# Tissue stiffness regulates serine/arginine-rich protein-mediated splicing of the extra domain B-fibronectin isoform in tumors

Francois Bordeleau<sup>a</sup>, Joseph P. Califano<sup>a</sup>, Yashira L. Negrón Abril<sup>b</sup>, Brooke N. Mason<sup>a</sup>, Danielle J. LaValley<sup>a</sup>, Sandra J. Shin<sup>c</sup>, Robert S. Weiss<sup>b</sup>, and Cynthia A. Reinhart-King<sup>a, 1</sup>

ªDepartment of Biomedical Engineering, Cornell University, Ithaca, NY 14853; <sup>b</sup>Department of Biomedical Sciences, Cornell University, Ithaca, NY 14853; and <sup>c</sup>Department of Pathology and Laboratory Medicine, The New York Presbyterian Hospital-Weill Cornell Medical College, New York, NY 10065

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Alternative splicing of proteins gives rise to different isoforms that play a crucial role in regulating several cellular processes. Notably, splicing profiles are altered in several cancer types, and these profiles are believed to be involved in driving the oncogenic process. Although the importance of alternative splicing alterations occurring during cancer is increasingly appreciated, the underlying regulatory mechanisms remain poorly understood. In this study, we use both biochemical and physical tools coupled with engineered models, patient samples, and a murine model to investigate the role of the mechanical properties of the tumor microenvironment in regulating the production of the extra domain-B (EDB) splice variant of fibronectin (FN), a hallmark of tumor angiogenesis. Specifically, we show that the amount of EDB-FN produced by endothelial cells increases with matrix stiffness both in vitro and within mouse mammary tumors. Matrix stiffness regulates splicing through the activation of serine/arginine rich (SR) proteins, the splicing factors involved in the production of FN isoforms. Activation of the SR proteins by matrix stiffness and the subsequent production of EDB-FN are dependent on intracellular contractility and PI3K-AKT signaling. Notably, matrix stiffness-mediated splicing is not limited to EDB-FN, but also affects splicing in the production of PKC βII and the VEGF 165b splice variant. Together, these results demonstrate that the mechanical properties of the microenvironment regulate alternative splicing and establish a previously unidentified mechanism by which cells can adapt to their microenvironment.

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alternative splicing | extracellular matrix | matrix stiffness | angiogenesis | cancer progression

Differential expression of protein isoforms through alterna-tive splicing is a key element to generating protein diversity and can result in widely different cell phenotypes and behaviors (1–3). Interestingly, tumors exhibit several major differences in protein isoform expression patterns compared with healthy tissue (2, 4), and some of these changes are thought to favor oncogenesis (1). Notably, splicing events are regulated at the pre-mRNA level by splicing regulatory factors that include a family of serine/arginine rich (SR) proteins (5). Elevated SR protein levels have been associated with cancer (5); however, the physiological cues that drive splicing are not well defined.

Among the various alternatively spliced proteins present in tumors, the splice variant of fibronectin (FN) that includes the extra domain-B (EDB) type III repeat has been of particular interest in the cancer community because inclusion of the EDB fragment has been proposed as a way to identify and target tumor vasculature (6). EDB-FN is produced by endothelial cells (ECs) in tumors and may favor angiogenesis (7–9). Splicing of FN is regulated by several SR proteins, including SRp40 and SRp20, in several different cell types (10–12). Although the presence of EDB-FN is fairly unique to tumor vasculature, the mechanisms governing its expression within the tumor microenvironment are not clear.

The splicing activity of SR proteins that leads to the expression of various protein isoforms including EDB-FN is tightly regulated by phosphorylation (13–15), and this phosphorylation has been shown to be mediated by AKT (14, 16). Interestingly, matrix stiffness can regulate AKT phosphorylation state (17–19). More specifically, recent data indicate that AKT activation and downstream phosphorylation of AKT substrates can occur through changes in the mechanical properties of the tissue in the tumor microenvironment (17). Importantly, tumor tissue stiffens during cancer due to increased collagen deposition and the action of cellsecreted enzymes that cross-link collagen fibrils (20, 21), and this stiffening is believed to be correlated with tumor aggressiveness and metastatic potential (18, 22–25). Elevated extracellular matrix (ECM) stiffness affects several cell behaviors associated with tumors including enhanced cell contractility, response to growth factors, and cell migration (18, 22, 24, 26, 27). Although stiffness has been shown to drive greater AKT activation, AKT activity drives SR protein phosphorylation, and SR proteins mediate splicing, it has not yet been determined whether stiffness-driven signaling can result in SR protein-mediated splicing events during tumorigenesis.

