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## **Effects of an opioid (proenkephalin) polymorphism on neural response to errors in health and cocaine use disorder**

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## **Abstract**

Chronic exposure to drugs of abuse perturbs the endogenous opioid system, which plays a critical role in the development and maintenance of addictive disorders. Opioid genetics may therefore play an important modulatory role in the expression of substance use disorders, but these genes have not been extensively characterized, especially in humans. In the current imaging genetics study, we investigated a single nucleotide polymorphism (SNP) of the protein-coding proenkephalin gene (*PENK*: rs2609997, recently shown to be associated with cannabis dependence) in 55 individuals with cocaine use disorder and 37 healthy controls. Analyses tested for *PENK* associations with fMRI response to error (during a classical color-word Stroop task) and gray matter volume (voxel-based morphometry) as a function of Diagnosis (cocaine, control). Results revealed whole-brain Diagnosis × *PENK* interactions on the neural response to errors (fMRI error>correct contrast) in the right putamen, left rostral anterior cingulate cortex/medial orbitofrontal cortex, and right inferior frontal gyrus; there was also a significant Diagnosis  $\times$ *PENK* interaction on right inferior frontal gyrus gray matter volume. These interactions were driven by differences between individuals with cocaine use disorders and controls that were accentuated in individuals carrying the higher-risk *PENK* C-allele. Taken together, the *PENK*  polymorphism – and potentially opioid neurotransmission more generally – modulates functioning and structural integrity of brain regions previously implicated in error-related processing. *PENK*  could potentially render a subgroup of individuals with cocaine use disorder (i.e., C-allele carriers)

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more sensitive to mistakes or other related challenges; in future studies, these results could contribute to the development of individualized genetics-informed treatments.

#### **Keywords**

cocaine addiction; proenkephalin; error processing; functional magnetic resonance imaging; imaging genetics

## **1. INTRODUCTION**

Error processing is a core executive function that allows for successful identification and correction of discrepancies between an intended and executed response [1, 2]. In health, the neural correlates of error-related processing typically encompass a network of regions of the medial prefrontal cortex (PFC) including the anterior cingulate cortex (ACC) [3–5]. Despite this common neural signature, error-related processing is also modulated by individual differences [6–9]. That is, certain individuals or groups may differ in the frequency with which they commit errors, and/or in the reactivity they show upon committing such errors. One important individual difference is the presence of a substance use disorder (SUD), a psychopathology marked by pervasive and disruptive neurocognitive disruptions (e.g., in error-related processing) that modulate the severity and course of the disease [10–19]. Our goal in the current study was to explore whether error-related processing in SUD is further modulated by another potentially important individual difference: opioid system genetics [specifically, a single nucleotide polymorphism (SNP) of the protein-coding proenkephalin gene (*PENK*: rs2609997)].

The opioid system forms a crucial component of the brain's reward circuit and importantly contributes to SUD symptomatology [20, 21]. Preclinical work has largely shown that knocking out proenkephalin – alone or in combination with related neuropeptides – reduces motivation, drug reward, and drug self-administration behavior [22–24]. In human SUD, opioid neurotransmission has been examined with positron emission tomography (PET). For example, [11C]carfentanil has been used to image mu opioid receptor binding in smokers  $[25–27]$ , and in abusers of heroin  $[28]$ , alcohol  $[29–31]$ , and cocaine  $[32–35]$ . More proximally to the current goals, *PENK* gene variants that have a functional relationship with gene expression levels have been associated with increased risk for marijuana use disorder [36] and opioid use disorder [37, 38]. In contrast, *PENK* was not associated with alcohol dependence [39], and a postmortem study of alcohol-dependent individuals and controls did not reveal differences in *PENK* expression [40]. These studies collectively provide some suggestive evidence that *PENK* is associated with a substance abuse phenotype, highlighting this SNP as a potentially interesting candidate for further study. However, the specific role of the gene in SUD remains unclear.

