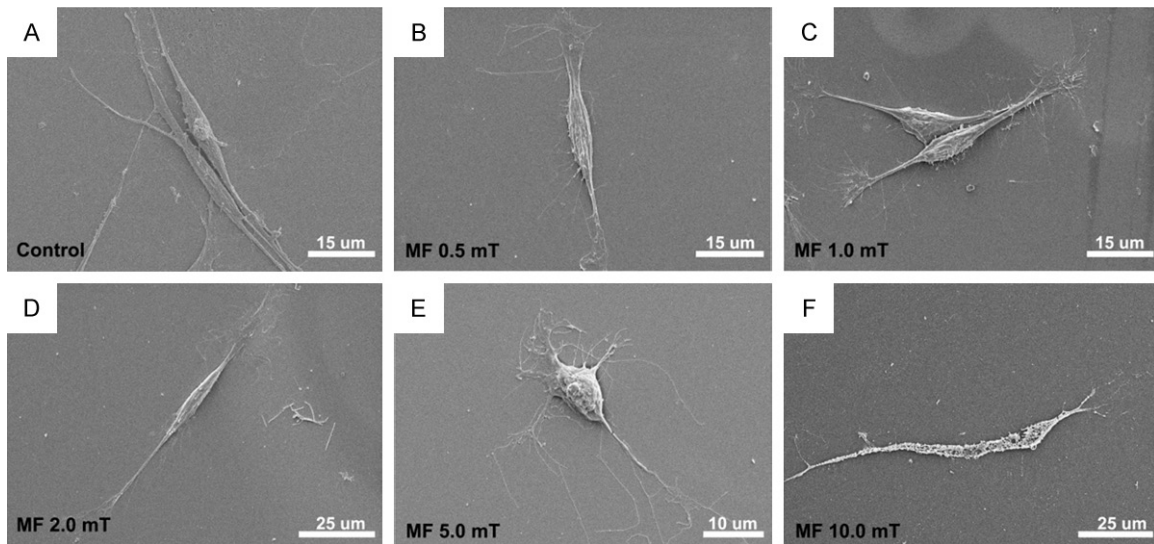


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**Figure 2.** Detection of apoptosis and proliferation in SCs. A-F: Flow cytometry assay of apoptosis in SCs following different PMF gradients (0.5 mT, 1.0 mT, 2.0 mT, 5.0 mT, 10.0 mT and 50 Hz). G: The percentage of apoptotic cells in each group was showed by averaging the results of four flow cytometry assays for each group. H: CCK-8 values of 24 h and 48 h after PMF exposure were obtained by averaging the results of four samples for each group. All data were expressed as the mean  $\pm$  SEM. \* $P < 0.05$ , \*\* $P < 0.01$ .

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**Figure 3.** Electron microscopy assay of SCs following different PMF gradients. A-D: SCs exhibited a spindle feature in the control group as well as in 0.5, 1.0 and 2.0 mT PMF stimulation. E: SCs were changed into round shape when the PMF increased to 5.0 mT. F: Damaged membranes were observed when the PMF increased to 10.0 mT.

magnetic field group, the cell culture plate was put correctly in a solenoid that was connected to the PMF generator but no output waveform.

### *Flow cytometry*

The SCs ( $1 \times 10^5$  cell/cm<sup>2</sup>) were cultured on culture plate for 24 h, and then different PMF gradients (0.5 mT, 1.0 mT, 2.0 mT, 5.0 mT, 10.0 mT; 50 Hz) were applied to the cells cultured on culture plate for 4 h. After PMF exposure, SCs were cultured for another 24 h, and then the percentage of viable cells was analyzed by flow cytometry within 30 min.

### *CCK-8 assay*

The viability of SCs was detected and quantified using the Cell Counting Kit 8 (CCK-8; Dojindo, Japan). Briefly, the SCs inoculated in 96-well plates were under different exposure times of the PMF (2.0 mT). At 24 and 48 hours after PMF exposure, SCs were washed with PBS and inoculated with DMEM/F12. Thereafter, the CCK-8 solution (10  $\mu$ L) was added to each well of the plate and incubated for 4 hours. The absorbance was measured at 492 nm using a microplate reader.