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In this study, we used a multidisciplinary approach, with in vitro and in vivo models and biochemical and physical tools, to study the relationship between matrix stiffness and FN splicing in ECs. Here, we demonstrate, for the first time to our knowledge, that EDB-FN expression increases with matrix stiffness, both in vitro and in mouse mammary tumors. Our data indicate that matrix stiffness

### **Significance**

Alternative splicing is the main mechanism that drives protein diversity; however, little is known about the physiological cues that control splicing. Here, we show that the stiffness of the extracellular matrix mediates protein splicing in cells both in vitro and in vivo. Alternative splicing mediated by matrix stiffness occurs through the phosphorylation of splicing regulatory factors, serine/arginine rich (SR) proteins, and depends on the PI3K signaling pathway. Because the SR family of proteins are conserved among both vertebrates and invertebrates and are known to also be involved in genome stabilization, translation, and mRNA export, these results suggest a previously unidentified mechanism by which cells can respond and adapt to their mechanical microenvironment in both healthy and diseased states.

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<sup>1</sup> To whom correspondence should be addressed. Email: [cak57@cornell.edu](mailto:cak57@cornell.edu).

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regulates the dynamics of EDB-FN splicing through Rhoassociated protein kinase (ROCK) mediated contractility and downstream SR protein phosphorylation. Moreover, phosphorylation of SR proteins correlates with in vivo PI3K/AKT pathway activity in response to tissue stiffness, whereas in vitro inhibition of PI3K prevents SR protein phosphorylation and EDB-FN splicing. Taken together, our data show, for the first time to our knowledge, that the stiffness of the tumor microenvironment modulates intracellular splicing events.

## Results

Extracellular Matrix Stiffness Regulates Protein Splicing. Expression of the EDB-FN splice variant is known to be characteristic of new angiogenic vessels within the tumor vasculature (9). As such, tumor vasculature of human patient samples stained strongly for EDB, whereas significantly less EDB was evident in normal tissue (Fig. 1A). Moreover, a strong EDB-FN signal was evident in tissue extracts from spontaneous mammary tumors formed in a polyoma middle T antigen (PyMT) mouse model of breast cancer, whereas EDB-FN was not evident in normal mammary gland tissue extract from a WT mouse (Fig. 1B).

Because increased tissue stiffness is a hallmark of most solid tumor progression and has been shown to affect fibronectin assembly and deposition (28, 29), we assessed whether tissue stiffness was affecting the expression of the EDB-FN splice variant within PyMT tumors. To that end, we decreased tumor tissue stiffness by preventing ECM cross-linking by treating the mice with the lysyl oxidase inhibitor β-aminopropionitrile (BAPN) (Fig. 2A) (17). Notably, we observed a significant reduction of EDB-FN in tumor extract from PyMT mice that had been treated with BAPN compared with the control (Fig.  $2 B$  and C). In addition, immunostaining of frozen sections also showed a reduction of EDB-FN in BAPN-treated mice (Fig. 2D). Quantification of the EDB-FN content of those tumors indicated a lower EDB content (Fig. 2E). In addition, EDB-FN fiber-like structures were shorter in BAPN mice. In contrast, total FN levels were only minimally affected (Fig.  $2 B$  and F and [Fig. S1](http://www.pnas.org/lookup/suppl/doi:10.1073/pnas.1505421112/-/DCSupplemental/pnas.201505421SI.pdf?targetid=nameddest=SF1)).

