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Hyperpolarized [^{13}C]ketobutyrate, a molecular analog of pyruvate with modified specificity for LDH isoforms

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Abstract

Purpose—The purpose of this study was to investigate ^{13}C hyperpolarization of α -ketobutyrate (αKB), an endogenous molecular analog of pyruvate, and its *in vivo* enzymatic conversion via lactate dehydrogenase (LDH), using localized MR spectroscopy.

Methods—Hyperpolarized (HP) ^{13}C MR experiments were conducted using [^{13}C] αKB with rats *in vivo* and with isolated LDH enzyme *in vitro*, along with comparative experiments using [^{13}C]pyruvate. Based on differences in the kinetics of its reaction with individual LDH isoforms, HP [^{13}C] αKB was investigated as a novel MR probe with added specificity for activity of LDHB expressed H (“heart”-type) subunits of LDH (e.g. constituents of LDH-1 isoform).

Results—Comparable T_1 and polarization values to pyruvate were attained ($T_1 = 52\text{s}$ at 3T, polarization = 10%, at C_1). MR experiments showed rapid enzymatic conversion with substantially increased specificity. Formation of product HP [^{13}C] α -hydroxybutyrate (αHB) from αKB *in vivo* was increased 2.7-fold in cardiac slabs relative to liver and kidney slabs. *In vitro* studies resulted in 5.0-fold higher product production from αKB with bovine heart LDH-1, as compared with pyruvate.

Conclusions—HP [^{13}C] αKB may be a useful MR probe of cardiac metabolism and other applications where the role of H subunits of LDH is significant (e.g. renal cortex and brain).

Keywords

^{13}C ; DNP; LDHB; LDHA; isoenzymes; hydroxybutyrate

Introduction

Dissolution dynamic nuclear polarization (DNP) for hyperpolarized (HP) ^{13}C MRI has enabled localized, non-invasive monitoring of real-time enzymatic conversions through key biochemical pathways *in vivo* (1-3). The observable conversion of HP substrate [$1\text{-}^{13}\text{C}$]pyruvate to HP [$1\text{-}^{13}\text{C}$]lactate catalyzed by lactate dehydrogenase (LDH) has generated particular interest as a glycolytic marker, with promising applications in cancer

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(4), cardiovascular disease (5,6), and diabetes (7), including a recent “first-in-man” HP ^{13}C MRI clinical Phase 1 safety trial in prostate cancer patients (8).

In contrast to many other important enzymes, for instance phosphoenolpyruvate carboxykinase (PEPCK) (9), LDH is characterized by relatively broad substrate specificity, exhibiting substantial activity with several α -keto acids (10). α -Ketobutyrate (αKB) is one such, endogenous structural analog of pyruvate that is also readily reduced via LDH as shown in Figure 1, to α -hydroxybutyrate (αHB). In this work we investigated HP [^{13}C] αKB as a potentially valuable [^{13}C]pyruvate analog with added specificity for measuring the activity of LDHB expressed H (“heart”-type) subunits of LDH, in cardiac and other tissues where H subunits are important (e.g. brain and renal cortex).

αKB actually differs biochemically from pyruvate in multiple potentially interesting ways, including 1) the aforementioned differential activity with individual LDH isoforms (10) as well as other enzymes that act on pyruvate (11), 2) possible differences in vascular permeability and/or cellular transport (12), and 3) different endogenous pool sizes ($\sim 0.1\text{mM}$ for pyruvate as compared with low μM range for αKB (13)). In this work we focused on the reported variable activity of individual LDH isoforms with αKB as compared to pyruvate (10). While the reported activity of LDHB expressed H subunits is similar between αKB and pyruvate, the activity of LDHA expressed M (“muscle”) subunits with αKB is greatly attenuated, indicating that HP αKB could provide useful added specificity for activity with H (“heart”) subunits. Moreover, the activity of pyruvate with H subunits in particular is inhibited by high concentrations of pyruvate, an effect which appears to be diminished in the case of αKB (14). The known differential activity of pyruvate and αKB was previously widely exploited clinically to measure serum isoenzyme fractions in the diagnosis of myocardial infarction (15), prior to supplantation by the current standard method of measuring serum cardiac troponin levels (16). Specific localized measures of cardiac LDH activity could be useful in the diagnosis and management of cardiovascular diseases.

