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# $^{99m}\text{Tc}$ -Technetium binding site in bone marrow mononuclear cells

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## Abstract

**Introduction:** The increasing interest in  $^{99m}\text{Tc}$ -labeled stem cells encouraged us to study the  $^{99m}\text{Tc}$  binding sites in stem cell compartments.

**Methods:** Bone marrow mononuclear cells were collected from femurs and tibia of rats. Cells were labeled with  $^{99m}\text{Tc}$  by a direct method, in which reduced molecules react with  $^{99m}\text{Tc}$  with the use of chelating agents, and lysed carefully in an ultrasonic apparatus. The organelles were separated by means of differential centrifugation. At the end of this procedure, supernatants and pellets were counted, and the percentages of radioactivity (in megabecquerels) bound to the different cellular fractions were determined. Percentages were calculated by dividing the radioactivity in each fraction by total radioactivity in the sample. The pellets were separated and characterized by their morphology on electron microscopy.

**Results:** The labeling procedure did not affect viability of bone marrow mononuclear cells. Radioactivity distributions in bone marrow mononuclear cell organelles, obtained in five independent experiments, were approximately 38.5 % in the nuclei-rich fraction, 5.3 % in the mitochondria-rich fraction, 2.2 % in microsomes, and 54 % in the cytosol. Our results showed that most of the radioactivity remained in the cytosol; therefore, this is an intracellular labeling procedure that has ribosomes unbound to membrane and soluble molecules as targets. However, approximately 39 % of the radioactivity remained bound to the nuclei-rich fraction. To confirm that cell disruption and organelle separation were efficient, transmission electron microscopy assays of all pellets were performed.

**Conclusions:** Our results showed that most of the radioactivity was present in the cytosol fraction. More studies to elucidate the mechanisms involved in the cellular uptake of  $^{99m}\text{Tc}$  in bone marrow cells are ongoing.

## Introduction

Stem cells derived from different sources hold therapeutic potential for the treatment of many diseases [1, 2]. Tracking these cells *in vivo* represents an ongoing challenge in cell-based therapies [3, 4]. Advanced technology, such as non-invasive imaging of transplanted cells to monitor their fate *in vivo*, has been extensively used and may provide important information for understanding the mechanism of action of these therapies [5, 6].

Cell tracking for *in vivo* detection of grafted cells can be performed by ultrasound, optical imaging, magnetic resonance imaging, micro-computed tomography imaging, and nuclear medicine techniques [7, 8]. In general, the ideal imaging modality is determined by the specificity, sensitivity, resolution, and radiation exposure of individual modalities [9].

All of the available imaging methods are based on different principles, having different properties and limitations. According to Frangioni and Hajar [10], there are eight characteristics of an ideal marker for stem cell tracking: to be biocompatible, safe, and non-toxic; not to produce genetic modification in the stem cell; to allow quantification of exact cell number at any anatomic location; to detect a small amount of cells; to be minimally or not diluted by cell division; to be minimally or not

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transferred to non-stem cells; to be detected by non-invasive imaging technology for months to years; and not demand contrast agent injection. Although some markers have many of these characteristics, none of them fulfills all eight of the criteria presented above.

The fluorescent dyes are the most used to track injected cells in pre-clinical trials. Among these fluorescent dyes, the most commonly used are DAPI (4'-6-diamidino-2-phenylindole) and Hoechst 33342 (bis-benzimide). They permeate through the plasma membrane and have strong affinity to DNA, binding predominantly to the nucleus [11, 12]. Another fluorescent dye widely used is Dil, a long chain of carbocynine that, unlike DAPI and Hoechst, binds to plasma membrane [13]. An advantage of labeling cells with these dyes is to find the possible location and integration of the cells to the tissue; however, these markers are diluted with each cell division. Furthermore, fluorescent dyes can be visualized only by microscopy, which is not compatible with *in vivo* analysis.

More recently, bioluminescence imaging has been extensively used to detect the biodistribution of transplanted cells in live small animals. The clinical application is restricted since this technique is reporter gene-based [14].

Nuclear medicine is characterized by an excellent *in vivo* sensitivity and whole-body imaging capabilities. This technique is suitable for tracking cells in both laboratory [15, 16] and clinical [17–20] settings. Radioisotope cell labeling is a well-established method, and the most commonly used radioisotopes are 111-indium or 99m-technetium ( $^{99m}\text{Tc}$ ) or 18F-fluorodeoxyglycose [18F]FDG [21].

