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# REGIONAL VARIATION OF THE INWARDLY RECTIFYING POTASSIUM CURRENT IN THE CANINE HEART AND THE CONTRIBUTIONS TO DIFFERENCES IN ACTION POTENTIAL REPOLARIZATION

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# Abstract

**Background**—The inward rectifier potassium current,  $I_{K1}$ , contributes to the terminal phase of repolarization of the action potential (AP), as well as the value and stability of the resting membrane potential. Regional variation in  $I_{K1}$  has been noted in the canine heart, but the biophysical properties have not been directly compared. We examined the properties and functional contribution of  $I_{K1}$  in isolated myocytes from ventricular, atrial and Purkinje tissue.

**Methods and Results**—APs were recorded from canine left ventricular midmyocardium, left atrial and Purkinje tissue. The terminal rate of repolarization of the AP in ventricle, but not in Purkinje, depended on changes in external  $K^+$  ( $[K^+]_0$ ). Isolated ventricular myocytes had the greatest density of  $I_{K1}$  while atrial myocytes had the lowest. Furthermore, the outward component of  $I_{K1}$  in ventricular cells exhibited a prominent outward component and steep negative slope conductance, which was also enhanced in 10 mM  $[K^+]_0$ . In contrast, both Purkinje and atrial cells exhibited little outward  $I_{K1}$ , even in the presence of 10 mM  $[K^+]_0$ , and both cell types showed more persistent current at positive potentials. Expression of Kir2.1 in the ventricle was 76.9-fold

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**Conclusions**— $I_{K1}$  and Kir2 subunit expression vary dramatically in regions of the canine heart and these regional differences in Kir2 expression likely underlie regional distinctions in  $I_{K1}$  characteristics, contributing to variations in repolarization in response to in  $[K^+]_0$  changes.

#### **Keywords**

ventricle; Purkinje; electrophysiology; atria; potassium channel

# 1. INTRODUCTION

Repolarization of the cardiac action potential (AP) is controlled by several voltagedependent K<sup>+</sup> currents. In the canine ventricle, four K<sup>+</sup> currents play important roles in controlling the cardiac action potential duration<sup>1–5</sup>: (i) a Ca<sup>2+</sup>-independent transient outward K<sup>+</sup> current ( $I_{to1}$ ) (in contrast to the Ca<sup>2+</sup>-dependent current,  $I_{to2}^{-6}$ ); (ii) a rapid and slow delayed rectifier K<sup>+</sup> current ( $I_{Kr}$  and  $I_{Ks}$ , respectively) and (iii) an inwardly rectifying K<sup>+</sup> current ( $I_{K1}$ ).  $I_{K1}$  has been identified in the myocardium of most mammalian species (for review see <sup>7, 8</sup>), but the density of  $I_{K1}$  among different species as well as among different cardiac tissue types is highly variable <sup>9–11</sup>. Previous studies have shown that the  $I_{K1}$  density is large in the ventricle, small in atria and largely absent in sinoatrial node <sup>12–14</sup>.

The salient features of  $I_{K1}$ , such as its negative slope conductance and the crossover of the I-V relation upon increases in external K<sup>+</sup> have long been identified<sup>15</sup>, and their physiological significance has been extensively studied <sup>16, 17</sup> (see Trautwein<sup>18</sup>). The strong rectification of  $I_{K1}$  is the result of voltage-dependent block by intracellular Mg<sup>2+ 19</sup> and polyamines <sup>20</sup>, primarily spermine and spermidine<sup>21</sup>. The channels that carry cardiac  $I_{K1}$  belong to the Kir2.x subfamily, namely Kir2.1 through Kir2.3<sup>8, 22</sup>. Each Kir2 channel is composed of four subunits which form monomeric channels, although native  $I_{K1}$  channels likely exist as heteromultimers<sup>23–25</sup>. When expressed in mammalian cells, all Kir2.x channels exhibit properties that are similar to native  $I_{K1}$ <sup>10</sup>, although each Kir2.x channel has a different current profile<sup>10</sup>, reflecting the differences in polyamine induced rectification<sup>26</sup>. For example, Kir2.1 and Kir2.2 channels show a prominent negative slope conductance and rectify 'completely' above -20 mV, while Kir2.3 channels pass significant current at these potentials <sup>10</sup>. The distinct properties of different Kir2.x channels have been implicated in regional and species differences in  $I_{K1}$ , as observed in sheep heart where the incomplete rectification of  $I_{K1}$  in atria is attributed to the predominant expression of Kir2.3<sup>10</sup>. Furthermore, individual reports 27-29 indicate the  $I_{K1}$  in canine heart appears to differ among ventricular, Purkinje and atrial myocytes. However, IK1 has never been directly compared between these three tissue types.

Since the canine heart is used as both a model for safety pharmacology and to stimulate cardiac electrophysiological diseases, such as atrial fibrillation<sup>30</sup>, Long QT<sup>31, 32</sup> and Brugada Syndromes<sup>33</sup>, the present study compares the electrophysiological and molecular constituents of  $I_{K1}$  in single myocytes isolated from the canine heart. Here we show that the

maximal rate of repolarization of the AP strongly depends on external  $K^+$  ([ $K^+$ ]<sub>o</sub>) in ventricle, but not in Purkinje. We also show that the biophysical and molecular properties of  $I_{K1}$  differ between ventricular, Purkinje and atrial cells. While Kir2.1 is highly expressed in the ventricle, the other putative Kir2 subunits, Kir2.2 and Kir2.3, were more equally distributed in the three cardiac tissue types. Taken together, our data suggest that prominent differences in the expression Kir2 subunits and the characteristics of  $I_{K1}$  contribute to the differences of AP repolarization and its response to [ $K^+$ ]<sub>o</sub> among atrial, ventricular and Purkinje tissues.

