

# Increased susceptibility of spontaneously hypertensive rats to ventricular tachyarrhythmias in early hypertension

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## Key points

- Hypertension is a risk factor for sudden cardiac death caused by ventricular tachycardia and fibrillation.
- Whether hypertension in its early stage is associated with an increased risk of ventricular tachyarrhythmias is not known.
- Based on experiments performed at the cellular and whole heart levels, we show that, even early in chronic hypertension, the hypertrophied and fibrotic ventricles of spontaneously hypertensive rats aged 5 to 6 months have already developed increased stress-induced arrhythmogenicity, and this increased susceptibility to ventricular arrhythmias is primarily a result of tissue remodelling rather than cellular electrophysiological changes.
- Our findings highlight the need for early hypertension treatment to minimize myocardial fibrosis, ventricular hypertrophy, and arrhythmias.

**Abstract** Hypertension is a risk factor for sudden cardiac death caused by ventricular tachycardia and fibrillation (VT/VF). We hypothesized that, in early hypertension, the susceptibility to stress-induced VT/VF increases. We compared the susceptibility of 5- to 6-month-old male spontaneously hypertensive rats (SHR) and age/sex-matched normotensive rats (NR) to VT/VF during challenge with oxidative stress ( $\text{H}_2\text{O}_2$ ;  $0.15 \text{ mmol l}^{-1}$ ). We found that only SHR hearts exhibited left ventricular fibrosis and hypertrophy.  $\text{H}_2\text{O}_2$  promoted VT in all 30 SHR but none of the NR hearts. In 33% of SHR cases, focal VT degenerated to VF within 3 s. Simultaneous voltage-calcium optical mapping of Langendorff-perfused SHR hearts revealed that  $\text{H}_2\text{O}_2$ -induced VT/VF arose spontaneously from focal activations at the base and mid left ventricular epicardium. Microelectrode recording of SHR hearts showed that VT was initiated by early afterdepolarization (EAD)-mediated triggered activity. However, despite the increased susceptibility of SHR hearts to VT/VF, patch clamped isolated SHR ventricular myocytes developed EADs and triggered activity to the same extent as NR ventricular myocytes, except with larger EAD amplitude. During the early stages of hypertension, when challenged with oxidative stress, SHR hearts showed an increased ventricular arrhythmogenicity that stems primarily from tissue remodelling (hypertrophy, fibrosis) rather than cellular electrophysiological changes. Our findings highlight the need for early hypertension treatment to minimize myocardial fibrosis, ventricular hypertrophy, and arrhythmias.

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**Abbreviations** AP, action potential; APD, action potential duration; APD<sub>90</sub>, action potential at 90% duration; CaMKII, calcium/calmodulin-dependent protein kinase II; CaT, calcium transient; CaTD<sub>90</sub>, calcium transient at 90% duration; CI, confidence interval; DBP, diastolic blood pressure; EAD/DAD, early/delayed after-depolarization; HR, heart rate; ICC, interclass correlation;  $I_{Ca,L}$ , L-type calcium current;  $I_{Ks}$ , slow delayed rectifier potassium current;  $I_{Na}$ , sodium current;  $I_{to}$ , transient outward potassium current; IVS(d,s) interventricular septum thickness (during diastole, during systole); LV, left ventricle; LVEF, left ventricular ejection fraction; LVFS, left ventricular fractional shortening; LVH, left ventricular hypertrophy; LVID(d,s) left ventricular internal diameter (during diastole, during systole); MV, mitral valve; NR, normotensive rats; PA peak vel, pulmonary artery peak velocity; (P)CL, (pacing) cycle length; PW, posterior wall; P-ECG, pseudo-electrocardiogram; RV, right ventricle; RWT, relative wall thickness; SHR, spontaneously hypertensive rats; SHHF, spontaneously hypertensive heart failure; SBP, systolic blood pressure; VT/VF, ventricular tachycardia and fibrillation.

## Introduction

Hypertension is recognized as an important and treatable contributor to cardiovascular disease, including heart failure, atherosclerosis, stroke, and sudden cardiac death (McLenachan *et al.* 1987; Wolf-Maier *et al.* 2003). With a prevalence of 30% in the USA in 1999–2010, up to 30% of hypertensive adults were unaware of their condition (Guo *et al.* 2012). Moreover, a 2012 report released by the Centres for Disease Control showed the lack of effective control of blood pressure in more than half of the 67 million Americans with hypertension (Go *et al.* 2014). Although it is established that chronic uncontrolled hypertension eventually leads to heart failure, which increases the risk of ventricular tachycardia and fibrillation (VT/VF) (Francis, 1986; McLenachan *et al.* 1987; Wolf-Maier *et al.* 2003), whether uncontrolled hypertension prior to the onset of severe hypertrophy and heart failure directly increases the susceptibility of the heart to VT/VF remains undefined.

Tremendous insight into the temporal progression of persistent pressure overload on cardiac structure and function has been achieved with the spontaneously hypertensive rat (SHR), a chronic hypertension model developed over 50 years ago through selective breeding of the Wistar-Kyoto strain (Okamoto & Aoki, 1963). In SHR, systolic blood pressure (SBP) exceeding 180 mmHg emerges 3–4 months after birth (Okamoto & Aoki, 1963). Although it is recognized that, by the time that SHR reach middle age (~1 year of age), the left ventricle (LV) has already manifested significant fibrosis and hypertrophy, contractile dysfunction and increased susceptibility to pacing-induced VT/VF (Pfeffer *et al.* 1979; Pahor *et al.* 1991; Zugg *et al.* 1997; Kapur *et al.* 2010; Maron, 2010), the risk of cardiac remodelling during earlier stages of uncontrolled hypertension on VT/VF, spontaneous or pacing-induced, remains unclear. Accordingly, we studied SHR rats at 5–6 months of age, some 2–3 months after the onset of significant uncontrolled hypertension.

To assess susceptibility to VT/VF, we exposed SHR hearts to oxidative stress using H<sub>2</sub>O<sub>2</sub>. There is a growing awareness of the contribution of oxidative stress and plasma H<sub>2</sub>O<sub>2</sub> elevation to the progression of various cardiovascular diseases, including hypertension. For signalling purposes at baseline, cells produce low steady-state levels of H<sub>2</sub>O<sub>2</sub> (10–20 μmol l<sup>-1</sup>) (Droge, 2002; Baek *et al.* 2012), which cause no appreciable oxidative injury (Rhee, 2006). Cytoplasmic peroxidases and catalases maintain steep H<sub>2</sub>O<sub>2</sub> membrane gradients such that intracellular concentrations rarely reach >10–14% of extracellular concentrations (Antunes & Cadenas, 2000; Stone & Yang, 2006). Still, even at baseline, patients with personal or family history of hypertension produce higher plasma H<sub>2</sub>O<sub>2</sub> levels compared to normotensive controls without genetic risk (Lacy *et al.* 2000). These differences in baseline H<sub>2</sub>O<sub>2</sub> levels are further amplified during oxidative stress. In inflamed or injured tissue during an oxidative burst, cells can produce significant amounts of H<sub>2</sub>O<sub>2</sub> (100 μmol l<sup>-1</sup>) (Droge, 2002) as rapidly as 2–6 × 10<sup>-14</sup> mol h<sup>-1</sup> cell<sup>-1</sup> (Droge, 2002; Rhee, 2006) or 40 nmol min<sup>-1</sup> g<sup>-1</sup> (Granger, 1988). For example, within 6 h after cardiac surgery, patients with new onset postoperative atrial fibrillation have significantly more H<sub>2</sub>O<sub>2</sub> elevation compared to patients in sinus rhythm (up to 8-fold vs. 2-fold increase, respectively) (Ramlawi *et al.* 2007). Similarly, upon reperfusion after ischaemia, rat hearts (Droge, 2002) and rat striata (Hyslop *et al.* 1995) produce substantial fluxes of superoxide and H<sub>2</sub>O<sub>2</sub> (Granger, 1988). Additionally, during oxidative stress in atherosclerosis, arterial binding of oxidized low-density lipoprotein activates macrophages, stimulating significant H<sub>2</sub>O<sub>2</sub> production.

In the present study, we examined whether SHR hearts at 5–6 months of age were susceptible to VT/VF if exposed to H<sub>2</sub>O<sub>2</sub> concentrations typical of a pathophysiological oxidative burst (Morita *et al.* 2009; Morita *et al.* 2011a). We found that even 2–3 months of uncontrolled hypertension was sufficient to promote mild structural and electrical

remodelling that increased susceptibility to H<sub>2</sub>O<sub>2</sub>-induced VT/VF.

## Methods

The present study was conducted in accordance with the National Institutes of Health Guide for the Care and Use of Laboratory Animals and approved by the University of California Institutional Animal Care and Use Committee. Age- and sex-matched male SHR and Wistar-Kyoto normotensive rats (NR) of 5–6 months of age were euthanized by an i.v. injection of heparin sulfate (1000 U) and sodium pentobarbital (100 mg kg<sup>-1</sup>). Adequacy of anaesthesia was confirmed by the lack of pedal withdrawal reflex, corneal reflex, and motor response to pain stimuli by scalpel tip.

