CROSSTALK

CrossTalk opposing view: The middle cerebral artery diameter does not change during alterations in arterial blood gases and blood pressure

R. Matthew Brothers¹ and Rong Zhang2,3 *1Department of Kinesiology, University of Texas at Arlington, Arlington, TX, USA 2Institute for Exercise and Environmental Medicine, Texas Health Presbyterian Hospital, Dallas, TX, USA 3Department of Internal Medicine, University of Texas Southwestern Medical Center, Dallas, TX, USA* Email: matthew.brothers@uta.edu

The cerebral circulation is regulated by arterial carbon dioxide tension (P_{aCO_2}) with hypercapnia and hypocapnia increasing and decreasing cerebral blood flow (CBF), respectively (Serrador *et al.* 2000; Ide *et al.* 2003). This relationship between CBF and P_{aCO_2} , termed cerebral vasomotor reactivity, provides a measure of cerebral vascular function. Reduction of cerebral vasomotor reactivity is associated with carotid artery disease (Ringelstein *et al.* 1988), diabetes (Kadoi *et al.* 2003) and hypertension (Lavi *et al.* 2006), and is a predictor and contributor to stroke (Gur *et al.* 1996; Nur *et al.* 2009). Furthermore, cerebral vascular dysfunction has been implicated in other conditions including cognitive dysfunction and Alzheimer's disease (Silvestrini *et al.* 2006; Bar *et al.* 2007). A number of approaches are used to assess cerebral vascular function during perturbations of arterial blood gases or blood pressure. Transcranial Doppler (TCD) assessment of cerebral blood flow velocity (CBFV) in the middle cerebral artery (MCA) is commonly used for measuring changes in CBF (Aaslid *et al.* 1989). Advantages of TCD include relative ease of use, being fairly inexpensive in comparison with other techniques, being non-invasive, and beat-to-beat data collection thus providing high temporal resolution. However, Doppler ultrasonography, and TCD in particular, cannot image the insonated intracranial blood vessels and thus relies solely on CBFV as an indirect measure of CBF assuming that the diameters of the insonated blood vessels do not change (Aaslid *et al.* 1989; Serrador *et al.* 2000; Claassen *et al.* 2007). Accordingly, any deviations from this assumption need to be considered carefully for TCD interpretation in that, based on the principle of the Hagen–Poiseuille law, a small change in the diameter of the insonated MCA would have an effect on CBF that is not reflected by CBFV.

Earlier work reported changes in diameter of smaller downstream cerebral resistance vessels during alterations in P_{aCO_2} (Huber & Handa, 1967; Giller*et al.* 1993). In the 1960s itwas reported that the downstream cerebral arterioles dilated by \sim 25% during hypercapnia (P_{aCO_2} of \sim 58 Torr) whereas the larger cerebral arteries remained constant during relative eucapnia (Huber & Handa, 1967). These findings are supported by other angiographic studies (Djurberg *et al.* 1998). Additionally, Giller *et al.* (1993) reported an \sim 25% dilatation in the anterior cerebral artery (ACA) and the M2 segment of the MCA during hypercapnia (ΔP_{aCO_2} of about $+14$ Torr); however, the diameter of the larger M1 segment of the MCA remained constant (*<* 4% change; Giller *et al.* 1993). More recently, Schreiber*et al.*(2000) imaged the M1 segment of the MCA, using magnetic resonance imaging (MRI; scans obtained at 1.5 T), before and during hypercapnia with

a range of ΔP_{aCO_2} of +1.4 to 17.2 Torr. There was no effect of this stimulus on the diameter of the M1 segment of the MCA (Schreiber *et al.* 2000). These findings support the notion of a constant diameter of the larger cerebral arteries during changes in P_{aCO} , and the validity of TCD assessment of CBF with CBFV since it is most commonly performed in the larger more proximal M1 segment of the MCA (Serrador *et al.* 2006; Coverdale *et al.* 2014; Yonan *et al.* 2014). However, the measures of Giller *et al.* (1993) were conducted during craniotomy under anaesthesized conditions while the individuals in the study by Schreiber *et al.* (2000) suffered from chronic internal carotid artery occlusion. It is unknown if these conditions would impact cerebral vascular function thereby masking potential effects of the perturbation. Serrador *et al.* assessed the diameter of the MCA during hypercapnia ($\Delta CO_2 \sim 8$ Torr) and hypocapnia ($\Delta CO_2 \sim 12$ Torr) using MRI scans at 1.5 T and reported no change in MCA diameter during either stimulus (Serrador *et al.* 2000). The findings in the hypocapnic range are in agreement with a previous study using MRI scans at 1.5 T that reported no change in MCA diameter during hypocapnia ($\Delta CO_2 \sim 12$ Torr; Valdueza *et al.* 1997). Importantly, these MRI studies were conducted in healthy individuals and thus lend support to the aforementioned findings of a constant MCA diameter of the M1 segment during alterations in blood gases (Huber & Handa, 1967; Giller *et al.* 1993; Djurberg *et al.* 1998; Schreiber *et al.* 2000).

