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# Axonal Terminals Exposed to Amyloid- $\beta$ May Not Lead to Pre-Synaptic Axonal Damage

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# Abstract

**Background**—Synaptic deficits and neuronal loss are the major pathological manifestations of Alzheimer's disease. However, the link between the early synaptic loss and subsequent neurodegeneration is not entirely clear. Cell culture studies have shown that amyloid- $\beta$  (A $\beta$ ) applied to axonal terminals can cause retrograde degeneration leading to the neuronal loss, but this process has not been demonstrated in live animals.

**Objective**—To test if  $A\beta$  applied to retinal ganglion cell axonal terminals can induce axonal damage in the optic nerve and optic tract in mice.

**Methods**—A $\beta$  was injected into the terminal field of the optic tract, in the left lateral geniculate nucleus of wildtype C57BL/6 mice. Following the injection, monthly diffusion tensor imaging was performed. Three months after the injection, mice underwent visual evoked potential recordings, and then sacrificed for immunohistochemical examination.

**Results**—There were no significant changes seen with diffusion tensor imaging in the optic nerve and optic tract 3 months after the  $A\beta$  injection. The myelin and axons in these regions remained intact according to immunohistochemistry. The only significant changes observed in this study were delayed transduction and reduced amplitude of visual evoked potentials, although both  $A\beta$  and its reversed form caused similar changes.

**Conclusion**—Despite the published *in vitro* studies, there was no significant axonal damage in the optic nerve and optic tract after injecting A $\beta$  onto retinal ganglion cell axonal terminals of wildtype C57BL/6 mice.

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### Keywords

Amyloid- $\beta$  injection; diffusion tensor image; mouse; retinal ganglion cell; retrograde degeneration; visual evoked potential

# INTRODUCTION

Alzheimer's disease (AD) is the leading cause of senior dementia. One in three seniors' die with dementia, and AD is the sixth leading cause of death in the United States. The initial symptoms of memory loss and cognitive decline have been associated with synaptic deficits caused by the toxic effects of amyloid- $\beta$  (A $\beta$ ) [1–8]. During the course of AD, many regions of the brain lose substantial numbers of neurons. Compared to the initial synaptic deficits, loss of neurons may constitute a later, more irreversible damage to the nervous system. However, the mechanisms leading to neuronal loss in AD are still not fully understood.

In the nervous system,  $A\beta$  is produced from the proteolysis of amyloid- $\beta$  protein precursor ( $A\beta$  PP) [9–11] and possibly released from axonal terminals into the extracellular space [12, 13]. To examine whether the axonal terminal associated  $A\beta$  can cause retrograde axonal degeneration, recent cell culture studies using microfluidic devices have demonstrated that selectively providing  $A\beta$  to axonal terminals not only reduce proximal synapses but also induce axonal fragmentation and neuronal apoptosis [14–16].  $A\beta$ -induced retrograde axonal degeneration could be a possible mechanism of  $A\beta$ -induced neuronal loss in AD, but this phenomenon has not been examined *in vivo*. We recently investigated the white matter integrity in mice after  $A\beta$  intracerebroventricular injection. Two months after the injection, severe axonal and myelin damage was found in the optic nerves (ON) and optic tracts (OT) [17]. Because the neuronal bodies of the axons of ON and OT are retinal ganglion cells (RGC) located in the eye, the damage to the ON and OT were not likely due to direct effects of  $A\beta$  on the somata or dendrites, but possibly due to the vicinity of nerve fibers to the injected  $A\beta$ . Altogether, data supports the idea that  $A\beta$  may induce retrograde axonal degeneration, providing a possible mechanism of neuronal loss in AD.

RGCs, whose cell bodies are within the eye, while their axons form the ON and OT in the brain, provide a novel *in vivo* model to allow selective exposure of axonal terminals to Aβ. In this study, we injected Aβ specifically into the OT terminal field located in the lateral geniculate nucleus (LGN). To evaluate the changes within the ON and OT longitudinally, diffusion tensor imaging (DTI) was used to track the degeneration process monthly for 3 months after the injection [17–21]. DTI is a non-invasive magnetic resonance imaging (MRI) modality, which quantifies molecular water diffusion in 3-dimensional space. Because water diffusion is restrained by cell membranes and organelles, DTI derived indices can reveal tissue microstructural changes, which can serve as *in vivo* surrogate markers for neural damage [20–25]. In white matter fiber tracts, water diffusion along various directions can be quantified as diffusion anisotropy, which includes relative anisotropy (RA) and fractional anisotropy (FA). White matter disruption usually leads to a decrease of diffusion anisotropy. Thus, diffusion anisotropy has been used as a non-invasive marker of white matter damage.