Interestingly, a recent metabolomics discovery study singled out αHB among 485 possible biochemicals as the single best predictor of early stage insulin resistance (13), and αHB appears to be the most promising existing plasma biomarker in early diabetes research (17,18). This endogenous αHB is normally generated via LDH from αKB according to the reaction in Figure 1. Under normal conditions αKB is a dilute product of amino acid catabolism (threonine and methionine) and glutathione anabolism (cysteine formation pathway), and is ultimately recycled through the Krebs cycle via succinyl CoA. The modulation of αHB levels in early diabetes thus may be related to changes in LDH and/or glutathione metabolism. The potential ability to obtain tissue-specific measurements of αHB metabolism using HP ^{13}C MRI may thus represent a useful new molecular imaging tool for diabetes research.

The purpose of this initial study was to investigate the feasibility of hyperpolarizing αKB via dissolution DNP and detecting its rapid enzymatic conversion to αHB catalyzed by LDH *in vivo*. Localized MR experiments demonstrating this conversion and comparing HP [^{13}C] αKB and [^{13}C]pyruvate metabolic imaging were conducted both *in vivo* in rats and *in*

vitro with isolated LDH in solution. These experiments also explored the specificity of HP [^{13}C] αKB for measuring the activity of LDHB expressed H subunits of LDH.

Methods

Modeling Reaction Rates of LDH Isoforms

LDH catalyzes the interconversion of pyruvate and lactate, permitting organisms to sustain a “temporary oxygen debt” in the form of accumulated lactate to be later reoxidized as oxygen becomes available (19). In higher vertebrates, functional LDH *in vivo* exists as a tetramer consisting of assembled combinations of any four individual M (“muscle”) and/or H (“heart”) subunits expressed by the genes LDHA and LDHB, respectively, giving five isoforms LDH1-5. Skeletal muscle and notably, rodent and human hepatocytes as well as most cancers, contain almost exclusively the homotetramer of M subunits (known as LDH-5 isoform), while the heart contains almost exclusively the H homotetramer (LDH-1 isoform). Most other tissues contain varying combinations of M and H subunits. The testicular isoform LDH-X is coded by a third gene whose expression is restricted to the testis. The individual isoforms differ greatly in their kinetic properties and substrate specificity.

Under Michaelis-Menten (MM) enzyme kinetics, the ratio of K_{cat} (the catalytic constant) to K_m (the Michaelis constant) is known as the specificity constant, indexing the specificity of an enzyme for alternative substrates. The specificity constant of rabbit muscle LDH-5 with αKB is 50x lower than pyruvate (for reduction), while the specificity constant of bovine heart LDH-1 with αKB is only 2.5x lower than pyruvate (10). αKB is thus 25x more specific for LDH-1 than LDH-5, relative to pyruvate. Calculated MM reaction rates based on published kinetic constants (10) and relevant substrate concentrations illustrate the potential specificity of HP αKB for LDH-1. Given the appropriate assumptions, the MM kinetic model predicts the initial reaction rate

where $[E]$ and $[S]$ denote the concentrations of enzyme and substrate, respectively. LDH-1 has lower K_m values ($K_m < 0.1\text{mM}$) and absolute K_{cat} values for reduction than LDH-5 ($K_m = 0.25\text{mM}$), features which are thought to contribute to its functional role in the oxidation of lactate as an energy source (19). Plots of predicted relative reaction rate versus substrate concentration are shown in Figure 2. Taking for example 10mM substrate concentration, the MM model predicts a relative reaction rate of 3.4x times lower for αKB with equal amounts of LDH-5 (isolated from rabbit muscle) as compared with pyruvate, but αKB retains 60% of activity with LDH-1 (bovine heart) relative to pyruvate. As the concentration of αKB is reduced below its K_m value for LDH-5 (7.4mM), such as by further dilution of the HP infusion and metabolic conversion, the specificity for LDH-1 may be further increased.

Hyperpolarization

The sodium salt of [^{13}C] αKB (Cambridge Isotopes Laboratories, Andover, MA) was dissolved to a concentration of 3.4M in 50/50 glycerol/water (vol/vol), and mixed with trityl radical OX063 (15mM) (Oxford Instruments, Abingdon, UK) as well as Gd-DOTA (1.0mM) (Guerbet, Roissy, France). For each experiment, ~60mg of this mixture was polarized using

a HyperSense dissolution DNP system (Oxford Instruments) and rapidly dissolved in 1X phosphate buffered saline (PBS) to yield 40mM solutions of HP [U-¹³C]αKB. For comparison, [1,2-¹³C]pyruvic acid was also polarized using similar methods to also yield 40mM solutions of HP [1,2-¹³C]pyruvate (with similar pH, close to neutral). Although only the C₁ resonances of both molecules were directly relevant to this study, doubly labeled pyruvate was used to produce a similar appearance of the NMR spectra as [U-¹³C]αKB, which is the form of ¹³C-labeled αKB that was readily available commercially. Hyperpolarized C₃ and C₄ resonances of αKB were not observable due to their very short T₁ relaxation times due to directly attached protons.

