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Abbreviations: BBB, Blood brain barrier; BCB, Blood CSF barrier; CBB, CSF-brain barrier; CNS, Central Nervous System; CSF, Cerebrospinal fluid; GLUT1, Glucose transporter-1; LAT1, Large neutral amino-acid transporter type 1; NP, Nanoparticle; P-gp, Pglycoprotein; Tf, Transferrin; TJ, Tight junction

While the role of the blood-brain barrier (BBB) is increasingly recognized in the (development of treatments targeting neurodegenerative disorders, to date, few strategies exist that enable drug delivery of non-BBB crossing molecules directly to their site of action, the brain. However, the recent advent of Nanomedicines may provide a potent tool to implement CNS targeted delivery of active compounds. Approaches for BBB crossing are deeply investigated in relation to the pathology: among the main important diseases of the CNS, this review focuses on the application of nanomedicines to neurodegenerative disorders (Alzheimer, Parkinson and Huntington's Disease) and to other brain pathologies as epilepsy, infectious diseases, multiple sclerosis, lysosomal storage disorders, strokes.

Introduction

The blood brain barrier (BBB)

The central nervous system (CNS) is protected from toxins and metabolic fluctuations by barriers, among which the blood-brain barrier (BBB) plays a key role in maintaining homeostasis. The BBB is composed of four major cellular components, the endothelial cells of the brain capillaries, pericytes, astrocytes, and the basement membrane. Together, they build a functional unit, the 'Neurovascular unit', mediating exchange between neurons, capillaries and glia. That way, the BBB supplies the brain with necessary nutrients, glucose and oxygen to sustain normal neural functioning. At the same time, the BBB plays a protective role against neurotoxic substances. Together, the BBB creates the neural microenvironment that is crucial for healthy brain function².

To fulfill this function, the brain has a very close-packed microvasculature.^{74,76} This enables very short distances between the nearest blood capillary and neuronal cells,⁹⁹ which allows a

Correspondence to: Giovanni Tosi; Email: gtosi@unimore.it Submitted: 12/29/2015; Revised: 02/02/2016; Accepted: 02/04/2016 http://dx.doi.org/10.1080/21688370.2016.1153568 fast delivery of substances after crossing the BBB. Further, the capillaries in the brain are quite different from capillaries found in the peripheral organs. Microvessels of the BBB are formed by non-fenestrated endothelial cells that contact each other forming tight junctions (TJs) (or zonula occludens). TJs prevent the passive diffusion of hydrophilic solutes via paracellular transport, the transfer of substances from the blood into brain parenchyma by passing through the intercellular space between the cells. Thus, water-soluble substances have to cross the BBB by mechanisms of transcellular transport that involve active transport via specific carriers.

In addition, brain capillaries are surrounded by pericytes protruding into the basement membrane, and astrocytic end feet encapsulating the surface (Grabrucker et al., 2014). Astrocytes release inductive signals that regulate the BBB ⁴³ and play a role in maintaining water, ionic, and amino acid homeostasis within the CNS.¹ With an electrical resistance estimated to be $\approx 1500-$ 2000 Ω cm², brain endothelium possesses a much higher electrical resistance than other systemic endothelia with $\approx 3-33 \ \Omega$ cm² ¹⁷ further limiting diffusion of certain molecules across the BBB. However, the BBB is a highly dynamic structure and its formation, maturity and integrity controlled by a collective action of all of its constituents. In addition, neurons have been shown to release growth or nutritional factors maintaining BBB functioning.

The consequence of this intricate interplay is a controlled and restricted transport of molecules across the BBB. Only very small (<400 Da) and lipophilic molecules can diffuse through the BBB, while the crossing of lipid insoluble or larger hydrophilic molecules is very limited. However, additionally to lipophilicity, other factors such as the affinity toward available transport system further control BBB crossing. For example, the transport of glucose through the BBB is mediated by glucose transporter-1 (GLUT-1).⁶⁰

The effectiveness of the BBB function depends on several factors such as the controlled expression of the major constituents of TJs, such as occluding proteins and proteins of the claudin family.² Further, molecules released during neural activity may act on receptors and transporters of endothelial cells and/or contacting astrocytes. Examples include neurotransmitters such as glutamate and serotonin, but also calcium, and adrenaline.⁷⁵ Through these modulatory agents, several parameters of the BBB such as capillary diameter (and thus local blood flow), expression of specific transporters, and the tightness of TJs can be regulated (Peppiatt et al., 2006; ^{14,27,47}; Zlokovic, 2008). Therefore, disrupted signaling between endothelial cells, pericytes and/or astrocytes may affect the integrity of the BBB.^{9,13,28}

In addition to regulating exchange of molecules between the peripheral blood circulation and the brain by its anatomical properties, the BBB is a metabolic barrier. A variety of degrading and metabolizing enzymes can be found at the membrane of brain capillary endothelial cells^{6,32} along with a large number of transporter proteins that strictly regulate the influx and efflux of substances.

Taken together, these unique features of the BBB control the homeostasis of a large variety of molecules in the brain. However, it is the same features that impose a major obstacle to successful delivery of drugs into the brain. For example, various phase l and phase ll enzymes of the drug metabolism system have been found in endothelial cells. The major drug efflux transporters include P-glycoprotein (P-gp),²⁴ ATP binding cassette (ABC), multidrug resistance-associated proteins (MRPs) and Breast Cancer resistance proteins (BCRP). Although in some conditions such as trauma, multiple sclerosis and Alzheimer Disease, the anatomical and functional state of the BBB may be altered, the delivery of active compounds into the CNS needs effective mechanisms to facilitate BBB crossing.

Although other barriers such as the blood-cerebrospinal fluid (CSF) barrier (BCB) and CSF-brain barrier (CBB) exist, the surface area of the BBB is far greater than the surface area of the BCB. Thus, the BBB is considered the main site for crossing of endogenous substances into the CNS. In addition, even despite

the entrance of a drug into the CSF, it does not necessarily results in its penetration into the brain parenchyma. The penetration of substances from CSF to brain parenchyma is facilitated through diffusion. However, the large distances create a diffusion barrier that can be referred to as the CSF-brain barrier (CBB). In addition to the aforementioned external barriers, after crossing the BBB, the presence of further internal barriers creates another obstacle for effective drug delivery, such as fast clearing mechanisms by glial cells.

Mechanism of BBB crossing by endogenous substances

Despite the restricted transport of molecules across the BBB, the brain has high demand for energy and nutrients. Therefore, multiple mechanisms exist that mediate the uptake of specific endogenous substances. Some of these provide a useful basis also for the development of strategies for drug delivery. In general, under physiological conditions, substances may cross the BBB by passive diffusion, carrier mediated transport, receptor mediated transport, and adsorptive transcytosis (Fig. 1).

The possibility for substances to passively cross the BBB by diffusion is very limited (see above) due to the BBB physiology. The exception are lipid soluble small molecules with an molecular weight of less than 400 Da. Uptake of such substances is possible by lipid-mediated free diffusion across the BBB. In contrast to diffusion through water, diffusion through lipid membranes is highly dependent on the correlating features of molecular volume, molecular weight, and surface area of a substance.⁸⁴

High lipid solubility in turn is correlated to low hydrogen bonding. It has been shown that the ability of a substance to permeate membranes is decreased by 10-fold with each pair of hydrogen bonds.¹¹² This rule has been confirmed in multiple studies i.e. investigating BBB transport of steroid hormones and oligopeptides.⁸⁴

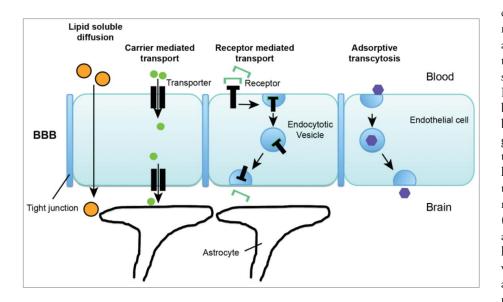


Figure 1. Transport pathways across blood brain barrier. Under physiological conditions, substances may cross the BBB by passive diffusion, carrier mediated transport, receptor mediated transport, and adsorptive transcytosis.