## Echocardiography

The transthoracic echocardiographic technique and protocols used in the present study were analogous to those recommended by the European Association of Echocardiography and the American Society for Echocardiography guideline for use in humans (Lang *et al.* 2015) and were validated for normotensive and hypertensive rats (de Simone *et al.* 1990). Echocardiographic examinations were performed as described previously for rats, particularly hypertensive rats (Haas *et al.* 1995; Ono *et al.* 2002), by a single technician blinded to the type of animal. Following anaesthesia induction, rats were placed supine on an electrical heating pad at 37°C under mild anaesthesia maintenance with 1.5% isoflurane/98.5% oxygen. Two-dimensional B-mode, M-mode, and pulsed-wave Doppler images were obtained using the high-frequency ultrasound scanner Vevo 2100 Micro-Ultrasound (VisualSonics, Toronto, Canada) equipped with an ultra-high frequency MS250 linear array transducer (13–24 MHz). Left ventricular internal diameter (LVID), as well as the thickness of the interventricular septum (IVS) and LV posterior wall (PW), were measured at end-diastole and end-systole from two-dimensional or M-mode tracings in short- and long-axis views using the leading-edge method, as recommended by the European Association of Echocardiography/American Society for Echocardiography guideline (Lang *et al.* 2015). Characterization of left ventricular hypertrophy (LVH) was achieved by evaluating the thickness of the IVS and PW during diastole (de Simone *et al.* 1994). Calculating the relative wall thickness (RWT) based on the formula [(PWd + IVSd)/LVIDd, where d is diastolic] (Haas *et al.* 1995) permitted further categorization of the LVH as either concentric (RWT >0.45) or eccentric (RWT ≤0.45)

(Ganau *et al.* 1992; Barbieri *et al.* 2012; Lang *et al.* 2015). Because no definite qualitative classification scheme exists for rodents, to classify the severity of LVH, we modelled in accordance with the existing classification scheme for human LVH (Ono *et al.* 2002; Lang *et al.* 2015) and determined *a priori* an increase of septal (IVSd) thicknesses over control NR in the range of 10–30% as mild, 40–60% as moderate, and ≥70% as severe LVH. Cardiac chamber volume and function were quantified in accordance with prevalent standards for rats (Schwarz *et al.* 1998; Brown *et al.* 2002), which are analogous to those for humans (Lang *et al.* 2015). Once the LVID measurement was obtained, the LV volume (LV Vol), LV fractional shortening (FS) and LV ejection fraction (EF) were calculated automatically using built-in formulas and algorithms (Folland *et al.* 1979) from the VisualSonics cardiac measurement software package for the Vevo 2100 imaging system (VisualSonics). Formulation for the LV Vol was based on a modified ellipsoid model (Teichholz *et al.* 1976):

$$\text{LV Vol} = [7.0/(2.4 + \text{LVID})] \times \text{LVID}^3$$

$$\text{FS}(\%) = 100 \times [(\text{LVIDd} - \text{LVIDs})/\text{LVIDd}]$$

$$\text{EF}(\%) = 100 \times [(\text{LV Vold} - \text{LV Vols})/\text{LV Vold}]$$

where 'd' is diastolic and 's' is systolic.

Pulsed-wave Doppler was used to measure pulmonary arterial peak velocity from the long-axis view. Mitral flow velocity patterns were obtained in the apical four-chamber view with colour Doppler mode. Sample volume (1 mm) was placed between the tips of the mitral leaflets and adjusted to the position where velocity was maximal and the flow pattern was laminar. Velocity recordings were made with simultaneous recordings of the electrocardiogram. Mitral flow velocity patterns were analysed to determine peak early diastolic filling velocity (E velocity) and peak late diastolic filling velocity during atrial contraction (A velocity), as well as their ratio (E/A ratio).

## Non-invasive blood pressure measurements

Conscious rats were restrained in a warming chamber at 38°C (model 306; IITC Life Science, Woodland Hills, CA, USA) for 10–20 min before non-invasive SBP measurements. An integrated sensor-cuff occluder (B60-1/4; IITC Life Science) stopped tail pulsation on manual inflation and detected the return of tail pulsations with each deflation cycle (Whitesall *et al.* 2004). The blood pressure monitor was set for desired sensitivity with maximum tail-cuff inflation pressure set to at least 40 mmHg above the anticipated SBP. The mean SBP is an average of triplicate measurements made over a 10-min period.

## Electrophysiological studies of isolated perfused Langendorff hearts

Using the Langendorff method, isolated spontaneously-beating rat hearts were perfused at a constant rate of  $5 \text{ ml min}^{-1}$  with standard normal Tyrode's solution at  $37^\circ\text{C}$  containing albumin ( $100 \text{ mg l}^{-1}$ ) and (in  $\text{mmol l}^{-1}$ )  $125 \text{ NaCl}$ ,  $5.4 \text{ KCl}$ ,  $1.8 \text{ NaH}_2\text{PO}_4$ ,  $24 \text{ NaHCO}_3$ ,  $1.8 \text{ CaCl}_2$ ,  $0.5 \text{ MgCl}_2$  and  $5.5 \text{ glucose}$  (pH 7.4 adjusted with NaOH). Hearts were also superfused with normal Tyrode's at  $37^\circ\text{C}$  and allowed 20 min to equilibrate. Cytochalasin D ( $1 \text{ } \mu\text{mol l}^{-1}$ ) was added to the arterial perfusate to suppress contraction, thereby reducing motion artefacts during optical mapping and microelectrode recording.

Hearts were stained with voltage- (RH-237;  $2 \text{ } \mu\text{mol l}^{-1}$ ) and calcium-sensitive (rhod 2 AM;  $2 \text{ } \mu\text{mol l}^{-1}$ ) fluorescent dyes for dual voltage and calcium optical mapping using a dual CMOS camera system (MiCAM Ultima; BrainVision, Tokyo, Japan). The emitted fluorescence was collected by the dual CMOS camera system using a 690-nm long-pass filter for RH-237 and a  $585 \pm 20 \text{ nm}$  filter for rhod 2 (Numata *et al.* 2012). The acquisition rate was  $1 \text{ ms frame}^{-1}$  and recordings made from  $100 \times 100$  pixels with a spatial resolution of  $0.35 \times 0.35 \text{ mm}^2$  per pixel covering the entire anterior left ventricular epicardial surface. A bipolar electrode was used to record pseudo-ECG (P-ECG) continuously during optical mapping and microelectrode recording. To simulate oxidative stress,  $\text{H}_2\text{O}_2$  of  $0.15 \text{ mmol l}^{-1}$ , consistent with reported concentrations during an oxidative burst *in vivo* (Droge, 2002), was added to the perfusate (Morita *et al.* 2009). To inhibit calcium/calmodulin-dependent protein kinase II (CaMKII), KN-93 ( $1 \text{ } \mu\text{mol l}^{-1}$ ) was added to the perfusate; KN-92 ( $1 \text{ } \mu\text{mol l}^{-1}$ ) was used as negative control. If no VF occurred spontaneously after at least 90 min of  $\text{H}_2\text{O}_2$  exposure, rapid pacing to induce VT/VF was attempted. Using electrical stimuli of 4-ms duration and at least 2.5 times the action potential threshold, pacing was also performed to measure action potential duration (APD) and calcium transient (CaT) duration at a constant cycle length (CL).

## Patch clamp studies of single myocytes

Single ventricular myocytes were freshly isolated for whole-cell patch clamp (Bapat *et al.* 2012; Nguyen *et al.* 2012). Hearts were perfused using the standard Langendorff retrograde perfusion method at  $22 \text{ ml min}^{-1}$ ,  $37^\circ\text{C}$  with  $\text{Ca}^{2+}$ -free Tyrode's solution for 4 min to remove blood from the vessels, then with the enzyme solution for 25–27 min and, finally, with  $0.05 \text{ mmol l}^{-1}\text{-Ca}^{2+}$  Tyrode's solution to wash out the enzyme solution. The enzyme solution for myocyte isolation was a calcium-free

Tyrode's solution containing  $2.0 \text{ mg ml}^{-1}$  collagenase (type II; Worthington Biochemical Corp., Lakewood, NJ, USA) and  $0.17 \text{ mg ml}^{-1}$  protease (type XIV; Sigma, St Louis, MO, USA). Hearts were subsequently removed from the perfusion apparatus and gently agitated to dissociate the myocytes. The  $\text{Ca}^{2+}$  concentration was gradually increased to  $1.8 \text{ mmol l}^{-1}$  over 60 min. Myocytes were stored at room temperature and used within 8 h.

The EGTA-free pipette solution for whole cell recordings contained (in  $\text{mmol l}^{-1}$ )  $110 \text{ K-aspartate}$ ,  $30 \text{ KCl}$ ,  $5 \text{ NaCl}$ ,  $10 \text{ Hepes}$ ,  $5 \text{ MgATP}$ ,  $5 \text{ creatine phosphate}$  and  $0.1 \text{ cAMP}$  (pH 7.2 adjusted with KOH). Standard normal Tyrode's solution containing (in  $\text{mmol l}^{-1}$ )  $136 \text{ NaCl}$ ,  $5.4 \text{ KCl}$ ,  $0.33 \text{ NaH}_2\text{PO}_4$ ,  $1.8 \text{ CaCl}_2$ ,  $1 \text{ MgCl}_2$ ,  $10 \text{ Hepes}$  and  $10 \text{ glucose}$  (pH 7.4 adjusted with NaOH) was used for myocyte isolation and for extracellular perfusion in patch clamp studies. Experiments were performed at  $34\text{--}36^\circ\text{C}$  (Nguyen *et al.* 2012). Action potentials were recorded using borosilicate glass electrodes (tip resistance  $2.0\text{--}2.5 \text{ M}\Omega$ ) and standard whole-cell patch clamp methods in the current clamp mode. Action potentials were triggered using stimuli of 2-ms duration and 2.5 times the threshold potential. Corrections were made for liquid junction potentials. Data were acquired by Axopatch 200B patch clamp amplifier, Digidata 1200 acquisition board and Clampex, version 8.0 (Axon Instruments, Inc., Foster City, CA, USA) and filtered at 2 kHz. To induce early after-depolarizations (EADs) in ventricular myocytes,  $\text{H}_2\text{O}_2$  ( $0.15 \text{ mmol l}^{-1}$ ) was added to the perfusate. Electrophysiological data were analysed using Clampfit, version 9.2 (Axon Instruments, Inc.) and Origin, version 7.5 (MicroCal Inc., Northampton, MA, USA).

## Quantification of tissue fibrosis, ventricular mass and myocyte dimensions

The extent of myocardial tissue fibrosis was assessed by Masson's trichrome staining of  $5\text{-}\mu\text{m}$  transverse sections of formalin-fixed, paraffin-embedded hearts. Ventricular mass was determined by weighing formalin-fixed isolated LVs and right ventricles (RVs). Cellular dimensions of freshly isolated ventricular myocytes were measured using bright-field microscopy. The isolated ventricular myocytes from both groups were imaged in the bright-field mode using QIClick Digital CCD Camera (QImaging, Surrey, BC, Canada) installed on a Leica DM5500 B microscope (Leica Microsystems CMS GmbH, Wetzlar, Germany). Single and multiple myocyte views were acquired using  $63\times$  and  $10\times$  magnification objectives, respectively. Myocyte length, width, and top surface area were measured using Image-Pro Premier, version 9.0 (Media Cybernetics, Rockville, MD, USA).