MR experiments

Liquid state polarizations and aqueous T₁ relaxation times at 3T were measured for both the HP [U-¹³C]αKB and HP [1,2-¹³C]pyruvate samples. To demonstrate the feasibility of detecting localized conversion of HP αKB to αHB *in vivo*, and perform a paired comparison with HP pyruvate, three rats were scanned by sequential slab-localized MRS acquisitions of HP [U-¹³C]αKB and HP [1,2-¹³C]pyruvate (2.5mL 40mM injections over 12s via tail vein). In all cases, the αKB experiment preceded the corresponding pyruvate experiment by approximately one hour. All MR experiments were conducted in a 3T clinical scanner (GE Healthcare, Waukesha, WI) equipped with multinuclear ¹³C capability, using a dual tuned ¹H / ¹³C volume transceiver radiofrequency coil designed for imaging rats. Rats were anesthetized using inhalational isoflurane delivered via nose cone (1.5%, 1L/min flow rate) and placed on a heated water pad inside the coil for the duration of the experiments. Typical physiologic parameters measured for rats handled in this manner in our lab are: body temperature= 36°C, respiration rate= 1 breath/s, heart rate= 300 beats/minute, blood glucose concentration= 100mg/dL. All animal studies were conducted in accordance with a protocol approved by the Institutional Review Board (IRB). A 5.5cm axial slab covering liver and kidneys was repeatedly excited (20°) every 3s over 30s (pulse bandwidth=2.8kHz, slice center frequency= ~178ppm), starting at the end of injection. MR signals were refocused using a pair of adiabatic spin echo pulses (TE=120ms), resulting in B₁-insensitive narrowing of the spectral linewidths (20). To investigate the conversion of HP αKB in the heart (which contains only LDH-1 isoform), three additional rats were again scanned by sequential slab-localized MRS experiments with both HP [U-¹³C]αKB and HP [1,2-¹³C]pyruvate, using identical study parameters as above, except in this case a 15mm axial slab through the heart was excited instead, every 5s from 25-40s from the start of injection, with increasing flip angle over time to fully utilize all of the HP magnetization. The experiments performed in this study are diagrammed in Figure 3.

To demonstrate the basic feasibility of MR spectroscopic imaging (MRSI) of HP αKB, one additional rat was imaged by 2D chemical shift imaging (CSI), again sequentially with HP [U-¹³C]αKB and then HP [1,2-¹³C]pyruvate approximately one hour later. For 2D CSI, the concentration of each injection was raised to 80mM. The acquisition was exactly identical for both compounds. The injection procedure was identical to the other experiments but in this case the scan was initiated 30s after the start of injection. The 2D CSI acquisition was encoded as a coronal projection image (matrix= 12x8) but excited with axial slice selection (12cm slab) in order to avoid signal wrap around from the tail and brain. The other

acquisition parameters were: spatial resolution= 1cm × 1cm, spectral resolution= 12.2Hz, spectral bandwidth= 25kHz, slice center frequency= ~178ppm, TR= 108ms, total scan time= 10s, centric view order, and increasing flip angle over phase encoding steps. Despite the potential benefit of narrower spectral linewidths, double spin echo refocusing was not employed in the 2D CSI acquisition for two reasons. First, extending the acquisition time well beyond 10s as required would introduce increased blurring due to T₁ decay, motion, and metabolic conversion. Second, the SNR could be significantly degraded at the longer TE, a potentially important effect given the higher degree of localization in this experiment as compared with the slab spectra.

In vitro studies were conducted to evaluate the potential specificity of αKB for activity of H subunits, by comparing the *in vitro* activity of both compounds with isolated LDH-5 and LDH-1 isoforms. For each compound, 30μmol aqueous HP substrate (0.5mL) was introduced into a previously mixed solution of ~100 “units” of either isolated LDH-5 or LDH-1 enzyme and a slight excess (~33μmol) of reduced β-nicotinamide adenine dinucleotide (NADH) coenzyme (Sigma Aldrich, St. Louis, MO), in 2.5mL 1X phosphate buffered saline (PBS) maintained at ~37°C. This solution was freshly prepared just prior to each HP experiment and then mixed rapidly with the HP substrate and a portion was quickly transferred to the RF coil for MR measurements. In this case, spectra with a 5° flip angle were acquired every 3s over 42s. This experiment was repeated using LDH derived from rabbit muscle (LDH-5) and bovine heart (LDH-1) (Sigma Aldrich). In each case, the concentration of HP substrate was ~10mM and the concentration of LDH was in the low nM range. Each experiment was repeated three times.

