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# Aspirin Has Limited Ability to Modulate Shear-Mediated Platelet Activation Associated with Elevated Shear Stress of Ventricular Assist Devices

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# Abstract

Continuous flow ventricular assist devices (cfVADs) while effective in advanced heart failure, remain plagued by thrombosis related to abnormal flows and elevated shear stress. To limit cfVAD thrombosis, patients utilize complex anti-thrombotic regimens built upon a foundation of aspirin (ASA). While much data exists on ASA as a modulator of biochemically-mediated platelet activation, limited data exists as to the efficacy of ASA as a means of limiting shear-mediated platelet activation, particularly under elevated shear stress common within cfVADs. We investigated the ability of ASA (20, 25 and 125  $\mu$ M) to limit shear-mediated platelet activation under conditions of: 1) constant shear stress (30 dyne/cm<sup>2</sup> and 70 dyne/cm<sup>2</sup>); 2) dynamic shear stress, and 3) initial high shear exposure (70 dyne/cm<sup>2</sup>) followed by low shear exposure – i.e. a platelet sensitization protocol, utilizing a hemodynamic shearing device providing uniform shear stress *in vitro*. The efficacy of ASA to limit platelet activation mediated via passage through a clinical cfVAD system (DeBakey Micromed) *in vitro* was also studied. ASA reduced platelet activation only under conditions of low shear stress (38% reduction compared to control, n = 10, *p* < 0.004), with minimal protection at higher shear stress and under dynamic conditions (n = 10, p > 0.5) with no limitation of platelet sensitization. ASA had limited ability (25.6% reduction in

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platelet activation rate) to modulate shear-mediated platelet activation induced via cfVAD passage. These findings, while performed under "deconstructed" non-clinical conditions by utilizing purified platelets alone *in vitro*, provide a potential contributory mechanistic explanation for the persistent thrombosis rates experienced clinically in cfVAD patients despite ASA therapy. An opportunity exists to develop enhanced pharmacologic strategies to limit shear-mediated platelet activation at elevated shear levels associated with mechanical circulatory support devices.

### Keywords

aspirin; thrombosis; platelets; shear; ventricular assist devices; mechanical circulatory support

# Introduction

Mechanical circulatory support (MCS) devices have emerged as vital life-saving therapeutic systems for failing patients with advanced and end-stage heart failure (1). Despite their efficacy, MCS systems remain limited by post-implantation thrombotic complications (2). Continuous flow Ventricular Assist Devices (cfVADs), in particular, are plagued by intradevice thrombus buildup, reduced pump output with recurrent heart failure, and thromboembolic events- e.g. stroke, pump stop, and potential death (3). The high incidence of thromboembolic events in cfVADs is largely due to non-physiological flows within these devices, where platelets, the principal cellular clotting elements in blood, are exposed to extremely elevated shear stresses. In an attempt to limit MCS thrombosis, patients are burdened with complex, life-long anti-thrombotic pharmacologic regimens (4). The foundation of all regimens employed today is Aspirin (5).

Aspirin, i.e. acetylsalicylic acid (ASA), has been utilized for over sixty years as a clinical antithrombotic agent (6), with initial use described by Craven (7). ASA has been shown to inhibit platelet function by permanently acetylating cyclooxygenase (COX), both COX-1 and COX-2 isoforms, responsible for prostaglandin and thromboxane synthesis (8, 9). Over the years, ASA has been increasingly employed as a vital agent in limiting intra-arterial thrombosis related to atherosclerotic coronary disease, acute coronary syndromes, vulnerable plaque, carotid artery disease and intra-arterial stent use (8, 10–13). While all of these conditions impart shear stress to platelets, the intensity of stress, the time of exposure to stress, and the number of platelets exposed is significantly less than the stress accumulation (total dose of shear stress and exposure time) experienced by platelets exposed to cfVADs. Furthermore, the increase in stress accumulation is generally linked with an increase in platelet activation (14, 15).

In the present study we hypothesized that ASA, while an effective antiplatelet agent targeting a biochemical, i.e. thromboxane  $A_2$  pathway of platelet activation, will have limited efficacy as an agent modulating shear-mediated platelet activation, particularly at significantly elevated or "hyper-shear" levels common in VADs. As such, utilizing gelfiltered platelets, we first examined the efficacy of ASA to modulate shear-mediated platelet activation *in vitro* – examining exposure to both constant and dynamic shear stress, extracted from platelet flight trajectories obtained from a clinical VAD (16, 17). Secondly, we

examined the ability of ASA to modulate shear-mediated "sensitization," i.e. continued platelet activation over time following initial rapid shear exposure – a phenomenon described previously by our group (18). Finally, we examined the efficacy of ASA to limit VAD-mediated platelet activation *in vitro*, utilizing platelets obtained from normal human volunteers following *in vivo* aspirin ingestion and exposure.

### Materials and Methods

#### Platelet preparation

Whole blood (30 ml) was drawn via venipuncture into 3 ml acid-citrate dextrose (ACD-A) from consenting healthy adult volunteers of both sexes who had not taken aspirin or ibuprofen for two weeks, in accordance with a University of Arizona IRB-approved protocol. Whole blood was centrifuged at 500g for 15 min to obtain platelet-rich plasma (PRP), which was filtered through a column of Sepharose 2B beads (Sigma-Aldrich, St. Louis, MO, USA) to collect gel-filtered platelets (GFP) (18, 19). GFP were diluted to a count of 20,000/µl in HEPES-modified Tyrode's buffer, with 3 mM CaCl<sub>2</sub> added 10 min prior to experiments (18, 20).