### Statistical analysis

We examined normal quantile plots and Shapiro–Wilk statistics to confirm that data followed a normal distribution in all cases. We also computed the inter-class correlation coefficients (ICC; ratio of inter-animal variation to total inter- and intra-animal variation) for all measurements to determine whether observations of different myocytes from the same rat were independent (ICC near 0 indicates no ‘clustering’) or non-independent (ICC near 1 indicates ‘clustering’). Because, overall, our ICCs ranged from 0 to 0.4, we demonstrated non-independence for almost all cases and had to account for both inter- and intra-animal variation. Therefore, means were compared using a ‘mixed’ analysis of variance model with both the usual random error effect and a random animal effect to take into account the non-independence of observations of different myocytes from the same rat. The mean, SD, SEM, confidence interval (CI), and *P* value were based on the mixed model. *P* < 0.05 was considered statistically significant.

## Results

### In vivo studies

Non-invasive SBP measurement confirmed hypertension at 5–6 months of age in the SHR group and normotension in the age- and sex-matched NR group ( $185 \pm 15$  vs.  $125 \pm 10$  mmHg, *P* < 0.01; *n* = 5 rats per group). Cardiac structure and function was assessed by echocardiography (*n* = 6 rats per group) (Fig. 1A and Table 1). SHR hearts had preserved systolic function as indicated by the normal left ventricular ejection fraction (LVEF). However, compared to NR hearts, mild-to-moderate concentric LVH was present in SHR hearts as indicated by a RWT of 0.78 (RWT >0.45 denotes concentricity) and global thickening with increased interventricular septum thickness by 37% and LV posterior wall thickness by 20% (Table 1).

### Gross pathology and histology

Despite comparable body weights between and among rats from the two groups (SHR  $312 \pm 20$  vs. NR  $300 \pm 12$  g; not statistically significant), SHR hearts demonstrated increased LV weight compared to NR hearts ( $607 \pm 96$  vs.  $455 \pm 77$  mg, *P* < 0.03; *n* = 6 hearts per group). By contrast, RVs isolated from the two groups revealed similar weights (SHR  $99 \pm 16$  vs. NR  $92 \pm 14$  mg, *P* = 0.48, *n* = 6 hearts per group), suggesting that early hypertension resulted in hypertrophy of primarily the LV but not the RV.

To further assess ventricular hypertrophy, we compared the size of isolated ventricular myocytes from the two groups (Fig. 1B). SHR myocytes (*n* = 350 myocytes from seven hearts) were significantly larger than NR

myocytes (*n* = 300 myocytes from six hearts) in both length ( $131 \pm 3$  vs.  $117 \pm 3$   $\mu\text{m}$ , *P* = 0.001) and width ( $29 \pm 0.9$  vs.  $25 \pm 0.9$   $\mu\text{m}$ , *P* = 0.001). The increased size of the SHR ventricular myocyte was consistent with hypertrophy, rather than hyperplasia, as the explanation for the increased mass of the SHR ventricles.

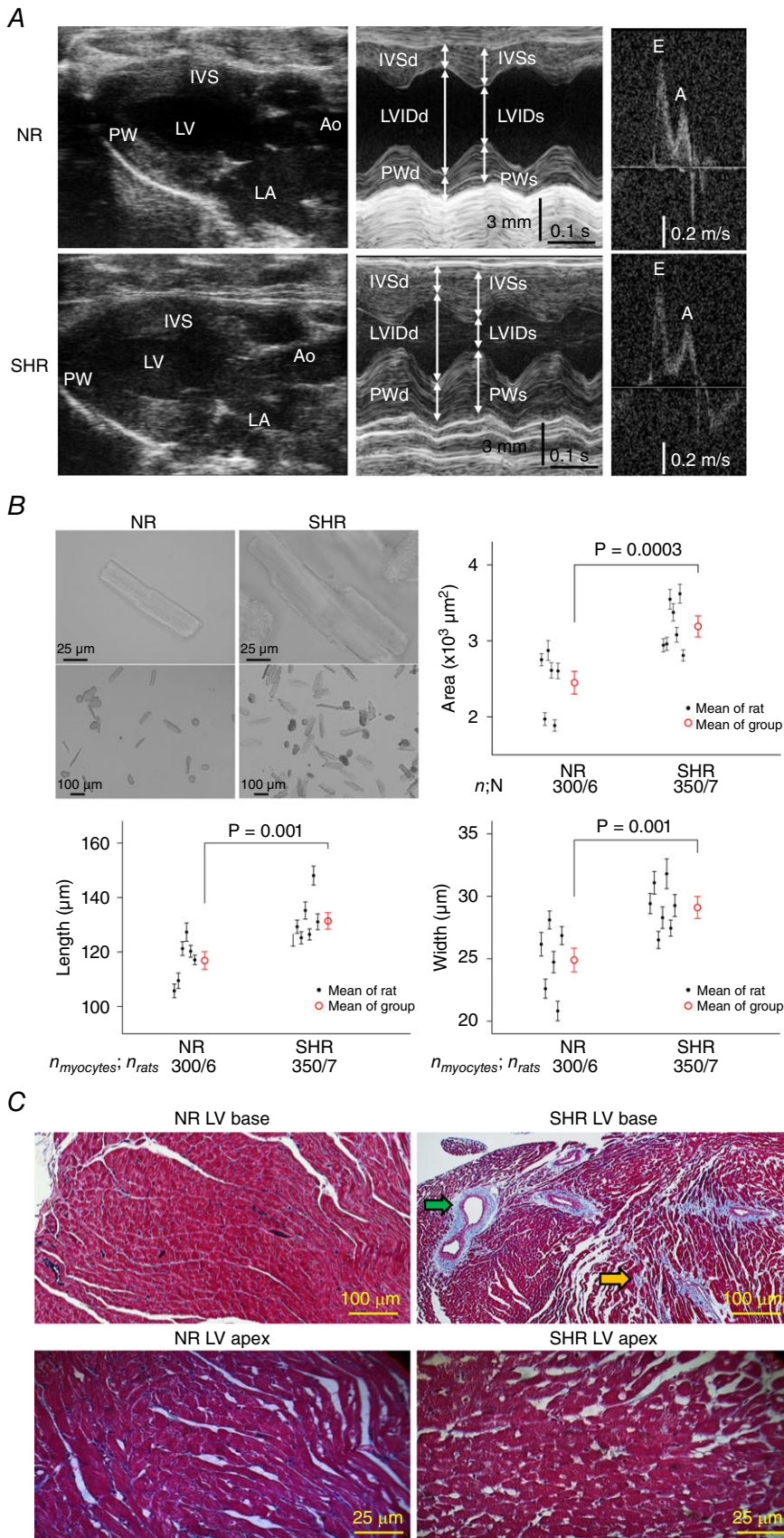
Additionally, histological studies (Fig. 1C) revealed that SHR hearts had increased fibrosis at the LV base compared to NR hearts ( $17.8 \pm 2$  vs.  $2.1 \pm 0.2\%$ , *P* < 0.05; *n* = 5 hearts per group) but not at the mid LV ( $2.5 \pm 0.1\%$  vs.  $2.2 \pm 0.2\%$ ; not statistically significant) or LV apex ( $1.7 \pm 0.1\%$  vs.  $1.2 \pm 0.2\%$ ; not statistically significant). The fibrosis pattern at the LV base of SHR hearts was perivascular and interstitial, as reported previously for pressure overload conditions (Lorell & Carabello, 2000).

### Ex vivo electrophysiological studies of intact hearts

**Spontaneous VT/VF induced by oxidative stress.** To assess susceptibility to VT/VF during oxidative stress with  $\text{H}_2\text{O}_2$ , we used bipolar electrodes to record P-ECG concurrently with epicardial microelectrode recordings and/or dual voltage-calcium optical mapping in isolated Langendorff-perfused hearts. At baseline, hearts from both SHR and NR groups were in sinus rhythm with similar cycle lengths (SHR CL  $395 \pm 145$  ms vs. NR CL =  $430 \pm 185$  ms; not statistically significant).

During 90 min of  $\text{H}_2\text{O}_2$  ( $0.15 \text{ mmol l}^{-1}$ ) perfusion, 13% of NR hearts (*n* = 3 of 24 NR hearts) manifested occasional ventricular premature ventricular complexes and <3-s runs of non-sustained VT, although no sustained VT (>30 s) or VF was observed. In three NR hearts, increasing the  $\text{H}_2\text{O}_2$  concentration to  $2.0 \text{ mmol l}^{-1}$  also failed to induce spontaneous VT/VF. In comparison, in all 30 SHR hearts, within only 10–17 min,  $\text{H}_2\text{O}_2$  initiated spontaneous VT that arose abruptly from sinus rhythm. VT was monomorphic in 54% of cases (CL  $94 \pm 12$  ms, 95% CI [85,110]) and polymorphic in 46% of cases (CL  $62 \pm 8$  ms, 95% CI [45,75], *P* < 0.05). In 33% of cases, spontaneous VT degenerated into VF within 3 s (Table 2).

Figure 2A illustrates the spontaneous initiation of monomorphic VT that arose during sinus rhythm at a CL of 350 ms and degenerated to VF after eight beats. Optical APs revealed that this monomorphic VT was initiated by late phase 3 EAD-mediated triggered activity arising from the LV base. The CL of locally recorded triggered activity averaged  $86 \pm 8$  ms, similar to the CL of the VT on the P-ECG ( $92 \pm 6$  ms). By contrast, the CL of the ensuing VF shortened to  $48 \pm 12$  ms. This sequence of sinus rhythm followed by late phase 3 EAD-mediated triggered VT at the LV base and subsequent degeneration to VF was captured by optical mapping in a total of eight SHR hearts. Figure 2B shows four isochronal activation maps for selected beats (red \*) of optical APs (traces 1–5)



**Figure 1. Cardiac remodelling in early hypertension of 5- to 6-month-old male SHR**

A, although both SHR and NR hearts had preserved LV systolic function, only SHR hearts manifested concentric LVH with global increased wall thicknesses seen on B-mode (longitudinal, panel 1) and M-mode (cross-section, panel 2). Ao, aorta. E and A, peak velocities in early and late filling. B, SHR hypertrophy at the myocyte level is evident on bright-field micrographs of representative myocytes and is confirmed by direct measurements of myocyte cross-sectional area, length, and width. The mean  $\pm$  SEM for each rat is represented by a small black circle with whiskers and, for each group by a large red circle with whiskers.  $n_{myocytes}/n_{rats}$ , number of myocytes/number of rats. C, although fibrosis is not apparent in the LV base from NR hearts (upper left) or the LV apex of both NR and SHR hearts (bottom), focal fibrosis (blue trichrome stain) is evident in the LV base from SHR hearts in the perivascular (green arrow) and interstitial (orange arrow) regions.

