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## Pluripotent Stem Cells and Skeletal Regeneration – Promise and Potential

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### Abstract

Bone is a regenerative tissue, capable of healing itself after fractures. However, some circumstances such as critical size defects, malformations, and tumor destruction may exceed the skeleton's capacity for self-repair. In addition, bone mass and strength decline with age, leading to an increase in fragility fractures. Therefore the ability to generate large numbers of patient-specific osteoblasts would have enormous clinical implications for the treatment of skeletal defects and diseases. This review will highlight recent advances in the derivation of pluripotent stem cells, and in their directed differentiation towards bone-forming osteoblasts.

### Keywords

Bone; Skeleton Regeneration; Stem Cells

### Introduction

The ancient Greek myth of Prometheus, forced to endure repeated destruction of his liver by an eagle as punishment for giving fire to humans, has underscored our enduring fascination with organ regeneration. Recent advances in stem cell biology hold promise that tissue regeneration may soon transition from mythology into reality. Stem cells are unique in their ability to both self-renew and give rise to differentiated tissues, and thus represent an appealing cellular population for regenerative medicine. In this review I will focus on pluripotent stem cells and their potential applications in skeletal biology and regenerative medicine in murine and human models.

The direct use of stem cells in diseases affecting the skeleton, particularly in combination with tissue engineering, can be readily applied to critical defects in bone, for example as a result of trauma or tumor-mediated destruction. In contrast, osteoporosis is one of the most common degenerative diseases of aging, resulting in fragility fractures in 50% of women and 25% of men over the age of 50, but characterized by diffuse bone loss. Comprised of over 206 discrete and uniquely shaped elements, the skeleton presents unique challenges to

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Compliance with Ethics Guidelines

Human and Animal Rights and Informed Consent

All studies by Joy Y. Wu involving animal and/or human subjects were performed after approval by the appropriate institutional review boards. When required, written informed consent was obtained from all participants.

efforts aimed at the regenerative process. However, stem cells may prove useful in disease modeling and drug screening to identify pathways and compounds that effectively increase bone mass or strength.

Within the bone marrow, mesenchymal stem cells can give rise to osteoblasts, adipocytes, and chondrocytes among other tissues of mesodermal origin (1-4). When needed, as in the case of fracture healing osteoblast progenitors can rapidly expand and form new bone. While adult bone marrow MSCs may be an appealing source of patient-derived osteoblasts, in reality their use for clinical applications is limited by low frequencies within the bone marrow, the need for invasive acquisition by bone marrow biopsy, limited self-renewal potential, and decreasing numbers and differentiation capacity with age (5). In recent decades the ability to derive and differentiate pluripotent stem cells has generated great excitement as a potential limitless source of cells and tissues for regenerative medicine. Here I will review the generation of murine and human embryonic stem (ES) cells and induced pluripotent stem (iPS) cells, and their potential applications in skeletal diseases.

## Embryonic stem cells

Embryonic stem cells are derived from the inner cell mass of the blastocyst, and are self-renewing and pluripotent. Mouse ES cells were first described in 1981 (6, 7), and combined with homologous recombination technology have made possible the generation of genetically engineered mice that have revolutionized disease modeling in vertebrate organisms. Human ES cells were first isolated in 1998 (8). The ability of ES cells to contribute to any tissue makes them ideal for regenerative purposes, and intensive efforts have focused on differentiating ES cells into various tissues. However, human ES cells in particular have the severe limitation that their derivation requires the destruction of human embryos, and it is not possible to generate patient-specific lines. This potentially limits their utility in cell transplant, although some have proposed that by generating banks of HLA-typed ES lines it would be possible to match most recipients (9).

A key component of any regenerative strategy involving stem cells is directed differentiation into the tissue of choice. As a model system for understanding lineage commitment and differentiation, embryonic stem cells have proven invaluable. Insights from the embryology and developmental biology have been used to direct the induction of endoderm, mesoderm, and ectoderm in differentiating ES cells (reviewed in (10)), with reports of directed differentiation into a variety of tissues including neurons (11-13), cardiomyocytes (14, 15), and pancreatic progenitors (16).