To confirm that matrix stiffness was driving FN splicing, we implemented an in vitro system. ECs were seeded on compliant  $(E = 1 \text{ kPa})$  and stiff  $(E = 10 \text{ kPa})$  polyacrylamide substrates, stained, and imaged for both total FN and EDB-FN (Fig. 3A). Both total FN and EDB-FN showed a visible increase on stiffer matrices (Fig. 3B). Similar to what we observed in vivo, quantification of EDB-FN levels revealed increased inclusion of the EDB variant on stiff matrices compared with the amount of total FN (Fig. 3C). Indeed, normalizing the ratio of EDB-FN to total FN as determined by Western blotting indicated that there was a 50% increase in EDB-FN relative to total FN with increasing matrix stiffness (Fig. 3D). To further confirm our observations, quantitative real-time RT-PCR was used to quantify the mRNA



Fig. 1. EDB-FN is expressed in human breast tumor vasculature. (A) Immunohistochemical staining of human breast tissue for EDB-FN showing strong EDB-FN staining in the tumor vasculature and no immunoreactivity for EDB-FN in the normal tissue vasculature (same exposure settings). (Scale bar, 50 μm.) (B) Western blotting on total protein extracts from normal mammary tissue of WT and cancerous tissue of PyMT mice showing the presence of EDB-FN in the tumor.



Fig. 2. Effects of BAPN modulation of in vivo stiffness on EDB-FN in mammary tumors. (A) Mechanical measurements performed on tumor tissue from PyMT mice by unconfined compression reveal that BAPN significantly lowers tissue stiffness compared with the mock treatment (water only, Ctrl). (B) Western blotting of cancerous tissue total protein extracts from PyMT mice given either the mock treatment or treated with BAPN showing EDB-FN and total FN. GAPDH was used as loading control. (C) Corresponding densitometric quantification showing both EDB-FN normalized against GAPDH content and the ratio of EDB-FN to total FN. (D) Confocal images of EDB-FN stained frozen tissue sections with or without BAPN treatment and  $(E)$  the corresponding quantification of the average EDB-FN fiber-like structures length and content. (F) Representative confocal images of total FN and CD31 with or without BAPN treatment. Plots are mean  $\pm$  SE, Student t test:  $*P < 0.05$ ,  $*P < 0.01$ . (Scale bars, 30 µm.)

expression of EDB-FN. Our results indicate that EDB-FN mRNA expression increased ∼2.5-fold on stiff matrices (Fig. 3E). When taken together with the in vivo data, these results clearly demonstrate that increasing matrix stiffness stimulates the inclusion of the EDB domain in FN.

There are several other splice variants known to be up-regulated in tumors apart from EDB-FN (1). Among the numerous proteins that are regulated by splicing and are also associated with tumor progression, the PKC βII and VEGF 165b splice variant are of particular interest because they are, respectively, pro- and antiangiogenic (30, 31). We assayed for the expression of the PKC βII isoform as a function of stiffness. Similar to what was observed for EDB-FN, PKC βII expression was lower in tumor tissue from BAPN-treated mice [\(Fig. S2](http://www.pnas.org/lookup/suppl/doi:10.1073/pnas.1505421112/-/DCSupplemental/pnas.201505421SI.pdf?targetid=nameddest=SF2)A). Interestingly, the antiangiogenic VEGF 165b isoform expression was higher in tumor tissue from BAPN-treated mice ([Fig. S2](http://www.pnas.org/lookup/suppl/doi:10.1073/pnas.1505421112/-/DCSupplemental/pnas.201505421SI.pdf?targetid=nameddest=SF2)B). Of note, both PKC βII and VEGF 165b expression modulation was observed in all of the cells present within the tumor and not found exclusively in ECs. In vitro experiments using polyacrylamide substrates recapitulated these results, where PKC βII expression by ECs was increased more than twofold on stiffer matrices, whereas VEGF 165b expression was de-creased in these conditions [\(Fig. S3](http://www.pnas.org/lookup/suppl/doi:10.1073/pnas.1505421112/-/DCSupplemental/pnas.201505421SI.pdf?targetid=nameddest=SF3)  $C$  and  $D$ ). Notably, these data indicate that matrix stiffness-mediated splicing is not limited solely to EDB-FN or solely to ECs, and it may constitute a