The majority of stem cell clinical trials use bone marrow mononuclear cells (BMMCs), and  $^{99m}\text{Tc}$  is the radionuclide predominantly employed. Our research group has successfully labeled stem cells with  $^{99m}\text{Tc}$ . We use a simple and efficient labeling technique that maintains cell viability and reaches high labeling efficiency and stability rates [15, 17, 18, 20, 22, 23].

The increasing interest in  $^{99m}\text{Tc}$ -labeled stem cells encouraged us to study the binding sites of  $^{99m}\text{Tc}$  to stem cell compartments. This study investigated the presence of  $^{99m}\text{Tc}$  taken up by different organelles in BMMCs. Cells were labeled with  $^{99m}\text{Tc}$  by a direct method previously described by our group [15, 24, 25]. The organelles were separated by means of differential centrifugation and characterized by their morphology on electron microscopy.

## Methods

### Animals

All procedures were performed in accordance with the Guide for Care and Use of Laboratory Animals (Department of Health and Human Services Publication #NIH 85–23, revised 1996; Office of Science and Health Reports, Bethesda, MD, USA). This study was approved by the Ethics

Committee for Animal Use of the Federal University of Rio de Janeiro under number IBCCF 028/2008.

Wistar rats were obtained from Instituto de Biofísica Carlos Chagas Filho (IBCCF) (Rio de Janeiro, Brazil). Animals were housed at a controlled temperature (23 °C) with daily exposure to a 12:12 light-dark cycle.

### Mononuclear cell isolation from bone marrow

Bone marrow cells obtained from Wistar rats were used for cell labeling. Femurs and tibia were harvested, and all adjacent muscle tissue was thoroughly removed. Bone epiphysis was removed, and bone marrow was flushed by using a syringe filled with Dulbecco's modified Eagle's medium (DMEM) (Gibco-Invitrogen, Carlsbad, CA, USA). The cell suspension was carefully placed on top of Ficoll Histopaque 1.083 (Sigma-Aldrich, St. Louis, MO, USA) on 15 ml tubes maintaining a proportion of 1:1 in volume. Tubes were centrifuged at 400×g for 30 min at room temperature. Mononuclear cells were collected from the interface formed between Ficoll Histopaque and DMEM. Cells were washed in phosphate-buffered saline (PBS) twice and counted in a hemocytometer, and viability was checked by using trypan blue.

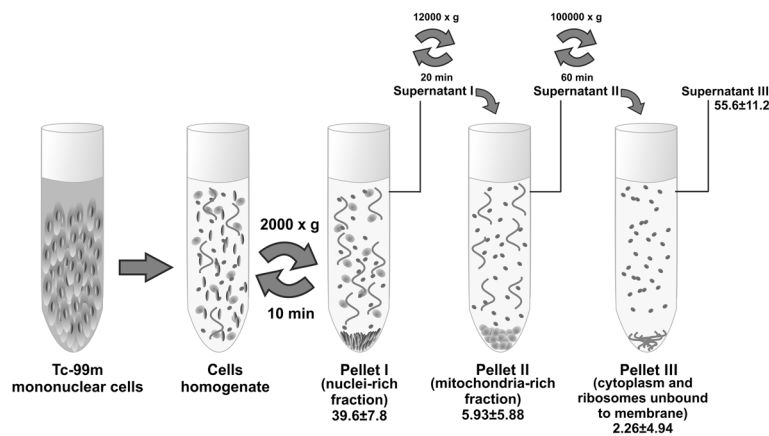
### Labeling the cells with $^{99m}\text{Tc}$

The BMMCs were labeled with  $^{99m}\text{TcO}_4^-$  on the basis of previously published protocols [15, 24, 25]. All the procedures for cell preparation and labeling were carried out in a laminar flow. Briefly, 500  $\mu\text{l}$  of fresh and sterile  $\text{SnCl}_2$  (stannous chloride) solution was added to the cell suspension in saline solution, and the mixture was incubated at room temperature for 10 min. Then 45 MBq of  $^{99m}\text{TcO}_4^-$  was added, and the incubation continued for another 10 min. After centrifugation (500×g for 5 min), the supernatant was removed, and the cells were washed once more with NaCl 0.9 % solution. The pellet was suspended in NaCl 0.9 % solution, and the viability of the labeled cells was assessed by trypan blue exclusion test. Labeling efficiency (percentage) was calculated by the activity in the pellet divided by the sum of the radioactivity in the pellet plus supernatant.

