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Relative ^{11}C -PiB Delivery as a Proxy of Relative CBF: Quantitative Evaluation Using Single-Session ^{15}O -Water and ^{11}C - PiB PET

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Abstract

The primary goal of this study was to assess the suitability of ^{11}C -Pittsburgh compound B (^{11}C -PiB) blood–brain barrier delivery (K_1) and relative delivery (R_f) parameters as surrogate indices of cerebral blood flow (CBF), with a secondary goal of directly examining the extent to which simplified uptake measures of ^{11}C -PiB retention (amyloid- β load) may be influenced by CBF, in a cohort of controls and patients with mild cognitive impairment (MCI) and Alzheimer disease (AD).

Methods—Nineteen participants (6 controls, 5 AD, 8 MCI) underwent MR imaging, ^{15}O -water PET, and ^{11}C -PiB PET in a single session. Fourteen regions of interest (including cerebellar reference region) were defined on MR imaging and applied to dynamic coregistered PET to generate time–activity curves. Multiple analysis approaches provided regional ^{15}O -water and ^{11}C -PiB measures of delivery and ^{11}C -PiB retention that included compartmental modeling distribution volume ratio (DVR), arterial- and reference-based Logan DVR, simplified reference tissue modeling 2 (SRTM2) DVR, and standardized uptake value ratios. Spearman correlation was performed among delivery measures (i.e., ^{15}O -water K_1 and ^{11}C -PiB K_1 , relative K_1 normalized to cerebellum [$\text{Rel-}K_{1\text{-Water}}$ and $\text{Rel-}K_{1\text{-PiB}}$], and ^{11}C -PiB SRTM2- R_f) and between delivery measures and ^{11}C -PiB retention, using the Bonferroni method for multiple-comparison correction.

Results—Primary analysis showed positive correlations ($\rho \approx 0.2\text{--}0.5$) between ^{15}O -water K_1 and ^{11}C -PiB K_1 that did not survive Bonferroni adjustment. Significant positive correlations were found between $\text{Rel-}K_{1\text{-Water}}$ and $\text{Rel-}K_{1\text{-PiB}}$ and between $\text{Rel-}K_{1\text{-Water}}$ and ^{11}C -PiB SRTM2- R_f (ρ

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DISCLOSURE

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$\approx 0.5\text{--}0.8$, $P < 0.0036$) across primary cortical regions. Secondary analysis showed few significant correlations between ^{11}C -PiB retention and relative ^{11}C -PiB delivery measures (but not ^{15}O -water delivery measures) in primary cortical areas that arose only after accounting for cerebrospinal fluid dilution.

Conclusion— ^{11}C -PiB SRTM2- R_f is highly correlated with regional relative CBF, as measured by ^{15}O -water K_1 normalized to cerebellum, and cross-sectional ^{11}C -PiB retention did not strongly depend on CBF across primary cortical regions. These results provide further support for potential dual-imaging assessments of regional brain status (i.e., amyloid- β load and relative CBF) through dynamic ^{11}C -PiB imaging.

Keywords

amyloid; blood flow; PiB PET; Alzheimer's disease; kinetic modeling

The development of β -amyloid (A β) plaque imaging agents, such as ^{11}C -Pittsburgh compound B (^{11}C -PiB), for PET has enabled measurement of A β deposition in living humans (1–3). These studies demonstrated 2-fold-greater ^{11}C -PiB cortical retention in Alzheimer disease (AD) patients (relative to cognitively normal controls), evidence of A β deposition in 50%–70% of patients with mild cognitive impairment (MCI) (4,5), and elevated ^{11}C -PiB retention in 10%–30% of elderly controls (average age, 64–74 y) (2,4,6–10).

Despite a multitude of ^{11}C -PiB studies, few were fully quantitative kinetic modeling studies (11–13) because this involves invasive arterial blood sampling and long scan duration that can be burdensome for subjects, and simplified PET methodologies were found to provide assessments of A β load that are consistent with quantitative outcomes (14,15).

Fully quantitative PET studies provide important information needed to evaluate radiotracer kinetics (e.g., blood–brain barrier radioligand delivery [K_1], specific binding [k_3]) and strengths and limitations of more feasible semiquantitative methods (e.g., reference Logan, simplified reference tissue model [SRTM], multilinear reference tissue model [MRTM], and standardized uptake value tissue ratios [SUVRs]) (14–18).

Meyer et al. reported on dual-biomarker imaging with ^{11}C -PiB using the 2-step SRTM method (SRTM2) to assess both A β plaque load and regional relative radioligand delivery R_f , showing good correlation between ^{11}C -PiB SRTM2- R_f and ^{18}F -FDG SUVR (40–60 min after injection) (19). Meyer et al. concluded that ^{11}C -PiB can provide information on not only A β load but also neuronal activity and neurodegeneration through SRTM2- R_f .