## Directed differentiation of ES cells into osteoblasts

The earliest reports of directed differentiation of murine (5, 17) and human (18) ES cells into osteoblasts relied on embryoid body formation, in which ES cells are aggregated into clusters, usually in hanging droplets, to induce tri-germ layer differentiation. After several days in culture embryoid bodies are disassociated and plated in osteogenic medium, typically consisting of ascorbic acid (AA) and an organic phosphate source such as  $\beta$ -glycerophosphate ( $\beta$ GP) (Table 1). Additional factors such as dexamethasone, retinoic acid (RA), bone morphogenetic proteins (BMPs) and vitamin D3 (VD3) have variously been

reported to enhance osteogenic differentiation of ES cells (19-23). Early studies relied predominantly on in vitro assays of osteogenic differentiation, including mineral deposition, alkaline phosphatase activity, and expression of markers of osteoblast differentiation (5, 17, 18, 20, 22, 23). However, these assays can be positive even when only a small percentage of cells have differentiated into the osteoblast lineage, and EB differentiation typically results in marked heterogeneity containing cells of multiple lineages. Therefore measuring the efficiency of osteogenic differentiation is challenging. Use of flow cytometry for cell surface markers of osteoblast lineage cells is one approach, however such markers must often be used in combination, and vary among research groups (3). Another strategy is the use of fluorescent reporters targeted to the osteoblast lineage. Xin et al. used zinc finger nuclease technology to direct the osteoblast-specific fluorescent reporter Col2.3GFP to a “safe harbor” site in human ES cells (24). This now enables the use of flow cytometry to quantify GFP+ cells that have differentiated into the osteoblast lineage.

To further increase the efficiency of osteogenic differentiation of ES cells, several groups have examined the use of 3-dimensional scaffolds in culture. Jukes et al. differentiated ES cells into a cartilage matrix to recapitulate endochondral ossification, and when these matrices were transplanted into critical-size cranial defects in rats, they underwent cartilage hypertrophy, calcification, and ultimately replacement by bone (25). Other scaffolds that have been tested include decellularized osteoblast-derived extracellular matrix alone (26, 27) or on a PLGA scaffold (28), microcarriers (29), type I collagen gel (30), and hydroxyapatite/tricalcium phosphate (HA/TCP) (24, 31). Furthermore, investigators have tried to simulate mechanical loading in culture with approaches such as cyclic loading in a compression chamber (32) or culture on BioFlex plates (33). In the future a combination of these approaches will likely further enhance our ability to differentiate ES cells into osteoblasts.

As a word of caution, as mentioned above osteogenic differentiation of ES cells is frequently assessed by in vitro assays such as mineral deposition and expression of osteoblast markers. However, in vitro assays do not reliably predict bone formation in vivo (31), therefore osteogenic capacity is ideally evaluated in vivo. The most common in vivo assays of bone formation are subcutaneous implantation (usually combined with a carrier) in immunocompromised mice (19, 27, 29, 31, 34), or healing of a critical-size defect in the calvaria (24, 25) or burr-hole fracture in mice (29, 30).

## Induced pluripotent stem cells

In 2006, Shinya Yamanaka reported the astonishing finding that introduction of only 4 factors – Oct3/4, Sox2, c-Myc, and Klf4 – was sufficient to convert murine fibroblasts into pluripotent stem cells (35), termed induced pluripotent stem (iPS) cells. The following year following the derivation of iPS cells from human somatic cells was reported using OCT4, SOX2, NANOG and LIN28 (36). These cells resemble ES cells in morphology and growth kinetics, and as confirmation of pluripotency form teratomas in vivo and contribute to chimeric embryos when injected into blastocysts. The ability to derive such induced pluripotent stem (iPS) cells from easily accessible somatic cells has transformed stem cell biology – it is now possible to generate unlimited numbers of patient-matched stem cells for

disease modeling, drug screening, and regenerative therapies – and for this discovery Dr. Yamanaka was awarded the 2012 Nobel Prize in Physiology or Medicine.

Since then there have been significant technical advances focused on increasing the safety of pluripotency factor delivery methods (reviewed in (37, 38)). Particularly when considering applications involving cells as regenerative therapy in humans, the importance of inducing pluripotency without permanent integration of genetic elements, as might occur with viral transduction, is paramount (39). To that end, recent promising studies have focused on delivery via episomal plasmids (40) or as recombinant proteins (41). In early studies the efficiency of pluripotency induction was very low, typically less than 1%; while reprogramming is likely initiated in a much higher percentage of somatic cells expressing the pluripotency factor, most fail to achieve a pluripotent state (38). A variety of small molecules targeting epigenetic modifiers, MAPK, Wnt and TGF- $\beta$  signaling pathways have been reported to enhance efficiency of pluripotency induction (42-46).