Therefore, the majority of substances is taken up into the brain by carrier mediated transport and receptor mediated transport. Here, the structure of the molecule possesses high affinity for specific carriers or receptor found at the BBB. For example, water-soluble metabolic substrates such as glucose, are bound by specific transporters, here the glucose transporter type 1 (GLUT1) that, however, has also affinity for other hexoses, including mannose and galactose.⁷⁹ Another example is the large neutral amino-acid transporter type 1 (LAT1), which is a carrier for phenylalanine, but also transports over 10 other large neutral amino acids and, although with lower affinity, small neutral amino acids.⁸² To date, many specific transporters have been identified. Their exact cellular location at the brain microvasculature and expression level, as well as their selectivity largely

determine the kinetics and turnover of the transported substances.

For example, the supply of Glucose for the brain is realized only by GLUT1. GLUT1 is enriched at the brain microvasculature only at the BBB on both luminal and abluminal membranes. This expression patterns enables not only uptake of Glucose from the blood into epithelial cells but indeed transport across the cells of the BBB. Due to the high energy - demand of the brain, the abundance of GLUT1 at the microvasculature is high, relative to other transporters, which enables rates of glycolysis in the brain that are over 100-fold greater than rates of amino-acid incorporation into brain proteins.⁸³ However, due to the demand of carriers, the process of carrier mediated transport of a substance across the BBB is saturable.

Carrier mediated transport is not only responsible for uptake of substances into the brain, but a process that regulates homeostasis in bi-directional manner. To that end, active efflux transporters can be found at the BBB that mediate the asymmetric efflux of metabolites from the brain back to the blood circulation. It is also these transporters that impose an obstacle to drug delivery into the brain. The classical active efflux transporter system within the BBB is P-glycoprotein (P-gp). This protein is encoded by the multidrug resistance gene 1 (MDR1) and its functional complex is not only modified by internal factors but also environmental clues such as the presence of toxins.³⁰

Receptor mediated transport processes additionally occur at the BBB as mechanism regulating the crossing of endogenous substances. These peptide receptors may mediate processes such as transcytosis of ligands from blood to brain or from brain to blood, or only uptake into the brain capillary endothelium without further export into the brain parenchyma. Well investigated examples include the transport of insulin or transferrin. Insulin is transported across the BBB by binding to an endogenous BBB insulin receptor.⁸¹ Similarly, for transferrin (Tf) a specific receptor, the Tf receptor (TfR) can be found at the BBB.⁸⁰ Similar to carrier mediated transport, the cellular location and expression levels of the receptors determine the kinetics and turnover of the transported substances. For example, the TfR mediates influx of holo-transferrin from blood to brain but also reverse transcytosis of apotransferrin from brain to blood due to expression on the luminal and abluminal membrane of the capillary endothelium.108,130

Finally, a mechanism of BBB crossing called adsorptive endocytosis has been described. This process requires an interaction between a ligand, such as a macromolecule or protein in the bloodstream and the cell surface. This interaction may be triggered by an electrostatic interaction between the positively charged ligand and negatively charged plasma membrane. Ultimately, this may result in adsorptive transcytosis of the ligand, which is mediated by clathrin-dependent endocytosis in most cases. This mode of BBB crossing seems to occur only unidirectional, from blood to brain. Adsorptive transcytosis has been described for some compounds and Nanoparticles (NPs). However, whether adsorptive transcytosis contributes significantly to the transport of endogenous substances across the BBB is still under investigation.¹¹⁹

Several of the mechanisms involved in BBB crossing of endogenous substances can be used for the development of strategies for drug delivery. For example, delivery of drugs that have structures that mimic the endogenous substrate of transporters at the BBB may be facilitated. The vast majority of carrier mediated transport systems has been identified and transporters can be expressed in in vitro systems to screen for drugs that have an acceptable affinity for a given BBB transporter. A drug that shows such an affinity for a carrier mediated transport system is L-DOPA. L-DOPA is used in the treatment of Parkinson Disease and is a dopamine precursor that is transported across the BBB via the LAT1 carrier.⁵⁵ Alternatively, drugs might be conjugated to substances that normally cross the BBB by carrier mediated processes. Further, the presence of endogenous receptors with specific ligands triggering BBB crossing mechanisms, such as the insulin receptor or the TfR, enables the engineering of peptides that attached to compounds or drugs mimic these ligands.

However, after successful crossing of the BBB, most drugs are taken up by cells. A major pathway mediating this uptake is clathrin-dependent endocytosis. This mode of uptake leads to the eventual delivery of substances into the endo-lysosomal compartments. Due to the low pH and the presence of degrading enzymes in lysosomal compartments, delivered biomolecule may be degraded creating a major obstacle in the delivery of active compounds, in particular of therapeutic proteins.

Thus, taken together, there is an urgent need to develop new strategies for the effective delivery of substances across the BBB. Therapeutic compounds need to be protected from degrading, metabolizing and inhibiting processes within the blood stream, need to be taken up into the CNS via the BBB with high efficiency, and need to be targeted to specific sites of action preventing lysosomal degradation. Here, Nanomedicines provide major advantages compared to common drug delivery systems

Nanomedicines

In this review, we would like to summarize the most interesting applications of the last 20 y of nanoparticles and liposomes in in vivo Brain experiments. Considering the variability of in vivo models, we skip to review the "proof-of-concept," but mainly focusing on "*In vivo* disease models." The "In vivo disease models" describes the application of nanoparticles and liposomes in brain pathology, pointing the critical attention on the animal models of pathology and on the possible mechanism involvement in the treatments. This section is divided into two main underchapter: "Neurodegenerative Diseases" and "Other Brain Pathologies." In "Neurodegenerative pathologies" section, we include Alzheimer, Parkinson and Multiple Sclerosis diseases. Finally, in "Other Brain Pathologies" section we include some of the most relevant papers on convulsive models, stroke, brain infectious diseases and prion diseases.

Firstly, we have to stress the difficulty to identify a "standard" *in vivo* model for each disease, thus the possible meta-analysis of the data, which could help the neuroscientist in the basic research, is virtually impossible. In particular, to our best

knowledge, in almost all neuro-pathologies conditions (such as Parkinson disease, HIV-dementia and some infectious brain diseases), the BBB permeability is seriously compromised, while in other brain diseases (stroke and brain tumors, as examples), the BBB integrity appears to be seriously damaged. As example, we must consider that the use of brain tumors (namely, gliomas) *in vivo* application must be thought as "glioma" delivery and not as brain targeting or BBB crossing exploitation, since over the progression of the pathology, it has been demonstrated that BBB is losing its integrity.¹⁰

Secondly, this field of science (namely, since "nanoneuroscience" or "neuro-nanomedicine") is relative new and young, the most of papers are based on "Proof-of-Concept," while the application on brain diseases models appears in constant increase, but still lower than the basic research. This evidence could be explained by the fact that a unique carrier for brain delivery does not exist, since it possible to take advantage of different ligands, receptors and mechanisms for BBB crossing and brain targeting. Then, the use of different starting polymer (poly-lactideco-glycolide, poly-buthyl/heaxil-cyano-acrylate, albumin, chitosan, and many others) for nanoparticle preparation or lipid composition (cationic/anionic/neutral, pegylated lipids and many others) for liposome preparation, results in different brain targeting mechanisms, different biodistribution profiles, different brain delivery efficacies and overall toxicities.

Notwithstanding all of these differences in animal models and carriers, with this review, we aimed to produce a useful tool for all the neuroscientist to access a plenary of *in vivo* evidences.

Nanoparticles and liposomes

Generally talking, polymeric nanoparticles (NPs) are solid colloid matrix-like particles sizing from 1 to 1000 nm, made of polymers of different nature, and encapsulating molecules during the preparation process, chosen depending on both the polymers and the drug to be delivered. There are several natural or synthetic polymers often mixed during the preparation of NPs, but considering the stringent request of FDA guidelines in terms of biodegradability and biocompatibility for in vivo administration, the list of polymers, that could be used to prepare NPs systems, results very short with few polymers available for drug delivery system preparation and approved for systemic administration. Among them, natural (e.g. Albumin) and poly-ester (poly-lactide and derivatives) polymers are the most accepted. In particular, it is a common opinion that the toxicology of a nanodevice should be related both to morphological and structural parameters of the systems (size, surface charge, shape) and the polymers used.

