

# PDGFB-based stem cell gene therapy increases bone strength in the mouse

Wanqiu Chen<sup>a</sup>, David J. Baylink<sup>a</sup>, Justin Brier-Jones<sup>a</sup>, Amanda Neises<sup>a</sup>, Jason B. Kiroyan<sup>a</sup>, Charles H. Rundle<sup>a,b</sup>, Kin-Hing William Lau<sup>a,b</sup>, and Xiao-Bing Zhang<sup>a,1</sup>

<sup>a</sup>Department of Medicine, Loma Linda University, Loma Linda, CA 92354; and <sup>b</sup>Musculoskeletal Disease Center, Jerry L. Pettis Memorial VA Medical Center, Loma Linda, CA 92357

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Substantial advances have been made in the past two decades in the management of osteoporosis. However, none of the current medications can eliminate the risk of fracture and rejuvenate the skeleton. To this end, we recently reported that transplantation of hematopoietic stem/progenitor cells (HSCs) or Sca1<sup>+</sup> cells engineered to overexpress *FGF2* results in a significant increase in lamellar bone matrix formation at the endosteum; but this increase was attended by the development of secondary hyperparathyroidism and severe osteomalacia. Here we switch the therapeutic gene to *PDGFB*, another potent mitogen for mesenchymal stem cells (MSCs) but potentially safer than *FGF2*. We found that modest overexpression of *PDGFB* using a relatively weak phosphoglycerate kinase (PGK) promoter completely avoided osteomalacia and secondary hyperparathyroidism, and simultaneously increased trabecular bone formation and trabecular connectivity, and decreased cortical porosity. These effects led to a 45% increase in the bone strength. Transplantation of PGK-PDGFB-transduced Sca1<sup>+</sup> cells increased MSC proliferation, raising the possibility that PDGF-BB enhances expansion of MSC in the vicinity of the hematopoietic niche where the osteogenic milieu propels the differentiation of MSCs toward an osteogenic destination. Our therapy should have potential clinical applications for patients undergoing HSC transplantation, who are at high risk for osteoporosis and bone fractures after total body irradiation preconditioning. It could eventually have wider application once the therapy can be applied without the preconditioning.

PDGFB | hematopoietic stem cells | bone formation | gene therapy

Osteoporosis is a major public health problem in the United States and in the world. Currently, there are almost 10 million osteoporosis-related fractures annually worldwide (1). Over the past two decades, the treatment of osteoporosis has advanced dramatically, primarily because of the successful development of several effective antiresorptive therapies (2), which can reduce the fracture rate by as much as 50% (3). An anabolic therapy, namely parathyroid hormone (PTH), was subsequently developed and approved by the Food and Drug Administration. This therapy increases bone formation as opposed to antiresorptive drugs that reduce bone resorption, but the efficacy of this anabolic therapy in terms of fracture reduction has been the same as that of antiresorptive drugs (4). Multiple newer and more potent anabolic agents are currently being evaluated in clinical trials (5–7), but none of these entities appear to have the potential to rejuvenate the osteoporotic skeleton back to one with normal bone density and strength.

All of the aforementioned medications fall into the realm of pharmaceutical or biologic therapies. However, we have now entered the era of the third pillar of medicine: cell therapy (8). “Cells uniquely sense their surroundings, make decisions and exhibit varied and regulable behaviors,” such as targeting (8). In this regard, we have initiated the development of an anabolic cell therapy for the skeleton (9). Our past work has focused on establishing proof-of-principle for this approach in the mouse model, using genetically engineered hematopoietic stem/progenitor

(HSC) cell therapy, which could be given intravenously and would result in rejuvenation of the skeleton (9). We have shown engraftment of donor HSCs that were genetically engineered to overexpress *FGF2* at sites where bone is lost in osteoporosis (i.e., the HSC niches), which in turn resulted in substantial augmentation of bone matrix formation at these sites (9). Despite these advances, we encountered several issues that severely compromised the efficacy of our therapy. Instead of being stronger, the resulting bones were actually weaker and sometimes fractured during tissue processing. This was associated with severe hypocalcemia, secondary hyperparathyroidism, and osteomalacia developed in response to the therapy.

In the present study, we sought to resolve these adverse side effects. Two changes in our therapy were made compared with our previous work. First, we switched the therapeutic gene from *FGF2* to *PDGFB*, because PDGF-BB is normally secreted after platelet activation and circulates at concentrations that are some 100-times higher than *FGF2* (and thus could be safer). We use the term *PDGFB* to refer the gene that encodes the human platelet-derived growth factor (PDGF) B chain, and the term PDGF-BB to refer the homodimeric protein. PDGF-BB is a major growth factor found in bone matrix (10) and has also been shown to increase bone formation after intravenous administration (11). In addition, there have been considerable successful applications of PDGF-BB-based therapies on various types of maladies, including tendon, periodontal ligament, and bone fracture repairs (12, 13). The safety of PDGF-BB has been demonstrated in several clinical trials (14, 15), and it has been approved by the Food and Drug Administration for treatment of patients with oral and maxillofacial bony defects (15). Second, we used various promoters of different strengths to express *PDGFB* to identify the optimal PDGF-BB dosage. In the present

## Significance

Osteoporosis is a morbid disease afflicting millions of people worldwide. To unlock the unique regenerative powers of the skeleton that have not yet been exploited, we used stem cell gene therapy to dramatically increase bone formation at sites where bone is lost during osteoporosis. Our therapy tremendously increased de novo trabecular bone formation and trabecular connections, resulting in a large increase in bone strength. Our therapy has clinical potential, may serve as a prototype for future skeletal stem cell gene therapies, and is a model for mechanistic studies of de novo trabecular bone formation.

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Conflict of interest statement: A provisional patent application has been filed on the basis of some of the findings. D.J.B., K.-H.W.L., X.-B.Z., and W.C. are the inventors.

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<sup>1</sup>To whom correspondence should be addressed. Email: xzhang@llu.edu.

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study, we showed that when a relatively weak physiologic promoter (i.e., phosphoglycerate kinase or PGK promoter) was used, the therapy yielded marked increases in endosteal/trabecular bone formation without significant elevation in the circulating level of PDGF-BB. It also avoided adverse effects, such as osteomalacia, and led to a 45% increase in bone strength (maximal load to failure). In this respect, no traditional monotherapy for osteoporosis has shown long-term beneficial effect on the bone strength of the treated bone (16). Moreover, our therapy uniquely produced a 20-fold increase in trabecular connectivity and substantial reduction in cortical porosity, both of which are relevant to the bone mechanical performance.

