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Arterial Stiffness and the Kidney

Clinical Considerations for the Association between Vascular Damage and Chronic Kidney Disease

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Key Words

Chronic kidney disease · Cardiovascular disease · Vascular damage · Intima-media thickness · Coronary artery calcium score

Abstract

Chronic kidney disease (CKD) is an independent risk factor for cardiovascular disease. Recently, noninvasive and simple morphological and functional methods have been introduced to assess atherosclerotic vascular damage. This review describes the association of CKD with vascular damage as assessed by these methods. Carotid intima-media thickness (IMT) and coronary artery calcium score (CACS) are morphological parameters of vascular damage, and an ankle-brachial index (ABI) <0.90 suggests the presence of peripheral arterial disease (i.e., it represents advanced atherosclerosis). Several prospective studies have demonstrated that CKD is a risk factor for an increased IMT, an increased CACS and a decreased ABI. While it has not been clarified whether measuring the IMT or CACS might be useful to predict the progression of renal function decline, a reduced ABI has been demonstrated as a predictor of accelerated renal function decline. On the other hand, pulse wave velocity (PWV) is a marker of arterial stiffness rather than atherosclerosis, reflecting functional abnormalities caused by vascular damage, and moderate-to-severe CKD may be a risk factor for the progression of arterial stiffness. The measurement of functional markers, especially of PWV or pulse pressure, has been demonstrated to be useful to predict the rate of progression of renal function decline. Thus, renal dysfunction and atherogenic states may be components of a vicious cycle, and vascular function abnormalities associated with atherosclerosis may accelerate this cycle. As the next step, we propose to examine whether improvement of vascular function abnormalities can interrupt this vicious cycle.
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Introduction

 In addition to conventional risk factors for cardiovascular (CV) disease, chronic kidney disease (CKD) is also an independent risk factor [1, 2] . Combined disorders of the heart and kidney are common and have been referred to as the cardiorenal syndrome [3, 4] . Atherosclerotic vascular disorder is one of the common pathways for heart failure and kidney disease [3, 4] . Clinically, atherosclerotic vascular damage is assessed by morphological and functional approaches. Those parameters of atherosclerotic vascular damage are used as predictors of future CV events [5], and they are a rather useful tool for the prevention and management of CV disease. On the other hand, the usefulness of the parameters of vascular damage for the management of renal dysfunction has not yet been fully clarified.

 This review summarizes the methodologies used for the morphological and functional assessment of vascular damage in clinical settings and describes the pathophysiological basis for the association between vascular damage and renal dysfunction.

Methodologies to Assess Vascular Damage

Morphological Assessments

Carotid Ultrasound

 Carotid intima-media thickness (IMT) is measured by B-mode ultrasound, in which the distance from the intimal to the adventitial layer is measured as the width of the typical double line of the arterial wall. Usually, IMT is measured in the common carotid artery [6] . IMT increases with the progression of atherosclerosis, and in cases with advanced atherosclerosis, atherosclerotic plaques can be detected by carotid ultrasonography (fig. 1). Assessing IMT, an increase of which is an independent risk factor for future CV events, has been demonstrated to show acceptable reproducibility [6, 7] . While the methodological consensus for standardization has been obtained and reference values have been reported [8] , experienced sonographers are required for the measurement [6, 7].

Coronary Artery Calcium Score

 Calcification of coronary arteries is strictly associated with the process of atherosclerotic plaque formation; therefore, the presence of calcific deposits in the coronary arteries is considered to be pathognomonic of coronary atherosclerosis. Electron beam or multislice computed tomography is used to measure the coronary artery calcium score (CACS). Using images of 3-mm slice thickness, CACS is calculated as the area of calcification per coronary segment. CACS is commonly classified into four categories: 0, 1–99, 100–399, and \geq 400 [9]. Recently, the Multi-Ethnic Study of Atherosclerosis (MESA) has reported that CACS allows a superior discrimination and risk reclassification as compared to other risk markers [10].

