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# **Calcium regulation of HCN channels supports persistent activity in a multiscale model of neocortex**

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# **Abstract**

Neuronal persistent activity has been primarily assessed in terms of electrical mechanisms, without attention to the complex array of molecular events that also control cell excitability. We developed a multiscale neocortical model proceeding from the molecular to the network level to assess the contributions of calcium regulation of hyperpolarization-activated cyclic nucleotidegated (HCN) channels in providing additional and complementary support of continuing activation in the network. The network contained 776 compartmental neurons arranged in the cortical layers, connected using synapses containing AMPA/NMDA/GABA<sub>A</sub>/GABA<sub>B</sub> receptors. Metabotropic glutamate receptors (mGluR) produced inositol triphosphate (IP<sub>3</sub>) which caused release of  $Ca^{2+}$ from endoplasmic reticulum (ER) stores, with reuptake by sarco/ER  $Ca^{2+}$ -ATP-ase pumps (SERCA), and influence on HCN channels. Stimulus-induced depolarization led to  $Ca^{2+}$  influx via NMDA and voltage-gated  $Ca^{2+}$  channels (VGCCs). After a delay, mGluR activation led to ER  $Ca^{2+}$  release via IP<sub>3</sub> receptors. These factors increased HCN channel conductance and produced

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firing lasting for  $\sim$  1 minute. The model displayed inter-scale synergies among synaptic weights, excitation/inhibition balance, firing rates, membrane depolarization, calcium levels, regulation of HCN channels, and induction of persistent activity. The interaction between inhibition and  $Ca^{2+}$  at the HCN channel nexus determined a limited range of inhibition strengths for which intracellular  $Ca<sup>2+</sup>$  could prepare population-specific persistent activity. Interactions between metabotropic and ionotropic inputs to the neuron demonstrated how multiple pathways could contribute in a complementary manner to persistent activity. Such redundancy and complementarity via multiple pathways is a critical feature of biological systems. Mediation of activation at different time scales, and through different pathways, would be expected to protect against disruption, in this case providing stability for persistent activity.

## **Keywords**

hyperpolarization-activated cyclic nucleotide-gated (HCN) channel; *I*h; persistent activity; neocortex; computer simulation; multiscale modeling

# **1 Introduction**

Computational models of functional neural activity patterns in neuronal networks have traditionally focused primarily on the role of electrical activity in shaping these patterns, neglecting the rich chemical complexity that complements electrical signaling in neurons. Persistent neuronal activity, lasting several seconds, has been proposed to underlie several functions in the central nervous system including short term working memory (Goldman-Rakic, 1995, Braver et al., 1997, Kane and Engle, 2002) and motor preparatory set (Ames et al., 2014). Additional functions probably also depend on similar mechanisms subserved by the "UP state," identified originally in sleep and in slice but now also demonstrated in visual cortex (Cossart et al., 2003) and other brain areas (Oikonomou et al., 2014, Zhou et al., 2015, Poskanzer and Yuste, 2011, Major and Tank, 2004). Computational models of network persistent activity that have been proposed largely rely on continued interactions of neurons maintaining activity in one another through mutual synaptic activation (Lim and Goldman, 2013, Lim and Goldman, 2014, Lisman et al., 1998, Wang, 1999a, Wang, 2001).

A separate class of studies have focused on modulation of the single neuron via chemical signaling sequences (Ramakrishnan and Bhalla, 2008, Fall et al., 2005, Fall and Rinzel, 2006, Tiganj et al., 2015, Egorov et al., 2002, Fransén et al., 2006, Loewenstein and Sompolinsky, 2003, Sidiropoulou and Poirazi, 2012, Ashhad et al., 2015, Honnuraiah and Narayanan, 2013). Many of these have demonstrated that calcium signaling pathways underlie a large repertoire of cell dynamics that complements electrical signaling – interactions of chemophysiology and electrophysiology. Calcium pathways can enable persistent activity at the single cell level through effects on hyperpolarization-activated cyclic nucleotide-gated (HCN) channels (*I*h) (Winograd et al., 2008, Destexhe et al., 1996). This molecular/cellular mechanism has also been proposed as one underpinning for working memory (Thuault et al., 2013). HCN channels are an important control point (Burdakov, 2005) in other respects as well, regulating somatic and dendritic responsivity and having effects on network oscillations (Neymotin et al., 2013, Kocsis and Li, 2004),

These network and molecular views of persistent activity and memory are entirely complementary. Indeed, it would be remarkable if multiple scales and multiple mechanisms were not involved in such a basic phenomenology (Lytton et al., 2014). In this paper, we combine these observations through a multiscale computer model of neocortex that ranges in scale from intracellular  $Ca^{2+}$  dynamics, up through cellular electrochemical coupling and on to network activity. Intracellular species simulated include  $Ca^{2+}$ , inositol triphosphate (IP<sub>3</sub>),  $Ca^{2+}$  buffers, and cAMP.

Both single cells and the network produced persistent activity following excitatory stimulation. Metabotropically, the stimulus triggered an intracellular signaling cascade which caused persistent increased firing rate in the individual pyramidal cell. Placing this cell into a network with realistic connectivity produced effects augmenting and altering the persistent activity patterns through the combination of metabotropic and ionotropic recurrent activations, with non-stimulated cells suppressed via feedback inhibition. Network firing rates differed across cortical layers, and oscillation frequency shifted. The network model also demonstrated multiple roles of excitation/inhibition balance in maintaining both optimal network activation, and in controlling membrane mechanisms mediated through the voltage sensitivity of  $I_h$ . Multiple calcium sources – extracellular and intracellular – played synergistic roles in induction of persistent activity. Calcium buffer in the model was critical for regulating cytosolic free calcium, and therefore buffer level had an inverse relationship with persistent activity. By bridging multiple interacting scales and signaling modalities, electrical and chemical, our model demonstrates novel inter-scale interactions providing complementary routes for induction and maintenance of persistent activity.

# **2 Experimental Procedures**

Network simulations consisted of 776 reduced compartmental cell models with single compartments for inhibitory cells and 5 compartments for pyramidal cells, arrayed by layer with connectivity taken from experimental results on motor cortex (Weiler et al., 2008) (Fig. 1a). Parallel-conductance electrophysiological simulation in the pyramidal cells was complemented by chemophysiological simulation focused on  $Ca^{2+}$  handling, based on a prior study (Neymotin et al., 2015) (Fig. 1b).

Simulations were run in the NEURON (version 7.4) simulation environment (Carnevale and Hines, 2006) utilizing the reaction-diffusion (RxD) Python module (McDougal et al., 2013a, McDougal et al., 2013b) and NMODL (Hines and Carnevale, 2000). 16 s of simulation time took ~6 minutes using 82 nodes on a Linux cluster with parallel NEURON, run with a fixed time-step of 0.1 ms. The full model is available on ModelDB (#185858).

We describe the scales of the multiscale model sequentially from smaller to larger in the following sections. **1.** The molecular scale of 10-100 microns: molecular interactions in the model primarily revolve around  $Ca^{2+}$  dynamics and the effects of  $Ca^{2+}$  on various intracellular properties, most notably on the HCN (*I*h) channel. **2.** The cellular scale of up to 1 mm: the description considers both cell morphology (anatomy) and electrophysiological properties. Although the primary electrophysiological mediators are ion channels at the molecular scale, they are encapsulated at the higher scale as electronic components. This

encapsulation and linking across scales occurs as part of multiphysics simulation – the electrophysiological simulation based on electrical circuit theory is coupled to reactiondiffusion formalisms. **3.** The local network scale of up to 1 cm. Description of the network is based on identification of synapse types. The overall simulation is multialgorithmic as well as multiphysical: event-driven algorithms for synapse and network interact with the ordinary and partial differential equation levels of electrophysiological and reaction-diffusion

#### **2.1 Intracellular molecular scale**

simulation.

Our *Ca*2+ dynamics (Fig. 1b), similar to those used in (Neymotin et al., 2015), were derived from (Wagner et al., 2004), itself a spatial variant of (Li and Rinzel, 1994). Parameters are shown in Table 1. We modeled a one-dimensional RxD system of intracellular neuronal  $Ca<sup>2+</sup>$  signaling in all compartments of neocortical pyramidal (PYR) neurons. Within each compartment, we modeled cytosolic and endoplasmic reticulum (ER) sub-compartments by using a fractional volume for each: for a given cell volume, *fER* denotes the fraction occupied by the ER, and  $f_{cyt}$  denotes the fraction occupied by the cytosol:  $f_{cyt} + f_{ER} = 1$ .

 $IP<sub>3</sub>$  was produced through a reaction sequence initiated by glutamate binding to the metabotropic glutamate receptor (mGluR), based on a reaction scheme developed by (Ashhad and Narayanan, 2013) (ModelDB  $#150551$ ). IP<sub>3</sub> diffused outward from the synapse location and decayed following first-order kinetics with  $\tau_{IP3}$  of 1 s. Baseline mGluR synaptic weight was normalized to represent the increase in the amount of glutamate bound to mGluR. Extracellular glutamate did not diffuse but was represented by a local Glu value that was incremented in response to an event delivered due to a presynaptic spike. Glu showed bind/unbind kinetics on mGluR and was eliminated by first-order degradation (lower left of (Fig. 1b).

The ER Ca<sup>2+</sup> model involves IP<sub>3</sub> receptors (IP<sub>3</sub>Rs), SERCA pumps, and a Ca<sup>2+</sup> leak. IP<sub>3</sub>R dynamics involved a slow  $Ca^{2+}$  inactivation binding site state (De Young and Keizer, 1992, Li and Rinzel, 1994). This IP<sub>3</sub>R bell-shaped dependence on calcium is evident in all mammalian isoforms of IP<sub>3</sub>Rs (Tu et al., 2005, Tu et al., 2005, Taylor and Tovey, 2010), and provides the basis of much modeling work in intracellular  $Ca^{2+}$  dynamics (Fall and Rinzel, 2006, Fall et al., 2004, Hartsfield, 2005, Peercy, 2008). We denote by  $J_{\text{IP3R}}$ ,  $J_{\text{SERCA}}$ , and  $J_{\text{leak}}$  the mass flux per unit volume due to the IP<sub>3</sub> receptor, SERCA pump, and leak channels, respectively. Dividing the mass flux by the volume fraction gives the change in concentration.

