

REVIEW

# Osteogenesis of Adipose-Derived Stem Cells

Brian E. Grottkau, Yunfeng Lin\*

Department of Orthopaedic Surgery, MassGeneral Hospital for Children and the Pediatric Orthopaedic Laboratory for Tissue Engineering and Regenerative Medicine, Harvard Medical School, Boston, Massachusetts, USA

**Current treatment options for skeletal repair, including immobilization, rigid fixation, alloplastic materials and bone grafts, have significant limitations. Bone tissue engineering offers a promising method for the repair of bone deficiency caused by fractures, bone loss and tumors. The use of adipose derived stem cells (ASCs) has received attention because of the self-renewal ability, high proliferative capacity and potential of osteogenic differentiation *in vitro* and *in vivo* studies of bone regeneration. Although cell therapies using ASCs are widely promising in various clinical fields, no large human clinical trials exist for bone tissue engineering. The aim of this review is to introduce how they are harvested, examine the characterization of ASCs, to review the mechanisms of osteogenic differentiation, to analyze the effect of mechanical and chemical stimuli on ASC osteodifferentiation, to summarize the current knowledge about usage of ASC *in vivo* studies and clinical trials, and finally to conclude with a general summary of the field and comments on its future direction.**

**Keywords:** adipose derived stem cells; osteogenesis; bone tissue engineering; osteogenic differentiation

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## Introduction

Mesenchymal stem cells (MSCs) are a group of multipotent adult-derived stem cells that can be isolated from organs and tissues including bone marrow, ligaments, muscular and adipose tissue (1-2). MSCs may undergo self-renewal for several generations while maintaining their capacity to differentiate into skeletal muscle, smooth muscle fat, cartilage, connective tissues, tendon and bone (3). Within bone marrow, mesenchymal cells are located in the stromal compartment and are unique from the hematopoietic compartment. These cells harvested from the marrow compartment of bone were named bone marrow derived mesenchymal stem cells (BMSCs), as one of the earliest multipotent stem cells attracting researchers' attention, which have been used for tissue engineering for years, including the study of bone formation for the spine (4-6). However, BMSCs harvest requires aspiration from the iliac crest

which only yields 10-40 mL of marrow or from bone marrow biopsies, both of which can be painful, and the stem cell incidence in bone marrow is estimated to be about 1 per 105 cells (7). This constraint has led to the study of stem cells derived from adipose tissue.

Fat has long been felt to be an inert tissue, and lipoaspirate has been discarded as surgical waste. The numerous cell types in lipoaspirate, including preadipocytes, adipocytes, fibroblasts, endothelial cells and resident monocytes, vascular smooth muscle cells or pericytes, lymphocytes and macrophages (8), had been ignored in the past. Within the stromal vascular layer, researchers have begun to investigate a vast population of cells with the potential to differentiate into mesodermal tissues. In 2001, Zuk *et al* firstly established ASCs as a multipotent stem cell population, with the ability to assume osteogenic as well as chondrogenic, adipogenic, and neurogenic phenotypes, through chemically induced differentiation (3, 9). In contrast to BMSCs, ASCs have abundant and autologous cell source, carry relatively lower donor site morbidity, grow fast, and are available in large number of stem cells at harvest from a small volume of adipose tissue (10). As a

\*Correspondence: Yunfeng Lin  
E-mail: yunfenglin@scu.edu.cn  
Tel: 86-28-85503487; Fax: 86-28-85582167

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result, ASCs have become an attractive and alternative multipotent cell population for use in tissue replacement therapies.

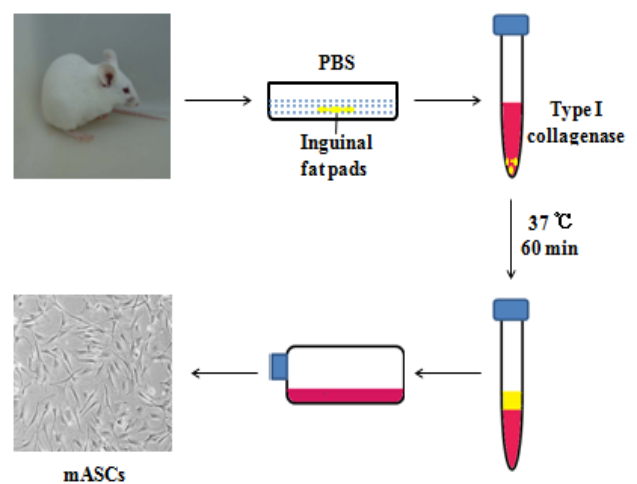
Bone tissue engineering offers a promising method for the repair of bone deficiencies caused by fractures, bone loss, and tumors. At present, the clinical gold standard for the treatment of skeletal defects is an autogenous bone graft. For the autogenous sources from which to harvest bone grafts are limited, clinicians have turned to allogenic bone substitutes such as demineralized bone matrix consisting of extracellular matrix proteins and growth factors without any cells, while the growth factors release is limited in duration failing to provide long term. The shortcomings of current methods indicate the need to combine cells which can form bone. ASCs have been demonstrated to undergo osteogenesis rapidly and with minimal stimulation by exogenous cytokines and thus be regarded as a promising option for bone tissue engineering trials (11). In this review, we will introduce how they are harvested, examine the characterization of ASCs, review the mechanisms of osteogenic differentiation, analyze the effect of mechanical and chemical stimuli on ASC osteodifferentiation, summarize the current knowledge about usage of ASC *in vivo* studies and clinical trials, and finally conclude with a general summary of the field and comments on its future direction.