From the first reports of iPS cells, there has been great interest in how similar they truly are to ES cells, and in a related vein, whether iPS cells derived from different somatic cell sources retain an epigenetic “memory” of their cells of origin. Initial reports focused on the similarities between iPS and ES cells; perhaps not surprisingly, these were then followed by reports that iPS and ES cells have differential gene expression (47) and DNA methylation (48, 49). Several groups have noted persistent donor cell gene expression in iPS cells (50, 51) and epigenetic memories of donor cells (34, 52, 53). However, these studies were generally performed with small numbers of iPS and ES cell lines. More recently researchers have noted that when large numbers of ES and iPS cell lines are compared, it becomes more difficult to distinguish differences between pluripotent cell lines (54-56) due to high inherent variability (reviewed in Yamanaka 2012).

Unfettered by the ethical and logistical constraints that overshadow the isolation of embryonic stem cells, induced pluripotent stem (iPS) cells can be derived from a wide array of tissues. From the first reports of patient-derived iPS cells (57, 58), iPS technology has enabled the generation of disease-specific stem cell lines that can be used for studying disease pathogenesis as well as screening for novel therapeutic targets. Combined with gene editing techniques, there is hope that iPS cells can also be used for regenerative and curative therapies (reviewed in (59)). Already in mice researchers have reported the treatment of sickle cell anemia and Fanconi anemia using iPS cells (60, 61).

Highlighting the potential of iPS cell modeling to study skeletal diseases, Matsumoto et al. generated iPS cells from skin fibroblasts of patients with fibrodysplasia ossificans progressiva (FOP). When induced to undergo endochondral development, FOP-iPS cells demonstrated increased mineral deposition and enhanced chondrogenesis in vitro. (62). iPS cells have also been used to investigate the molecular mechanisms underlying osteosarcoma development in patients with Li-Fraumeni familial cancer syndrome, and identified dysregulation of the imprinted gene H19 during osteogenesis as a key factor (63). Other potential skeletal diseases amenable to iPS cell modeling include fibrous dysplasia/McCune Albright syndrome and osteogenesis imperfecta. For monogenic diseases, gene editing approaches may one day provide a source of healthy replacement cells. For any potential

cell-based therapy involving iPS cells, several safety issues remain to be resolved including risks of teratoma or other neoplasm formation, immunogenicity of transplanted cells, and heterotopic differentiation (reviewed in (64)).

## Directed differentiation of iPS cells into osteoblasts

Both murine (65, 66) and human (67) iPS cells have been differentiated into osteoblasts, following protocols similar to those used to direct ES cells into the osteoblast lineage (Table 2) (reviewed in (37)). Some groups have relied on differentiation into mesenchymal stem cell (MSC) intermediates followed by osteogenic differentiation (65, 67). In addition to AA,  $\beta$ GP and dexamethasone, other factors that have been studied for their abilities to improve the differentiation of iPS cells into osteoblasts include RA (65, 66, 68-70), transforming growth factor  $\beta$  (TGF- $\beta$ ) (70-73), fibroblast growth factors (FGFs) (70, 71, 73) and BMPs (70, 73). Adenoviral expression of the osteoblast transcription factor Runx2 can also increase osteoblast differentiation from iPS cells (66). More recently, Kanke et al. developed a stepwise approach based on serum-free monolayer culture without EB formation, using small molecule inducers to direct iPS cells first into mesodermal intermediates followed by skeletal progenitors and then osteoblasts with high yield (74). As with ES cells, in vitro assays of osteogenic differentiation do not predict successful formation of bone in vivo (70), therefore iPS-derived osteoblasts should also be tested by in vivo assays of bone formation such as subcutaneous implantation in syngeneic (68) or immunocompromised (70, 75, 76) mice. In another model, iPS-derived MSCs have been used to rescue a murine model of hind-limb ischemia (67).