Cytosolic Ca<sup>2+</sup> concentration ( $Ca_{cy}^{2+}$ ), ER Ca<sup>2+</sup> concentration ( $Ca_{ER}^{2+}$ ), and IP<sub>3</sub> concentration  $(IP_3)$  followed:

$$
\frac{\partial Ca_{cyt}^{2+}}{\partial t} = D_{Ca_{cyt}^{2+}} \cdot \frac{\partial^2 Ca_{cyt}^{2+}}{\partial x^2} + \frac{J_{IP3R} - J_{SERCA} + J_{leak}}{f_{cut}} + J_{memb} \quad (1)
$$

$$
\frac{\partial Ca_{ER}^{2+}}{\partial t} = D_{Ca_{ER}^{2+}} \cdot \frac{\partial^2 Ca_{ER}^{2+}}{\partial x^2} + \frac{J_{IP3R} - J_{SERCA} + J_{leak}}{f_{ER}} \quad (2)
$$
\n
$$
\frac{\partial IP_3}{\partial t} = D_{IP_3} \cdot \frac{\partial^2 IP_3}{\partial x^2} \quad (3)
$$

*J*memb denotes the net flux into the cytosol due to channels on the plasma membrane. Fluxes from the IP<sub>3</sub>R(*J*<sub>IP3R</sub>), SERCA pump (*J*<sub>SERCA</sub>), and leak channels (*J*<sub>leak</sub>) follow:

$$
J_{IP3R} = g_{IP3R} \cdot m_{IP_{3}\infty}^{3} \cdot m_{Ca\infty}^{3} \cdot h_{IP3R}^{3} \cdot \left( Ca_{ER}^{2+} - Ca_{cyt}^{2+} \right) / \Xi
$$
 (4)  

$$
J_{SERCA} = -\frac{g_{serca} \cdot Ca_{cyt}^{2+2}}{\left( k_{serca}^{2} + Ca_{cyt}^{2+2} \right) \cdot \Xi}
$$
 (5)  

$$
J_{leak} = g_{leak} \cdot \left( Ca_{ER}^{2+} + Ca_{cyt}^{2+} \right) / \cdot \Xi
$$
 (6)

Here,  $\Xi = N_A/10^{18} \approx 6.02 \cdot 10^5$ , the number of molecules in a cubic micron at a concentration of 1 mM, where *NA* is Avogadro's constant.

 $J_{IP3R}$  has 3 gating parameters. Activation gates  $m_{Ca}$  and  $m_{IP3}$  are represented by their steady state values  $m_{Ca\infty}$  and  $m_{IP3\infty}$  due to their rapid activation rates (Li and Rinzel, 1994). Inactivation via  $h_{IP3R}$  is a slow Ca<sup>2+</sup>-dependent process with  $\tau_{IP3R}$  of 400 ms.

$$
m_{IP_3\infty} = \frac{IP_3}{IP_3 + k_{IP_3}}
$$
 (7)  

$$
m = \frac{Ca_{cy}^{2+}}{2}
$$

$$
m_{ca\infty} = \frac{c_{gt}}{Ca_{cyt}^{2+} + k_{act}} \quad (8)
$$

$$
\dot{h}_{IP3R} = \frac{h_{IP3R\infty} - h_{IP3R}}{\tau_{IP3R}}
$$
 (9)

$$
h_{IP3R\infty} = \frac{k_{inh}}{k_{inh} + Ca_{cut}^{2+}} \quad (10)
$$

The SERCA pump is a pump rather than a channel and so is modeled with Hill-type dynamics. Initial conditions for  $Ca_{cyt}^{2+}$ ,  $Ca_{ER}^{2+}$ , IP<sub>3</sub>, and *h*<sub>IP3R</sub> were set to 0.0001 mM, 1.25

mM, 0.0 mM, and 0.8, respectively.  $Ca_{FB}^{2+}$  was set to 1.25 mM to reflect primed ER calcium stores. This 1.25 mM is consistent with experimentally-obtained values (Bygrave and Benedetti, 1996, Neymotin et al., 2015).

Calcium buffering followed

$$
Ca + B \underset{9.5 \cdot 10^{-4}}{\xrightarrow{5}} CaB
$$
 (11)

where *B* is diffusible buffer with diffusion coefficients D=0.043 *μm*<sup>2</sup> /*ms* for both *B* and *CaB*, about half the rate of  $Ca^{2+}$ diffusion (Table 1) (Anwar et al., 2012). Calcium extrusion across the plasma membrane was modeled by first-order decay with  $\tau_{ex} = 5$  ms except where varied in Fig. 13.

Chemical dynamics are typically slower than electrical dynamics but vary more quickly with position (less stiff in time but more stiff in space). We therefore increased chemical discretization to make sure that our baseline compartmentalization was adequate. Testing  $Ca<sup>2+</sup>$  dynamics using 1 µm subcompartments demonstrated that the calcium values were well-approximated (Fig. 2).

## **2.2 Synapses**

AMPA/NMDA synapses were modeled by standard NEURON double-exponential mechanisms with parameters based on previous papers (Neymotin et al., 2013, Neymotin et al., 2011b, Neymotin et al., 2011a). All excitatory projections were mixed AMPA (rise, decay  $\tau$  : 0.05,5.3 ms) and NMDA (rise, decay  $\tau$  : 15,150 ms). NMDARs were scaled by 1/(1 + 0.28 · *M g* · *exp*(−0.062 · *V*)); *M g* = 1*mM* (Jahr and Stevens, 1990b). 13% of  $I_{NMDA}$  was carried by Ca<sup>2+</sup>(Spruston et al., 1995). AMPA and NMDA receptors had reversal potentials of 0 mV.

Inhibitory synapses were mediated by GABA<sub>A</sub> and GABA<sub>B</sub> receptors. GABA<sub>A</sub> synapses were modeled with a double-exponential mechanism. The  $GABA_B$  synapse had second messenger connectivity to a G protein-coupled inwardly-rectifying potassium channel (GIRK), as described in (Destexhe et al., 1996). LTS cells connected to apical dendrites of PYR cells using  $GABA_A$  receptors ( $GABA_AR$ ; rise,decay  $\tau$ : 0.2,20 ms) and  $GABA_B$ receptors (GABA<sub>B</sub>R; (Destexhe et al., 1996, Pérez-Garci et al., 2006)) and onto somata of FS and other LTS cells with  $GABA_A$  Rs (rise, decay  $\tau$ : 20,40 ms) (Bartos et al., 2007). GABA<sub>A</sub>Rs had reversal potentials of -80 mV, and GABA<sub>B</sub>Rs -95 mV.

#### **2.3 Cell scale**

The network consisted of pyramidal cells (PYR; 3 apical dendrite compartments, 1 basal dendrite compartment, 1 somatic compartment), fast spiking soma-targeting interneurons (FS; one compartment) , and dendrite-targeting low-threshold spiking interneurons (LTS; one compartment) (Neymotin et al., 2011b, Neymotin et al., 2011a, Wang and Buzsaki, 1996, Wang, 2002, Bartos et al., 2007, Monyer and Markram, 2004). Reaction-diffusion mechanisms  $(Ca^{2+}, IP_3$ , buffer) were restricted to the PYR cells in this network. Properties of pyramidal neurons in the different layers were identical except for apical dendrite length

which is longer in deep pyramidal neurons than in superficial (Castro-Alamancos, 2013, Hay et al., 2011): 900 *μ*m in L5-6; 450 *μ*m in L2/3.

Voltage-gated ionic current models were based on prior models of our own and others (McCormick and Huguenard, 1992b, Migliore et al., 2004, Stacey et al., 2009, Neymotin et al., 2011b, Neymotin et al., 2011a, Neymotin et al., 2013). Voltage sensitive channels generally followed the Hodgkin-Huxley parameterization, whereby  $\dot{x} = (x_{\infty} - x)/\tau_{\rm x}$  ( $x = m$ for activation particle and *h* for inactivation particle). Steady-state  $x_{\infty}$  and time constant  $\tau_x$ are either related to channel opening  $\alpha(V)$  and closing kinetics  $\beta(V)$  as  $x_{\infty} = \alpha/(\alpha + \beta)$ ,  $\tau_x =$  $1/(α + β)$ , or are directly parameterized:  $x_∞(V)$ ,  $τ_0(V)$ . Kinetics for channels were scaled by  $Q_{10}$  from an experimental temperature (where available) to simulation temperature of 37° Celsius.  $Q_{10}=3$  was used when no experimental value was available. All cells contained leak current, transient sodium current *IN a*, and delayed rectifier current *IK−DR*, to allow for action potential generation. Additionally, PYR cells contained in all compartments *IK−A*, *IK−M*  providing firing-rate adaptation (McCormick et al., 1993). Pyramidal cells also had *Ih*, voltage-gated calcium channels (VGCCs) in all compartments:  $I_L$ ,  $I_T$ ,  $I_N$  (McCormick and Huguenard, 1992a, Kay and Wong, 1987, Safiulina et al., 2010, Neymotin et al., 2015), and SK and BK calcium-activated potassium currents  $(I_{KCa})$ . LTS cells contained  $I_L$ , non-Ca<sup>2+</sup>dependent  $I_h$ , SK, and Ca<sup>2+</sup> decay. LTS  $I_h$  parameterization used Hodgkin-Huxley parameterization:  $\bar{g} = 0.00015 \text{ S/cm}^2\text{k}$ ;  $E_{rev} = -40 \text{ mV}$ ; with  $\tau = 5 + 200/(exp((v + 70)/20) +$  $exp(-(v+70)/20)$ ,  $m_{\infty} = 1/(exp((V+80)/10) + 1)$ ;  $Q_{10} = 2.2$ .