### Differential centrifugation with lysed cells

After labeling and washing procedures, 1 ml of NaCl 0.9 % solution was added, and the cells were carefully disrupted on ice with 10 cycles of 2 sec, with 1 sec of rest between cycles, in an ultrasonic apparatus (GEX 600 Model; Sigma-Aldrich) by using a standard probe (13 mm radiating diameter), operating at 10 % of total amplitude. Disruption procedure was monitored by phase contrast microscopy, and 0.5 ml of each homogenate sample was separated.

Cell homogenate was added to 10 ml of PBS and centrifuged (Beckman Optima™ Ultracentrifuge, model XL-100 K; Beckman Coulter, Pasadena, CA, USA, rotor 90 Ti) at



**Fig. 1** Schematic diagram of differential centrifugation procedure applied to bone marrow mononuclear cells labeled with 99m-technetium (*Tc-99m*). Percentages of radioactivity bound to each fraction are presented as mean ± standard deviation

2000×g for 10 min. The pellet, referred to as pellet I, was reserved, and the supernatant was collected (supernatant I) in a new centrifuge tube. A centrifugation of supernatant I at 12,000×g for 20 min generated the second pellet (pellet II) and supernatant (supernatant II). Pellet II was reserved, and supernatant II was collected in a new centrifuge tube. A third centrifugation at 100,000×g for 60 min resulted in pellet III and supernatant III [24, 26–28]. At the end of this procedure, supernatants and pellets were counted in a well counter (PerkinElmer, Waltham, MA, USA), and the percentages of radioactivity bound to the different cellular fractions were determined.

**Transmission electron microscopy**

The three pellets were fixed with 2.5 % glutaraldehyde in 0.1 M sodium cacodylate buffer (pH 7.2). The supernatants were directly fixed by adding glutaraldehyde to the final concentration of 2.5 %.

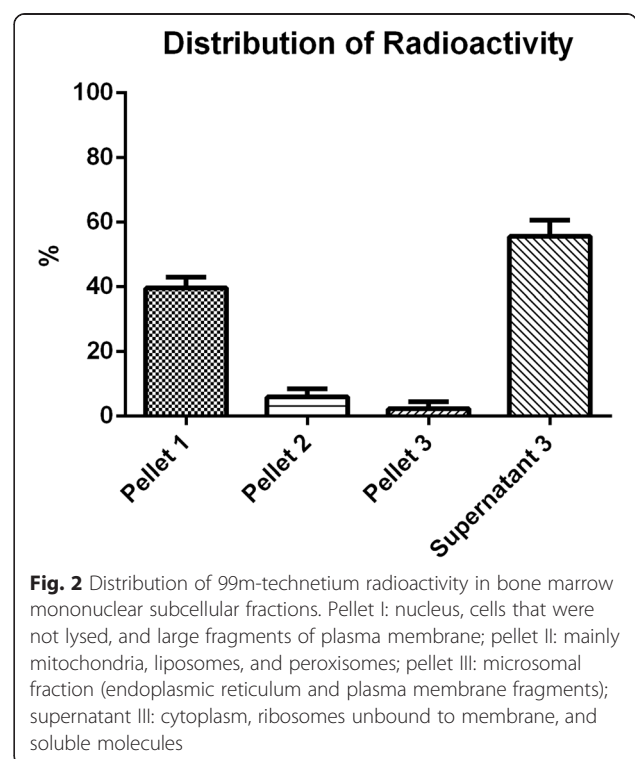
All samples were prepared for transmission electron microscopy on the basis of previously published protocols [29]. In short, fixed samples were washed with saline solution, adopting the same centrifugation used to obtain the fractions. Washed fractions were post-fixed in 1 % osmium tetroxide, 0.8 % potassium ferrocyanide, and 5 mM calcium chloride in 0.1 M cacodylate buffer (pH 7.2) for 60 min, dehydrated in an acetone series, and embedded in Epoxy resin. Ultrathin sections were stained with 5 % uranyl acetate and lead citrate and observed in a Zeiss 900 transmission electron microscope (Carl Zeiss AG, Oberkochen, Germany) operating at 80 kV.