# 2. MATERIALS AND METHODS

#### 2.1 Isolated tissue action potential recordings

This investigation conformed to the Guide for the Care and Use of Laboratory Animals published by the National Institutes of Health (Eighth Edition, 2011), and all protocols were approved by the Animal Care and Use Committee at the Masonic Medical Research Laboratory, and hearts from 39 total canines were used in the study. The mongrel canines of either sex were anti-coagulated with heparin and anesthetized with pentobarbital (30-35 mg/kg, i.v.). The chest was opened via left thoracotomy, the heart excised, placed in a cardioplegic solution (4 °C-Tyrode's solution with 12 mM  $[K^+]_0$ ). Left ventricle midmyocardial (Mid-LV) (approximately  $1.0 \times 0.5 \times 0.1$  cm), left atrial tissue and Purkinje tissue were isolated from hearts. The preparations of ventricle consisted of dermatome shavings (Davol Simon Dermatome Power Handle 3293 with cutting head 3295, Cranston, R.I.) obtained from the left ventricular free wall. The tissues were superfused with oxygenated (95% O<sub>2</sub>/5% CO<sub>2</sub>) Tyrode's solution maintained at 36–37 °C. The composition of the Tyrode's solution was (in mM): NaCl 129, KCl 5.4, NaH<sub>2</sub>PO<sub>4</sub> 0.9, NaHCO<sub>3</sub> 20, CaCl<sub>2</sub> 1.8, MgSO<sub>4</sub> 0.5, and D-Glucose 5.5; pH=7.4. All preparations were allowed to equilibrate until the action potentials achieved steady-state (usually 3–4 hours). The tissues were stimulated at basic cycle lengths (BCL) ranging from 1000 and 2000 ms using rectangular stimuli (2-5 ms duration, 2-2.5 times diastolic threshold intensity) delivered through thin silver bipolar electrodes. Transmembrane action potentials were recorded from the two tissues simultaneously using glass microelectrodes filled with 2.7 M KCl (10-30 Mohms: DC resistance) connected to a high input-impedance amplification system (Electro 705 Electrometer, World Precision Instruments). The signals were digitized (model 1401 AD/DA system, Cambridge Electronic Designs [C.E.D.]) and analyzed (Spike 2 acquisition and analysis module, C.E.D.).

#### 2.2 Isolation of canine cardiomyocytes

Left ventricular or left atrial preparations were dissected and cells dissociated as described previously<sup>3</sup>. For isolation of mid-left ventricular cells (Mid-LV), thin slices of tissue from the Epi and Endo were shaved from the wedge using a dermatome to expose the midmyocardium, and the midmyocardium was subsequently shaved and removed for further digestion. For atrial cells, the pectinate and appendage muscle were isolated. The tissue was then agitated in the enzyme solution at 37 °C for cell dissociation. Canine Purkinje cells were isolated using techniques previously described <sup>34</sup>. Briefly, Purkinje fibers from both ventricles were dissected out and placed in a small dish. Fibers were then subjected to

enzyme digestion with the nominally  $Ca^{2+}$ -free solution supplemented with 1.0 mg/ml collagenase (Type II, Worthington) and 30 mM 2,3-butanedione monoxime (Sigma-Aldrich) at 36 °C. Dissociation of cells from the fibers was aided by agitation of the enzyme solution with a small stir bar. Periodically, enzyme solution containing Purkinje cells in suspension was removed and added to a modified storage solution. Fresh enzyme solution was added to the undigested Purkinje fibers to maintain a volume of about 2 ml. Digestion of the Purkinje fibers into individual myocytes typically required 15–35 min. The cells were kept in the 0.1 mM Ca<sup>2+</sup> solution at room temperature until use.

