



Published in final edited form as:

J Trauma Acute Care Surg. 2015 October ; 79(4 0 2): S116–S120. doi:10.1097/TA.0000000000000740.

Preclinical Evaluation of Injectable Reduced Hydroxocobalamin as an Antidote to Acute Carbon Monoxide Poisoning

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Abstract

Background—Current management of acute inhalational carbon monoxide (CO) toxicity includes hyperbaric or normobaric O₂ therapy. However, efficacy has not been established. The purpose of this study was to establish therapeutic proof of concept for a novel injectable antidote consisting of the combination of hydroxocobalamin and ascorbic acid into a reduced form (B_{12r}) as demonstrated by clinically-significant increase (> 500 ppm) in CO₂ production, reduced carboxyhemoglobin (COHgb) half-life (COHgb *t*_{1/2}), and increased cerebral O₂ delivery and attenuation of CO-induced microglial damage in a preclinical rodent model of CO toxicity.

Methods—B_{12R}-mediated conversion of CO to CO₂ and COHgb *t*_{1/2} in human blood were measured by gas analysis and Raman resonance spectroscopy. Rats were exposed to either air or CO, then injected with saline or B_{12r}. Cognitive assessment was tested in a Morris water maze. Brain oxygenation was measured with Licox. Brain histology was assessed by fluorescent antibody markers and cell counts.

Results—B_{12r} resulted in significant CO₂ production (1170 ppm), compared to controls. COHgb *t*_{1/2} was reduced from 33 min (NS) to 17.5 (p < 0.001). In rat models, severe CO-induced brain hypoxia (Pb_iO₂ 18 mmHg) was followed by significant reduction in τ_{25} to 12 min for B_{12r} rats vs

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Disclosure: The authors declare no conflicts of interest.

40 min for NS-treated rats ($p < 0.0001$). There was major attenuation of CO-induced microglial damage, although cognitive performance differences were minimal.

Conclusion—Our preclinical data suggest that the novel synergism of hydroxocobalamin with ascorbic acid has the potential to extract CO through conversion to CO₂, independently of high-flow or high-pressure O₂. This resulted in a clinically-significant off-gassing of CO₂ at levels 5 to 8 times greater than controls, a clinically-significant reduction in COHgb half-life, and evidence of increased brain oxygenation and amelioration of myoglia damage in rat models. Reduced hydroxocobalamin has major potential as an injectable antidote for CO toxicity

Keywords

antidote; hydroxocobalamin; ascorbic acid; carbon monoxide toxicity

Carbon monoxide (CO) exposure is the leading cause of unintentional poisoning death and long-term morbidity in the US. In 2012 alone, there were over 13,000 cases reported to US poison centers, with 143 serious outcomes and 54 deaths¹. However serious delayed sequelae such as persistent and recurrent neurological deficits may occur in up to 30% of patients following apparent recovery from acute symptoms; these delayed neurological complications (DNS) may not become evident until weeks or months after exposure². Reduction in O₂ delivery to the tissues is thought to result from binding of CO to hemoglobin (Hgb) to form carboxyhemoglobin (COHgb). This results in conformational changes in Hgb that reduces its ability to offload O₂ to the tissues and subsequently causes decreased O₂ utilization, mitochondrial dysfunction, and hypoxic injury. As a result, current acute-care management involves either normobaric (NBO) or hyperbaric (HBO) oxygen therapy; however, efficacy for prevention of DNS is uncertain and has not been evaluated systematically³. Further limitations include unpredictable availability of equipment and delays between point of exposure, recognition of signs and symptoms, and initiation of therapy⁴. No antidotes for CO toxicity currently exist.

To be clinically useful, proposed antidotes for CO toxicity must be readily available, field-deployable, targeted, rapidly effective, and safe. We propose a solution of hydroxocobalamin (OHCbl), an FDA-approved antidote for cyanide poisoning, and ascorbic acid (vitamin C), a safe and powerful reducing agent. Other chemically-reduced forms of OHCbl (B_{12r}) have been demonstrated to convert CO to CO₂ in simple solutions *in vitro*⁵. We hypothesized B_{12r} could also facilitate conversion of CO to CO₂ in blood, resulting in the rapid reduction of the total body CO load via respiratory off-gassing of CO₂. The speed of this reaction should avert or reduce CO-induced DNS by early prevention of inflammatory changes associated with elevated intracellular CO levels. Antidote effectiveness can therefore be defined as both the demonstration of either irreversible binding or conversion of CO, and clinically-significant reduction of delayed neurological and cognitive deficits. We performed a two-part test of this hypothesis to establish therapeutic proof of concept: (1) *in vitro* CO removal from blood as demonstrated by a clinically-significant increase (> 500 ppm) in CO₂ production and reduction of carboxyhemoglobin (COHgb) half-life ($t_{1/2}$), and (2) *in vivo* demonstration in a preclinical rodent model of cognitive function, increased cerebral oxygen delivery, and attenuation of CO-induced microglial damage.