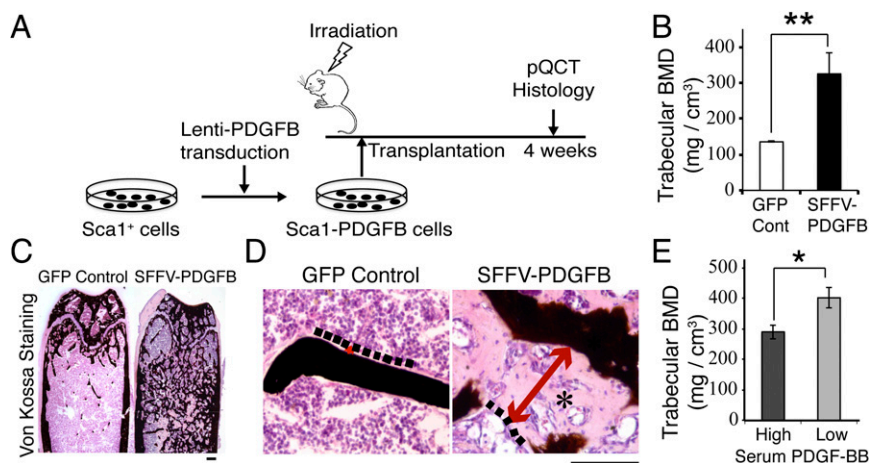
## Results

**Transplantation with Lenti-SFFV-PDGFB-Transduced Sca1<sup>+</sup> Cells Leads to Massive Endosteal/Trabecular Bone Formation but also Induces Osteomalacia.** Our cell-based therapy consists of isolation of HSCs from a donor mouse, genetically engineering these cells to overexpress *PDGFB*, and transplantation of these modified HSCs into a syngeneic recipient mouse after irradiation (Fig. 1A) (9). HSCs are used as a vehicle because these cells specifically target to the HSC niche at the endosteal bone surface and the HSC niches at the marrow vascular surfaces: the two major sites of bone loss in humans with osteoporosis. We first used a strong promoter, spleen focus-forming virus (SFFV), to overexpress *PDGFB*. Four weeks following transplantation with Lenti-SFFV-PDGFB-transduced Sca1<sup>+</sup> cells, the femoral bone mineral density (BMD) was significantly greater than that of control mice (325 mg/cm<sup>3</sup> vs. 135 mg/cm<sup>3</sup>,  $P < 0.01$ ) (Fig. 1B). However, the von Kossa staining, which stains mineralized bone (17), reveals that the newly formed bone was largely unmineralized (Fig. 1C and D). When we stratified the PDGFB-treated mice into the low-serum PDGF-BB (<1,000 pg/mL) and the high-serum PDGF-BB (>1,000 pg/mL) subgroups, the BMD of the low-serum PDGF-BB group was significantly higher than that of the high-serum PDGF-BB group (402 vs. 290 mg/cm<sup>3</sup>,  $P < 0.05$ ) (Fig. 1E). These data indicate that the PDGFB-based HSC cell therapy promotes de novo trabecular bone formation in the mouse, but high levels of PDGF-BB have unintended negative effects on BMD.

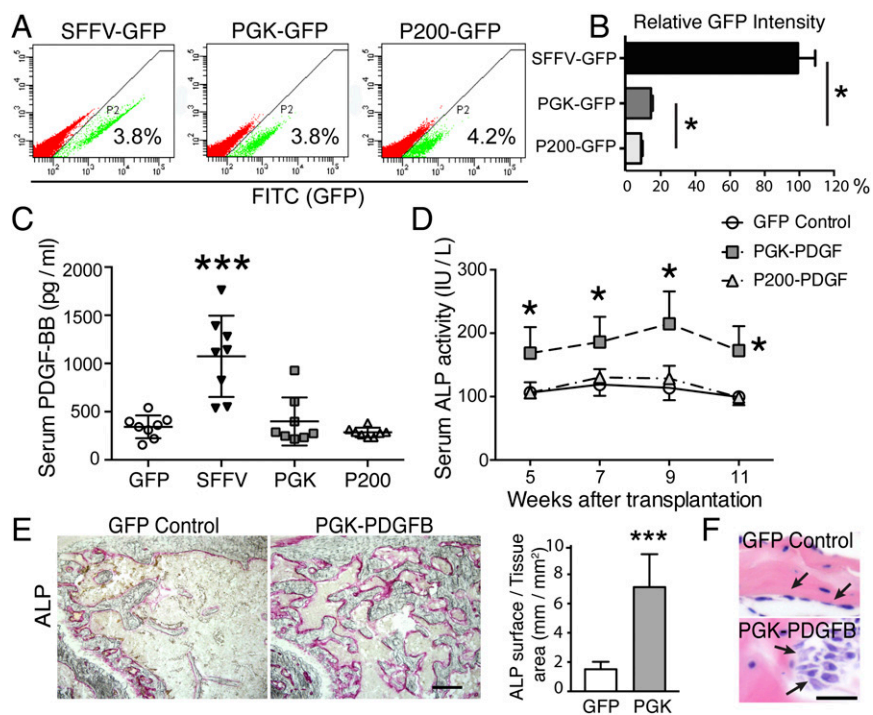
**Optimal PDGFB Expression Driven by a Weaker Promoter Promotes Endosteal/Trabecular Bone Formation Without Osteomalacia or Secondary Hyperparathyroidism.** Because mice with low-level serum PDGF-BB showed higher BMD, we decided to reduce PDGFB expression by using two weaker promoters: that is, the PGK promoter (~500 bp in length) and the truncated PGK promoter, P200 (~200 bp in length) (Fig. S1). The P200 truncated promoter is less potent compared with the original PGK promoter. To assess relative potency of these different promoters in Sca1<sup>+</sup> cells, we used GFP as the reporter gene. Sca1<sup>+</sup> cells were transduced with the Lenti SFFV-GFP, PGK-GFP, or P200-GFP, each at the same low multiplicity of infection (MOI) of 0.1. A low MOI was used because it would allow a better comparison of the transduction efficiency among strong and weak promoters. As shown in Fig. 2A, the transduction efficiency for the three test vectors in Sca1<sup>+</sup> cells was very similar (i.e., ~4% in each transduced cell population). As expected, the level of GFP expression driven by the PGK promoter was ~85% lower than that driven by the SFFV promoter (15% vs. 100%), and the GFP expression level controlled by the P200 promoter was ~50% lower than PGK promoter (9% vs. 15%) (Fig. 2B).