## Direct reprogramming

While iPS cells hold great promise given the ability to derive patient-matched cells as a source for regenerative therapy, the low efficiency of iPS cell derivation from specific patients, potential risk of teratoma formation, and protracted time required for directed differentiation into tissues of choice are still practical limitations. The discovery of MyoD demonstrated that a single master transcription factor had the ability to directly convert fibroblasts into myoblasts (77). Since then there has been great interest in identifying master transcription factors for other lineages; now with the understanding that induction of pluripotency requires multiple transcription factors, investigators have begun to identify combinatorial factors that can directly reprogram one differentiated cell type into another without the need for a pluripotent intermediate (38). The cell of origin typically shares a common developmental origin with the target cell (reviewed in (78)). In 2008 the conversion of exocrine to endocrine pancreas cells was accomplished with 3 factors (79). This has been followed by protocols for reprogramming fibroblasts into neuronal cells (80), hepatocytes (81), cardiac myocytes (82), and hematopoietic progenitors (83). More recent studies have demonstrated direct reprogramming in vivo in mice to generate pancreatic beta cells (79), cardiomyocytes (84, 85), and neurons (86, 87). To date, there have not been any studies of directed reprogramming into osteoblasts. However, it is reasonable to expect that a combination of transcription factors, likely including Runx2, required for osteoblast differentiation, can be similarly identified to reprogram cells into osteoblasts.

## Conclusions

Recent advances in the study of pluripotent stem cells may soon enable the generation of unlimited numbers of osteoblasts. Induced pluripotency and direct reprogramming further provide the opportunity to derive disease-specific and patient-matched cell lines that have tremendous potential for regenerative approaches to skeletal disease, in addition to understanding disease pathogenesis and screening for novel therapeutic compounds. Further improvements in differentiation efficiency and tissue engineering will likely accelerate this translational process. Several issues remain to be clarified, including the ideal cell types for reprogramming, as well as safety from teratoma formation.

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Conflict of Interest

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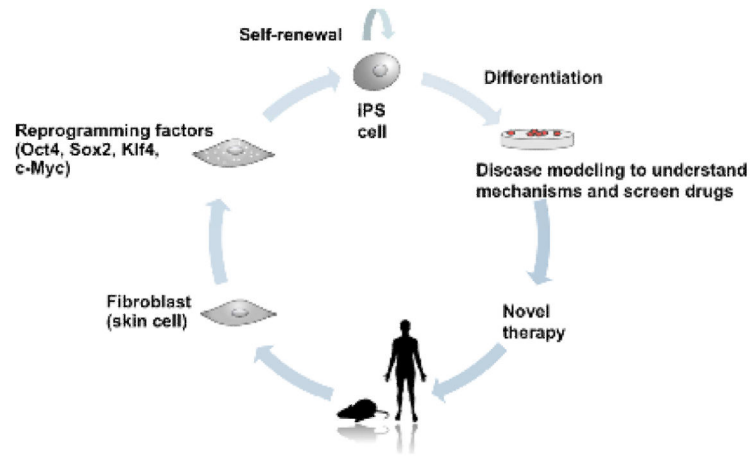
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**Figure 1. Derivation and applications of induced pluripotent stem cells**

iPS cells can be derived from patient-derived somatic cells by the introduction of the reprogramming factors Oct4, Sox2, Klf4 and c-Myc. Self-renewing iPS cells can then be directed to differentiate into cell lineages of choice, and can be used for either disease modeling or drug screening, or as cell-based regenerative therapies. Figure courtesy of James Oh.

**Table 1**

Osteogenic differentiation of embryonic stem cells.