In addition, from DTI, one can also derive the trace of diffusion tensor (Tr), which quantifies the average water diffusion in all directions, axial diffusivity ( $\lambda_{\parallel}$ ), the diffusion along the axis of fiber bundles, and radial diffusivity ( $\lambda_{\perp}$ ), the diffusion across the fiber bundles. We have previously demonstrated that  $\lambda_{\parallel}$  and  $\lambda_{\perp}$  are sensitive to the axonal and myelin damage respectively in mouse ON and OT [21].

At the end of the time course, visual evoked potentials (VEPs) were recorded to examine the electrophysiological condition of the visual system of each animal. Animals were then sacrificed for tissue examination by immunohistochemistry. Antibodies against neurofilament and myelin basic protein were utilized to assess the integrity of axon and myelin of nerves affected by  $A\beta$  [26, 27].

## MATERIALS AND METHODS

All experimental procedures were in accordance with National Institutes of Health guidelines and were approved by the Institutional Animal Care and Use Committee of the Loma Linda University.

#### Injection

Human A $\beta_{1-42}$  (A9810, Sigma Aldrich, USA) or the reverse peptide (rA $\beta$ , SCP0048, Sigma Aldrich, USA) were dissolved in sterile saline and incubated at 37°C for 72 h [28–30]. This process allowed A $\beta$  to form aggregates before being injected into the animals. Twelve female C57BL/6 mice at 12-weeks old were anesthetized by 1.5% isoflurane/oxygen using an isoflurane vaporizer (VetEquip, Pleasanton, CA). The body temperature was maintained using an electric heating pad. Mice were placed in a stereotactic apparatus. Fur above the incision site was shaved and skin was cleaned with iodine. A $\beta$  4 nmole/3 µl (n = 8) or 10 nmole/3 µl (n = 5), or rA $\beta$  4 nmole/3 µl (n = 5) was injected 0.1µl/min into the left OT terminal area located in LGN (coordinates: posterior 2.0mm from the bregma, lateral 2.0mm left lateral to midline, and 2–2.5mm ventral to the cortical surface), using a 10-µl Hamilton syringe [28–30]. The needle was kept in the injection site for 5 min and then withdrawn 0.5mm every 5 min until completely removed from the skull.

#### Imaging procedure

Before injection and monthly after injection, mice were examined with DTI. Mice were anesthetized with a mixture of oxygen and isoflurane. Core body temperature was maintained at  $37.0 \pm 0.5$  °C using warm water circulating in a pad. Mice were placed in a holder to immobilize the head. A 7-cm inner volume coil was used as a transmitter coil and a 1.5-cm inner diameter surface coil was used as a receiver to collect data in a Bruker 4.7T BioSpec small animal MRI instrument. Images with slice thickness 0.5 mm, field of view of 2 cm × 2 cm and matrix 128 × 128 (zero filling to 256 × 256) were collected to cover the visual system from the eye to superior colliculus. Spin-echo DTI was performed with TR 3 s, TE 29 ms, duration between a diffusion gradient pair ( ) = 20 ms, diffusion gradient duration ( $\delta$ ) = 3 ms, and six-direction diffusion scheme with b-values of 0 and 0.85 ms/µm<sup>2</sup>. Using software written in Matlab (MathWorks, Natick, MA, USA), the eigenvalues ( $\lambda_1$ ,  $\lambda_2$ ,

and  $\lambda_3$ ) derived from diffusion tensor were used to calculate  $\lambda_{\parallel}$ ,  $\lambda_{\perp}$ , RA, and Tr defined by the following equations:

$$Tr = \lambda_1 + \lambda_2 + \lambda_3 \quad (1)$$
$$\lambda_{\parallel} = \lambda_1 \quad (2)$$
$$\lambda_{\perp} = 0.5 \times (\lambda_2 + \lambda_3) \quad (3)$$

$$RA = \frac{\sqrt{(\lambda_1 - Tr/3)^2 + (\lambda_2 - Tr/3)^2 + (\lambda_3 - Tr/3)^2}}{\sqrt{3}(Tr/3)} \quad (4)$$

Regions of interest (ROI) were selected in the ON and OT referenced to the mouse brain atlas [31]. Data were presented as mean  $\pm$  standard deviation. Paired *t*-tests were used to compare DTI indices between the ipsilateral and contralateral sides for each ROI. Repeated measures analysis of variance (ANOVA)was carried out to compare the time course of each measurement between A $\beta$ -treated and control mice. *P*-values were considered to be statistically significant at  $\alpha < 0.05$ . All statistical analyses were conducted with Matlab (MathWorks, Natick, MA, USA).