HCN channels in different cell types have somewhat different voltage dependence and different kinetics (Hagiwara and Irisawa, 1989, Wang et al., 2002, Robinson and Siegelbaum, 2003, Chen et al., 2001, Schwindt et al., 1992). The hyperpolarization-activated HCN current  $I_h$  used in pyramidal cells showed second messenger and calcium dependence taken from (Winograd et al., 2008) (ModelDB #113997; Fig. 3), modified to provide the faster voltage-sensitivity time constants found in cortex (Harnett et al., 2015). The mechanism for  $Ca^{2+}$  regulation of HCN channels in PYR cells in (Winograd et al., 2008) is modeled empirically in order to produce the relationship between cytosolic  $Ca^{2+}$  levels and  $I_h$  activation without simulating the details of  $Ca^{2+}$  effects on adenyl cyclase (see schematic for *HCN chan* in Fig. 1b). This empiric model provides combined control of conductance by cAMP (represented as a normalized level 'p1') and voltage using the following:

$$
I_h = g_h \cdot (01 + 2 \cdot 02) \cdot (V - E_h) \quad \text{where} \quad E_h = -30mV \quad (12)
$$

$$
p0 \stackrel{k_2 \cdot (\frac{Ca}{.006})^4}{\frac{L}{k_2}} p1 \text{ where } k_2 = 10^{-4} \quad (13)
$$
  

$$
C \stackrel{\alpha}{\underset{\beta}{\rightleftharpoons}} O1 \stackrel{0.8 \cdot p1}{\underset{0.008}{\rightleftharpoons}} O2 \quad (14)
$$

$$
\alpha = \exp(-9.63 - 0.0458 \cdot V) \quad (15)
$$

$$
\beta = \exp(-1.30 + 0.0447 \cdot V) \quad (16)
$$

was 0.0025 S/cm<sup>2</sup> in PYR soma, basal dendrites and exponentially-increasing in apical dendrites with distance from soma with 325 *μ*m space constant, hence *e*-fold augmented at 325 microns as described by (Kole et al., 2006). Apical dendrite *IK−DR*, *IK−A*, *IK−M* density also increased with the same length constant, based on data showing HCN and Kv channel colocalization (Harnett et al., 2015, Harnett et al., 2013).

We evaluated basic properties of the PYR model. A 0.01 nA depolarizing current provided 1.68 mV depolarization which decayed to 28% at 160 *μ*m in apical dendrite, and 65% at 110 *μ*m in basal dendrite (Larkum et al., 2009, Nevian et al., 2007). R*in* was 54 Mohm, sag 0.28 in soma (−0.8 nA, *sag* = (*vpeak* − *vsteady*)/*vsteady*). With HCN blocked, R*in* was 174 Mohm and sag was abolished (Sheets et al., 2011, Suter et al., 2013).

#### **2.4 Network scale**

The network consisted of 776 cells: 582 five-compartment pyramidal cells (PYR; 3 apical dendrite compartments, 1 basal dendrite compartment, 1 somatic compartment), 97 onecompartment fast-spiking (FS) soma-targeting interneurons, and 97 one-compartment lowthreshold spiking (LTS) dendrite-targeting interneurons (Neymotin et al., 2014, Neymotin et al., 2011b, Neymotin et al., 2011a, Wang and Buzsaki, 1996, Wang, 2002, Bartos et al., 2007, Monyer and Markram, 2004). The network contained 30,486 synapses for an overall connection density of ~5% (see Table 2). PYR cells synapsed onto each-other's dendrites. PYR-to-PYR synaptic locations on the dendrite were randomized between basal and apical compartments (Markram et al., 1997). PYR cells synapsed onto somata of FS and LTS cells (single-compartment models).

Neuronal populations were arranged by cortical layer based on our prior models (Neymotin et al., 2011, Neymotin et al., 2011a, Chadderdon et al., 2014), with additional data from direct measurements from mouse motor cortex (Weiler et al., 2008, Shipp, 2005, Hooks et al., 2013, Kiritani et al., 2012a). The network consisted of 150 layer 2/3 pyramidal cells (E2; E represents excitatory and 2 represents layer 2/3), 25 layer 2/3 fast-spiking interneurons (I2; I represents fast-spiking interneuron), 25 layer 2/3 low-threshold spiking interneurons (I2L; I2L represents low-threshold spiking interneuron in layer 2/3), 95 layer 5A pyramidal neurons (E5A), 145 layer 5B pyramidal neurons (E5B), 40 layer 5 fast-spiking interneurons (I5), 40 layer 5 low-threshold spiking interneurons (I5L), 192 layer 6 pyramidal neurons (E6), 32 layer 6 fast-spiking interneurons (I6), and 32 layer 6 low-threshold spiking interneurons (I6L).

Connection probabilities  $p_{ij}$  in the network were dependent on pre- and post-synaptic type

and inversely scaled based on distance (Table 2)  $p_{ij} = \bar{p}_{ij} \cdot \exp\left(-\sqrt{(dx^2+dz^2)}/15\right)$ , in x,z plane perpendicular to the y-direction of layering, based on data from rodent motor cortex mapping (Weiler et al., 2008, Kiritani et al., 2012a). Individual neurons were placed randomly with uniform distribution. Weights from E cells displayed in Table 2 are for the AMPA synapses, with colocalized NMDA weights at 10% of AMPA weights. This provided

for AMPA/NMDA current ratio of approximately 1.2, consistent with experiment (Wang et al., 2008). Since connectivity was random, specific divergence could vary. Synaptic delays were randomized between 1.8–5 ms with additional delay based on distance. Other parameters were based on the literature where available, as well as on previous models (Neymotin et al., 2013, Neymotin et al., 2011b, Neymotin et al., 2011a, Chadderdon et al., 2014, Song et al., 2013).

Background activity was simulated by excitatory and inhibitory synaptic inputs following a Poisson process, sent to all cells (Table 3), representing ongoing drive from other cortical areas and other inputs (Destexhe et al., 2003a). High background rates were required to maintain activity in the model, due to small network size (Neymotin et al., 2011a).

The synaptic stimulus used to assess persistent activity for both single cell and network simulations was provided to apical dendrites. For most simulations, a single period of stimulation was applied to 50% of PYR cells across all cortical layers. In Fig. 7, stimulation was provided selectively to a fixed number of cells in individual layers. Our current neocortical model, based on motor cortex, does not have cells in the L4 layer so that L4 inputs only synapse onto apical dendrites of L5 cells, an important part of L4 projections in sensory cortex (Shipp, 2005, Hooks et al., 2013, Suter and Shepherd, 2015).

To quantify the extent to which population firing rates changed during and after the stimulus, we formed multiunit activity (MUA) time-series, which count the number of spikes in each bin for a given population. We used several bin sizes (10 ms, 100 ms, 1000 ms) to display temporal activity at multiple resolutions. To quantify the efficacy of the network's response to a stimulus we used firing-rate distinction (FRD): the average ratio of firing rates of stimulated to non-stimulated E cells using 10 ms bin size over the 5 s following the end of stimulation (measured from 0.5 s after the end of input events, to avoid ongoing effects from NMDAR activation). Average measures of calcium and HCN channelrelated variables were also taken from the same period. For single cell simulations, FRD was calculated as the ratio of firing rate after the stimulus to the firing rate before the stimulus. To quantify long-term ensemble dynamics, we used population firing rate vectors formed by setting each entry in the vector as the corresponding cell's spikes in a 1000 ms interval. To quantify similarity of these firing-rate vectors over time, we took the pairwise Pearson correlation, forming a firing-rate vector similarity matrix (Neymotin et al., 2010, Kelemen and Fenton, 2010).

# **3 Results**

#### **Simulation overview**

Over 1600 simulations, with simulation durations of 10–245 s, were analyzed. Simulations of individual pyramidal neurons and simulations of entire networks of neurons were run. A typical simulation of 16 s of network time took ~6 minutes using 82 nodes on a Linux cluster with parallel NEURON. We ran simulations with initial calcium concentration in the ER set to 1.25 mM (Bygrave and Benedetti, 1996), to mimic the effects of ER calcium priming via prior excitatory synaptic stimulation (Fitzpatrick et al., 2009, Hong and Ross,

2007, Neymotin et al., 2015, Ross et al., 2005). This allowed the ER calcium to contribute to HCN channel regulation after mGluR stimulation.

#### **3.1 Persistent activity in a single pyramidal neuron**

A single layer 5 pyramidal neuron (E5) receiving random background synaptic activation followed by strong excitatory (AMPAR/NMDAR/mGluR) stimulation displayed a persistent increase in firing rate, via the effects of a set of molecular signaling cascades (Fig. 4). Prior to the stimulus, the E5 cell displayed a low firing rate of 1.6 Hz due to approximately balanced excitatory and inhibitory synaptic currents. After stimulation, the cytosolic calcium concentration increased due to voltage-gated calcium channel (VGCC) and NMDAR calcium influx (Fig. 4b). At the same time, the mGluR-activated cascade produced IP<sub>3</sub> (Fig. 4c), causing  $Ca^{2+}$  efflux from ER to cytosol (Fig. 4d). These multiple sources of cytosolic  $Ca<sup>2+</sup>$  augmented cAMP, an HCN channel-regulating second-messenger, over tens of seconds (Fig. 4e). Prior to the stimulation, HCN channel conductance (*gh*) in soma and dendrite were at similar levels (Fig. 4e), but diverged after stimulation. During the upstroke of individual action potentials, *gh* in the soma followed spiking rapidly while *gh* in dendrite did not vary as much due to more moderate alterations in dendritic voltage but showed a persistent >7× activation due to the second messenger effect (Fig. 4f). During the excitatory stimulus,  $I_h$  (Fig. 4g) briefly decreased (note negative inward current) due to membrane depolarization. Afterwards, dendritic *Ih* increased, following *gh* despite some negative feedback due to depolarization effects on both activation and driving force. The associated dendritic depolarization drove spiking in the soma (Fig. 4h). Elevated dendritic voltage lasted  $>65$  s with somatic action potential firing increasing to 52 Hz, a 32 $\times$  increase over baseline, during the 10 s after stimulation. The single cell's firing remained elevated above 10 Hz for  $\sim$  62 s after stimulation. The continued activation of  $I_h$  depended on an ongoing balance between excitation and inhibition. In the absence of inhibition,  $I_h$  turned off due to its voltage dependence (hyperpolarization activates; depolarization deactivates).

#### **3.2 Persistent activity in network**

Adding cell-based *Ih*-dependent persistent activity to a network produced a model with synergistic network- and cell/molecular-effects. Individual cells in the network model demonstrated the same pattern of persistent activity after stimulation seen in the single neuron model (Fig. 5). Activation provided augmented inhibition as well as increased excitation. This ongoing inhibition helped maintain  $I_h$  effect by preventing excessive depolarization that would deactivate  $I_h$ . The relative isolation of  $I_h$  in the dendrites also helped prevent this deactivation in the setting of high ongoing activity.