Methods

Reduced OHCbl (B_{12r}) was produced by combining 300 mg analytical grade hydroxocobalamin (OHCbl) and 300 mg ascorbic acid (AA) (Sigma-Aldrich, St. Louis, MO) in 5 mL deoxygenated 0.9% NaCl solution (NS_{deox}) in 100% N_2 environment to prevent auto-oxidation⁶.

***In vitro* experiments: B_{12r} -mediated CO reduction in blood**

IRB-exempt waste human venous blood was obtained from VCU Apheresis clinic; 600 mL was collected into standard blood collection bags and anti-coagulated with 70 mL of CPD-A1. Blood was used within 24-48 hours following collection. Blood was circulated through a closed-loop hollow-fiber membrane oxygenator (Pediatric Quadrox-iD[®], Maquet, Hirrlingen, Germany) and roller pump (Stöckert/Shiley[®], Soma Technology Inc, Bloomfield CT) at 250 mL/min, and maintained at 37°C with a countercurrent water-flow heat exchanger (DC 10, Thermo Haake, Fisher Scientific). The system was equilibrated with medical air (20-22% v/v O_2 ; <400 ppm CO_2 ; 78-80% v/v N_2) then 'poisoned' with 6000 ppm CO in research grade air (0.5838% v/v CO, balance air) for 20 minutes; all air flow rates were 178 mL/min. The system was then injected with 5 mL of either B_{12R} or one of three negative controls: NS_{deox} , AA (350 mg in 5 mL NS_{deox}), or B_{12A} (350 mg OHCbl in 5 mL NS_{deox}). CO_2 concentration (volume %) was sampled at 10 Hz (BIOPAC Inc., Goleta CA) over 30 minutes from the time of B_{12r} injection or when carboxyhemoglobin (COHgb) concentration reached 50%; in-flow gas was then switched back to medical grade air. Gas-out concentration of CO_2 was continuously measured at 10 Hz for 30 min post-infusion. Signals were amplified (CO2100C interface; BIOPAC Systems, Goleta, CA), and analog-digital conversions were performed online (AcqKnowledge[™] v. 4 software; BIOPAC Systems, Goleta, CA). Median CO_2 concentration for each solution was calculated from the normalized area under the curve (AUC) of the CO_2 -time response curves⁶.

Confirmation that CO_2 was derived from B_{12R} -mediated conversion of CO (and not an unidentified exogenous source) was obtained by radiocarbon tracing in separate trials. Twenty-mL of ^{13}C labeled CO (Cambridge Isotope Laboratories, Tewksbury, MA) was injected into the system 30 min prior to infusion with 5 mL B_{12R} . Gas samples were taken at baseline and 20 min post-infusion; the difference in the $^{13}CO_2/^{12}CO_2$ ratio between baseline and post- B_{12r} infusion was quantified by infrared spectral analysis (POCone[®], Otsuka Electronics Co., Japan)⁶.

Carboxyhemoglobin (COHgb) concentrations were determined by Resonance Raman (RR) spectroscopy. CO-poisoned blood with a COHgb concentration of 50% was treated with either high-flow atmospheric pressure O_2 alone, or with a combination of high-flow O_2 and B_{12r} solution. Blood samples were obtained at baseline and every 10 min for 120 min. RR spectra of COHgb were obtained for 20 μ L subsamples sealed into melting-point capillary tubes; excitation lines were obtained from a 406.7 nm krypton-ion laser excitation source (Coherent Saber) and attenuated output power of 0.07-0.08 mW, collected using a 600-mm single-grating monochromator, and imaged using a back-illuminated CCD camera (Python CCD, Princeton Instruments, Trenton, NJ). Scans were completed in 3-5 min⁷. COHgb half-life $t_{1/2}$ was calculated as $(\ln 2)/\lambda$, where λ is the rate constant for the decay function $P_t = P_0 \cdot$

$\exp(-\lambda \cdot t)$; P_t is peak height at time t , and P_0 is initial peak height. Calculations were performed in PROC NLIN (SAS 9.4).