Van Berckel et al. recently examined longitudinal changes in ^{11}C -PiB retention using voxel-based parametric approaches, ranging from SUVR to a voxel-level reference tissue analog of SRTM2 (RPM2) and found sensitivity of longitudinal changes in ^{11}C -PiB SUVR to changes in flow (20).

The primary goal of this study was to clarify, through quantitative evaluation of ^{15}O -water and ^{11}C -PiB delivery parameters, the extent to which ^{11}C -PiB SRTM2- R_f can be a robust surrogate index of relative cerebral blood flow (CBF). Secondarily, regional relationships

between ^{15}O -water and ^{11}C -PiB delivery parameters and ^{11}C -PiB retention were examined to further clarify independence between these measures, on a cross-sectional basis, particularly for simplified retention measures.

MATERIALS AND METHODS

Human Subjects

Nineteen subjects (6 controls, 8 MCI, 5 AD) were recruited, as previously described (13,15). Subject characteristics are shown in Table 1. This study was approved by the local Institutional Review Board, and informed consent was obtained from all subjects or their caregivers. Some ^{11}C -PiB PET results were previously published (8,13,15,17) with exceptions noted below. The basic imaging methodology is described below, with further details in earlier publications (13,15,21).

Imaging

MR imaging (spoiled-gradient recalled sequence) was performed on a 1.5-T Signa (GE Healthcare) scanner for region-of-interest (ROI) definition and determination of atrophy-related cerebrospinal fluid (CSF) dilution. A Siemens/CTI ECAT-HR+ PET scanner was used with a Neuro-insert (CTI PET Systems), as previously reported (13). PET corrections included scanner normalization, deadtime, attenuation, scatter, random coincidences, and radioactive decay. PET data were reconstructed by filtered backprojection (direct Fourier method; final spatial resolution, ~6 mm).

^{15}O -water was synthesized using a mixed gas flow system, trapped in saline solution (5–7 mL), and administered as a rapid bolus (444 MBq) using an automated injector system, with simultaneous initiation of a 3-min 20-frame dynamic acquisition (10×3 , 3×10 , 4×15 , and 3×20 s). Ten minutes after ^{15}O -water imaging, a transmission scan ($^{68}\text{Ge}/^{68}\text{Ga}$ rods) was acquired. ^{11}C -PiB, synthesized as previously described (13), was administered as a slow 20-s bolus (~500 MBq, 50 GBq/ μmol) with simultaneous start of a 90-min 34-frame dynamic acquisition (4×15 , 8×30 , 9×60 , 2×180 , 8×300 , and 3×600 s).

Plasma input functions were determined using dynamic arterial blood sampling (radial artery) performed over 3.5 min for ^{15}O -water using a Siemens Liquid Activity Monitoring System and over 90 min for ^{11}C -PiB by manual collection of 35 samples (0.5 mL), with 20 collected within 2 min and 5–6 additional samples (2–3 mL) collected over the study, to measure radiolabeled metabolites.

Image Processing and ROI Definition

The ^{15}O -water and ^{11}C -PiB PET data were separately coregistered to MR images using automated registration methods (22,23), as described previously (15,24). The ^{15}O -water and ^{11}C -PiB data were integrated over the initial 3 and 15 min, respectively. Each integrated PET image was aligned to a MR image, and the MR image was resliced to match PET space ($128 \times 128 \times 63$; pixel size, $2.06 \times 2.06 \times 2.43$ mm).

ROIs were manually defined on coregistered MR images using criteria that resulted in higher reliability (24). ROIs included anterior cingulate gyrus (ACG), anterior ventral striatum

(AVS), cerebellum (CER), frontal cortex (FRC), lateral temporal cortex (LTC), mesial temporal cortex (MTC), occipital cortex (OCC), occipital pole (OCP), parietal cortex (PAR), pons (PON), precuneus (PRC), sensorymotor cortex (SMC), subcortical white matter (SWM), and thalamus (THL). A global cortical region (CTX5) was defined as the voxel-weighted average of ACG, FRC, LTC, PAR, and PRC (primary cortical regions). ROIs were applied to sample dynamic PET data and generate regional time–activity curves. CER was used as the reference region to approximate the kinetics of nondisplaceable (ND) uptake and defined to minimize white matter uptake and spillover effects from OCC. For ^{15}O -water, CER was also used as a reference, because it is less prone to age-related atrophy and changes in CBF (25).