To investigate the dosage effects of PDGF-BB on bone formation, we transduced Sca1<sup>+</sup> cells with Lenti SFFV-PDGFB, PGK-PDGFB, P200-PDGFB, or GFP control (each at an MOI of 2). Each transduced cell population ( $1 \times 10^6$  cells) was then transplanted into recipient mice after preconditioning with 6 Gy irradiation ( $n = 8$  per group). At 5 wk posttransplantation, the serum PDGF-BB levels of the SFFV-PDGFB mice were two- to threefold higher than those of the GFP control mice ( $1,074 \pm 422$  vs.  $342 \pm 118$  pg/mL,  $P < 0.001$ ) (Fig. 2C). Conversely, there was no significant difference in the serum PDGF-BB level among the PGK-PDGFB group ( $398 \pm 248$  pg/mL), the P200-PDGFB group ( $285 \pm 49$  pg/mL), and the GFP control group ( $342 \pm 118$  pg/mL,  $P > 0.05$ ).

Because the SFFV-PDGFB-treated mice showed severe osteomalacia, we focused on mice treated with the two PGK promoters. To monitor the dynamics of bone formation, we measured serum alkaline phosphatase (ALP) activity [a bone formation bio-marker (18)] at 5, 7, 9, and 11 wk posttransplantation (Fig. 2D). The serum ALP activity in the PGK-PDGFB group was 50% higher than that in the GFP control



**Fig. 1.** Transplantation with Lenti-SFFV-PDGFB-transduced Sca1<sup>+</sup> cells leads to massive endosteal/trabecular bone formation but also induces osteomalacia. (A) Schematic representation of the experimental design. (B) Femoral trabecular BMD (determined by pQCT) at 4 wk after transplantation.  $**P < 0.01$ . Control group:  $n = 8$ ; SFFV-PDGFB group:  $n = 13$ . (C) Von Kossa staining of frozen sections of femur from SFFV-PDGFB-treated or control mice. Black color: mineralized bone. (Scale bar, 200  $\mu$ m.) (D) High-magnification images of Von Kossa staining. Osteomalacia-like phenotype was seen in SFFV-PDGFB-treated mice (indicated by an asterisk). Dash lines indicate the edge of osteoid. Red arrows indicate the osteoid width. (Scale bar, 100  $\mu$ m.) (E) pQCT data from SFFV-PDGFB-treated animals was stratified into the low-serum PDGF-BB group (200–600 pg/mL,  $n = 4$ ) and the high-serum PDGF-BB group (1,000–3,000 pg/mL,  $n = 9$ ).  $*P < 0.05$ .



**Fig. 2.** Optimal *PDGFB* transgene expression with the PGK promoter increases serum ALP levels. (A) FACS analysis of the transduction efficiency of *Sca1*<sup>+</sup> cells with Lenti SFFV-GFP, PGK-GFP, or P200-GFP, each at the MOI of 0.1. (B) Quantitative analysis of GFP intensity. \**P* < 0.05. (C) Serum PDGF-BB levels in each test group of animals at 5 wk posttransplantation. \*\*\**P* < 0.001. *n* = 8 per group. (D) Serum ALP activity in recipient mice after transplantation of Lenti-GFP<sup>-</sup>, Lenti-PGK-PDGFB<sup>-</sup>, or Lenti-P200-PDGFB<sup>-</sup> transduced *Sca1*<sup>+</sup> cells. \**P* < 0.05. *n* = 8 per group. (E, Left) Cytochemical staining of ALP activity on femur frozen sections. (Scale bar, 200  $\mu$ m.) (Right) Quantification of ALP surface showed a significant increase in the bone section of PGK-PDGFB-treated mice compared with GFP control animals. \*\*\**P* < 0.001. (F) Representative images of H&E staining showed more activated osteoblasts (arrows in PGK-PDGFB group) than in control group. (Scale bar, 25  $\mu$ m.)

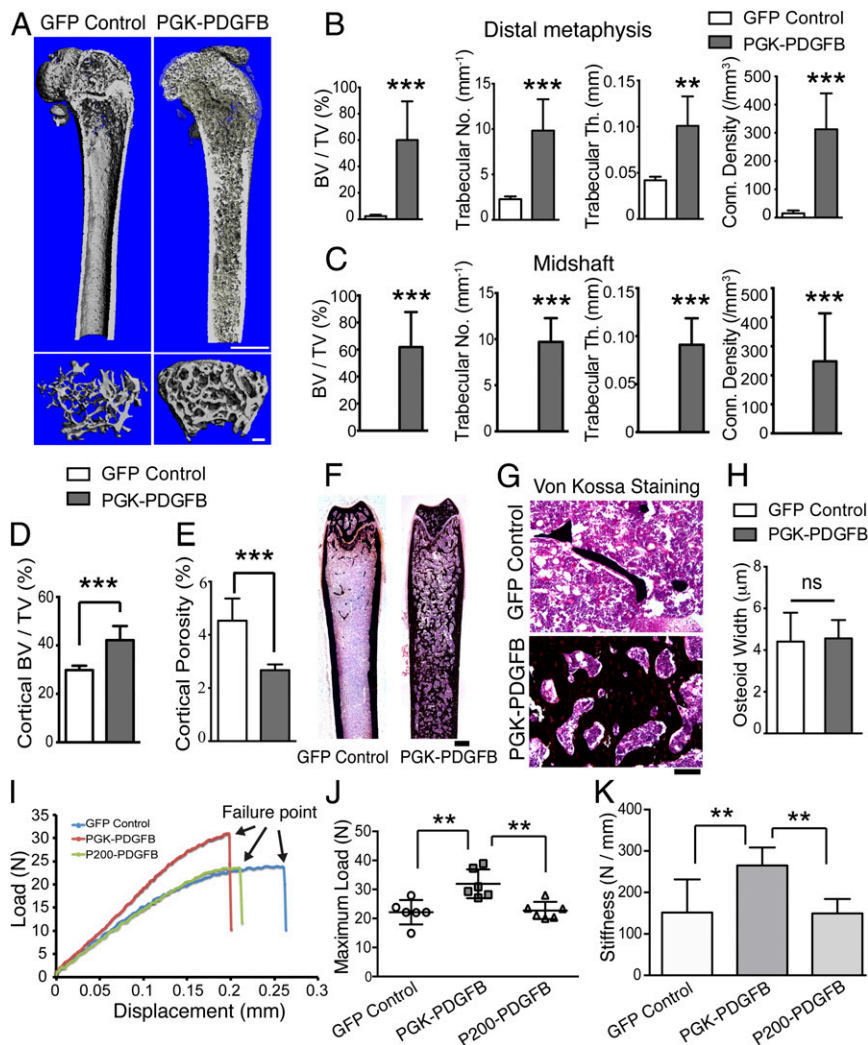
animals from 5 to 11 wk posttransplantation. Cytochemical staining for ALP activity in femur sections indicated that the surface of ALP-expressing osteoblast cells along the endosteal bone surface in PGK-PDGFB-treated mice was increased by ~fivefold compared with that of the control mice ( $7.1 \pm 2.3$  vs.  $1.5 \pm 0.5$  mm<sup>2</sup>/mm<sup>2</sup>) (Fig. 2E). H&E staining showed that bone-lining cells were spindle-shaped in the control group, whereas osteoblasts in the PGK-PDGFB group were of cuboidal shape (Fig. 2F) with increased cell size (Fig. S2A), suggesting that osteoblasts in PGK-PDGFB-treated bone are highly activated. In contrast, P200-PDGFB cells transplanted femur did not show any increases in ALP activity in serum (Fig. 2D). Consistent with increased bone formation in PGK-PDGFB-treated mice, the serum levels of osteocalcin, another bone formation biomarker, in PGK-PDGFB-treated mice was ~150% higher than that in control animals ( $12.1 \pm 6.1$  vs.  $5.4 \pm 1.2$  ng/mL; *P* < 0.01) (Fig. S2B).