#### 2.3 Single cell electrophysiology

Voltage-clamp recordings were made using a MultiClamp 700A amplifier and MultiClamp Commander (Molecular Devices, Foster City, CA). Patch pipettes were fabricated from borosilicate glass capillaries (1.5 mm O.D., Fisher Scientific, Pittsburgh, PA). The pipettes were pulled using a gravity puller (Narishige, Tokyo, Japan) and the pipette resistance ranged from 1–3 M $\Omega$ . The cardiomyocytes were superfused with a HEPES Buffer of the following composition (mM): NaCl 135, KCl 5.4, MgCl<sub>2</sub> 1.0, CaCl<sub>2</sub> 1.8, HEPES 10, NaH<sub>2</sub>PO<sub>4</sub> 0.33 and D-Glucose 10, pH adjusted to 7.4 with NaOH. The patch pipette solution (K<sub>INT</sub>) had the following composition (mM): K-aspartate 125, KCl 10, MgCl<sub>2</sub> 1.0, EGTA 5, MgATP 5, HEPES 10, NaCl 10, pH=7.2 with KOH. All experiments were performed at 37  $^{\circ}$ C. After a whole-cell patch was established cell capacitance was measured by applying -5mV voltage steps. Series resistance was compensated to 60–70%. All analog signals were acquired at 10-50 kHz, filtered at 4-6 kHz and digitized with a Digidata 1322 converter (Molecular Devices).  $I_{K1}$  currents were elicited by step increments of 10 mV between -120 and 0 mV from a holding potential of -80 mV and currents were evaluated at the end of the 500-ms step pulse, in the absence and presence of 100  $\mu$ M BaCl<sub>2</sub>, where  $I_{K1}$  was considered to be the  $Ba^{2+}$ -sensitive current. For analysis of kinetics of  $I_{K1}$  activation, hyperpolarizing steps down to -110 mV were applied to the cells in 10 mV decrements from a holding potential of -30 mV. The P/5 method was used to subtract the capacitance transient from fast activating  $I_{K1}$  currents, or K<sup>+</sup>-free HEPES buffer was rapidly eliminate  $I_{K1}$  in order to isolate it from the capacitance currents, as similarly performed in Panama et al<sup>11</sup>. For action potential clamp experiments, pre-recorded action potentials from ventricular, Purkinje and atrial myocytes served as voltage waveforms. Action potentials of single cells were recorded using whole cell patch pipettes. The resistance of the electrodes was 1-3 Mohm when filled with the K<sub>INT</sub> pipette solution. Action potentials were elicited using a 3 ms current pulse at 120% threshold amplitude.

### 2.4 Electronic Expression of IK1

The electronic expression of  $I_{K1}$  was performed in the whole cell configuration, similarly as previously described<sup>35</sup> using a Cybercyte system (Cytocybernetics Inc., Pendleton, NY).  $I_{K1}$  I-V relations for Mid-LV and Purkinje were fit with the following function:

$$I_{\scriptscriptstyle K1} {=} G \times \left( g_{\scriptscriptstyle K1} \times \frac{V_m {-} V_{\scriptscriptstyle rev}}{1 {+} \exp \left( k^{-1} \times \left( V_m {-} V_{\frac{1}{2}} \right) \right)} {+} g_{linear} \times \left( V_m {-} V_{\scriptscriptstyle rev} \right) \right)$$

Cells were bathed in Tyrode solution and experiments were conducted at room temperature for increased patch stability. Model parameters were fit by adjusting g,  $g_{K1}$ ,  $g_{linear} V_{rev}$ ,  $V_{1/2}$ , and k to experimental data manually using a visual goodness of fit procedure, comparisons of data and model currents are given in the Supplementary figure 1S. Subtraction of currents was obtained by using a negative conductance using a model for  $I_{K1}$ from the 5.4 mM ventricular parameters, similar to that used for other ionic current cancelling procedures<sup>36–38</sup>. Differing  $I_{K1}$  models were simulated on a separate computer and added in as a command current<sup>35</sup>.

#### 2.5 Analysis of mRNA expression

Tissue was washed in Tyrode's solution and immediately frozen in liquid nitrogen before storage at -80 °C. For RNA isolation, the tissue was disrupted with a mortar and pestle and then homogenized with a sterile syringe and needle. After homogenization, the RNeasy Fibrosis Tissue kit was used to isolate the RNA (Qiagen). A NanoDrop<sup>®</sup> spectrophotometer (Thermo Scientific) was used to quantify RNA samples. Samples were treated with DNase I to remove contaminating genomic DNA. The Superscript<sup>TM</sup> III Reverse Transcriptase kit (Life Technologies) approach was used to synthesize cDNA from 1–5 µg of RNA, exactly according to the manufacturer protocol. cDNA synthesis reactions were run without reverse transcriptase (-RT) showed no amplification (Supplementary Figure 2S), indicating genomic DNA was not affecting the quantification.

Both SYBR green<sup>®</sup> and TaqMan systems (Life Technologies) used.

Probes sets:

KCNJ2- Cf03022918\_s1 - TaqMan FAM (Life Technologies)

KCNJ12- Cf02713141\_s1 - TaqMan FAM (Life Technologies)

*KCNJ4* – Forward 5' GGACTTTGAGATCGTGGTCA 3'; Reverse 5' CGCGAGTAGTCCACCTTGTA 3' – SYBR Green

*18S* rRNA- Forward 5' TCCGACTTTCGTTCTTGATTAATG 3'; Reverse 5' CGCCGCTAGAGGTTGAAATTC 3' – SYBR Green

Maxima SYBR Green and Maxima Probe ROX master mixes (Thermo Scientific) were used for SYBR Green oligos and TaqMan probes, respectively, in the amplification reaction. A Real-Time thermal cycler PCR System 7000 (Life Technologies) was used to amplify the particular gene amplicons from the cDNA. All no template control wells, containing the reaction mix but water instead of cDNA, were negative in all PCR runs. The mRNA levels were referenced to 18S rRNA. For relative quantification, the Ct method was used <sup>39</sup>.

### 2.6 Analysis of polyamine concentrations

Tissues were washed in HEPES Buffer, gently blotted dry and weighed. The samples were minced in RNase free water (2 ml/gram of tissue) and homogenized in a 50 ml conical tube, followed by a spin for 2 minutes at 3000g. The supernatant was transferred to a 1 ml tube and centrifuged for 15 minutes at 11,500g. Exactly 100  $\mu$ l of supernatant was removed for later protein quantification. The remaining supernatant was transferred to a clean tube and

perchloric acid was added to make a 0.2 N final concentration. Following thorough mixing, the sample was incubated for 10 minutes at room temperature. After, the sample was centrifuged for 10 minutes at 11,500g. The supernatant was removed and stored at -80 °C. Polyamines spermine, spermidine and putrescine were quantified by HPLC, as described previously<sup>40</sup>.