In Vivo Studies

Ethics statement and animals—This study was approved in advance by the Institutional Animal Care and Use Committee (IACUC) of Virginia Commonwealth University (IACUC Protocol # AD10000569), and conforms to the Public Health Service Policy on Humane Care and Use of Laboratory Animals (2002). All rats were obtained from Harlan Laboratories (Indianapolis, IN) at 5-8 weeks of age. Before experimentation, animals were housed in pairs in ventilated cages and maintained at 25°C and 12L:12D, with *ad lib* access to food (commercial rat chow) and water. Animals were weighed daily for a minimum of 5 days prior to surgical procedures.

Brain oxygen tension—The experimental design was a 2×2 factorial on the factors *exposure* (medical air SHAM or CO) and *intervention* (NS or B_{12r}). Thirty male adult Sprague-Dawley rats (mass 315-370 g) were randomly allocated to one of four groups (SHAM-NS, SHAM-B_{12r}, CO-NS, CO-B_{12r}) with EXCEL random numbers algorithm; 10 animals were allocated to each CO group, and 5 to each sham group.

All surgical procedures were aseptic. Animals were anesthetized with isoflurane (4% for induction, 2% for maintenance, balance medical air). Core temperature was monitored with a rectal probe and maintained at 36-38°C for the duration of each trial with a thermostatically-controlled feedback heating blanket (Harvard Apparatus, Holliston, MA). The head was stabilized in a stereotaxic frame, the skull exposed along the midline, and two 2-mm burr holes were drilled 1-mm posterior to bregma and 3-mm lateral to midline. The duramater was gently incised to allow placement of calibrated Licox® brain oxygenation (CC.1.R.) and temperature (CB.8) probes (Integra Neuroscience, Plainsboro, NJ); probes were inserted 2.3 mm into the parenchyma. Animals were allowed to stabilize for 30 min. Animals were then exposed for 30 minutes to either 2500 ppm CO or medical air, followed by a single dose of intervention solution, either B_{12r} at 100 mg/kg or the weight-based equivalent volume of NS (2 mL/kg, IP); total volumes were 0.6-0.85 mL. Brain oxygen tension Pb_tO₂ was recorded every 5 min from initial exposure to 60 min post-infusion. Animals were then euthanized with sodium pentobarbital (Euthasol®, 40 mg/kg IV, Virbac Animal Health, Fort Worth, TX).

Post-infusion change of Pb_tO₂ over time t for both CO-exposure groups was described by the parametric nonlinear mixed-effects model $Pb_tO_2 = a \cdot [1 - b \cdot \exp(-k \cdot t)] + Z(t)$, where a is the maximum value of Pb_tO₂, b is a scaling parameter, k is the rate constant, and $Z(t)$ describes the random effects component for each animal. Differences between control and antidote were evaluated by contrasts on each parameter estimate⁹. Primary outcome was time to achieve Pb_tO₂ of 25 mmHg (τ_{25}); this is the approximate hypoxic brain tissue threshold established for humans¹⁰, and is approximately 75% of baseline Pb_tO₂ levels (33-35 mmHg) for rats. Calculations were performed in PROC NLMIXED (SAS 9.4).

Spatial learning—Forty-two male young adult Long-Evan rats (average initial weight 219 g; average terminal weight 300 g) were randomly assigned (RANDOM.ORG) to one of

three treatment groups: medical air only (SHAM, n = 12), CO exposure with NS infusion (CO-NS, n = 19) or CO-exposure with B_{12r} antidote infusion (CO-B_{12r}, n = 21). CO-exposed animals received 2500 ppm CO (0.25% CO, 27% O₂, balance N₂) for 60 min, followed by 6000 ppm CO (0.6% CO, 27% O₂, balance N₂) for 10 min or until loss of righting response; animals were then removed from the exposure chamber and immediately administered B_{12r} antidote or NS (2 mL/kg IP, 0.6-0.8 mL). Animals were allowed to recover in temperature-controlled recovery cages until they regained normal response to stimuli, and then returned to their primary housing cage.