Liposome (LPs) are surely the most studied and old *smart* systems, applied in different fields of medicine research, representing the first innovative approach for the treatment of challenging pathologies, like cancer, HIV, strokes and many other diseases which require selective therapies.^{42,68} As described for NPs, LPs need a surface modification in order to promote specific delivery and targeting of the embedded drugs. Generally speaking, good in vitro results on LPs experimentations do not reflect in vivo confirmations, leading to a very low applicability of the liposome-approach in the treatment protocols. This event, connected

with a very quick elimination and degradation when LPs are injected in the bloodstream, along with the type and properties of phospholipids which are constituents of the liposomes, was faced with different strategies such as using stabilizers or modification of preparation procedures. Particularly, the conjugation with molecules, able to protect the LPs from the degradation (GM1, poloamine, polaxamer and PEG) or able to induce an increased affinity to the diseased cells, represented one of the most applied strategies. The pegylation technology offers a potential resolution of the problem of liposome's bio-stability, connected to the liposomal intravenous administration.^{50,91} Finally, in order to increase the minimal affinity to the diseased cells and to avoid the toxic effect on non diseased tissues, an active targeting due to functionalization of the surface of the liposome is hardly needed.¹²⁸

In vivo disease models

If in the previous examples the integrity of the BBB was maintained and the brain was considered as a "non-pathologic" brain, in the following examples, several researches have been reviewed concerning neuro-pathologies in which the BBB integrity and permeability is seriously compromised.^{12,51,103,135} These pathologies could vary from neurodegenerative diseases (Parkinson, Alzheimer and Huntigton's) to epilepsy, infectious brain diseases, strokes and many others.

Neurodegenerative disease

Alzheimer disease

Alzheimer disease (AD) is a chronic and progressive neurodegenerative disorder that begins with cognitive and memory impairments, accompanied with behavioral disturbances such as aggression, depression, hallucination, delusion, anger and agitation and eventually progresses to dementia, physical impairment and death.²⁶ AD is the most common form of dementia, and the greatest risk factor for AD is age. It is estimated that 10% of people over the age of 65 are affected by AD ⁴ and by 2050, the number of people with AD in the US will increase threefold.⁴⁵ The definite diagnosis of AD is made upon histological verification, established by biopsy or at autopsy, of two main hallmarks: extracellular amyloid plaques and intracellular neurofibrillary tangles, which enclose hyperphosphorylated tau protein.^{26,102} Furthermore, the neuropathology of AD is characterized by a progressive loss of synapses and neurons in a region- and celltype-specific manner.95 In Alzheimer disease, microglia and astrocytes are activated by β-amyloid protein and related oligopeptides, leading to a cascade of events producing toxic molecules, neuronal damage, synaptic dysfunction and alteration of the permeability of the BBB.¹⁰

To study this pathology, a model of acute amnesia is induced in rats or mice by subcutaneous injection of scopolamine.⁸⁶ These animals are submitted to the passive avoidance reflex (PAR) test¹¹⁸ to determine the memory changes; the PAR is based on the measurement of the retention latency times, necessaries for the animals to avoid a painful stimulus; these latencies are directly proportional to the decrease of amnesia, thus representing a useful tool to describe the effectiveness of anti-amnesia drug injected. Kurakhamaeva and colleagues⁵⁹ used Nerve Growth Factor (NGF) loaded in PBCA NPs covered with PS-80 to reduce amnestic effect. With this study, they demonstrated that brain-targeted NPs loaded with NGF allowed an improvement of amnesia with a significant increase of the latent period of 2-fold, if compared to animals treated with NGF-free solution. In another paper, Abdel-Wahab³ demonstrated the efficacy of 2 different systems: PBCA Np covered with polysorbate-80 and PBCA Np covered with PEG5000, both loaded with tacrine (reversible inhibitor of acetylcholinesterase) able to improve cognitive function. These NPs formulations increased the latency period in treated animals of 1,2-fold and 1,4-fold, respectively, compared to the injection of tacrine-free solution (Table 1).

In our opinion, the greater effect obtained with drug loaded PBCA NPs covered with PEG5000 as compared to the drug-free solution and to the drug loaded PBCA-NPs covered with Polisorbate-80 could be due to the alteration of the BBB permeability rather than a specific targeting: in fact, the presence of PEG onto the NPs surface confers stealth properties to the NPs, allowing them to remain over a longer time in the systemic circulation, thus improving the chances to reach the pathological site.

Moreover, the role of surfactants (polysorbate 80 as well as polaxamers or PEG) as possible pathways for BBB permeability increase was deeply debated by several authors, without any effective and clear result.^{7,87} The only evidence was achieved by 2-D electrophoresis (2-D PAGE) showing that PBCA NPs coated with polaxamer 188 (Pluronic F68[®]) and Ps80 showed a considerable adsorption of apolipoprotein A-I (ApoA-I), leading to a possible interaction with BBB receptors. This finding could induce to propose a general pathway for BBB crossing of PBCA coated Ps80 (or Pluorinc), based on a great absorption of APO A-I allowing a receptor-mediated transcytosis. This hypothesis cannot be generalized, since it should be taken into consideration the close interaction between polymer and surfactants as well as the whole NPs interaction with the BBB.

Parkinson disease

Parkinson disease (PD) is a multicentric neurodegenerative disease. Estimates state that 1% of people over age 60 are affected by PD, the leading cause of the movement disorder called Parkinsonism.⁴ Clinical features of PD include tremor at rest, bradykinesia, rigidity and flexed posture.⁴⁸

Pathologically, the key deficit in PD has been considered to be the loss of dopaminergic neurons in the substantia nigra, which causes consequent reduction of dopamine level.⁹⁸ Cell loss and Lewy body formation (abnormal intraneuronal aggregates of protein, predominantly a-synuclein) occur in the locus coeruleus, dorsal motor nucleus, and substantia innominata.¹⁵ Consequently, nor-adrenergic, serotonergic and cholinergic neurons are also lost and this widespread neurodegeneration leads to the emergence of a variety of features known as "non-motor" symptoms in PD that include cognitive decline, apathy, depression,

anxiety disorders, hallucinations, gait and balance disturbances, sleep disorders, sexual dysfunction, bowel problems, drenching sweats and pain.⁴⁶ At present, for this pathology no significant evidences of BBB permeability alteration are described.

As there is currently no permanent rescue and cure for Parkinson disease, and there are no known agents to slow the progression of PD, the current treatments are used to decrease the symptoms of PD.^{64,122} Although symptomatic therapy of PD is effective (Levo-Dopa), novel therapeutics are required as well as advanced delivery methods, as the active substances will need to enter the CNS to exploit their effects (Table 1).

Animal PD model is obtained through injection of neurotoxins: the most used toxin is 6-hydroxydopamine (6-OHDA stereotaxical injected),¹⁶ but also 1-methyl-4-phenyl-1,2,3,6tetrahydropyridine (MPTP i.p. injected) is used¹⁸: both agents destroy neurons by generating active oxygen species such as superoxide radicals. Kurakhamaeva and colleagues⁵⁹ used mice treated with MPTP to test the efficacy of NGF entrapped in PBCA NPs covered with polysorbate-80. This mice were submitted to many tests to evaluate the improvement in Parkinson symptoms: i) open field test, that allows to check the orientationresearch reaction; ii) locomotor activity in the actometer, to value the quality and the quantity of movement; iii) rigidity, through the registration of the alteration of gain dynamic; iv) tremor, through the registration of intensity and duration of tremor. With all these tests, the researchers observed that the administration of targeted NPs allowed a significant improvement in PD symptoms already after 90 minute and maintained for 21 day.