Here, we used an imaging genetics approach to test for *PENK* associations with fMRI response to error (during a classical color-word Stroop task) and gray matter volume as a function of cocaine use disorder (CUD) diagnosis. The C-allele of *PENK* SNP rs2609997, associated with increased *PENK* expression compared with the T/T genotype, has been characterized as the "riskier" allele because of its association with increased negative

emotionality and a higher prevalence of cannabis abuse [36]. Nevertheless, because the literature on the functional effects of this particular *PENK* SNP – and, indeed, of *PENK* in general – is minimal, the findings of the current study can add crucial new information to the field by clarifying the neurobiological and psychological implications of carrying this Callele. More specifically, uncovering this kind of intermediate imaging phenotype can provide important clues about this gene's operation vis-à-vis SUD [41]. Our decision to focus on CUD in the context of *PENK* was informed by prior research showing that *PENK*  mRNA expression is impaired in monkeys that self-administered cocaine [42] and in humans who used cocaine [43], and that variants of this gene have been linked to other addictive disorders [36]. Our decision to focus on errors in the context of *PENK* was informed by prior research showing that *PENK* mRNA is expressed in limbic brain regions (e.g., amygdala) [36], relevant to a Stroop task insofar as these regions participate in the assigning of negative valence to errors and other negative action outcomes [44]. More importantly, *PENK* is also expressed in regions of the PFC [40, 45–48], of core relevance for performing Stroop tasks (recently reviewed in [49]). In the current study, participants performed an event-related color-word Stroop task while undergoing functional magnetic resonance imaging (fMRI) [50]; we have previously used this task to evaluate error-related processing in CUD [51–53]. During these same scanning sessions, structural MRI was also collected. We hypothesized that the "riskier" C-allele of the *PENK* SNP rs2609997 (i.e., compared with the less risky T/T genotype) (A) would be associated with more frequent and severe cocaine use; and (B) would accentuate group differences between CUD and controls in structure and responsiveness to error in limbic and PFC brain regions as indicated by significant whole-brain  $\text{CUD} \times \text{PENK}$  interactions in these respective measures.

## **2. METHODS**

#### **2.1 Participants**

Fifty-five CUD and 37 healthy controls, recruited through advertisements, local treatment facilities, and word of mouth, participated in this research; all provided written informed consent in accordance with the local Institutional Review Board. Some of these participants have been included in prior imaging genetics studies in our lab, but these studies have always included different genes and/or different neural probes, and accordingly have reported activations in different brain regions [54–56]. More specifically, we previously reported on polymorphisms of the dopamine transporter (*DAT1*) [54] and the protein-coding monoamine oxidase A gene (*MAOA*) [55, 56] while participants performed a *drug-word*  inhibitory control task during fMRI [54], viewed unpleasant images during EEG [55], or simply while they underwent structural MRI scans [56]. For these reasons, overlap in variance with the current study is likely minimal. Exclusion criteria for the current study were: (A) history of head trauma or loss of consciousness (> 30 min) or other neurological disease of central origin (including seizures); (B) abnormal vital signs at time of screening; (C) history of major medical conditions, encompassing cardiovascular (including high blood pressure), endocrinological (including metabolic), oncological, or autoimmune diseases; (D) history of major psychiatric disorder, with some exceptions (for both groups: nicotine dependence; for CUD: comorbidities of known high co-occurrence including other SUD, major depression, and/or post-traumatic stress disorder [57, 58]); (E) pregnancy as

confirmed with a urine test in all females; (F) contraindications to the MRI environment; (G) except for cocaine in CUD participants, positive urine screens for psychoactive drugs or their metabolites (amphetamine or methamphetamine, phencyclidine, benzodiazepines, cannabis, opiates, barbiturates and inhalants) (note that although participants were permitted to have a current comorbid SUD as described below, participants who tested positive for other drugs indicating active use were excluded from all study procedures in the lab); (H) current evidence of intoxication from alcohol or any illicit drug. Protection against acute intoxication (alcohol and other drugs including cocaine) was afforded by our trained research staff, which has extensive experience with recognizing signs of intoxication in individuals with CUD (note that cigarette smoking was not restricted to avoid possible confounding effects on the fMRI results of cigarette withdrawal).