**Table 1. Transthoracic echocardiographic parameters**

	NR ( <i>n</i> = 6)	SHR ( <i>n</i> = 6)	<i>P</i> value	Mean difference [95% CI]
HR (beats min <sup>-1</sup> )	310 ± 21	333 ± 48	0.3	22 [-18,58]
IVSd (cm)**	1.9 ± 0.2	2.6 ± 0.2	0.001	0.7 [0.5,0.9]
IVSs (cm)**	3.0 ± 0.1	3.7 ± 0.3	0.002	0.7 [0.4,0.9]
LVIDd (cm)	6.7 ± 0.4	6.5 ± 0.9	0.7	-0.2 [-0.9,0.6]
LVIDs (cm)	3.8 ± 0.3	3.8 ± 1.1	0.9	0.0 [-0.8,0.9]
LVPWd (cm)*	2.0 ± 0.3	2.4 ± 0.3	0.03	0.4 [0.1,0.8]
LVPWs (cm)*	2.9 ± 0.2	3.4 ± 0.5	0.03	0.5 [0.2,0.9]
RWT	0.58 ± 0.07	0.78 ± 0.16	0.02	0.2 [0.07,0.33]
LVFS (%)	44 ± 2	43 ± 9	0.9	-1 [-8,6]
LVEF (%)	74 ± 3	72 ± 11	0.6	-2 [-11,6]
MV E (mm s <sup>-1</sup> )	652 ± 76	729 ± 128	0.2	77 [-29,188]
MV A (mm s <sup>-1</sup> )	460 ± 106	477 ± 63	0.7	17 [-66,113]
MV E/A	1.5 ± 0.4	1.5 ± 0.3	0.7	0.0 [-0.3,0.4]
PA peak vel (mm s <sup>-1</sup> )	1048 ± 92	1080 ± 130	0.6	32 [-82,146]

Data are reported as the mean ± SD. \**P* < 0.05, \*\**P* < 0.005; the bootstrap method. LV thickness was measured at the mid LV level. HR, heart rate; IVSd and IVSs, interventricular septal thickness during diastole and systole, respectively; LVIDd and LVIDs, left ventricular internal diameter during diastole and systole, respectively; LVPWd and LVPWs, left ventricular posterior wall thickness during diastole and systole, respectively; LVFS, left ventricular fractional shortening; E, early ventricular filling phase; A, ventricular filling during atrial contraction; MV E, mitral valve E velocity; MV A, mitral valve A velocity; MV E/A, mitral valve E/A ratio; PA peak vel, pulmonary artery peak velocity.

**Table 2. Incidence of spontaneous and pacing-induced VT/VF**

		Non-sustained VT (≤30 s)	Sustained VT (>30 s)	VF
NR ( <i>n</i> = 24 hearts)	Spontaneous	13% (3/24)	0%	0%
	Rapid pacing	38% (9/24)*	0%	0%
SHR ( <i>n</i> = 30 hearts)	Spontaneous	73% (22/30)	27% (8/30)	33% (10/30)
	Rapid pacing	NA	NA	66% (13/20)*

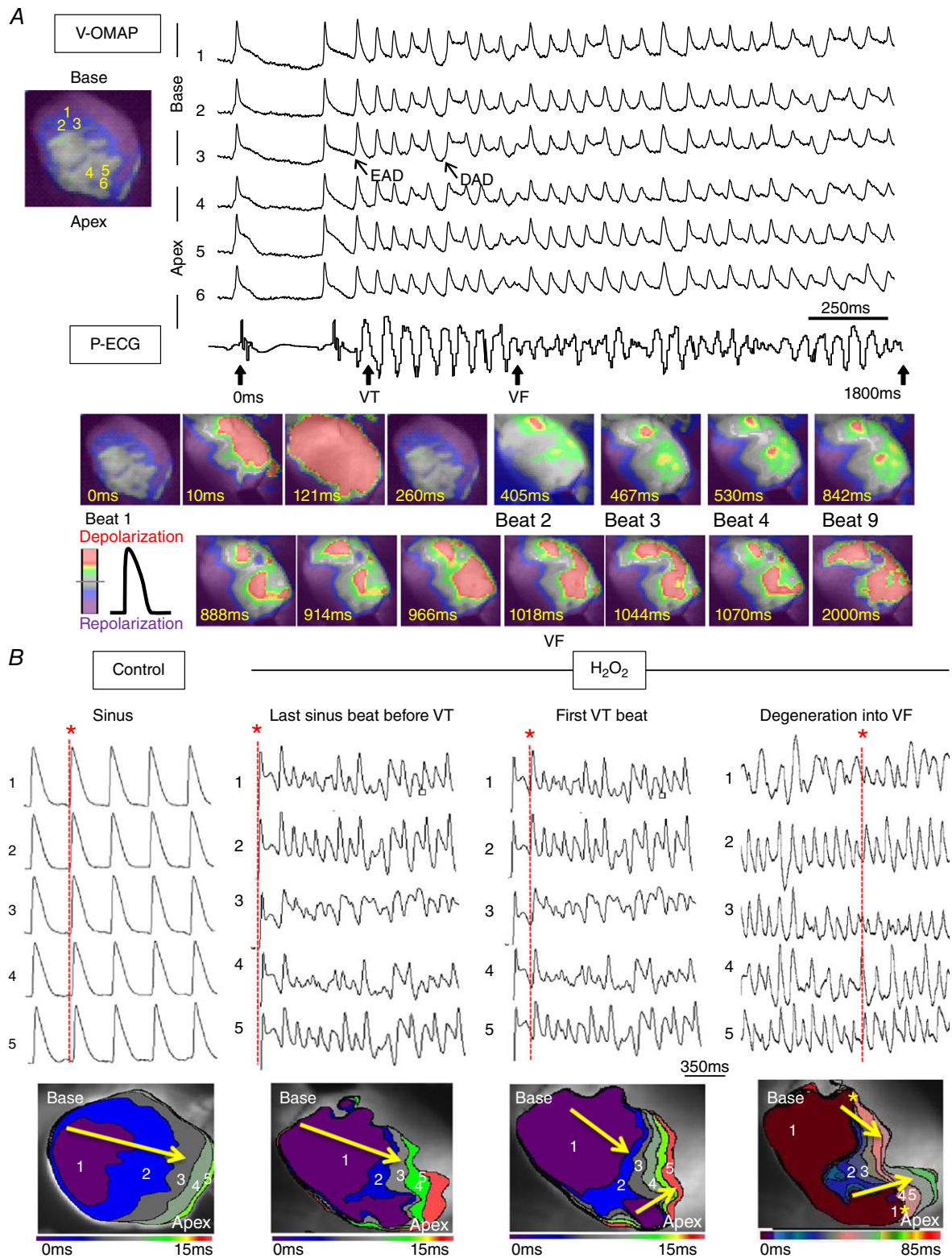
Intact hearts were perfused with H<sub>2</sub>O<sub>2</sub> to induce spontaneous VT/VF. \*Rapid pacing to induce VF was attempted only on the hearts that had not manifested spontaneous VF. NA, not available.

propagating from base to apex of the SHR LV during sinus under control condition prior to H<sub>2</sub>O<sub>2</sub> exposure (panel 1), then during the onset of VT (panels 2 and 3) and the subsequent degeneration of VT into VF (panel 4) following H<sub>2</sub>O<sub>2</sub> exposure. The activation map in panel 1 (Fig. 2B) shows a sinus beat propagating under control condition from left to right (or base to apex) as the arrow indicates. The activation map in panel 2 shows the last sinus beat under H<sub>2</sub>O<sub>2</sub> condition immediately preceding VT onset; panel 2 is similar to panel 1 except for slightly slower conduction and the presence of H<sub>2</sub>O<sub>2</sub>-induced EAD in the corresponding optical AP traces that lengthened APD, thereby lengthening the wavelength (which is defined as the product of APD and conduction velocity and often used as a surrogate estimate of the refractory period). Panel 3 shows two foci during the onset of spontaneous VT originating from the top left and bottom right that collided and fused to propagate from left to right. Panel 4 shows at least two foci originating during the degeneration of VT into VF from the top left and bottom left, and propagating

from left to right, consistent with multifocal and probably also mixed focal-re-entrant VF, although re-entry was not evident in the panels illustrated.

To further explore possible EAD and afterdepolarization (DAD) mechanisms underlying VT/VF as captured by optical mapping, we performed microelectrode recording at the LV base, where most VT foci arose. In eight spontaneous VT episodes from six SHR hearts, VT was typically initiated by EAD-mediated triggered activity (representative case in Fig. 3). In three such hearts, once VT was initiated, in addition to EADs, DADs also emerged, consistent with findings from optical mapping. However, DADs never initiated VT (Fig. 3).

**Pacing-induced VT/VF under oxidative stress.** For the 24/24 NR and 20/30 SHR hearts that failed to manifest spontaneous VF after at least 90 min of H<sub>2</sub>O<sub>2</sub> exposure, we investigated their susceptibility to pacing-induced VF by rapidly pacing from the LV base at pacing cycle lengths (PCLs) of 120–250 ms. In SHR hearts, rapid pacing



**Figure 2. Degeneration of EAD-mediated focal VT into VF in SHR hearts exposed to  $H_2O_2$**   
**A**, voltage epifluorescence optical mapping (V-OMAP) from the LV base (AP traces 1–3) and apex (AP traces 4–6) of a representative SHR heart exposed to  $H_2O_2$  with simultaneous P-ECG recording (bottom trace) captured the onset of a spontaneous focal 8-beat VT episode arising from prior baseline sinus rhythm. The initial five VT beats were initiated by late phase 3 EADs (APs 1–3) at the base of heart. The subsequent two VT beats (6 and 7) were DAD-mediated triggered beats, whereas the very last VT beat (8) was another EAD-mediated triggered beat.