### *Morphological characteristics of SCs under PMF*

Twenty-four hours after PMF stimulation, the morphological feature of SCs was observed by scanning electron microscopy (SEM; JSM-

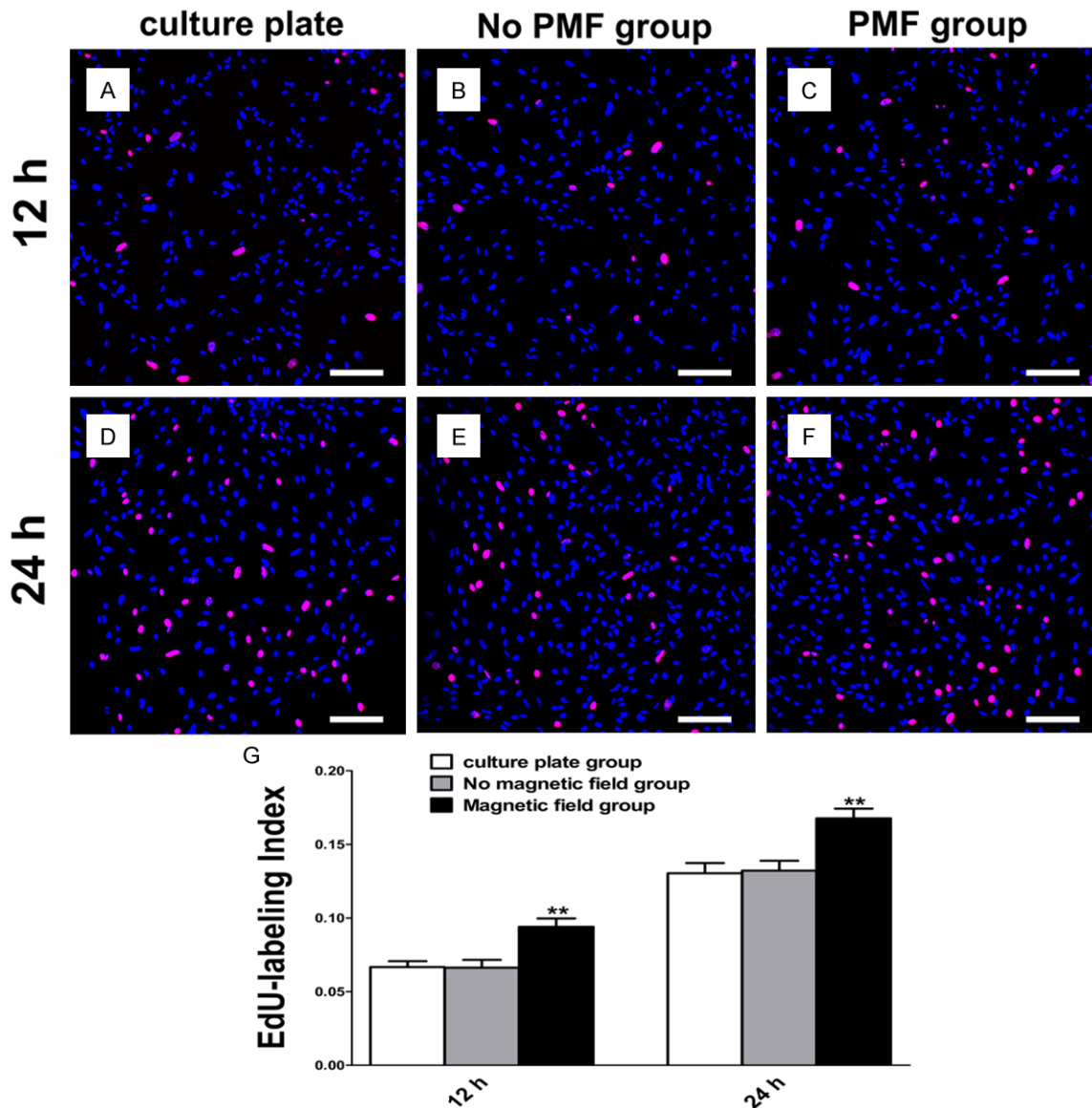
4800; Hitachi). In brief, SCs were rinsed with PBS and fixed with 4% paraformaldehyde for 30 minutes, washed three times with deionized water, and then dehydrated and later dried in vacuum environment. Thereafter, the specimens were sputter-coated with gold, and then visualized with SEM.

### *EdU-labeling assay*

Cell proliferation assays were performed using the Cell Light™ 5-ethynyl-2-deoxyuridine (EdU) deoxyribonucleic acid (DNA) cell proliferation kit (RiboBio, PRC). In brief, 12 and 24 hours after PMF exposure, EdU was applied 4 hours prior to fixation of SCs and the EdU immunostaining. Then, EdU-labeling index was calculated as the amount of EdU-stained nuclei divided by the amount of DAPI-stained nuclei calculated from five random fields. Assays were done three times using triplicate wells.