Embryoid body (EB) vs monolayer (ML)	Factors tested	Additional conditions (eg bioreactor)	Assays (mineral deposition, gene expression, implant)	Reference
<i>Mouse</i>				
EB	AA, $\beta$ GP, dex		<ul style="list-style-type: none"> <li>Mineral deposition</li> <li>Immunostaining for osteocalcin</li> </ul>	(5)
EB	AA, $\beta$ GP, RA, BMP2		<ul style="list-style-type: none"> <li>Mineral deposition</li> <li>Osteogenic marker expression</li> </ul>	(70)
EB	AA, $\beta$ GP, VD3		<ul style="list-style-type: none"> <li>Mineral deposition</li> <li>Osteogenic marker expression</li> <li>ALP activity</li> </ul>	(22)
EB	AA, $\beta$ GP, dex		<ul style="list-style-type: none"> <li>Osteogenic marker expression</li> <li>Microarray</li> <li>Mineral deposition</li> </ul>	(20)
EB	AA, $\beta$ GP, VD3, RA, BMP2		<ul style="list-style-type: none"> <li>Osteogenic marker expression</li> <li>Microarray</li> <li>Mineral deposition</li> </ul>	(23)
		ESCs seeded on scaffold to form cartilage matrix	<ul style="list-style-type: none"> <li>Healing of rat critical-size cranial defect</li> </ul>	(25)
EB	AA, $\beta$ GP, dex	Decellularized osteogenic extracellular matrix	<ul style="list-style-type: none"> <li>Mineral deposition</li> <li>Osteogenic marker expression</li> </ul>	(26)
ML	AA, $\beta$ GP, dex	CultiSpher S microcarrier	<ul style="list-style-type: none"> <li>Osteogenic marker expression</li> <li>Mineral deposition</li> <li>Subcutaneous implant in SCID mice</li> <li>Healing of burr-hole fracture in mice</li> </ul>	(29)
EB	AA, $\beta$ GP, dex		<ul style="list-style-type: none"> <li>Mineral deposition</li> <li>Osteogenic marker expression</li> <li>Compared to BMSCs and calvarial osteoblasts</li> </ul>	(88)
EB	AA, $\beta$ GP, VD3	3D type I collagen gel	<ul style="list-style-type: none"> <li>Healing of burr-hole fracture in mice</li> </ul>	(30)
EB	AA, $\beta$ GP, dex, PPAR $\gamma$ inhibitor, RA		<ul style="list-style-type: none"> <li>Mineral deposition</li> <li>Osteogenic marker expression</li> <li>Immunostaining for Runx2, osterix</li> </ul>	(89)

Embryoid body (EB) vs monolayer (ML)	Factors tested	Additional conditions (eg bioreactor)	Assays (mineral deposition, gene expression, implant)	Reference
EB	AA, $\beta$ GP, VD3	Cyclic loading	<ul style="list-style-type: none"> <li>Osteogenic marker expression</li> </ul>	(32)
EB	AA, $\beta$ GP, dex, BMP4		<ul style="list-style-type: none"> <li>Osteogenic marker expression</li> </ul>	(21)
<b>Human</b>				
EB	AA, $\beta$ GP, dex		<ul style="list-style-type: none"> <li>Mineral deposition</li> <li>Osteogenic marker expression</li> </ul>	(18)
EB	AA, $\beta$ GP, dex		<ul style="list-style-type: none"> <li>Mineral deposition</li> <li>Osteogenic marker expression</li> <li>Subcutaneous implant in SCID mice on PDLA scaffold</li> </ul>	(19)
ML	Various	HA/TCP particles or carpet	<ul style="list-style-type: none"> <li>Osteogenic marker expression</li> <li>Subcutaneous implant in immunodeficient mice</li> <li>Teratoma formation</li> </ul>	(31)
EB		Lentiviral expression of Runx2 and BMP-2-enriched hydrogel	<ul style="list-style-type: none"> <li>Osteogenic marker expression</li> <li>Immunostaining for osteocalcin and type I collagen</li> <li>Mineral deposition</li> <li>Subcutaneous implant in immunodeficient mice</li> </ul>	(90)
ML	AA, $\beta$ GP, dex	Decellularized bone scaffolds and perfused bioreactor culture	<ul style="list-style-type: none"> <li>Immunostaining for osteocalcin</li> <li>Subcutaneous implant in immunodeficient mice</li> </ul>	(27)
ML	AA, $\beta$ GP, dex	Mechanical strain on BioFlex plates	<ul style="list-style-type: none"> <li>Immunostaining for osteocalcin and type I collagen</li> <li>Mineral deposition</li> <li>Osteogenic marker expression</li> </ul>	(33)
ML	AA, $\beta$ GP	Decellularized osteogenic matrix on PLGA scaffold	<ul style="list-style-type: none"> <li>Mineral deposition</li> <li>Immunostaining for osteocalcin</li> <li>Osteogenic marker expression</li> </ul>	(28)
ML		Zinc finger nuclease targeting of Col2.3GFP and hydroxyapatite/collagen matrix scaffold	<ul style="list-style-type: none"> <li>Teratoma formation</li> <li>Implant into mouse calvarial defect model</li> </ul>	(24)

Abbreviations: AA – ascorbic acid;  $\beta$ GP –  $\beta$ -glycerophosphate; RA – retinoic acid; VD3 – 1,25OH-vitamin D3; PDLA – poly-D, L-lactide; ALP – alkaline phosphatase; BMSC – bone marrow stromal cell; PLGA – poly(lactic-co-glycolic acid); HA/TCP – hydroxyapatite/tricalcium phosphate

**Table 2**

Osteogenic differentiation of induced pluripotent stem cells.