During baseline conditions, the average firing rates of excitatory  $(E)$  and inhibitory  $(I)$ neurons ranged between 2.5–5.4 and 2.3–9.4 Hz, respectively, with rhythmic population oscillations at a high alpha/low beta frequency of  $\sim$  14 Hz. A brief, single stimulation period applied to a randomly selected 50% of the excitatory neurons across layers was used to represent the *activation pattern*. The immediate effects were depolarization of the stimulated cells and increase in cytosolic IP3. During stimulation, average membrane potential was increased, causing a reduction in AMPAR/NMDAR driving-force and a brief fall-off of firing rate.

After stimulation was turned off, the firing rate of stimulated E cells remained elevated for  $\sim$  60 s, dropping below 10 Hz after 35 s. Rates of the stimulated pyramidal cells increased from 3.7 to 20.0 Hz while rates of the non-stimulated pyramidal cells decreased from 3.6 to 0.8 Hz. The population rhythm increased from 14 Hz to ~20 Hz. This resultant oscillation was at the firing rates of the stimulated cells, and was of lower amplitude, being carried primarily by these cells.

The network connectivity enabled several emergent effects produced via synaptic interactions. The higher activity of stimulated E cells produced increased drive from E to I cells: I rates transiently increased to  $\sim$  20 Hz during stimulation (Fig. 5b gray), and then remained elevated throughout the persistent activity. This dynamic increase in inhibition throughout the network was the cause of depressed firing rates of the non-stimulated E cells (>75% reduction) which allowed the stimulated cells to dominate network dynamics. The increased activation of I cells also shortened the network's response duration, compared to the isolated single cell.

Although the stimuli were identical across cortical layers, there was a larger post-stimulus response in layers 2/3 and 6, compared to the two E populations in layer 5 (L5A and L5B). These differences in response correlated with different ratios of convergent inhibitory inputs to convergent excitatory inputs for the E cells in the different layers (L2:0.4, L5A:0.2, L5B: 0.1, L6:0.4). Higher I $\rightarrow$  E connectivity would translate into greater hyperpolarization of E cells in a layer, greater activation of  $I<sub>h</sub>$ , and greater activation despite the countervailing direct effect of inhibition.

#### **3.3 Molecular cascades within cells within network**

The same sequence of molecular activations that led to persistent activity in the simulation of the individual E5 cell (Fig. 4) was also seen in the E5 cells within the full network (Fig. 6). Stimulation-induced depolarization caused further opening of NMDA channels, as well as the activation of VGCCs, which admitted additional calcium into the cytosol. On average, E5 cells in the stimulated population showed a transient elevation in the cytosolic calcium of ~0.01 mM (Fig. 6a). mGluR stimulation occurred at the same time as AMPA/NMDA synapse activation and produced IP<sub>3</sub>, with subsequent IP<sub>3</sub> binding to ER IP<sub>3</sub>Rs. Together with the available calcium, this caused the endoplasmic reticulum (ER) to release additional calcium from its stores into the cytosol after a short interval, further contributing to the population calcium increase (Fig. 6b).

Upon stimulus-induced calcium influx, the level of calcium buffering proteins (*B*) bound to calcium (*CaB*) increased rapidly for the stimulated population (Fig. 6c), preventing the high levels of free cytosolic calcium which can cause excitotoxicity (Neymotin et al., 2013, Taxin et al., 2014, Seidenstein et al., 2015). After stimulation, the calcium-bound buffer levels gradually decayed as calcium was taken up into the ER and expelled via the calcium extrusion pumps. *CaB* for the non-stimulated population decayed due to hyperpolarization in non-stimulated cells reducing influx and decreasing intracellular calcium.

Upon stimulation, the calcium influx into the cytosol provided the *preparatory* steps for persistent activity, causing cAMP to increase and remain high in the stimulated population

(Fig. 6d). During the stimulation itself, HCN channel conductance (*gh*) declined briefly due to the immediate effect of stimulus-induced depolarization (Fig. 6e). Thereafter, increased inhibition from feedback interneurons reduced stimulated-cell potential, thereby permitting rapid conductance increase, due to the quick responsivity of conductance to voltage change (Harnett et al., 2015), contrasted with the slower second messenger effects. In this way, HCN channel activation and its role in persistent dynamics was critically dependent on network effects, namely ongoing inhibition from the highly activated  $E \rightarrow I$  pathway, as well as on the intrinsic chemophysiological effects of increased second messenger. Similarly, the non-stimulated population showed a slight increase in *gh*, caused by hyperpolarization due to augmented inhibitory input. However, in the absence of second messenger, this had little effect on the non-stimulated population.

#### **3.4 Targeted stimulation of cortical layers**

Cortical layers receive layer-specific inputs from other parts of cortex and from other brain areas (Hooks et al., 2013, Suter and Shepherd, 2015). We tested the effects of inputs into individual layers, stimulating the same number of cells in each case (Fig. 7). In the baseline simulation, activity in the stimulated layer remained confined to that layer. Duration of activity, measured by time from stimulus until the activated neuron rates dropped below 10 Hz, was about 40 s with either individual or all-layer stimulation (Fig. 7a). This differed considerably from the ~60 s seen with stimulation of an isolated L5 pyramidal cell (not shown), due to feedback inhibition in the network. Compared with the other 2 stimulation locations, L5 stimulation provided a different activation pattern with lower rate but with an initial plateau period of 15 s before activity decay. This appeared to be a network consequences of the higher density of interconnectivity among E5 cells compared to other layers. The only prominent cross-layer effect was seen with stimulation of L2/3 (Fig. 7a left column) which provided strong feedforward inhibition in L5. Activation across all layers largely overcame this downward inhibition (Fig. 7 right column). As with L5 focal stimulation, all-layer activation produced an initial plateau and abbreviated activity duration in L5..

In order to assess the influence of excitatory/inhibitory balance (Table 2) (Weiler et al., 2008), we also assessed the network with higher internal excitatory gain (Fig. 7b). This gain increase generally produced longer response durations, except that L5 stimulation paradoxically produced a weaker and shorter response (32 s) despite the increase in excitatory strength compared to the baseline network. Instead of interlayer feedforward inhibition from L2/3 to L5, this network showed feedforward excitation with interlayer activity propagation. Stimulation of all layers now produced more prolonged activation with some spread from stimulated to non-stimulated cells.

#### **3.5 Prolonged weak stimulation also activated network**

Prolonged weak (10% strength) stimulation also produced increases in the firing rate of the stimulated population with further augmentation with greater duration of stimulation (Fig. 8). Weak stimulation produced a less sharp increase in firing rates than was seen with the stronger stimulation and peak rates were reduced, even with 20 seconds of stimulation. In this low-strength case, the stimulated cells' calcium transients were broader due to lengthier

stimulation, but reached a lower peak. Post-stimulus firing-rates of stimulated neurons increased from 7.8–11.2 Hz with stimulus duration. Increased excitatory firing promoted higher firing of interneurons, which also increased slightly with stimulus duration (average from 6.0–6.8 Hz). As a result of increasing inhibition, the non-stimulated E neurons decreased their post-stimulus rates with increased duration (average 2.6–1.8 Hz). We quantified the degree of activation of the stimulated population by comparing it to the firing rate of the non-stimulated cells. We defined a firing-rate distinction (FRD) measure as the average ratio of firing rates for stimulated versus non-stimulated E cells measured by multiunit activity (MUA) over the first 5 s following stimulation (Fig. 5b). FRD increased nearly linearly over stimulus durations from 1–14 s, and then saturated with longer duration stimulation (Fig. 8c). As with the brief, strong stimulation, high firing rates persisted after the stimulation was turned off, albeit at a lower level, and produced suppression of the nonstimulated E neurons (purple line).

#### **3.6 Neuronal ensemble dynamics during persistent activity**

Stimulation of persistent activity was repeatable with similar overall activity as well as specific activity pattern (Fig. 9). The baseline state ensemble activity could be distinguished from that of the stimulated state by noting the change in activity vectors (Fig. 9b), with different elements and layers showing somewhat different degrees of persistence – note that the strands of activation are of different lengths in different layers. The activated state provided a reproducible firing pattern (Fig. 9c). The strong correlations in the block starting at  $(x, y)$  coordinates (185 s, 60 s) in Fig. 9c demonstrates that the activity after the second stimulation starting at 185 s is very similar to the activity after the first stimulation at 60 s. The pattern of the activated ensemble is also highly self-similar in each case (red at both the  $(60,60) - (100,100)$  block and and  $(185,185) - (250,250)$  block), demonstrating the persistent activity in the same subset of cells. Baseline activity  $((0,0) - (60,60)$  block and (150,150) – (185,185) block) also shows self-similarity but was less stereotyped (lower overall correlation). This baseline activity was also recurrent as seen in the correlation in the block from 150,0 – 185,60. Values for the overall correlations are given in Table 4. Low similarity across pre-stimulation and post-stimulation states can be seen in the blue-green blocks –  $e.g.,$  that between the first persistent-activity state (after 60 s) and the first baseline state (starting at time 0 s) is 0.45 as seen in the block from  $60,0 - 80,60$ .

### **3.7 Excitation/inhibition (E/I) balance modulates persistent activity**

Classically E/I balance is considered as a fundamental attribute of network dynamics, balancing activity between the pathological extremes of epileptiform activity (too much E) and inactivity (too much I). This balance also plays this primary role in the current simulation. However, in addition, inhibition was permissive for stimulation-induced persistent activity due to its role in preventing deactivation of *I*h through excessive depolarization due to synaptic excitation and due to depolarization from *I*h itself (*E*h) at −30 mV with  $m_{\infty h}$  inflection at about the same voltage location depending on  $[Ca^{++}]_i$  (Fig. 3).