The research group of Pardridge performed several studies using rodents 6-OHDA treated with apomorphine or amphetamine to induce rotation: the reduction in the number of rotations, promoted by administration of anti-parkinson drugs, demonstrated a improvement in PD induced syndrome. In fact, Xia and co-worker¹²⁶ prepared a LPs formulation loaded with GDNF plasmid (Glial-derived neurotrophic factor) and targeted to the brain with OX-26 (mAb against the mouse TfR). The single administration of that system to 6-OHDA rat treated with apomorphine, showed a general improvement of PD symptoms, as they observed a decrease in rotational behavior of 58% and a great increase of Tyrosine Hydroxylase (TH) activity as compared with saline control. In another paper, Zhang and colleagues improved the results obtained by Xia, using a multiple injection of the LPs,¹³² achieving a decrease in the rotational behavior until 90% and an increase in the TH activity until 77%, compared with saline control. Besides, Zhang performed another test, namely the Vibrissae-Elicited Forelimb Placing Test, aiming to evaluate the forelimb response to ipsilateral facial whisker stimulation⁸ This test showed an improvement of response up to 4fold, if compared to saline control, thus allowing the authors to corroborate the results obtained before. In another article,¹³¹ Zhang showed the results obtained with the same kind of targeted LPs loaded with 877 cDNA (a cDNA of TH gene). It was seen that the LPs, administered at a different dose of loaded drugs, allowed a decrease in rotational behavior of 70% until 3 day post injection, but after 6 d the TH enzyme activity decreased and after 9 d it was comparable to the control. Xia and

PATHOLOGY	TARGETING (BBB/tumor)	APPROACH	DRUG	MODEL	TEST	RESULTS	REF
Alzheimer	LDL Receptor	PBCA-NPs-Ps80	NGF	Mice treated with scopolamine. ⁸⁶	PAR test. ¹¹⁸	Increase of retention latency (2,12-fold vs drug free)	Kurakhmaeva et al., 2009
	LDL Receptor	PBCA-NPs-Ps80	Tacrine	Rats injected with scopolamine	PAR test and HPLC biodistribution	Increase of retention latency (1,20-fold vs drug free;	Abdel-Wahab et al 2009
						increase brain delivery (1,43 fold vs drug free)	
	/	PBCA-NPs-PEG500	Tacrine	Rats injected with	PAR test and HPLC	Increase of retention latency	
				scopolamine	biodistribution	(1,37 fold vs drug free; increase brain delivery (1,75 fold vs drug free)	
Parkinson	LDL Receptor	PBCA-NPs-Ps80	NGF	C57Bl/6 mice treated	Open field test (<i>Schmidt</i>	Significant reduction of	Kurakhmaeva
				with MPTP. ¹⁸	et al., 2001);	Parkinson symptoms;	et al, 2009
					actophotometer test;	reduction of rigidity;	
					rigidity test (<i>Amende</i> <i>et al.</i> . 2005): tremor test.	improvement of locomotor activity	
	/	LPs (CHOL:LEC:	Dopamine	Rats treated	Rotarod test and	Increase of muscular	88
		Span 80:Tween		with Haloperidol	actophotometer test	coordination activity (3,5-	
		20 1:9:2:1)				fold); increase of locomotor	
						activity (3,4-fold)	
	Transferrin Recentor	LPs (POPC:DDAB: DSPE-PEG	877 cDna (TH gene)	Rats treated with 6-OHDA (RMFB)	Count of controlateral rotation	After 3 day post i.v. decrease of rotational hehavior (> 70%)	Zhang et al. 2003
	- - -	47:1:2)-OX26		(16) injected		decrease of TH enzyme	
				with apomorphine		activity during time (after	
				to induce rotation		9 day is like control);TH	
						enzyme activity is \propto to	
						injected dose.	C
	/	LPs (PC:Chol:	Dopamine	Chlorpromazine-induced	Reduction in degree of	83% of animal obtain complete	cc
		(1:5:0 AS			catatOTIIa	150 minuto affor injortion	
						(0% with dopamine	
	,					solution)	
	Transferrin	LPs (POPC:DDAB:	GDNF plasmid	Rats treated with	Count of controlateral and	Decrease of rotational behavior	Zhang
	Receptor	DSPE-PEG 47:1:2) -OX26	DNA	6-OHDA (RMFB) than iniacted with	ipsilateral rotation; Vihricsaa-Elicitad Eoralimh	(> 87-90%); increase of 1H enzyme activity (< 77 %).	et al., 2008
				and apomorphine	Placing Test $(^{8})$	improvement of response to	
				or amphetamine to)	Vibrissae test (4-fold vs	
				induce rotation		saline control)	
	Transferrin Receptor	LPs (POPC:DDAB: DSPE-PEG 47:1:2)-OX26	GDNF plasmid DNA	Rats treated with 6-OHDA (RMFB) then	Count of controlateral rotation induced by apoM	Decrease of rotational behavior after 4 week post i.v. (>58	971
				injected with apomorphine		%); increase of TH enzyme activity (>19 fold vs saline	
				-		control)	

Table 1. Neurodegenerative diseases models and Nanotech applications.

ola ost i. nt	d 10 -fold	fold sst i. ion	, eerol reas,	odels ¹⁰⁰ , Schmidt sis ¹⁰⁰ , Schmidt t the <i>et al., 2003b</i> 42 h t of ng of	56 ted
function (86%) and 26 fold increased TH enzyme activity Day 6 and 10 post i. v.: No great improvement	Day 3 post i.v.: No great improvement Day 6 and 10 post i.v.: increase motor function (69%); 2 and 4-fold increased TH enzyme	activity Day 3 post i.v.: increase motor function (73%) and 13-fold increased TH enzyme activity Day 6 and 10 post i. v.: increase motor function (71%) and 6 –5-fold increased TH enzyme	activity Ability of NPs to deliver cholesterol in the brain, confirmation of cholesterol localization in specific areas,	rescue in KO animal models Reduction in Tcells apoptosis and Tcells infiltration in the CNS (spinal cord) after 42 h of treatment; reduction of inflamation and restoring of	BBB integrity Inhibition of Cytokine expression in mice treated with L-TMN.
rotation induced by apoM			Pharmacology Behavior Pathological evidences Confocal Microscopy	Immunohistochemistry	PCR-Real time and expression of HPRT mRNA (proinflammatory cytokines)
6-OHDA (RMFB) then injected with apomorphine.			KO HD mice	Rats with EAE induced injection of freshly activated, MBP-specific T cells (Gold et al., 1995)	Mice with acute EAE (<i>Pollak et al 2003</i>) <i>and</i> chronic EAE (<i>Offen et al 2000</i>)
(TH gene) (10 ug/rat)	PrgTH3 (TH plasmid) (10 ug/rat)	877 cDna (TH gene) (10 ug/rat) and PrgTH3 (TH plasmid) (10 ug/rat)	Cholesterol	Prednisolone	MMT
47:1:2)-OX26			PLGA	PEG-LPs (DPPC: DSPE-PEG ₂₀₀₀ : CHOL 1.85:0.15:1)	PEG-LPs (EPC:CHOL: DSPE- PEG ₂₀₀₀ 54:41:5)
Receptor			BBB-crossing glycopeptides	~	~
			Huntigton's Disease	Multiple Sclerosis	

distearyl phosphatidylethanolamine polyethylene glycol; OX26, murine monoclonal antibody against the mouse transferring receptor; TH: tyrosine hydoxylase; 6-OHDA, 6-hydroxydopamine; RMFB, right medial forebrain bundle; PC, phosphatidylcholine; SA, stearylamine; GDNF, glial-derivedneurotrophic factor; apoM, apomorphine. DPPC, dipalmitoyl phosphatidylcholine; EAE, experimental autoimmune encephalomyelitis; CNS, central nervous system; EPC, egg phosphatidylcholine; TMN, tempamine. PCR, polymerase chain reaction.

colleagues, in a following article,¹²⁷ demonstrated that the incorporation of a TH plasmid in the same targeted systems can allow a prolongation of the neuroprotective effect but, unfortunately, without showing the effect 3 d after the injection.

Haloperidol and chlorpromazine were also used to induce extra pyramidal effects in rat or mice. In particular, Pichandy and colleagues⁸⁸ treated rats with haloperidol to test the anti-PD effect of Dopamine loaded in LPs formulated with the use of span 80 and tween 80. Both formulations allowed an increase in muscular coordination activity, tested with the rotarod test, along with in locomotor activity, tested with actophotometer. On the contrary, Jain and coworkers,⁵³ took advantage of rats, injected with chlorpromazine (inducing catatonia) to test non targeted LPs loaded with dopamine, showing a complete reduction of catatonia state in the 83% of animals treated 150 min after injection.