Participants underwent a comprehensive diagnostic interview, which consisted of: (A) Structured Clinical Interview for DSM-IV axis I Disorders [59]; (B) Addiction Severity Index [60], a semi-structured interview instrument used to assess history and severity of substance-related problems in seven problem areas (medical, employment, legal, alcohol, other drug use, family-social functioning, and psychological status); (C) Cocaine Selective Severity Assessment Scale [61], measuring cocaine abstinence/withdrawal signs and symptoms (i.e., sleep impairment, anxiety, energy levels, craving, and depressive symptoms) 24 hours within the time of interview; (D) Severity of Dependence Scale [62]; and (E) Cocaine Craving Questionnaire [63]. This interview identified the following cocaine-related diagnoses in CUD participants: current cocaine use disorder (N=43), cocaine use disorder in partial remission (N=8), and cocaine use disorder in full remission (N=4). Current Axis-I comorbidities were identified in 11 CUD participants, including marijuana use disorders  $(N=2)$ , alcohol use disorders  $(N=5)$ , ecstasy abuse  $(N=1)$ , and major depression  $(N=1)$ . Forty-two participants reported past comorbidities, including marijuana use disorder (N=27), alcohol use disorder (N=26), other stimulant use disorder (N=1), opiate (heroin) use disorder  $(N=2)$ , phencyclidine use disorder  $(N=2)$ , major depression  $(N=6)$ , and post-traumatic stress disorder (N=2). Because all CUD participants indicated that cocaine was their primary drug of choice and/or that cocaine had led to their most severe substance-related consequences, other drug use disorders were considered as secondary to the cocaine diagnosis. Nevertheless, we controlled for histories of alcohol and cannabis use in follow-up analyses.

A subset of participants (12 CUD, 10 controls) was culled from a protocol that included administration of a dopaminergic partial agonist (methylphenidate) or counterbalanced placebo. In this case, the placebo data were used for the current analyses. Importantly, participants in this administration study were not overrepresented in any of the study groups  $(\chi^2$ <sub>3</sub>=3.99, *p*>0.26). Yet, we controlled for this procedural issue in follow-up analyses.

#### **2.2 Genetics Screening**

Participants' genotype was determined using an ABI 7900HT available at the Mount Sinai Quantitative PCR Shared Resource Facility, ascertained with whole blood samples. The chosen *PENK* SNP (rs2609997) was selected for inspection based principally on a prior study that linked this SNP to addictive behavior (cannabis dependence) in a fully independent sample of participants [36]. This SNP was also chosen based on pairwise

linkage disequilibrium (LD) relationships of an  $r^2$  threshold of 0.8 and on haplotype data [\(www.hapmap.org\)](http://www.hapmap.org) showing a minimum allele frequency of 0.10 in the population. The call rate was 100%, and the genotypes conformed to Hardy-Weinberg equilibrium. Following prior work [36], we partitioned the study participants into those with the T/T genotype versus C-allele carriers. C-allele carriers included 21 CUD and 15 controls, and T/T genotype included 34 CUD and 22 controls; analysis of the cross-tabulations did not reveal significant differences ( $\chi^2$ <sub>1</sub>=0.05, *p*>0.8). Demographic and drug use information on the current study sample, split by *PENK* and Diagnosis, are provided in Tables 1 and 2, respectively.

#### **2.3 fMRI Procedures**

Participants performed three runs of an event-related fMRI color-word Stroop task, with instructions to press for the ink color of color-words (red, blue, yellow, green) printed in their congruent or incongruent colors [50–53]. Each task run contained 12 incongruent events, totaling 36 such events per participant; there were 188 congruent events, totaling 564 such events. Participants committed an average of  $28.7 \pm 26.2$  errors over the course of the task (i.e., summed across congruent and incongruent trials, and averaged across the 3 runs). No word or color of an incongruent stimulus mirrored the preceding congruent color-word; otherwise, stimuli were presented randomly. On each trial, a color word was presented for 1300 ms, which was also the time allotted for response (intertrial interval=350 ms); participants were not given performance feedback. Remuneration for task completion was \$25 (fixed).