Changing the *static* synaptic weights from  $E \rightarrow I$  neurons, and from  $I \rightarrow E$  neurons, set the overall *dynamic* level of inhibition in the network. The dynamics of this feedback inhibition was approximately proportional to the product of  $E \rightarrow I$  and  $I \rightarrow E$  synaptic strengths, due to

the E→I increasing I cell firing which then produced negative feedback via the I→E weights. Due to this relationship, inhibition increases from bottom-left to top-right in Fig. 10. The dynamic level of inhibition was reflected in neuronal firing rates (Fig. 10a,b) and in the overall activation of *g*h (Fig. 10e). Increasing the synaptic weights along the E→I pathway tended to cause the I firing rates to increase (Fig. 10a). As the E cells activated I cells more strongly, the extra feedback inhibition decreased E firing rates (Fig. 10b). Increasing synaptic weights from I→E cells hyperpolarized the E cells and dampened their activity. When weights from E→I cells were set to zero, the I firing rates were sparse.

The modulation of firing rates and the overall depolarization level of E cells influenced the level of stimulus-induced calcium transients via VGCCs and voltage-sensitive NMDA *Ca*2+ flux (Fig. 10c). Calcium transients in E cells were largest when there was minimal inhibition in the network. Elevated calcium, as a second messenger, then produced additional intracellular molecular effects. The availability of cytosolic calcium after a stimulus translated directly into the level of cAMP (Fig. 10d), with values increasing in parallel with cytosolic calcium. Once cAMP increased, it contributed to regulating HCN channel activation ( $g_h$ ; Fig. 10e). However, in addition to  $Ca^{2+}$  control,  $g_h$  is also voltage-sensitive, being deactivated by depolarization. Activation of *gh* (Fig. 10e) therefore did not follow the patterns of cAMP (Fig. 10d) but instead nearly mirrored it, with large values at high levels of inhibition.

The ratio of *gh* for stimulated vs. non-stimulated cells supported stimulus-specific representations due to these molecular/cellular mechanisms (Fig. 10f). This ratio was maximally activated over a relatively narrow crescent-shaped region of  $E \rightarrow I$  and I $\rightarrow E$  gains with moderate overall inhibition. At values above and to the right of the crescent, high inhibition controlled HCN channels through voltage effects so that the calcium transients no longer provided primary regulation of the HCN channel dynamics of the stimulated population.

FRD followed a similar crescent-shaped pattern, with maximal activation at moderate levels of inhibition (Fig. 10g). At these levels of inhibition, there was sufficient cytosolic calcium to regulate HCN channels in a population-specific manner, and adequate inhibition to activate HCN channels (Fig. 10f,h). At the lowest  $E \rightarrow I$  synaptic weights interneuron firing rates were sparse (left-most column in Fig. 10a), and when  $I \rightarrow E$  weights were also low, there was not sufficient inhibition/hyperpolarization to activate HCN channels and produce substantial FRD. Increasing  $I \rightarrow E$  weights at these low  $E \rightarrow I$  levels caused enhanced inhibition within the network, enhanced activation of *I*h, and increased FRD (rising portion of FRD in Fig. 10h). FRD then peaked at intermediate levels of inhibition. At higher  $E \rightarrow I$ weights, increasing  $I \rightarrow E$  weights caused high feedback-inhibition within the network, dampening the FRD response (decaying portion of Fig. 10h).

Fig. 10h shows the discrepancy between molecular and network effects, demonstrating that the molecular effects seen in the single cell model do not fully explain the persistent activity differences in the network model. Relative activation of *gh*, decreasing with increasing inhibition in the network (symbol color in Fig. 10h), only partially explained FRD, shown on the y-axis of Fig. 10h. Peak FRD did not occur with lowest inhibition both because low

inhibition did not adequately suppress the non-stimulated population and because excessive depolarization in the stimulated cells deactivates HCN Fig. 10e.

Stimulation of both E cells and I cells rather than E cells alone produced results qualitatively similar to Fig. 10, but with reduced FRD (peaking at 31 vs 39). Stimulating the I cells directly produced additional inhibition in the network which reduced activation of the stimulated cells and reduced  $Ca^{2+}$  entry, consequently reducing  $I<sub>h</sub>$  effects.

# **3.8 Internal vs external calcium stores**

Induction of persistent activity in our model relies on calcium, which comes to the cytosol from both extracellular stores via NMDARs and VGCCs, and from ER via IP<sub>3</sub>R. We investigated the effects of modulating the relative contribution of external and internal calcium sources by regulating the strength of stimuli influencing each store (Fig. 11) and by adjusting properties of the neurons (VGCC density, calcium in ER) that lead to different relative strengths of each calcium store (Fig. 12).

Varying the strength of ionotropic (AMPAR/NMDAR) vs metabotropic (mGluR) stimulation regulated FRD (Fig. 11). The AMPAR/NMDAR stimulus strength both directly regulated depolarization/firing produced by stimulation, and also admitted calcium via both NMDARs and VGCCs, and produced augmentation of both  $[Ca^{2+}]$  and activity. Peak  $[Ca^{2+}]$ was less in the absence of AMPAR/NMDAR stimulus, since  $Ca^{2+}$  was then sourced from the limited ER stores. With increased AMPAR/NMDAR stimulus strength calcium continued to increase, whereas it plateaued with increased mGluR strength (Fig. 11a). The differences in calcium transients from differential AMPAR/NMDAR activation translated into differences in the FRD (Fig. 11b). There was a nearly linear  $\lceil Ca^{2+} \rceil$  increase with AMPAR/NMDAR translated into a sigmoidal FRD while the saturating  $[Ca^{2+}]$  response from mGluR produced a more rapid increase in FRD, with both plateauing at an FRD value of ~25. In the regime of 0-1 gain of AMPAR/NMDAR, it appeared that stimulus strength could be encoded by the FRD, the differential activation of the two populations of neurons.

Simultaneously increasing the AMPAR/NMDAR and mGluR stimulus strengths had only a small additional impact on calcium transients, with increases adding sublinearly. Increases in calcium transients at high stimulus strengths did not translate into substantial increased FRD, due to  $Ca^{2+}$  buffering and extrusion pumps quickly clearing cytosolic  $Ca^{2+}$ , and preventing it from impacting HCN channel dynamics.

With low  $Ca^{2+}$  availability from both sources (VGCCs and ER; Fig. 12d and lower left), the FRD was low, because of insufficient calcium to trigger a post-stimulus response. High entry from external stores only (high VGCC density) produced an increase in pre-stimulus firing, a small increase in post-stimulus firing, and weak suppression of non-stimulated neuron activity, resulting in moderate FRD (lower right and Fig. 12e). High entry from from both stores (upper right and Fig. 12c) caused a substantial increase in FRD due to higher post-stimulus firing rates which led to more suppression of non-stimulated neurons. The highest FRD was seen with low flux from external and low to mid flux from internal stores (upper left, Fig. 12b and left middle), which resulted in the largest increase in stimulated neuron firing, and the largest suppression of non-stimulated neurons. Overall, FRD

increased along the y-axis of Fig. 12a, in proportion to initial ER calcium levels, because ER  $Ca^{2+}$  only contributes to cytosolic calcium due to stimulation. In contrast, FRD tended to have an inverted-U relationship with VGCC density (x-axis around  $y=1.0$ ) because increasing VGCC density allowed post-stimulus  $Ca^{2+}$  influx, but at high levels produced increases in baseline firing of both populations both before and after the stimulus, which reduced firing-rate distinction.

We also modified the FRD measure for use in single cell simulations by taking the ratio of post-stimulus firing rate to baseline firing rate; across the same set of variations in VGCC density and initial ER  $Ca^{2+}$ , qualitatively similar results were found (data not shown).

## **3.9 Free calcium regulates persistent activity**

Modulating the plasma membrane calcium extrusion pump time constant ( $\tau_{ex}$ ) altered calcium levels, with downstream effects on the network's ability to display calciumdependent persistent activity and stimulus-specific representations (Fig. 13). Both stimulation-induced calcium transients and post-stimulus calcium levels increased as the calcium extrusion pump  $\tau_{ex}$  increased (Fig. 13a). This pattern was evident for both the stimulated (light-blue) and non-stimulated (purple) population, although at any  $\tau_{ex}$ , the stimulated population had a higher calcium concentration due to stimulation it received. At a fast  $\tau_{ex}$  of 0.5 ms the extrusion pump cleared cytosolic calcium quickly, with pre-stimulus calcium levels for both populations being reduced to low levels. The fast action of the extrusion pump also reduced the stimulation-induced calcium transient, which was considerably smaller than at the baseline  $\tau_{ex}$  of 5 ms (2.5 vs 13  $\mu$ M). With this fast  $\tau_{ex}$ , the calcium was more quickly cleared after stimulation, leaving only a small amount of calcium available to impact HCN channels, and producing a relatively low FRD (1.2). With slow calcium extrusion ( $\tau_{ex}=20$  ms), pre-stimulus calcium levels were rising for both populations prior to stimulation, since the calcium clearance rate was less than the rate of cytosolic calcium entry from NMDA/VGCC/ER leak calcium channels. Stimulation also produced a large calcium transient of 50 *μ*M, which decayed more gradually. As a result of the slow clearance rate of calcium, the calcium remained elevated in the stimulated population longer, contributing to positive feedback and increasing modulation of the stimulated population's *gh*. These factors allowed the stimulated population to dominate the network dynamics, creating a large overall FRD (20). As <sup>τ</sup>*ex* increased, the ratio of calcium in the two populations showed an initial sharp rise followed by a slower rise (Fig. 13a black points). FRD, which depends on calcium-regulation of HCN channels, also showed a similar relationship with the calcium extrusion pump  $\tau_{ex}$  (Fig. 13b).

IP<sub>3</sub>R density increase allowed release of more  $Ca^{2+}$  from ER after mGluR activation (not shown). Changes between  $0-3\times$  baseline modulated calcium transients (0.003–0.014 mM) and increased FRD over a substantial range (12–28). The value with low IP<sub>3</sub>R density reflected a situation where primary  $Ca^{2+}$  came in from extracellular sources, less effective in the absence of any internal release as shown in Fig. 12. Increasing IP<sub>3</sub>R demonstrated a synergy between  $Ca^{2+}$  sources.