Fig. 3. Expression of the EDB-FN splice variant increases with ECM stiffness in vitro. ECs were plated on compliant ( $E = 1$  kPa) and stiff ( $E = 10$  kPa) substrates (100,000 cells/mL), grown over 3 d, and subjected to immunofluorescence staining or Western blot. (A) Immunofluorescent staining of both EDB-FN and total FN increases with increasing substrate stiffness (images were acquired with the same exposure settings). (Scale bar, 50  $\mu$ m.) (B) Representative Western blot of total protein extracts showing EDB-FN and total FN on compliant and stiff substrates. GAPDH was used as loading control. (C) Densitometric quantification of EDB-FN and total FN normalized against GAPDH content. (D) Corresponding ratio of EDB-FN to total FN showing a 30% increase in EDB-FN expression with increasing stiffness (three independent experiments). (E) EDB-FN expression as determined by quantitative real-time RT-PCR indicates a significant increase in mRNA expression with increasing stiffness (three independent experiments). Plots are mean  $\pm$ SE, Student t test:  $*P < 0.05$ ,  $***P < 0.001$ .

fundamental mechanotransduction mechanism within multiple different cell types.

EDB-FN Splice Variant Expression Is Mediated by Cell Contractility. The ability of cells to adapt to ECM stiffness is known to rely on cell contractility (27). Cellular contractility has been found to typically increase on stiffer matrices and is required for proper activation of several signaling pathways that control gene expression (32–34). As such, we investigated whether cell contractility mediated by the Rho-ROCK pathway could regulate EDB-FN expression. ECs were plated on stiff matrices  $(E = 10 \text{ kPa})$  and treated with the ROCK inhibitor Y27632. Notably, both Western blotting and immunofluorescent staining revealed that ROCK inhibition greatly reduced the amount of EDB-FN present (Fig. 4 A and  $B$ ). We confirmed this observation by using a siRNA-based approach to knock down ROCK in ECs (Fig. 4C). Depletion of ROCK also led to decreased levels of observable EDB-FN (Fig. 4 C and D). Furthermore, direct inhibition of RhoA with the C3 transferase resulted in lower EDB-FN expression (Fig.  $S3A$  and B). Inhibition of cell contractility with either blebbistatin or the myosin light chain kinase inhibitor ML-7 show a similar trend ([Fig. S3](http://www.pnas.org/lookup/suppl/doi:10.1073/pnas.1505421112/-/DCSupplemental/pnas.201505421SI.pdf?targetid=nameddest=SF3)C). Overall, these results indicate that expression of the EDB-FN isoform by ECs depends on Rho-ROCK–mediated cell contractility.

ECM Stiffness Regulates SRp40 Phosphorylation in Culture and in Vivo. In light of the above data implicating ECM stiffness and cell contractility as modulators of EDB-FN splicing, and because SRp40 is one of the main regulators of EDB-FN expression (11, 12), we extended our analysis to the SR proteins. Remarkably, phosphorylation levels of SR proteins increased with matrix stiffness in vitro (Fig.  $5 \land A$  and  $B$ ). Inhibition of cell contractility with the Y27632 inhibitor significantly lowered the phosphorylation of several SR proteins, including SRp40 (Fig. 5C). Immunostaining of PyMT tumors showed a similar effect of BAPN on SR protein

phosphorylation levels, where decreasing tumor stiffness decreased SR protein phosphorylation (Fig. 5D). These data indicate that both matrix stiffness and cell contractility influence the activation of SR proteins involved in splicing regulation.

PI3K Is Required for SRp40-Mediated Splicing of EDB-FN. There are several kinases that are known to phosphorylate SR proteins (14, 15). Among those, AKT has previously been reported as being involved in SRp40-mediated FN splicing (35). Additionally, recent in vivo evidence points to a prominent role of the PI3K/ AKT pathway in regulating cell response to matrix stiffness (17). Therefore, we assessed the extent to which matrix stiffnessmediated EDB-FN splicing occurs through PI3K involvement. Using an antibody against phosphorylated substrates of AKT, we confirmed in vivo that lowering tumor tissue stiffness with BAPN reduced the activity of the PI3K/AKT pathway (Fig. 6A). Similarly, we detected higher phosphorylation levels of AKT when EC were seeded on stiffer matrix  $(Fig. S4)$  $(Fig. S4)$ . We then inhibited PI3K using the pharmacological inhibitor wortmannin in ECs seeded on stiff matrices and assayed for the presence of