Huntington's disease

Huntington's disease (HD) is a genetic neurological disorder caused by a CAG expansion in the gene encoding the huntingtin (HTT) protein. HD is featured by motor, cognitive and psychiatric disturbances, neuronal dysfunction, atrophy of the striatum and other brain regions, and progressive loss of striatal mediumsized spiny neurons (MSNs) and of cortical pyramidal neurons (Vonsattel et al 1998). Several molecular and cellular dysfunctions have been identified (Zuccato et al 2010) and one affected pathway implicates brain cholesterol. Brain cholesterol biosynthesis and cholesterol level are reduced in Huntington's disease (HD) mice suggesting that locally synthetized, newly formed cholesterol is less available to neurons. This might be detrimental for neuronal function, especially given that locally synthesized cholesterol is implicated in synapse integrity and remodeling. Biodegradable and biocompatible polymeric nanoparticles (NPs) modified with glycopeptides (g7) and loaded with cholesterol (g7-NPs-Chol), which per se is not blood-brain barrier (BBB) permeable, were successfully apply in order to obtain high rate brain delivery after intraperitoneal injection in HD mice. g7-NPs, in contrast to unmodified NPs, efficiently crossed the BBB and localized in glial and neuronal cells in different brain regions. We also found that repeated systemic delivery of g7-NPs-Chol rescued synaptic and cognitive dysfunction and partially improved global activity in HD mice.¹¹⁶

Multiple sclerosis

Multiple Sclerosis (MS) is a disorder of the CNS with inflammatory and neurodegenerative components, and characterized by a variable clinical pattern, which ultimately leads to a progressive neurological dysfunction.⁶³ Its pathological hallmarks are demyelination and cellular infiltration of T cells and macrophages (Mf). Despite long-term immunotherapy, relapses occur, which are commonly treated by repeated i.v. injections of high dose (pulse) glucocorticosteroids (GS) as a potent antiinflammatory drug (Table 1).

The most applied in vivo experimental model of MS is the experimental autoimmune encephalomyelitis (EAE) with a high tissue inflammation and the partial disruption of the BBB.^{73,115}

Considering MS-diseased BBB, it has been shown that disease severitiy could be correlated with alteration of BBB integrity, as confirmed by loss and delocalization of brain endothelilal junction proteins, like occluding., VE-cadherin and others.^{67,123} Schmidt and co-workers, in two different works, ¹⁰⁰; 2003b) demonstrated that long-circulating prednisolone LPs (PL) were able to localize the high tissue therapeutic levels of glucocorticalsteroid in the inflamed cerebral area of autoimmune EAE rats model³⁹ as compared with an equivalent dose given as free drug with a following reduction of inflammation and a significantly improvement in the disease course of (AT)-EAE. Moreover, the drug targeting by LPs appears highly effective in restoring the BBB integrity, ameliorating the disease activity of active and adoptive transfer (AT)-EAE without detectable side effects. The authors hypothesized a selective targeting, but in our opinion the altered permeability of BBB surely increases the penetration and the localization of LPs in inflamed tissue. Similarly, Kizelsztein at al.⁵⁶ demonstrated the ability of long-circulating LPs to transport a potent antioxidant (Tempamine, TMN) to the brain tissue in a concentration able to significantly attenuate clinical symptoms of EAE in the mouse model.⁸⁹ The authors hypothesized that the size and the long circulation properties of these LPs could promote their extravasation into a well permeable inflammation sites.

Other brain pathologies

Epilepsy

Epilepsy is defined as a condition characterized by recurrent (two or more) epileptic seizures, unrelated to any immediate identified cause⁴⁴ Epilepsy is one of the oldest known conditions to mankind and still the most common neurological condition affecting individuals of all ages. At any given time, it is estimated that 50 million individuals worldwide have a diagnosis of epilepsy¹²⁴; 2001b). Recently an excellent descriptive review concerning the epidemiology of epilepsy was published.¹¹ Several evidences demonstrated that the epileptic seizures alter bloodbrain barrier (BBB) properties and permeability.^{31,54,117} Particularly, a recently in vivo study demonstrated the dynamic changes of BBB permeability during epileptogenesis. The long-lasting increased permeability of the BBB indicated that it may contribute to increased excitability in the epileptogenic foci, leading to the progression of epilepsy and seizure development.¹¹⁷ Considering the application of drug delivery systems as a treatment strategy in epilepsy (Table 2), Mori and coworkers, in two different papers, compared the anticonvulsivant effect of valproic acid and y-butyrolactone-y-carbonyl-L-histidyl-L propynamide citrate (DN-1417) entrapped in LPs with that obtained after free drug i. v. administration in amygdaloid-kindled rats⁷⁰; 1992b). The animal models were obtained implanting a bipolar electrodes in the right area amygdalaris anterior that are stimulated at a defined time intervals and frequency as described by Löscher and coworkers.⁶² In all cases, while the administration of free drug suppressed amygdaloid kindled seizure for few time, the drug encapsulated in positive charged LPs showed a prolonged anticonvulsivant effect. The authors hypothesized that LPs protected

PATHOLOGY	TARGETING (BBB/tumor)	APPROCHES	DRUG	MODEL	TEST	Results	REF
Epilepsy		LPs (PC:CHOL: Sterylamine 7:2:1)	PHT or HRP	Rats with status epilepticus	Anticonvulsivant effect Analysis of HRP reaction products in the brain	Suppression of AM discharges by two doses of L-PHT; accumulation of HRP (by L-HRP admin.) in the AM epileptogenic focus (2 of 5 animals tested)	71
	~	LPs (PC:CHOL: Sterylamine 7:2:1)	DN-1417	Amygdaloid kindled rats	Anticonvulsivant effect	Suppression of kindled seizure and prolonged anticonvulsivant effect after L-DN 1417 admin. than free DN 1417	20
	~	LPs (cationic)	VPA	Amygdaloid kindled rats	Anticonvulsivant effect	Prolonged anticonvulsivant effect after cationic L-VPA admin (2 days) than anionic L-VPA admin and free VPA (1 h)	3
	LDL Receptor	PBCA-NPs-Ps80	MRZ 2/576	Convulsion model in mice	Anticonvulsivant effect (MES test)	Longer duration in MES taffer coated Np-MRZ 2/576 admin. (up to 210 min) than uncoated Np admin. (60 min)	8
Lysosomal storage disorders	Transferrin receptor (BBB)	LPs (POPC: DDAB : DSPE-PEG2000: DSPE-PEG2000 -maleimide + 8D3 mAb)	pCMV-GUSB plasmid DNA	MPS type VII GUSB null mice	GUSB enzyme activity measurement Protein concentration determination	GUSB enzyme activity in the brain of adult mice = 13.3 \pm 0.9 nmol/ hr/mg protein; GUSB enzyme activity in the brain of GUSB null mice after L/plasmid DNA treatment = 1.7 \pm 0.1 nmol/hr/ mg protein; GUSB enzyme activity in the brain of GUSB null mice after saline admin. < 0.2 nmol/hr/mg mortein.	132
Cerebral Ischemia (Traumatic Injury)	~	LPs (DPPC:CHOL: Sterilamine 14:7:4)	CuZn-SOD	Rats cold- injury brain model (Chan et al 1983)	Determination of CuZn-SOD; determination of superoxide radicals; Evans Blue Permeability (BBB permeability)	Protection of drug; increase of CuZn-SOD brain level 8from 30 min to 2 h); reduction in brain level of superoxide radicals and water content and ameliorated BBB permeability	Chan et al 1987
	~	LPs (PC:CHOL: Sulfatides)	Calpain inhibitor (ALL NA1)	Gerbil model of forebrain ischemia (Yokota et al 1995)	Immunohistochemistry and immunoblot analysis	Dose dependent prevention after L- ALL Na1of CA1 neuronal damage	Yokota et al., 1999
		LPs (DPPC:CHOL: Sterilamine 14:7:4)	CuZn-SOD	Rats model of focal cerebral ischemia (<i>Chen</i> <i>et al., 1986</i>)	CuZn-SOD activity and measure of infarct size	Increase of CuZn-SOD activities in the brain; reduction of infarct size (33%, 25% and 18% for the anterior, middle and posterior slices reservivelv)	49
	~	NPs	MRZ 2/566		Quantification of infarct lesion	Increased neurological score vs placebo Reduction at 53% of	111