Functional Assessments

Endothelial Function

Flow-Mediated Vasodilatation. Flow-mediated vasodilatation (FMD) is calculated as the percent change of the diameter of the brachial artery (i.e., the diameter before reactive hyperemia vs. the maximum dilatation induced by reactive hyperemia) [5, 11]. Usually, reactive hyperemia is induced by compression of the forearm by inflation of a pressure cuff to 200–250 mm Hg for 5 min. The limitation of this method is that it is operator-dependent, although recently, semiautomated devices have been introduced to overcome this disadvantage (fig. 2).

Fig. 1. Carotid ultrasound images with the progression of carotid atherosclerosis.

Fig. 2. Results of FMD measurement under normal and disease (impaired) conditions.

Fig. 3. Description of RH-PAT.

Reactive Hyperemia Index Measured by Peripheral Arterial Tonometry. The reactive hyperemia index measured by peripheral arterial tonometry (RH-PAT) is based on the noninvasive measurement of changes in the pulsatile volume at the fingertip (before and after reactive hyperemia) by PAT (fig. 3) [11]. The procedure for inducing reactive hyperemia is the same as that used for the measurement of FMD. PAT probes are placed on the index finger of each arm, and the post- to preocclusion ratio is calculated. The RH-PAT signals are corrected for the signals in the contralateral arm. FMD reflects endothelial function in the conduit arteries, while RH-PAT reflects endothelial function in the peripheral resistance arteries, and the two parameters have not been demonstrated to show a close association with each other [5, 11] . However, while the two parameters may not be interchangeable markers, several prospective studies have demonstrated that they are independently useful for predicting future CV events [5, 7, 11] . Measurements of both show acceptable reproducibility, although that of FMD is more operator-dependent. At present, some methodological differences exist in the measurement of FMD among institutions (e.g., in the placement of the pressure cuff above vs. below the elbow, duration of cuff occlusion, method used to determine the vascular diameter, and definition of maximal dilatation of the brachial artery), and there are no reference values. On the other hand, RH-PAT is measured by a uniform method, although reference values have not been established for this parameter either.

Pulse Wave Velocity

 Pulse wave velocity (PWV) reflects segmental arterial elasticity [5, 7] . Contraction of the left ventricle generates a pulse wave, which is propagated throughout the arterial tree. PWV

is calculated as the distance traveled by the pulse wave divided by the time taken by the wave to travel the distance: PWV = $\Delta L/\Delta T$, where ΔL m is the distance between the two sites of pulse wave recording (in meters) and ΔT is the time delay in the appearance of the pulse wave from the proximal to the distal site of the recording (in seconds). The Moens–Korteweg equation states that the PWV is proportional to the square root of the incremental elastic modulus of the vessel wall, given a constant ratio of the wall thickness to the vessel radius and blood density. Therefore, increased arterial rigidity and arterial wall thickness act to increase the PWV. PWV can be measured in any arterial segment between two pulse-wave palpable regions.

Carotid-Femoral PWV. Carotid-femoral PWV (cfPWV) is the most commonly used noninvasive method for determining the PWV and is considered the gold standard [5, 10, 12] . Usually, it is measured using the 'foot-to-foot' velocity method [10, 12] and recorded transcutaneously at the right common carotid artery and right femoral artery, and the time delay is measured between the feet of the two waveforms. While several methodological differences existed in the measurement of the cfPWV (e.g., in the method used to determine the foot of a waveform or in the calculation of the path length), now, a standardized method has been established [13].

Brachial-Ankle PWV. Brachial-ankle PWV (baPWV) is measured using a volume-plethysmographic apparatus. Since baPWV only involves wrapping a pressure cuff around the four limbs for its measurement, it is easier to measure than cfPWV, and the measurement is also well-standardized. The brachial and posterior tibial arterial pressure waveforms are recorded by a plethysmographic sensor. baPWV reflects the stiffness of the large- to middle-sized arteries [5, 12] . The method has been primarily used in Asian populations. In the measurement of baPWV, the ankle-brachial pressure index (ABI) is simultaneously obtained, and when the ABI is <0.95, the accuracy of baPWV is diminished [14] . Meta-analyses have already confirmed that not only an increased cfPWV, but also an increased baPWV, is an independent risk factor for CV events and that there is a significant positive relation between the baPWV and cfPWV $(r = 0.73)$ [15]. The standard value of cfPWV is 10 m/s and that of baPWV is 18 m/s [5, 11].

