

X-ray microtomography using correlation of near-field speckles for material characterization

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Nondestructive microscale investigation of objects is an invaluable tool in life and materials sciences. Currently, such investigation is mainly performed with X-ray laboratory systems, which are based on absorption-contrast imaging and cannot access the information carried by the phase of the X-ray waves. The phase signal is, nevertheless, of great value in X-ray imaging as it is complementary to the absorption information and in general more sensitive to visualize features with small density differences. Synchrotron facilities, which deliver a beam of high brilliance and high coherence, provide the ideal condition to develop such advanced phase-sensitive methods, but their access is limited. Here we show how a small modification of a laboratory setup yields simultaneously quantitative and 3D absorption and phase images of the object. This single-shot method is based on correlation of X-ray near-field speckles and represents a significant broadening of the capabilities of laboratory-based X-ray tomography.

X-ray imaging | near-field speckles | phase-contrast imaging | refractive index measurement | microtomography

Near-field speckles are observed when the granular diffraction pattern created by a random phase modulator (diffuser) is recorded in the near-field regime. This speckle intensity pattern has interesting properties: it is not dependent on the propagation distance if the near-field condition is satisfied (1), near-field speckles can be observed also with beams of low longitudinal coherence, and the speckle pattern reflects the spatial properties of the scatterers used to generate it (2).

Although speckles are a well-known phenomenon especially in the far field and for different wavelengths, e.g., from radio waves to visible light, the first observation and characterization of near-field speckles with X-rays was achieved in 2008 by Cerbino et al. who reported on measurements performed with synchrotron radiation (1). After this first experiment, X-ray near-field speckles have been used at synchrotron facilities for, among other applications, coherence measurements, optics characterization, and imaging (3–5).

The principle of speckle-based imaging is to quantify the effect on the speckle pattern by the sample through a windowed correlation between a pair of images taken with and without sample. This correlation quantifies the distortion of the speckles caused by the sample and yields accurate information on its refraction and thus phase-shifting properties. Moreover, it simultaneously provides the complementary absorption image of the investigated object (4–6). Because near-field speckles exhibit sufficient contrast also when a beam with a low degree of temporal coherence is used, near-field speckle-based techniques are not limited to large-scale synchrotron facilities, but can also be implemented with polychromatic laboratory X-ray sources. Such an experiment has been demonstrated using a high-brightness liquid-metal-jet source (7) making this imaging method available for widespread use (6).

Up until now, near-field speckle-based X-ray imaging has been performed only in projection mode (2D imaging). No extension to 3D imaging (tomography) has been reported up to now,

neither with synchrotron nor with laboratory-based source data. Although simple and fast at detecting inner structures in the sample, projection imaging does not provide the location of features within the volume, nor the spatially dependent complex-valued refractive index $[n(x, y, z) = 1 - \delta(x, y, z) + i\beta(x, y, z)]$ of the object. To access this quantitative 3D information, one has to acquire a tomographic volume, obtained by combining the projections taken at different viewing angles of the sample. With speckle-tracking tomography, two inherently registered volumes that carry complementary information are obtained simultaneously from the same dataset: (i) the spatial distribution of the decrement of the refractive index δ from the phase projections and (ii) the spatial distribution of the linear attenuation coefficient μ (which is proportional to the imaginary part of the refractive index β according to $\mu = 4\pi\beta/\lambda$) from the absorption projections. Thus, the full refractive index (at X-ray wavelength) of the entire object can be accessed with a single measurement.

We demonstrate the potential of near-field speckle-based tomography and the importance of the phase information to complement the conventional absorption signal on a phantom sample made of known low-absorbing materials with similar refractive indices. As represented in Fig. 1, the X-ray generator was a liquid-metal-jet source, and the diffuser, a piece of sandpaper, was located between the source and the sample. More details on the setup and experimental parameters are reported in *Methods*.