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ΡΑΤΗΟΓΟΘΥ	TARGETING (BBB/tumor)	APPROCHES	DRUG	MODEL	TEST	Results	REF
				Rats models of focal cerebral ischemia	and neurological severity score	total infarct size (60% of cortical and 42% of striatal infarction)	
	~	PLGA-NPs	SOD	Rats models of focal cerebral ischemia -perfusion injury model	Quantification of infarct lesion and neurological severity score	5% of survival after SOD-Np admin. at 28 d (Infarct volume after SOD-Np = 20%, saline control=56%, SOD- SOL=75%. Ischemic lesion area after SOD-	8
						Np=25%, saline control =50%, SOD-SOL =80%. Neurological severity score after SOD-Np=3.5, saline control=10, SOD-SOL=11)	5
		PLA-NPs	QC	Rats model of cerebral ischemia	Diene level, index of lipid peroxidation and GSSG/GSH ratio	Significant protection to endogenous antioxidant enzymes against ischemia induced oxidative damage in neuronal cells	67
Arsenic induced oxidative damage	~	PLGA-NPs	Q	Rats with neuronal cell damage after NaASO ₂ injection	Intracellular GSH, GPX, GR, GST and G6PDH activity in the brain	QC-Np prevent the antioxidant deplection in brain cells (levels of GPx from Np 4.98 ± 0.31 vs 2.17±0.09 µmol NADPH oxidation/Main/Mac provisio-	38
						GePDH muol NADPH reduced/ min/mg protein 6.07 \pm 0.39 vs animal model 3.61 \pm 0.29; GR µmol NADPH oxidation/min/mg protein 17.92 \pm 2.33 vs 9.92 \pm 0.87;GST mmol product/min/ mm 97 86 \pm 7 \pm 7 vs vs 60 36 \pm 0.88)	
Traumatic Brain Injury		PANAM dendrimers	N-acetyL-cysteine, valproic acid	Traumatic brain injury, rats	In vivo administration, biodristribution and pharmacological test	PANAM localize in the injured neurons and microglia in the brain -loading with N-acetyl cysteine and valproic acid	69
		self-assembling peptide nanofiber scaffold	/	Traumatic brain injury, rats	In vivo administration	Redúction of acute brain injury and brain cavity formation	8
	1	pegylated PLGA NP (100-200-800 nm)	/	Traumatic brain injury animal model	In vivo administration, brain localization	Smaller NPs are facilitated in BBB crossing	25
		PLGA NPs	Cerebrolysin	Traumatic brain injury, rats	In vivo administration, brain edema formation, rescue tests	Ability in delivering cerebrolysin to site of action; - reduction of brain patholooy features	94
Infectious diseases	1	LPs (PC:CHOL:DSPG -AmBisome)	AMB	Candida Albicans infected rabbits	CFU in the brain tissue	Reduction of infection in the brain	41

Table 2. Other brain pathologies models and Nanotech applications. (Continued)

citrate; ¹ nal elect NAb, moi	, liposomes; PC, phosphatidylcholine; CHOL, cholesterol; PHT, phenytoin; HRP, horseradish peroxidase; AM, amygdala; DN-1417, y -butyrolactone- y-carbonyl-L-histidyl-Lpropinamide citrate; VPA, val- ic acid; PBCA, poly(butylcyanoacrylate); NPs, nanoparticles; MRZ 2/576, 8-chloro-4-hydroxy-1-oxo-1,2-dihydropyridazino[4,5-b]quinoline-5-oxide choline salt; MES, prevention of maximal electroshock; PC, 1-palmitoyl-2-oleoyl-sn-glycerol-3-phosphocholine; DDAB, dimethyldioctadecylammonium bromide; DSPE-PEG ₂₀₀₀ distearoylphosphatidylethanolamine polyethylene glycol; 8D3 mAb, monoclonal	ygdala; DN-1417, γ -butyrolact yridazino[4,5-b]quinoline-5-oxic PEG ₂₀₀₀ distearoylphosphatidyle	iorseradish peroxidase; AM, am -4-hydroxy-1-oxo-1,2-dihydrop cylammonium bromide; DSPE-I	T, phenytoin; HRP, h MRZ 2/576, 8-chlorc B, dimethyldioctade	noline; CHOL, cholesterol; PH (crylate); NPs, nanoparticles; / erol-3-phosphocholine; DDAI	omes; PC, phosphatidylch 1; PBCA, poly(butylcyanoa 2almitoyl-2-oleoyl-sn-glyce
	prain ussue (vp rearment < 2CFU/g; control ≥15/g).	plodistribution studies (FITC-loaded Np)	neorormans meningitis rabbit model			
121	Suppression of yeast growth in brain tissue (ND treatment <	CFU in the brain tissue and biodistribution studies	Criptococcal neoformans	CG ₃ R ₆ TAT	CG ₃ R ₆ TAT NPs	
	decreasing the degree of the infection		model			
	CFU/g tissue; Suppression of bacterial growth in the brain,		Aureus induced meningitis rabbit			
61	Np 2 lg CFU/g tissue; control 3.7 lg	CFU in the brain tissue	Staphilococcus	CG ₃ R ₆ TAT	CG ₃ R ₆ TAT NPs	
			Bearing Mice			
92	Survival: twice than controls	Fungal growth and	Cryptococcal	AMB	PLA-b-PEG-NPs-Ps 80	(¿) FDFr
	than other combinations	of animals			with other VCZ, CAS, MICA)	
	demonstrated higher efficacy	therapeutic activity			Association	
	with VCZ from days 4 to 10	tissue and	CNS aspergillosis		DSPG-AmBisome)	
22	control 1 ma//ra Amhiroma from 1 +م ع ط	cell in the brain	Murino modale of	AMA		
	treatments. CFU reduction vs					
	clears the fungus from the brains (3/8 rabbits). None with other	and therapeutic activity	rabbits with Coccidioides immitis		DSPG-AmBisome)	
53	3x15mg/kg Ambisome for 3 weeks	CFU in the brain tissue	Immuno-suppressed	AMB	LPs (PC:CHOL:	/
	Ambisome=50–60% survival; 1 mg/kg fungizone = 12–30%.					
	CFU/brain. Ten mg/kg		neoformans)			
	log ₁₀ CFU/brain; 1 mg/kg fungizone = 6.92±0.50 log ₁₀	in the brain tissue	cryptococcidiosis (Cryptococcus		-Ambisome)	
113	10 mg/kg AmBisome = 5.69 ± 0.38	Therapeutic activity	Murine model of	AMB	LPs (PC:CHOL:DSPG	/
	respectively)		neoformans)			
	(44 and 78% clearance,		(Cryptococcus			
	yeast from the brains of the mice		meningitis			
		urerapedue acuvity	ri y prococcai			

toyl phosphatidylserine; MR2 2/566, (8-chloro-4-hydroxy-l-oxo- 1,2-dihydropyridazino(4,5-b]quinolin-5-oxide choline salt; PANAM, polyamidoamine; PLGA, poly(D,L-lactide co-glycolide); SOD, superoxide dismutase; OC, Quercetin; GSSG, oxidized glutathione; GSH, reduced glutathione; PLA, Polylactide; NaASO₂, sodium arsenite; GSH, glutathione; GPX, glutathiane peroxidase; GR, glutathione reductase; GST, glutathione-5-transferase; G6PDH, glucose-6-phosphate dehydrogenase; NADPH, nicotinamide adenine dinucleotide phosphate-oxidase; DSPG, distearoylphosphatidylglycerol; CFU, colony forming units; VCZ, voriconazole; CAS, caspofungin; MICA, micofungin; Ps80, Polysorbate 80; AMB, amphotericin B; CG₃R₆TAT, cholesterol conjugated 3 glycine, six arginine and TAT peptide; FITC, fluorescein isothiocyanate. LPs, lip proic a POPC, antibo

the drug from the enzymatic degradation and that LPs surface charge played an important role in allowing the rapidly cross of the BBB, by taking advantage of adsorbtive-mediated endocytosis. Recently, the same group of research evaluated the effect of phenytoin (PHT), entrapped in LPs (PHT-LPs), on the status epilepticus, induced in rats by injecting a combination of dibutyryl-cAMP (db-cAMP) and ethylenediaminetetraacetic acid (EDTA) into the amygdala (AM).

The researchers observed the suppression of AM discharges by two injections of PHT-L. The authors hypothesized that the AM epileptogenic focus created by db-cAMP/EDTA has a high affinity for LPs, and this factor participates in the local suppression of AM discharges by PHT-L. Even if, the mechanism underlying the selective augmentation of LPs in the epileptogenic AM is not known, the amount of LPs in the circulation may be important for the understanding of this finding, since two injections of PHT-L caused preferential suppression of AM discharges as well as two injections of horseradish peroxidase (HRP; to which the blood-brain barrier is impermeable) loaded LPs increased their augmentation in the AM. Since, the blood flow is reliably increased in the epileptogenic focus, it is our opinion that the possible cause of LPs local augmentation could lie in the bloodflow increase, along with the permeability of BBB increasing over the disease progression, consequently promoting the brain localization of LPs (Mori et al., 1995).