**Results**

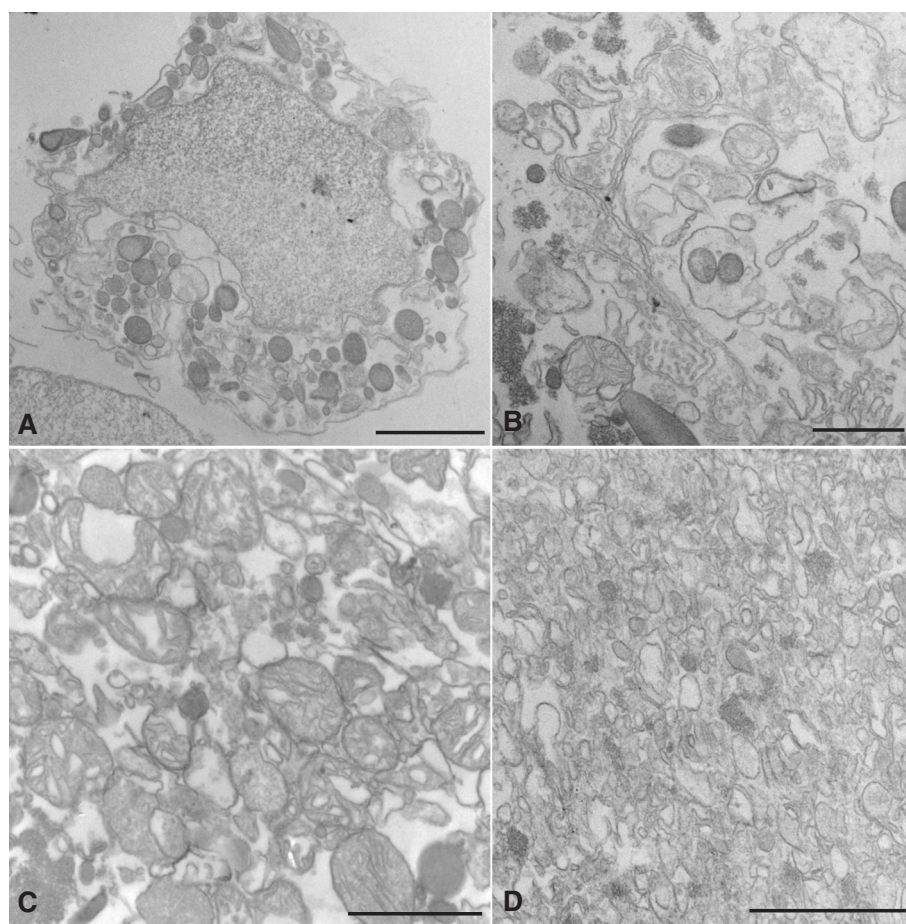
The viability of labeled cells was higher than 93 % in all cases. The distribution of <sup>99m</sup>Tc radioactivity in BMSC organelles is shown in Figs. 1 and 2. The labeling efficiency results are presented as mean ± standard deviation of five

independent experiments. Most of the radioactivity remained in the third supernatant (Figs. 1 and 2), which contained the cytosol fraction formed by ribosomes unbound to membrane and soluble molecules. However, approximately 39 % of the radioactivity remained bound to the first pellet, containing the nuclei-rich fraction.

To confirm that cell disruption and organelle separation were efficient, transmission electron microscopy assays of all pellets were performed. Figure 3 shows that the first pellet contained cells that were not lysed (Fig. 3a) and nuclei and large cell fragments (Fig. 3b).



**Fig. 2** Distribution of 99m-technetium radioactivity in bone marrow mononuclear subcellular fractions. Pellet I: nucleus, cells that were not lysed, and large fragments of plasma membrane; pellet II: mainly mitochondria, liposomes, and peroxisomes; pellet III: microsomal fraction (endoplasmic reticulum and plasma membrane fragments); supernatant III: cytoplasm, ribosomes unbound to membrane, and soluble molecules



**Fig. 3** Ultrathin sections of bone marrow mononuclear subcellular fractions observed under transmission electron microscope. Partially disrupted cells (a) and large cell fragments (b) were found in pellet I, whereas mitochondria and lysosomes were the major component of pellet II (c). Many membrane profiles were observed in pellet III (d). Bars correspond to 20  $\mu\text{m}$  (a), 10  $\mu\text{m}$  (b), and 1  $\mu\text{m}$  (c and d)

The second pellet consisted mainly of mitochondria, lysosomes, and peroxisomes (Fig. 3c), and the third pellet (Fig. 3d) was a typical microsomal fraction, constituted by endoplasmic reticulum and plasma membrane fragments.