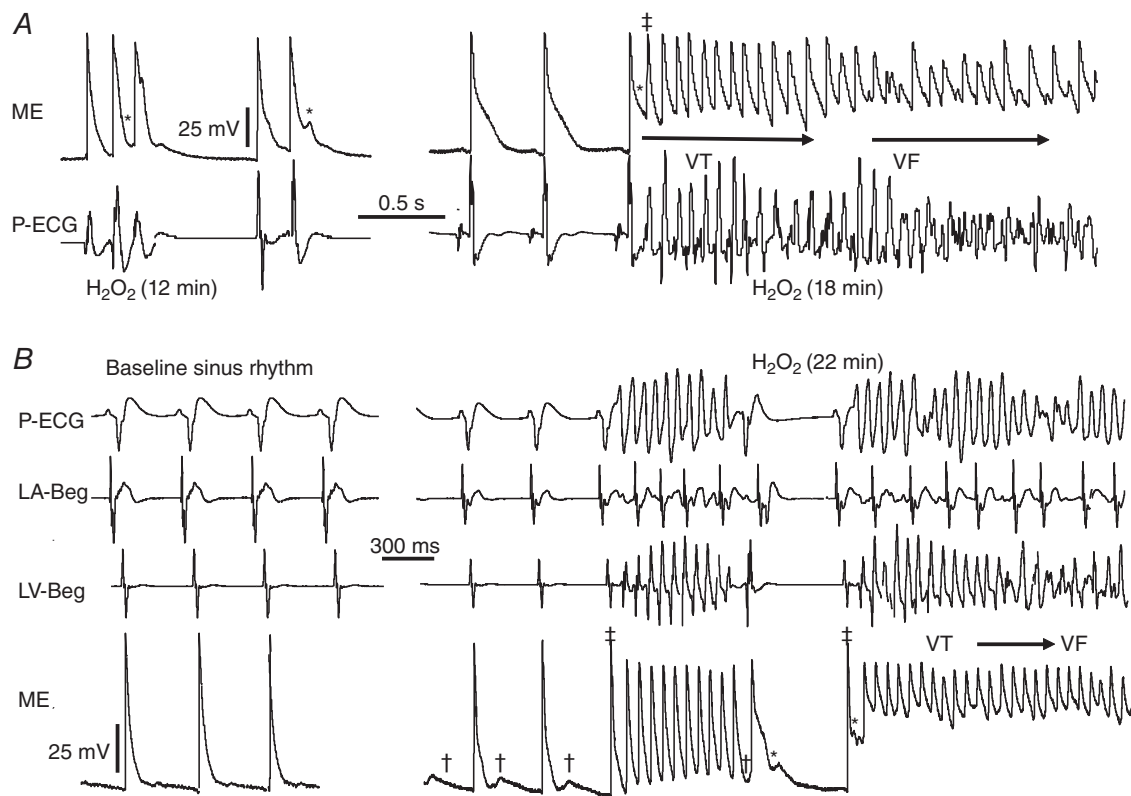
After this initial eight rapid triggered beats, the activation pattern degenerated into VF with multifocal irregular wavelets. The snapshots (bottom) illustrate the onset of VT and degeneration of VT into VF. *B*, isochronal activation maps (lower row) were constructed for selected beats (red \* and red dashed lines) from optical APs propagating from base to apex (traces 1–5, upper row) during sinus under control conditions prior to H<sub>2</sub>O<sub>2</sub> exposure (panel 1), then during the onset of VT (panels 2–3) and subsequent degeneration of VT into VF (panel 4) following H<sub>2</sub>O<sub>2</sub> exposure. During VT degeneration into VF, base-to-apex epicardial activation was prolonged and multiple foci (yellow \*) of conduction slowing and heterogeneous wavelengths emerged and collided, predisposing the LV to wavebreak and re-entry.

induced VF in 66% of cases. In NR hearts, rapid pacing induced only non-sustained VT ( $\leq 30$  s) in 38% of cases, although degeneration into VF was not observed (Table 2).

**H<sub>2</sub>O<sub>2</sub>-induced VF aborted by CaMKII inhibition.** We have previously shown, in isolated rabbit ventricular myocytes, that H<sub>2</sub>O<sub>2</sub> induces EADs through activation of CaMKII, which in turn enhances late sodium current ( $I_{Na}$ ) and L-type calcium current ( $I_{Ca,L}$ ) by channel phosphorylation (Xie *et al.* 2009). Similarly, in intact SHR hearts in the present study, we found that KN-93 ( $1 \mu\text{mol l}^{-1}$ ;  $n = 4$  hearts) converted H<sub>2</sub>O<sub>2</sub>-induced VF in three of four fibrillating hearts to sinus rhythm and, in the fourth heart, to a sustained VT that self-terminated within 20 s. We inter-

pret this finding to indicate that, even when CaMKII had been activated by phosphorylation, phosphatase activity was sufficient to decrease CaMKII activity significantly when rephosphorylation was prevented by KN-93. By contrast, the inactive isoform KN-92 ( $1 \mu\text{mol l}^{-1}$ ) failed to suppress H<sub>2</sub>O<sub>2</sub>-induced VF ( $n = 3$  SHR hearts), implicating CaMKII activation in the maintenance of H<sub>2</sub>O<sub>2</sub>-induced VF.

**APD dispersion and calcium handling dynamics.** We next compared AP and intracellular CaT characteristics between SHR and NR hearts during rapid pacing at four different PCLs of 300, 350, 200 and 150 ms using simultaneous dual voltage-calcium fluorescence optical



**Figure 3. Microelectrode recording of EAD-mediated triggered activity degenerating into VF in SHR hearts**

*A*, microelectrode (ME) with simultaneous P-ECG recording 12 and 18 min post-H<sub>2</sub>O<sub>2</sub> exposure illustrates longer lasting triggered activity (†) that degenerates to VF. *B*, another representative SHR heart manifests no EADs at stress-free baseline. After 22 min of H<sub>2</sub>O<sub>2</sub> exposure, DADs (†) emerge, followed by EAD (\*)-mediated triggered activity (†) causing VT, then VF ensues. LA/LV-Beg, left atrial/left ventricular bipolar electrogram.

**Table 3.** Left ventricular epicardial APD<sub>90</sub> and CaTD<sub>90</sub>

PCL (ms)		Baseline				H <sub>2</sub> O <sub>2</sub>			
		LV base		LV apex		LV base		LV apex	
		APD <sub>90</sub>	CaTD <sub>90</sub>	APD <sub>90</sub>	CaTD <sub>90</sub>	APD <sub>90</sub>	CaTD <sub>90</sub>	APD <sub>90</sub>	CaTD <sub>90</sub>
300	NR	112 ± 2	195 ± 4	115 ± 6	190 ± 3	113 ± 3	195 ± 16	116 ± 1	185 ± 15
	SHR	128 ± 7 <sup>***†††</sup>	178 ± 21	108 ± 4 <sup>†</sup>	170 ± 8 <sup>†††</sup>	135 ± 14 <sup>**††</sup>	200 ± 2 <sup>*</sup>	107 ± 7	185 ± 3
250	NR	98 ± 9	167 ± 7	96 ± 5	164 ± 8	100 ± 4	143 ± 4	99 ± 12	136 ± 12
	SHR	114 ± 19	142 ± 7 <sup>†††</sup>	99 ± 18	141 ± 9 <sup>††</sup>	125 ± 11 <sup>**†††</sup>	149 ± 4 <sup>†</sup>	104 ± 19	149 ± 20
200	NR	94 ± 8	123 ± 3	93 ± 17	125 ± 2	94 ± 9	125 ± 12	92 ± 10	124 ± 18
	SHR	110 ± 9 <sup>†</sup>	120 ± 3	99 ± 15	121 ± 7	119 ± 14 <sup>**††</sup>	130 ± 7	102 ± 18	124 ± 7
150	NR	88 ± 16	112 ± 9	87 ± 14	114 ± 1	91 ± 6	115 ± 7	88 ± 10	114 ± 2
	SHR	100 ± 8	116 ± 6	88 ± 15	115 ± 6	115 ± 7 <sup>**†††</sup>	124 ± 6 <sup>†</sup>	89 ± 17	120 ± 11

Simultaneous voltage and calcium imaging (four pairs of recordings at the LV base and four pairs at the LV apex per heart, per PCL) were performed for six NR and six SHR hearts before and after perfusion with H<sub>2</sub>O<sub>2</sub>. Data are reported as the mean ± SD. Intragroup comparison: \**P* < 0.05, \*\**P* < 0.005, \*\*\**P* < 0.0005; intergroup comparison: †*P* < 0.05, ††*P* < 0.005, †††*P* < 0.0005; the bootstrap method.

mapping of the LV epicardium (*n* = 6 hearts per group), both before and after H<sub>2</sub>O<sub>2</sub> perfusion (Table 3). In the absence of EADs and EAD-mediated triggered activity during rapid pacing, only modest intergroup differences in action potential at 90% duration (APD<sub>90</sub>) and CaT at 90% duration (CaTD<sub>90</sub>) existed between SHR and NR hearts both before and after H<sub>2</sub>O<sub>2</sub> exposure. In the intragroup analysis of NR hearts under both baseline and H<sub>2</sub>O<sub>2</sub> conditions, the APD<sub>90</sub> and CaTD<sub>90</sub> were essentially uniform over the entire LV epicardial surface. However, in the intragroup analysis of SHR hearts at baseline, a slight APD prolongation at the LV base compared to apex was seen during PCL of 300 ms (*P* = 0.0001). After H<sub>2</sub>O<sub>2</sub> exposure, the APD<sub>90</sub> base-to-apex gradient was seen for other PCLs tested as well. Also, a new CaTD<sub>90</sub> base-to-apex gradient developed for PCL of 300 ms. Additionally, exclusively in the SHR (but not NR) ventricles, CaT alternans was detected throughout the LV epicardium from base to apex during pacing at PCL of 150 ms (Fig. 4), as indicated by the increased ratio of minimal-to-maximal peak CaT amplitudes (SHR 0.6 ± 0.2 vs. NR 0.05 ± 0.02, *P* = 0.01, 95% CI [0.49,0.77]). Tall-short CaT alternans was closely associated with short-long APD alternans (Fig. 4C), suggesting a state of increased dispersion of refractoriness, which could potentially predispose the SHR ventricles to wavebreak and initiation of re-entry.