#### 2.7 Data and statistical analysis

Data are presented as mean  $\pm$  SEM. Statistical comparisons were made using paired or unpaired Student's t-test when appropriate. A one-way ANOVA was used for multiple comparisons, and p<0.05 was considered statistically significant (\*). The V<sub>min</sub> was obtained finding the minimum of derivative (dV/dt) of the AP, excluding the first 50 ms after AP upstroke. For atrial cells, the dV/dt was continuously decreasing, and thus a reliable minimum could not be obtained.

# 3. RESULTS

#### 3.1 Action potential recordings from different regions of the canine heart

The canine heart is used as a model in pharmacological safety testing and experimental cardiac electrophysiology, and extracellular K<sup>+</sup> ([K<sup>+</sup>]<sub>o</sub>) is often varied to mimic pathophysiological hypo- or hyperkalemic states. We recorded APs from Mid-LV, atrial and Purkinje tissue at a pacing rate of 0.5 Hz (Figure 1) under different concentrations of [K<sup>+</sup>]<sub>o</sub>. As expected, APs in all tissue types decreased with an increase in [K<sup>+</sup>]<sub>o</sub> from 5.4 to 10 mM and increased in the presence of 2 mM [K<sup>+</sup>]<sub>o</sub> (p<0.05) in addition to hyperpolarization of the resting membrane potential, as previously noted<sup>41</sup> (Table 1). The beat to beat variability was minimal, as shown in Supplementary Figure 3S. The V<sub>min</sub>, which is an indicator of the maximal terminal rate of repolarization, also increased with elevations [K<sup>+</sup>]<sub>o</sub> for Mid-LV but not Purkinje tissue (Figure 2A). V<sub>min</sub> for atria could not be reliably measured since V<sub>min</sub> was continuously decreasing. Similar differences in V<sub>min</sub> were obtained for a pacing rate of 1 Hz (-1.39 ± 0.19 and -0.71 ± 0.11 V/s for Mid-LV and Purkinje, respectively (n=5 for each; p<0.05) (Supplementary Table 1S).

#### 3.2 Action potential recordings from single cells

To compare the AP changes observed in tissue to those of isolated myocytes, we recorded from Mid-LV, atrial and Purkinje cells at a pacing rate of 0.5 Hz. Figure 1B shows representative AP records obtained from a Mid-LV cell when the  $[K^+]_o$  was again varied from normal (5.4 mM) to 2 mM and then to 10 mM, as well as AP recordings from a Purkinje and atrial cell, respectively, following the same changes in  $[K^+]_o$ . As seen with tissue experiments, Purkinje cells exhibited a more prominent phase 1 repolarization and had a longer AP. Following exposure to 10 mM  $[K^+]_o$ , the APD of all cell types markedly shortened; however, the degree of APD shortening was greatest in Purkinje cells, as seen in tissue experiments. Exposure of all cell types to 2.0 mM  $[K^+]_o$  resulted in prolongation of the APD. Importantly, like that of tissue, the V<sub>min</sub> strongly changed with  $[K^+]_o$  in Mid-LV myocytes but not for Purkinje (Fig. 2B). Taken together, the AP parameters from the isolated myocytes paralleled those from tissue, both of which showed stark differences in the terminal phase of repolarization.

#### 3.3 IK1 recordings from different regions of the canine heart

The AP data in both myocytes and tissue showed that the rate of terminal repolarization is different in the three cell types. Since  $I_{K1}$  strongly contributes to the late phase of repolarization of the AP and shifts proportionally with the  $[K^+]_0$  we hypothesized that the magnitude, and perhaps the biophysical properties, of  $I_{K1}$  is different in each cell type. We measured  $I_{K1}$  by application of square-wave voltage-clamp pulses (Figure 3). Large steady-state inward currents could be observed in Mid-LV cells, whereas intermediate sized currents were found in Purkinje cells in response to hyperpolarizing voltage, and currents were smallest in atrial cells. Analysis of the I-V relation shows that  $I_{K1}$  is largest in ventricle and smallest in atrial ( $-26.7 \pm 2.8, -9.0 \pm 3.4, \text{ and } -2.6 \pm 0.32 \text{ pA/pF}$  at -120 mV for ventricular, Purkinje, and atrial, respectively (p < 0.05)). In addition, the outward component of Mid-LV  $I_{K1}$  showed a prominent negative slope and rectified 'completely,' meaning that only a very small current persisted at depolarized potentials ( $0.26 \pm 0.14 \text{ pA/pF}$  at 0 mV for Mid-LV). On the other hand, the outward component of  $I_{K1}$  in Purkinje and atrial showed a weak negative slope and persistent current at depolarized potentials ( $(1.4 \pm 0.79 \text{ and } 0.5 \pm 0.14 \text{ pA/pF}$  at 0 mV for Purkinje and atria, respectively).