Data Analysis

^{15}O -water data were analyzed using a 1-tissue compartment model with iterative curve-fitting to estimate ^{15}O -water K_1 ($\text{mL cm}^{-3} \text{min}^{-1}$) and brain efflux k_2 (min^{-1}), while accounting for input function timing delays, as previously described (21). In this work, $K_{1\text{-Water}}$ was used as a direct index of CBF (i.e., $K_{1\text{-Water}} = F \times E = F \times [1 - e^{-\text{PS}/F}]$, where E = extraction fraction, F = CBF, and PS = permeability surface area product), although limitations in ^{15}O -water single-pass extraction (~90%) are well known (26). Relative $K_{1\text{-Water}}$ ($\text{Rel-}K_{1\text{-Water}}$) was computed regionally as the $K_{1\text{-Water-ROI}}$ -to- $K_{1\text{-Water-CER}}$ ratio.

Multiple modeling approaches were used to analyze ^{11}C -PiB. As previously described (13,15), a 2-tissue, 4-parameter compartment model (2T-4k), Logan analysis (using arterial [ART90] or cerebellar reference [CER90] [90 is the total length of the scan, 90 min] data as input), and SRTM2 were applied (15). SRTM2 was applied by constraining k_2' (reference tissue clearance rate) to the mean of the k_2' values initially determined using SRTM across all ROIs except CER for each subject.

For the primary analysis, ^{11}C -PiB delivery measures were obtained from compartmental modeling, including $K_{1\text{-PiB}}$ and relative $K_{1\text{-PiB}}$ ($\text{Rel-}K_{1\text{-PiB}} = K_{1\text{-PiB-ROI}}$ -to- $K_{1\text{-PiB-CER}}$ ratio), and SRTM2- R_1 (representing $K_{1\text{-PiB-ROI}}$ -to- $K_{1\text{-PiB-CER}}$ ratio). For the secondary analysis, ^{11}C -PiB retention measures were based on 2T-4k distribution volumes (i.e., $V_T = K_1/k_2[1 + k_3/k_4]$) used to compute distribution volume ratios (DVR), that is, $\text{DVR} = V_{T\text{-ROI}}/V_{T\text{-CER}} = \text{BP}_{\text{ND}} + 1$, where BP_{ND} (binding potential nondisplaceable) is directly related to density of available binding sites (B_{avail}) and radioligand affinity (27). DVR was computed using the 2T-4k model, Logan analysis, and SRTM2 (i.e., $\text{BP}_{\text{ND}} + 1$). ^{11}C -PiB retention was also measured using SUVs measured over 50–70 min after injection ($\text{SUV}_{\text{ROI}} = \text{SUV}_{\text{ROI}}/\text{SUV}_{\text{CER}}$ (15)).

The delivery and ^{11}C -PiB retention measures were adjusted for dilutional effects of expanded CSF spaces, using an MR imaging–guided approach routinely used at our site (28,29). Most processing and analysis software was developed and validated in-house, except for SRTM/SRTM2 analyses performed in PMOD 3.204 (PMOD Technologies Ltd.). Parametric images were generated for $\text{Rel-}K_{1\text{-Water}}$ using a voxel-based in-house implementation of the 1-tissue model, and SRTM- R_1 and DVR images were generated using PMOD.

Statistical Methods

Descriptive statistics included mean \pm SD or counts, as appropriate. Relative SD (RSD, expressed as percentages) was calculated for delivery measures to assess differences in intersubject variability. Group differences in subject characteristics were determined using the Kruskal–Wallis test, with the Mann–Whitney U test for post hoc comparisons. The Bonferroni method was used for multiple-comparison correction.

Relationships between outcome measures were examined using Spearman correlation, on a region-by-region basis across all subjects. The primary correlations were between measures of CBF and ^{11}C -PiB delivery ($K_{1-\text{Water}}$ vs. $K_{1-\text{PiB}}$, $\text{Rel-}K_{1-\text{Water}}$ vs. $\text{Rel-}K_{1-\text{PiB}}$, $\text{Rel-}K_{1-\text{Water}}$ vs. ^{11}C -PiB $\text{SRTM2-}R_I$, and $\text{Rel-}K_{1-\text{PiB}}$ vs. ^{11}C -PiB $\text{SRTM2-}R_I$). Secondary correlations were between delivery parameters ($K_{1-\text{Water}}$, $\text{Rel-}K_{1-\text{Water}}$, $\text{Rel-}K_{1-\text{PiB}}$, and ^{11}C -PiB $\text{SRTM2-}R_I$) and ^{11}C -PiB retention (2T-4k-DVR, ART90-DVR, CER90-DVR, $\text{SRTM2-}R_I$, and SUVR70). Correlations were performed with and without CSF dilution adjustment. All analyses were 2-sided and underwent Bonferroni adjustment where appropriate. Statistical analyses were performed using SPSS 20.0.0 (IBM Corp.).