#### Visual evoked potential

Core body temperature was maintained at  $37.0 \pm 0.5^{\circ}$ C using a heating pad. To minimize discomfort, Lidocaine was applied to all incision sites and soft tissue pressure points. A midline incision was made to expose the skull. Two small holes were drilled and silver wires were placed over the visual cortex (0.5 mm anterior and 2.5 mm lateral to the Lambda point) and cerebellum (1.5 mm posterior to Lambda) for recording and reference, respectively [32]. After dark adaption for 10 min, light stimulation was produced by a LED light source (Radioshack, Fort Worth, TX), at frequency of 0.2 Hz with a duration of 5ms [33]. Field potentials were recorded using a CyberAmp380 amplifier (Molecular Devices, Sunnyvale, CA) and a Digidata1440A interface (Molecular Devices, Sunnyvale, CA), with a sampling rate of 20 KHz and a bandpass filter of 0.1–300 Hz, controlled by Clampex 10.2 (Molecular Devices, Sunnyvale, CA). Averaged data from 100 continuous traces was used to calculated implicit time and amplitude of major negative component for each mouse.

#### Immunohistochemistry examination

At 3 months after Aβ treatment, animals were intracardially perfused with4%paraformaldehyde in PBS.A 4-mm-thick coronal section (-1 to +3mm of bregma) was obtained from each brain and embedded in paraffin. Brain tissue slices, 3µm thickness, matching the MRI imaging sections, were cut and deparaffinized in xylene for immunohistochemical examinations. The integrity of axons was evaluated using a primary antibody against phosphorylated neurofilament (SMI-31, 1:1000; Sternberger Monoclonals, Lutherville, Maryland), and myelin integrity was assessed with a primary antibody against

myelin basic protein (MBP, 1:250; Zymed Laboratories Inc., South San Francisco, CA) at 4°C overnight [34]. Following a 15-min wash in PBS, sections were incubated in fluorescent secondary antibodies for 1 h at room temperature (1:200, Goat anti-mouse conjugated to Texas red for SMI-31, 1:200, Goat anti-rabbit conjugated to green for MBP; Molecular Probes). Immunohistochemistry of glial fibrillary acidic protein (GFAP, 1:1000, Cell Signaling) was also performed. Histological sections were examined using an Olympus Fluoview confocal microscope equipped with a 60× oil objective. The red SMI-31 positive staining, representing the normal axons, was captured. Axons were counted through the central  $70 \times 70 \mu m^2$  regions. The counts per 100  $\mu m^2$  were presented as mean ± standard deviation.

# RESULTS

Representative DTI maps, including  $\lambda_{\parallel}$ ,  $\lambda_{\perp}$ , RA, and TR, of mouse brains from the Aβtreated and control mice are shown in Fig. 1. White matter tracts, including ON and OT, can be easily identified. DTI maps of Aβ-treated mice appear similar to those acquired from the control mice. Quantitative analysis, including  $\lambda_{\parallel}$ ,  $\lambda_{\perp}$ , RA, and TR from ON and OT are summarized in Fig. 2. The time course of DTI indices show small fluctuations, but these changes are not statistically significant. Increasing the dosage of Aβ from 4 to 10 nmole did not lead to significant differences in DTI either; DTI of ON and OT from both groups are statistically indistinguishable from control mice.

Immunohistochemistry using SMI-31 and MBP was performed to examine the integrity of axons and myelin of ON and OT in 3 months after A $\beta$  treatments (Fig. 3). The A $\beta$ -treated nerves did not show significant damage compared to control nerves. We also stained for GFAP to examine potential astrocytic reaction in these nerves. Again, astrocyte morphology appeared normal in ON and OT of A $\beta$ -treated mice (Fig. 4).

The only significant changes in the A $\beta$ -treated mice were observed in the recorded VEP (Fig. 5), which quantifies the nerve transduction from retina to visual cortex. Three months after the injection of 4 nmole A $\beta$ , A $\beta$ -affected visual pathways showed a significant 40–50% reduction of VEP amplitude; in contrast, the VEPs from contralateral eyes of the same mice remained normal. Similar effects were found in mice after a 10 nmole A $\beta$  injection, which showed a significant 60–70% reduction of the VEP amplitude and a significant 16–26% increase of the VEP latency in the A $\beta$ -affected pathway, with normal VEPs recorded from contralateral eyes. Mice injected with reverse A $\beta$  peptide (rA $\beta$ , 4 nmole) also had changes in VEP. The rA $\beta$ -affected eyes showed a significant 56–67% reduction of the VEP amplitude and a significant 10–16% increase of the VEP latency, and the contralateral eyes showed normal VEPs recorded.

