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# A Comparative Evaluation of EPR and OxyLite Oximetry Using a Random Sampling of $pO_2$ in a Murine Tumor

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# Abstract

Methods currently available for the measurement of oxygen concentrations (oximetry) in viable tissues differ widely from each other in their methodological basis and applicability. The goal of this study was to compare two novel methods, particulate-based electron paramagnetic resonance (EPR) and OxyLite oximetry, in an experimental tumor model. EPR oximetry uses implantable paramagnetic particulates, whereas OxyLite uses fluorescent probes affixed on a fiber-optic cable. C3H mice were transplanted with radiation-induced fibrosarcoma (RIF-1) tumors in their hind limbs. Lithium phthalocyanine (LiPc) microcrystals were used as EPR probes. The  $pO_2$  measurements were taken from random locations at a depth of ~3 mm within the tumor either immediately or 48 h after implantation of LiPc. Both methods revealed significant hypoxia in the tumor. However, there were striking differences between the EPR and OxyLite readings. The differences were attributed to the volume of tissue under examination and the effect of needle invasion at the site of measurement. This study recognizes the unique benefits of EPR oximetry in terms of robustness, repeatability and minimal invasiveness.

# INTRODUCTION

Many types of solid tumors are characterized by significant spatial and temporal heterogeneity in oxygenation. This is due in part to chaotic vasculature under elevated interstitial fluid pressure leading to compromised blood flow and regions of hypoxia. Tumor hypoxia is strongly linked to the poor outcome after chemotherapy or radiotherapy in several human malignancies (1, 2). Further, hypoxic tumors are biologically more aggressive. For example, it has been reported that hypoxic sarcoma or cervical cancers tend to metastasize (3, 4). Reports that poorly oxygenated tumors are more aggressive and less susceptible to treatment suggest that the tumor oxygenation status is an important parameter for cancer treatment (5, 6). The observation of substantial inter- and intratumor heterogeneities among tumors of similar histology and location further emphasizes the importance of the measurement of hypoxia in individual tumor/patients. In addition, the ability to monitor changes in the partial pressure of oxygen ( $pO_2$ ) after treatment could also have profound implications in the planning of effective follow-up therapeutic strategies (5, 6). In particular, radiotherapy could benefit from modulated treatment based on regional variations in  $pO_2$ .

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Thus there has been considerable interest in techniques capable of measuring spatial and temporal heterogeneity in tumors that may help predict treatment outcomes (7).

Some of the techniques reported to be useful for the measurement of oxygen concentration in tumors include polarographic electrodes (8), fluorescence-based techniques (9), comet assays (10), immunohistochemical techniques (11–13), optical spectroscopy (14), magnetic resonance spectroscopy (7, 15), and positron emission tomography (16). Electron paramagnetic resonance (EPR) and OxyLite oximetry are two novel methods that share several similarities including their suitability for point measurements of  $pO_2$  in tissues and a higher sensitivity at the hypoxic conditions that occur in tumors. A comparison of the features of EPR and OxyLite oximetry is provided in Table 1. EPR oximetry uses implantable paramagnetic particulates (17–19), while OxyLite uses a fluorescent probe attached to a fiberoptic cable (9). Both techniques use probes that do not consume oxygen. EPR oximetry uses changes in the EPR linewidth caused by the interaction of paramagnetic molecular oxygen with the paramagnetic probe to determine  $pO_2$  (20). OxyLite consists of an optical fiber that carries light pulses that are used for inducing fluorescence in the ruthenium (II) chloride complex attached to the tip of the fiberoptic cable. The lifetime of fluorescence determines  $pO_2$ , because it is inversely proportional to the oxygen tension at the tip (9). Although neither of these methods has been used clinically, they have the potential to be useful for oxygen measurements in humans. The goal of this study was to compare the two methods in an experimental tumor model. The study used a radiationinduced fibrosarcoma (RIF-1) tumor implanted in the hind limb of mice. The measurements were made from random locations within the tumor immediately and 48 h after implantation of the LiPc probe. The present study established EPR oximetry for reliable measurements of oxygen concentration in viable tissues and emphasized the unique capability of noninvasive and repeated measurements from the same site.