Results

For both HP [U-¹³C]αKB and HP [1,2-¹³C]pyruvate, doublets were observed for C₁ resonances due to J coupling with co-labeled C₂. Estimated liquid state polarizations of [U-¹³C]αKB were 10% for C₁ and 9% for C₂, back-calculated to time of dissolution. Aqueous T₁'s at 3T were 52s for C₁ and 38s for C₂. For [1,2-¹³C]pyruvate, the estimated liquid state polarizations were 17% for C₁ and 16% for C₂ (back-calculated), and the T₁'s were 50s for C₁ and 37s for C₂. Thus the liquid state polarizations and T₁ relaxation times of both molecules are comparable, with the neat pyruvic acid preparation attaining somewhat higher polarization.

Rapid *in vivo* conversion of HP αKB to HP αHB via LDH was detected in all *in vivo* spectra. In the liver and kidney slab spectra of the first three rats scanned with both αKB and pyruvate, the mean summed HP αKB-to-αHB ratio was 5.2 ± 0.6 (mean ± s.d.) times the HP pyruvate-to-lactate ratio observed after HP pyruvate infusion in the same animals (Figure 4A,B). Unlike HP pyruvate spectra which show a significant alanine peak, no transamination product (i.e. α-aminobutyrate) was observed after HP αKB infusions, and only a very small degree of decarboxylation by PDH was detected in these spectra (11), by the appearance of a small HP [¹³C]bicarbonate peak in some of the data. By contrast, the cardiac slab yielded much more αHB signal than the liver and kidney slab, relative to lactate produced in the corresponding pyruvate experiment (Figure 4C,D). In scans from the second group of three rats scanned with both αKB and pyruvate, the cardiac mean summed αKB-to-αHB ratio was

only 1.9 ± 0.1 times the HP pyruvate-to-lactate ratio, representing a 2.7-fold increase in product production over the liver and kidney slab, relative to pyruvate. Interestingly, some cardiac α KB spectra (e.g. Figure 4C) also revealed a large bicarbonate peak, despite the much slower predicted decarboxylation rate of α KB (11).

Spectroscopic images derived from the 2D CSI experiments (obtained by integrating the localized HP metabolite peaks) in one additional rat are shown in Figure 5. Injections of both HP compounds resulted in substantial HP product formation (i.e. α HB or lactate) in multiple anatomic regions. In the case of α KB, the largest product formation was in the region of the heart (Fig. 5B), while in the case of pyruvate the largest product formation was in the kidneys and liver. Since these images were acquired at relatively low true spatial resolution ($1\text{cm} \times 1\text{cm}$), the localization of HP signals to these tissues was not extremely precise, but it appears that the signals largely originate from these tissues as described.

The *in vitro* HP experiments evidenced high specificity of α KB for LDH-1, even higher than predicted by the MM model with published kinetic constants. Dynamic metabolic curves for the LDH-5 and LDH-1 reactions from one set of experiments are plotted in Figure 6. In the LDH-1 reactions, the integrated area of the HP α HB-to- α KB ratio was actually *higher* than the integrated HP lactate-to-pyruvate ratio by a factor of 5.0 ± 2.9 across the three sets of experiments. Meanwhile, the LDH-5 experiments yielded lower activity with α KB by a factor of 3.1 ± 1.6 , by the corresponding calculation for that experiment.

Discussion

We have demonstrated the hyperpolarization and rapid *in vivo* enzymatic conversion via LDH of [^{13}C] α KB, a molecular analog of [^{13}C]pyruvate which attains comparable polarization levels and has similar T_1 relaxation times, but exhibits varying specificity for LDH isoforms. Prior *in vitro* studies as well as our own *in vitro* experiments indicate relatively high specificity of this molecule for activity with LDHB expressed H subunits, in comparison with pyruvate. The results of our *in vivo* rat studies are consistent with such specificity, since HP α KB yielded much higher fractional conversion in the heart, a site where only LDHB has significant expression, as compared with the liver and kidney. Furthermore, the 2D CSI experiments with α KB resulted in greatest HP product α HB formation in the heart, in contrast with experiments with pyruvate which resulted in the most lactate being formed in the kidneys and liver. Results observed *in vivo* are of course complicated by many factors including NADH availability, fractional blood volume, and vascular permeability and cellular transport. However, the high numerical consistency of these results is persuasive. The potential influence of any other potential differences from pyruvate, such as differences in vascular permeability and cellular transport of α KB and its metabolites, requires further study.