By contrast, during spontaneous rhythm typically at a rate (sinus CL ≥ 350 ms) slower compared to the rapid pacing rate (PCL ≤ 300 ms), H<sub>2</sub>O<sub>2</sub> often induced the chaotic irregular emergence of a variable number of EADs and/or EAD-mediated triggered activity per AP, thereby causing a marked increase of APD dispersion. For example, in this representative SHR heart exposed to H<sub>2</sub>O<sub>2</sub> (Fig. 2A), APD was 102 ± 7 ms and maximal APD dispersion was 15 ms during sinus rhythm. However,

during spontaneous VT, APD was irregularly lengthened up to 200 ± 150 ms, causing maximal APD dispersion to increase to 265 ms. During the subsequent degeneration of VT into VF, APD was irregularly lengthened to 192 ± 172 ms, causing maximal APD dispersion to further increase to 400 ms.

### Patch clamp studies of isolated single ventricular myocytes

To determine whether the increased susceptibility of SHR hearts to arrhythmias during oxidative stress was also observed at the isolated myocyte level, we performed current clamp studies on LV myocytes isolated from SHR and NR hearts. After 4–6 min of exposure to H<sub>2</sub>O<sub>2</sub> (0.15 mmol l<sup>-1</sup>), myocytes from both SHR and NR hearts readily developed EADs and repolarization failure during slow pacing (PCL from 6 to 0.5 s). As the PCL was shortened further to 0.25 s, EADs were eventually suppressed in myocytes from both SHR and NR groups to a similar extent (Fig. 5 and Table 4). Compared to NR myocytes (*n* = 24 myocytes from nine NR hearts), SHR myocytes (*n* = 22 myocytes from six SHR hearts) displayed slightly larger EAD amplitudes (SHR 39 ± 5 vs. NR 24 ± 6 mV, *P* = 0.02) but no significant baseline APD<sub>90</sub> prolongation (Fig. 5B). These findings suggest that, although there may be ion channel expression differences between myocytes from the two groups, their susceptibility to H<sub>2</sub>O<sub>2</sub>-induced EAD formation was similar.

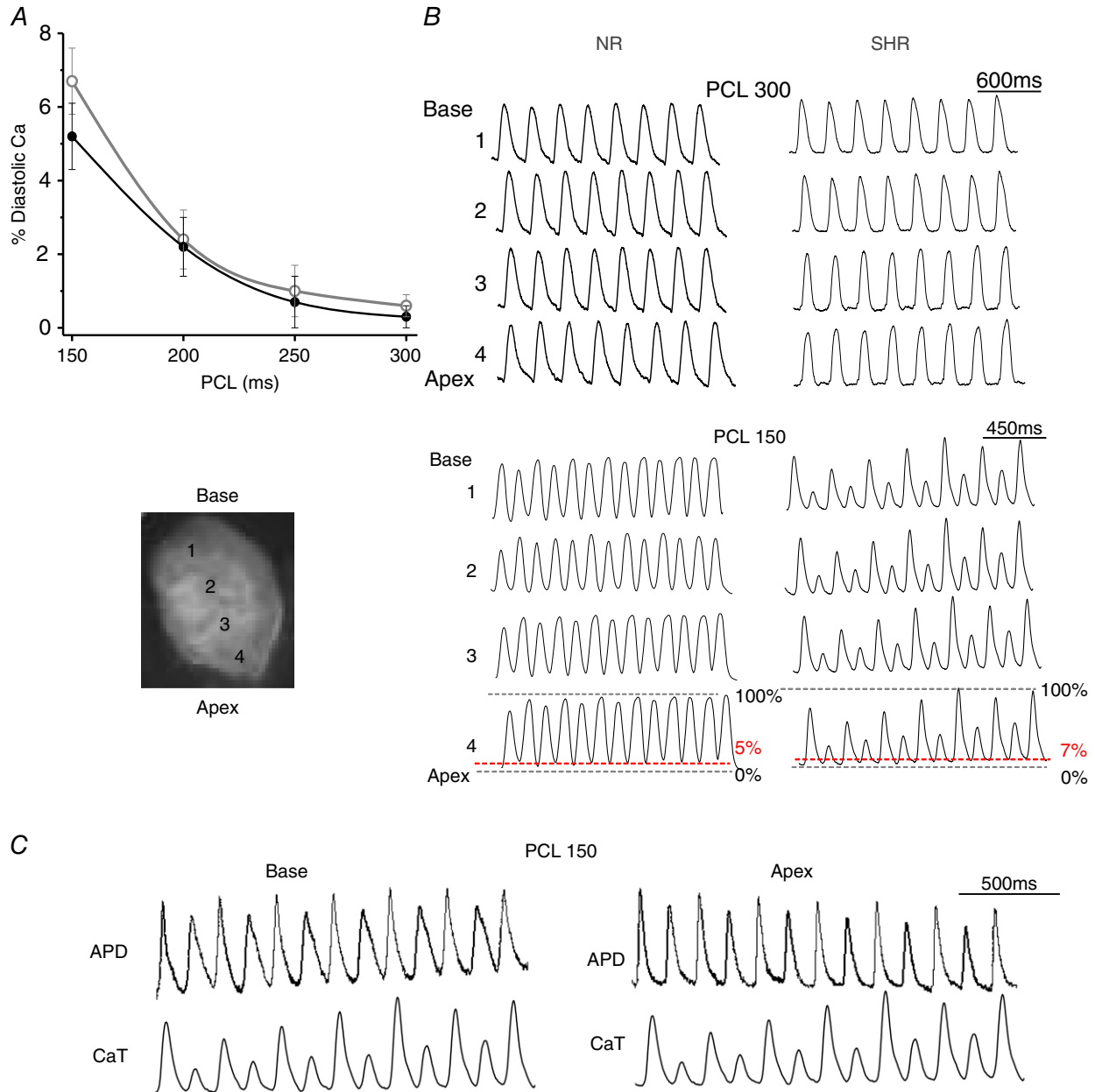
### Discussion

A major finding of the present study is the novel demonstration that, long before the development of overt heart failure, hearts from 5- to 6-month-old SHR have already

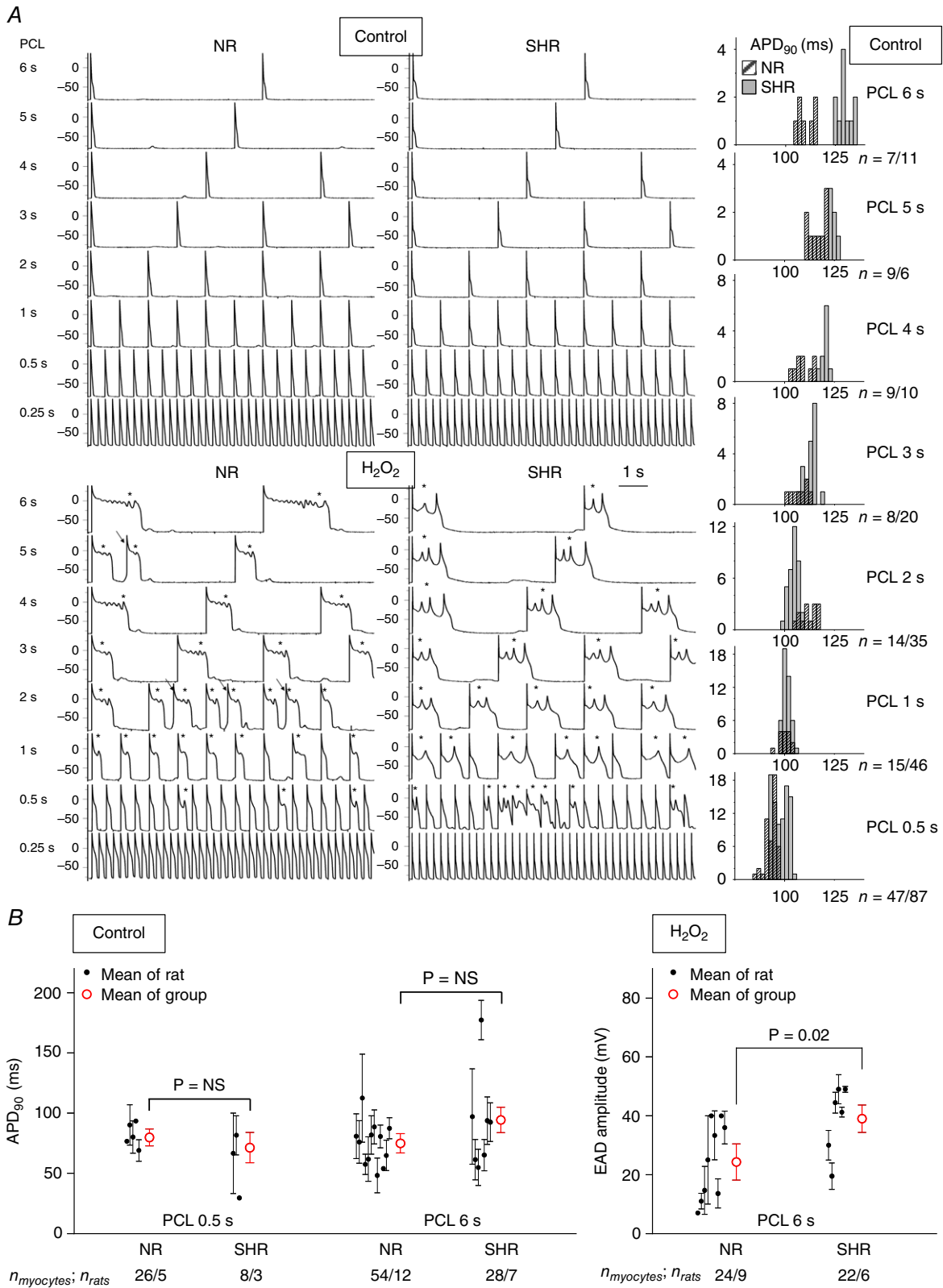
manifested an increased susceptibility to spontaneous VT/VF mediated by oxidative stress. Moreover, the increased susceptibility to H<sub>2</sub>O<sub>2</sub>-induced VT/VF appears to be primarily attributable to tissue (rather than cellular) electrophysiological differences between SHR and NR ventricles because isolated ventricular myocytes from SHR and NR responded similarly to oxidative stress.

### Cardiac remodelling in early hypertension

The inexorable progression to ventricular failure in chronic hypertension entails costly pathophysiological alterations. In the present study, we determined that adverse structural and electrical remodelling changes have already started in early hypertension, long before any clinical signs of heart failure.