In recent years, several studies have assessed blood flow in the extracranial arteries that feed the cerebral circulation including the internal carotid artery (ICA) and vertebral artery (VA). This approach combined with simultaneous measures of

R. Matthew Brothers is an Associate Professor in the Department of Kinesiology at The University of Texas at Arlington. His research focuses on investigation of mechanisms of cerebral and peripheral vascular control in healthy individuals and at risk or diseased populations. This includes the assessment of blood flow responses to environmental conditions as well as lifestyle interventions to assess impairments in physiological function. **Rong Zhang** is an Associate Professor of Internal Medicine, Neurology and Neurotherapeutics at the University of Texas Southwestern Medical Center and is the Director of the Cerebrovascular Laboratory at the Institute for Exercise and Environmental Medicine at Texas Health Presbyterian Hospital Dallas. The focus of his Laboratory is age-related changes in brain perfusion, structure and function under normal and diseased conditions with the ultimate goal to improve brain health and quality of life in older adults.

CBFV in the MCA during changes in arterial blood pressure to assess cerebral autoregulation (Liu *et al.* 2013) and changes in arterial blood gases to assess extracranial and intracranial vascular reactivity has led to conclusions that there are some discrepancies between changes in blood flow in the ICA and CBFV assessed in the MCA by transcranial Doppler (Willie *et al.* 2012; Coverdale *et al.* 2014, 2015). Such findings may imply that the diameter of the MCA does in fact change during alterations in blood gases and/or arterial blood pressure. However, as of now there is no definitive evidence that changes in extracranial blood flow are linearly linked with changes in specific intracranial blood vessels (Thomas *et al.* 2015). This is particularly true of the ICA, which in addition to the MCA also delivers blood to the anterior cerebral artery (Willie *et al.* 2012; Liu *et al.* 2013). More direct measures are achievable using MRI. The aforementioned studies reporting no change in the M1 segment of the MCA were conducted using MRI scans at 1.5 T using imaging parameters that may have low spatial resolution (Serrador *et al.* 2000). Recent studies have been performed using high magnetic field strength of 3.0 T (Coverdale *et al.* 2014, 2015) and 7.0 T (Verbree *et al.* 2014) with high spatial resolutions (*<* 1mm). These studies reported a significant vasodilatation in the MCA of approximately 8% during higher degrees of hypercapnia $(\Delta CO_2 \sim 10-15$ Torr; Coverdale *et al.* 2014, 2015; Verbree *et al.* 2014), while no changes in the MCA diameter during a less severe hypercapnia (ΔCO_2 about +7 Torr; Verbree *et al.* 2014). Thus, whether or not the diameter of the MCA changes is likely to be dependent on the magnitude of changes in P_{aCO_2} (Ainslie & Hoiland, 2014; Coverdale *et al.* 2014, 2015; Verbree *et al.* 2014). Hypercapnia results in increases in mean arterial pressure (MAP) and changes in cerebral autoregulation (Coverdale *et al.* 2014, 2015). Therefore, changes in MCA diameter during higher degrees of hypercapnia may be related to cerebral autoregulation in response to changes in blood pressure rather than hypercapnia *per se*. These studies also reported relatively small vasoconstriction in the MCA of \sim 1–4% during hypocapnia $(\Delta CO_2$ about -7.5 (Verbree *et al.* 2014) and about −13 Torr (Coverdale *et al.* 2014, 2015)), interpreted as the cerebral circulation being in a tonic state of vasoconstriction resulting in a reduced

effect of hypocapnia to induce further constriction (Coverdale *et al.* 2014, 2015; Verbree *et al.* 2014).