### Harvest and culture of ASCs

The methods gaining ASCs from different species have some differences. We will introduce the method of harvesting ASCs from mice.

ASCs isolated from inguinal fat pads of mice are harvested as follows. Eight-week-old BALB/c mice were used in the study, in accordance with the International Guiding Principles for Animal Research (1985). All surgical procedures were performed under approved anaesthetic methods using Nembutal at 35 mg·kg<sup>-1</sup>. Inguinal fat pads were harvested from the mice and extensively washed with sterile phosphate-buffered saline (PBS) to remove contaminating debris. Then, they were incubated with 0.075% type I collagenase in PBS for 60 min at 37 °C with agitation. After removing of collagenase by dilution with PBS, cells released from adipose specimens were filtered through a 100 µm mesh to remove tissue debris, and collected by centrifugation at 1 200 g for 10 min. This results in separation of harvested fat into three layers: infranatant (lowest layer composed of blood, tissue fluid and local anaesthetic), middle portion (primarily fatty tissue), and supranatant (upper layer, least dense and consisting of lipids). The pellet

from the infranatant was resuspended and incubated to remove contaminating red blood cells. And then, it was washed three times with PBS and seeded on the plastic tissue culture dishes in growth medium containing α-MEM, 10% fetal bovine serum (FBS), 100 U·mL<sup>-1</sup> penicillin, and 100 mg·mL<sup>-1</sup> streptomycin. ASCs were maintained in a humidified atmosphere of 5% CO<sub>2</sub> at 37 °C. They would be passaged three times prior to osteogenic differentiation. After transferred into specific medium containing dexamethasone (10<sup>-8</sup> mol·L<sup>-1</sup>), ascorbic acid (50 mg·L<sup>-1</sup>), and β-glycerophosphate (10 mmol·L<sup>-1</sup>), the ASCs showed obvious phenotype alteration and turned to osteogenesis. The medium was replaced every 3–4 days for 14 days till differentiated cells were confluent (Figure 1).



**Figure 1** Isolation of adipose-derived stem cells.

### Characterization and localization

ASCs display fibroblast-like morphology and preserve their shape after expansion *in vitro*. Similar to other types of MSCs, ASCs remain difficult to define due to lack of definitive cellular markers. Mitchell *et al* found that stromal cell-associated markers, including CD13, CD29, CD44, CD63, CD73, CD90, CD166, were initially low on stromal vascular fraction (SVF) cells and increased significantly with successive passages (12). Dominici *et al* demonstrated that ASCs must express CD105, CD73 and CD90, and lack expression of CD45, CD34, CD133, CD14 or CD11b, CD79α or CD19 and HLA-DR surface molecules (13). Lin *et al* found that ASCs exist as CD34<sup>+</sup>/CD31<sup>-</sup>/CD104b<sup>-</sup>/SMA<sup>-</sup> cells in the capillary and in the adventitia of larger vessels (14). Researchers also found another interesting characteristic of ASCs that the surface immunophenotype partially changes in different passages. At the early passages (primary to 4th) of ASCs, the hematopoietic-associated markers (CD11a, CD14,

CD45, CD86 and HLA-DR) decreased and the MSCs-associated markers (CD13, CD29, CD34, CD44, CD63, CD73, CD90 and CD166) increased significantly (12, 15). In general, markers that are uniformly reported to have strong positive expression are CD13, CD29, CD44, CD73, CD90, CD105, CD166 and MHC-I, while markers of the hematopoietic and angiogenic lineages, such as CD31, CD34, CD45, CD117 (16), CD133 and STRO-1, have been reported to show low or lack of expression on ASCs. MHC-II has also been found to be absent on ASCs. Moderate expression has been reported for markers CD9, CD49d, CD106 and CD146.

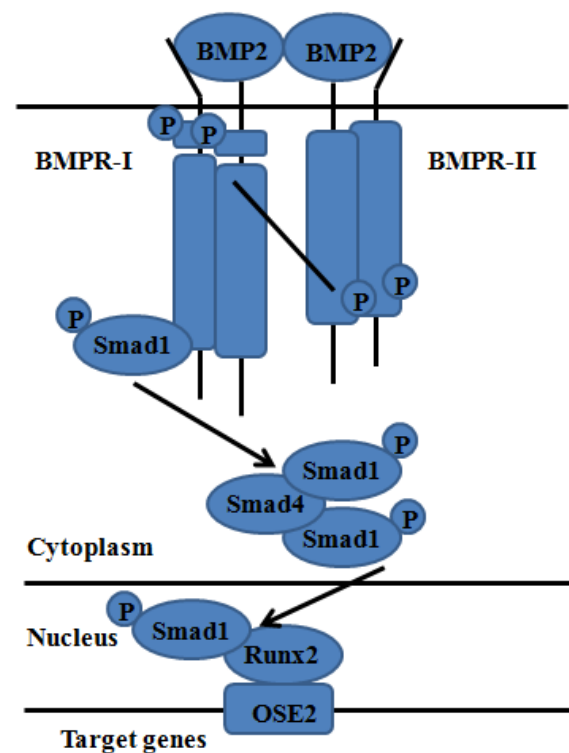
### Mechanisms of osteogenic differentiation