#### 3.4 IK1 in response to changes in [K<sup>+</sup>]o

Given the differences in  $I_{K1}$  rectification among the three cell types we wondered how  $I_{K1}$  would change with changes in  $[K^+]_o$ . Whole cell currents were activated by a step to -10 mV followed by a 500-ms ramp to -120 mV from a holding potential of -80 mV. No blockers were added to the recording solution as the activation pulse would activate and eliminate Na<sup>+</sup> ( $I_{Na}$ ) and Ca<sup>2+</sup> currents ( $I_{Ca}$ ). Similar to results using square wave pulses, the inward current at the end of the ramp was largest in Mid-LV cells, intermediate in Purkinje cells and smallest in atrial cells (Figure 4A). Furthermore, increasing  $[K^+]_o$  increased the magnitude of inward  $I_{K1}$  in all 3 cell types. The lower panels (Figure 4B) show an enlargement of the outward component of  $I_{K1}$ . In Mid-LV cells, changing  $[K^+]_o$  resulted in an increase in magnitude of  $I_{K1}$ , as previously described <sup>7, 17, 42</sup>. In contrast, Purkinje and atrial cells showed little increase in outward  $I_{K1}$  in response to the ramp protocol.

#### 3.5 Kir2 mRNA and polyamine analysis in different regions of the canine heart

Previous studies have shown that homomeric channels formed by Kir2.1, 2.2 and 2.3 subunits each have different current profiles and polyamine induced rectification properties  $^{26, 43}$ . The striking differences in I-V relations of  $I_{K1}$  seen in ventricular, Purkinje and atrial myocytes prompted us to investigate the differences in Kir2 subunit mRNA expression, as well as the polyamine concentrations, between the three regions. Kir2.1, 2.2 and 2.3 subunits were all expressed in the three regions, but the expression of Kir2.1 in the left ventricle was 76.9-fold higher than in atria (p<0.001) and 5.8-fold higher than in Purkinje (p<0.05) (Fig. 5). The expression of Kir2.2 and Kir2.3 subunits was more evenly distributed in Purkinje and atria. On the other hand, total polyamine concentrations were not different between ventricle and atria for spermine, spermidine and putrescine (Table 2). Polyamines in Purkinje tissue could not be measured due to small tissue amounts.

#### 3.6 Kinetics of activation in canine cardiomyocytes

The weak negative slope seen in the I-V relations from Purkinje and atrial myocytes is reminiscent of the I-V relations from whole-cell recording of Kir2.3 channels expressed in HEK293 cells <sup>26, 43</sup>. We next determined whether the rate of  $I_{K1}$  activation (unblocking of polyamines) was different between the three cell types to assess the contribution of Kir2.3 subunits, which have slower activation rates. Hyperpolarizing steps were applied to the cells in 10 mV steps from a holding potential of -30 mV. As described previously<sup>11, 20, 26</sup>, a double exponential was needed to fit the two components of activation: 1) a quasi-instantaneous activation and 2) slower activation which results from time-dependent polyamine unblock from the channels<sup>20</sup> (Figure 6). Ventricular myocytes had the fastest rate of time-dependent activation at -110 mV (1.56 ± 0.15 ms, n=7) while atrial myocytes had the slowest (13.1 ± 4.7 ms, n=5) (p<0.05). Purkinje (2.24 ± 0.14 ms, n=9) myocytes had  $I_{K1}$  which was slower (p<0.01) than that of ventricle.

#### 3.7 Action potential clamp studies

Given the large differences in  $I_{K1}$  between the cell types, we evaluated the functional contribution of  $I_{K1}$  to the AP using the action potential clamp technique (Figure 7). Previously recorded ventricular, Purkinje and atrial cell action potentials served as the templates for the AP clamp experiments (Figure 7A). A train of 10 pulses were applied to the cell at a rate of 1 Hz in the absence and presence of 100  $\mu$ M Ba<sup>2+</sup>. Subtraction of the Ba<sup>2+</sup> trace from the control trace resulted in the Ba<sup>2+</sup>-sensitive difference current shown in Figure 7B. In LV-Mid cells, the outward component of  $I_{K1}$  in contributes 366.3±20.7 pA (n=8) or 1.86±0.05 pA/pF when normalized for cell size. In Purkinje cells,  $I_{K1}$  was 140.1±30.2 pA (n=5) or 0.62±0.11 pA/pF when normalized for cell size. In atrial cells,  $I_{K1}$  was 64.3±11.3 pA (n=7) or 0.48±0.06 pA/pF when normalized for cell size. Results show that while  $I_{K1}$  contributes predominantly to final portion of phase 3 in the cell types the profile of the outward component of  $I_{K1}$  was dramatically different. In atrial cells  $I_{K1}$  is likely influencing the AP at more positive potentials, because of the persistent  $I_{K1}$  outward current seen more depolarized voltages, which is consistent with the model proposed in Dhamoon et al<sup>10</sup> (see Discussion).

### 4. DISCUSSION

While the hallmark features of cardiac  $I_{K1}$  have been well characterized, such as the negative slope and 'crossover' effect upon increases  $[K^+]_0$  (for review see references 44, 45 41), regional differences in  $I_{K1}$  have been noted in canine and other species. For example, we previously observed minimal changes in outward  $I_{K1}$  rabbit Purkinje myocytes in response to changes in  $[K^+]_0^9$ . Furthermore, atrial-ventricular differences in  $I_{K1}$  have been noted in mouse<sup>11</sup>, sheep<sup>43</sup> and human<sup>46</sup>. Since the canine heart is used as model for both safety pharmacology and for studying electrophysiological disorders, such as atrial fibrillation, Long QT<sup>31, 32</sup> and Brugada Syndromes<sup>33</sup>, it is important to fully understand the regional differences in  $I_{K1}$ . As such, the novel findings of our study are as follows: 1) the outward currents of  $I_{K1}$ , which until now have not been directly compared in canine, are different between ventricular, Purkinje and atrial myocytes, 2) the outward component of current increased with  $[K^+]_0$  in ventricle, while it did not in Purkinje or atria, 3) the kinetics

of activation of  $I_{K1}$  is slower in Purkinje and atrial myocytes compared with those ventricle, and **4**) the contribution of  $I_{K1}$  is not limited to the terminal phase of repolarization in atrial myocytes (Figure 7).