RESULTS

Subjects and CSF Correction

Neither age nor education was significantly different across subject groups (Table 1). Mini Mental State Examination (MMSE) scores were significantly different ($P = 0.010$). Post hoc analysis showed higher MMSE for controls than AD ($P = 0.009$) and higher MMSE for MCI than AD ($P = 0.011$), which survived Bonferroni adjustment. CSF dilution factors (Supplemental Table 1; supplemental materials are available at <http://jnm.snmjournals.org>) were not significantly different across subject groups, after Bonferroni adjustment, as previously reported (15).

Delivery Parameters

Table 2 shows mean regional delivery parameters. On average, $K_{1-\text{PiB}}$ was 40%–50% lower than $K_{1-\text{Water}}$ for most ROIs. In contrast, average relative ^{15}O -water and ^{11}C -PiB delivery parameters were more similar. Supplemental Figure 1 plots $K_{1-\text{Water}}$ and $K_{1-\text{PiB}}$ for primary cortical ROIs, CER, and PON grouped by diagnosis. Comparison of RSD for absolute and relative delivery measures generally revealed lower intersubject variability for relative delivery, including primary cortical regions in which RSD was 4.1%–6.3% lower for $\text{Rel-}K_{1-\text{Water}}$ than for $K_{1-\text{Water}}$ and 4.1%–8.6% lower for $\text{Rel-}K_{1-\text{PiB}}$ than for $K_{1-\text{PiB}}$. The ^{11}C -PiB $\text{SRTM2-}R_I$ RSD was 0.4%–3.8% lower than that for the $\text{Rel-}K_{1-\text{PiB}}$.

Figure 1 visually shows the relationship between CTX5 delivery parameters. Figure 2 shows example parametric images of $\text{Rel-}K_{1-\text{Water}}$ and ^{11}C -PiB $\text{SRTM-}R_I$ and DVR for an AD subject, demonstrating similar regional distribution for $\text{Rel-}K_{1-\text{Water}}$ and ^{11}C -PiB $\text{SRTM-}R_I$.

Table 3 lists correlations between ^{15}O -water and ^{11}C -PiB delivery parameters (adjusted for CSF dilution). Correlations between $K_{1-\text{Water}}$ and $K_{1-\text{PiB}}$ were low to moderate ($\rho \approx 0.2$ – 0.5) and mostly not significant after Bonferroni adjustment. Stronger correlations ($\rho \approx 0.5$ – 0.8)

were observed between $\text{Rel-}K_{1\text{-Water}}$ and $\text{Rel-}K_{1\text{-PiB}}$ (significant for most cortical ROIs after Bonferroni adjustment), with more ROIs showing significant correlation between $\text{Rel-}K_{1\text{-Water}}$ and $^{11}\text{C-PiB SRTM2-}R_f$. Highest correlations ($\rho \approx 0.8\text{--}0.9$, $P < 0.001$) were observed between relative $^{11}\text{C-PiB}$ delivery parameters ($\text{Rel-}K_{1\text{-PiB}}$ and $^{11}\text{C-PiB SRTM2-}R_f$). Correlation between $^{15}\text{O-water}$ and $^{11}\text{C-PiB}$ delivery measures without CSF dilution correction yielded similar results (data not shown).

Delivery and Retention Measures

Table 4 shows mean $^{11}\text{C-PiB}$ retention measures for CTX5 that are consistent with previously described group differences (30). Correlations between delivery parameters and $^{11}\text{C-PiB}$ retention for CTX5 are shown in Table 5, noting lack of significant correlations after Bonferroni adjustment. Full correlation results between delivery parameters and $^{11}\text{C-PiB}$ retention are shown in Supplemental Table 2. Correlations between $K_{1\text{-Water}}$ and $^{11}\text{C-PiB}$ retention (CSF-adjusted) were generally negative and low and lacked statistical significance in primary cortical regions. Similar correlations were present when $K_{1\text{-Water}}$ and $^{11}\text{C-PiB}$ retention were not CSF-adjusted (data not shown). In contrast, statistically significant correlations were evident but variable between $^{11}\text{C-PiB}$ relative delivery and retention, mostly with nonarterial-based retention measures (CER90-DVR, SUVR70, SRTM2-DVR; Supplemental Table 2). ACG was the only primary cortical region that showed significant correlations (after Bonferroni adjustment) between relative $^{11}\text{C-PiB}$ delivery and retention measures ($\rho \approx 0.8\text{--}0.9$, $P < 0.001$). In contrast, without CSF dilution adjustment, no significant correlations were found between $^{11}\text{C-PiB}$ delivery and retention (after Bonferroni adjustment, data not shown).