**2.3.1 MRI Data Acquisition—**MRI scanning was performed on a 4T whole-body Varian/ Siemens MRI scanner. The blood-oxygenation-level-dependent (BOLD) fMRI responses were measured as a function of time using a T2\*-weighted single-shot gradient-echo planar sequence (TE/TR=20/1600 ms,  $3.125 \times 3.125$  mm<sup>2</sup> in-plane resolution, 4 mm slice thickness, 1 mm gap, typically 33 coronal slices, 20 cm FOV,  $64 \times 64$  matrix size, 90 $^{\circ}$ -flip angle, 200kHz bandwidth with ramp sampling, 207 time points, and 4 dummy scans to avoid nonequilibrium effects in the fMRI signal). Anatomical images were collected using a T1 weighted 3D-MDEFT (three-dimensional modified driven equilibrium Fourier transform) sequence [64] and a modified T2-weighted hyperecho sequence [65].

**2.3.2 BOLD-fMRI Analyses—**Image processing and analysis were performed with Statistical Parametric Mapping (SPM8) (Wellcome Trust Centre for Neuroimaging, London, UK). Echo-planar image reconstruction was performed using an iterative phase correction method that produces minimal signal-loss artifacts [66]. A six-parameter rigid body transformation (3 rotations, 3 translations) was used for image realignment and correction of head motion. Criteria for acceptable motion were 2 mm displacement and 2° rotation. All task runs from all participants meeting these motion criteria were included in the analyses (i.e., to maximize sample size in this imaging genetics study and similarly to our prior work [51, 52], we did not exclude participants listwise). The realigned datasets were spatially normalized to the standard Montreal Neurological Institute (MNI) stereotactic space using a 12-parameter affine transformation [67] and a voxel size of  $3 \times 3 \times 3$  mm. An 8-mm fullwidth-half-maximum Gaussian kernel spatially smoothed the data.

Two general linear models [68], which each included six motion regressors (3 translation and 3 rotation) and one task condition regressor convolved with a canonical hemodynamic response function and a high-pass filter (cut-off frequency: 1/90 s), were used to calculate individual BOLD-fMRI maps. Our primary design matrix of interest was constructed with one task regressor collapsed across both error trials (Congruent Incorrect and Incongruent Incorrect), leaving both correct trials (Congruent Correct and Incongruent Correct) to serve as the active, implicit baseline. Because the task contained mostly correct events, the beta weights for this incorrect (error) regressor reflected the variance to error events that remained after removing the variance related to correct events. Importantly, we have provided evidence that activations resulting from this design matrix reflect the error events, not the correct events [52]. Using this design matrix, we calculated a 1<sup>st</sup> Level contrast defined as (Incongruent Error + Congruent Error) – (Incongruent Correct + Congruent Correct). A secondary design matrix was constructed with one task regressor collapsed across both conflict trials (Incongruent Incorrect and Incongruent Correct), leaving both congruent trials (Congruent Incorrect and Congruent Correct) to serve as the implicit baseline. Using this second Design Matrix, we calculated a 1st Level contrast defined as (Incongruent Error + Incongruent Correct) – (Congruent Error + Congruent Correct).