Additionally, we found differences in the terminal phase of repolarization  $(V_{min})$  in APs from canine ventricular and Purkinje tissue and myocytes at both normal and different  $[K^+]_0$ (Table 1), and  $V_{min}$  changed with  $[K^+]_0$  in ventricle but not in Purkinje (Fig. 2). We hypothesized that the shape and the lack of increase in the outward component of  $I_{K1}$  in Purkinje, in response to increases in  $[K^+]_0$  (Fig. 4), could account for the nearly constant V<sub>min</sub> despite increase of [K<sup>+</sup>]<sub>0</sub> in this cell type/tissue. In support of this hypothesis, we synthetically applied different  $I_{K1}$  I-V relations<sup>35</sup> to Mid-LV cells and measured AP, using electronic expression of  $I_{K1}$ . Here we electronically subtracted the native  $I_{K1}$  and "expressed" our own synthetic  $I_{K1}$  which was modelled from previous Mid-LV  $I_{K1}$ recordings at different  $[K^+]_0$ . This technique gives us the ability to modulate only  $I_{K1}$ without changing other currents. Figure 8 shows the data for Vmin, MDP, APD50 and APD90 for Mid-LV cells under the following conditions: Control (Con), subtracted  $I_{K1}$  $(-I_{K1})$ , the  $I_{K1}$  I-V for Mid-LV at 5.4 mM K<sup>+</sup> (+ $I_{K1}$  5.4 mM K<sup>+</sup>), the  $I_{K1}$  I-V for Mid-LV at 10 mM K<sup>+</sup> ( $+I_{K1}$  10 mM K<sup>+</sup>) and the  $I_{K1}$  for Purkinje at 5.4mM K<sup>+</sup> ( $+I_{K1}$  Purkinje). The  $V_{min}$  increased from  $-0.62 \pm 0.01$  V/s in  $-I_{K1}$  to  $-1.39 \pm 0.2$  V/s and -2.35+0.23 V/s for + $I_{K1}$  5.4 mM K<sup>+</sup> and + $I_{K1}$  10 mM K<sup>+</sup>, respectively (p<0.01). Consistent with Fig. 2, the Purkinje V<sub>min</sub> was smaller than that of Mid-LV at 5.4 mM. The MDP was also more negative for  $+I_{K1}$  5.4 mM K<sup>+</sup> compared with  $+I_{K1}$  10 mM K<sup>+</sup>, and with APD90 was increased with  $I_{K1}$  subtracted. Overall, the data show the cell specific  $I_{K1}$  properties are likely responsible for Purkinje and ventricular differences in the AP terminal rate of repolarization, as assessed by V<sub>min</sub>.

Differences in Kir2.x subunit expression likely contribute to the regional variations in  $I_{K1}$ . We<sup>26</sup> and others<sup>10, 47</sup> previously showed that Kir2.x have different sensitivities to polyamines and have different rectification profiles with Kir2.1 and Kir2.2 channels passing outward current with a 'steep' negative slope and rectifying completely. On the other hand, the outward current profile from Kir2.3 channels has a more 'shallow' negative slope and does not rectify completely at positive potentials. In addition, under whole-cell recording conditions Kir2.1 outward currents increase with  $[K^+]_0$  while currents from Kir2.3 channels do not show increases in outward current with  $[K^+]_0$ . These distinct properties of Kir2 channels have been attributed to atrial-ventricular difference in  $I_{K1}$ . For example, Dhamoon et al<sup>48</sup> showed that  $I_{K1}$  did not rectify completely in sheep atrial myocytes, which expressed Kir2.3 subunits predominantly, and the outward component of  $I_{K1}$  did not increase with elevations in  $[K^+]_0$ . However, in guinea pig atrial myocytes (which strongly express Kir2.1)  $I_{K1}$  showed an increase in outward currents in 10 mmol/L  $[K^+]_0$ .

Similar to Dhamoon et al, we found that the outward component of  $I_{K1}$  in Mid-LV myocytes showed a prominent negative slope and rectified 'completely,' whereas the outward component of  $I_{K1}$  in Purkinje and atrial showed a weak negative slope and persistent current at depolarized potentials. In addition, elevating  $[K^+]_0$  in Mid-LV myocytes resulted in an increase in magnitude of outward  $I_{K1}$  and a 'cross-over' effect, as previously described <sup>7, 17, 42</sup>, but Purkinje and atrial cells showed little, if any, increase in outward  $I_{K1}$ .