### Discussion

When coupled to  $^{99\text{m}}\text{Tc}$ , cells can be labeled with a relatively inexpensive and widely available radionuclide. Many studies show the feasibility of labeling stem cells with  $^{99\text{m}}\text{Tc}$  to track their homing [10, 15–21]. Usually, molecules such as peptides and antibodies are labeled with  $^{99\text{m}}\text{Tc}$  in order to become probes to monitor cell migration.

There are many mechanisms of labeling molecules. Essentially six major methods are employed in the preparation of labeled compounds for clinical use. The majority of cell labeling methods use a chelating agent. Here, we used a direct method of labeling with high cell viability and stability rates [15, 17–20, 22–25].

Radionuclide cell labeling has already been applied for tracking cells in cell therapy for myocardial infarction

[30–32], cirrhosis [20], and acute stroke [18, 19, 33] in humans. The 6-h half-life of  $^{99\text{m}}\text{Tc}$  is an important advantage over the half-life of 110 min of [18F]FDG. 111-Indium-oxine, another commonly used radiopharmaceutical, allows cell tracking for up to 96 h but has disadvantages that include suboptimal photon energies, low-resolution images, and the requirement of an 18- to 24-h interval between injection and imaging [34, 35].  $^{99\text{m}}\text{Tc}$  allows imaging for 24–48 h and results in higher image resolution and a lower radiation burden to the patient [34, 35].

Previous work by our group evaluated the binding sites of  $^{99\text{m}}\text{Tc}$  to mononuclear leukocytes since radiolabeled leukocytes have a potential for clinical use in detecting sites of inflammation [24]. In this work, we analyzed the binding sites of  $^{99\text{m}}\text{Tc}$  to BMMCs, which have a different composition when compared with peripheral blood.  $^{99\text{m}}\text{Tc}$ -labeled bone marrow mononuclear fraction has been widely used in cell therapy experiments [17–20] with the objective of tracking them after systemic infusion.

Moreover, our findings were improved by the addition of electron microscopy data.

One of the most famous and most used radiopharmaceuticals to label leukocytes is  $^{99m}\text{Tc}$ -hexamethylpropyleamine oxime (HMPAO). Some studies showed that  $^{99m}\text{Tc}$ -HMPAO has high selectivity for eosinophils from blood compared with neutrophils and other blood leukocytes [26, 36]. In these cases, it was also shown that  $^{99m}\text{Tc}$ -HMPAO is stored in the eosinophils mainly in nuclear and cytoplasmic compartments.

As a crucial step to understanding the mechanism of radiopharmaceutical localization in a specific target organ for cell therapy, the interaction of the  $^{99m}\text{Tc}$  with bone marrow cells was evaluated. Our results showed that this is an intracellular labeling procedure that has cytoplasm, ribosomes unbound to membrane, and soluble molecules as targets. However, the natural interaction between  $^{99m}\text{Tc}$  to the cytosolic substrate still has to be elucidated.

Other radiopharmaceuticals, such as  $^{99m}\text{Tc}$ -methoxyisobutylisonitrile (MIBI) and  $^{99m}\text{Tc}$ -dimercaptosuccinic acid (DMSA), have had their binding sites studied before [27, 28, 37]. Similar to our results, data from whole heart preparations, largely derived from differential centrifugation techniques, indicated that most of  $^{99m}\text{Tc}$ -MIBI appears to be associated with the cytosolic fraction. In this study, especially designed to compare results of subcellular fractionation obtained with  $^{99m}\text{Tc}$ -(N-ethoxy,N-ethyl dithiocarbamate) nitrido (N-NOEt) and  $^{99m}\text{Tc}$ -MIBI, interesting results emerged [37, 38]. The fact that  $^{99m}\text{Tc}$ -N-NOEt activity was not released into the cytosol after membrane and organelle disruption suggested that this lipophilic marker remained tightly bound to the hydrophobic components of the cells. On the other hand, the monocationic  $^{99m}\text{Tc}$ -MIBI complex, in the same situation, was removed from disrupted mitochondria and transferred to the aqueous cytosolic phase. However, experiments that use subcellular fractionation procedures should be observed with caution because of dependence of the results on two important parameters: time of homogenization and centrifugation rates. In the mentioned study, if centrifugation time was extended to 180 sec, it was observed that approximately 70 % of  $^{99m}\text{Tc}$ -MIBI activity was released to cytosolic fraction as a result of disruption of mitochondria [38]. This result is in agreement with those reported by Crane et al. [37].