Twenty-four hours following experimental exposures described above, animals began four-stage Morris Water Maze (MWM) testing. Deficits in MWM performance are associated with damage to specific regions of the brain involved with spatial navigation and learning, such as the hippocampus^{11,12}. Tests were conducted in a standard water maze pool (diameter 183 cm; depth 63.5 cm) with a submerged platform 2.5 cm below the water surface; non-toxic white paint was added as a water opacifier. The four test stages occurred on post-injury days 1, 3, 6, and 8. Each stage consisted of blocks of four swimming trials of 60 sec each, starting from one of four randomly-chosen compass positions, with a ten-minute inter-trial rest interval. Platform location was constant between trials, but moved to a new location for each stage. Testing was performed by a technician blinded to group assignment, and not involved with injury protocol or analyses. Animal movements were tracked and quantified with a ceiling-mounted video camera and computer-assisted tracking software (Med Associates Inc., St Albans, VT). Spatial learning was quantified by path efficiency (PE, %) estimated as the straight-line distance from start to platform divided by observed total swim path length⁷. Differences between treatments for median PE were assessed by nonlinear mixed-model analysis (PROC NL MIXED, SAS 9.4¹³).

Immunohistochemistry—Nine male Long-Evans rats (300-350 g), three from each of the above groups were killed on post-injury-day 10 with Euthazol (150 mg/kg IP), and fixed with 4% formalin via transcardial perfusion. Neuronal tissue was preserved in 4% formalin for 24 hours, then sectioned into 40 µm sections from bregma +3 to -7 on a Leica VT1000[®] vibratome. Sections were simultaneously blocked and incubated with primary antibodies at 4°C for 24 h utilizing a double-staining protocol for ionized calcium-binding adapter molecule-1 (Iba-1) and glial fibrillary acidic protein (GFAP). Tissue sections were then rinsed and incubated at room temperature for 60 min with secondary antibodies (DyLight-488 and DyLight-549) specific to the IBA-1 and GFAP antibodies. Control sections using only single antibodies and blocking solutions were prepared to examine non-specific binding. After curing for 24 hours sections were examined with a Zeiss LSM 710 laser scanning confocal microscope. Cell counts were obtained using an automated cell counting routine in NIH ImageJ (www.imagej.nih.gov). Microglial activation state was determined by morphometric analysis based on cell body size, process length, and thickness¹⁴. Astrocyte status was determined by manual morphometric analysis.

Results

In vitro studies

Median CO₂ concentration for B_{12r} averaged 1170 ppm, compared to < 200 ppm for controls. This represents a five- to eight-fold increase in the gas-out concentration of CO₂ (Fig. 1). We detected a 16.7% increase in the ¹³CO₂/¹²CO₂ ratio over baseline with B_{12r} infusion whereas infusing a standard sample with ¹³CO caused no interference in the analysis of ¹³CO₂. COHgb half-life *t*_{1/2} was 33 (95% CI 27, 42) min under O₂ alone, but was reduced to 18 (95% CI 15, 21) min with B_{12r} infusion, a difference of 15 min (*p* < 0.001).

In vivo studies

Pb_tO₂ of both sham-exposure groups of rats averaged 31 (95% CI 28, 35) mmHg throughout the procedure, with no change upon administration of antidote or NS control. Substantial brain hypoxia was induced with CO-exposure; Pb_tO₂ averaged 18 mmHg (95% CI 17, 19 mmHg) at 30 min. After administration of either NS or B_{12r} there was a nonlinear asymptotic increase to baseline Pb_tO₂ by the end of the monitoring period (Fig. 2); maximum Pb_tO₂ (33 mmHg) did not differ between CO-exposure groups (*p* = 0.61) or from sham groups. However *τ*₂₅ differed significantly between CO-exposed groups (*p* < 0.0001); *τ*₂₅ averaged 40 (95% CI 36, 45) min for CO-NS controls, compared to only 12 (95% CI 10, 13) min for CO-B_{12r} animals.

Median path efficiencies obtained from Morris water maze testing are shown in Fig. 3. There were no statistical differences between treatments at any time point (*p* > 0.2) although weak differences in learning trajectories were suggested by examination of medians. Rats exposed to medical air only showed the expected daily increase in path efficiency; efficiencies increased by an average of 8-10% per day over eight days of testing. In contrast, both CO-exposed groups showed a plateau in performance with either no change (CO-B_{12r}) or a modest decline (CO-NS 7%).

Preliminary immunochemistry data suggest loss in overall cell count (Fig. 4.A), increased demyelination (Fig. 4.B) and reduction of microglial activity (Fig. 4.C) associated with CO-exposure; however B_{12r} treatment appeared to partially reverse CO-induced damage. Myelinated axons were abundant in cortical layers 2-5 in control animals compared to CO-exposed animals. However whereas rats exposed to CO showed obvious deficit; CO- B_{12r} rats showed partial preservation of myelinated axons (Fig. 4.B). CO-exposed rats also exhibited microglia with morphology consistent with activation; cells had enlarged cell bodies and thicker, less-branched processes, compared to microglia of either control or CO-B_{12r} treated rats (fig. 4.C).