DISCUSSION

This study focuses on single-session PET measurements of both quantitative CBF and $\text{A}\beta$ plaque binding in controls, MCI, and AD subjects. The results show statistically significant correlations between relative delivery parameters of $^{15}\text{O-water}$ and $^{11}\text{C-PiB}$ PET (i.e., $\text{Rel-}K_{1\text{-PiB}}$ and $\text{SRTM2-}R_f$) and lower trend level correlation between $K_{1\text{-Water}}$ and $K_{1\text{-PiB}}$ for primary cortical regions. Secondly, minimal significant correlations were found between measures of delivery and $^{11}\text{C-PiB}$ retention.

It is well established that the capacity of any radioligand to reflect specific binding is limited if ligand binding is rapid relative to ligand delivery from blood to brain (i.e., $k_3 \gg K_1$ and delivery-limited). This was not the case for $^{11}\text{C-PiB}$, with early results showing a K_1 of $0.22\text{--}0.23 \text{ mL cm}^{-3} \text{ min}^{-1}$ (13), relative to k_3 of $0.04\text{--}0.05 \text{ min}^{-1}$ (for AD subjects). Early $^{11}\text{C-PiB}$ studies also reported regional bias among semiquantitative binding measures, with an overestimation by SUVR and underestimation by reference-tissue binding measures (relative to arterial-based binding measures) (13). Limitations of SUVR are well established (31), and a $^{11}\text{C-PiB}$ SUVR time-dependency study showed that 40- to 60-min and 50- to 70-min SUVR provided a reasonable compromise between physiologic validity, stability, sensitivity, and clinical feasibility (17). The current study includes data from these published $^{11}\text{C-PiB}$ studies and unpublished paired $^{15}\text{O-water}$ PET studies.

The primary study findings include lack of statistically significant correlations between $K_{1-\text{Water}}$ and $K_{1-\text{PiB}}$ in primary cortical areas, which may partly reflect technical differences including $^{11}\text{C-PiB}$ injection over 20 s that reduces accuracy of $K_{1-\text{PiB}}$ estimation, as compared with $K_{1-\text{Water}}$ determined after rapid $^{15}\text{O-water}$ bolus injection. Even lower correlations were observed between $K_{1-\text{Water}}$ and relative $^{11}\text{C-PiB}$ delivery parameters (data not shown). However, after normalizing both $K_{1-\text{Water}}$ and $K_{1-\text{PiB}}$ to cerebellum, significant positive correlations emerged between $\text{Rel-}K_{1-\text{Water}}$ and $\text{Rel-}K_{1-\text{PiB}}$ in 4 of 5 primary cortical regions. This positive correlation is not likely driven by CER, as correlation between CER $K_{1-\text{Water}}$ and CER $K_{1-\text{PiB}}$ was not statistically significant ($P = 0.064$) and $K_{1-\text{Water}}$ RSD was similar across ROIs (~17%–20%, including CER). These findings may reflect, in part, lower intersubject variability across relative (compared with absolute) delivery measures, as ratios may minimize some variability (e.g., scanner-related measurement variation, variation in intersubject physiologic state). Stronger correlations were observed between $\text{Rel-}K_{1-\text{Water}}$ and $\text{SRTM2-}R_I$ (than for $\text{Rel-}K_{1-\text{PiB}}$), presumably because of greater variance in $\text{Rel-}K_{1-\text{PiB}}$ as a calculated ratio of 2 independent parameter estimates, compared with R_I as a single ratio parameter directly estimated by SRTM2. As expected, correlations were strongest between $\text{Rel-}K_{1-\text{PiB}}$ and $\text{SRTM2-}R_I$. Overall, these correlations were independent of CSF dilution correction, suggesting robustness against this confound.

The secondary findings showed variable significance for regional correlations between delivery (mostly $^{11}\text{C-PiB}$ relative delivery parameters) and $^{11}\text{C-PiB}$ retention that appear to be partly, if not mostly, related to CSF adjustment, as no significant correlations were observed without CSF correction. Correlations between $^{11}\text{C-PiB}$ relative delivery and retention were most notable in ACG, a primary cortical region that exhibits early $^{11}\text{C-PiB}$ deposition and cortical atrophy.