#### MATERIALS AND METHODS

#### Materials

Lithium phthalocyanine (LiPc) was synthesized in our laboratory as described (21). OxyLite probes were purchased from Oxford Optronix, UK.

#### **Animal Preparation**

The animal studies were done under a protocol approved by the Institutional Laboratory Animal Care and Use Committee of The Ohio State University. Female C3H mice, obtained from Charles River Laboratories (Wilmington, MA) were used. One million RIF-1 cells were implanted in the subcutaneous tissue of the right hind limb. The tumors were ~350 mm<sup>3</sup> in volume at the time of  $pO_2$  measurements. All surgical procedures and measurements were performed under ketamine/xylazine anesthesia (200 mg/kg body weight, 14 mg/kg body weight i.p.). Two groups of mice were used: (1) a day 0 group of 58 mice in which the EPR and OxyLite  $pO_2$  measurements were performed immediately after the implantation of the EPR probe and (2) a day 2 group of 43 mice in which the EPR and OxyLite measurements were performed 48 h after implantation of the EPR probe.

#### **EPR Measurements**

For EPR oximetry, about 10 µg of LiPc microcrystalline powder was implanted within the tumor at a depth of ~3 mm using a 22-gauge needle. The EPR measurements were performed, after 30 min of implantation, using an L-band (1.2 GHz) spectrometer with the following settings: incident microwave power, 210 µW; sweep width, 0.2 mT; modulation amplitude, 5 µT; modulation frequency, 100 kHz. The peak-to-peak widths of the first-derivative EPR spectra were converted to  $pO_2$  using a calibration curve (21). The duration of the EPR readings was ~5 min. An infrared lamp was used to maintain the body temperature within 36–37°C.

#### **OxyLite Measurements**

OxyLite probes (with ruthenium chloride complex) come precalibrated at 37°C. Their response is non-linearly dependent on temperature. A 22-gauge needle was used to place the probe into the tumor, but the needle was withdrawn, leaving the probe (attached to the cable) behind in the tissue. Readings were taken for about 10 min after stabilization, while stabilization took anywhere from 10 to 30 min. A heating pad was used to keep the body temperature of the mice within 36–37\_C. In a few selected experiments in each group, the temperature of the tumor tissue was monitored using a dual ( $pO_2$  and temperature) OxyLite probe. The OxyLite measurements were performed at multiple sites (up to four) within the same tumor at a depth of ~3 mm.

#### **Histological Study**

Tumors were isolated and fixed in 10% paraformaldehyde, made into paraffin blocks, and sectioned into 4- $\mu$ m slices. The slices were stained with  $\alpha$ -actin (smooth muscle, stained for blood vessels) and DAPI (a nuclear stain). Slides were observed under an inverted light microscope with an epifluorescence attachment that enabled collection of fluorescent images (Nikon TE-2000U). Digital macrophotographs of the paraffin blocks were also taken.

#### Statistical Analysis and Reporting

The mean  $pO_2$  values are expressed as means  $\pm$  SEM. The significance levels between mean  $pO_2$  values were determined using the Student's unpaired *t* test. Values of P < 0.05 were considered significant. The Mann-Whitney *U* test was used to determine significance levels between median values.

## **RESULTS AND DISCUSSION**

One EPR and up to four OxyLite readings were taken from each tumor. The data were obtained from independent sites at a depth of ~3 mm in the tumor. Two sets of data were collected. In the first set, both the EPR and OxyLite data were obtained immediately after the implantation of the EPR probe (day 0). In the second set, the data were obtained 48 h after the implantation of the EPR probe (day 2). Figure 1 shows the OxyLite  $pO_2$  values plotted relative to the EPR  $pO_2$  values for each tumor on day 0 and day 2. Both sets of data showed significant scatter within the set as well as differences in the nature of scatter between sets. In general, the OxyLite values were more scattered than the EPR values. Whereas the scatter of data within the set is attributed to the well-established spatial

heterogeneity of  $pO_2$  in RIF-1 tumors, the differences between the sets (day 0 and day 2) are most likely due to measurement artifacts. The EPR implant occupies a considerably larger volume (~400-µm diameter of a spherical deposit) when compared to the size of the OxyLite probe (220 µm) (22). The smaller size of the OxyLite probe could allow display of a large variance among multiple sites in the heterogeneous tumor. On the other hand, the EPR probe would report the mean value of  $pO_2$  averaged over a relatively large volume in the tumor, thereby resulting in a reduced variance/scatter of readings compared to OxyLite.