While the *in vitro* results showed that the activity of α KB with LDH-5 was greatly reduced in comparison to pyruvate, as expected, they also showed greatly *increased* activity with LDH-1. While unproven, this could be due to less inhibition by the formation of an abortive ternary complex (e.g. LDH-NAD⁺-substrate) involving α KB, such as is known to occur at high pyruvate concentration (19). LDHB expressed H subunits are known to be much more

sensitive to such inhibition than M units. A relative absence of inhibition of chicken LDH-1 by α KB, as compared to pyruvate (despite both being effective substrates), has been noted previously (14). This apparent reduced potential for inhibition could prove valuable if H subunits of LDH are in fact inhibited by pyruvate administered during HP experiments. Substantial conversion of pyruvate to lactate was however observed in the cardiac slab *in vivo*. This could be due to differences between the *in vitro* and *in vivo* situations as alluded to above, or the lactate could be generated outside the heart.

Universally labeled α KB was used in this study due to practical reasons of availability as noted above, although co-labeling at the C₂ position does result in some moderate shortening of the T₁ relaxation time of the C₁ carbon in both α KB and pyruvate (21). For comparison, we polarized natural abundance α KB (where co-labeling is essentially negligible) and measured an aqueous T₁ of 65s for the C₁ carbon at 3T, in comparison with ~52s for [U-¹³C] α KB and [1,2-¹³C]pyruvate. Therefore, we anticipate somewhat improved performance with singly labeled α KB due to increased polarization as well as improved discrimination of individual spectral resonances due to elimination of carbon-carbon coupling. The sodium salt form of α KB, as opposed to the neat acid, was also selected based on availability. As in the case of pyruvate, the increased concentration of a neat acid form of α KB should greatly benefit its polarization, even though unlike pyruvate α KB is also a solid at room temperature.

Notably, one prior related HP MR study sought to exploit the low substrate specificity of LDH (specifically the testicular LDH-X isoform, which has especially broad specificity) in the design of a reporter protein system based on a HP [¹³C]pyruvate analog that was desired to react specifically with LDH-X but not LDH1-5 (22). The selected molecule (“pyruvic acid derivative Y”) is apparently identical to keto-isocaproate (KIC), which was previously proposed by another group as a novel HP ¹³C probe of branched chain amino acid metabolism (23). α KB was not among the candidate molecules for the reporter system, presumably because it reacts much too greatly with LDH1-5, as shown in this study.

Based on limited published data and our own initial experience with HP ¹³C MRI of α KB in rats, the acute toxicity of α KB appears to be low. Published mouse LD50 values of α KB (2960 mg/kg, subcutaneous route) (24) and pyruvate (3533 mg/kg, also subcutaneous) (25) are similar. Accumulation of α KB is thought to be toxic to certain bacteria (26). Further study is required to investigate any potential acute toxicity of α KB in the context of HP ¹³C MRI. Should α KB lack the potential inotropic effects of pyruvate (27), it may be an attractive alternative for monitoring localized LDH activity in cardiovascular patients.

Potential value of the described approach might be seen by analogy with positron emission tomography (PET). In that modality, [¹⁸F]fluorodeoxyglucose (FDG) is an ideal probe by virtue of its difference from the endogenous substance (glucose), which greatly increases its specificity. It remains to be seen whether molecular analogs of key biomolecules could be similarly useful for HP ¹³C MRI, even though much higher concentrations are of course required. In this case, both pyruvate and α KB are endogenous substances, although α KB is normally far less abundant. It also remains to be seen what the most useful applications of HP α KB could be, but they could extend beyond cardiovascular disease and diabetes as

described above. A recent study showed that LDHB is an essential gene in triple negative breast cancer, and high LDHB expression correlated with poor clinical outcome, indicating a localized non-invasive assay of LDHB expression could provide value in that context as well. In the near term, future technical developments will include improved localization of α KB signals, which would be facilitated by a C₁-labeled version and obtaining a neat acid form with potentially improved polarization.