At the  $2<sup>nd</sup>$  Level, we conducted two whole-brain 2 (Diagnosis: CUD, control)  $\times$  2 (*PENK*: T/T vs. C/T or C/C) analyses of covariance (ANCOVA), one for each fMRI contrast, in SPM8; demographic variables that differed between the groups inclusive of race, smoking history, age, education, verbal IQ, and depression (Tables 1 and 2) were included in the models as covariates of no interest. We specified a height threshold of *p*<0.005 voxel-level uncorrected (*T*=2.68). We then used a Monte Carlo procedure [69], a program similar to AlphaSim, to identify the number of contiguous voxels necessary for a  $p<0.05$  clustercorrected threshold (i.e., given our imaging parameters and a height threshold of *T*=2.68), which was calculated to be 26 contiguous voxels [52]. Moreover, we applied additional statistical correction considering that we analyzed separate design matrices for incorrect>correct and incongruent>congruent; thus, we only report activations at a  $p<0.01$ (rather than  $p<0.05$ ) cluster-corrected threshold. The BOLD signals from significant clusters were extracted to inspect for outliers, for use in correlation analyses (see below), and to ensure that our main effects were not attributable to substance use histories of alcohol or marijuana (Tables 2) or to administration of a placebo pill [which occurred in a minority of participants (see above)]. For all analyses, anatomical specificity was corroborated using the AAL atlas in MRIcron. Note that because group differences between CUD and controls have been previously explored in this sample [51, 53], in the current study we only report *PENK* main effects and Diagnosis  $\times$  *PENK* interactions.

**2.3.3 Gray Matter Volume Analyses—**Voxel-based morphometry (VBM) analysis was conducted with the VBM toolbox (VBM8) (Gaser, C, University of Jena, Department of Psychiatry, Germany; <http://dbm.neuro.uni-jena.de/vbm/>), which combines spatial normalization, tissue segmentation, and bias correction into a unified model. The MDEFT scans, which produce especially precise characterization of gray matter tissue [70], were first spatially normalized to standard proportional stereotaxic space (voxel size:  $1 \times 1 \times 1$ mm) and segmented into gray matter, white matter, and cerebrospinal fluid tissue classes

according to *a priori* tissue probability maps [71, 72]. A hidden Markov random field [73] maximized segmentation accuracy. Jacobian modulation compensated for the effect of spatial normalization and restored the original absolute gray matter volume in the gray matter segments. After smoothing the normalized and modulated gray matter segments with a 10 mm<sup>3</sup> full-width at half maximum Gaussian kernel, we again estimated a 2 (Diagnosis: CUD, control)  $\times$  2 (*PENK*: T/T vs. C/T or C/C) ANCOVA (with the same covariates of no interest as for the functional analyses). The number of contiguous voxels for significance was estimated to be 16 [69]; otherwise, the same statistical significance criteria as for the functional data were also applied for these analyses (*p*<0.01 cluster-corrected). Prior research has indeed revealed gray matter volume differences between CUD and controls [52,

**2.3.4 Correlation Analyses—**We first tested for functional-structural correspondence (correlations) between regions that showed parallel Diagnosis × *PENK* interactions for both methodologies. We then tested correlations between these functional activations or gray matter volume (i.e., limited to those activations that showed significant interactions) with behavior (task errors and reaction time) and current cocaine use frequency and severity (marked in Table 2). These correlations were conducted split by *PENK*; more exploratory correlations were also conducted to localize the source of any significant correlations that emerged (i.e., was a particular correlation driven by one diagnosis or significant across diagnoses?). Significance for all correlation analyses was set at *p*<0.002 to minimize Type I error (6 regions  $\times$  4 behavioral/drug use variables).

74–76], and one study showed gray matter differences as a function of a different gene

polymorphism (the monoamine oxidase A gene) [56].

## **3. RESULTS**

#### **3.1 Associations with Disease Severity**

In contrast to our first hypothesis, *PENK* was not associated with cocaine use frequency (days per week) or cocaine use severity (amount spent per use) within the CUD group (Table 2). The risk C-allele was also not more prevalent in CUD than controls.

#### **3.2 Task Behavior**

Our main interest in behavior was inspecting task errors, which were analyzed with a 2 (Diagnosis: CUD, control) × 2 (*PENK*: T/T, C-allele) × 2 (Trial: congruent, incongruent) mixed ANCOVA (that included all the same covariates as the SPM analyses). There were no main effects or interactions with *PENK*. We also examined reaction time, using a similar  $2 \times$  $2 \times 2$  mixed ANCOVA. This analysis revealed only a main effect of Trial [incongruent trials (891.8 ± 9.9 ms) > congruent (693.8 ± 7.0 ms) [*F*(1,82)=8.69, *p*=0.004], indicative of the reliable Stroop interference effect. Thus, neural effects of *PENK* (described below) are not attributable to group differences in task performance.