Modulating calcium buffer efficacy (*F Rate*× buffer concentration) altered the ability of free calcium to contribute to persistent activity (Fig. 14). Buffering affects the motility and

amount of free calcium. Increased buffer prevented calcium from being taken up and stored in the ER. Overall, the amount of calcium released from the ER upon stimulation was inversely proportional to the buffer efficacy, with 1.1 vs. 1.2 mM calcium released at high and low buffering efficacy, respectively. However, with low buffering efficacy, the ER calcium levels were only slightly larger than low buffering efficacy, since ER stores were initialized to 1.25 mM and were only allowed 5 s to refill. Increased buffering efficacy meant more  $Ca^{2+}$  bound prior to stimulation and less available to be taken into the ER, while at the same time reducing baseline  $Ca^{2+}$  effects on HCN channels. Increases in buffering efficacy also decreased the Ca<sup>2+</sup> transient with stimulation (Fig. 14a) – free Ca<sup>2+</sup> availability was primarily a function of buffer concentration with an effect of *F Rate* primarily at the left margin. HCN channel activation showed a similar response profile (Fig. 14b) but FRD alterations were more patchy since FRD is based on effects on the non-stimulated as well as on the stimulated cells (Fig. 14c).

# **4 Discussion**

We developed a multiscale neocortical model from molecular to network level by evaluating a model of HCN modulation via a second-messenger signaling cascade at cell and network scales. This model displayed the persistent activity that has been hypothesized to contribute to cognitive, mnemonic and behavioral functions that require the maintenance of state over a period of seconds (Ames et al., 2014, Cossart et al., 2003, Goldman-Rakic, 1995, Major and Tank, 2004). The model confirmed prior simulations that showed how the molecular dynamics of calcium regulation of HCN channels Fig. 6) could produce persistent electrical activity at the single cell level (Fig. 4). Embedding these molecular models into cells within a network produced emergent effects based on interactions between excitatory and inhibitory neurons (Fig. 5, Fig. 10), and the specific details of neocortical architecture (Fig. 7).

## **4.1 Scale overlaps in neural systems**

To a greater extent than in other bodily organ systems, the nervous system features an interplay of scales which makes encapsulation of one scale for use in a higher scale difficult. A weakness of the widely-used point-neuron model is the encapsulation of activity in a single input-output dynamic which not only omits obvious non-point interactions such as dendrodendritic synapses (Rall and Shepherd, 1968), but also subtle interactions such as that between signal integration in apical dendrite and signal integration in local microcircuit (Lytton et al., ). By contrast, the multiscale modeling approach used here builds interacting scales into a coherent model which allows us to explore these interactions across levels of organization (Sejnowski et al., 1988). In the present simulations, we focused on calcium and on multiple roles for inhibition, bridging from the molecular to cellular and network scales (Lytton and Sejnowski, 1991, Neymotin et al., 2011). Synaptic connectivity and  $Ca^{2+}$ handling intersected at multiple locations, including the interplay between extracellular and intracellular sources of  $Ca^{2+}$ .

Due to these second-messenger roles, inhibition plays a major role in activity maintenance through its influence on preventing depolarization with deactivation of *I*h, while at the same

time contributing to activity suppression. Hence the activity maintenance that is classically attributed to excitatory/inhibitory balance is here also provided within the context of inhibitory tone (Fig. 10). We defined *dynamic inhibition* as a network balance which itself depends on balance provided by  $E \rightarrow I$  and  $I \rightarrow E$  strength across multiple cell subpopulations in neocortex, as well as on the excitability of the inhibitory cells. Changes in  $V_{\text{memb}}$  alters  $Ca^{2+}$  flux through VGCCs based on both  $V_{\text{memb}}$  and  $[Ca^{2+}$  ] via the Goldman-Hodgkin-Katz equation, as well as through NMDARs based on voltage sensitivity. As has been noted in other models and in tissue, synaptic bombardment greatly altered both membrane potential and input impedance with multiple subsequent effects (Bernander et al., 1991, Destexhe et al., 2003b). Overly high inhibition dampened neuronal firing while moderate inhibition was consistent with persistent activity over a wide range of parameter settings.

Calcium plays a pivotal role as a second messenger in many neural signaling pathways (Blackwell, 2013, Evans and Blackwell, 2015). Our model evaluated various scenarios regarding  $Ca^{2+}$  sourcing,  $Ca^{2+}$  removal,  $Ca^{2+}$  binding, and time constants of interaction with target molecules. Calcium in cytosol comes from the extracellular space, modeled here as an inexhaustible source, and from organelles which are exhaustible. Compared to mitochondria, ER is likely to be a more accessible  $Ca^{2+}$  source across multiple locations including spines – it spreads diffusely throughout the neuron, foliating at key points to provide additional surface area (Shemer et al., 2008, Berridge, 1998).

As part of being exhaustible, intracellular sources need to be replenished. Therefore our model implicitly required priming in order to be set up to produce  $Ca^{2+}$ -mediated persistent activity. We predict that interventions that reduce intracellular stores or prevent their replenishment would have an adverse effect on these mechanisms.  $Ca^{2+}$  handling is strongly affected by binding, made more complex by the existence of different binding proteins with different affinities and mobilities, many specific to particular cell types (Schwaller, 2010). In our highly simplified model, we considered only a single diffusible binding protein. Increased binding reduced calcium availability which led to reduced priming for persistent activity as well as less availability for its direct effects after stimulation.

# **4.2 Predictions**

Our model makes the following experimentally testable predictions.

- **1.** Relative activation of E and I neurons has indirect effects on excitability via  $Ca^{2+}$ mediated second-messenger cascades as well as direct effects. Testable with stimulation of different subsets of neurons (*i.e.*, E vs. I) using optogenetics (Tonnesen et al., 2009, Suter et al., 2014) while imaging calcium (and ideally cAMP as well).
- **2.** Stimulus-specific persistent activity is only viable in the presence of moderate inhibition. Excessive inhibition dampens activity and prevents calcium influx from enabling persistent activity. Disinhibition produces high cytosolic calcium levels in all neurons, causing all neurons to fire at high rates, and lose stimulus-specific information. Testable *in vitro* by regulating excitability of localized populations of

neurons via injectrode application of muscimol (GABA<sub>A</sub>R agonist) to increase inhibition or bicuculline/gabazine (GABA<sub>A</sub>R antagonists) to decrease inhibition.

**3.** In contrast to attractor network models that display a permanent up-state (Wang, 1999a, Wang, 2001), our model predicts that persistent activity will have a limited duration with an upper bound dictated by the multiple time constants associated with *Ca*2+ and cAMP regulation of HCN channels. Testable *in vitro* (Winograd et al., 2008) with intracellular recordings while providing tonic low-grade electrical stimulation followed by heightened stimulation to induce persistent activity, and measuring the duration of increased firing rates.

#### **4.3 Compensation, complementarity and synergy**

Nervous systems, and biological systems in general, utilize multiple pathways for critical functions. This multiplicity is the key to the adaptability and robustness of these complex systems. This seeming extravagance of mechanism can be arrayed along a spectrum from full redundancy at the one extreme, to the case where a separate system B with an entirely non-overlapping function can nonetheless be called into service to compensate when a system A is compromised or lost. Full redundancy provides a full backup copy – such redundancy may be present in the case of critical messenger peptides or proteins that might be produced without relevant variation from different genes to forestall disastrous mutation. Our simulations showed some degree of redundancy: activation of persistent activity depended on two stores of calcium. The internal store is potentially exhaustible; in case of failure, additional  $Ca^{2+}$  can be drawn from extracellular stores.

Systems that feature both compensation and complementarity rather than full redundancy are likely to be more common. Complementarity implies some degree of redundancy, but with major differences that give additional features and advantages. The simulations evinced complementarity in the ability of stronger excitatory mechanisms (Fig. 7b) to provide transfer of activation along the network circuitry, while large internal  $Ca^{2+}$  stores provide the substrate for activating the *I*h mechanism. Additionally, the different sources of cytoplasmic calcium, intra- and extracellular, each introduced different time courses of activation that could be utilized for nuanced learning algorithms based on relative degrees of activation of ionotropic and metabotropic glutamate receptors.

Moving further along this spectrum, we can consider to what extent these systems are synergistic, working together in a way that produces advantages that neither system would provide individually. We can infer synergy from the many points of interaction between the molecular and network mechanisms which demonstrate persistent activity. For example, excitation has its effects at two very different time scales associated with the mechanisms at different spatial scales. It has immediate effects on membrane potential to activate sets of cells. This activity can then be prolonged due to the relatively long voltage-dependent currents provided by NMDARs. Still slower and longer activations can then be provided by the molecular effects via IP<sub>3</sub> and interaction with internal stores. These activations work together synergistically, boosting the duration of persistent activity. This is still only the tip of this iceberg since the triggering of these multiple intracellular signaling pathways will produce subsequent interactions with the nucleus and genome.

The network showed emergent effects not predictable from the single neuron simulations, through recurrent network loops that provided both excitation and inhibition. Inhibition dominated in our baseline network, strongly reducing activity in non-stimulated cells. This feedback-driven inhibition provided our simulated network with an off switch to terminate persistent activity earlier than in the single cell. Truncating the activation would also ready a network to more quickly switch internal representations, and also provide energy-saving. Differences in wiring among different layers of cortex produced longer persistent activity in L2/3 and L6 compared to L5. These differences are likely to have functional consequences due to the different sources/targets of each layer's inputs/outputs (Hooks et al., 2011). Temporally precise interactions between excitatory and inhibitory neurons also produced alpha (14 Hz) oscillations (Lytton and Sejnowski, 1991, White et al., 2000, Neymotin et al., 2011), which shifted to beta (20 Hz) upon induction of persistent activity, due to the increased firing rates of stimulated excitatory neurons.

In addition to providing a memory mechanism, persistent activation in the network could enhance input/output for a column or for a layer in a column in a number of ways. Neurons in an activated layer are "prepared cells," with enhanced responsiveness to subsequent synaptic inputs due to having depolarized potentials nearer to threshold and having fast time constants that enable them to respond quickly to inputs (Bernander et al., 1991). We found that individual cortical layers could also be turned on into a persistent firing state (Fig. 7). An activated layer would better respond to inputs in order to route information to its distinct cortical and subcortical targets (Hunter et al., 2006, Fukushima et al., 2012, Schroeder and Lakatos, 2012, Kumar et al., 2013).