### *Gene-expression analysis*

At 12 and 24 hours after PMF stimulation, SCs were first counted and then homogenized in Trizol reagent (Sigma-Aldrich). Total ribonucleic acid (RNA) was isolated and normalized to cell numbers. Complementary DNA was synthesized using Superscript III reagents (Invitrogen, US). Then, quantitative real-time PCR (QRT-PCR) analysis was performed. The forward (f) and reverse (r) primers are used as follows: fBDNF AGTATTAGCGAGTGGGTC, rBDNF GTTC-



**Figure 4.** EdU-labeling assay of SCs. A-C: EdU-labeling of SCs after PMF exposure at 12 h. Scale bars: 100  $\mu$ m. D-F: EdU-labeling of SCs after PMF exposure at 24 h. Scale bars: 100  $\mu$ m. G: EdU-labeling index of SCs obtained by averaging the results of four samples for each group. All data were expressed as the mean  $\pm$  SEM. \*\* $P < 0.01$ .

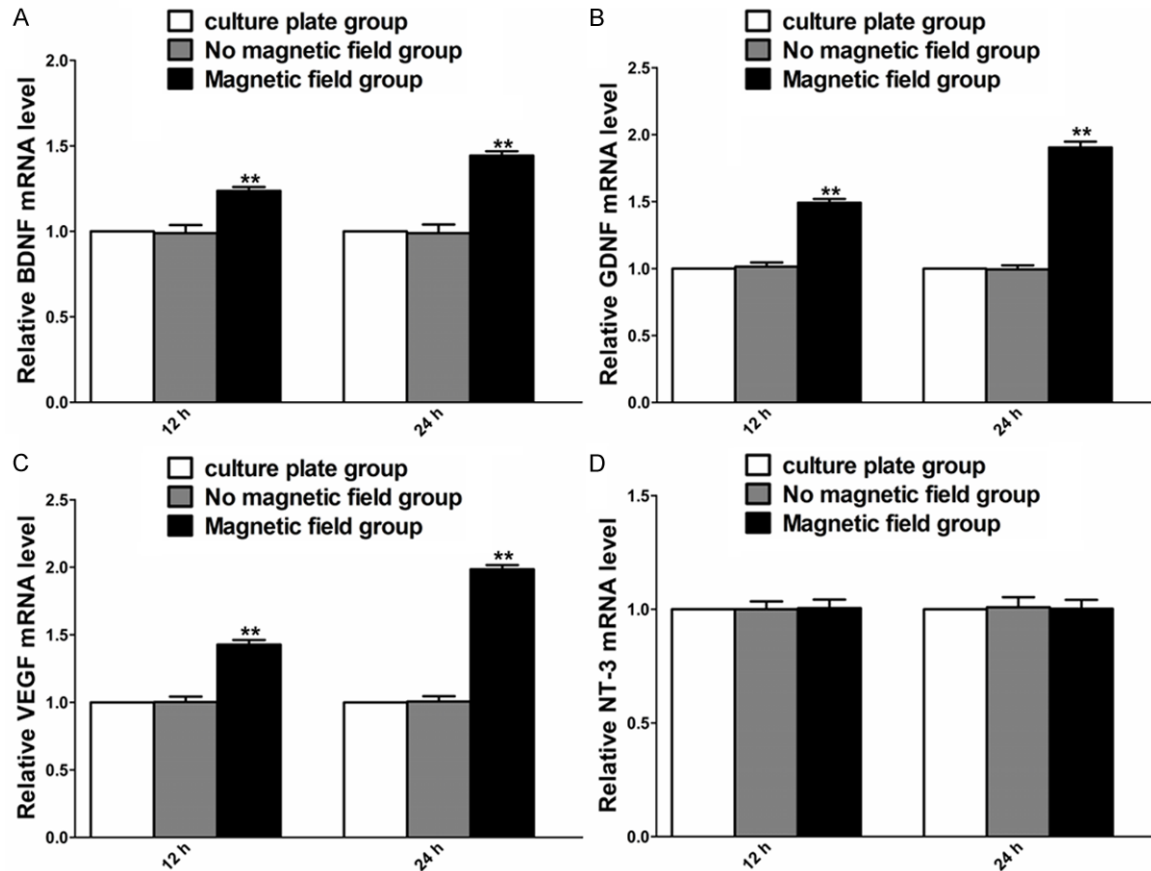
CAGTGCCTTTTGTGTC, fGDNF CAGAGGGAAAGG-TCGCAGAG, rGDNF ATCAGTTCCTCCTTGTTTT-CGTAG, fVEGF-A AACTTCTACCCGTGCCTT, r VEGF-A ACTTAGGTCAGCGTTTTCC, fNT-3 GCAG-GGTGAAGGGGAAAAC, rNT-3 GCCACGGAGAT-AAGCAAGAAA, fACTB (internal control) ATGA-AGATCCTGACCGAG and rACTB GCTCATTGCC-GATAGTGA. QRT-PCR conditions were as follows: denaturation at 95°C, 30 seconds; primer annealing at 59°C, 30 seconds; and elongation at 72°C, 40 seconds. Quantification of PCR products was performed using the  $2^{-\Delta\Delta Ct}$  method. Quantities of messenger RNA (mRNA) were normalized to the housekeeping gene