The near-field speckle pattern obtained using this arrangement is shown in Fig. 2. The image of the sample superimposed on the speckle pattern is shown in panel a. The sample was a polypropylene (PP) cylinder filled with water containing three plastic spheres with a diameter of 1.5 cm: two spheres of polymethylmethacrylate (PMMA) and one sphere of polytetrafluoroethylene

Significance

We present X-ray speckle tracking tomography, a simple, robust, and versatile method to obtain simultaneously phase and absorption tomograms of the sample at the micrometer scale with a laboratory X-ray source. The method is based on correlation of near-field speckles and yields quantitative measurements of the full X-ray refractive index of the object with high sensitivity. X-ray speckle tracking tomography broadens the capabilities of X-ray imaging at laboratory sources with strong potential in materials and life sciences.

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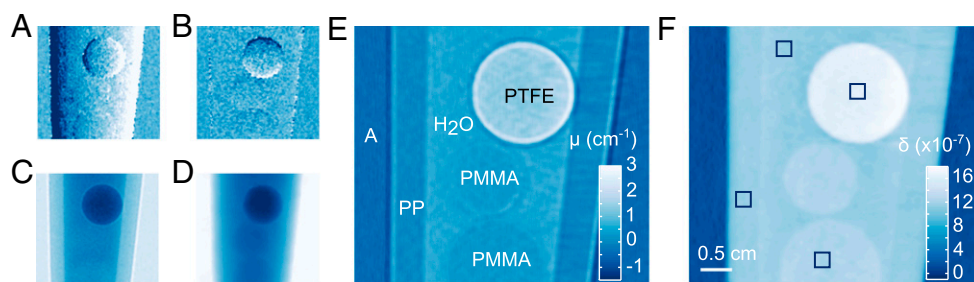


Fig. 3. Projections and sagittal slices of the phantom sample measured with speckle-based X-ray tomography. Refraction angle projections in the horizontal (A) and vertical (B) direction of the phantom sample. The intensity window in these images is from -3 to $3 \mu\text{rad}$. The absorption image, which also exhibits edge enhancement, is shown in C with an intensity window from 0.4 to 1.1 , and the integrated phase map is shown in D. The maximum phase shift measured in this projection is ~ 300 rad for the region occupied by the PTFE sphere at the top of the image. E and F show an example of a sagittal slice through the absorption and phase volumes respectively. The measured values of δ and μ are indicated in the color bars in the figures. In E, the materials forming the phantom are given: air (A), different polymers (PMMA, PP, and PTFE), and water (H₂O). The squares in F surround the regions of interest used for the calculation of refractive indices and CNRs (Table 1).

pixels centered in the different materials compared with a ROI in water of the same size according to the formula:

$$\text{CNR}_m = |\bar{S}_m - \bar{S}_w| / \sqrt{\sigma_m^2 + \sigma_w^2}, \quad [1]$$

where the subscript m indicates the chosen material (PMMA, PP, or PTFE) and w indicates the water used as reference. The CNRs have been calculated in this way for both phase and absorption signals.

In Fig. 3E, the edge-enhancement signal already observed in the absorption projection data remains visible also in the tomographic reconstruction and highlights the boundary between the PMMA and the surrounding water, which has similar attenuation coefficient. The values of the refractive indices of the materials of the phantom calculated in the ROIs indicated in Fig. 3F are reported in Table 1. By comparison with the values reported in literature (9), our measured refractive indices vary in the interval 14.5 keV for PP (external layer) to 20.5 keV for PTFE (inner structure). These values are consistent with the average energies calculated from the detected energy spectra when considering the effect of “beam hardening” (SI Text).

The quantitative analysis of the volume is completed using the 2D (μ vs. δ) histogram calculated from all voxels in the volumes. The 2D histogram, shown in Fig. 4A, is compared with the histogram plots of the two volumes separately (right and top of the 2D histogram). Although some peaks in the 1D histograms coincide, all of the materials composing the phantom form distinct peaks in the 2D histogram (labels in Fig. 4A).

This analysis demonstrates that the distinction and quantification of all materials in the sample volume is made possible through a combination of the absorption and phase information.