Figure 2 shows the mean  $pO_2$  values of EPR and OxyLite on day 0 and day 2. The mean  $pO_2$  of the EPR/day 0 set was 7.7 ± 0.6 mmHg. A significant reduction in the mean  $pO_2$  (5.5 ± 0.7 mmHg) was observed on day 2. A similar trend was observed in the case of median  $pO_2$  values. The EPR measurements on day 0 were made immediately after the implantation of the probe, i.e. from a freshly implanted site. The trauma associated with the implant, as well as possible rupture of microvasculature, could lead to a higher  $pO_2$  on day 0. The lower  $pO_2$  on day 2 could be due to the fact that, by then, the tissue had been able to recover from the trauma caused by the needle insertion. It might be argued that an increase in the tumor size during this period (48 h) could also contribute to the observed decrease in  $pO_2$ . Our earlier study (23) using repeated measurements during RIF-1 tumor growth did not show any significant variation of  $pO_2$  in the size range used in the present experiments. Thus the decrease in  $pO_2$  on day 2 cannot be attributed to the effect of increasing tumor size.

Further, EPR oximetry showed a higher mean  $pO_2$  on day 0 compared to that of the OxyLite on day 0. The EPR probe implant would occupy a greater volume  $(33.5 \times 10^6 \,\mu\text{m}^3,$ assuming a 400-µm-diameter spherical deposit) in the tissue compared to the OxyLite probe  $(5.7 \times 10^6 \,\mu\text{m}^3,$  corresponding to a diameter of 220 µm). The approximately six-fold larger volume of the EPR probe would result in a higher probability of the probe being closer to a well-perfused region of tissue, such as the proximity of a major blood vessel. This could explain why the EPR  $pO_2$  data values are higher compared to the OxyLite values on day 0. Further, the 22-gauge needle (0.71 mm diameter) used for the implantation of the probes would cause microvascular rupture and bleeding. Although the needles were removed in both cases, leaving the probes in the tissue, the OxyLite probe was still attached to the fiberoptic cable, while the EPR probe was left in the tissue. Thus the OxyLite probe could exert pressure at the site of measurement causing decreased perfusion and hence lower  $pO_2$  at the site. Furthermore, movement of the fiber-optic cable may cause fluctuations in pressure, causing instability in the measurements.

There was a reasonable agreement between the mean  $pO_2$  values obtained using the two techniques on day 2. The difference between the mean  $pO_2$  values of EPR/day 2 (5.5 ± 0.7 mmHg) and OxyLite/day 2 (6.2 ± 0.7 mmHg) was not significant. On the other hand, the OxyLite values showed a significant difference between day 0 (3.9 ± 0.5 mmHg) and day 2 (6.2 ± 0.7 mmHg). The fact that the OxyLite/day 2 value is more comparable to that of EPR day 0/2 suggests that the OxyLite day 0 readings may be suspect. At present there is no good explanation for this observation. It is possible that the trauma associated with the fresh implantation of the EPR probe on day 0 prior to OxyLite measurements could be responsible. However, this needs to be verified.

To understand the nature of tissue damage caused by the probe implantation, we performed histological analyses on excised tissues. Figure 3 shows visual images as well as stained sections of the tumor. The unstained visual image of EPR/day 0 tissue (panel A) shows significant hemorrhage (red color), suggesting rupture of microvasculature and bleeding. The hemorrhage is not observed on day 2. Also, OxyLite probe insertion seems to cause extensive hemorrhage, as is evident by the red surrounding tissue. The histological staining also reveals tissue damage in both cases. The smooth muscle  $\alpha$ -actin staining of blood vessels (red color in panel B), nuclear staining (blue color, panel C), and bright-light image (panel D) indicate a void space (indicated by dashed enclosure in panel C) in the tissue at the sites of EPR implant on day 2 and OxyLite. The histological results strongly emphasize the difference between an invasive measurement made immediately after implantation of the probe and a noninvasive measurement performed later (day 2 in this case) using EPR oximetry. While EPR oximetry enables the noninvasive measurements to be made days and weeks after implantation of the probe, this is not possible with OxyLite.