Conclusions

Victims of inhalational CO toxicity show a reduction of COHgb half-life from 5 hours on room air to 30-60 min with NBO and only 5 min with HBO. However neither of these interventions has been conclusively demonstrated to reduce the incidence of DNS, and may be difficult to deploy in a timely way. Our preclinical data suggest that the reduced form of

hydroxocobalamin, with ascorbic acid as the reducing agent, results in a clinically-significant off-gassing of CO₂ at levels 5 to 8 times greater than controls, a clinically-significant reduction in COHgb half-life, and evidence of increased brain oxygenation, and amelioration of myoglial damage in rat models. These data suggest a novel synergism of these two compounds when combined at high dose, with the potential to extract CO through conversion to CO₂, independently of high-flow or high-pressure O₂. Furthermore, these findings have significant clinical implications, as both hydroxocobalamin and ascorbic acid are safe and approved for use in humans, even at high doses^{15,16}. Reduced hydroxocobalamin has major potential as an injectable antidote for CO toxicity.

Acknowledgments

Financial Support: Microscopy was performed at the VCU department of Anatomy and Neurobiology Microscopy Facility, supported in part, with funding from NIH-NINDS Center Core grant (5P30NS047463). We thank the VCU Apheresis Clinic staff, the perfusion team (especially H. McCarthy and B. Chui), K. Luu, G. DeCosta, L. Thompson, and especially J. Turner (Chemistry) for their generous assistance. This work was supported by internal funds from the departments of Surgery and Anesthesiology (VCU Health System) and by generous donations of supplies and equipment from the departments of Surgery, Gastroenterology, and Perfusion (VCU Health System). L. G. S. is an active-duty member of the US Air Force on civilian institute status from the AF Institute of Technology. J. D. R. is a reserve member of the US Navy on HPSP scholarship.

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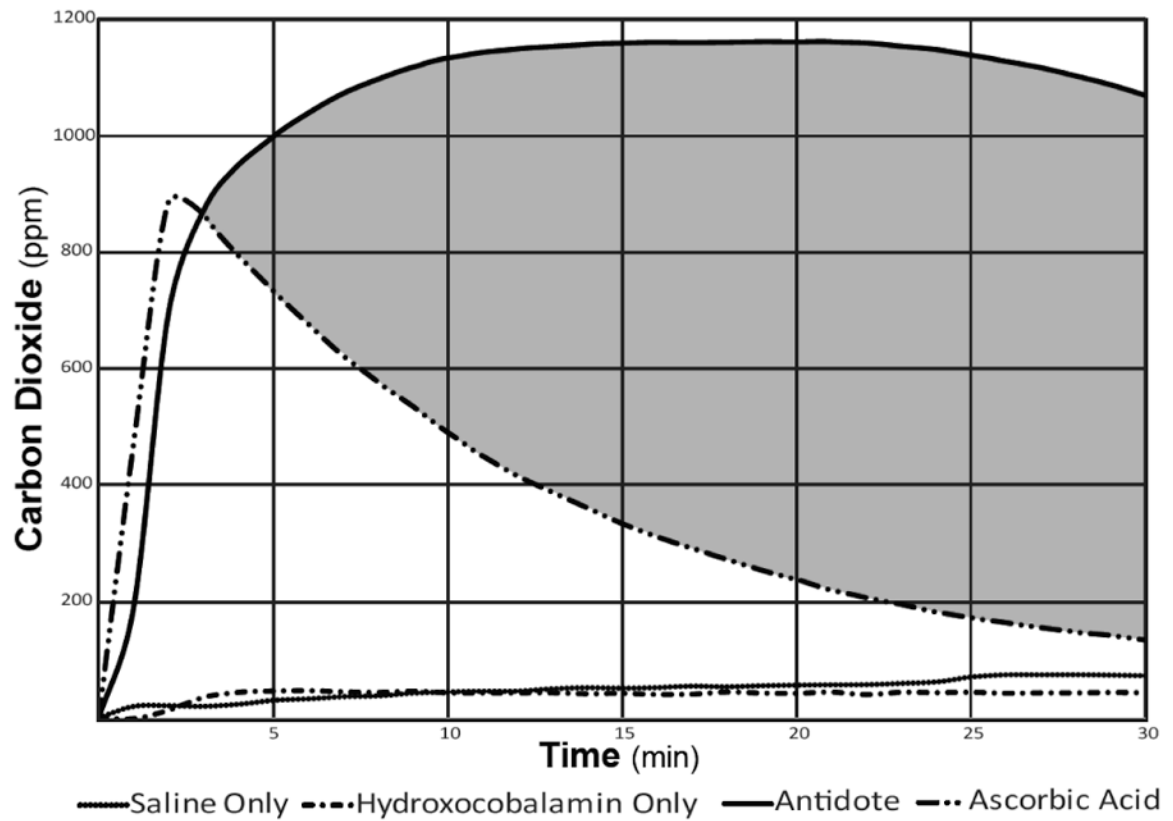