Similarly the major interlaminar route from L2/3 to L5 could be primed and set up to permit signal flow-through. In this respect our simulated network displayed *suppressive* and *facilitating* output modes (Fig. 7 left column). The switch between modes could be effected by neuromodulation by acetylcholine which can increase excitatory tone in neocortex (Carcea and Froemke, 2013, Hasselmo and McGaughy, 2004, Hsieh et al., 2000, Giocomo and Hasselmo, 2007). Excitatory strength determined the magnitude of L5 activation, the major cortical output layer for both intratelencephalic and descending outputs (Kiritani et al., 2012b, Yamawaki and Shepherd, 2015, Anderson et al., 2010). In suppressive mode (Fig. 7a left), targeted stimulation of L2/3 suppressed L5 via strong top-down inhibition from activated  $E2 \rightarrow I5L \rightarrow E5$  cells. In this mode, the cortical circuit might monitor signals arriving at L2/3, a major input layer (Petersen and Crochet, 2013) without passing that information on. Increasing  $E \rightarrow E$  synaptic weights shifted the network into a facilitating mode (Fig. 7b left), which activated the strong top-down excitatory projections from  $L/3 \rightarrow$ L5 (Fig. 7b left) (Weiler et al., 2008). The network model also showed that stimulation of all cortical layers together with  $E \rightarrow E$  augmentation, produced an additional degree of facilitation (Fig. 7b right).

The simulated network could also sense stimulus magnitude (Fig. 11) and duration (Fig. 8) in progressive levels of persistent activation providing further gradations of encoding. During tonic low-strength stimulation, the stimulated neurons displayed a gradual rise in

firing rates, which may allow the neurons to slowly accumulate stimulus-related evidence. As stimulus-related evidence gathers in competing neuronal assemblies, the assembly with the highest firing rate could dominate cognitive representations (winner-take-all) or multiple assemblies could remain active to varying degrees.

The model demonstrated repeatable persistent activity patterns which could contribute to identifiable features of neural representation and memory function in vivo. Stimulation caused activation of an ensemble, which then represented the pattern in a reproducible ensemble activation pattern across the network (Fig. 9). This dynamic representation could be utilized as a form of short-term memory via ensemble encoding for a particular stimulation pattern (Durstewitz et al., 2000, Goldman-Rakic, 1995, Quiroga and Panzeri, 2009, Ghitza, 2011, Barbieri et al., 2005).

### **4.5 Inter-scale interactions produce persistent activity**

Many prior models of persistent activity have focused only on cellular, or only on network, dynamics. Our model is unusual in that we develop a multiscale composite of a subcellularscale model of calcium-induced calcium release (CICR) (Neymotin et al., 2015), a cellularscale model of hyperpolarization-activated graded persistent activity based on *I*h modulation (Winograd et al., 2008), and a network-scale neocortical model (Neymotin et al., 2011a, Chadderdon et al., 2014, Neymotin et al., 2011). The multiscale model demonstrates many points of inter-scale interaction that would not be fully captured by a series of simplifications, encapsulations and embeddings, such as the classical approach of the pointneuron approximation with its simple input/output function. Due to the inter-scale interactions, our cellular model showed additional dynamics based on the endoplasmic reticulum's role in  $Ca^{2+}$  handling. Inter-scale interactions are perhaps most clearly seen where network effects meet  $Ca^{2+}$  effects at the nexus of  $I<sub>h</sub>$ : calcium control of HCN is preparatory for *I*h activation through relative hyperpolarization from inhibitory network effects. The network model largely followed the pattern of activity set by the cellular model, but showed additional features due to the complexities of multiple types of inputs, to the competing roles of excitation and inhibition, and to the complexity of inter-laminar wiring.

*I*h, appears to have a major role to play in the dynamics of both cells and networks. In addition to the role in providing persistent activity, it also has large effects in maintaining resting potential, augmenting somatic sub-threshold resonance, and determining dendritic subthreshold responses (Accili et al., 2002, Chen et al., 2001, Santoro and Baram, 2003, Zemankovics et al., 2010, Dyhrfjeld-Johnsen et al., 2008, Dyhrfjeld-Johnsen et al., 2009, Poolos et al., 2002). Further complexity at the network levels, not explored in this study, arises from inhomogeneous distributions of HCN isoforms and HCN density in different cell types, differential dendritic expression in pyramidal neurons and colocalization with other ion channels (Accili et al., 2002, Aponte et al., 2006, Bender et al., 2001, Santoro and Baram, 2003). Additionally *I*h is under subtle second messenger control, likely through more than the one effect used in this model. Multiple functions, multiple types, and multiple routes for modulation make HCN channels potent control points in the circuit.

Our model is consistent with a variety of experiments which have demonstrated that *I*<sup>h</sup> contributes to neuronal persistent activity: calcium regulates HCN channels and firing

dynamics in cat sensorimotor cortex neurons (Schwindt et al., 1992); blocking *I*<sup>h</sup> pharmacologically with ZD7288 abolishes persistent activity in supra- and infra-granular pyramidal neurons from prefrontal cortex of ferrets and guinea pigs (Winograd et al., 2008), and in mouse prefrontal cortex pyramidal neurons (Thuault et al., 2013); HCN channels dynamically regulate resting membrane potential and cellular excitability (Thuault et al., 2013, Neymotin et al., 2013) after neuromodulators increase *I*h (Heys and Hasselmo, 2012, Tsuno et al., 2013, Wang et al., 2007). However, cAMP reduced persistent activity in primates suggesting that it also has plays some countervailing roles (Arnsten et al., 2010, Wang et al., 2007). cAMP controls a number of other channels and other cytosolic processes that were not included in our model, including augmentation of  $K^+$  flux (*e.g.*, KCNQ) that would reduce cellular excitability (Arnsten and Jin, 2012). HCN channels and certain voltage-sensitive  $K^+$  channels  $(Kv)$  are colocalized along the apical dendrites (Harnett et al., 2013) which would allow HCN and  $K^+$  channels to interact competitively, with HCN channels contributing to a neuronal excitability dampened by Kv (Poolos et al., 2002, Migliore and Migliore, 2012). Overall effects would then depend on relative sensitivity to cAMP, which could be effected through a level of meta-modulation via both intrinsic factors and external neuromodulators.

In the current study, we see how a persistent activity attractor landscape can be formed by complementing the effects of mutual excitation with the multiple complementary effects of excitatory and inhibitory interactions across cortical layers (Papoutsi et al., 2013, Papoutsi et al., 2014, Nelson et al., 2003, Marder et al., 1996). By contrast, Wang's "bump attractor" network model was based on localized connectivity in a single layer of integrate-and-fire neurons (Compte et al., 2000, Wang, 2001). That model produced persistent activity through reverberant NMDAR excitatory activation. In that model NMDAR activation outlasted the effects of fast  $GABA_A$  activation, with no slower effects from slower dendritic  $GABA_A$  or from  $GABA_B$  inputs. Although adding many features, our model is generally consistent with the Wang model, since it demonstrates the importance of excitatory tone in shaping the network's response to targeted stimulation and eliciting interlayer activity propagation. However, a major difference from the bump attractor model is that our network wiring has cortical layering (y-direction) as the major geometrical feature in addition to minor lateral fall-off in connectivity (x-z plane). Our network therefore did not produce enhanced activation of a highly localized subset of strongly interconnected cells – the localized bump.

We attempted to include major neurobiological features that would allow us to assess the many inter-scale interactions that make the dynamics of the local neocortical network so complex and so fascinating. We necessarily left out many important features, both due to computational limitations and due to the fact that many of these are not understood in sufficient detail for us to adequately portray. Additionally, we of course left out many *unimportant* features, a key role of modeling being to eventually determine which are the important and which the unimportant parameters related to a given functional outcome. Additional features that would be valuable to more fully understand persistent activity include *ICAN* cationic currents (Egorov et al., 2002, Tiganj et al., 2015), persistent sodium channels (Oikonomou et al., 2014, Zhou et al., 2015), and neuromodulatory synaptic receptors such as acetylcholine and dopamine (Sawaguchi and Goldman-Rakic, 1991,

Sidiropoulou et al., 2009). A further omitted feature that is believed to be important is the aforementioned distribution of HCN isoforms by cell type and location. An additional unexplored consideration is our limited approximation of  $Ca^{2+}$  handling due to the use of homogeneous diffusion that does not incorporate the important roles of localized subdomains due to molecular barriers, fixed buffers, and colocalizations of targets. Incorporation of some of these considerations will bring us near to the domain of molecular dynamics, a further scale of exploration that remains to be incorporated at some, perhaps remote, future date.

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# **Abbreviations**



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## **Figure 1. Model schematics**

**(A) Schematic of neocortical network architecture.** Red rectangles represent populations of 5-compartment excitatory cells (largest rectangle represents soma, 3 apical-dendrite compartments point upward, basal dendrite compartment points downward); green circles represent fast-spiking interneurons; blue ellipses represent low-threshold firing interneurons. Lines (with arrows) indicate connections between the populations. E cells synapse with AMPAR/NMDARs; I cells synapse with  $GABA_AR / GABA_BRs$ . Filled circles represent  $GABA_A R / GABA_R Rs$ . Open circles and rectangles represent AMPAR/NMDARs. (B) Schematic of chemical signaling in pyramidal cells showing fluxes (black arrows) and second- (and third- *etc*) messenger modulation (red back-beginning arrows). We distinguish membrane-associated ionotropic and metabotropic receptors and ion channels involved in reaction schemes in red (in reality, it is likely that almost every membrane-bound protein is modulated). External events are represented by yellow lightning bolts – there is no extracellular diffusion; the only extracellular reaction is glutamate binding, unbinding and degradation on mGluR1 after an event.  $Ca^{2+}$  is shown redundantly in blue – note that there is only one  $Ca^{2+}$  pool for extracellular, 1 pool for cytoplasmic, and 1 pool for ER. (PLC: phospholipase C, DAg: diacyl-glycerol, cAMP: cyclic adenosine monophosphate; PIP<sub>2</sub>: phosphatidylinositol 4,5-bisphosphate).



**Figure 2. Simulation of a single neuron with high (blue; 1** *μ***m) and low (red; 300** *μ***m) spatial resolution shows similar calcium concentrations**

Calcium concentration is displayed as a function of position along the apical dendrite at four different times in the simulation (time from top to bottom). Excitatory stimulus at 10 s admits  $Ca^{2+}$  into the cytosol.