A histogram representation of the  $pO_2$  data obtained using EPR and OxyLite is shown in Fig. 4. The OxyLite data show more hypoxia and right-skewness compared to EPR data. In many tumors, including RIF-1 tumors, Eppendorf electrode measurements have always shown significantly right-skewed  $pO_2$  histograms (24). The present observation that the EPR  $pO_2$  values are significantly less skewed seems to suggest the importance of the probe size in the measurement of  $pO_2$ . As we noted before, the probe sizes are significantly different among the three methods. To explain the differences in the distribution of data obtained from OxyLite, EPR and Eppendorf microelectrode methods, computer simulations were performed. The diameters of microelectrode and OxyLite probe were 12 µm and 220 µm, respectively. The diameter of the deposit of LiPc crystals (EPR) was assumed to be 400 µm, approximated to a spherical deposit. Since most tumors are reported to have a right-skewed distribution because of their hypoxic nature and wide variance, we included both a rightskewed and normal distribution input model in the simulation.

The simulation was performed as follows. The tumor was represented by a  $512 \times 512$  matrix where the value of each matrix element represented the local  $pO_2$ . The ratios of areas for microelectrodes, OxyLite and EPR probes were 1:9:25 pixels. Although these ratios do not map to the exact ratios of the actual probe sizes, they were nevertheless sufficient to describe the effect of probe size on the data distribution. The simulation used a random selection of a set of pixels, for example, 1 pixel for microelectrode, 9 contiguous pixels for OxyLite, or 25 contiguous pixels for EPR. The average value was calculated from the selected set of pixels. Two kinds of initial random  $pO_2$  distributions (inputs) were used: a normal distribution and a right-skewed distribution. The results from the three oximetry methods were plotted in a histogram, and the mean, median and skewness values were calculated.

The simulation results, as shown in Table 2 and Fig. 5, revealed the microelectrode data distribution to be very close to the actual distribution (skewness 2.17 compared to the input skew of 2.31). OxyLite, which used a larger probe than the microelectrode, showed a decrease in the amount of skewness (skewness 1.07), while EPR showed a more normal distribution (skewness 0.39). The EPR probe, being present in a large volume in the tissue,

is expected to report the average of  $pO_2$  values that would most likely include both poorly oxygenated and well-oxygenated regions. On the other hand, in the case of a skewed input, the smaller probes like the microelectrode would show higher numbers of low  $pO_2$  values because of less averaging. Thus, while a single  $pO_2$  reading using EPR is a better representation of the overall  $pO_2$  of the tumor, the averaging effect due to the larger EPR probe size has a tendency to alter skewness that may be inherent to the  $pO_2$  distribution in the tumor. In the case of a normal distribution of inputs, all three methods showed a normal distribution.

The magnitude of the skewness also depended on the type of input (actual distribution of  $pO_2$ ). If the input contains gradually varying hypoxic regions with a large core of severely hypoxic region, as shown in Fig. 6A, a large probe size may *increase* the skewness (panels B and C). This type of input was used by Braun *et al.* (22) for simulating the effect of probe size between microelectrodes and OxyLite. On the other hand, if the input distribution is random, as shown in Fig. 6D, the skewness *decreases* as the probe size increases (panels E and F). The random distribution (panel D) is a more accurate representation of input data for our measurements. This is because most of our experimental measurements were away from the core of the tumor. Consequently, our measurements did not include contiguous regions of severe hypoxia, which usually occurs at the center of the tumor. This would explain why the skewness decreased with increasing probe size in our data.

It must be noted that the simulation did not take the following into account: (1) Measurements using microelectrodes are usually obtained by stepped movement of the probe, while OxyLite and EPR measurements are from a single site; (2) there are differences in the degree of invasiveness of the three methods; and (3) the EPR implant may not be spherical. Nevertheless, the differences in the probe sizes appear to be a contributing factor in the observed differences in the distribution of data obtained using OxyLite and EPR.