Wave Reflections/Central Hemodynamics

 Cardiac contraction generates a pressure pulse wave, which propagates from the heart to the periphery [5, 9, 16] . On the other hand, in the arterial tree, the arteries branch and taper as they reach the periphery, which is associated with an increase in the arterial resistance. A reflected pressure pulse wave (from the periphery towards the heart) occurs at sites of abrupt increase of arterial resistance. Then, an interaction between the forward and reflected pressure pulse waves occurs in the arterial tree. Under physiological conditions, this interaction is observed at a distal site of the arterial tree; therefore, blood pressure is lower at the level of the kidney than at the level of the brachial artery. Under the condition of increased arterial stiffness, on the other hand, the travelling speed of the pressure pulse wave is increased and the interaction between the forward and reflected pulse wave is observed at a more proximal site of the arterial tree (i.e., the aorta). Pressure wave analysis is conducted at the carotid, radial or brachial artery. Since the radial bone is backboned, the radial arterial pressure wave can be easily recorded. Therefore, recently, radial pressure wave analysis has become a common approach. The AtCor and the OMRON devices are popularly used for radial pressure wave analysis (fig. 4) [5, 12, 16]. The AtCor device estimates the central systolic blood pressure derived by the general transfer function of the radial pressure wave, and the OMRON device estimates the central systolic blood pressure derived by the regression equation from the directly measured late systolic shoulder of the radial pressure waveform. Estimation of the central systolic blood pressure based on the late systolic shoulder of the radial pressure wave provides comparable accuracy to that of the validated general transfer

Fig. 4. Devices used for radial pressure waveform analysis.

function [17] . However, standard values of pressure wave analyses/central hemodynamics have not yet been clearly established, and an international project to determine the reference values of the central hemodynamic indices is ongoing.

Ankle-Brachial Index

 Normally, systolic blood pressure is higher in the lower extremities than in the arms. The ABI is the ratio of the ankle-to-brachial systolic pressure. The standard mode of measurement requires a (hand-held) continuous-wave Doppler device and a manual blood pressure cuff [18] . This method allows measuring the systolic blood pressures of the posterior tibial and dorsalis pedis arteries. Recently, an oscillometric device has become available to measure the ABI [5, 19]. This method is easier as compared to the method using the Doppler device because the former only involves wrapping of a pressure cuff around the four limbs. The ABI measured by the oscillometric method has an acceptable accuracy (fig. 5) [19]. An ABI <0.90 reflects the presence of peripheral arterial disease. The sensitivity and specificity of an ABI <0.90 for >50% stenosis in the lower limb arteries are 90 and 95% [20] , respectively. The meta-analysis demonstrated that not only an ABI <0.90, but also an ABI >1.40 is an independent risk factor for future CV events [21].

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Vascular Damage and Renal Dysfunction

 Effect of CKD on the Progression of Vascular Damage as Assessed from the Morphological and Functional Aspects

 Recent meta-analyses have confirmed that CKD is an independent risk factor for clinical outcomes such as mortality and dialysis/kidney transplantation [1, 2] . Anemia, sympathetic nerve activation, oxidative stress/inflammation, endothelial dysfunction, coagulation disorders, abnormal mineral metabolisms, and/or uremic toxins are thought to be additional risk factors for atherosclerotic vascular damage in patients with CKD [22] .

IMT and CACS

Carotid IMT has been reported to be increased even in subjects with early-stage CKD [23], and this association is especially pronounced in subjects with hypertension [24]. Desbien et al. [25] conducted a 2-year prospective study to examine the association between CKD of different severities and the carotid IMT in a community cohort ($n = 3,364$) and demonstrated that decreased renal function was associated with accelerated increase of the IMT. Furthermore, Yilmaz et al. [26] reported that kidney transplantation was associated with a decrease of the IMT within 90 days of the transplantation, and this decrease was associated with the improvement of the glomerular filtration rate (GFR). Thus, even early-stage CKD may affect the rate of increase of the carotid IMT. CACS can be assessed by electron-beam or multislice computed tomography. The Chronic Renal Insufficiency Cohort (CRIC) study [27] reported the existence of a significant relationship between the estimated GFR (eGFR) and CACS: the lower the eGFR, the higher the CACS. Among prospective studies, the MESA ($n =$ 2,795) demonstrated that the incidence of coronary artery calcification (CACS >0) was higher in subjects with eGFR values of 30–59 ml/min/1.73 m² (27%) than in those with eGFR values of >90 ml/min/1.73 m² (12%) during a 2.4-year follow-up period [28]. The Spokane Heart Study (n = 883) also reported similar findings over a 6-year follow-up period [29].