Fig. 4. EDB-FN splice variant expression is mediated by cell contractility. (A) Western blot of total protein extract from cells plated on 10-kPa substrates and treated with or without the ROCK inhibitor Y27632 showing a decrease in EDB-FN compared with control. Corresponding densitometric quantification showing both EDB-FN normalized against GAPDH content and the ratio of EDB-FN to total FN.  $(B)$  Representative images of EDB-FN and total fibronectin of EC cells cultured overnight on 10-kPa substrates and treated with or without Y27632. (C) Western blot for ROCK, EDB-FN, and total FN expression after treatment with siRNA against ROCK compared with control. Corresponding densitometric quantification showing both EDB-FN normalized against GAPDH content and the ratio of EDB-FN to total FN. (D) Fluorescent staining for EDB-FN after treatment with siRNA against ROCK on stiff ( $E = 10$  kPa) substrates. Images were acquired using the same exposure settings. Plots are mean  $\pm$  SE, Student t test: \*P < 0.05, \*\*P < 0.01. Images were acquired using the same exposure settings. (Scale bars, 30 μm.)



Fig. 5. The interplay of ECM stiffness and cell contractility regulates SRp40 phosphorylation. (A) Fluorescent staining for phosphorylated SR protein of ECs plated on compliant ( $E = 1$  kPa) and stiff ( $E = 10$  kPa) substrates. (B) Western blot of whole protein extract from ECs plated on either compliant ( $E = 1$  kPa) or stiff ( $E = 10$  kPa) substrates showing an increase in SR protein phosphorylation with increasing substrate stiffness. (C) Western blot of whole protein extract from EC cells plated on stiff ( $E = 10$  kPa) substrates showing that Y27632-mediated inhibition of cell contractility prevent SR protein phosphorylation compared with control (Ctrl). Actin was used as a loading control. (D) Representative image of frozen tissue sections stained for phosphorylated SR protein and CD31 showing that the BAPN treatment lowered SR protein phosphorylation compared with the mock treatment (Ctrl) (images were acquired with identical exposure settings). (Scale bars, 30 μm.)

EDB-FN after 20 h (Fig. 6 B and C). Notably, EDB-FN expression was decreased in wortmannin-treated samples. In agreement with the decreased level of EDB-FN observed at 20 h, both SR protein phosphorylation and AKT phosphorylation decreased after 1-h wortmannin treatment (Fig. 6 D–F and [Fig. S5\)](http://www.pnas.org/lookup/suppl/doi:10.1073/pnas.1505421112/-/DCSupplemental/pnas.201505421SI.pdf?targetid=nameddest=SF5). Together, these data indicate that EDB-FN splicing occurs

through the involvement of the PI3K/AKT pathway most likely downstream of cell contractility, thus further describing the mechanism by which microenvironmental mechanics regulates alternative splicing.

## Discussion

Here, we provide, to our knowledge, the first direct evidence that alternative splicing is regulated by ECM stiffness. Specifically, both in vitro and in vivo data indicate that the stiffness of the microenvironment regulates EDB-FN splicing. ECM stiffness mediates splicing by regulating SR protein phosphorylation and requires both cell contractility and activation of the PI3K/AKT pathway. Moreover, our in vivo data suggest that regulation of alternative splicing by ECM stiffness likely occurs in many cell types and may not be unique to only ECs or the EDB isoform of FN. As such, ECM stiffness may be a significant mediator of the production of the diverse array of protein isoforms present in a broad range of tissues and disease states.

FN is one of the most well-characterized ECM proteins. Alternative splicing of FN has been studied extensively, in part, because it is tightly linked to angiogenesis (9, 36–39). In ECs, the splicing events resulting in the inclusion of either the EDA or the EDB domains are correlated with tumor angiogenesis (36). It has been shown that both of these events can be regulated by SRp40 (11, 12). However, the physiological cues that mediate this splicing are largely unknown. Our data indicate that matrix stiffness can control SR protein phosphorylation, including that of SRp40, which regulates the splicing of numerous other proteins including proangiogenic molecules such as VEGF, notably by limiting the expression of the antiangiogenic VEGF 165b splice variant in favor of more proangiogenic forms (40–43). Moreover, the SR protein response to matrix stiffness is controlled by a signaling pathway that involves PI3K/ATK and requires cellular contractility. Indeed, inhibition of either cell contractility or PI3K prevented SR protein phosphorylation and inclusion of the EDB domain of fibronectin. Interestingly, AKT signaling has previously been implicated in SRp40-mediated splicing of the PKC family (14, 16), suggesting that AKT is likely to be involved in a similar way in both stiffness-mediated PKC and EDB-FN splicing. In addition,