The osteogenesis process is not completely understood, it has been paid increasingly attentions on the molecular mechanisms recently. Researchers believe that osteogenesis is defined by a series of events which starts with a commitment to an osteogenic lineage by mesenchymal cells. And then, these cells proliferate and demonstrate an up regulation of osteoblast-specific genes and mineralization. After attachment, the medium of ASCs was then changed to basic osteogenic differentiation medium (b-ODM) containing  $\alpha$ -MEM, 10% FBS, 100 mg·mL<sup>-1</sup> of ascorbic acid, 10 mmol·L<sup>-1</sup>  $\beta$ -glycerophosphate. Retinoic acid can be supplemented to promote mASCs differentiation but is not necessary for hASCs.

The mechanisms of driving the ASCs into the osteoblast lineage are still not clear, researches on signaling pathways have provided much information on the effect of signaling molecules on cell migration, adhesion, proliferation, differentiation, and ultimately bone formation. Multiple signaling pathways have been demonstrated to participate in the differentiation of an osteoblast progenitor to a committed osteoblast including transforming growth factor- $\beta$  (TGF- $\beta$ )/bone morphogenetic proteins (BMPs), Wnt/ $\beta$ -Catenin, Notch, Hedgehog and Fibroblast Growth Factor (FGF), etc.

BMP is a member of the TGF- $\beta$  superfamily except BMP-1, it was originally isolated from bovine bone extracts and found to induce ectopic bone formation subcutaneously in rats (17). This group of proteins includes sixteen BMPs and comprises nearly one-third of the TGF- $\beta$  superfamily. Studies have demonstrated that it is a promising candidate cytokine in osteoblast differentiation and osteogenesis. BMP initiates its signaling cascade through ligand binding to the heteromeric complex of types I and II serine/threonine kinase receptors on the cell surface (18). Subsequently, these activated receptor kinases phosphorylate transcription

factors signaling mothers against decapentaplegic (Smad) proteins 1, 5 and 8 (19). These phosphorylated Smads form a heterodimeric complex with Smad4 and effect target gene expression and promote the osteogenic differentiation. BMPs have also been shown to increase transcription of core-binding factor-1/Runt-related family 2 (Cbfa1/Runx2), a molecule known to be necessary for commitment along an osteoblastic lineage, to regulate osteoblast differentiation (20) (Figure 2). The 16 subtypes of BMPs are observed to express obviously in relevant tissues, such as BMP-2 expresses in cartilage, periosteum and compact bone; BMP-2,-4,-7 show good bone-forming activity when combined with collagen, hydroxyapatite (HA) and degradable high molecular polymer (HMP) in different animal bone defects experiments (20). In general, BMP-2, 4, 6, 7 and 9 are considered to be the most osteoinductive (21). However, the osteoinductive effect of BMPs is affected by some factors. Some studies found that BMPs are more potent at inducing bone formation as heterodimers than as homodimers. In culture, BMP-2/6, BMP-2/7, and BMP-4/7 heterodimers have been shown to promote higher alkaline phosphatase levels than homodimer combinations *in vitro* and *in vivo* (22-25). The effect of BMPs has also been noted to be concentration dependent. At low concentrations, they foster chemotaxis and cellular proliferation, while BMPs induce bone



**Figure 2** BMP Signal and osteogenesis of adipose-derived stem cells.

formation at high concentrations (26).

Among the subtypes of BMPs, BMP-2, as a pleiotropic regulator, governs the key steps in bone induction cascade such as chemotaxis, mitosis, and differentiation of mesenchymal stem cells in the process of bone healing (27-28). Although some reports described the effectiveness of BMP-2 for the osteogenesis in BMSCs and ASCs, it is unclear whether BMP-2 enhanced ASCs can heal the large bone defects (29-30). In our previous study, ASCs were harvested from normal Sprague-Dawley (SD) rats and transfected by BMP-2 gene before they were loaded on alginate. The ability of bone regeneration was determined in rat critical-size cranial defects, which were 8-mm diameter defects created in the calvarias of 36 rats. These rats were divided into three groups. In experimental group, the defects were filled with alginate gel combined with BMP-2 transfected ASCs; in negative control group, the defects were filled with alginate gel mixed with normal ASCs; in blank controls, the defects were filled with cell-free alginate gel. Four rats of each group were killed and the cranial defect sites were observed at 4, 8 and 16 weeks after surgery. At 4 weeks in experimental group, the initial resorption of alginate scaffolds was clear and the newly formed bone extended. The consolidated whitish bone was found within the defect margin in experimental group from 8 weeks on. At 8 weeks, there was a great extent of reduction of cranial defects and they accomplished complete osseous healing at 16 weeks when the experiment finished. The bone formation in the negative control groups was only presented disorderly along the periphery of the defects and the central domain showed fibrous healing. There was few new bones formation at the blank control group. To clarify the molecular events leading to the formation of new bone, we investigated expression of biochemical markers using RT-PCR and western blotting along the course of BMP-2 enhanced ASCs differentiation. The RT-PCR analysis of OCN, OPN, RUNX2 and BMP-2 demonstrated that there was significant difference in expression between experimental and control groups. Continued high expression of OCN, OPN, RUNX2 and BMP-2 was observed throughout the progression of the experiment group both *in vitro* and *in vivo*. In negative control groups, these genes were not observed *in vitro* and 8 weeks *in vivo*, only at the 16 weeks after surgery, weak expression of these genes was observed; in the blank control group, these genes were not detected at 8 and 16 weeks. The western blotting analysis was similar to the RT-PCR results. In the experiment group, these proteins were observed in the monolayer cells after BMP-2 transfection *in vitro* and *in vivo*, but not observed