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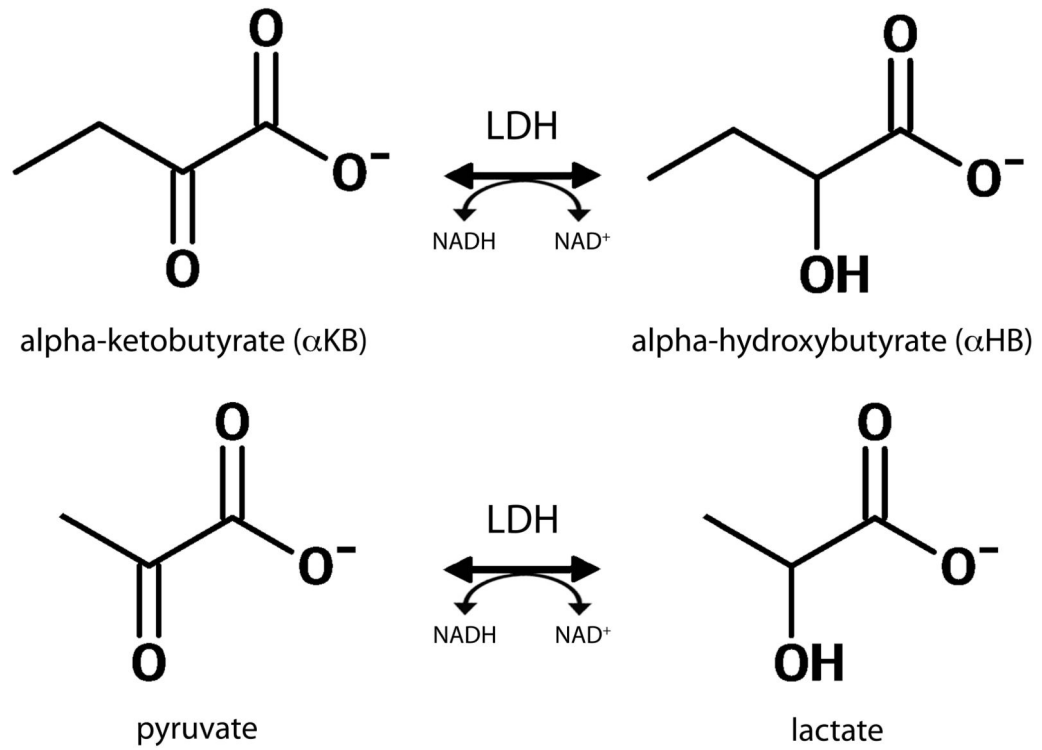


Figure 1. Redox interconversion of α KB and α HB also catalyzed by LDH (top row), as compared with the standard interconversion of pyruvate and lactate (bottom row).