To examine the architectural structure of the newly formed bony tissue, we performed microcomputed tomography ( $\mu$ CT) analysis on femurs of the Lenti-PGK-PDGFB-treated and control mice. After the PGK-PDGFB treatment, the marrow cavity at the sites of metaphysis and midshaft was packed with thick and well-connected trabeculae. In contrast, there were substantially fewer trabeculae in the metaphysis and virtually no trabeculae in the midshaft of the femur of Lenti-GFP-treated control mice (Fig. 3A). The relative trabecular bone volume (Tb.BV/TV), trabecular thickness (Tb.Th), trabecular number (Tb.N), and connectivity density (ConnD) were substantially increased in PGK-PDGFB-treated bones compared with control bones (*P* < 0.001 for each) (Fig. 3B and C). De novo bone formation was seen only on the endosteal surface but not on the periosteal surface. The cortical bone volume (Ct.BV/TV) was also increased

by 20–30% (Fig. 3D). Of note, the cortical porosity of PGK-PDGFB-treated bones was significantly reduced by 40% compared with control bones ( $4.5\% \pm 0.8$  vs.  $2.7\% \pm 0.2$ ; *P* = 0.0003) (Fig. 3E).

To investigate whether the large increase in de novo bone formation in PGK-PDGFB-treated animals would also cause incomplete mineralization of the newly formed bone (i.e., osteomalacia), we conducted Von Kossa staining on longitudinal thin bone sections. The newly formed bone in PGK-PDGFB-treated animals was mostly mineralized with similar osteoid width (O.Wi) compared with control animals (Fig. 3F–H), indicating that the PGK-PDGFB therapy does not impair mineralization of the newly formed bone matrix. Moreover, serum levels of calcium, phosphate, PTH, and FGF23 in PGK-PDGFB-treated animals were also not significantly different from those of control animals (Fig. S3), suggesting the PGK-PDGFB treatment does not perturb serum Ca<sup>2+</sup>/Pi/PTH homeostasis in recipient mice. Taken together, these data suggest that the HSC-based PGK-PDGFB treatment does not cause hypocalcemia or secondary hyperparathyroidism, which may have attributed to the absence of impaired mineralization of the newly formed bone. The bone formation response to PDGF-BB was dose-dependent, as reduction in *PDGFB* expression by 50% with the use of the P200 promoter did not yield significant de novo bone formation. These data strongly suggest that maintaining an appropriate PDGF-BB dose is critically important for an optimal bone formation response that would simultaneously avoid the adverse effect of osteomalacia.

**PGK-PDGFB Treatment Increases Bone Strength.** The mechanical strength of the bone is the ultimate predictor of fracture risks (19). To investigate whether the increase in bone formation



**Fig. 3.** PGK-PDGFB treatment promotes de novo bone formation and enhances bone strength without causing osteomalacia. (A) The  $\mu$ CT 3D reconstruction images of a representative femur from the GFP control mice and the PGK-PDGFB-treated mice at 12 wk posttransplantation. (Upper) The bisected longitudinal image of the femur that shows trabecular structure within the marrow cavity. (Scale bar, 1 mm) (Lower) The cross-sectional area at secondary spongiosa of distal metaphysis of the femur. (Scale bar, 200  $\mu$ m.) (B and C) Summary of the trabecular bone parameters at the distal metaphysis (B) and midshaft (C) of femurs of the PGK-PDGFB group and the GFP control group.  $n = 6$  for each group.  $*P < 0.05$ .  $n = 6$  per group. (D and E) Cortical bone volume (D) and cortical porosity (E) were determined at the midshaft of the PGK-PDGFB group and GFP control group.  $***P < 0.001$ . (F and G) Von Kossa staining of femurs. Increased de novo bone formation in the marrow space in the Lenti-PGK-PDGFB group was observed. (Scale bars, 500  $\mu$ m in F and 100  $\mu$ m in G.) (H) Quantification of osteoid width (O.Wi). ns, not significant. (I) A representative loading force displacement curve of each test group. (J and K) Maximum load-to-failure (J) and stiffness (K) was significantly increased in the PGK-PDGFB-treated femurs compared with control or P200-PDGFB-treated bones.  $n = 6$  per group.  $**P < 0.01$ .

following the PGK-PDGFB treatment can be translated into an increase in bone strength, we subjected the Lenti-PGK-PDGFB-treated and the Lenti-GFP-treated control femur to three-point bending mechanical testing. Fig. 3I shows the loading force-displacement curves of a representative femur from each test group. The PGK-PDGFB treatment caused a 45% increase in maximum load-to-failure in the midshaft of the femurs ( $32.0 \pm 5.0$  vs.  $22.1 \pm 4.2$  N,  $P = 0.001$ ) and a 46% increase in its stiffness (the slope of the force displacement curve) ( $265.1 \pm 43.5$  vs.  $181.7 \pm 33.5$  N/mm,  $P = 0.0037$ ) (Fig. 3J and K). Femurs of the P200-PDGFB-treated group showed very similar maximal load-to-failure force ( $22.7 \pm 3.0$  vs.  $22.1 \pm 4.2$  N,  $P = 0.56$ ) and stiffness as those of femurs of the GFP control mice. Moreover, the maximum load-to-failure force correlated positively with both cortical bone mass (Ct.BV/TV) and trabecular bone mass (Tb.BV/TV) at the midshaft ( $R^2 = 0.75$ ,  $P = 0.0005$  for each) (Fig. S4). These data

indicate that the newly formed bone is mechanically functional and of high quality.