Embryoid body (EB) vs monolayer (ML)	Factors tested	Additional conditions (eg bioreactor)	Assays (mineral deposition, gene expression, implant)	Reference
<i>Mouse</i>				
EB	RA, AA, $\beta$ GP, dex	Adenoviral expression of Runx2	<ul style="list-style-type: none"> <li>Osteogenic marker expression</li> <li>Teratoma formation</li> <li>Alkaline phosphatase activity</li> <li>Mineral deposition</li> </ul>	(66)
EB	RA, TGF- $\beta$ 1, AA, $\beta$ GP, dex		<ul style="list-style-type: none"> <li>Teratoma formation</li> <li>Flow cytometry</li> <li>Mineral deposition</li> <li>Osteogenic marker expression</li> </ul>	(65)
EB	RA, AA, $\beta$ GP, dex	Gelfoam sponges	<ul style="list-style-type: none"> <li>Mineral deposition</li> <li>Osteogenic marker expression</li> <li>Subcutaneous implant into syngeneic mice</li> </ul>	(68)
EB	RA, AA, $\beta$ GP, dex		<ul style="list-style-type: none"> <li>Mineral deposition</li> <li>Electron microscopy</li> <li>Osteogenic marker expression</li> </ul>	(69)
<i>Human</i>				
		iPSC-derived MSCs	<ul style="list-style-type: none"> <li>FACS for CD24<sup>-</sup> CD105<sup>+</sup> cells</li> <li>In vitro osteogenic, chondrogenic and adipogenic differentiation</li> <li>Mineral deposition</li> <li>Transplant into mouse model of hind-limb ischemia</li> </ul>	(67)
ML	AA, $\beta$ GP, dex	Decellularized bone scaffolds and perfused bioreactor culture	<ul style="list-style-type: none"> <li>Mineral deposition</li> <li>Alkaline phosphatase activity</li> <li>Osteogenic marker expression</li> <li>Subcutaneous implant into immunodeficient mice</li> </ul>	(75)
	AA, $\beta$ GP, dex	PCL scaffold	<ul style="list-style-type: none"> <li>Flow cytometry for osteopontin</li> <li>Osteogenic marker expression</li> <li>Subcutaneous implant into immunodeficient mice</li> </ul>	(76)
EB	AA, $\beta$ GP, dex FGF-2, TGF- $\beta$ 1, BMP-2/7		<ul style="list-style-type: none"> <li>Alkaline phosphatase activity</li> <li>Osteogenic marker expression</li> <li>FACS for TNAP<sup>+</sup> cells</li> <li>Electron microscopy</li> </ul>	(73)

Embryoid body (EB) vs monolayer (ML)	Factors tested	Additional conditions (eg bioreactor)	Assays (mineral deposition, gene expression, implant)	Reference
ML	Various	HA/TCP particles or carpet	<ul style="list-style-type: none"> <li>Osteogenic marker expression</li> <li>Mineral deposition</li> <li>Subcutaneous implant in immunodeficient mice</li> </ul>	(70)
EB	AA, $\beta$ GP, dex, VD3	Calcium phosphate cement scaffold	<ul style="list-style-type: none"> <li>Flow cytometry for MSC markers</li> <li>Mineral deposition</li> <li>Alkaline phosphatase activity</li> </ul>	(91)
EB	AA, $\beta$ GP, dex, FGF-2, IGF-1, TGF- $\beta$		<ul style="list-style-type: none"> <li>FACS for TNAP+ cells</li> <li>Osteogenic marker expression</li> </ul>	(71)

TNAP – tissue-nonspecific alkaline phosphatase; PCL – poly(caprolactone); MSC – mesenchymal stem cell