**Figure 4. Rate-dependent CaT alternans in SHR hearts**  
 A, calcium epifluorescence optical mapping of SHR and NR hearts exposed to H<sub>2</sub>O<sub>2</sub> (*n* = 5 hearts per group) during four different PCLs of between 300 and 150 ms reveal similar rate-dependent diastolic calcium level. During PCL of 150 ms, the diastolic calcium amplitude averages 5–7% of the peak CaT in both groups. B, however, only SHR hearts manifest CaT alternans during PCL of 150 ms (bottom right). C, concurrent CaT alternans and APD alternans during PCL of 150 ms in SHR hearts, but not in NR hearts, may facilitate wavebreak and re-entry.



**Figure 5. Arrhythmia triggers in patch-clamped ventricular myocytes**

A, although even 2 mmol l<sup>-1</sup> H<sub>2</sub>O<sub>2</sub> cannot induce VT/VF in NR intact hearts, 0.15 mmol l<sup>-1</sup> H<sub>2</sub>O<sub>2</sub> induces VT/VF arrhythmia triggers, such as EADs (\*) and triggered activity (arrows) in this representative NR myocyte just as readily as in the representative SHR myocyte. Compared to the NR myocyte, the SHR myocyte has slightly more prolonged APs during slow pacing (PCL ≥ 3 s) at baseline (upper panels and histograms) and EADs with lower

frequencies and larger amplitudes during H<sub>2</sub>O<sub>2</sub> exposure (bottom). *n*, number of APs from the representative NR/or SHR myocyte. *B*, compared to NR myocytes, SHR myocytes do not have excessively prolonged APD<sub>90</sub> during either PCL at stress-free baseline but have slightly larger stress-induced EAD amplitudes during of PCL 6 s. The mean ± SEM for each rat is represented by a small black circle with whiskers, for each group by a large red circle with whiskers. *n*<sub>myocytes</sub>/*n*<sub>rats</sub>, number of myocytes/number of rats.

**Table 4. Incidence of EADs and triggered activity induced by H<sub>2</sub>O<sub>2</sub>**

Incidence of EADs (% , <i>n</i> )				
PCL	6 s	1 s	0.5 s	0.25 s
NR	100 (25)	86 (14)	60 (15)	14 (14)
SHR	100 (25)	57 (21)	50 (16)	6 (18)
<i>P</i> value	1.0	0.1	0.7	0.6
Incidence of triggered activity (% , <i>n</i> )				
PCL	6 s	1 s	0.5 s	0.25 s
NR	60 (25)	50 (14)	40 (15)	7 (14)
SHR	76 (25)	57 (21)	31 (16)	11 (18)
<i>P</i> value	0.4	0.2	0.7	1.0

Summary of the incidence, or fraction of myocytes, in which EADs or triggered activity were successfully induced by H<sub>2</sub>O<sub>2</sub> in single patch-clamped ventricular myocytes from NR vs. SHR hearts (*n*): number of myocytes. The statistical significance was assessed by a two-tailed Fisher's exact test.

Structurally, even when biventricular systolic function was preserved, SHR LV developed interstitial myocardial fibrosis (Fig. 1C) and, in keeping with systemic hypertensive haemodynamics, LV geometry adopted a concentric hypertrophy pattern (Fig. 1A) with markedly elevated RWT > 0.45, increased LV wall thickness (Table 1) and increased LV mass, which are all reliable prognostic markers associated with elevated peripheral resistance (Ganau *et al.* 1992). LVH reflected increases in ventricular myocyte length, diameter, and cross-sectional area (Fig. 1B), consistent with previously reported remodelling of myocyte shape prior to heart failure development in age-matched spontaneously hypertensive heart failure (SHHF) rats, which are related to SHR (Onodera *et al.* 1998). When investigating the temporal development of hypertrophy in 1- to 12-month-old SHHF rats prior to the development of heart failure at ~24 months of age, Onodera *et al.* (1998) found that the increase of LV myocyte length paralleled the continuous rise of systolic wall stress, although the myocyte transverse growth plateaued after reaching its upper limit by 3 months of age, such that the myocyte cross-sectional area reached a terminal upper value of twice the upper normal range at 3 months of age without further growth thereafter; therefore, the LV was 'robbed' of an important adaptive mechanism to normalize wall stress.

In conjunction with structural remodelling, electrical remodelling has also begun early in hypertension long before pump failure. In the present study, when isolated NR and SHR ventricular myocytes were exposed to H<sub>2</sub>O<sub>2</sub>, both readily developed EADs during PCL ≥ 0.5 s (Fig. 5). However, the EADs in NR myocytes had

smaller amplitudes and higher frequencies, whereas the EADs in SHR myocytes had larger amplitudes and lower frequencies, with the last EAD before full repolarization having the largest amplitude, typical of a Hopf-homoclinic bifurcation (Tran *et al.* 2009; Chang *et al.* 2012; Qu & Chung, 2012). To the best of our knowledge, these divergent EAD behaviours are reported in the present study for the first time and suggest underlying basic differences in intracellular calcium cycling dynamics, wherein ventricular myocytes from SHR as young as 5–6 months of age have steeper slopes of *I*<sub>Ca,L</sub> activation and inactivation kinetics (Qu *et al.* 2013). Other reported differences in SHR ionic current remodelling include a reduction of transient outward potassium current (*I*<sub>to</sub>) current density (Li & Jiang, 2000; Goltz *et al.* 2007), similar to that occurring in heart failure and a reduction of inward rectifier potassium current density (Brooksby *et al.* 1993), which may also account for the larger amplitude of EADs. Despite distinct characteristic profiles of ionic currents contributing to EAD genesis, both SHR and NR ventricular myocytes displayed remarkably similar EAD responses to H<sub>2</sub>O<sub>2</sub> induction, which could not *per se* account for the divergent arrhythmogenic vulnerability of the fibrotic SHR ventricular tissue.

#### Bradycardia-dependence of EAD emergence and APD lengthening by H<sub>2</sub>O<sub>2</sub>

Arising in the setting of reduced repolarization reserve and often serving as triggers for VT/VF, EADs are membrane voltage oscillations that interrupt and retard repolarization of the cardiac action potential, resulting in

the lengthening of APD (Qu & Chung, 2012). In the present study, when SHR ventricular tissue and myocytes were exposed to  $150 \mu\text{mol l}^{-1}$   $\text{H}_2\text{O}_2$ , EADs emerged during  $\text{CL} \geq 350$  ms (Figs 2 and 5A,  $\text{H}_2\text{O}_2$  panel,  $\text{PCL} \geq 0.5$  s) but were suppressed during  $\text{CL} \leq 300$  ms (Fig. 5A,  $\text{H}_2\text{O}_2$  panel,  $\text{PCL}$  of 0.25 s and Table 3), indicating that the emergence  $\text{H}_2\text{O}_2$ -induced EADs is 'bradycardia'-related. With complete suppression of EADs and EAD-mediated triggered activity during rapid pacing ( $\text{PCL} \leq 300$  ms), there was very little  $\text{H}_2\text{O}_2$ -induced lengthening of APD (Table 3,  $\text{H}_2\text{O}_2$  panel,  $\text{PCL}$  of 0.25 s), consistent with our previous observations in isolated rabbit ventricular myocytes exposed to higher doses of  $\text{H}_2\text{O}_2$  (Sato *et al.* 2010; Nguyen *et al.* 2012). By contrast, during a slower rate ( $\text{CL} \geq 350$  ms), either arising spontaneously from the tissue (Fig. 2) or by slow pacing of the patch-clamped myocytes (Fig. 5A,  $\text{H}_2\text{O}_2$  panel,  $\text{PCL} \geq 0.5$  s), the same  $\text{H}_2\text{O}_2$  concentration ( $150 \mu\text{mol l}^{-1}$ ) caused significant irregular lengthening of APD with the presence of variable numbers of EADs and EAD-mediated triggered activity such that the resultant repolarization failure caused APD to increase up to 2-fold during VT and up to 5-fold during VF (Fig. 2). Our findings of the bradycardia-dependence of APD lengthening reported in the present study are consistent with prior simulated predictions (Qu & Chung, 2012) and experimental observations of significant APD lengthening (recorded by glass microelectrode) in aged rat hearts by  $\text{H}_2\text{O}_2$  ( $100 \mu\text{mol l}^{-1}$ ) only during slow rate (spontaneous  $\text{CL}$  of 350 ms in Pezhouman *et al.* 2014;  $\text{CL}$  of 410 and 600 ms in Morita *et al.* 2011b).

The underlying mechanisms for these bradycardia-dependent effects of  $\text{H}_2\text{O}_2$  were demonstrated by our group (Xie *et al.* 2009) and others (Ward & Giles, 1997; Zhao *et al.* 2012) to include (1) impairment of  $I_{\text{Na}}$  inactivation; (2) enhancement of the window and pedestal  $I_{\text{Ca,L}}$ ; both (1) and (2) through activation of CaMKII; and (3) enhancement of the conductance, retardation of inactivation, and acceleration of the recovery from the inactivation of the  $I_{\text{to}}$ . These effects of  $\text{H}_2\text{O}_2$  on induction of EADs and triggered activity leading to AP prolongation are eliminated by either increasing the pacing rate or inhibiting CaMKII or  $I_{\text{to}}$ . However, it is worth noting that this rate-dependence of EAD emergence and suppression is independent of the stress intervention used to induce EADs (Bapat *et al.* 2012; Pezhouman *et al.* 2015) and has been observed across species (Sato *et al.* 2010; Nguyen *et al.* 2012; Nguyen *et al.* 2015), assumed to be related, at least in part, to the delayed activation kinetics of the slow delayed rectifier potassium current ( $I_{\text{Ks}}$ ) from more deeply closed states during bradycardia, as reported previously (Zeng & Rudy, 1995; Qu *et al.* 2013).