ACTB. Assays were done three times using triplicate wells.

*ELISA assay*

For enzyme-linked immunosorbent assay (ELISA) analysis, the SCs were cultured in fresh DMEM/F12 medium without FCS. At 12, 24, and 36 hours after PMF exposure, the number of SCs was counted, and the amount of BDNF, GDNF, VEGF, and NT-3 secreted by the cultured SCs was determined by culture mediums. Cell culture supernatants were centrifuged, and the assays were carried out using an ELISA kit

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**Figure 5.** Gene expression of BDNF, GDNF, VEGF and NT-3 in each cultured group at different time points after PMF exposure. A-D: The mRNA levels of BDNF, GDNF, VEGF and NT-3 were determined at 12 and 24 h. Each test was repeated three times. All data were expressed as the mean  $\pm$  SEM. \*\* $P < 0.01$ .

(Antibodies Online, Germany). The absorbance of each well was measured using a micro-ELISA reader (Multiscan MK3; Thermo Labsystems, Finland) at 450 nm. Then, the amount of BDNF, GDNF, VEGF, and NT-3 secreted by SCs was normalized to cell numbers in each group.

### Statistical analysis

All data presented here are expressed as means  $\pm$  standard error of the mean (SEM). The data were analyzed using one-way analysis of variance with SPSS 13.0 software (SPSS, USA). Values of  $P < 0.05$  were considered statistically significant.

## Results

### SC survival under different intensities of PMF

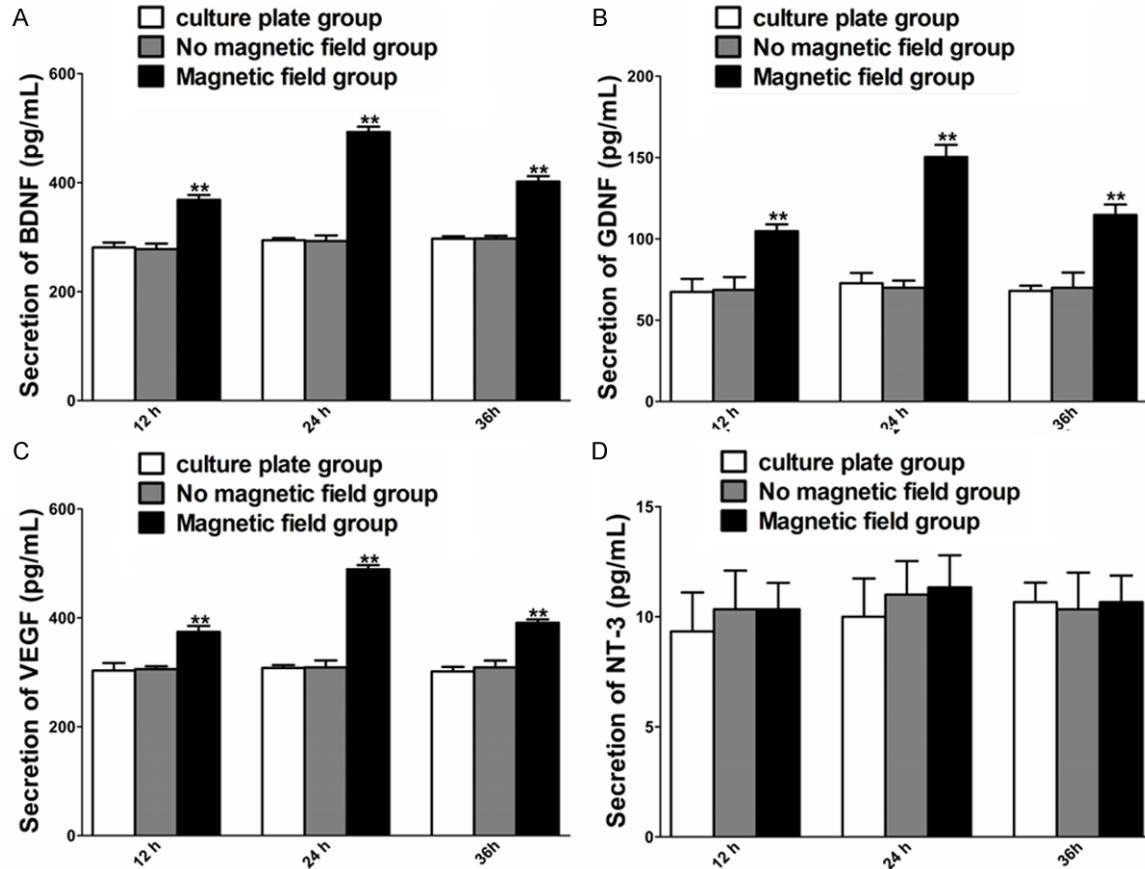
The effect of PMF on the survival of SCs was investigated by flow cytometry. As shown in **Figure 2A-G**, the apoptosis ratio of SCs after 24