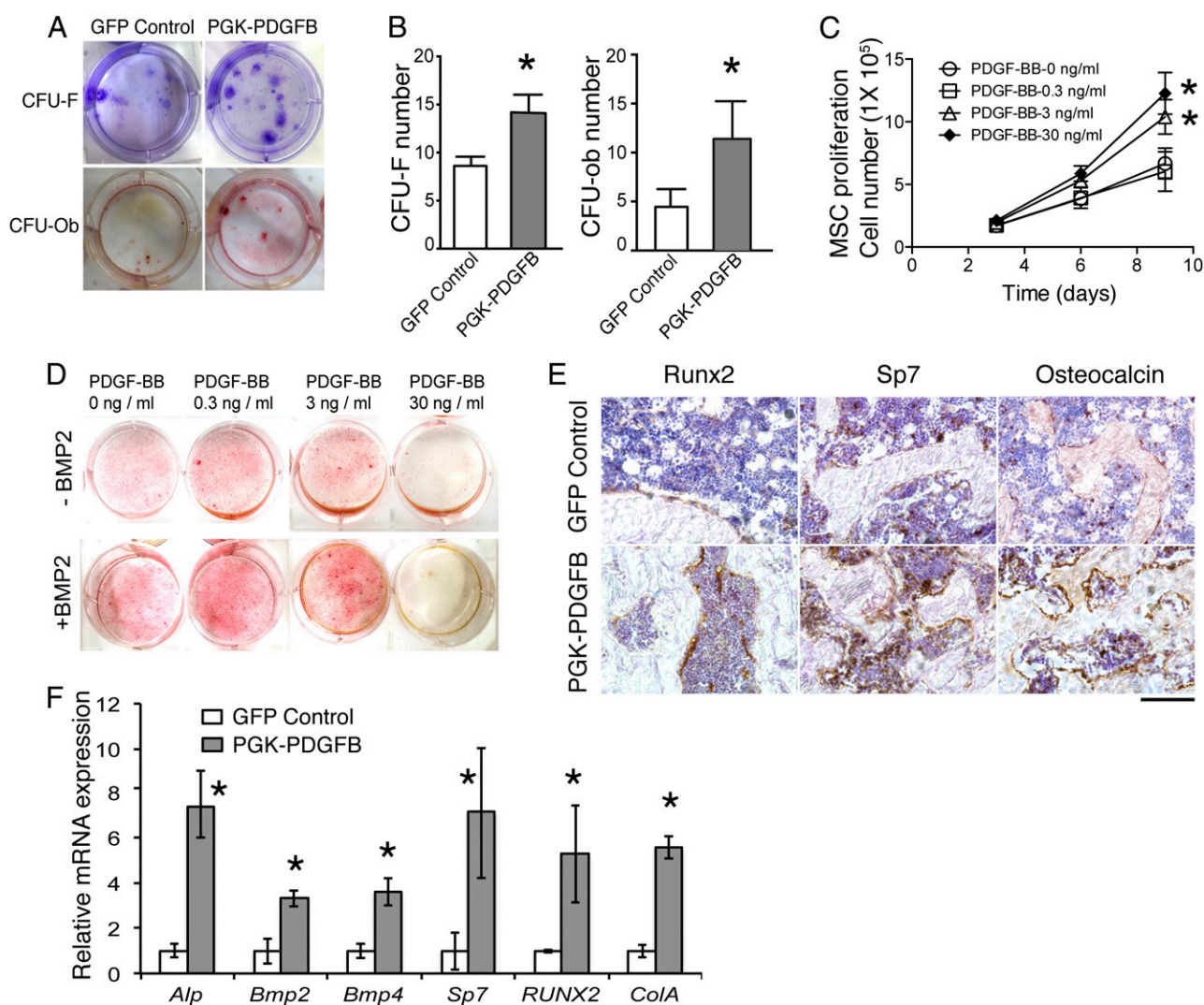
**PDGFB Treatment Promotes Proliferation of Mesenchymal Stem Cells and Angiogenesis.** Previously, we have tested several different bone growth factors in our HSC-based gene therapy regimen (9, 20, 21); only FGF2 and PDGFB are effective in increasing bone formation. There are several possible mechanisms for the effectiveness of these two growth factors, such as: (i) HSC proliferation and thereby providing a competitive proliferative advantage over the host cells, (ii) bone marrow mesenchymal stem cell (MSC) proliferation, and (iii) angiogenesis that is essential for bone formation (22, 23). To examine the effects of PDGF-BB on HSC proliferation, we cultured Sca1<sup>+</sup> cells transduced with Lenti-PDGFB or Lenti-GFP and observed no significant difference in cell proliferation rate between the two groups after 6 d in vitro culture (Fig. S5), ruling out this possibility.

To investigate the effects of PDGF-BB on MSC proliferation and their osteoblastic potential, we quantified MSCs and osteoblasts in the bone marrow of recipient mice at 12 wk posttransplantation using the CFU-fibroblast (F) and CFU-osteoblast (Ob) assay, respectively. There was an ~50% and 100% increase in the CFU-F and CFU-Ob number in the marrow cells from the PGK-PDGFB-treated mice compared with the control mice (Fig. 4*A* and *B*). We next measured the effects of PDGF-BB on proliferation of marrow-derived MSC *in vitro*. Bone marrow cells were cultured in MSC medium supplemented with PDGF-BB at various concentrations (0, 0.3, 3, or 30 ng/mL). Both 3 and 30 ng/mL PDGF-BB significantly increased MSC proliferation (Fig. 4*C*), suggesting that PDGF-BB can promote MSC expansion.

We further evaluated the effects of PDGF-BB on angiogenesis by assessing relative vascularization in marrow cavity. Immunohistochemical staining of the endothelial marker, vWF, showed significantly more small vessels in the marrow cavity of

PGK-PDGFB-treated mice compared with control mice (Fig. S6). These findings together suggest that increases in MSC proliferation and angiogenesis are two tenable mechanisms that might explain the effectiveness of PDGF-BB in our therapeutic regimen. However, further work is required to determine if other factors might also be contributory.