in the negative and blank control groups. Our research demonstrated that load-bearing alginate with BMP-2 enhanced ASCs can repair the large bone defects, and therefore applied in the bone tissue engineering for further clinical usage (31).

The Wnt family consists of a large number of secreted glycol-proteins that are involved in embryonic development, tissue induction, and axis polarity (32-33). Most Wnt proteins are thought to act as ligands for cell surface receptor complexes composed of frizzled (Fz) and low-density lipoprotein (LDL)-receptor-related protein 5/6 (LRP5/6) family members. Downstream of Fz-LRP5/6 complexes, canonical Wnt signaling results in stabilization and translocation of  $\beta$ -catenin to the nucleus, where it binds to T-cell factor/lymphoid enhancer factor (TCF)/Lef transcription factors (Figure 3).  $\beta$ -Catenin-TCF/Lef complexes activate transcription of a variety of Wnt-responsive genes, including genes involved in proliferation, osteoblast differentiation and osteogenesis (34-36). Derogowski's report observed that Notch-1 overexpression inhibited osteoblastogenesis by suppressing Wnt/beta-catenin but not BMPs signaling (37). Chen *et al* found that alcohol not only inhibits mature osteoblast activity but also influences the balance between osteoblast and adipocyte differentiation and mesenchymal stem cell commitment in bone marrow. Their observations are consistent with the

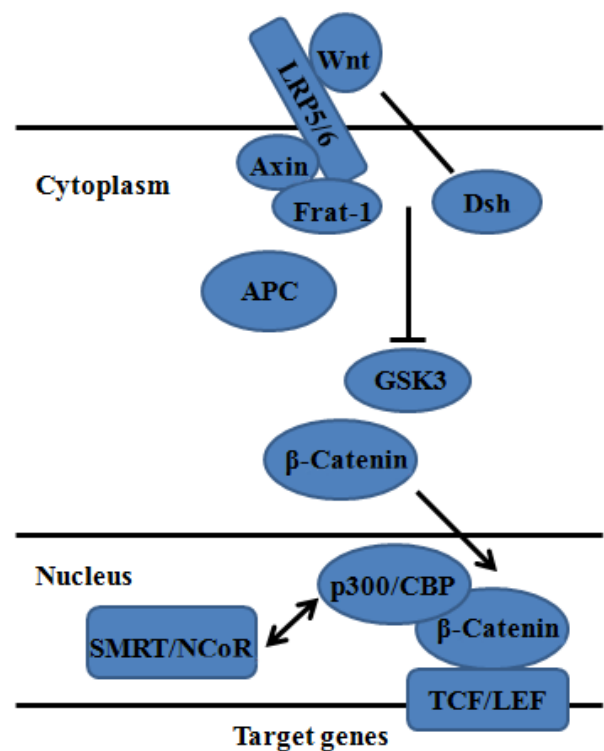
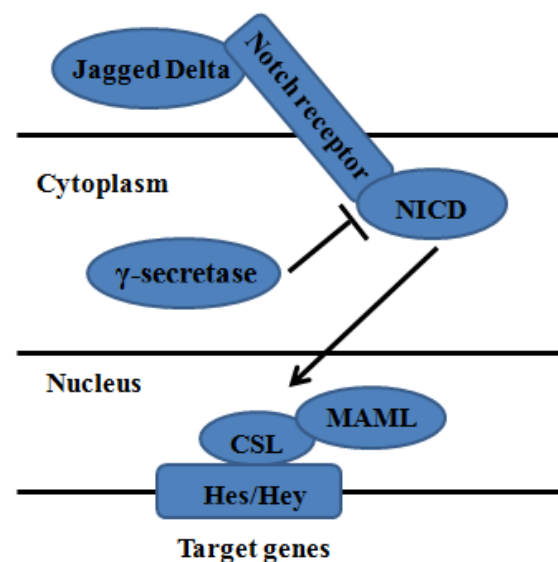


Figure 3 Wnt Signal and osteogenesis of adipose-derived stem cells.

hypothesis that ethanol inhibits bone formation through stimulation of oxidative stress to suppress Wnt signaling (38). Si *et al* found that tightly regulated CCN1/Cyr61 expression may play an important role in Wnt3A-induced osteoblast differentiation of mesenchymal stem cells (39). Stevens *et al* indicated that Wnt10b, as the only Wnt ligand linking to mesenchymal progenitor function in both humans and mice, is uniquely required for maintenance of mesenchymal progenitor activity in adult bone (40). Some studies revealed that non-canonical Wnt signaling could also play a role in osteogenic differentiation. Such as, non-canonical Wnt5a signaling involving Ror2 and RhoA as well as N-cadherin mediated  $\beta$ -catenin signaling are necessary for mechanically induced osteogenic differentiation (41). And Wnt-4 may have a potential use in improving bone regeneration and repair of craniofacial defects (42).