Friese and coworkers evaluated the prevention of maximal electroshock induced convulsions in mice model after i.v. administration of a novel non-competitive NMDA receptor antagonist MRZ 2/576 (potent but rather short-acting anticonvulsant, rapidly discharged from the central nervous system by transport processes that are sensitive to probenecid) bound to PBCA NPs coated with PS-80; this formulation prolonged the length of the anticonvulsive effect up to 210 min and after probenecid pretreatment up to 270 min compared to 150 min with probenecid and MRZ 2/576 alone.³⁶ Reasonably, the NPs operated as drug delivery systems, able to protect and to prolong the release of drugs to the CNS. Moreover, the coating of NPs with PS-80 seems to be necessary to target and to achieve an uptake of the particles into the brain. It is also important to consider that the BBB properties can be altered by the treatment performed to achieve animal model, thus promoting and enhancing NPs BBB crossing.

Lysosomal storage disorders

The lysosomal storage diseases (LSDs) are a heterogeneous group of disorders that affect 1/7,000 live-born infants, the majority of which develop CNS disease. Each LSD results from a deficiency of a single lysosomal enzyme, pivotal for degrading macromolecules that must be turned over in lysosomes.¹¹⁰ More than 40 LSDs have been described. The neurological compromission is generally refractory to treatment, which will require long-term correction of lesions dispersed throughout the central nervous system to be effective. A promising approach is enzyme replacement therapy (ERT) or gene therapy by gene transfer methods enable the treatment of these diseases by transferring a wild-type copy of the gene of interest to some target organ, where

the production and export of the protein proceed for extended periods of time.¹⁰⁹ In this contest, Zhang and co-workers¹³³ treated a mice model for type VII mucopolysaccharidosis (MPS-VII), deficient for the β -glucuronidase (GUSB) lysosomal enzyme, with GUSB expression plasmid (p-CMV GUSB) encapsulated in LPs and superficially engineered with the rat 8D3 MAb to the mouse transferrin receptor (TfR) to achieve BBB crossing. The results demonstrated that sub-normal, yet therapeutic levels of GUSB enzyme activity, are achieved in brain following the i.v. administration of the TfR mAb-targeted LPs encapsulating p-CMV GUSB plasmide. This kind of strategy, even if interesting, will required repeat administrations, considering the chronic progression of disease and the inability of the plasmid delivered by LPs to integrate into the host genome.²¹

Stroke

After heart disease and cancer within the developed world, stroke is the third largest killer, second most common cause of neurologic disability after AD.⁷⁸ There are over five million deaths/year from stroke and over nine million stroke survivors. Between the ages of 45 and 85, 20-25% of men and women, respectively, can expect to have at least one incident of stroke. Atherosclerosis, heart disease, hypertension, diabetes, and lifestyle habits are risk factors correlated with disease. Unlike AD and PD, many of the risk factors for developing this disease can be modified. The etiology of stroke is brain vascular occlusions (thrombotic stroke) or rupture (hemorrhagic stroke). The neuropathological hallmarks of stroke are necrotic infarcts of variable size with inflammatory gliosis.

The effect of hypoxia-ischemia on the BBB has been extensively investigated⁵⁷; Bolton et al., 1998;^{34,65}: this disease sets in motion a series of events, which leads to disruption of TJ and increased BBB permeability, probably mediated by cytokines, VEGF, and NO. Moreover, elevated levels of proinflammatory cytokines, IL-1 β , and TNF- α have been demonstrated in animal brains after focal and global ischemia³³ and in cerebrospinal fluid of stroke patients.¹¹⁴

The potential of LPs and NPs in protecting and modulating the delivery of un-stable drug during the ischemic insult was deeply investigated in several researches with interesting positive results (Table 2): the success of the use of nanocarriers is not to be correlated to the need of an active targeting, but better to the facilitate diffusion of these systems through the compromised and broken BBB. LPs and NPs were used to deliver drugs able to prevent ischemic neuronal damage. Several researchers used rats as animal models, in which the focal cerebral ischemia was produced by the method described by Chen and colleagues²⁰ based on an extensive, but reproducible infarct. In an old study, Chan and coworkers¹⁹ described the ameliorated condition of animals manifesting the reduction in brain level of superoxide radicals when treated with superoxide dismutase (SOD) loaded into LPs. This success could be firstly searched both in the protection exploited by LPs along with their ability to operate a prolonged delivery of drug. More recently, Imaizumi and co-workers, using the same animal model, demonstrated that LPs facilitate the delivery of SOD, thus elevating SOD activities into the brain, not only in the infarct, but also in the non-infarcted subcortical areal. The authors try to justify these results hypothesizing the penetration of SOD loaded LPs across the leaky BBB in the ischemic zone and subsequently LPs uptake by adjacent neurons and microglia extending the area of action; otherwise, SOD loaded LPs could exert their action on extracellular superoxide on the luminal side of capillaries, without penetrating the BBB.⁴⁹ More recently, Reddy and coworkers demonstrated the ability of PLA NPs to encapsulate and to stabilize SOD from degradation and to provide a localized modulated brain delivery that assures the protective effect of the enzyme by neutralizing the deleterious effect of reactive oxygen species which are the mediators of reperfusion injury.⁹⁰ By using focal cerebral ischemia model rats, Sopala and co-workers¹¹¹ evaluated the neuroprotective activity of the novel glycine-ß site NMDA (N-methyl-Daspartate) receptor antagonist MRZ 2/576, formulated in NPs that provide a system able to protect and to modulate the delivery of the drug to the CNS.

In another study, citicoline-loaded LPs were administered in ischemic reperfused mice; the LPs formulations produced an increase in rat survival rate of about 24% and a reduction of 60% in diene levels (index of lipid peroxidation) compared to the free drug.³⁵ Yokota and colleagues (Yokota et al., 1999) administered a calpain inhibitor to gerbils to rescue ischemic neuronal damage, but with a little beneficial effect due to BBB crossing inability of the inhibitor. On the contrary, the calpain inhibitor-LPs complex was able to produce a potently and selectively inhibition of calpain activation. LPs protect the drugs and maintain a higher concentration in the brain than free drug.

Querciein is an interesting herbal compound that exhibits antioxidant properties against many neurological diseases. Initially, Das and coworkers^{29,97} proposed the use of LPs encapsulating quercetin, administered i.v. to rats (pre-treated with arsenic) as a good formulation to attenuate the oxidative damage induced by ischemia reperfusion injury in the rat brain. Recently, they proposed the use of PLGA NPs as quercitin carriers in combating arsenic induced oxidative damage in brain of rats. A singular dose of sodium arsenite was sub-cutaneously injected in rats to obtain a model of arsenic toxicity. Nanoencapsulated quercitin, orally administered before the arsenite injection, prevented the arsenic cerebral oxidative damage.³⁸ The authors hypothesized the ability of these NPs to cross the BBB via particle uptake mechanism based on an endocytotic pathway by the brain capillary endothelial cells. It is not clear if the treatment of rats with arsenic maintained the BBB integrity, thus it is difficult to give an absolute conclusion on the real efficacy and BBB crossing pathway. The increased efficacy of these formulations should be found in their ability to stabilize the drug and to prolong the brain delivery.

Traumatic brain injury

Traumatic brain injury (TBI), happens when an external force traumatically injures the brain. TBI can be classified on severity, mechanism (closed or penetrating head injury) and area (specific or widespread area). TBI is now considered as one the major major causes of death and disability worldwide, especially in children and young adults.. It could vary on severity depending on the casues, but the common features are mainly consiting on alterations in cerebral blood flow and the pressure within the skull, contributing substantially to the damage from the initial injury. In this kind of pathology, blood-brain barrier features are strongly altered, as permeability and transport across the BBB are dramatically changed.

Several attempts in prevention and "quick" interventions were performed in the past years, also dealing with nanomedicines, able to transport and deliver efficiently in the traumatic areas those drugs needed to restore "altered" parameters.^{105,107}

In particular, a recent study⁶⁹ demonstrates that the administration of polyamidoamine (PAMAM) dendrimers could be taken up in the brain of injured animals and selectively localize in the injured neurons and microglia in the brain. Besides, these dendrimers were also able to deliver two clinically approved drugs, N-acetyl cysteine (attenuating neuroinflammation) and valproic acid (attenuating excitotoxicity), building on positive outcomes in a rabbit model of perinatal brain injury.

In another elegant research,⁹⁶ self-assembling peptide nanofiber scaffold were used to reduce acute brain injury and brain cavity formation, and to improve sensorimotor functional recovery. SAPNS serves as biocompatible material in the hemorrhagic brain cavity. Local delivery of this nanomaterial may facilitate the repair of ICH related brain injury and functional recovery.