We sought to minimize bias in all kinetic methods but given that SRTM is key to this work, it is important to note potential sources of SRTM bias in its application to $^{11}\text{C-PiB}$ kinetics that are described by 2-tissue compartments (rather than 1 compartment) and that range from specific AD kinetics to nonspecific controls kinetics that may be similar to cerebellum (32). SRTM2 was applied using an average subject-specific $\text{SRTM-}k_2'$ constraint determined across ROIs (except CER). We acknowledge that this imperfect estimate of reference tissue clearance rate can bias retention measures, particularly when time–activity curves in CER and target ROIs are similar (i.e., $^{11}\text{C-PiB}$ –negative), as reported for muscarinic-2 receptor-binding MRTM simulations (33). The k_2' constraints herein were not statistically different between $^{11}\text{C-PiB}$ –positive and $^{11}\text{C-PiB}$ –negative subjects (Mann–Whitney U test $P = 0.278$; cutoffs determined by Cohen, et al. (34)), yielded SRTM2–DVR values that were comparable to other binding measures, and most importantly did not strongly affect R_I that was a primary focus of this work. $\text{SRTM-}R_I$ and $\text{SRTM2-}R_I$ values were highly correlated (r^2 range, 0.92 [MTC] to 0.99 [CTX5]). Bias in $\text{SRTM2-}R_I$ (relative to $\text{SRTM-}R_I$) was less than 10% for primary cortical regions (–3.6% for CTX5), low for PON (1%) and SWM (3.6%), but greater for THL (–8.4%). Yaqub et al. used SRTM as a reference tissue standard for evaluation of simplified voxel-based $^{11}\text{C-PiB}$ analyses (e.g., SUVR, reference Logan, MRTM2 (35), RPM2, SRTM) and reported only a slight difference in quantitative performance across methods, strong correlations across binding outcomes ($R^2 > 0.95$, except

SUVR60–90), best performance by MRTM2 and RPM2, and simulations (6% noise) showing bias in RPM2- BP_{ND} of 0%, SUVR40–60 of 40%, and SUVR60–90 of 50% (14). We do not observe this level of high bias in SUVR using ROI-based analyses with lower noise than voxel-based, using SUVR determined within 40–70 min, and when the reference standard is arterial-based (SUVR50–70 bias 15%) rather than reference-based (SUVR50–70 bias 30%) (17).

The overall findings of this study are consistent with and relevant to findings by others that involved less direct comparisons of delivery. Blomquist et al. reported that changes in PaCO₂ (e.g., from 5.0 to 7.2 kPa) led to changes of similar magnitude in both K_{1-PiB} and CBF ($\approx 50\%$ – 100%) in an anesthetized rhesus monkey, suggesting that K_{1-PiB} may be a useful index of CBF (36). Meyer et al. reported on dual-biomarker imaging of regional A β load and neuronal activity with ¹¹C-PiB using SRTM2 to assess both A β plaque load and relative delivery (19). The high correlations observed herein between Rel- $K_{1-Water}$ and PiB SRTM2- R_I provide direct quantitative evidence that ¹¹C-PiB SRTM2- R_I may be a robust surrogate of regional relative CBF. In addition, ¹¹C-PiB delivery was generally independent of retention, lending further support for determining dual-imaging measures from dynamic ¹¹C-PiB imaging. Lastly, despite flow independence for cross-sectional ¹¹C-PiB retention, a recent report by van Berckel et al. describes how longitudinal ¹¹C-PiB SUVR can be sensitive to longitudinal flow changes (e.g., cortical flow change when reference flow is stable), and this is important to consider and better understand in future studies (20), including those performed with ¹⁸F-labeled A β PET imaging agents (37,38).

CONCLUSION

This study provides quantitative evidence supporting relative ¹¹C-PiB delivery measures as surrogate indices of regional relative CBF. The results also offer further direct evidence that cross-sectional ¹¹C-PiB retention is generally independent of CBF, including SUVR. This study contributes to a body of methodology work that seeks to better understand and define the capabilities of A β PET imaging that is needed to address long-term challenges.

Supplementary Material

Refer to Web version on PubMed Central for supplementary material.

Acknowledgments

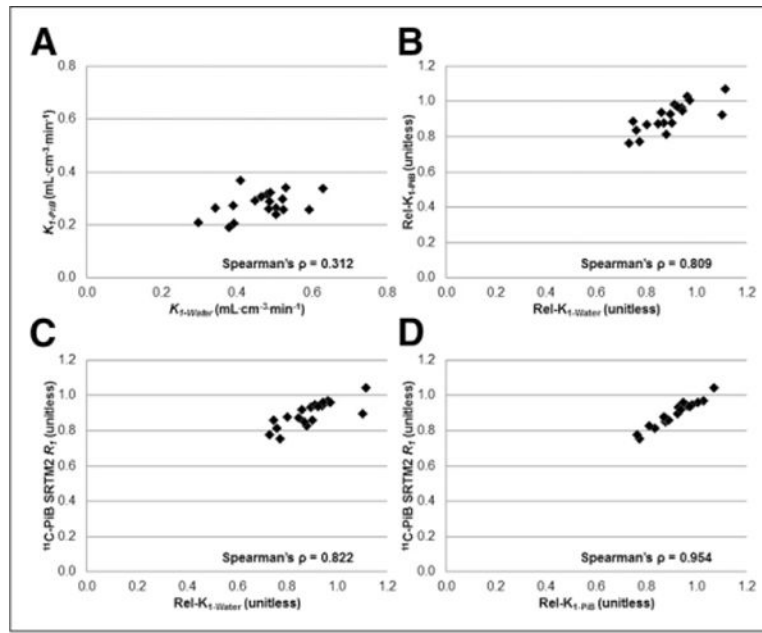
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**FIGURE 1.**