The mRNA expression of Kir2.1 in Mid-LV was 76.9-fold higher than that of atria and 5.8fold higher than that of Purkinje. The large expression of Kir2.1 in the Mid-LV is consistent with steep negative slope profile of  $I_{K1}$  and the increase in current with elevations in  $[K^+]_0$ . On the other hand, mRNA of Kir2.2 and Kir2.3 subunits were more evenly distributed in Purkinje and atria. Therefore, we hypothesized that Kir2.3 channels are playing a greater role in Purkinje and atria since  $I_{K1}$ 's properties in these cell types are reminiscent of those seen from Kir2.3 current (i.e. lack of strong negative slope in the outward component and a lack of current increase with elevations in  $[K^+]_0$ ). To understand the functional role of Kir2.3 subunits in Purkinje and atria, we measured the kinetics activation in all three cell types. Kir2.3 channel currents activate more slowly than those of Kir2.2 and Kir2.1 channels <sup>26</sup>. The rate activation is proportional to the number of Kir2.3 subunits in a heterotetrameric channel<sup>11</sup>, and even the presence of one Kir2.3 subunit in a heteromeric channel (such as a Kir2.1–2.1–2.3 heterotetramer for example) slows activation<sup>11</sup>. Indeed the kinetics of activation was slower in Purkinje and atria when compared with Mid-LV, thus providing evidence for the role Kir2.3 subunits in generating distinct properties of  $I_{\rm K1}$  in these two cell types.

As shown above in the AP and  $V_{min}$  data, the regional variation in  $I_{K1}$  contributes to differences in rate of the late phase of repolarization of the AP. It also likely that regional variation in  $I_{K1}$  contribute to differences in arrhythmia susceptibility between the three cell/ tissue types. The data in Figure 7 show that while  $I_{K1}$  contributes predominantly to final portion of phase 3 in the cell types the profile of the outward component of  $I_{K1}$  is different in atrial cells, where  $I_{K1}$  contributes to the AP at positive potentials. Our experimental data largely agree with the model presented by Dhamoon<sup>49</sup>, which suggests that a myocyte with "Kir2.3-like" properties (i.e. shallow negative slope and persistent current) will contribute to the plateau phase of the AP, in addition to the late phase of repolarization. Furthermore, data from Pogwizd<sup>50</sup> established that a robust  $I_{K1}$  current can prevent the development of delayed afterdepolarizations by stabilizing the membrane potential. However, a diminished  $I_{K1}$  (in myocytes from failing hearts for example) is less able to mitigate spontaneous membrane depolarizations. It is important to note that canine differs somewhat from that of human. For example, Jost et al<sup>51</sup> shows that  $I_{K1}$  in ventricle is more than 2-fold larger in canine verses human, and provides evidence that IK1 plays a greater role in the repolarization reserve in canine compared with human. In contrast,  $I_{K1}$  densities from human failing heart are only moderately less than canine (-6 pA/pF for human<sup>52</sup> verses -9 pA/pF at -120 mV). How these differences affect repolarization reserve and arrhythmia propensity will have to be examined in further investigations.

Several limitations and considerations exist in our study. First, it is important to note that while the terminal rate repolarization is highly dependent on  $I_{K1}$ , the AP durations (APD50 and 90) in Purkinje still change with elevations in  $[K^+]_o$  despite the lack of change in outward current. This must be attributed to other  $K^+$  currents, such as  $I_{Kr}$ , which are changing with  $[K^+]_o$ . Second, we did not perform protein analysis of Kir2.x subunits, which would provide further validation of the subunit expression between the three cell types, although the results can be explained by mRNA measurements. Third, we did not record single-channels from myocytes, which we believe would be complicated, since Kir2

channels can have multiple sub-levels<sup>53</sup> and single-channel conductances are altered by the number and particular Kir2.x isoform in a heteromeric channel, as we have shown previously<sup>54</sup>. Finally, intracellular polyamines likely also contribute to the regional variation between cell types. Despite the lack of differences in total polyamine content between ventricle and atria (Table 2), it is within the realm of possibility that differences in free intracellular polyamines<sup>11</sup> exist, which are not reliably quantifiable in these conditions.

In conclusion,  $I_{K1}$  and Kir2 subunit expression vary dramatically in regions of the canine heart, suggesting tissue-specific differences of Kir2 isoforms. Differences in the expression and properties of  $I_{K1}$  contribute to tissue-specific difference in AP characteristics, namely the terminal rate of repolarization, and their response to pathophysiological factors including variations in plasma K<sup>+</sup> concentration. The mechanisms underlying tissue-specific differences in expression of in  $I_{K1}$  will need to be addressed in future studies.

# Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

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# Highlights

- *I*<sub>K1</sub> and Kir2 subunit expression vary dramatically in different regions of the canine heart.
- The rate of repolarization of the action potential changes with external K<sup>+</sup> concentration in ventricle but not in Purkinje.
- The contribution of  $I_{K1}$  is not limited to the terminal phase of repolarization in atrial myocytes.



# Figure 1. Representative action potentials from Mid-LV, Purkinje and atrial tissues and myocytes in different $[K^+]_0$ paced at 0.5 Hz

Action potentials for tissues (A) and myocytes (B) were characteristic of what has been previously observed. Several sweeps are shown for myocytes voltage clamp recordings.



Figure 2.  $V_{min}$  dependence on  $[\mathrm{K+}]_0$  in tissue and cardiac myocytes

**A.** Plot of  $V_{min}$  vs.  $[K^+]_0$ .  $V_{min}$  changes with  $[K^+]_0$  for ventricle but not Purkinje tissue. **B.**  $V_{min}$  vs.  $[K^+]_0$ .  $V_{min}$  changes with  $[K^+]_0$  for ventricle but not Purkinje myocytes. (n=5; N=2 hearts for Mid-LV; n=3; N=3 hearts for Purkinje).