O'Hara *et al.* (25) have cited differences between EPR oximetry and OxyLite readouts from rat brain and attributed the differences to the variations in the volume, depth and location of measurement. Significant hemorrhage was observed in all the OxyLite tracks, while no bleeding was observed at the site of EPR implants. On the other hand, Elas *et al.* (26) performed EPR imaging on a murine FSa fibrosarcoma tumor by perfusing with a water-soluble probe and found a good correlation between the EPR and OxyLite data. The goal of our study was to compare "point" measurements of  $pO_2$  using particulate probe-based EPR spectroscopy and OxyLite.

Previously, OxyLite had been compared with other techniques, for example, microelectrodes (22, 27), paired cell survival assay (28), BOLD MRI (29, 30), and EPR (25, 31, 32). Braun *et al.* (22) reported that the discrepancy between microelectrodes and OxyLite was greater in tumors compared to normal tissue. With microelectrodes, less than 20% of the values were <1 mmHg, while over 50% of the OxyLite values were <1 mmHg. A good agreement between the hypoxic cell fractions measured by OxyLite and paired cell survival assays has been observed in tumors of less than 500 mm<sup>3</sup> (28). However, OxyLite showed higher hypoxic cell fractions for tumors larger than 500 mm<sup>3</sup>. Difficulties in the use of OxyLite, such as the stability of the readings, fragile probes, and the probe being extremely sensitive

to minor movement, have also been reported (28). It is also evident that the OxyLite method, being an invasive procedure, cannot be used for repeated measurements from the same site. Furthermore, OxyLite requires 10 to 20 min, or sometimes even longer, to stabilize, while EPR oximetry can be done in less than 1 min.

Microelectrodes have also been used for measurement of  $pO_2$  in RIF-1 tumors. Adam *et al.* (24) have reported a median  $pO_2$  of 1.2 mmHg in RIF-1 52 to 924-mm<sup>3</sup> tumors. Pogue *et al.* (33) have reported a median  $pO_2$  of 12.9 mmHg in 634 ± 203-mm<sup>3</sup> tumors. Kavanagh *et al.* (34) have reported a median  $pO_2$  of 1.2 mmHg and a mean of 4.5 ± 0.5 mmHg using Eppendorf.

In summary, the present study compared the oximetric capabilities of EPR and OxyLite for a random sampling of  $pO_2$  in a solid tumor. Both EPR oximetry and OxyLite reported  $pO_2$  values that were less than 10 mmHg, consistent with the hypoxic nature of the RIF-1 tumors. Despite some common features, including their applicability for point measurements and enhanced sensitivity for  $pO_2$  measurements in hypoxic tissues, the two methods showed considerable differences in the measured  $pO_2$  values. The differences can be attributed to the spatial heterogeneity of tumor oxygenation and the "examined" area/volume of measurements. The OxyLite data showed a right-skewed distribution while the EPR data showed a more normal distribution. The EPR oximetry, on the other hand, is more consistent, particularly when the measurements are performed 48 h or more after implantation of the probe. The EPR oximetry is not subjected to probe-pressure artifacts and subsequent measurements can be performed noninvasively and repeatedly over long periods.