Fig. 6. PI3K-AKT signaling is required for splicing of EDB-FN. (A) Representative image of frozen tissue sections stained for phosphorylated AKT substrates and VE-cadherin showing that the BAPN treatment influences PI3K/AKT signaling pathway activation. (Scale bar, 50 μm.) (B) Confocal images of EDB-FN and total FN on EC cells plated on 10-kPa substrates and kept in culture for 24 h with or without (Ctrl) wortmannin (Wort). (C) Western blot of whole protein extract from EC cells seeded on 10-kPa substrates showing that wortmannin (Wort)-mediated inhibition of PI3K decreases EDB-FN compared with control. Corresponding densitometric quantification showing both EDB-FN normalized against GAPDH content and the ratio of EDB-FN to total FN. (D) Representative image of ECs stained for phosphorylated SR proteins and AKT phosphorylation on Ser-473 showing that 1-h treatment with wortmannin prevents both SR protein and AKT phosphorylation. (Scale bar, 30 μm.) (E) Corresponding quantification of SR protein phosphorylation computed from at least 18 different fields of view from three independent experiments. (F) Western blot of whole protein extract from EC cells plated on stiff  $(E = 10$  kPa) substrates showing that wortmannin (Wort)-mediated inhibition of PI3K lowered SR protein phosphorylation compared to control (Ctrl). Actin was used as a loading control. Plots are mean  $\pm$  SE, Student t test: \*P < 0.05,  $*P < 0.01$ . Images were acquired with identical exposure settings.

the regulation of PI3K/AKT pathway by matrix stiffness is increasingly well documented in a number of different experimental tumor models (17–19, 44). Taken together, our data uncover a fundamental mechanism regulating EDB-FN expression in ECs. Indeed, considering the ubiquitous expression of EDB-FN in many aggressive solid tumors  $(7, 45-47)$  and the altered splicing patterns found in tumors (2, 4), the present findings are most likely representative of a general mechanism that extends beyond ECs and EDB-FN.

Interestingly, each of the hallmarks of cancer is associated with a switch in protein isoform expression patterns (2, 48). It has been suggested that tumor progression may be associated with coordinated control of splicing events (2, 31, 40). Efforts to uncover the regulators of the splicing machinery have identified several signaling pathways associated with growth factors and tumor progression (11, 49). Importantly, our results define a previously unidentified mechanism by which alternative splicing is regulated in cells through changes in the mechanical properties of the ECM. This regulatory mechanism could act through either direct activation of integrin signaling pathways or indirectly through the modulation of other pathways. In the case of direct activation, mechanical cues at ECM-cell adhesion sites can be converted directly into biochemical signals (50). Notably, there is compelling evidence implicating ECM stiffness in the regulation of PTEN and PI3K activation in epithelial cells (17). For the indirect case, we and others have shown that the interplay between the ECM stiffness and cell contractility can modulate growth factor-induced signaling pathways (27, 32, 51). Notably, both myosin light chain kinase and Rho-ROCK mediated contractility have been shown to be important in matrix stiffness regulation of growth factor signaling (51). Because our data link splicing and Rho/ROCK-mediated contractility and given that growth factors are known to regulate alternative splicing (16, 40), the interplay between ECM stiffness and growth factors could lead to a wide variety of splicing patterns.