Figure 3. Whole cell currents from Mid-LV, Purkinje and atria myocytes at physiological  $K^+$ A. Example current trances from Mid-LV, Purkinje and atria myocytes. Step increments of 10 mV between -120 and 0 mV from a holding potential of -80 mV B. Averaged current density vs. voltage plots for the Ba<sup>2+</sup>-sensitive currents for the three cell types. (*Insert*: Averaged current density for all the cell types plotted on the same graph). n=10, N=7 hearts for Mid-LV; n=4, N=3 hearts for Purkinje; n=9, N=2 hearts for atria;



# Figure 4. $I_{K1}$ currents in different $[K^+]_0$ from cardiac myocytes

Representative currents for the three cell types in the presence of different external  $K^+$  concentrations, 2, 5.4, 10 and 20 mM  $K^+$ . **A.** inward currents dramatically increase with elevations in  $K^+$ . **B.** the outward current component increases in Mid-LV cells with increasing  $K^+$ , but not in Purkinje and atrial cells.





The long horizontal bars represent the mean fold change and error bars denote the confidence interval (95%). The expression of Kir2.1 in the left ventricle was 76.9-fold higher than that of atria (p<0.001) and 5.8-fold higher than that of Purkinje (p<0.05).



Figure 6. Kinetics of activation (unblock) from Mid-LV, Purkinje and atrial myocytes Representative traces of  $I_{K1}$  in response to hyperpolarizing steps from Mid-LV, Purkinje and atrial myocytes, and double exponential fits are shown. At -110 mV slower tau values were  $1.56 \pm 0.15$  ms (n=7),  $2.24 \pm 0.14$  ms (n=9) and  $13.1 \pm 4.7$  ms (n=5), for Mid-LV, Purkinje and atria, respectively. N=3, 5 and 5 hearts for Mid-LV, Purkinje and atria, respectively.



Figure 7. Action potential clamp waveforms and  $I_{K1}$  in cardiac myocytes *Top*, previously recorded action potential waveforms from ventricular, Purkinje and atria myocytes were used as voltage protocols. *Bottom*, representative Ba<sup>2+</sup> sensitive currents.



#### Figure 8. Electronic Expression of different IK1 profiles in Mid-LV cells

**A.** Representative AP with different synthetic I-V relations of  $I_{K1}$  recorded in the whole-cell configuration. The first panel shows an AP before and after subtraction of  $I_{K1}$ , the second panel shows the relative stability after both subtracting and adding  $I_{K1}$ , the third panels shows the effects of increasing  $I_{K1}$  in 10 mM  $[K^+]_0$  (note this action only changes the inward rectifier), the fourth panel show the effects of using a Purkinje type current. **B.** Data for  $V_{min}$ , MDP, APD50 and APD90 for Mid-LV cells electronically expressing different properties of  $I_{K1}$ . Abbreviations: Control (Con), subtracted  $I_{K1}$  ( $-I_{K1}$ ), the  $I_{K1}$  I-V for Mid-LV at 5.4 mM K<sup>+</sup> ( $+I_{K1}$  5.4 mM K<sup>+</sup>), the  $I_{K1}$  I-V for Mid-LV at 10 mM K<sup>+</sup> ( $+I_{K1}$  10 mM K<sup>+</sup>) and the  $I_{K1}$  for Purkinje at 5.4 mM K<sup>+</sup> ( $+I_{K1}$  Purkinje). n=5, N=1 heart.

#### Table 1

Action potential parameters from tissue in response to extracellular K<sup>+</sup> changes at 0.5 Hz pacing.

	<i>Ventricle</i> N=4 hearts	<i>Purkinje</i> N=4 hearts	<i>Atria</i> N=5 hearts
MDP (mV) 5.4 mM $[K+]_0$	-90.0±0.61	-89.2±1.7	-77.3±1.5*
MDP (mV) 2 mM $[K+]_0$	-98.3±1.0	-97.8±1.2	-86.6±2.6*
MDP (mV) 10 mM [K+] <sub>o</sub>	-75.3±3.5	-77.9±0.9	-64.7±5.1
APD50 (ms) 5.4 mM [K+] <sub>o</sub>	211±19.1	183±20.1	28.0±8.8*
APD50 (ms) 2 mM [K+] <sub>o</sub>	252±43.6	232±38.6	36.8±9.7*
APD50 (ms) 10 mM [K+] <sub>o</sub>	164±16.7	147±20.6	25.1±5.8*
APD90 (ms) 5.4 mM [K+] <sub>o</sub>	275±17.7	307±55.3	123±15.1*
APD90 (ms) 2 mM [K+] <sub>o</sub>	350±51.3	355±49.2	153±19.5*
APD90 (ms) 10 mM [K+] <sub>0</sub>	199±14	217±27.9	102±14.4*

Abbreviations: MDP (mean diastolic potential), APD (action potential duration at 50 or 90 repolarization, APD50 and APD90.

p<0.05 vs. ventricle

# Table 2

Total polyamine concentrations in ventricular and atrial tissue.

	Spermine	Spermidine	Putrescine
Ventricle n=8 (nmol/mg protein)	$1.54\pm0.06$	$0.64\pm0.05$	$0.19\pm0.02$
Atria n=7 (nmol/mg protein)	$1.39\pm0.15$	$0.59\pm0.08$	$0.19\pm0.03$