#### **3.3 Color-Word Stroop (Table 3)**

**3.3.1 Error>Correct Activations—**Main effects of *PENK* emerged in the superior frontal gyrus (C-allele>T/T genotype) and insula (T/T genotype>C-allele). Of greater interest, and supporting our second hypothesis, there were also Diagnosis  $\times$  *PENK* 

interactions to the error>correct contrast in the right putamen, left rostral ACC extending into medial orbitofrontal cortex (rACC/mOFC), and the right IFG extending to the middle frontal gyrus (dorsolateral prefrontal cortex). These interactions were driven by robust group differences between CUD participants and controls in individuals with the higher-risk *PENK*  C-allele (in putamen and rACC/mOFC: reduced error-related activations in CUD; in IFG: increased error-related activations in CUD). These group differences were either absent (putamen, IFG) or reversed (rACC/mOFC) in individuals with the T/T genotype (Figure  $1A-C$ ).

**3.3.2. Incongruent>Congruent Activations—**For this fMRI contrast of the classical Stroop effect, there were no Diagnosis × *PENK* interactions; only main effects of *PENK*  were observed. C-allele carriers showed greater activity to the incongruent>congruent contrast in the hippocampus, insula, postcentral gyrus, precentral gyrus, and supplementary motor area. Individuals with the T/T-genotype showed greater activity to this contrast in the cerebellum (vermis), middle/superior temporal gyrus, calcarine fissure, and bilateral thalamus. Given the lack of interactions with Diagnosis, these incongruent>congruent effects were not analyzed further.

#### **3.4 Structure (Table 3)**

A Diagnosis  $\times$  *PENK* interaction emerged in the right IFG, showing the same pattern of effects as the functional right IFG effect during error (Figure 1D). Other interaction effects were limited to visual and auditory areas.

#### **3.5 Brain-Behavior Correlations**

Across all task- and drug use variables, only one correlation reached significance. In the T/T genotype, the higher the IFG fMRI response to error, the fewer total errors were committed during the task [*r*(55)=−0.43, *p*=0.001]; a subsequent follow-up analysis (for this effect only) showed that this correlation was driven by controls, although it did not reach nominal significance  $[r(22) = -0.57, p=0.006]$ . Nevertheless, these effects could indicate that in this less risky genotype, all participants (and particularly controls) performed the task better when this IFG response to error was enhanced. Because this direction of activation in this genotype characterized the healthy controls (Figure 1), this correlation suggests that activation of this region in this context may be adaptive. IFG structure and function did not correlate.

#### **3.6 Other Substance Use History**

We repeated the analyses above that reached significance (brain interactions and brainbehavior correlations) while (separately) controlling for history of alcohol use to intoxication, history of cannabis use, and placebo administration (through ANCOVAs or partial correlations as appropriate). Even when controlling for these variables, interactions were still detected across the whole sample in the putamen ( $p$ <0.002), rACC/mOFC ( $p$ <0.004), and IFG function ( $p$ <0.055 for cannabis; otherwise,  $p$ <0.024) and structure (*p*<0.032). The negative correlation between the number of errors and fMRI response to error in the IFG also remained significant  $(p<0.001)$ . Thus, it is unlikely that our effects are

driven by histories of alcohol use or cannabis, or by the medication administration procedure.

## **4. DISCUSSION**

The current study explored whether the *PENK* SNP rs2609997 (*PENK*) modulates brain function (error-related processing, assessed with fMRI BOLD during an event-related colorword Stroop task) and structure (gray matter integrity, assessed with VBM) in health and CUD. Although *PENK* did not directly associate with CUD severity (unsupportive of our first hypothesis), group differences between CUD and controls on the neural response to error and gray matter integrity were accentuated in individuals carrying the riskier C-allele of *PENK* (supporting our second hypothesis).