# DISCUSSION

In this study, we examined whether  $A\beta$  can induce retrograde degeneration in live mice. We took the advantage of the unique anatomical features of RGCs to selectively expose their axon terminals to  $A\beta$ . *In vivo* DTI and postmortem immunohistological examinations confirmed that the axons of RGCs, which form ON and OT in the brain, remained intact 3

months after A $\beta$  injection. However, the VEP examinations showed ~50% reduction of amplitude and ~20% delay in the A $\beta$ -affected visual pathways compared to the controls. These findings indicate that the injected A $\beta$  did impede flow of visual information from the retina to visual cortex, though it did not cause noticeable RGC degeneration.

Although the manifestation of AD is likely due to many factors,  $A\beta$ , a key component of amyloid plaques, is important in the pathogenesis of AD [2]. A $\beta$  is produced from the cleavage of A $\beta$  PP [35], which is transported centrifugally along axons from somata to the axonal terminals [13]. Thus, it has been speculated that AB released from axonal terminals may have detrimental effects on its cell of origin. In the brains of AD patients, a reduction of basal forebrain cholinergic neurons has been commonly reported [36]. However, their cell bodies are located in nuclei physically remote from areas of preferential A $\beta$  accumulation [37, 38], indicating possible A $\beta$ -induced retrograde degeneration [39]. Results from *in vitro* experiments support this idea [16, 40, 41]. Novel microfabrication and microfluidic technologies have enabled the development of cell culture devices with multiplecompartmental chambers connected with micron-size grooves. Neurons plated in one compartment can grow axons across the compartments while maintaining fluidic isolation [16]. Using these devices, studies have found that selective exposure of axons and axon terminals to A $\beta$  can cause axonal destruction, which leads to nuclear apoptosis [14–16]. In sum, evidence suggests that exposing axon terminals to  $A\beta$  may play a critical role in initiating retrograde neurodegeneration in patients with AD.

We have previously investigated white matter integrity in mice after an A $\beta$  injection into the lateral ventricle [17]. Two months after the injection, the OTs, which are located adjacent to the A $\beta$ -injected ventricle, showed a significant 83% increase in  $\lambda_{\perp}$  and a significant 31% decrease in RA of measurements from in vivo DTI. Similar damage extended to ON of the same mice. This damage was confirmed by the immunohistochemistry showing significant 30–40% loss of axons and myelin. Given that the axons of ON and OT have their cell bodies located in the eyes, the data supported the idea that  $A\beta$  could precipitate axonal degeneration without affecting soma or dendrites first. However, the exact route of A $\beta$  exposure necessary to trigger the damage is unclear. In the present study, exposing OT axonal terminal areas to A $\beta$  did not cause significant damage to ON and OT. We suspect that A $\beta$ intracerebroventricular injection may cause more profound effects on mice perhaps by triggering immune responses and enhancing the cellular stress, leading to a larger degree of damage compared to focal injection of A $\beta$  in this study. It is also possible that the A $\beta$ intracerebroventricular injection directly affected myelin and axons of the visual pathway, in addition to axonal terminals as in this study [42-44]. Further investigations are needed to better understand the mechanisms responsible for retrograde axonal degeneration in AD.

A unique feature of the present study is that both structural and functional assessments were taken to evaluate the visual system in mice affected by  $A\beta$ . DTI provided high resolution measurements for microstructural changes in ON and OT. Meanwhile, VEP provided functional assessments for the visual system. We found no evidence of structural change based on DTI, but all animals suffered from functional declines based on VEP. Structural and functional assessments offer complementary information about the condition of the nervous system. In most cases, structural imaging provides better spatial information to

characterize location of damage. However, as shown in this study, the functional declines can be significant even if there are no detectable changes by structural imaging. Both functional and structural examinations need to be taken into account to provide a better evaluation of the nervous system.

Visual problems are commonly observed in AD patients. Low-level measures of visual ability in tests of stereo acuity, color discrimination, contrast sensitivity, visual processing speed, and visual field coverage are worse in AD patients, compared to the similarly aged controls [45–55]. Although visual problems are not usually considered as a disease hallmark of AD, the visual deficits have been found to correlate with the severity of dementia [56], suggesting that visual declines and dementia may share the same pathogenesis in AD. Assessing retinal degeneration in patients may serve as an important biomarker in improving the diagnosis and therapeutic outlook for AD patients [57, 58].