**Optimal Doses of PDGF-BB Enhance Osteoblast Differentiation.** We next investigated the effects of PDGF-BB on osteoblastic differentiation with the *in vitro* bone nodule formation assay. In the absence of bone morphogenetic protein 2 (BMP2), no significant difference was seen in the number of mineralized nodules in either the 0.3 or the 3 ng/mL PDGF-BB group compared with control group, whereas nodules in the 30 ng/mL PDGF-BB groups did not mineralize. However, when BMP2 was added, substantial increases in the number of mineralized nodules were seen in cells treated with 0.3 ng/mL or 3 ng/mL PDGF-BB

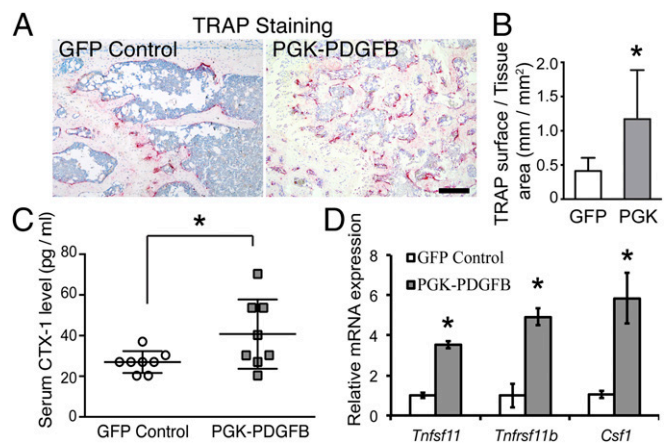


**Fig. 4.** The PDGF-BB therapy promotes bone formation by increasing numbers of MSC, preosteoblasts and osteoblasts, as well as enhancing osteogenesis-related gene expression. (A) Representative images of CFU-F colonies stained with Crystal violet (Upper) and CFU-Ob colonies stained with Alizarin red (Lower). CFU-F and CFU-Ob assays were conducted with bone marrow cells harvested from GFP control or PGK-PDGFB-treated mice. (B) Quantification of the CFU-F and CFU-Ob numbers. GFP control vs. PGK-PDGFB,  $*P < 0.05$ . (C) MSC proliferation curve. GFP control vs. PDGF-BB (3 or 30 ng/mL),  $*P < 0.05$ . (D) Alizarin red staining for osteoblastic differentiation of MSCs. Bone nodule formation was enhanced by PDGF-BB protein at 0.3 ng/mL and 3 ng/mL when BMP2 was added, but reduced by PDGF-BB at 30 ng/mL. Red stained are bone nodules after 3 wk of culture in osteogenic medium. (E) Immunohistochemical staining for Runx2, Sp7, and osteocalcin on thin sections of mouse femurs. (Scale bar, 100  $\mu$ m.) (F) Real-time qPCR analysis of osteogenesis-related genes in the tibias. GFP control vs. PGK-PDGFB,  $*P < 0.05$ .

compared with the control group (Fig. 4D). PDGF-BB at 30 ng/mL remained to be inhibitory even in the presence of BMP2. These data suggest that PDGF-BB at optimal doses synergizes with BMP2 to enhance osteoblast differentiation. These in vitro findings are consistent with in vivo observation that optimal doses of local marrow concentration of PDGF-BB in Lenti-PGK-PDGFB-treated mice strongly induce bone formation, whereas high-level local PDGF-BB in Lenti-SFFV-PDGFB-treated mice induce osteomalacia by compromising osteoblastic differentiation of MSCs.

To further evaluate the effect of the PGK-PDGFB treatment on osteogenesis in vivo, we performed immunostaining for Runx2 and Sp7 (two transcription factors expressed by preosteoblasts), as well as osteocalcin (a marker for mature osteoblasts). As expected, expression levels of Runx2 and Sp7 as well as osteocalcin were considerably increased in PGK-PDGFB-treated femurs compared with control femurs (Fig. 4E). Expression of ALP mRNA and type I $\alpha$  collagen (*Coll1a1*) mRNA was increased sevenfold and fivefold, respectively, in the PGK-PDGFB-treated femurs (Fig. 4F), strongly supporting that the PGK-PDGFB therapy enhances osteogenesis in vivo. Next, we measured the expression levels of two mediators of osteoblastic differentiation, *Bmp2* and *Bmp4*. Both were significantly increased in the PGK-PDGFB-treated mice (Fig. 4F). To investigate whether PDGF-BB directly stimulates *Bmp2* and *Bmp4*, we treated MSCs and MC-3T3E1 cells, an osteoblast progenitor cell line, with or without PDGF-BB. Quantitative RT-PCR (RT-qPCR) analysis showed that PDGF-BB did not increase expression of *Bmp2* or *Bmp4* in either MSCs or MC-3T3E1 cells (Figs. S7 and S8). To assess the effects of PGK-PDGFB treatment on osteoblast proliferation and the Bmp-mediated osteoblast differentiation in vivo, we stained *K<sub>f</sub>-67* (a proliferation marker) and pSmad1/5 (a major downstream mediator of Bmp2 signaling) in femur sections. There was a marked increase in *K<sub>f</sub>-67*<sup>+</sup> cell number in the marrow space of femur of the PGK-PDGFB group compared with the control group. Similarly, there were also substantially more pSmad1/5-expressing cells in PGK-PDGFB group compared with control group (Fig. S9), suggesting that activation of the BMP signaling was involved in the osteogenic response following the PGK-PDGFB treatment. Taken together, these data demonstrate that an optimal dose of PDGF-BB enhances osteoblastogenesis both in vitro and in vivo.

**PDGFB Treatment Increases Bone Remodeling.** Finally, we asked whether osteoclastogenesis was also affected by the PGK-PDGFB treatment. We measured the activity of tartrate-resistant acid phosphatase (TRAP), a marker of osteoclasts. The bone surface of the PGK-PDGFB-treated femur was occupied by significantly more osteoclasts, as indicated by the ~threefold increase in TRAP<sup>+</sup> surface, compared with the control ( $1.2 \pm 0.7$  vs.  $0.4 \pm 0.2$  mm<sup>2</sup>/mm<sup>2</sup>,  $P = 0.031$ ) (Fig. 5A and B). These observations, along with the finding that PGK-PDGFB treatment leads to heightened osteoblast activities at bony surfaces, indicate that the PGK-PDGFB-treated animals have an increased bone remodeling. Consistent with an increased bone turnover, serum C-telopeptide of type I collagen (CTX-1), a biochemical marker of bone resorption (24), was increased by 30–40% in PGK-PDGFB mice compared with control mice ( $P < 0.05$ ) (Fig. 5C). The expression of several osteoclastogenesis-related genes in the tibias of PGK-PDGFB-treated mice at 12 wk posttransplantation was also significantly increased (Fig. 5D). Specifically, *Tnfrsf11* (which encodes Rankl) and *Csf1* (which encodes M-CSF) was up-regulated by ~threefold and sixfold, respectively. These results suggest that PGK-PDGFB treatment also promotes bone remodeling. Intriguingly, expression of *Tnfrsf11b* (which encodes osteoprotegerin, a decoy receptor for Rankl) was also increased in PGK-PDGFB-treated tibia. Although the Rankl to Opg ratio is often