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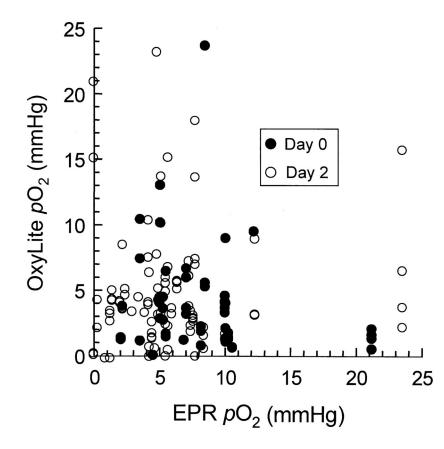
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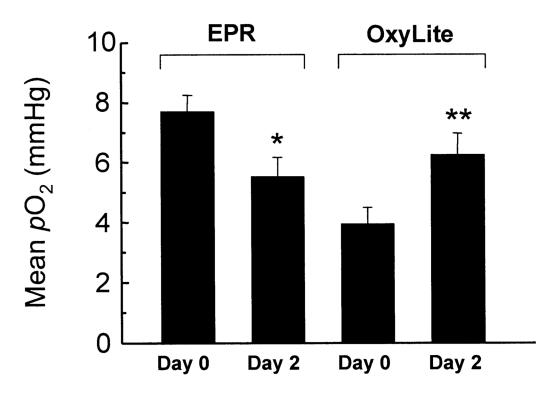
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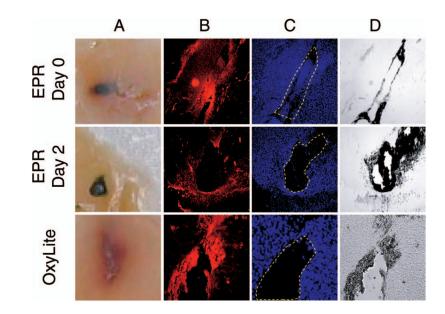
#### FIG 1.

EPR and OxyLite  $pO_2$  values in RIF-1 tumor. The plot shows the  $pO_2$  values obtained from random sites in the tumor using EPR and OxyLite oximetry. Two sets of data are shown: (1) measured immediately after implantation of EPR probe (day 0) and (2) measured 48 h after implantation of the EPR probe (day 2). The OxyLite measurements were made at multiple sites (up to four) and plotted as a function of a single EPR measurement obtained from the same tumor. The measurements were made on a total of 53 tumors. The data show significant scatter within the set as well as differences in the nature of scatter between sets.



### FIG 2.

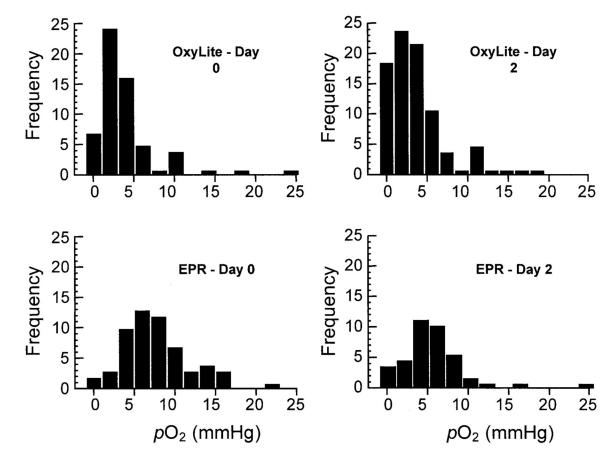
Mean ± SEM EPR and OxyLite readings. The number of values (N) and median of the groups shown in the plot are (Group: N, median): EPR/day 0: 58, 7.3 mmHg; EPR/day 2: 43, 5.0 mmHg; OxyLite/ day 0: 60, 2.8 mmHg; OxyLite/day 2: 105, 3.9 mmHg. \*Significantly different from EPR/day 0; \*\*significantly different from OxyLite/day 0.



#### FIG 3.

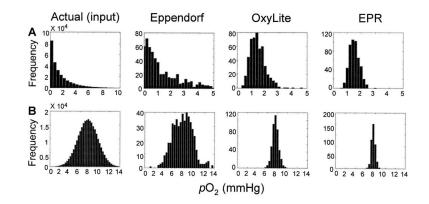
Effect of the probe implant on the tissue. Sections from RIF-1 tumor prepared after completion of  $pO_2$  measurements on the day of implantation (EPR day 0 and OxyLite) and 48 h after (EPR day 2) are shown. Panel A: Unstained visual image (macrophotography) showing the deposition of EPR and OxyLite probes; panel B: fluorescence image of smooth muscle ( $\alpha$ -actin) staining showing blood vessels; panel C: fluorescence image of DAPI staining showing nuclei; panel D: a bright-light image of panels B/C. The probe implants are recognized from the void space indicated by the dashed enclosure in panel C.