Fig. 1. Comparative CO₂ production (ppm/min) over 30 min induced by B_{12r} antidote (hydroxocobalamin B₁₂ + ascorbic acid) added to whole human blood containing 50% COHgb. The shaded area is the difference between CO₂ produced from ascorbic acid alone, and that produced by B_{12r}. Little or no CO₂ was produced by infusion of normal saline (NS) or oxidized hydroxocobalamin.

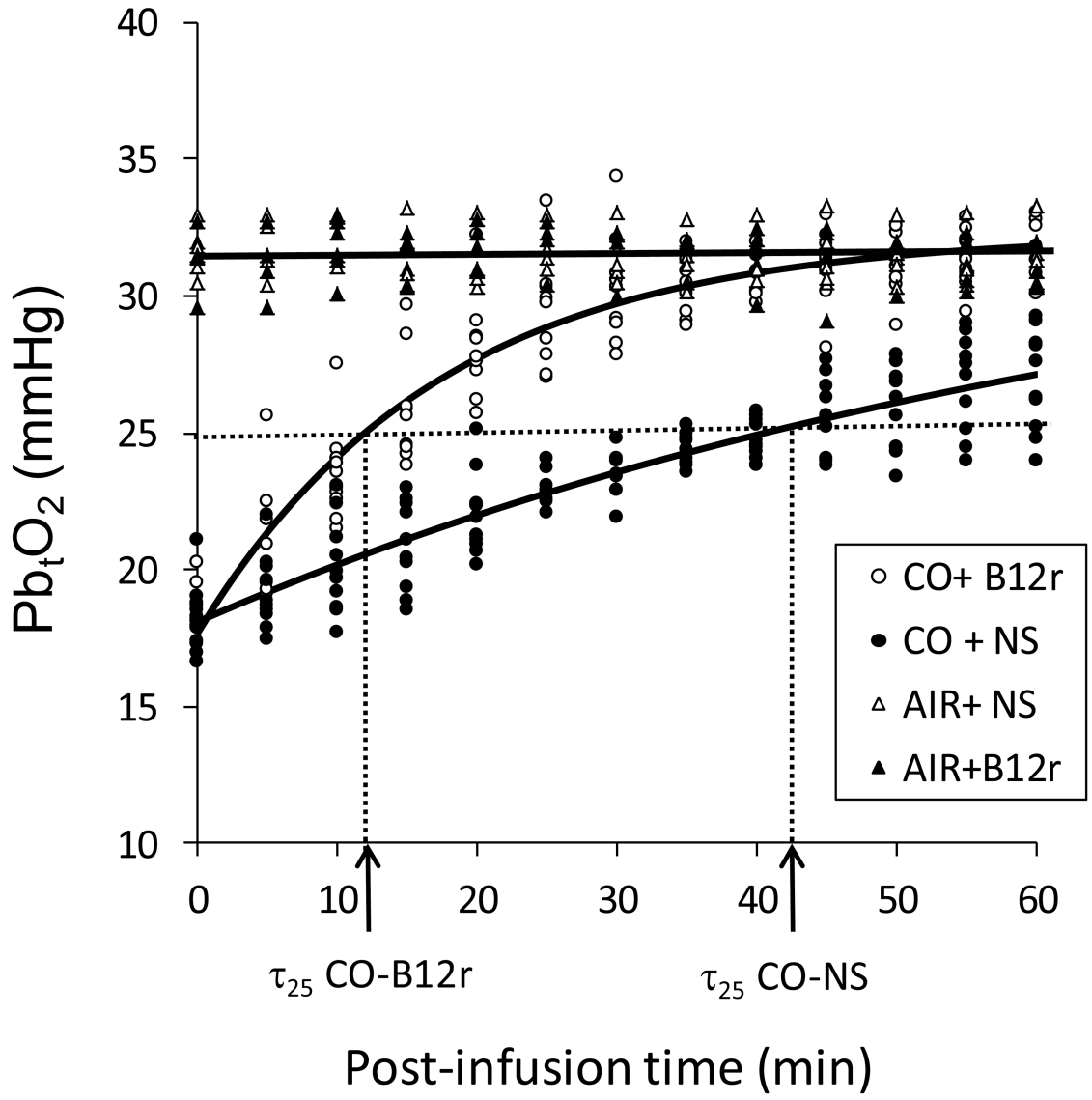