**Fig. 5.** PGK-PDGFB treatment increases bone turnover. (A) Histocytochemical staining for TRAP at the secondary spongiosa of distal femur of a representative GFP control or a representative PGK-PDGFB-treated mouse. Osteoclasts are stained red. (Scale bar, 200  $\mu$ m.) (B) Quantification of TRAP<sup>+</sup> bone surface showed a significant increase in the bone section of PGK-PDGFB-treated mice compared with GFP control animals.  $*P < 0.05$ . (C) Serum CTX-1 levels at 9 wk after transplantation. PGK-PDGFB-treated mice showed significant increase in serum CTX-1 level ( $*P < 0.05$ ).  $n = 8$  per group. (D) Real-time qPCR analysis of osteoclastogenesis-related genes in the tibias. GFP control vs. PGK-PDGFB,  $*P < 0.05$ .

viewed as an indicator of bone resorption, this assumption may be an oversimplification of the role of Rankl itself.

## Discussion

Here we show that transplantation of mouse HSCs that were engineered to overexpress PDGF-BB driven by the PGK promoter results in a rapid, robust, and persistent formation of mineralized trabecular bone on the endosteum, leading to a 45% increase in the bone strength as measured by three-point bending. Importantly, net bone formation was seen at all of the critical sites where bone is lost during osteoporosis and aging in humans: at the endosteum of cortical surfaces, intracortical canals, and in the trabecular compartment. One of the most remarkable findings with respect to the sites of bone formation was a 20-fold increase in trabecular connections and a 50% decrease in cortical porosity, both of which have mechanical performance implications. In relation to this, we also found evidence for de novo bone formation in the marrow cavity: trabecular bone was found in situ where no trabeculae existed in the control animals. Accordingly, our strategy has the potential to completely replace all bone lost in the osteoporotic process, in a sense of a complete rejuvenation of the skeleton.

One of the most important aspects of our therapy is targeting. We used HSCs because sites of bone loss correspond to hematopoietic niches. Accordingly, transplanted HSCs are able to home to the bone marrow cavity and specifically engraft at the endosteal niches (25), where aging-induced bone loss occurs.

One of the potential problems currently in developing anabolic therapies is a resistance to therapy after a year or so of treatment (26). We did not address this issue directly, but we did not see any decrease in ALP levels that were increased after PGK-PDGFB treatment over the 3-mo experimental period. Moreover, in the context of our experimental animal (normal bone mass), bone formation was occurring robustly despite the fact that the additional bone was not mechanically required. This raises the possibility that our therapy has the potential to cause large increment in skeletal mass in diseased skeleton.

The most critical issue in osteoporosis therapy is bone strength and resistance to fractures. We tested only the bone strength with the three-point bending test. In the future, it would be

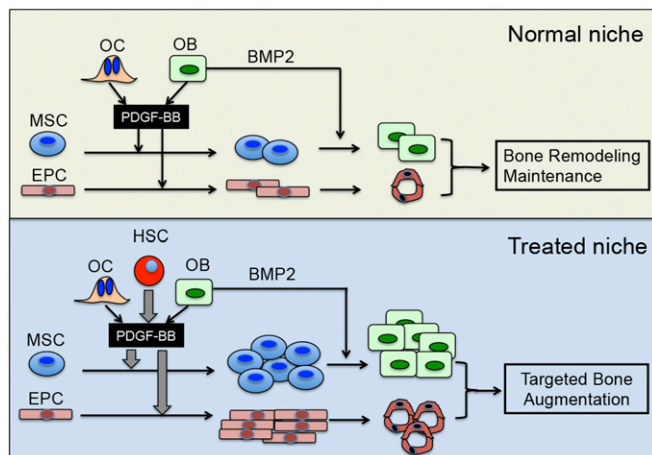
important to do torsional testing as well as finite element analysis to determine trabecular orientations and whether we have achieved optimal distribution of bone mass for the optimal mechanical performance. Our animals were studied under normal conditions of loading. It will be necessary in the future to determine if additional loading at certain sites would result in a complementary increase in de novo trabecular bone formation at such sites. If so, this stem cell gene therapy could be used in combination with a specific exercise program to enhance the trabecular compartment at mechanically appropriate sites.

In the past, we have used several different growth factors in our HSC-based transplantation strategy (9, 20, 21). BMP4, the first growth factor that we tested, showed no positive effects on bone formation (20). The growth factor that did show a positive response was FGF2, which is a strong mitogen to increase MSC proliferation (27). One of the reasons for studying PDGF-BB was that, similar to FGF2, PDGF-BB also dramatically increases MSC proliferation (28). In aggregate, the studies raise the possibility that to have substantial osteogenic activity, the transplanted cells need to be able to promote MSC proliferation. Accordingly, our findings that the PGK-PDGFB treatment yielded a marked increase in  $K_{i-67}^{+}$  cells in the marrow space (Fig. S9) and ~fivefold increase in the ALP-stained bone surface (Fig. 2E) in PGK-PDGFB-treated animals compared with the control group are entirely consistent with an increase in mitogenic activity of mesenchymal bone progenitor cells as a consequence of PDGF-BB in our study. We have proposed a mechanism of action for our therapeutic regimen, which is shown in Fig. 6. Following transplantation, PDGF-BB-overexpressing  $Sca1^{+}$  cells home in on the HSC niches at the endocortical surfaces and at the trabecular surfaces. PDGF-BB released from  $Sca1^{+}$  cells stimulates MSC proliferation and recruits MSCs to the niches. It also promotes angiogenesis (29). PGK-PDGFB treatment was associated with an increase of *Bmp2* and *Bmp4* production (Fig. 4F), which,

however, was probably caused by an increased number of mature osteoblasts rather than an increased *Bmp* production per cell (Figs. S7 and S8). On the other hand, the increased osteoblast size and higher levels of pSmad1/5 in the PGK-PDGFB-treated femurs, along with the findings that PDGF-BB-induced nodule formation was increased in the presence of BMP2, raises the strong possibility that there is a cross-talk between the PDGF-BB and BMP2 signaling pathways in our study. However, the exact nature of the interaction between the two signaling pathways will require additional investigation. Nevertheless, the fact that the bone formation-inducing effects of PDGF-BB require the presence of BMPs may raise the interesting possibility that BMP signaling is involved in our PDGF-BB-based stem cell gene therapy, which also would explain why PDGF-BB increases bone formation in bone but not in other tissues. Accordingly, we interpret that the osteogenic milieu facilitates MSCs differentiation toward osteogenic cells around the HSC niches, resulting targeted bone augmentation where bone loss occurs.