Scatterplots for global cortical region (CTX5) depicting relationship between direct delivery ([A] $K_{1-Water}$ and K_{1-PiB}) and relative delivery ([B] Rel- $K_{1-Water}$ and Rel- K_{1-PiB} ; [C] Rel- $K_{1-Water}$ and ¹¹C-PiB SRTM2- R_f ; [D] Rel- K_{1-PiB} and ¹¹C-PiB SRTM2- R_f), with respective Spearman ρ values. There are different axes ranges for A and B–D.

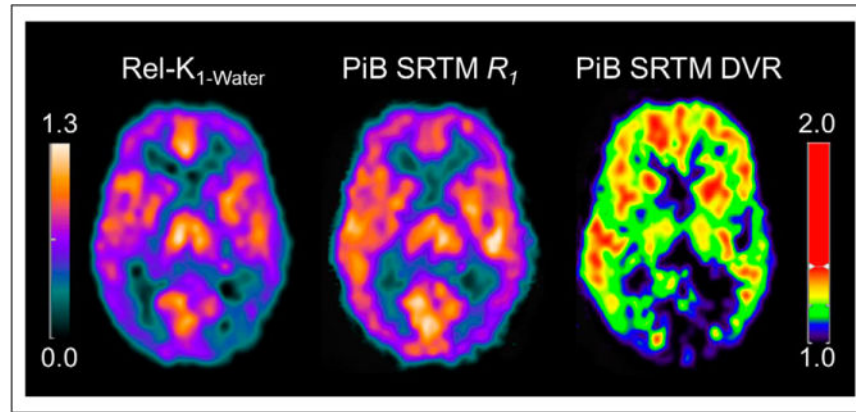


FIGURE 2. Example parametric images of Rel- $K_{1\text{-Water}}$ and ^{11}C -PiB SRTM- R_1 and DVR for AD subject (age, 54 y; MMSE, 19) show that Rel- $K_{1\text{-Water}}$ and ^{11}C -PiB SRTM- R_1 provide similar distribution of relative flow (images not CSF-corrected).

TABLE 1

Subject Characteristics

Characteristic	Controls (<i>n</i> = 6)	MCI (<i>n</i> = 8)	AD (<i>n</i> = 5)	Group comparison (Kruskal–Wallis <i>P</i>)
Sex				–
Male	1	6	4	
Female	5	2	1	
Age (y)	62.8 ± 11.8	69.0 ± 10.5	67.0 ± 9.0	0.529
MMSE	28.5 ± 1.4	27.8 ± 1.0	24.0 ± 3.4	0.010
Education (y)	14.2 ± 2.4	17.5 ± 3.4	17.4 ± 3.6	0.137

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TABLE 2

Delivery Parameters

Parameter	$K_{1\text{-Water}}^*$	$K_{1\text{-PiB}}^*$	Rel- $K_{1\text{-Water}}^\dagger$	Rel- $K_{1\text{-PiB}}^\dagger$	SRTM2- R_I^\dagger
ACG	0.520 ± 0.096	0.280 ± 0.045	0.994 ± 0.14	0.920 ± 0.11	0.911 ± 0.096
FRC	0.455 ± 0.079	0.271 ± 0.046	0.868 ± 0.096	0.886 ± 0.080	0.869 ± 0.071
LTC	0.408 ± 0.079	0.251 ± 0.045	0.780 ± 0.10	0.821 ± 0.078	0.835 ± 0.072
PAR	0.444 ± 0.088	0.277 ± 0.049	0.850 ± 0.13	0.909 ± 0.098	0.888 ± 0.079
PRC	0.531 ± 0.010	0.316 ± 0.058	1.013 ± 0.13	1.035 ± 0.11	0.988 ± 0.089
CTX5	0.467 ± 0.083	0.278 ± 0.048	0.891 ± 0.11	0.912 ± 0.083	0.894 ± 0.073
MTC	0.446 ± 0.074	0.199 ± 0.028	0.855 ± 0.098	0.660 ± 0.089	0.713 ± 0.069
OCC	0.537 ± 0.11	0.335 ± 0.061	1.029 ± 0.19	1.097 ± 0.10	1.028 ± 0.091
AVS	0.467 ± 0.093	0.287 ± 0.052	0.887 ± 0.081	0.940 ± 0.097	0.915 ± 0.074
SWM	0.180 ± 0.032	0.098 ± 0.024	0.350 ± 0.087	0.319 ± 0.060	0.367 ± 0.059
PON	0.402 ± 0.081	0.238 ± 0.042	0.764 ± 0.076	0.777 ± 0.061	0.796 ± 0.059

* In mL·cm⁻³·min⁻¹.