Our results collectively showed that *PENK* modulated the neural response to errors in largely anticipated regions. In particular, diagnosis  $\times$  *PENK* interactions emerged during error-related processing in the rACC/mOFC, putamen, and IFG; and a similar Diagnosis  $\times$ *PENK* interaction emerged in IFG gray matter volume. A consistent pattern in these interactions was a robust group difference between CUD participants and controls especially in the C-allele carriers; in the rACC/mOFC, there was also an opposite Diagnosis difference in those with the T/T genotype. The rACC is a core region involved in error-related processing even during emotionally-neutral cognitive tasks, implicated in generating the affective response that occurs shortly after error commission [77–79]; the rACC is also a main region of interest in PET studies probing the opioid system (e.g., [11C]carfentanil imaging of mu opioid receptors [80, 81]). Interestingly, in the current study the more dorsal component of the ACC was not identified, possibly indicating that *PENK* modulation may have impacted emotion rather than cognition. Other regions activated in our study such as the putamen and IFG, although not as consistently identified during error-related processing as the ACC, are indeed often reported as supporting this function [82–89]. Furthermore, the putamen forms part of a limbic striatal circuitry that, in addition to the amygdala, is expected to be modulated by *PENK* [36].

One interpretation of these findings is that lower error>correct rACC/mOFC and putamen response, in this case conferred by the C-allele of *PENK*, might render this CUD subgroup more insensitive to mistakes. It is unclear from the current data whether such putatively reduced error sensitivity conferred by *PENK* translates into increased drug-taking (i.e., rACC/mOFC activations did not correlate with drug use variables), but our prior research suggests that this hypothesis merits follow-up in future studies [52]. It is also possible that this CUD subgroup might have compensated with increased IFG response, enabling comparable performance/behavior to the other groups (and in agreement with the negative correlation between this region and errors). Although the mechanisms of these collective effects require further clarification in future studies – and accordingly the current results/ conclusions should be interpreted with a degree of caution – our findings nonetheless support and justify additional investigation of this potentially interesting C-allele CUD subgroup.

Limitations of this study include the following. First, the sample size was relatively small for an imaging genetics approach. Importantly, however, all Diagnosis  $\times$  *PENK* cells always contained at least 15 participants. Moreover, we observed a similar interaction pattern for the IFG across function and structure, strengthening confidence in these effects. We also leaned heavily on results of a prior study with a completely independent sample that examined this same gene [36]. Second, we were unable to examine homozygote carriers of the C-C genotype, who were scarce in our sample  $(N=2 \text{ across all available participants})$ . If future studies can recruit C-C genotype participants, graded effects as a function of C-allele load could be inspected, similarly to research that has been conducted with the dopamine transporter gene [90–92]. Third, the study groups differed with respect to several demographic variables including race (Table 1), largely because assignment into genetic groupings did not reflect *a priori* recruitment; groups also differed with respect to multiple substance-related variables including use of cigarettes, alcohol, and marijuana (Table 2). For the former (demographics), results cannot be attributed to demographic covariates that differed between the groups because we controlled for these variables in the analyses. Further supporting this point, an exploratory examination of our main interaction effects in only African Americans showed that the average partial  $\eta^2$  across the four interactions only dropped in magnitude from 0.098 to 0.077, suggesting that this variable (or the other demographics that differed between the groups) did not drive the results. Also note that we elected to use this covariation strategy instead of between-group matching, as our foremost priority was to maximize sample size for this study (i.e., in recognition of the first limitation). For the latter (drug use history), it is difficult to recruit healthy controls with the same levels of cigarette, alcohol, and cannabis use who do not also meet criteria for a SUD. Although we controlled for these variables in follow-up ANCOVAs/partial correlations, future work should aim to validate these findings using an active control group of substanceusing but not dependent individuals. Fourth, we examined a single gene variant, and other genes could be involved in these effects. Importantly, however, the current study was conducted with firm *a priori* hypotheses regarding the impact of this *PENK* SNP on addictive disorders [36].