Notch signalling plays a critical role in development and regeneration of stem/progenitor cells as well as in controlling their fate (43-46). The Notch system is known to be an evolutionarily conserved mechanism that balances proliferation and differentiation of stem/progenitor cells (47). Previous investigations showed Notch signaling positively regulated the osteoblastogenesis in several kinds of cells, such as ST-2 marrow stromal cells (37), murine bone marrow mesenchymal progenitors (48), osteoblastic cells M3T3-E1 (49), mesenchymal progenitor cells Kusa (50), C2C12 myoblasts (51) and COS-7 cells (52). The Notch receptor is a single pass trans-membrane protein which, during maturation, may be cleaved by a furin-like convertase (at S1) in the trans-Golgi to generate a noncovalently associated heterodimer at the cell surface. Canonical Notch signalling is initiated when a cell-surface expressed Delta/Serrate/LAG-2 (DSL) ligand binds to the Notch receptors (Notch-1, -2, -3 and -4) expressed on an opposing cell surface. Endocytosis of the Notch-ligand complex by the ligand-expressing cell leads to ADAM metalloprotease mediated cleavage at S2 and removes the extracellular fragment of the heterodimer. The membrane tethered fragment is then cleaved by  $\gamma$ -secretase complex at S3 to release the Notch intracellular domain (NICD). This transports to the nucleus and assembles into a transcriptional activation complex, CCAAT-binding protein (CBF-1), which includes a DNA binding protein of the CSL family and its co-activator Mastermind-like (53). This new assembly acts as a transcriptional repressor without existence of NICD, which recruits a co-repressor complex and inhibits transcription of target genes that containing CCAAT binding sites (54-55). As a sequence of binding, NICD displaces the repressor complex of CSL and recruits

nuclear co-activators, such as mastermind-like 1 (MAML1) and histone acetyltransferases (56), converting CSL into a transcriptional activator. Notch activation through CSL-NICD interactions can in turn activate transcription of various target genes, including Hes (Hairy/Enhancer of Split) (57), Hes-related repressor protein (HERP) (58-59), per-oxisome-proliferator-activated receptor (PPAR) (60) and nuclear factor- $\kappa$ B (NF- $\kappa$ B) (61) (Figure 4). In addition to trans-activating Notch-ligand complexes, the receptor can also form cis-inhibitory complexes when Notch and ligand are expressed on the same cell surface. Cis-inhibition serves to limit the zone of Notch activity and is particularly important in developmental programs in *Drosophila* such as the wing disc and eye (53).



**Figure 4** Notch Signal and osteogenesis of adipose-derived stem cells.

N-[N-(3,5-Difluorophenacetyl)-L-alanyl]-S-phenylglycine t-butyl ester (DAPT) is a  $\gamma$ -secretase inhibitor that can block Notch signaling by preventing the cleavage of Notch receptors, which has been widely used to evaluate the biological behaviors and Notch signaling pathway in various cells such as muscle stem cells, neural stem cells, BMSCs, human tongue carcinoma cells, etc (62). Our group investigated the effects of DAPT on proliferation and osteogenesis in ASCs for the first time by using an *in vitro* 1,25-Dihydroxyvitamin D3 (VD3) induced osteogenic differentiation system. The DAPT treated cells showed a dose-dependent increase compared to non-DAPT group. Results indicated that the addition of DAPT to VD3 treatments significantly increased osteogenesis in ASCs. In this study, we attempted to assess the biological effects of DAPT on the proliferative capacity of ASCs. Results showed that

ASCs cultured in DAPT significantly decreased in CFU numbers compared with those cultured in control medium during 2-week culture period. DAPT clearly inhibited ASCs proliferation at all doses, which revealed the inhibition of ASCs proliferation by DAPT and indicated that ASCs responded with decreased growth when the Notch pathway was blocked. Real-time PCR showed the expressions of Notch downstream target genes *Hes-1* and *Hey-1* were decreased significantly after DAPT treatment. Immunofluorescence staining also revealed that *Hey-1*, expressing in the nucleus of ASCs to act as a transcriptional repressor, was down-regulated when Notch signaling was inhibited by DAPT. While, Real-time PCR and Western Blot showed expressions of the genes encoding osterix (*OSX*) or *Runx2*, as an essential transcription factor required for osteogenesis, increased during osteogenic induction in the presence of DAPT. These results indicated that the *Runx2* dependent osteogenic differentiation of ASCs was enhanced when the interaction between *Runx2* and Notch target gene *Hey-1* was suppressed in the presence of DAPT (63). Previous study reported that Notch repressed osteoblastic differentiation through its target genes and *Runx2* (64), which was similar to our results.