† Unitless.

Parameters adjusted for CSF dilution.

TABLE 3

Correlation Between ^{15}O -Water and ^{11}C -PiB Delivery Parameters^{*†}

ROI	Spearman ρ			
	$K_{1\text{-Water}}$ and $K_{1\text{-PiB}}$	Rel- $K_{1\text{-Water}}$ and Rel- $K_{1\text{-PiB}}$	Rel- $K_{1\text{-Water}}$ and ^{11}C -PiB SRTM2- R_I	Rel- $K_{1\text{-PiB}}$ and ^{11}C -PiB SRTM2- R_I
ACG	0.311 (0.195)	0.726* (<0.001)*	0.688* (0.001)*	0.984* (<0.001)*
FRC	0.468 (0.043)	0.816* (<0.001)*	0.793* (<0.001)*	0.968* (<0.001)*
LTC	0.422 (0.072)	0.809* (<0.001)*	0.782* (<0.001)*	0.963* (<0.001)*
PAR	0.512 (0.025)	0.628 (0.004)	0.677* (0.001)*	0.967* (<0.001)*
PRC	0.295 (0.221)	0.809* (<0.001)*	0.840* (<0.001)*	0.919* (<0.001)*
CTX5	0.312 (0.193)	0.809* (<0.001)*	0.822* (<0.001)*	0.954* (<0.001)*
MTC	0.234 (0.335)	0.693* (0.001)*	0.784* (<0.001)*	0.901* (<0.001)*
OCC	0.350 (0.141)	0.623 (0.004)	0.707* (0.001)*	0.895* (<0.001)*
OCP	0.486 (0.035)	0.523 (0.019)	0.704* (0.001)*	0.839* (<0.001)*
SMC	0.186 (0.446)	0.689* (0.001)*	0.721* (<0.001)*	0.968* (<0.001)*
AVS	0.509 (0.026)	0.576 (0.010)	0.499 (0.030)	0.839* (<0.001)*
SWM	0.699* (0.001)*	0.613 (0.005)	0.673* (0.002)*	0.902* (<0.001)*
PON	0.247 (0.307)	0.402 (0.088)	0.462 (0.047)	0.921* (<0.001)*
THL	0.225 (0.354)	0.780* (<0.001)*	0.786* (<0.001)*	0.968* (<0.001)*
CER	0.433 (0.064)	NA	NA	NA

* Statistically significant correlations; threshold of $P < 0.0036$ after Bonferroni adjustment.

† Parameters adjusted for CSF dilution.

Data in parentheses are P values.

NA = not applicable.

TABLE 4CTX5 ¹¹C-PiB Retention Measures

Clinical diagnosis	2T-4k-DVR	ART90-DVR	CER90-DVR	SUV70	SRTM2-DVR
Controls	1.286 ± 0.267	1.381 ± 0.276	1.310 ± 0.244	1.488 ± 0.345	1.240 ± 0.299
MCI	1.659 ± 0.660	1.781 ± 0.599	1.634 ± 0.565	1.891 ± 0.733	1.645 ± 0.681
AD	1.896 ± 0.582	2.025 ± 0.213	1.997 ± 0.240	2.398 ± 0.334	2.022 ± 0.303

Measures adjusted for CSF dilution.

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TABLE 5Correlation Between Delivery Parameters and 11C-PiB Retention for CTX5^{*†}

Parameter	Spearman ρ				
	2T-4k-DVR	ART90-DVR	CER90-DVR	SUVr70	SRTM2-DVR
K_1 -Water	-0.341 (0.196)	-0.281 (0.244)	-0.093 (0.705)	-0.130 (0.596)	-0.093 (0.705)
Rel- K_1 -Water	0.326 (0.217)	0.160 (0.514)	0.202 (0.408)	0.189 (0.437)	0.132 (0.591)
Rel- K_1 -PiB	0.447 (0.083)	0.426 (0.069)	0.528 (0.020)	0.516 (0.024)	0.533 (0.019)
SRTM2- R_f	0.434 (0.093)	0.385 (0.103)	0.481 (0.037)	0.469 (0.043)	0.489 (0.034)

* Threshold of $P < 0.0036$ for statistically significant correlations after Bonferroni adjustment.

† Measures adjusted for CSF dilution.

Data in parentheses are P values.