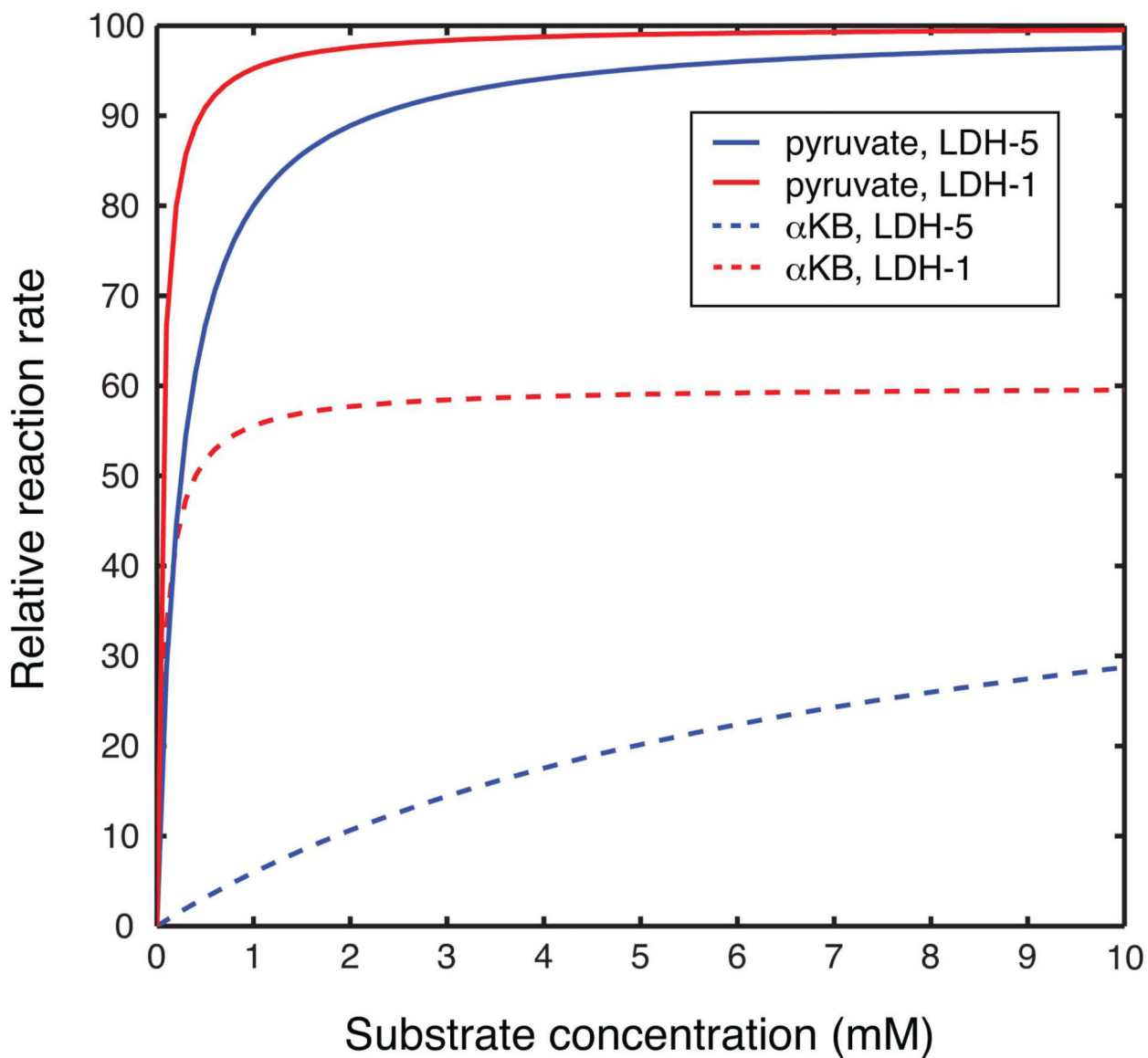


Figure 2. Relative reaction rates for the reduction of pyruvate (solid lines) and α KB (dotted lines) via LDH-5 (blue) and LDH-1 (red) as a function of substrate concentration, as predicted by Michaelis-Menten kinetics. Curves for each isoform were normalized to the maximum rate with pyruvate.

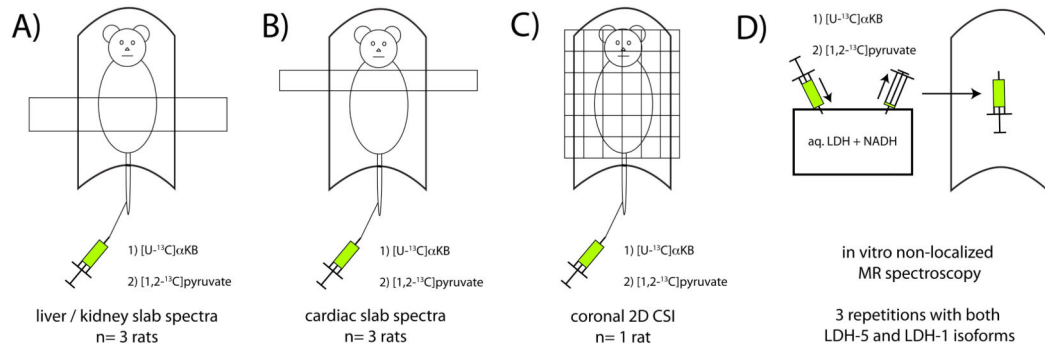


Figure 3. Schematic representation of *in vivo* (A-C) and *in vitro* (D) MR experiments conducted using both HP [U-¹³C]αKB and HP [1,2-¹³C]pyruvate.