hours PMF exposure was in a similar range to that without PMF exposure or at 0.5 mT, 1.0 mT, and 2.0 mT stimulation. When the PMF was increased to 5.0 mT and 10.0 mT, the percentage of apoptotic cells was significantly increased. Therefore, PMF at 2.0 mT was used in the remaining experiments for the observation that it caused no significant cell apoptosis.

### CCK-8 assay

Twenty-four hours after PMF exposure, the CCK-8 value of SCs less than 4 hours of PMF stimulation was significantly higher than that of fewer hours' stimulation. No significant difference was observed among stimulation under 4, 5, 6 and 8 hours. The CCK-8 value showed a similar outcome after 48 hours PMF exposure. Therefore, a 4-hour exposure time of PMF was applied in the remaining experiments (**Figure 2H**).

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**Figure 6.** Concentration of BDNF, GDNF, VEGF and NT-3 in each cultured group at different time points after PMF exposure. A-D: Secretion of BDNF, GDNF, VEGF and NT-3 in culture supernatants was determined at 12, 24 h and 36 h. Each test was repeated three times. All data were expressed as the mean  $\pm$  SEM. **\*\*** $P < 0.01$ .

### SC morphology under PMF

Twenty-four hours after PMF stimulation (2.0 mT), SCs exhibited a spindle feature which was in a similar shape to that under 0.5 and 1.0 mT, as well as those without PMF stimulation. When the PMF increased to 5.0 mT, the SCs were changed into round shape, losing its characteristic morphology. In addition, when the PMF increased to 10.0 mT, the SCs were almost broken with damaged membranes. The SEM results were consistent with the apoptosis assay (Figure 3).

### EdU-labeling assay

The cell proliferation was quantified by an EdU-labeling assay. Twelve hours after PMF exposure, the EdU-labeling index of SCs was significantly higher than the culture plate group and the no magnetic field group, respectively. The EdU-labeling index of SCs was in a similar range

to that of the other two groups after 24 hours (Figure 4).

### Expression of regeneration-related genes

The effect of PMF on expression of BDNF, GDNF, VEGF, and NT-3 of SCs was examined by RT-PCR 12 and 24 hours after PMF exposure. Under PMF stimulation, the mRNA levels of BDNF, GDNF and VEGF were higher than that without PMF at 12 and 24 hours. The NT-3 mRNA level at 12 and 24 hours was in a similar range to that without PMF (Figure 5).

### Secretion of regeneration-related protein

The effect of PMF on the secretion of BDNF, GDNF, VEGF and NT-3 was tested 12, 24 and 36 hours after PMF stimulation. Under PMF exposure, the secretion of BDNF, GDNF and VEGF was higher than that without PMF at 12, 24 and 36 hours (Figure 4E-G). The secretion of



NT-3 at 12, 24 and 36 hours was in a similar range to that without PMF (Figure 6).