Table 1. Refractive indices and CNRs of the materials in the sample

Material	μ (cm^{-1})	δ ($\times 10^{-6}$)	CNR of μ	CNR of δ
PMMA	0.77 ± 0.06	1.13 ± 0.02	2.6	3.5
PP	0.46 ± 0.07	1.05 ± 0.01	5.6	0.1
PTFE	1.84 ± 0.11	1.53 ± 0.02	6.5	18.9
H ₂ O	1.01 ± 0.07	1.05 ± 0.02	—	—

The table reports the measured values of δ and μ of the materials in the sample with the corresponding uncertainties. A comparison with the tabulated values of the refractive indices for these materials is discussed in the SI Text. The phase and attenuation CNRs of the materials composing the specimen compared with water clearly illustrates the complementarity of the two image signals. The values in this table are extracted from the ROIs in Fig. 3F.

The 3D rendering shown in Fig. 4B was produced with a segmentation based on the 2D phase-absorption histogram.

Speckle-based multicontrast X-ray tomography is a simple, fast, and sensitive method to precisely measure the distribution of the full refractive index within the sample, in three dimensions and at the micrometer scale, with a resolution ultimately limited by the speckle size in the pattern used a reference. For a fixed experimental geometry, the speckle size on the observation plane depends only on the size of the diffuser structures. Thus, speckle-based imaging has the potential to be implemented with detectors of different pixel sizes.

To increase the spatial resolution, more sophisticated methods such as speckle scanning can be used (10). This method, however, introduces complexity in the setup and significantly increases the acquisition time. Improvements in the algorithm used to track the speckles, for example, by modeling speckle distortions and the decrease in visibility, might also be beneficial to increase image contrast and spatial resolution.

Compared with grating-based methods (11–17), some of which have been recently implemented in rapid single-shot modality, speckle-based imaging does not require a series of sophisticated and strongly absorbing optical elements. Moreover, it inherently provides the 2D differential phase information, and the use of the random diffuser does not impose limitations on the geometry or energy of the experiment.

Propagation-based methods, on the other hand, are very flexible and provide high-resolution data using only the effect of X-ray propagation from sample to detector (18), but with these methods, the phase can be quantitatively separated from the absorption signal only in very special cases (8, 19).

Because of its simplicity and potential, we believe that X-ray imaging based on near-field speckle correlation as presented here has important applications in such diverse fields as materials science and biomedicine.

Methods

Setup and Experimental Parameters. The liquid-metal-jet source was operated at a voltage of 50 kVp and a power of 30 W with a liquid anode formed of Ga, In, and Sn. The size of the source was $s = 6.0$ (h) $\times 7.9$ (v) μm^2 . The static diffuser, a piece of sandpaper with grains of size of $\sim 22 \mu\text{m}$, was placed at $d_d = 1.2$ m from the source and upstream from the sample. The latter sat on a translation stage, for collection of reference beam images, and on a rotation stage used for tomography. The sample was positioned at $d_s = 1.5$ m from the source.

The detector, located at $d_{\text{tot}} = 2.8$ m from the source, was a CCD camera with an effective pixel size of $p_s = 9 \mu\text{m}$ coupled through an optic plate to a $15\text{-}\mu\text{m}$ -thick $5\text{-mg}/\text{cm}^2$ Gadox (gadolinium oxysulfide) scintillator. The measured point spread function of the detector had a full width at half maximum of $25 \mu\text{m}$.

With this geometry, the magnification of the near-field speckles was $M_{\text{speckles}} = d_{\text{tot}}/d_d = 2.3$, and the magnification of the image of the sample was $M_{\text{sample}} = d_{\text{tot}}/d_s = 1.9$. Thus, the pixel size at the sample plane was $4.7 \mu\text{m}$.