Fig. 2. Brain oxygen tension (Pb_tO_2 , mmHg) measured in 30 Sprague-Dawley rats exposed to medical air (AIR) or CO, and injected with either saline (NS) or antidote (B12r). Solid lines are fitted equations; dotted lines show estimated threshold τ_{25} for each CO-exposure treatment.

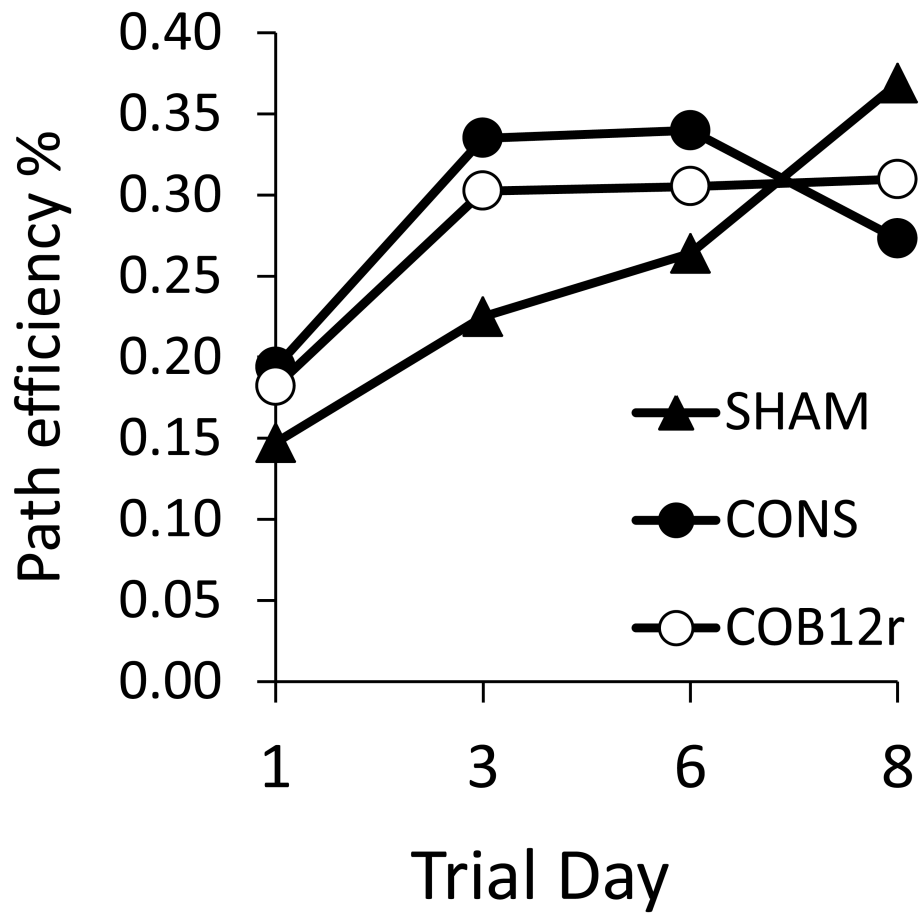
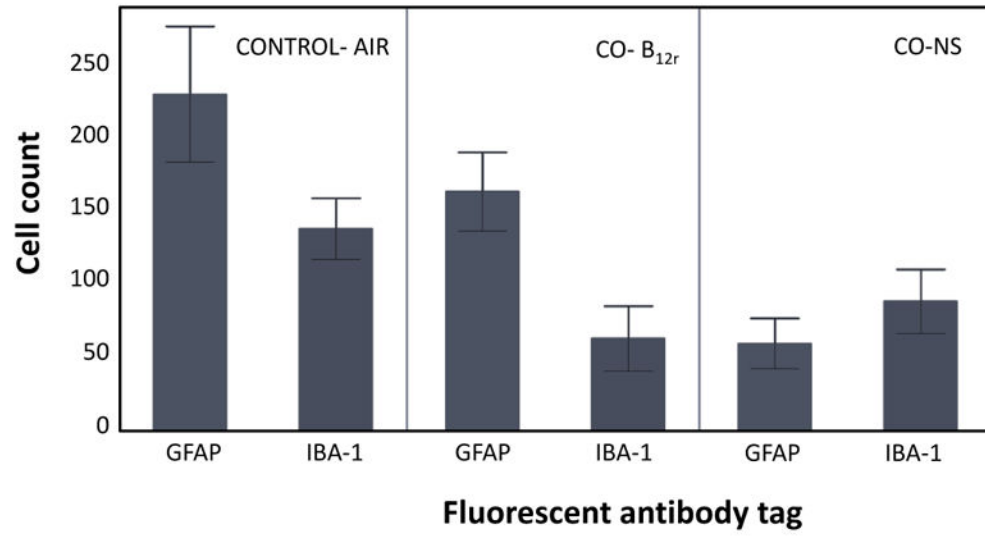
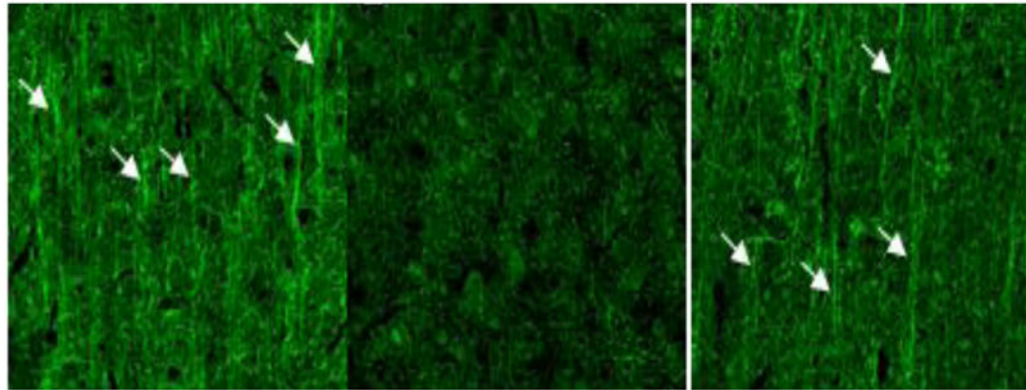