Hedgehog proteins, like Wnt proteins, are important signaling molecules which play critical roles in the control of pattern formation and cellular roles in the control of pattern formation and cellular proliferation/differentiation (65). *In vitro*, Sonic Hedgehog (*Shh*) induces ALP expression (66-67), and also increases selectivity in the differentiation of multipotent mesenchymal cells into the osteoblast lineage (68). Thus, osteogenesis is a complex process that can likely be modulated by small molecules acting on a number of signaling pathways. Wu *et al* demonstrated that purmorphamine induces osteogenesis by activation of the Hedgehog signaling pathway (69).

FGF signaling participates in skeletal development from the earliest stages of limb bud development through the final stages of the ossification process. Several FGFs are expressed in the developing endochondral bone (70). FGF2 expression, which was first isolated from growth plate chondrocytes, has also been observed in osteoblasts and in periosteal cells. Despite the widespread expression of FGF2, targeted deletion of FGF2 caused a relatively subtle defect in bone, leading to decreased bone density, but no defects in skeletal size or patterning (71). In addition, no defects in chondrogenesis were observed, suggesting that if FGF2 is involved in chondrogenesis that it may be redundant with other FGFs (72). Both FGF9 and FGF18 are expressed around the condensing mesenchyme and in the peri-

chondrium/periosteum, which are also good candidates for redundant factors (73-74). The perichondrium also expresses FGF7, FGF8, and FGF17. Some or all of these FGFs may signal directly to chondrocytes in the growth plate (72). Genetic studies have identified a defect in chondrogenesis and osteogenesis in mice lacking FGF18 (75-76). Requirements for FGF7, FGF8 and FGF17 in skeletal development have not been identified. Hormones can also influence the skeletal metabolism directly or indirectly. Parathyroid hormone promoted bone growth or filled up lacunas caused by osteoclast when decomposing, or synthesizing bone while in mature bone tissue (77). Estrogen up-regulates the transcriptional expression of osteoblast-related genes such as BMP-2, ALP, TGF-1 and *Cbfa1*. Physiological concentration of glucocorticoid can stimulate osteoblast differentiation of MSCs. However, if applying with large dose of glucocorticoid in long period, osteoblast proliferation, apoptosis and reduction of active osteoblast-composition can be inhibited, and ultimately this may lead to osteoporosis.

### Osteogenesis of ASCs via stimulation

In general, two major approaches have been used to regulate the mechanical environment of cells and tissue engineering constructs in culture: mechanical signals such as tensile, compressive strain, fluid shear and electrical stimulation, and biochemical composition.

Mechanical force is a fundamental biological factor that stimulates fracture healing and bone remodelling processes (78), and most studies indicate that mechanical stress is an anabolic factor for osteogenic differentiation of BMSCs or osteoblasts (79-80).

Mechanical stretch has been believed to be a regulating factor of osteo-adipogenic axis differentiation of mesenchymal stem cells. In our previous study, mASCs, after being osteo-induced for 48 h, were subjected to uniaxial cyclic tensile stretch by a 4-point bending mechanical loading device with the long duration continuous pattern (6 h cyclic stimulation for 1 day, 1 Hz, 2 000  $\mu\epsilon$ ) and short duration consecutive pattern (17 min cyclic stimulation a day for 10 days, 1 Hz, 2 000  $\mu\epsilon$ ). The results showed that mASCs are sensitive to cyclic tensile strain. Compared to 17 min of consecutive stretching, cyclic tensile strain of 6 continuous hours' duration could significantly increase gene expression of BMP-2 and *Runx2* and depress OCN mRNA expression. We indicated that ASCs may sense mechanical loading in a duration-dependent manner and cyclic tensile stretch may modulate the osteogenic differentiation of ASCs via the BMP-2 signalling pathway (81). Moreover,

we hypothesized that mechanical force was one of the pivots that modulate osteogenic differentiation, depending on the induction environment of progenitor cells. So we studied the differentiation of mASCs in adipogenesis-induced environment under mechanical stress. Cells were randomly divided into four groups. Loading groups were exposed to uniaxial cyclic tensile stretch for 2 000  $\mu\epsilon$ , 1 Hz for 6 and 2 h, respectively, after ASCs were adipo-induced for 72 h. ASCs that were retained in adipogenic medium without being loaded were used as induced-control group. In the third group, ASCs were exposed to mechanical loading under the same conditions, but without prior induction, and correspondingly, the non-induced control (NIC) group was kept in static medium without any mechanical loading. We found that conversion of ASCs into adipocytes driven by adipogenic conditions can be inhibited by mechanical signals that also allow osteoblastic lineage selection, and ERK1/2 activation may be involved in this mechanical stress-induced trans-differentiation. Mechanical stress may function as a pivotal regulation factor in reciprocal relationships of osteogenic and adipogenic differentiation (82). Hanson *et al* demonstrated that ASC exhibit enhanced osteogenic differentiation when exposed to both continuous (10% strain, 1 Hz) and rest inserted strain (10% strain, 1 Hz, 10 rest between each cycle) (83). A study also showed that tensile strain can mechanically mediate age-related variations in mASC proliferation and differentiation potential (84).