Overall, matrix stiffness-mediated alternative splicing could potentially provide cells with a mechanism to adapt to mechanical stimulation. Changes in signaling proteins expression due to altered splicing patterns in response to altered ECM mechanical properties could result in changes in cell phenotype. For example, each of the PKC isoforms has been implicated in affecting actin dynamics and cell motility (52–55), suggesting that alternative splicing due to matrix stiffness could contribute to the known changes in cell motility that occur on compliant matrices compared with stiff matrices (24, 26). Stiffness-mediated down-regulation of the antiangiogenic isoform of VEGF, which would result in the alternative splicing of more proangiogenic isoforms (31), could play an important role in regulating angiogenesis. In addition, adipocyte differentiation has been shown to be independently driven by SRp40-mediated splicing (41) and tissue stiffness (56), hinting at a possible role of splicing in tissue stiffness induced differentiation. Therefore, our findings have important ramifications for the fundamental understanding of how changes in the mechanical microenvironment ultimately regulate cell-ECM interactions in normal physiological responses, such as tissue morphogenesis, and abnormal responses, like tumorigenesis.

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### Materials and Methods

Mouse Studies. All mice were maintained following a protocol approved by the Cornell University Institutional Animal Care and Use Committee. MMTV-PyMT transgenic and WT control mice, both on the FVB strain background, were obtained from the Jackson Laboratory. To alter tumor stiffness in vivo, mice were treated beginning at 4 wk of age with BAPN (3 mg/kg body weight; Sigma) in the drinking water ( $n = 12$  per group). After 8 wk of treatment, mice were euthanized by  $CO<sub>2</sub>$  asphyxiation and necropsied. Mammary tumors were collected and snap frozen in liquid nitrogen.

Mechanical Testing. The mechanical properties of mammary gland tumors from PyMT mice were assayed using unconfined compression on a Bose Enduratec 3200 (Bose) equipped with a 250  $\times$  g load cell with a load capacity of 5.11 N. Freshly isolated tumor samples were snap frozen and allowed to thaw only immediately before performing the mechanical testing (57, 58). The tissue sample was kept in PBS for 15 min to allow rehydration, after which a 3- or 4-mm cylindrical tissue section was excised using a biopsy punch (58). The tissue section height was measured and then subjected to a 3–15% strain in 3% increments (59). The elastic modulus was computed from the stress-strain relaxation curves using a poroviscoelastic model and a custom Matlab code (The Mathworks) (59, 60).

Cell Culture. Bovine aortic endothelial cells (BAECs) and human umbilical vein endothelial cells (HUVECs) were maintained and plated as described previously (61, 62). BAECs were maintained in medium supplemented with 10% (vol/vol) FetalClone III (Fisher), and 1% each of penicillin–streptomycin, MEM amino acids (Invitrogen), and MEM vitamins (Mediatech). HUVECs were maintained and plated at 37 °C and 5% (vol/vol)  $CO<sub>2</sub>$  in Medium 200 with 5% (vol/vol) FBS and 2% (vol/vol) low serum growth supplement (LSGS). For inhibitor studies, the cells were allowed to attach and spread for 2 h before adding the inhibitors at concentration of 10 μM for Y27632 or 2 μM for wortmannin. For the wortmannin treatment, an equivalent amount of DMSO vehicle was added to the controls.

Polyacrylamide Gel Synthesis and Stiffness Characterization. Polyacrylamide (PA) gels were prepared and characterized as described previously (61, 63, 64). The range of substrate stiffness used (0.2–10 kPa) was chosen to mimic the stiffness of vascular and tumor tissue as described previously (63, 65, 66).

Fibronectin Fiber Quantification. Evaluation of the fibronectin fiber lengths was performed using  $40\times$  confocal images as described previously (67). Briefly, 10 confocal images acquired in frozen sections from two different mice were analyzed using the Tubeness plugin in the ImageJ software. A threshold was applied to the resulting images, before fibronectin fragment length measurements.

Statistical Tests. Parametric one-way or two-way ANOVAs with post hoc Tukey's honest significance test were performed where appropriate.  $P < 0.05$ was considered statistically significant.

All reagents and a detailed description of additional protocols used in this study, including Western blotting, immunofluorescence of fixed samples, immunohistochemistry and immunofluorescence on tissue sections, quantitative real-Time PCR, and ROCK knockdown experiments are described in [SI Materials and Methods](http://www.pnas.org/lookup/suppl/doi:10.1073/pnas.1505421112/-/DCSupplemental/pnas.201505421SI.pdf?targetid=nameddest=STXT).

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