The size of LGN is relatively substantial, with its middle transactional size similar to a lateral ventricle [31]. Thus, micro injection into the LGN was not technically challenging, compared to the ventricular injection, which is a common procedure in a neuroscience lab. It would be ideal in this study if the needle traces could be examined in all mice to confirm the correct location of the injection. When examining these animals using MRI and postmortem histology in this study, however, we were only able to characterize partial but not the complete needle traces. Since the MRI and histology were performed months after injection, we suspect that the brain tissue separated by the needle may have been partially repaired. Although the misallocation of an injection site could be a concern, deteriorated VEPs were consistently recorded from the injected mice suggesting that the injection affected the visual system in all mice. Altogether, the data support that the injection successfully delivered A $\beta$  to the LGN, which caused significant delay in VEPs but did not lead to detectable damage in ON and OT.

It is not clear why both  $A\beta$  and its reversed form (rA $\beta$ ) altered VEPs. rA $\beta$  injection was used as a control group because it was assumed to be inactive with same molecular weight of A $\beta$ . However, the exact biological effects of rA $\beta$  are not known. Despite its reversed form, rA $\beta$ may contain fragments which are toxic to synapses, and possibly damage neurons [59, 60]. Based on the studies from literature, it is not uncommon for reversed or scrambled forms of A $\beta$  to be excluded from control groups in studies using A $\beta$ . rA $\beta$  may have biological effects which warrant further investigations.

It is worth to note that prior studies have demonstrated that the monomeric A $\beta$  is less toxic than its oligomeric or fibrillar forms [61]. Thus, before the injection into animals, A $\beta$  was incubated at 37°C for 72 h to form aggregates [28–30]. These aggregates can be detected microscopically using Congo red staining. The injected aggregates may be neurotoxic due to several features: 1) They can serve as a reservoir to gradually release toxic A $\beta$  oligomers to injure the brain [61]; 2) The released aggregates may serve as seeds to spread the damage to larger brain areas [62]; and 3) Aggregates may induce microglial activation and precipitate neuro-inflammatory damage [63]. Altogether, the incubation process is a critical step to vender strong A $\beta$  toxic effects in the animals [28–30].

In conclusion, this study examined whether exposing OT axonal terminals to  $A\beta$  could cause axonal damage in the ON and OT. Three months after the  $A\beta$  treatment, we did not find significant damage to the ON and OT. The only deficits we observed were the alteration of recorded VEPs. Our data suggest that a single dose of  $A\beta$  (4 nmole and 10 nmole) can alter neural conduction but not cause significant retrograde axonal degeneration in the visual pathway of live animals.

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# Fig. 1.

DTI maps of control and A\beta-treated mice. Representative DTI of mice 3 months after A\beta showed images similar to those acquired from mice 3 months after rA\beta injection. The arrows indicate the optic nerves and tracts on RA,  $\lambda_{\parallel}$ ,  $\lambda_{\perp}$ , and TR maps.

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# Fig. 2.

DTI measurements of the optic nerves and tracts after A $\beta$  (4 n or 10 n mole) and rA $\beta$  injection in the left OT axonal terminals. The L and R indicate the left and right side of the ON and OT, respectively. The unit for  $\lambda \parallel$ ,  $\lambda_{\perp}$ , and TR is  $\mu m^2/ms$ . RA is dimensionless. There was no significant change compared to the normal nerves.



#### Fig. 3.

Immunohistochemistry (SMI-31 and MBP) of optic tracts and optic nerves of  $A\beta$ -treated mice. Because  $A\beta$  was injected in the left OT axonal terminal, left OT and right ON were expected to be directly affected by  $A\beta$ . However, both left and right ON and OT appeared no difference, compared to normal nerves. The bar graphs quantified the axonal numbers from left (green bars) and right (red bars) of ON and OT of  $A\beta$ -treated mice and normal mice (blue bars). The axonal counts showed no significant difference among these groups.



# Fig. 4.

GFAP staining of the left (contralateral) and right (A $\beta$ -affected) ON. Both showed normal morphology of astrocytes with no significant sign of injury.

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# Fig. 5.

VEP amplitude and latency of left (white bars) and right eyes (black bars) of normal controls, and mice after A $\beta$  and rA $\beta$  injection in the left side of OT axonal terminals. # and \* indicates significant differences (p < 0.05) compared to the normal controls and between left and right, respectively.