The effect of changes in blood pressure on the MCA diameter is even less understood than that of arterial blood gases. The ACA and M2 segment of the MCA dilated \sim 25% whereas the M1 segment of the MCA was unaffected during large alterations in blood pressure (Δ range of 30 mmHg during nitroprusside and phenylephrine infusion; Giller *et al.* 1993). Furthermore, the M1 segment of the MCA was unchanged during moderate hypotension in healthy humans as assessed using 1.5 T MRI (Serrador *et al.* 2000). Currently, there are few studies that have been designed to directly assess the relationship between changes in blood pressure and diameter of the MCA.

In conclusion, strong evidence indicates that the M1 segment of the MCA averaged over cardiac cycles under steady-state haemodynamic conditions remains relatively constant during moderate changes in arterial blood gases and blood pressure. However, we caution that the findings opposing this view, particularly during larger changes in blood gases and blood pressure, cannot be ignored. This degree of uncertainty combined with the physiological and clinical significance of regulation of the cerebral vasculature in health and disease highlights the importance of continued research in this area. With the advent of more innovative study designs and high temporal and spatial resolution neuroimaging methodologies it is likely that more definitive answers to this highly debated and relevant topic are to come.

Call for comments

Readers are invited to give their views on this and the accompanying CrossTalk articles in this issue by submitting a brief (250 word) comment. Comments may be submitted up to 6 weeks after publication of the article, at which point the discussion will close and the CrossTalk authors will be invited to submit a 'Last Word'. Please email your comment, including a title and a declaration of interest, to [jphysiol@physoc.org.](http://jphysiol@physoc.org) Comments will be moderated and accepted comments will be published online only as 'supporting information' to the original debate articles once discussion has closed.

References

Aaslid R, Markwalder TM & Nornes H (1989). Noninvasive transcranial Doppler ultrasound recording of flow velocity in basal cerebral arteries. *J Neurosurg* **57**, 769–774.

- Ainslie PN & Hoiland RL (2014). Transcranial Doppler ultrasound: valid, invalid, or both? *J Appl Physiol (1985)* **117**, 1081–1083.
- Bar KJ, Boettger MK, Seidler N, Mentzel HJ, Terborg C & Sauer H (2007). Influence of galantamine on vasomotor reactivity in Alzheimer's disease and vascular dementia due to cerebral microangiopathy. *Stroke* **38**, 3186–3192.
- Claassen JA, Zhang R, Fu Q, Witkowski S & Levine BD (2007). Transcranial Doppler estimation of cerebral blood flow and cerebrovascular conductance during modified rebreathing. *J Appl Physiol* **102**, 870–877.
- Coverdale NS, Gati JS, Opalevych O, Perrotta A & Shoemaker JK (2014). Cerebral blood flow velocity underestimates cerebral blood flow during modest hypercapnia and hypocapnia. *J Appl Physiol (1985)* **117**, 1090–1096.
- Coverdale NS, Lalande S, Perrotta A & Shoemaker JK (2015). Heterogeneous patterns of vasoreactivity in the middle cerebral and internal carotid arteries. *Am J Physiol Heart Circ Physiol* **308**, H1030–H1038.
- Djurberg HG, Seed RF, Evans DA, Brohi FA, Pyper DL, Tjan GT & al Moutaery KR (1998). Lack of effect of $CO₂$ on cerebral arterial diameter in man. *J Clin Anesth* **10**, 646–651.
- Giller CA, Bowman G, Dyer H & Mootz L (1993). Cerebral arterial diameters during changes in blood pressure and carbon dioxide during craniotomy. *Neurosurgery* **32**, 737–741.
- Gur AY, Bova I & Bornstein NM (1996). Is impaired cerebral vasomotor reactivity a predictive factor of stroke in asymptomatic patients? *Stroke* **27**, 2188–2190.
- Huber P & Handa J (1967). Effect of contrast material, hypercapnia, hyperventilation, hypertonic glucose and papaverine on the diameter of the cerebral arteries. Angiographic determination in man. *Invest Radiol* **2**, 17–32.
- Ide K, Eliasziw M & Poulin MJ (2003). The relationship between middle cerebral artery blood velocity and end-tidal PCO₂ in the hypocapnic-hypercapnic range in humans. *J Appl Physiol* **95**, 129–137.
- Kadoi Y, Hinohara H, Kunimoto F, Saito S, Ide M, Hiraoka H, Kawahara F & Goto F (2003). Diabetic patients have an impaired cerebral vasodilatory response to hypercapnia under propofol anesthesia. *Stroke* **34**, 2399–2403.
- Lavi S, Gaitini D, Milloul V & Jacob G (2006). Impaired cerebral CO₂ vasoreactivity: association with endothelial dysfunction. *Am J Physiol Heart Circ Physiol* **291**, H1856–H1861.
- Liu J, Zhu YS, Hill C, Armstrong K, Tarumi T, Hodics T, Hynan LS & Zhang R (2013). Cerebral autoregulation of blood velocity and volumetric flow during steady-state changes in arterial pressure. *Hypertension* **62**, 973–979.
- Nur E, Kim YS, Truijen J, van Beers EJ, Davis SC, Brandjes DP, Biemond BJ & van Lieshout JJ (2009). Cerebrovascular reserve capacity is impaired in patients with sickle cell disease. *Blood* **114**, 3473–3478.
- Ringelstein EB, Sievers C, Ecker S, Schneider PA & Otis SM (1988). Noninvasive assessment of CO2-induced cerebral vasomotor response in normal individuals and patients with internal carotid artery occlusions. *Stroke* **19**, 963–969.
- Schreiber SJ, Gottschalk S, Weih M, Villringer A & Valdueza JM (2000). Assessment of blood flow velocity and diameter of the middle cerebral artery during the acetazolamide provocation test by use of transcranial Doppler sonography and MR imaging. *AJNR Am J Neuroradiol* **21**, 1207–1211.
- Serrador JM, Hughson RL, Kowalchuk JM, Bondar RL & Gelb AW (2006). Cerebral blood flow during orthostasis: role of arterial $CO₂$. *Am J Physiol Regul Integr Comp Physiol* **290**, R1087–R1093.
- Serrador JM, Picot PA, Rutt BK, Shoemaker JK & Bondar RL (2000). MRI measures of middle cerebral artery diameter in conscious humans during simulated orthostasis. *Stroke* **31**, 1672–1678.