# **Figure 3. Pyramidal cell HCN channel activation**

(a) Steady-state HCN channel activation as a function of  $Ca^{2+}$  and  $V_{memb}$ . Vertical lines are levels by color in **(b)**. **(b)** *Ihm* voltage-dependence shifts right- and upward with increasing Ca2+. red: baseline at 100 nM; green: 2 *μ*M; blue: 12 *μ*M. Maximum steady-state activation is 2 because the second open state has twice the conductance of the first open state. At resting  $Ca^{2+}$  maximum steady state activation is 1.



#### **Figure 4. Isolated L5 pyramidal neuron model demonstrates persistent increase in firing after stimulation to AMPAR/NMDAR/mGLUR via** *a* **–** *h* **sequence of coupled electrical-molecularelectrical activations**

(soma levels in blue; apical dendrite levels in red, except in *a*) **(a)** Synaptic currents in apical dendrite (blue: GABAAR; red: AMPAR; green: NMDAR) **(b)** produces cytosolic calcium concentration increase due to calcium influx via VGCC and NMDAR, **(c)** while also increasing IP<sub>3</sub> via mGluR-activated cascade, **(d)** which together with Ca<sup>2+</sup> activates IP<sub>3</sub>R causing efflux of ER Ca<sup>2+</sup>. **(e)** cAMP is augmented by higher Ca<sup>2+</sup> **(f)** persistently increasing normalized HCN conductance  $(g_h)$  (g) persistently increasing  $I_h$ . (soma values out of range due to lower HCN density) **(h)** resulting in high rate of firing.





**(a)** Raster plot of spike times (red: PYR, blue: LTS, green: FS cells) **(b)** Multiunit activity (MUA; thick: 100 ms bin; thin: 10 ms bin) for stimulated E neurons (light-blue), nonstimulated E neurons (purple), interneurons (gray). (Stimulation added to background activation between black lines: 180× weight 500 Hz Poisson process.)



**Figure 6. Stimulation produces both Ca2+ influx and release from intracellular stores** Stimulated E5 cell averages (light-blue) vs. non-stimulated E5 cell averages (purple). **(a)**  Transient cytosolic Ca2+ rise. **(b)** ER calcium depletion (non-stim value out of range). **(c)**  Buffered  $Ca^{2+}$  increases in stimulated. Decrease in non-stimulated due to reduced influx with hyperpolarization. **(d)** cAMP. **(e)** Normalized HCN conductance (*gh*).



**Figure 7. Targeted stimulation of individual layers produces localized persistent activity**

Activation duration of L5 cell with L5 input  $\sim$ 30-40 s, considerably less than the  $\sim$ 60 s activation duration seen in isolated L5 cell. (Layer simulation locations indicated at top of each column. Layer activity by color:  $E2 - red$ ;  $E5 - green$ ;  $E6 - black$ ; inhibitory LTS cells in L5 – gray; within-layer non-stimulated cells – purple; stimulated cells all layers – lightblue in right column.) **(a)**: Baseline network shows no interlaminar excitatory spread for any single layer stimulation. Layer 2/3 stimulation produces spread to L5 inhibitory cells producing reduction in firing in L5. **(b)**: Augmented excitatory connectivity within the network (no change in strength of stimulation or background drive) produces increased durations (except paradoxical decrease with L5 stimulation) and spread of excitation from L2/3 to L5. With all-layer stimulation (right column) some spread of excitation to nonstimulated cells is also seen (purple line). (MUAs with 1000 ms bins; 75 neurons stimulated in each layer. Vertical dotted lines at times where rates drop < 10 Hz.)



**Figure 8. Longer-duration weak stimulation produces firing-rate distinctions**

Stimuli were 0.1× baseline strength used in other figures. **(a)** MUAs in response to 1 s stimulus. **(b)** MUAs in response to 20 s stimulus. **(c)** FRD in response to 1–20 s stimulus durations (red dots from **(a)**, **(b)**) (50% E cells all layers; MUAs with 1000 ms bins of stimulated: light-blue; non-stimulated: purple)



#### **Figure 9. Network ensemble dynamics show distinct states at baseline and during expression of persistent activity**

**(a)** Persistent activity lasts >60 s after each identical AMPAR/NMDAR/mGLUR stimulation. Vertical lines represent the stimulus times (60, 185 s; same population of 50% of E neurons across layers). MUA created with 1 s bins. Purple (light-blue) represent stimulated (non-stimulated) E neurons; gray MUA of interneurons. **(b)** Firing-rate vectors (1 s intervals) transition at onset/offset of persistent activity. Color at time= *x*, neuron= *y*  represents the firing rate of neuron *y* during the 1 s interval at time *x*. Neurons arranged in layers from top (L2/3) to bottom (L6). **(c)** Pairwise Pearson correlations between all firing rate vectors from **(b)**. Color at times  $t_1 = x$ ,  $t_2 = y$  indicates Pearson correlation between firing-rate vectors at those times.



**Figure 10. Modulating E**→**I (15 levels) and I**→**E (8 levels) synaptic weights shapes firing rates and intracellular molecular activations**

**(a)** Interneuron and **(b)** excitatory neuron firing rates after stimulation. **(c)** Peak cytosolic calcium (mM) in stimulated excitatory cells. **(d)** cAMP and **(e)** *gh* of stimulated E cells. **(f)**  Stimulated to non-stimulated *gh* ratio. **(g)** FRD (firing-rate distinction). **(h)** FRD as a function of network inhibition estimated by  $E \rightarrow I \times I \rightarrow E$  (16 s simulations; color indicates average ratio of *gh* in stimulated P1 vs non-stimulated P2 populations).



**Figure 11. Persistent activity can be induced via either AMPAR/NMDAR (external stores) or mGLUR (internal store) activation**

AMPAR/NMDAR and mGLUR stimulus strength were each varied independently from 0-3× baseline ( $n = 31$ ), while holding the other stimulus strength constant at 1× baseline. **(a)** Average cytosolic calcium in the 5 s after stimulus as a function of stimulus strength of AMPAR/NMDAR (circles) and mGLUR (triangles). **(b)** Ratio of stimulated to nonstimulated population firing rates (FRD) as a function of stimulus strength of AMPAR/ NMDAR (circles) and mGLUR (triangles).



**Figure 12. Firing-rate distinction depends on both external (VGCC) and internal (ER) calcium stores, determined respectively by voltage-gated calcium channels (VGCC) density and ER**   $[Ca^{2+}]$ 

(a)  $N = 33621$  s simulations were run varying the density of VGCCs (x-axis) from 0–0.015  $nS/cm<sup>2</sup>$  ( $n = 16$  levels), and the concentration of calcium in the ER (y-axis) from 0–2.8 mM (*n* = 21 levels). **(b–d)** Differences in MUA (light blue: stimulated; purple: non-stimulated; bin size 100 ms) and FRD; examples taken from four corners of **(a)**. **(b)** High internal stores (upper left of Fig. 12): Absence of VGCCs (0.0) with high ER calcium concentration (2.8 mM) allows for high FRD (26.48); **(c)** High internal and external stores (upper right of Fig. 12): High density of VGCCs (0.015 nS/*cm*<sup>2</sup> ) with high ER calcium (2.8 mM) produces moderate FRD (4.48); **(d)** No  $Ca^{2+}$  stores (lower left of Fig. 12): Absence of VGCCs with zero initial ER calcium produces low FRD (0.97); **(e)** High external stores (lower right of Fig. 12): High density of VGCCs (0.015 *nS*/*cm*<sup>2</sup> ) with zero initial ER calcium produces moderate FRD (2.35).



**Figure 13. Slowing calcium extrusion pump allows retention of**  $Ca^{2+}$  **and increases firing-rate distinction (FRD)**

**(a)** Average calcium concentration (left y-axis) averaged over 5 s post-stimulus. for stimulated (light-blue) and non-stimulated (purple) populations. Black points (right y-axis) show ratio. **(b)** Firing-rate distinction (FRD) as a function of pump speed.  $(n = 40)$ 



# **Figure 14.**  $Ca^{2+}$  buffering alters free  $Ca^{2+}$  availability for modulation of  $I<sub>h</sub>$

Forward rate (FRate) of binding (x-axis) and buffer concentration (y-axis) varied. **(a)**  Cytosolic calcium transient in response to stimulus. **(b)** HCN activation (*gh*) in response to stimulus. **(c)** Firing-rate distinction: average ratio of firing rate of stimulated population to non-stimulated population during 5 s interval after stimulus. ( $n = 16 \times 16$ )

#### **Table 1**

Baseline parameters.



 $g_{IP3R} = 120400.0$  molecules/mM/ms

 $k_{IP3} = 0.00013$  mM

 $k_{act} = 0.0004 \text{ mM}$ 

 $k_{inh} = 0.0019 \text{ mM}$ 

*gleak* = 18.06 molecules/mM/ms

*gserca* = 1.9565 molecules/ms

*kserca* = 0.0001 mM

 $\tau_{IP3} = 1000 \text{ ms}$ 

 $\tau_{IP3R} = 400$  ms

 $\tau_{ex}$  = 5 ms

 $DCa_{cyt}^{2+} = 0.08 \ \mu m^2$ /ms

 $DCa_{ER}^{2+} = 0.08 \ \mu m^2/\text{ms}$ 

 $D_{IP_3} = 1.415 \ \mu m^2 \text{/ms}$ 

 $D_B = 0.043 \ \mu m^2 \text{/ms}$ 

 $D_{CaB} = 0.043 \ \mu m^2 / \text{ms}$ 

 $FRate = 5ms^{-1}mM^{-1}$ 

 $BRate = 9.5 \times 10^{-4} \text{ms}^{-1}$ 

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# **Table 2**

Network Connectivity.  $\bar{p}_{ij}$  and  $w_{ij}$  are distance-independent probability of connections from Pre to Post neuronal types and synaptic weights, respectively.





# **Table 3**

Parameters for modeling background activity. Dend indicates inputs to all dendritic compartments, consistent with experiments (Chen et al., 2013). Background inputs were not applied to GABABR synapses.



# **Table 4**

Firing rate correlation vectors demonstrate distinct network states. Baseline and Persistent indicate baseline activity and persistent activity states, respectively. Average Pearson correlations ± standard deviation for all pairs of firing rate vectors across states are reported.  $\times$  indicates value reported above.