### Discussion

With its convenient and practical property, PMF is identified as an ideal option that can be used easily in patients with nervous system injuries. Until now, several lines of evidence have demonstrated that PMF plays an important role in nerve regeneration [13, 14]. Despite PMF has been shown promising in the stimulation of axonal regenerative processes, the underlying cellular and molecular mechanism is still unclear. On the other hand, SCs can be activated to expand the production of neurotrophic factors in response to various external stimuli. In this field, we have previously proven that electrical stimulation is capable of promoting SCs neurotrophic function [15]. Considering the close relationship between electrical currents and magnetic field, we hypothesized that controlled PMF could activate SCs to enhanced biological function, which is thought to be beneficial for nerve regeneration.

To our knowledge, this study is the first report addressing the application of PMF in the activation and functional influence of SCs *in vitro*. Here, we found that PMF was capable of stimulating SCs to enhanced viability and biological properties. A magnetic field (50 Hz, 2.0 mT) was detected to improve viability and proliferation of SCs with almost no impact on apoptosis. Furthermore, we demonstrated that neurotrophic factors were up-regulated by PMF in SCs. These findings might shed a light on the potential utilization of PMF in nerve regeneration via SCs activation.

Different intensities of PMF have been used in the studies of biological properties in various cell types [16, 17]. In the present study, we applied a range of magnetic gradients to detect an optimal intensity. We found that 2.0 mT was the maximum intensity that promoted proliferation and caused relatively little apoptosis in SCs. Higher magnetic gradients were found to cause dramatically increased apoptotic ratio, suggesting that high magnetic stimulation is detrimental for SCs proliferation. These data was confirmed by SEM analysis, which showed different morphology in the applied magnetic gradients. When SCs were subjected to lower magnetic gradients than 2.0 mT, the morpholo-

gy of SCs stayed unchanged. However, the SCs shrunk and broken membrane fragment was detected in higher magnetic gradients. It has been reported that long-term cultured SCs failed to support regeneration and neuronal survival, which might be attributable to the low survival rate of SCs [18, 19]. Our data suggested that 2.0 mT might be an optimal intensity to improve SCs proliferation with less detrimental effect, indicating that this magnetic gradient might be used in further SCs stimulation for sufficient nerve regeneration application.

SCs has been shown to be capable of enhancing nerve regeneration in both PNS and CNS [20]. It has been indicated that one of this beneficial effects is partly due to the synthesis and release of neurotrophic factors [21, 22]. However, SCs cultured *in vitro* was found to lose their neuroprotective effect with the reduction of neurotrophic factors. Therefore, we examined the neurotrophic factors level in SCs following PMF stimulation. We found that the expression of BDNF, GDNF and VEGF was up-regulated in gene level after PMF stimulation (2.0 mT). Moreover, their secretion was observed in the culture medium. BDNF has been shown to promote survival and outgrowth of motor neurons in both PNS and CNS [23]. GDNF is a classical factor that facilitates the survival, growth, and differentiation of motoneurons and central noradrenergic neurons [24]. Moreover, VEGF is an effective protein that support SCs proliferation and axonal outgrowth [25]. Therefore, our study showed that the simultaneously increased expression of these factors may help to establish a supportive environment for nerve regeneration. On the other hand, it has been demonstrated that PMF can regulate neurotrophic factor activity and levels in neurons [26, 27]. However, the underlying mechanism is unclear. Our results suggested that the PMF-induced secretion of neurotrophic factors in SCs and their crosslink with neurons might contribute to this phenomenon. Interestingly, we found that the expression of the neurotrophic factors achieved the highest level at 24 h and decreased over time afterwards. This information suggests that PMF exerted a delayed function on SCs in neurotrophic factors secretion and provides information in therapeutic time window for further PMF application clinically.

Notwithstanding our study deepen the understanding of SCs in PMF stimulation; we acknowl-

edge that the mechanism by which PMF regulates the functions of SCs is unclear. PMF has been shown to affect cell in metabolism activation, mitochondrial membrane potential and ATP synthesis in different cell types [28]. In addition, it has been noted that PMF plays an important role in Ca<sup>+</sup> flux, which is thought to crucially participate in nerve system [29, 30]. However, whether these were involved in the PMF-mediated effect on SCs is still unclear. Further studies are needed to elucidate the coupling process between the PMF energy and conformational changes in biomolecules and how the “electromagnetic” information transfers to certain signaling pathways.

In conclusion, the current study provides evidence in the influence of PMF on SCs proliferation and function for the first time. We found the viability and biological properties of SCs were enhanced by PMF with up-regulated neurotrophic factors secretion. Consequently, PMF might be used as an activator in further application of SCs for nerve regeneration.

### Acknowledgements

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### Disclosure of conflict of interest

None.

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