- Silvestrini M, Pasqualetti P, Baruffaldi R, Bartolini M, Handouk Y, Matteis M, Moffa F, Provinciali L & Vernieri F (2006). Cerebrovascular reactivity and cognitive decline in patients with Alzheimer disease. *Stroke* **37**, 1010–1015.
- Thomas KN, Lewis NC, Hill BG & Ainslie PN (2015). Technical recommendations for the use of carotid duplex ultrasound for the assessment of extracranial blood flow. *Am J Physiol Regul Integr Comp Physiol* **309**, R707–R720.
- Valdueza JM, Balzer JO, Villringer A, Vogl TJ, Kutter R & Einhaupl KM (1997). Changes in blood flow velocity and diameter of the middle cerebral artery during hyperventilation: assessment with MR and transcranial Doppler sonography. *AJNR Am J Neuroradiol* **18**, 1929–1934.
- Verbree J, Bronzwaer AS, Ghariq E, Versluis MJ, Daemen MJ, van Buchem MA, Dahan A, van Lieshout JJ & van Osch MJ (2014). Assessment of middle cerebral artery diameter during hypocapnia and hypercapnia in humans using ultra-high-field MRI. *J Appl Physiol (1985)* **117**, 1084–1089.
- Willie CK, Macleod DB, Shaw AD, Smith KJ, Tzeng YC, Eves ND, Ikeda K, Graham J, Lewis NC, Day TA & Ainslie PN (2012). Regional brain blood flow in man during acute changes in arterial blood gases. *J Physiol* **590**, 3261–3275.
- Yonan KA, Greene ER, Sharrar JM, Caprihan A, Qualls C & Roldan CA (2014). Middle cerebral artery blood flows by combining TCD velocities and MRA diameters: in vitro and in vivo validations. *Ultrasound Med Biol* **40**, 2692–2699.

Additional information

Competing interests

None declared.

Author contributions

Both authors have approved the final version of the manuscript and agree to be accountable for all aspects of the work. All persons designated as authors qualify for authorship, and all those who qualify for authorship are listed.