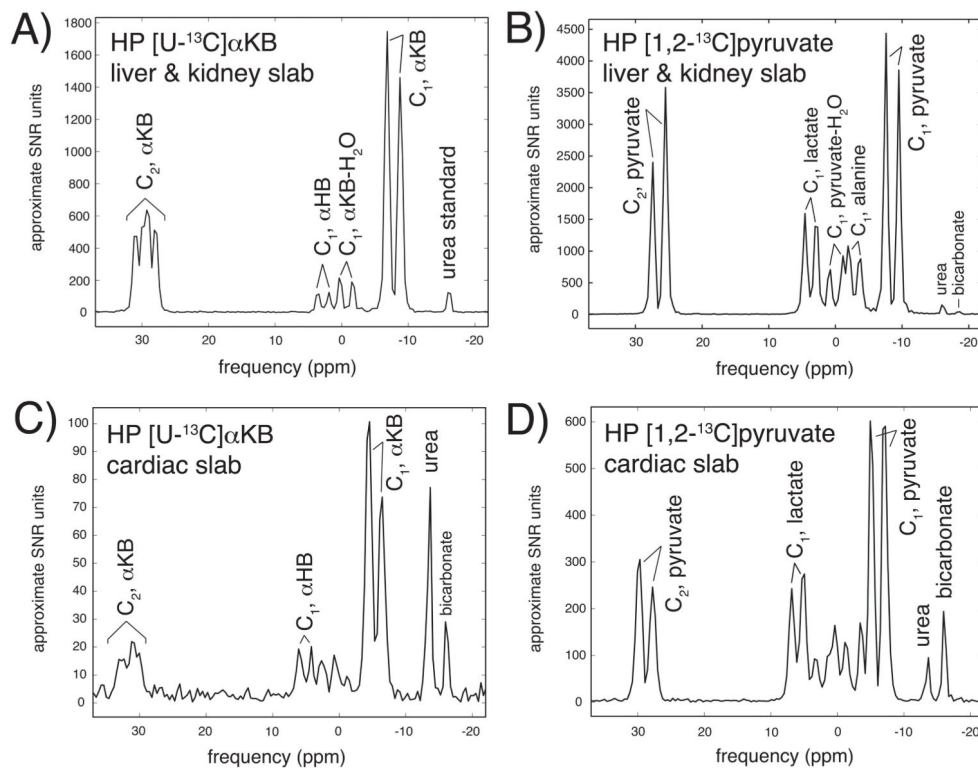


Figure 4. Slab-localized ^{13}C spectra (summed over acquisition) obtained after infusion of HP [$U\text{-}^{13}\text{C}$]αKB (A,C) and HP [$1,2\text{-}^{13}\text{C}$]pyruvate (B,D), in liver / kidney slab (A,B) and cardiac slab (C,D). NMR signal is scaled to approximate SNR level, and frequency is referenced to slab center frequency (i.e. ~ 178 ppm in absolute units).

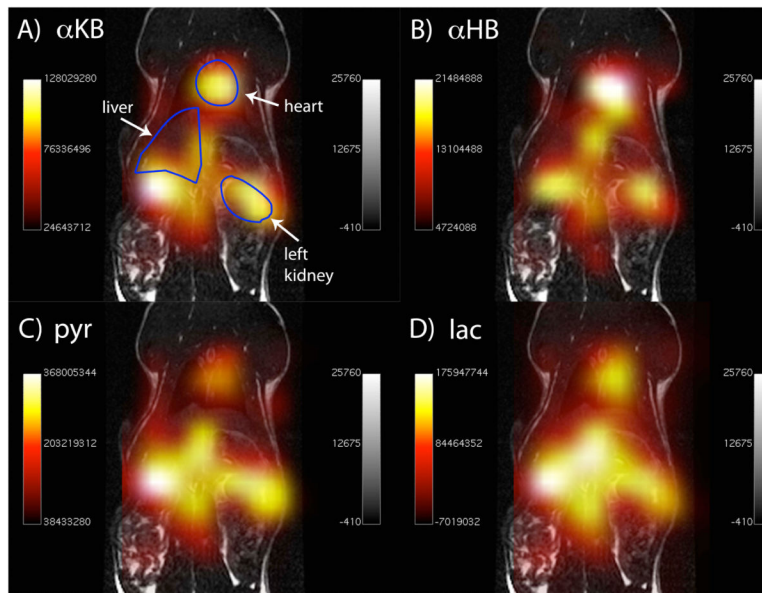


Figure 5. Spectroscopic images (coronal projection) of injected HP ^{13}C αKB (A) and product ^{13}C αHB (B), in comparison with images of injected HP ^{13}C pyruvate (C) and product ^{13}C lactate (D). ^{13}C metabolite images are overlaid in color on anatomic ^1H images shown in grayscale.

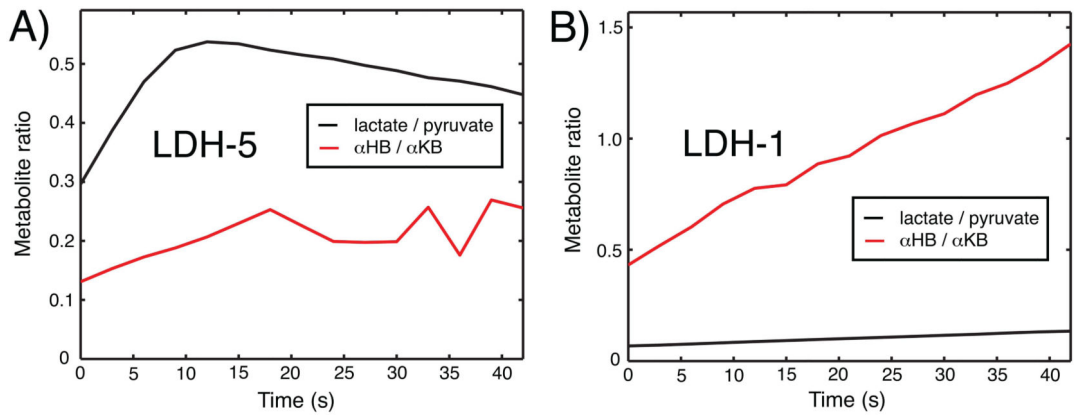


Figure 6. *In vitro* activity of HP α KB (red lines) and HP pyruvate (black lines) with LDH-5 (A) and LDH-1 (B) isoforms, measured by dynamic ^{13}C MR with experimental conditions described in text.