In conclusion, results of this study increase understanding of the *PENK* gene's modulation of brain structure and function in CUD. To our knowledge, this is one of the first studies to examine the functional correlates of this gene in human SUD – and the first to use functional neuroimaging for this purpose. This research augments work aiming to clarify the mechanisms underlying opioid genes' modulation of addictive disorders in humans [25, 26, 93] and of error-related processing more generally [94]. More importantly, our results suggest an intermediate phenotype that can increase understanding of the *PENK* gene's contribution to disease-relevant phenotypes such as SUD [41]. Investigation of the opioid system inclusive of the C-allele of *PENK* could ultimately aid in the development of individualized, genetics-informed treatments and medications in SUD that target specific deficits in this system. This approach could ultimately enable more appropriate and efficient allocation of scarce clinical resources and improved clinical outcomes in this difficult-totreat psychopathology.

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#### **Figure 1.**

 $PENK \times$  Diagnosis effects on brain function and structure. During an event-related fMRI Stroop task, interactions for the fMRI contrast error>correct were observed in the (A) putamen, (B) rostral anterior cingulate cortex extending to the medial orbitofrontal cortex (rACC/mOFC), and (C) inferior frontal gyrus/dorsolateral prefrontal cortex. For all regions, these interactions were at least partially driven by a more pronounced difference between ocaine abusers and controls in individuals carrying the "riskier" C-allele. (D) As assessed with voxel-based morphometry (VBM), there was a similar *PENK* × Diagnosis interaction on IFG gray matter volume, again such that differences between cocaine abusers and controls were accentuated in C-allele carriers. All images are displayed in neurological convention; for display purposes only, they are thresholded at  $2.0 \text{ T}$  5.0. Functional effects are in red shades; structural effects are in blue shades.

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**Table 1**



*b*significantly different from *PENK* T/T cocaine participants

 $b$  significantly different from  $PENK$  T/T cocaine participants

*c*significantly different from *PENK* C-allele carrier control participants

 $\stackrel{\textstyle\rm c}{\scriptstyle\rm sign}$  if<br>cantly different from  $PENK$  C-allele carrier control participants

*d*significantly different from *PENK* T/T control participants; all variables that differed between the groups were covaried in all analyses.

 $d$  significantly different from PENK T/T control participants; all variables that differed between the groups were covaried in all analyses.

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Drug use information of all study participants. Drug use information of all study participants.



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Note.

 $\alpha_{\rm Significantly}$  different from  $PENK$  C-allele carrier cocaine participants  $a_{\text{Significantly different from }PENK$  C-allele carrier cocaine participants

 $b$  significantly different from  $\it{PENK}$  C-allele carrier control participants *b*significantly different from *PENK* C-allele carrier control participants

 $c$  ,<br>significantly different from  $PENK$  T/T cocaine participants *c*significantly different from *PENK* T/T cocaine participants

 $d$  significantly different from  $PENK$  T/T control participants  $d$ <sub>significantly different from *PENK* T/T control participants</sub>

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 $\stackrel{e}{\mbox{'}}$  included in brain-behavior correlation analyses *e*included in brain-behavior correlation analyses

 $f_{\rm data~missing}$  from 3 cocaine participants and 6 controls *f*data missing from 3 cocaine participants and 6 controls

 $^g$  data missing from 2 cocaine participants and 8 controls. *g*data missing from 2 cocaine participants and 8 controls.

**Table 3**

Main- and interaction effects of PENK on brain function and structure. Main- and interaction effects of *PENK* on brain function and structure.





Note. Analyses are one-way ANCOVAs (controlling for variables that significantly differed between the groups as displayed in Table 1); rACC/mOFC=rostral anterior cingulate cortex/medial orbitofrontal<br>cortex; IFG/DLPFC=infe Note. Analyses are one-way ANCOVAs (controlling for variables that significantly differed between the groups as displayed in Table 1); rACC/mOFC=rostral anterior cingulate cortex/medial orbitofrontal cortex; IFG/DLPFC=inferior frontal gyrus/dorsolateral prefrontal cortex; BA=Brodmann Area; R=right, L=left, M=medial; fMRI=functional magnetic resonance imaging; VBM=voxel-based morphometry.