Subcellular distribution of  $^{99m}\text{Tc}$ -DMSA (dimercaptosuccinic acid) complex in the rat kidney has also been studied. One hour after intravenous injection of labeled DMSA, kidney tissue homogenate preparations were subjected to differential subfractionation to obtain cell organelles. Radioactivity distribution in relation to total radioactivity of kidney homogenate obtained in five repeated experiments was similar to our results [27, 28].

## Conclusions

In conclusion, the mechanisms involved in the cellular uptake of  $^{99m}\text{Tc}$  in bone marrow cells are not known, but the fact that the activity is distinctly localized in unique compartments indicates some specificity and not just a general distribution among structures.

Molecular imaging is undergoing constant change and is rapidly expanding. It spans all current life sciences and is being used at the frontiers of modern research. For the clinical radiologist, the future will bring applications of molecular imaging techniques into the standard diagnostic workflow.

## Abbreviations

BMMC: Bone marrow mononuclear cell; DAPI: 4'-Diamidino-2-phenylindole; DMEM: Dulbecco's modified Eagle's medium; DMSA: Dimercaptosuccinic acid; [ $^{18}\text{F}$ ]FDG: 18F-Fluorodeoxyglycose; HMPAO: Hexamethylpropyleamine oxime; MIBI: Methoxyisobutylisonitrile; N-NOEt: (N-ethoxy,N-ethyl dithiocarbamate) nitrido; PBS: Phosphate-buffered saline;  $^{99m}\text{Tc}$ : 99m Technetium.

## Competing interests

The authors declare that they have no competing interests.

## Authors' contributions

BG and RCSG helped to design the research, to analyze the data, and to write the manuscript. LMBF helped to design the research and to analyze the data. GDS helped to design and perform the research, to analyze the data, and to write the manuscript. SALS helped to perform the research, to analyze the data, and to write the manuscript. RPR helped to perform the research. NLCS and ACCC helped to analyze the data. ABC helped to analyze the data and to write the manuscript. LMBF helped only to analyze the data. All authors have read and approved the manuscript.

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## References

1. Frey-Vasconcelis J, Whittlesey KJ, Baum E, Feigal EG. Translation of stem cell research: points to consider in designing preclinical animal studies. *Stem Cells Transl Med.* 2012;1:353–8. doi:10.5966/sctm.2012-0018.
2. Liu X, Wang Z, Wang R, Zhao F, Shi P, Jiang Y, et al. Direct comparison of the potency of human mesenchymal stem cells derived from amnion tissue, bone marrow and adipose tissue at inducing dermal fibroblast responses to cutaneous wounds. *Int J Mol Med.* 2013;31:407–15. doi:10.3892/ijmm.2012.1199.
3. Gul H, Lu W, Xu P, Xing J, Chen J. Magnetic carbon nanotube labelling for haematopoietic stem/progenitor cell tracking. *Nanotechnology.* 2010;21:155101. doi:10.1088/0957-4484/21/15/155101.
4. Andreas K, Georgieva R, Ladwig M, Mueller S, Notter M, Sittlinger M, et al. Highly efficient magnetic stem cell labeling with citrate-coated superparamagnetic iron