The bradycardia-dependence of EAD emergence and APD lengthening during oxidative stress may have clinical relevance in at least two respects: (1) anti-tachycardia pacing (also known as overdrive pacing or entrainment),

which has been routinely used by electrophysiologists to terminate refractory ventricular tachycardia in human patients (Llewellyn & Ramsdale, 1987) or mammalian models (Furukawa *et al.* 1990; Arnar *et al.* 2005) by taking advantage of a  $\text{CL}$  that is more rapid than the  $\text{CL}$  of the VT to minimize the APD lengthening induced by a state of reduced repolarization reserve in the vulnerable cardiac substrate and (2) the differential rate-related fatal cardiac arrhythmias in LQT2 and LQT3 vs. LQT1 patients: sudden cardiac deaths of LQT2 and LQT3 patients are bradycardia-related and tend to occur during sleep or at rest because repolarization reserve is reduced disproportionately during bradycardia as a result of delayed activation kinetics of  $I_{\text{Ks}}$  from deeply closed states of the channel. By contrast, cardiac events of LQT1 patients tend to be tachycardia-related and are often exercise-induced because of the drastic reduction of  $I_{\text{Ks}}$  such that repolarization reserve is reduced during tachycardia when adrenergic stimulation of  $I_{\text{Ca,L}}$  overwhelms adrenergic stimulation of  $I_{\text{Ks}}$  (Qu *et al.* 2013).

### The dynamics of ventricular tachycardia

A potentially important risk factor for the increased arrhythmogenicity in SHR hearts is the regional fibrosis at the LV epicardial base (Fig. 1C), where EAD-mediated triggered activity most frequently, as revealed by both optical mapping and microelectrode recording (Fig. 2). Fibrosis can increase arrhythmia risk by altering tissue properties (diffusive coupling between myocytes), without otherwise altering the arrhythmogenic properties of individual cells in the tissue (Nguyen *et al.* 2014). This is because the loading (source-sink) effects in well-coupled tissue make it very difficult for a small number of myocytes with an EAD or DAD (the source) to excite adjacent myocytes without an EAD or DAD (the sink). As gap junction coupling between myocytes decreases (either as a result of gap junction remodelling or fibrosis, which equivalently eliminated gap junction coupling by interposing collagen bundles), the sink effect is markedly weakened, allowing EADs or DADs to emerge and trigger focal activity. In addition, fibrosis also slows conduction, allowing those triggers to induce re-entry. This phenomenon has been readily demonstrated in computer simulations (Xie *et al.* 2010; Nguyen *et al.* 2012), in which the cells exhibiting the exact same EAD or DAD regime are unable to generate triggered activity in well-coupled tissue, whereas, when gap junction coupling is reduced either directly or by simulating fibrosis, triggered activity readily emerges.

Why the SHR LV epicardial base is preferentially susceptible to fibrosis remains unknown, although it may relate to a higher wall tension at the LV base because of its greater radius of curvature compared to the LV apex (Sandler & Dodge, 1963). A previous study in 1-year-old SHR rats showed that the extent of fibrosis in the

foci of replacement fibrosis in the LV correlated with the occurrence of VF (Pahor *et al.* 1991). Moreover, chronic treatment with the angiotensin-converting enzyme inhibitor, enalapril, attenuated myocardial fibrosis and decreased VF vulnerability (Pahor *et al.* 1991). Besides LV fibrosis, LVH is another feature of structural remodelling that may also contribute to the vulnerability to oxidative-stress-induced VT/VF (Wachtell *et al.* 2007). Even though the underlying mechanisms for such a contribution are not precisely known, a similar correlation between LVH and sudden cardiac death was reported for patients with isolated LVH and sudden cardiac death (Tamarappoo *et al.* 2012).

### Degeneration of ventricular tachycardia into fibrillation

In the present study, we found that, in 5- to 6-month-old SHR hearts, CaT alternans emerged readily during PCL of 150 ms (Fig. 4B) in both the LV base and apex exclusively in SHR hearts, coinciding with APD alternans (Fig. 4C), although, during this very rapid pacing rate, there was only mild APD lengthening at the LV base. This is an important issue because APD alternans reflects a marked increase in dispersion of refractoriness that can predispose the ventricles to wavebreak and initiation of alternans-induced re-entry for VT/VF (Qu *et al.* 2000). The vulnerable window of re-entry is much larger for SHR compared to NR ventricles as a result of the presence of fibrosis because the structural barriers to wave propagation that developed during fibrotic remodelling lower the threshold for repolarization alternans (Pastore & Rosenbaum, 2000; Krogh-Madsen & Christini, 2007). Although the mechanism underlying CaT alternans resides in the disturbance of calcium signalling, APD alternans is a secondary consequence, mediated by calcium-dependent AP modulation.

Previous simulation studies on different animal models have demonstrated that the degeneration of VT into VF is associated with the breakup of a spiral wave of the action potential in the ventricular tissue with steep APD restitution (Qu *et al.* 1999; Xie *et al.* 2014). In the present study, although rapid pacing could induce VT in NR hearts, progression to VF failed. This failure of pacing-induced VT to degenerate into VF in the NR hearts may stem from the protective shallow APD restitution slope. By contrast, because fibrosis causes random cellular uncoupling that promotes APD dispersion and alternans (Qu *et al.* 2004), the fibrotic SHR ventricles were more vulnerable to re-entry as a result of a steeper APD restitution slope. When APD restitution is shallow, such as in NR hearts, wavebreak may be induced through conduction slowing but only in regions with very large pre-existing electrical heterogeneity and, even then, re-entry cannot be easily induced because the wavelength

(hence refractoriness) of the NR tissue in this region is long and the broken wave does not have sufficient surrounding excitable local tissue to execute a full turn. However, when APD restitution is sufficiently steep to produce alternans, such as in SHR hearts (Fig. 4B and C), the vulnerable window of re-entry is much larger because alternans can promote wavebreak through dynamical instability with wavelength oscillation, conduction slowing, and markedly increased dispersion of refractoriness (Qu *et al.* 2000). In the present study, the fact that multiple foci were perpetuating the spontaneous VF in SHR hearts (Fig. 2B, panel 4) explains why the ongoing VF could be terminated by KN-93, which suppressed the foci necessary for the maintenance of wavebreak and VF.

### Limitations

Although our method of blood pressure measurement has the advantage of being non-invasive, the disadvantage is that such a method precludes reliable concomitant measurement of diastolic blood pressure (DBP). Accurate assessment of DBP often requires the invasive surgical implantation of a catheter into a rat artery (e.g. a carotid artery); we did not employ such an invasive method in the present study to avoid potential data confounding with the inevitable post-surgical stress, inflammation, and associated elevated oxidant state possibly altering the SHR and NR hearts differently. However, another group of investigators recently performed direct intravascular recordings using a catheter inserted into the abdominal aorta of 4- to 5-month-old SHR and found SBP elevation of  $181 \pm 5$  mmHg (comparable to our findings of SBP  $185 \pm 15$  mmHg) associated with DBP elevation of  $138 \pm 3$  mmHg (Jackson *et al.* 2015). It is also worth noting that pure systolic hypertension in humans predisposes to cardiovascular disease and is a harbinger of increased morbidity and mortality.

Another limitation in our methods is the use of cytochalasin D in optical mapping studies to suppress cardiac contraction and reduce motion artefacts. The well-studied side effects of cytochalasin D on ion channels and intracellular signalling pathways reportedly develop, especially with concentrations  $\geq 3 \mu\text{mol l}^{-1}$ , although concentrations as high as  $10 \mu\text{mol l}^{-1}$  were used in some studies (Hayashi *et al.* 2003; Nygren *et al.* 2006). However, we have not noted any arrhythmogenic adverse effects for NR hearts under basal or stress conditions or for SHR hearts under basal conditions with the use of  $1 \mu\text{mol l}^{-1}$  of cytochalasin D.

As a prototype for oxidative stress, in the present study, we used  $\text{H}_2\text{O}_2$  and did not test other reactive oxygen species. However, we have previously shown that, similar to  $\text{H}_2\text{O}_2$ , angiotensin II (which activates CaMKII and endogenous reactive oxygen species generation via NADPH oxidase) produced EAD-mediated arrhythmias, including

VT/VF, in aged fibrotic rat hearts as well as EADs and triggered activity in isolated adult rat ventricular myocytes (Bapat *et al.* 2012). Our group used yet a third oxidant-generating system, the xanthine-xanthine oxidase system, and discovered that oxidative stress-mediated afterpotentials were not unique to H<sub>2</sub>O<sub>2</sub> because they could also be induced by xanthine-xanthine oxidase (Goldhaber, 1996). Additionally, although the KN-93 experiments demonstrated that CaMKII activation is a necessary component of H<sub>2</sub>O<sub>2</sub>-induced VT/VF, CaMKII activation alone may not be sufficient. Other effects of H<sub>2</sub>O<sub>2</sub>, such as the redox effects on proteins or the activation of other signalling pathways (e.g. guanylate cyclase), may also be important and could be tested with guanylate cyclase inhibitors in the absence of KN-93.

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## Additional information

### Competing interests

The authors declare that they have no competing interests.

### Author contributions

HSK and TPN conceived, designed, supervised the project, and drafted the manuscript. AAS, AP, HC, AB and NV performed electrophysiological experiments on intact perfused hearts. SI performed echocardiography. CYK performed gross pathological measurements. MCF performed histology studies. TPN performed electrophysiological experiments on isolated myocytes. TPN, AAS, AP, SI, CYK, MG, MCF and HSK analysed data. TPN, AP, SI, CYK, MCF and HSK interpreted the experimental findings. TPN, AAS, AP, SI, HC, CYK, AB, NV, MG, MCF and HSK prepared the figures. TPN, AP, SI and CYK performed statistical analyses with the invaluable assistance of Dr Jeffrey Gornbein from the Statistical/Biomathematical Consulting Clinic of the UCLA Department of Biomathematics. TPN and HSK edited and revised the manuscript with the invaluable assistance of Dr James N. Weiss. Experiments were performed in the Cardiovascular Research Laboratory at UCLA. All authors approved the manuscript final version and agreed to be accountable for all aspects of the work in ensuring that questions related to the accuracy or integrity of any part of the

work were appropriately investigated and resolved. All persons designated as authors qualify for authorship, and all those who qualify for authorship are listed.

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### Translational perspective

We show that, long before pump failure in hypertension, 5- to 6-month-old hypertensive rat hearts have already manifested increased susceptibility to both spontaneous and pacing-induced ventricular tachycardia and fibrillation when challenged with oxidative stress. This increased susceptibility to ventricular arrhythmias is attributable to properties primarily at the tissue level (rather than cellular level), such as left ventricular hypertrophy or fibrosis. The implication of our findings, to the extent that they can be extrapolated to humans, is that uncontrolled hypertension prior to overt development of systolic dysfunction and congestive heart failure increases the risk of ventricular tachyarrhythmias. Early treatment of hypertension with the goal towards the optimization of blood pressure control and the regression of left ventricular hypertrophy may be warranted.