Besides, in another paper,²⁵ the impact on the size of nanomedicines (pegylated PLGA NPs sizing 100nm, 200 nm and 800nm) on distribution in TBI animal models was studied. The results highlighted that smaller NPs are facilitated in BBB crossing while bigger NPs may result in a lower permeation. This finding would be extremely important in order to understand the rationale in planning nanomedicine for this kind of interventions and may help in designing NPs with a higher performance in targeting traumatic brain areas depending on the size and on the BBB permeability under TBI events.

In the treatment of TBI, the use of mixture of peptides activating growth factors was deeply studied in the last 5 y^{106} Cerebrolysin is a peptide mixture able to ameliorate symptomatology and to delay progression of neurological disorders such as Alzheimer disease and dementia. Cerebrolysin loaded PLGA NPs were therefore designed, formulated, tested on stability over time in plasma and finally in animal models, where they were able to deliver cerebrolysin to reduce brain pathology following traumatic brain injury.⁹⁴

Infectious disease

Brain inflammatory diseases such as meningitis and encephalitis are among the top ten infection causes of death; they are caused by bacteria (such as Bacillus anthrax, Staphylococcus aureus), fungi (ex Candida albicans, Cryptococcus neoformans) or viruses (Jafari et al. 1994;^{77,93} Despite the general efficacy of antibiotic treatment, high mortality and morbidity is frequently recovered due to the difficulty of drugs to the BBB and access the brain (Table 3).

The LPs approach in brain infectious therapy could be mainly refereed to the use of Ambisome[®], a liposomal formulation of amphotericine B in which the drug is strongly associated with the bilayer structure of unilamellar LPs.

Several works, using different animal models, provided evidences of AmBisome effectiveness against brain infections. Groll and colleagues⁴¹ evaluated groups of un-infected and Candida albicans-infected rabbits treated with AmBisome and the other commercially formulation of amphotericine B (Amphotec), showing AmBisome treatment able to completely clear Candida albicans from the brain of infected animals. Several years ago, Albert and colleagues⁵ described a mouse model of meningitis caused by Cryptococcus neoformans; also in this case, the AmBisome therapy (20 and 30 mg/kg) produced a disappearance of Cryptococcus in the brain. Several years later, Takemoto and coworkers¹¹³ treated the same animal model with a lower dose of Ambisome (10 mg/kg) in comparison with other antifungal drugs as fungizone. AmBisome exhibited greater efficacy and, more importantly, it is distributed into the brain as the penetration enhanced by the progression of cryptococcal meningitis correlating with the in vivo activity. Clemons and colleagues administered AmBisome to treat different brain infections: in a first study, AmBisome was compared with other drugs (as fluconazole or amphotericin B alone) to treat coccidioidal meningitis in rabbits. The animal model was represented by immune-suppressed rabbits, challenged intra-cisternally with Coccidioides immitis²³ Recently, the authors studied the efficacy of AmBisome, micafungin (MICA), caspofungin (CAS), amphotericin B, voriconazole (VCZ), given alone or in combination, after administration in immune-suppressed mice, infected intracerebrally with Aspergillus fumigates. In the first study, the brain infection was significantly reduced by Ambisome treatment if compared with fluconazole and amphotericine B treatments. On the contrary, only the combination therapy at suboptimal doses of AmBisome and VCZ improved the outcome in CNS aspergillosis.²² Thus, AmBisome seems to have an important role in treating brain infections, in which the inflammation, due to pathogens, alters the permeability of BBB; in fact AmBisome could allow to deliver high and active concentrations of drug in the tissue, reducing or eradicating the fungal burden.

Only in the last two years, polymeric NPs were investigated as an alternative treatment in brain infection diseases. Liu and coworkers tested a new kind of NPs in rabbit models to treat the brain infections disease. Amphiphilic cholesterol-conjugated G3R6TAT peptide (CG3R6TAT), which contains TAT sequence, was designed and assembled into core/shell NPs. These NPs possessed a broad spectrum of strong antimicrobial activities, much stronger than the hydrophilic peptide, incapable of forming NPs. The Nps were firstly examined for in vivo activity against Staphylococcus Aureus in comparison with vancomycin, a therapeutic agent widely used for the prophylaxis, suppression, and treatment of S. Aureus meningitis. The NPs were found to be as efficient as vancomycin in treating the meningitis in rabbits (Liu at al., 2009). In another experiment, CG3R6TAT NPs showed a good antimicrobial activity against the brain infections caused by Cryptococcus neoformans in rabbit model, in which the meningitis was induced inoculating intracisternally the yeast suspension. The authors demonstrated that the NPs crossed the BBB and suppressed the yeast growth in the brain tissues with similar efficiency as amphotericin B did.¹²¹ They hypothesized that cationic peptide-decorated NPs may be taken up by the BBB through adsorptive endocytosis, diffusing into the brain tissue and suppressing bacterial growth in the brain.

Finally, starting from the hypothesis that^{37,58} in NPs coated with polisorbate 80 seem to be uptaken by the brain capillary endothelial cells due to specific interaction with LDL receptors, Ren and co-workers prepared polysorbate 80 coated amphotericin B/PLA-b-PEG NPs to target cryptococcal meningitis-bearing mice. The results confirmed the therapeutic efficacy of these formulations in fungal infection in the brain, decreasing the speed of colony growth and the count of colony, thus increasing the survival time of animals.⁹²

Conclusion

The interest in developing targeted systems, able to reach the CNS, represented one of major section of neuroscience, over the last 20 y The pathologies affecting the "Brain" are surely the most difficult to be treated and the less favorable in term of rescue of the integrity of the neuronal structures. These pathologies, meaning gliomas, PD and AD, neurodegenerative diseases as MS, or infectious and stroke diseases, all have similar features, which are common and could represent a possible target for innovative therapies. Moreover, the presence of the BBB is usually a great limitation for drugs, which are normally unable to enter in the CNS.

Thus, the application of nanotechnology to CNS diseases (namely Nano-Neuroscience) is surely representing one of the most innovative strategy to improve the current treatments and, possibly, to find newer and, most of all, more efficacious therapies. Both NPs and LPs have been deeply investigated with several in vitro and in vivo models. In this review, we tried to summarize the most interesting and valuable in vivo evidences, since we do consider extremely risky to translate in vitro results (on BBB co-coltures) to in vivo outlooks of efficacy.

Moreover, in some of the cited pathologies, the integrity of BBB is seriously compromised, such as in glioma or stroke, as well as in other diseases, like in AD and PD, the permeability across the inflamed BBB is actually implemented. In these cases, a brain targeting has not to be considered as BBB crossing goal, but better as "pathology-targeted" aim.

Several experiments on polymeric NPs and LPs have been reviewed considering a general aim of understanding both the rate of brain delivery and the biodistribution; in particular, the last aim is pivotal for the scale-up of neuro-nanomedicine, since scientists must strongly assess both brain delivery efficiency and safety of nanocarriers. Moreover, beside a number of proof-ofconcept experiments, relatively few pre-clinical data have been reached by using in vivo models (mice and rats, mainly), assessing the efficacy against brain disease of active molecules (gene, drugs, enzyme, etc..) by means of nanocarrier-mediated delivery. These results pointed out a batch of data which would be useful for improving, developing and finalizing this new, non-invasive and efficacious strategy for the treatment of the brain diseases, such as AD and PD, gliomas, infectious disease, MS and LSD. A final remark should be given regarding the possible development of nanocarriers for CNS and hopefully to drive a complete research project for neuro-nanomedicine.

Firstly, the choice of biodegradable and biocompatible starting materials is pivotal in speeding up the acceptability and FDA approval of new nanocarriers; secondly, the targeting strategy (meaning surface engineering with CNS targeting ligands) should be chosen in function of the pathology, since the BBB integrity and permeability is varying from disease to disease. It could be possible that the need for BBB crossing would not be required, especially in the case of stroke and gliomas, while it is fundamental in other BBB-healthy pathologies (such as AD or MS). Third, the choice of the carriers should be considered as function of the kind of drugs to be delivered: in particular, polymeric NPs could be useful in both hydrophilic and hydrophobic active substance encapsulation, while LPs would better contribute to an effective gene therapy. Finally, the overall fate of carriers and, most of all, their stability in the bloodstream should be accurately investigated a-priori and the proper corrections and tricks should be taken in great consideration, to definitively allow nanocarriers to exploit their job at their best.

Disclosure of Potential Conflicts of Interest

No potential conflicts of interest were disclosed.

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