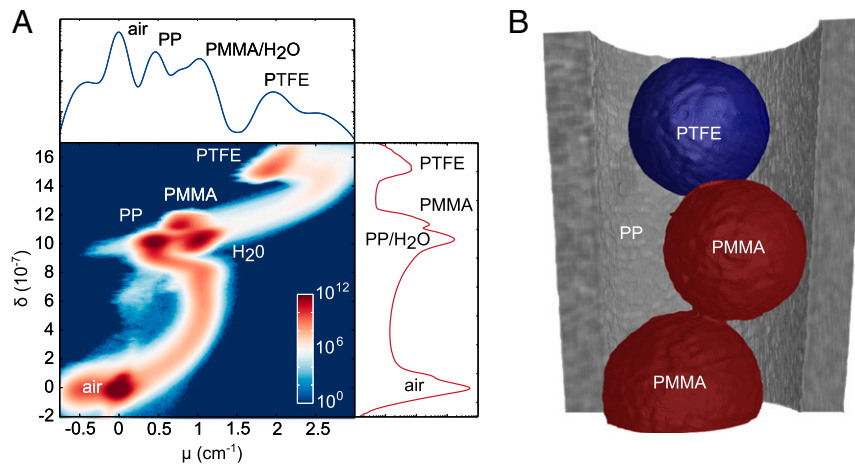


Fig. 4. Quantitative analysis of the sample using absorption and phase signals. (A) 2D histogram (δ vs. μ) of the entire volume, complemented by one-dimensional phase (Right) and absorption (Top) histograms generated by projecting the 2D histogram on the two orthogonal axes. The colors in the 2D histogram indicate, in logarithmic scale, the number of voxels with given values of (δ , μ) in the reconstructed volumes. The peaks are labeled with the name of the corresponding material. (B) 3D false-color rendering of the volume with segmentation based on the 2D histogram of A. The diameter of the spheres is 1.5 cm. For better visualization water is made transparent and only half of the container is rendered.

During the tomography scan, 200 projections were collected over 180° , with 0.9° of angular spacing. The acquisition time per frame was 2 min. Two reference (flat field) images without sample in the beam but with the same exposure time were collected every 10 projections to correct for beam instabilities. A series of five dark images (without beam) were recorded, and their median was used to correct the raw data for the dark current of the detector.

Processing and Reconstruction. First, all images have been corrected for diffuser drift using an area in the background as reference. For the processing of each sample image of the tomographic scan, the pair of reference images recorded closest in time has been averaged to be used as reference pattern. The algorithm used to obtain refraction angle and absorption data are based on cross-correlation with subpixel precision using the model described in detail by Zanette et al. (6). The window size used for these data is 30×30 pixels. The resulting refraction angle images have been combined together with a regularized integration routine that uses the residual error of the correlation algorithm to obtain the quantitative phase map (6). The phase and absorption volumes have been calculated by applying the filtered-back projection algorithm (20) to the series of phase and absorption images, respectively. The same Ram-Lak filter has been used for both signals.

As the filtered back-projection algorithm reconstructs the phase volume in the form of a stack of slices orthogonal to the rotation axis, the refraction angle projections along x could be used alone to reconstruct the quantitative phase tomogram. This approach, combined with integration in Fourier space incorporated in the filter of the back-projection algorithm, is commonly used in other phase-contrast imaging techniques such as X-ray grating interferometry (21). In the proposed speckle-tracking method, the availability of the refraction angle signal in the orthogonal y direction allows significant reduction of artifacts generated from noise in the projection data, as illustrated in *SI Text*.

Calibration of Refractive Index Values and Calculation of Contrast-to-Noise Ratios. The quantity measured at the position (x, y) in the absorption projections is described, in absence of edge enhancement, by the integral of the linear attenuation coefficient

$$I(x, y) = I_0(x, y) \exp \left[- \int \mu(x, y, z) dz \right], \quad [2]$$

where I_0 is the intensity distribution impinging on the sample, and z is the direction of propagation of the X-ray beam. Thus, the tomographic reconstruction of the logarithm of the normalized absorption data, $-\ln[I(x, y)/I_0(x, y)]$, yields the 3D distribution of μ within the specimen.

The phase shift Φ obtained in the integrated phase map is related to the real part of the refractive index δ as

$$\Phi(x, y) = \frac{2\pi}{\lambda} \int \delta(x, y, z) dz, \quad [3]$$

where λ is the wavelength of the radiation. The tomographic reconstruction from phase projections directly yields the volume data for δ . The phase Φ is obtained as integration of the two refraction angle projections α_x and α_y (6). The signal in the refraction angle data are related to the geometry of the experiment and measured speckle displacements d_x and d_y as

$$\alpha_x = \frac{\lambda}{2\pi} \frac{\partial \Phi(x, y)}{\partial x} = \frac{d_x(x, y) \times p_s}{d_{\text{tot}} - d_s}, \quad [4]$$

and analogously for y . The calibration of δ and μ has been performed, for both volumes, using the air region surrounding the specimen.

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