Fig. 3. Median path efficiencies (straight line distance/observed swim path length) for rats exposed to medical air (SHAM) or CO and injected with either NS (CO-NS) or antidote (COB12) and tested in a Morris Water maze over 8 days.

A



B



C

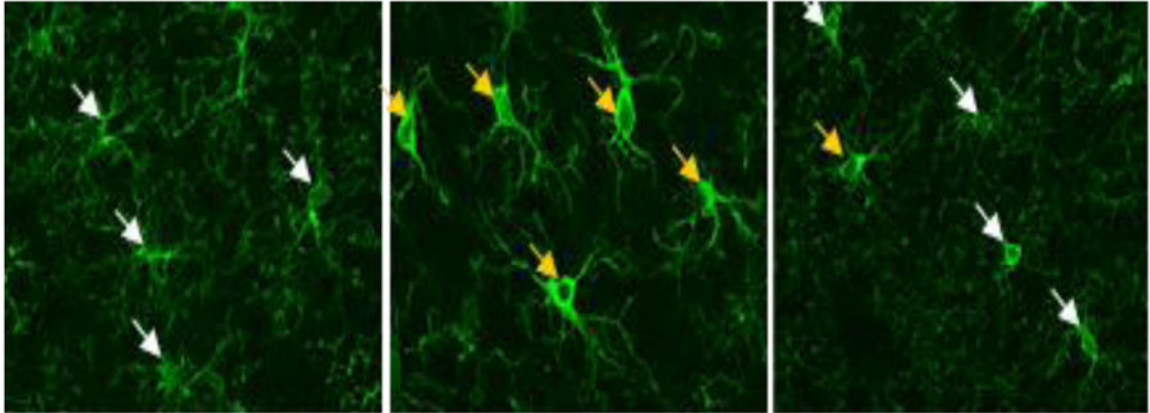


Fig. 4. Immunofluorescence of brain tissue of rats exposed to medical air (CONTROL) or CO with either antidote (B12r) or NS control solution. A. Mean (SD) microglial and astrocyte cell counts of GFAP and Iba-1 tagged cells; B. Relative myelination: Myelinated axons are indicated by white arrows. Note the paucity of myelin in the CO poisoned rats (center panel); C. Microglial activation. Yellow arrows highlight activated microglia based on increased Iba-1 staining density, thickened processes, and loss of arborization.