Fluid flow and shear stress are believed to impose a physical signal on osteogenic proliferation and differentiation in both MSC and ASC (85-88). Some studies also found that fluid flow could increase dimensionality and cellular distribution throughout a scaffold material, enhance nutrient transport and create a more functional construct (88-89). And PFF had been found to be the direct osteogenic signaling via fluid shear in ASC (87, 90). Cyclic compression has been demonstrated to enhance osteogenic differentiation and bone formation *in vitro* and *in vivo* (91-93), but there has been lack of work on the effect of compression on ASC osteoblast differentiation.

As bone formation by implantation of ASCs must be preceded by the *in vitro* osteogenic differentiation of these cells, it is important to develop techniques to ensure a well characterized and consistent cell population following the differentiation process. ASC can be osteogenic differentiated by chemical stimulation using media supplements and growth factors to induce lineage specification, such as 1, 25-dihydroxyvitamin D3 (VD3), dexamethasone,  $\beta$ -glycerolphosphate and

ascorbic acid (3, 63, 94). Besides, additional growth factors and components including BMP-2, growth and differentiation factor-5, retinoic acid, and tumor necrosis factor- $\alpha$  among others have also been researched as osteogenic stimulators (31, 95-97). However, the differentiation procedure has the shortcomings of requiring additional culture time and steps including the use of large amounts of costly growth factors and some supplements which could be cytotoxic to cells, before implantation to achieve therapeutic efficacy. New methods are required in order to not only reduce the culture period, the amount of demanded growth factors, but also enhance the efficiency of osteogenesis and thus of bone regeneration. One approach is delivery of cytokines involving incorporation of these molecules into scaffolds such as liposome and microspheres. This makes the growth factor to be retained at the site of interest for an extended period while maintaining its biological activity. Moreover, engineered ASCs with gene transfection by various virus-vectors have evolved to be an attractive option to ameliorate bone repair, especially large bone defects. Genes like Runx-2, BMP-2, BMP-4, BMP-7, or Osterix-transfected ASCs are considered to promote the bone formation *in vivo* implantation (28-30).

### ***In vivo* studies**

To adequately translate *in vitro* findings to the clinical realm, robust *in vivo* data must be obtained to demonstrate the osteogenesis capacity of ASCs. *In vivo*, ASCs survive in low oxygen environments making them good candidates for cell-based therapies in which the oxygen supply may be limited during the post implantation period when a blood supply is lacking (98). However, ASCs secrete angiogenic cytokines such as hepatocyte growth factor and vascular endothelial growth factor, which are considered to contribute to the angiogenic properties of ASCs (99). The transplanted ASCs produce cytokines and chemokines that act as homing signals for endogenous stem cells and progenitor cells to the site of injury. Therefore, presence of ASCs may promote the osteogenic and angiogenic conditions of the construct *in vivo* (100).

Besides the cells, the molecular growth factors and components as we mentioned previously, the bone defect models and the scaffolds also play an important role *in vivo* study. The ideal model should represent the characteristic of clinical condition of the bone injury or defect. And there are several models such as rat critical-size cranial defect models and long bone skeletal defect models, which are generally acknowledged in

the area of ASCs *in vivo* studies. Biomaterial scaffolds can not only potentially provide a controlled environment protecting implanted cells from harmful stimuli and a highly modifiable vehicle for inductive factors, but also deliver genetic material and/or inductive biochemical cues, which allow for some degree of developmental control over the delivered stem cells (101). Many studies have combined biomaterial scaffolds with ASCs to repair bone defects, for example, biphasic calcium phosphate nanocomposite (NanoBCP) (102), poly (lactic-co-glycolic acid) (PLGA) (103), HA/tricalcium phosphate (TCP) (104), chitoooligosaccharide (COS) (105), fibrin/HA (106), and so on. Prichard *et al* (107) examined cell coverage and cell function of ASCs on different biomaterials, including fibronectin, silicone rubber, dualigand, polyimide, oxygen plasma plus fibronectin and polyurethane. The results showed that cell attachment was very strong on both polyurethane and polyimide for all attachment methods. None of the attachment methods caused any differences in basic cell proliferation, metabolism, caspase-3 activity and intracellular ATP concentration. However, ectopic bone formation inside porous ceramic blocks revealed that material properties such as size, composition, geometry, porosity and microstructure might be important but not sufficient parameters for appropriate bone formation (108). Moreover,  $\beta$ -TCP granules, named as CEROS 82, have been in clinical use in Europe for over 20 years. And the investigations have been published concerning the clinical value of Chronos1  $\beta$ -TCP in bone environment (109).

Our group has done some research on bone regeneration of ASCs combined with NanoBCP and alginate gel. NanoBCP is a composite biomaterial formed by microporous BCP with NanoHA and  $\beta$ -TCP, which has high strength and porous structures. The NanoBCP constructs containing osteogenic ASCs were transplanted to nude mice subcutaneously for 8 weeks to acquire the physiological behavior of induced ASCs during ectopic differentiation *in vivo* and rat critical-size cranial defects were taken as the model to determine the efficiency of engineered constructs in the generation of new bone *in situ*. Histological analysis of the retrieved specimens from nude mice in experimental group showed obvious ectopic bone formation and there were positive expression of osteopontin (OPN) and osteocalcin (OCN) at RNA and protein level. As for the cranial defects, there was complete repair in experimental group, but only partial repair in negative controls. Combining osteogenic ASCs with NanoBCP can lead to formation of ectopic new bone. Furthermore, the approach can also stimulate bone regeneration and repair for the