- oxide nanoparticles for MRI tracking. *Biomaterials*. 2012;33:4515–25. doi:10.1016/j.biomaterials.2012.02.064.
5. Kiessling F. Noninvasive cell tracking. *Handb Exp Pharmacol*. 2008;305–21. doi:10.1007/978-3-540-77496-9\_13.
  6. Hong H, Yang Y, Zhang Y, Cai W. Non-invasive cell tracking in cancer and cancer therapy. *Curr Top Med Chem*. 2010;10:1237–48.
  7. Bonekamp D, Smith MA, Zhu H, Barker PB. Quantitative SENSE-MRSI of the human brain. *Magn Reson Imaging*. 2010;28:305–13. doi:10.1016/j.mri.2009.11.003.
  8. Banerjee SR, Pullambhatla M, Byun Y, Nimmagadda S, Foss CA, Green G, et al. Sequential SPECT and optical imaging of experimental models of prostate cancer with a dual modality inhibitor of the prostate-specific membrane antigen. *Angew Chem*. 2011;50:9167–70. doi:10.1002/anie.201102872.
  9. Miroslavov AE, Sidorenko GV, Suglobov DN, Lumpov AA, Gurzhiy VV, Grigor'ev MS, et al. Technetium(I) carbonyl dithiocarbamates and xanthates. *Inorg Chem*. 2011;50:1098–104. doi:10.1021/ic1019313.
  10. Frangioni JV, Hajjar RJ. In vivo tracking of stem cells for clinical trials in cardiovascular disease. *Circulation*. 2004;110:3378–83. doi:10.1161/01.CIR.0000149840.46523.FC.
  11. Leiker M, Suzuki G, Iyer VS, Canty Jr JM, Lee T. Assessment of a nuclear affinity labeling method for tracking implanted mesenchymal stem cells. *Cell Transplant*. 2008;17:911–22.
  12. Zink D, Sadoni N, Stelzer E. Visualizing chromatin and chromosomes in living cells. *Methods*. 2003;29:42–50.
  13. Weir C, Morel-Kopp MC, Gill A, Tinworth K, Ladd L, Hunyor SN, et al. Mesenchymal stem cells: isolation, characterisation and in vivo fluorescent dye tracking. *Heart Lung Circ*. 2008;17:395–403. doi:10.1016/j.hlc.2008.01.006.
  14. Li SC, Tachiki LM, Luo J, Dethlefs BA, Chen Z, Loudon WG. A biological global positioning system: considerations for tracking stem cell behaviors in the whole body. *Stem Cell Rev*. 2010;6:317–33. doi:10.1007/s12015-010-9130-9.
  15. Carvalho AB, Quintanilha LF, Dias JV, Paredes BD, Mannheimer EG, Carvalho FG, et al. Bone marrow multipotent mesenchymal stromal cells do not reduce fibrosis or improve function in a rat model of severe chronic liver injury. *Stem Cells*. 2008;26:1307–14. doi:10.1634/stemcells.2007-0941.
  16. Quintanilha LF, Mannheimer EG, Carvalho AB, Paredes BD, Dias JV, Almeida AS, et al. Bone marrow cell transplant does not prevent or reverse murine liver cirrhosis. *Cell Transplant*. 2008;17:943–53.
  17. Battistella V, de Freitas GR, da Fonseca LM, Mercante D, Gutfilen B, Goldenberg RC, et al. Safety of autologous bone marrow mononuclear cell transplantation in patients with nonacute ischemic stroke. *Regen Med*. 2011;6:45–52. doi:10.2217/rme.10.97.
  18. da Fonseca LMB, Gutfilen B, de Castro PHR, Battistella V, Goldenberg RC, Kasai-Brunswick T, et al. Migration and homing of bone-marrow mononuclear cells in chronic ischemic stroke after intra-arterial injection. *Exp Neurol*. 2010;221:122–8. doi:10.1016/j.expneurol.2009.10.010.
  19. Barbosa da Fonseca LM, Battistella V, de Freitas GR, Gutfilen B, Dos Santos Goldenberg RC, Maiolino A, et al. Early tissue distribution of bone marrow mononuclear cells after intra-arterial delivery in a patient with chronic stroke. *Circulation*. 2009;120:539–41. doi:10.1161/CIRCULATIONAHA.109.863084.
  20. Couto BG, Goldenberg RC, da Fonseca LM, Thomas J, Gutfilen B, Resende CM, et al. Bone marrow mononuclear cell therapy for patients with cirrhosis: a Phase 1 study. *Liver Int*. 2011;31:391–400. doi:10.1111/j.1478-3231.2010.02424.x.
  21. Zhang SJ, Wu JC. Comparison of imaging techniques for tracking cardiac stem cell therapy. *J Nucl Med*. 2007;48:1916–9. doi:10.2967/jnumed.107.043299.
  22. Vasconcelos-dos-Santos A, Rosado-de-Castro PH, Lopes de Souza SA, da Costa Silva J, Ramos AB, Rodriguez de Freitas G, et al. Intravenous and intra-arterial administration of bone marrow mononuclear cells after focal cerebral ischemia: Is there a difference in biodistribution and efficacy? *Stem Cell Res*. 2012;9:1–8. doi:10.1016/j.scr.2012.02.002.