Endothelial Function

 Endothelial dysfunction is an early-stage abnormality in atherosclerotic vascular damage [5, 10], and several cross-sectional studies have demonstrated the existence of endothelial dysfunction in patients with CKD. Yilmaz et al. [30] reported that endothelial dysfunction was observed even in cases with early-stage CKD; however, Lilitkarntakul et al. [31] reported that endothelial dysfunction was significant only in subjects with stage 5 CKD. Hypertension and diabetes mellitus, both of which can cause endothelial dysfunction, are common disorders in CKD, and they might be confounding factors when evaluating the association of CKD with endothelial dysfunction [32] . Thus, a further prospective study is proposed to examine whether early-stage CKD might be a risk factor for the progression of endothelial dysfunction.

PWV and Wave Reflection/Central Hemodynamics

 Several cross-sectional studies have reported the existence of a significant association between accelerated GFR decline and increased arterial stiffness [33, 34] . Previously, however, we reported, based on a 5.6-year follow-up study ($n = 2,053$), that early CKD was not a risk factor for arterial stiffening as assessed by the baPWV [35] . Tholen et al. [36] reported that loss of renal function had no significant impact on the increase of cfPWV during a 1-year follow-up period in subjects with mild CKD ($n = 70$, mean eGFR 52 ml/min/1.73 m²). On the other hand, Benetos et al. [37] demonstrated that high serum creatinine (>1.0 mg/dl) was associated with an accelerated increase of cfPWV over a 6-year observation period in subjects with treated hypertension ($n = 483$). Furthermore, in subjects under maintenance hemodialysis, Utescu et al. [38] suggested that CKD-related risk factors such as advanced glycation end products may contribute to the accelerated worsening of the cfPWV. Therefore, moderateto-severe CKD may affect the progression of arterial stiffening.

Ankle-Brachial Index

 ABI <0.90 is a risk factor for CV disease and reflects peripheral arterial disease, and ABI >1.40, which is partially related to medial layer calcification, is also a risk factor for CV disease [7, 18] . In the cross-sectional Cardiovascular Health Study (CHS), Ix et al. [39] reported that CKD was associated with both high and low ABI values. Recently, Garimella et al. [40] have

demonstrated in a 9.8-year follow-up study of MESA ($n = 6.814$) that albuminuria is a risk factor for both high and low ABI values and that elevated serum cystatin C is a risk factor for low ABI values.

 In summary, CKD may affect the rate of progression of morphological vascular damage, as assessed by IMT or CACS, even in the early stages, and also serves as an atherogenic factor in the advanced stage of atherosclerosis. However, the effect of CKD on the rate of progression of functional vascular damage, such as arterial stiffening, may be significant in cases with moderate-to-severe CKD.

 Can Morphological and Functional Assessments of Vascular Damage be Useful to Predict the Progression of Renal Function Decline? IMT and CACS

The MESA ($n = 4,878$) reported that increased carotid IMT is a risk factor for the progression of albuminuria [41] . To the best of our knowledge, however, no study has been conducted to examine whether increased IMT and/or a high CACS might be a risk factor for accelerated GFR decline.