large size bone defects. On the basis of the results we thought load-bearing NanoBCP with ASCs could therefore applied in the engineering approach for further clinical usage (102). The alginate gel is one of the most extensively applied biomaterials in bone tissue engineering, which have a high porosity, ideal porous structure, biodegradable, biocompatibility, and high affinity to water. In the presence of calcium ions, the semisolid gel can be formed with cross-linking of alginate chains under mild conditions (31). The critical-size cranial defect is one that will not regenerate spontaneously during the term of an experiment, which was a defect of 8 mm diameter on the calvaria of a rat in our studies. However, some researchers believe that a 4 mm mouse parietal bone model can offer a reliable, easily replicated and easily followed defect model (98).

In 2005, Cowan *et al* reported successful calvarial critical defect healing by in rat with implantation of ASC-seeded, apatite-coated PLGA scaffolds (110). In 2006, Conejero *et al* successfully repaired the surgically created palatal bone defects in rats by using osteogenically differentiated ASC on a PLA scaffold (111). Dudas *et al* used rabbit ASCs seeded on gelatin foam (GF) scaffolds to regenerate bone in the rabbit calvarial defects (112). In 2007, Yoon *et al* implanted osteogenically differentiated ASC-seeded PLGA scaffolds into critical-sized rat calvarial defects and found robust bone healing after 12 weeks (113). Cui *et al* repaired the cranial bone defects with ASCs seeded on coral scaffold in a canine model (114). In 2010, Lee *et al* found ectopic bone formation by implanting PLGA biodegradable scaffolds with BMP-2 (BMP-2-ASC) or BMP-2/ Runx2 genes (BMP-2/ Runx2-ASC) transfected ASCs into the dorsal subcutaneous spaces of the mice (115). These studies suggest that the osteogenic phenotype of pre-differentiated ASC is functionally maintained *in vivo* and that they can operate in regenerative capacity at a bone defect site.

### Clinical trails

Based on so many *in vitro* and *in vivo* research results, cell therapies using ASCs are widely promising in various clinical fields, such as breast reconstruction and augmentation (116-117), facial lipoatrophy reconstruction (118), cardiovascular tissue regeneration (119), and craniofacial tissue (98, 120).

ASCs of patients' own would be an ideal cell source for bone tissue engineering, and autologous non-immunogenic bone tissues could be easily regenerated with this approach for the repair of large size bone defects. And the defects of facial bones and the



cranium have been demonstrated to heal or enhancing healing with the use of ASCs. However, many countries have not yet approved the use of ASCs. To date, only two clinical case studies about bone regeneration by hASCs have been reported. In the first case, the patient, a 7-year-old female, had sustained severe head injury in a fall accident, which led to a closed multifragment calvarial fracture. The calvarial defect was treated with autologous ASCs isolated and applied in a single operative procedure in combination with milled autologous bone from the iliac crest. ASCs were supported in defect area using autologous fibrin glue, and mechanical fixation was achieved with two large, resorbable macroporous sheets acting as a soft tissue barrier. The new bone formation and near complete calvarial continuity was observed 3 months after the reconstruction (120). Harvesting of bone tissue or a composite microvascular flap is frequently followed by morbidity and a donor site defect despite usually being in an area of lesser importance. Furthermore, a large amount of autologous blood is needed for plasmapheresis, which may in some cases be difficult to obtain. It is known that ASCs can secrete angiogenic factors that promote neovascularization and vessel-like structure formation. In the second case, Mesimäki *et al* harvested autologous fat tissue from a 65-year-old male patient, who underwent a hemimaxillectomy 28 months earlier, due to a large keratocyst, expanded the cells in culture, mixed with BMP-2, and seeded them on a  $\beta$ -tricalcium phosphate scaffold formed into the shape of the defect. The patient finally regained full oral function after about 12 months. It was the first clinical case where ectopic bone was produced using autologous ASCs in microvascular reconstruction surgery. The successful outcome of this clinical case paves the way for extensive clinical trials using ASCs in custom-made implants for the reconstruction craniofacial bone defects.

The results of early studies are inspiring, but they only offered level 4 and 5 data, and lack significant power to impel clinical practice. Larger scale researches such as prospective, randomized control trials must be executed to verify these findings.

## Conclusions

The field has made huge strides toward engineering bone tissue replacements from the development of Wolff's law in the late 19th century to the principles of mechanobiology applied to stem cell osteogenesis. ASCs are easy to isolate through liposuction, available in large quantities, and a abundant cell type with the capability to undergo robust osteogenesis, which makes

them an exciting candidate *in vivo* studies. Furthermore, the ability of undergoing osteogenic differentiation without any stimulation when seeded on an osteoconductive scaffold *in vivo* makes ASCs a promising candidate for bone tissue engineering. However, some studies showed that immunosuppressive capacity of the ASCs may favor the growth of tumor cells in some cases (121-122). Hence, further studies of the mechanism of osteogenic differentiation and ways to improve ASC osteodifferentiation and verify the safety of using ASCs in the clinical procedure are required in the future.

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