  23. Barbosa da Fonseca LM, Xavier SS, de Castro PH R, Lima RS, Gutfilen B, Goldenberg RC, et al. Biodistribution of bone marrow mononuclear cells in chronic chagasic cardiomyopathy after intracoronary injection. *Int J Cardiol*. 2011;149:310–4. doi:10.1016/j.ijcard.2010.02.008.
  24. Gutfilen B, Rossini A, Martins FP, da Fonseca LM. Tc-99m-leukocytes—is it an intracellular labelling? *J Clin Lab Immunol*. 1999;51:1–7.
  25. Lopes de Souza SA, Barbosa da Fonseca LM, Torres Gonçalves R, Salomão Pontes D, Holzer TJ, Proença Martins FP, et al. Diagnosis of renal allograft rejection and acute tubular necrosis by 99mTc-mononuclear leukocyte imaging. *Transplant Proc*. 2004;36:2997–3001. doi:10.1016/j.transproceed.2004.11.100.
  26. Puncher MR, Blower PJ. Autoradiography and density gradient separation of technetium-99m-exametazime (HMPAO) labelled leucocytes reveals selectivity for eosinophils. *Eur J Nucl Med*. 1994;21:1175–82.
  27. Vanlic-Razumenic N, Petrovic J. Biochemical studies of the renal radiopharmaceutical compound dimercaptosuccinate. I. Subcellular localization of 99mTc-DMS complex in the rat kidney in vivo. *Eur J Nucl Med*. 1981;6:169–72.
  28. Vanlic-Razumenic N, Petrovic J. Biochemical studies of the renal radiopharmaceutical compound dimercaptosuccinate. II. Subcellular localization of 99Tc-DMS complex in the rat kidney in vivo. *Eur J Nucl Med*. 1982;7:304–7.
  29. Cunha-e-Silva NL, Atella GC, Porto-Carreiro IA, Morgado-Diaz JA, Pereira MG, De Souza W. Isolation and characterization of a reservoir fraction from *Trypanosoma cruzi*. *FEMS Microbiol Lett*. 2002;214:7–12.
  30. Penicka M, Horak J, Kobyłka P, Pytlík R, Kozak T, Belohlávek O, et al. Intracoronary injection of autologous bone marrow-derived mononuclear cells in patients with large anterior acute myocardial infarction: a prematurely terminated randomized study. *J Am Coll Cardiol*. 2007;49:2373–4. doi:10.1016/j.jacc.2007.04.009.
  31. Pessoa PM, Xavier SS, Lima SL, Mansur J, de Almeida AS, Carvalho PA, et al. Assessment of takotsubo (ampulla) cardiomyopathy using iodine-123 metaiodobenzylguanidine scintigraphy. *Acta Radiol*. 2006;47:1029–35. doi:10.1080/02841850600928482.
  32. Kang WJ, Kang HJ, Kim HS, Chung JK, Lee MC, Lee DS. Tissue distribution of 18F-FDG-labeled peripheral hematopoietic stem cells after intracoronary administration in patients with myocardial infarction. *J Nucl Med*. 2006;47:1295–301.
  33. Correa PL, Mesquita CT, Felix RM, Azevedo JC, Barbirato GB, Falcao CH, et al. Assessment of intra-arterial injected autologous bone marrow mononuclear cell distribution by radioactive labeling in acute ischemic stroke. *Clin Nucl Med*. 2007;32:839–41. doi:10.1097/RLU.0b013e318156b980.
  34. Palestro CJ, Love C, Bhargava KK. Labeled leukocyte imaging: current status and future directions. *Q J Nucl Med Mol Imaging*. 2009;53:105–23.
  35. Banerjee SR, Maresca KP, Francesconi L, Valliant J, Babich JW, Zubieta J. New directions in the coordination chemistry of 99mTc: a reflection on technetium core structures and a strategy for new chelate design. *Nucl Med Biol*. 2005;32:1–20. doi:10.1016/j.nucmedbio.2004.09.001.
  36. Moberg L, Karawajczyk M, Venge P. (99m)Tc-HMPAO (Cereteq) is stored in and released from the granules of eosinophil granulocytes. *Br J Haematol*. 2001;114:185–90.
  37. Crane P, Laliberte R, Heminway S, Thoolen M, Orlandi C. Effect of mitochondrial viability and metabolism on technetium-99m-sestamibi myocardial retention. *Eur J Nucl Med*. 1993;20:20–5.
  38. Uccelli L, Giganti M, Duatti A, Bolzati C, Pasqualini R, Cittanti C, et al. Subcellular distribution of technetium-99m-N-NOEt in rat myocardium. *J Nucl Med*. 1995;36:2075–9.

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