Endothelial Function

 For the assessment of endothelial function, FMD and RH-PAT are available in clinical settings. The former assesses endothelial function in the brachial artery, a conduit artery, and the latter assesses endothelial function in the peripheral resistance arteries of the forearm [5, 10] . They are thought to reflect different facets of pathophysiological abnormalities in the endothelium. While the risk factors for CV disease are also risk factors for renal dysfunction [22] , controversial results have been reported concerning the significance of the association between endothelial and renal dysfunction. Perticone et al. [42] reported that endothelial dysfunction, as assessed by strain-gauge plethysmography during intra-arterial infusion of acetylcholine, which reflects the endothelial nitric oxide bioavailability in peripheral resistance arteries, was a risk factor for the accelerated renal function decline during at least a 2-year follow-up period in subjects with treated hypertension. On the other hand, in the MESA, Peralta et al. [43] reported that decreased FMD, which reflects the nitric oxid bioavailability in conduit arteries, was not a risk factor for accelerated renal function decline during a 4.8-year follow-up period. Lerman and Zeiher [44] described that endothelial dysfunction was a predictor of CV events, which may occur remotely from the site at which the endothelial dysfunction was initially detected. Further study is needed to clarify whether endothelial dysfunction in the peripheral resistance arteries, rather than in the conduit arteries, might be a better predictor of accelerated renal function decline.

PWV and Wave Reflections/Central Hemodynamics

 Differing from other parameters of vascular damage, arterial stiffness is thought to serve as a risk factor for accelerated renal function decline, independent of the conventional risk factors for CV disease, via abnormal central hemodynamics and/or pulsatile nephropathy [5, 12, 16] . Elevated blood pressure is a risk factor for accelerated renal function decline, and conventionally, blood pressure is determined in the brachial artery. As mentioned above, the arterial tree has a blood pressure gradient, and under physiological conditions, the blood pressure is lower at more central sites than at distal sites [5, 12, 16] . When the arterial stiffness increases, the travelling speeds of both the forward and the reflected pressure wave in the arterial tree are increased, and interaction between the two pressure waves is observed at a more proximal site in the arterial tree. This results in a decrease of the pressure gradient in the arterial tree. For the same blood pressure measured in the brachial artery, the blood pressure at the level of the kidney is higher in cases with increased arterial stiffness than in

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 brPP = Brachial pulse pressure; eGFRcr = estimated glomerular filtration rate from the serum creatinine; eGFRcys = estimated glomerular filtration rate pressure obtained from the second peak of the radial pressure waveform; AI = augmentation index; cPP = central pulse pressure.

those without increased arterial stiffness, and the renal function may decline more rapidly in the former cases [5, 12, 16] . Conventionally, blood pressure is measured in mm Hg, and the specific gravity of mercury is 13. Therefore, a blood pressure of 140 mm Hg would correspond to the energy that can push up water up to a height of 180 cm. Thus, the heart generates

a large amount of energy during in every cardiac contraction, which is mostly absorbed in the aorta by its shock absorber effect. However, increased aortic stiffness attenuates this cushioning effect and increases the transmission of the pulsatile energy generated in the heart to the peripheral microcirculation. These phenomena cause the condition referred to as pulsatile nephropathy that results in accelerated renal function decline [5, 12, 16, 45] . Based on these logical backgrounds, several prospective studies have been conducted to examine whether increased arterial stiffness might be a risk factor for accelerated renal function decline [35, 46–53] . The results of these studies are summarized in table 1 . Most studies demonstrated that parameters related to arterial stiffness and/or wave reflection/central hemodynamics are useful to predict the rate of renal function decline.

Ankle-Brachial Index

 The Atherosclerosis Risk in Communities (ARIC) study [54] and the Framingham study [55] demonstrated that a low ABI represents a risk factor for accelerated renal function decline. Foster et al. [55] describe two plausible mechanisms for this association: (1) subjects with a low ABI may have subclinical vascular damage in the renal arterial bed, which cannot be detected by GFR and/or microalbiminuria, and (2) they might also have the shared risk factors or preexisting systemic disease that could lead to both peripheral vascular damage and decreased renal function.

 In summary, both vascular morphological and functional abnormalities are risk factors for the progression of renal dysfunction. Arterial stiffness/central hemodynamics are thought to serve as a risk factor for accelerated renal function decline, independent of the conventional risk factors for CV disease.

Conclusion

 A vicious cycle may exist between renal dysfunction and atherogenic states even from their early stages. Vascular function abnormalities associated with atherosclerosis may accelerate this cycle. Not only renal but also vascular assessment, especially measurements of arterial stiffness markers and/or wave reflection/central hemodynamics, is needed to evaluate the progression of this vicious cycle. As the next step, we propose to examine whether improvement of vascular function abnormalities, especially arterial destiffening, can interrupt this vicious cycle.

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