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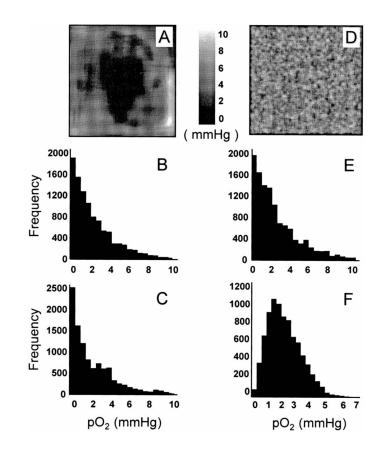
#### FIG 4.

Histogram of the  $pO_2$  data. The OxyLite data for day 0 and day 2 show a substantial population of lower  $pO_2$  values and considerable right-skewness. On the other hand, the EPR data show a normal distribution.



#### FIG 5.

Simulation of the differences in the distribution of  $pO_2$  data obtained from OxyLite, EPR, and Eppendorf microelectrode methods. The simulation assumed a  $512 \times 512$  matrix of  $pO_2$ values with a normal and right-skewed distribution and calculated the output ( $pO_2$  readings) as a function of probe size (Eppendorf microelectrode, OxyLite and EPR). The plots show the histogram of actual input (panel A: right-skewed; panel B: normal distribution) and corresponding outputs by Eppendorf, OxyLite and EPR methods. The mean, median and skewness values are given in Table 2. For methods with a larger probe size, the distribution tends to be normal. While a normal input distribution is preserved in the output irrespective of probe size, a skewed input distribution may tend to become a normal distribution if measured using a relatively large probe.



#### FIG 6.

Effect of  $pO_2$  heterogeneity and probe size on the shape of measured  $pO_2$  histograms. Tumors with (panel A) a smooth variation of  $pO_2$  with severely hypoxic contiguous region and (panel D) a randomly distributed  $pO_2$  were used as inputs. The corresponding histograms obtained using microelectrodes (panels B and E) and OxyLite (panels C and F) are shown. In the case of input A, the skewness increases with increasing probe size (panel B, microelectrode, skewness 1.28, compared to panel C, OxyLite, skewness 1.31). In the case of panel D, the skewness decreases with increasing probe size (panel E, microelectrode, skewness 1.26, compared to panel F, OxyLite, skewness 0.64).

# TABLE 1

# A Comparison of Important Features of EPR and OxyLite Oximetry

Feature	EPR	OxyLite
Operation/principle	Oxygen-induced changes in the EPR linewidth	Oxygen-induced changes in the fluorescence lifetime
Probe	Paramagnetic microcrystalline particulate (LiPc)	Fluorescent probe (solid ruthenium chloride)
Probe size	Large number of crystals 2–5 $\mu m$ wide and 10–60 $\mu m$ long	220-µm diameter
Oxygen consumption	None	None
Mode	Temporal (spatial possible under certain conditions)	Temporal (point measurement only)
Data acquisition	Seconds	Seconds, but requires several minutes stabilization
Range	0–760 mmHg or higher	0–100 mmHg
Accuracy	0.1 mmHg (LiPc)	0.7 mmHg up to 10 mmHg 10% above 10 mmHg
Sensitivity/drift	Sensitivity increases at low $pO_2$ No drift	Sensitivity increases at low $pO_2$ Drift increases at low $pO_2$
Response time to 90%	1 s	5 s
Effect of Temperature	Negligible	Yes
Repeatability	Repeatable for days/months from the same site of implantation	No

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Simulation Results Demonstrating the Effect of Probe Size on the  $pO_2$  Readout

	Sk	Skewed distribution		βN	Normal distribution	
Method of measurement Mean (mmHg) Median (mmHg) Skewness Mean (mmHg) Median (mmHg) Skewness	Mean (mmHg)	Median (mmHg)	Skewness	Mean (mmHg)	Median (mmHg)	Skewness
Actual (input)	1.50	0.91	2.31	7.59	7.59	0
Microelectrode	1.53	0.89	2.1	7.61	7.61	0.12
OxyLite	1.47	1.39	1.22	7.60	7.60	0.14
EPR	1.51	1.49	0.37	7.60	7.58	0.09