Previous studies have shown that PDGF receptor  $\beta$  is detected on osteoclasts (30). In addition to enhancing bone formation, PDGF-BB directly stimulates bone resorption (31). Our findings of increased expression of *Csf1* and *Tnfsf11*, an increased number of TRAP<sup>+</sup> osteoclasts at the bone surface, and elevated serum CTX-1 levels in PGK-PDGFB-treated mice are entirely consistent with a PDGF-BB-induced increase in bone resorption. Accordingly, inasmuch as the serum PTH was normal in the PGK-PDGFB-treated group, we interpret this finding to be consistent with previous reports on the innate ability of PDGF-BB to stimulate bone resorption (11). Such an increase in bone resorption is indicative of an increase in bone remodeling, which could increase bone quality and improve the mechanical performance of bone. Although we favor that the increased osteoclastogenesis is the direct effect by PDGF-BB, there is no data to rule out the possibility that PDGF-BB-induced osteoclastogenesis is coupled through osteoblastogenesis. Future experiments are needed to determine the mechanism of PDGF-BB-induced osteoclastogenesis in our system.

This study has several limitations: First, our experimental animal model was the C57BL/6 mouse with a normal skeleton. Future work is needed to determine if similar results can be achieved in osteoporotic models. In this regard, it is worth noting that anabolic therapy is effective in ovariectomized mice and osteogenic therapy is effective in aged humans (26). Second, we used promoters of different strengths to obtain an appropriate dose of PDGF-BB, which is far too rigid for appropriate dosage control. Future studies will need to evaluate transcriptional regulation of PDGF-BB doses. Of note, except for the spleen weight, we did not observe any difference in the weight of major organs and in the body weight between the control and the PGK-PDGFB-treated mice (Fig. S10), suggesting that our therapy does not appear to have serious detrimental effect on other major organs. The reason for the enlarged spleen in the PGK-PDGFB-treated mice was probably the result of an increase in extramedullary hematopoiesis in the spleen, because a substantial amount of the marrow cavity was now occupied by newly formed bone tissue. This is not expected to be an inherent adverse effect because in the future it should be possible to adjust the dose of PDGF-BB to regenerate the skeleton without compromising marrow hematopoiesis. Third, we used three-point bending to assess the mechanical capacity of our treatment regime. It will be important in future studies to measure the more osteoporotic-relevant parameters of torsional stress and axial compression strength. Fourth, the requirement of irradiation for preconditioning is unacceptable for a non-life-threatening disease. However, it may be possible to use our therapy without irradiation because there are established protocols for donor cell engraftment without irradiation (32, 33). It is important to note



**Fig. 6.** Schematic diagram of PDGF-BB- $Sca1^{+}$  cells induced bone formation at the endosteal niche. (Upper) Normal niche: Under normal conditions, PDGF-BB produced by osteoblasts and osteoclasts/preosteoclasts (and perhaps other local cells) promotes the proliferation of MSCs and endothelial progenitor cells. (Lower) Treated niche: The intravenously injected PDGF-BB- $Sca1^{+}$  cells homed to the HSC niche at the endosteum following preconditioning. After engraftment in the niche, the HSCs constitutively produce large amounts of PDGF-BB (large gray arrow), which acts as potent mitogen for nearby MSCs and endothelial progenitor cells. The local production of the Bmps is sufficient to promote the differentiation of MSCs ultimately to osteoblasts. PDGF-BB may also activate *Bmp* signaling in osteoblasts. As a result, there is a robust increase in endosteal bone formation (Lower, treated niche). We propose the same sequence of events for the perivascular niches, which leads to increased trabecular bone formation.

that the osteogenic response with our therapy is so robust that only a low engraftment level would lead to a substantial increase in bone formation. Moreover, patients who are already receiving HSC transplantation and are at high risk for osteoporosis (34) could be considered for this therapy.

In conclusion, transplantation of mouse HSCs engineered to express PDGF-BB by the PGK promoter in the normal mouse results in a rapid, robust, and persistent formation of mineralized bone, leading to a considerable increase in bone strength, which is attributed to large increase in de novo trabecular formation and trabecular connectivity, and a significant reduction in cortical porosity. The stem cell gene-therapy approach may be potentially safer than intravascular injection of PDGF-BB, because optimal levels of PDGF-BB in bone marrow can be achieved without affecting PDGF-BB baseline levels in circulation. These data suggest that our HSC-based PDGF-BB treatment may be developed into a novel anabolic therapy for bone loss-related disorders in the future.

## Materials and Methods

Detailed information is provided in *SI Materials and Methods*.

All animal work was approved by the Institutional Animal Care and Use Committee of the Loma Linda University and the Animal Care and Use Review Office of the United States Department of the Army. Bone marrow Sca1<sup>+</sup> cell

isolation and lentivirus preparation and transduction were performed as previously described (35). Trabecular BMD was measured with a STRATEC XCT 960M peripheral quantitated computed tomography (pQCT) using XCT software v5.40 (Roche Diagnostics) as previously described (35).  $\mu$ CT analysis of the femoral bone was performed using a Scanco VivaCT 40 instrument (Scanco Medical). The mechanical strength of the femurs was evaluated at midshaft by the three-point bending test, using an Instron DynaMight 8841 servohydraulic tester (Instron). The RT-qPCR was done as previously reported (35). Primer sequences are listed in [Table S1](#). A total of  $2 \times 10^5$  marrow cells were plated into 0.01% gelatin-coated plates for CFU-F and CFU-Ob assays. Crystal violet staining was stained for CFU-F assay after 14 d, and Alizarin red staining was used for CFU-Ob assay after 21 d.

Data are presented as mean  $\pm$  SD. Data comparison between two groups was analyzed using Student's *t* test. Data comparison between more than two groups was analyzed using one-way ANOVA followed by Turkey's multiple comparisons test. We measured the linear relationships between maximum load force and femur cortical bone volume, as well as that between maximum load force and trabecular bone volume in the midshaft of femurs using Pearson's correlation coefficient. The *P* value of  $< 0.05$  was considered statistically significant. Sample sizes were  $n = 8$  for each group, or otherwise indicated.

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