#### Exposure of gel-filtered platelets to Aspirin

Platelets were treated with ASA dissolved in sodium bicarbonate solution (324 mg ASA, 965 mg citric acid, and 1744 mg sodium hydrogen carbonate in 50 ml double-distilled  $H_2O$ ), diluted to 20, 25 or 125  $\mu$ M final concentration, and incubated at 37°C for ten min. prior to shear exposure. For each ASA-treated platelet sample, a paired control experiment with platelets exposed to solvent vehicle alone (control) was performed on the same day. To verify the consistent reactivity of ASA, GFP were pre-incubated with ASA (125  $\mu$ M) and then treated with Arachidonic Acid (AA, 25  $\mu$ M). Samples for platelet activation measurements were taken at 0, 10 and 30 min.

#### Exposure of Aspirin-treated platelets to constant and dynamic shear stress

Platelets were exposed to shear stress in the Hemodynamic Shearing Device (HSD), a computer-controlled cone-plate-Couette viscometer that replicates dynamic shear conditions found in blood recirculating devices (14, 15, 21). GFP were pre-treated with ASA (25 or 125  $\mu$ M) ten min prior to shear exposure, which included either constant or dynamic conditions. In the constant shear stress experiments, platelets were exposed to 30 dyne/cm<sup>2</sup> or 70 dyne/cm<sup>2</sup> for a total exposure time of 10 min, with samples taken at 0, 2, 5 and 10 min (Figure 1a). At each time point, the HSD was slowed down to 1 dyne/cm<sup>2</sup> for 30 s for sampling. For the dynamic experiments, the waveforms utilized were extracted from the probability density function (PDF) of the shear stress conditions found in the DeBakey VAD (16). This function describes the stress accumulation, or product of shear stress and exposure time, experienced by the platelets and is calculated along thousands of simulated platelet trajectories (16). The PDF represents the device thrombogenicity "footprint" and highlights potential thrombotic "hotspot" trajectories. For the purpose of the study, we exposed platelets to waveforms corresponding to the 30<sup>th</sup> and 50<sup>th</sup> percentiles of the PDF (Figure 1b). The magnitude of the waveforms was scaled by a factor of 52.5 due to the limitation of the HSD (maximum shear stress of 108 dyne/cm<sup>2</sup> at 1 cP). Shear stress exposure was repeated

at 110 passages per min for 10 min. Platelets were sampled at 0, 2, 5 and 10 min. Platelet activation was measured as detailed below.

#### Shear-induced sensitization of in vitro aspirin-treated platelets

GFP, prepared as above, were pre-treated with 20  $\mu$ M ASA 10 min prior to shear experiments. Control GFP were prepared with the addition of the solvent vehicle alone 10 min prior to exposure. Both forms of GFP were then exposed to shear stress in the HSD. Platelets were sheared at 70 dyne/cm<sup>2</sup> for 40 s, followed by a subsequent low shear period of 1 dyne/cm<sup>2</sup>, for a total experimental duration of 15 min. Exposure to 1 dyne/cm<sup>2</sup> for 15 min served as the negative shear control. Samples for activation measurements were taken at time 0, 40 s, 3 min, and every 3 min thereafter.

#### In vitro flow loop study with platelets pre-treated with ASA in vivo

Healthy adult volunteers were utilized for this study after providing informed consent in accordance with a Stony Brook University IRB-approved protocol (22). Whole blood, 30 ml, was obtained from all subjects as a baseline. Subjects then ingested 1000 mg buffered ASA (two 500 mg Ascriptin tablets, Novartis, East Hanover, NJ) and returned 2 h later for a second 30 ml blood donation. GFP were isolated from both samples as described above and diluted to a count of 15,000/µl in HEPES-modified Tyrode's buffer with 5 mM Ca<sup>++</sup> added 10 min prior to experiments. The platelet mixture, 120 ml, was then exposed to shear stress via circulation through an *in vitro* flow loop for 30 min at 37°C. The circuit included a DeBakey VAD (MicroMed Cardiovascular Inc., Houston, TX, USA), with the inlet and outlets connected via a short 0.5″ I.D. Tygon R3603 loop tubing and a 0.25″ I.D. Tygon R3603 flow resistor tubing of 47″ length. The VAD was operated at 4L/min and 9500 rpm, corresponding to a pressure rise of ~70 – 80 mmHg across the pump (16). Platelet samples were then taken via a silicone sampling port downstream of the VAD at 0, 10, 20, and 30 min for measurement of platelet activation.

#### Platelet activation measurement

Platelet activation state (PAS) was measured using a modified prothrombinase based assay (23) which is routine in our laboratory and correlates strongly with P-selectin expression, as quantified with flow cytometry (24) as well as with phosphatidylserine expression (FITC-Annexin V) (25). Briefly, this technique employs acetylated prothrombin to determine the rate of thrombin generation. The use of acetylated prothrombin blocks the feedback action of generated thrombin on platelets, ensuring linear kinetics during the assay and quantitative measurement of PAS (23). PAS values were normalized against fully activated platelets obtained by sonication (10 W for 10 s, Branson Sonifier 150 with microprobe, Branson, MO) (18, 19, 22). PAS values are therefore expressed as a fraction of the maximal thrombin-generating capacity, with a maximum value of 1.0.

#### **Statistical Analysis**

Prior to statistical analyses, the Shapiro-Wilk normality test was run for all data populations. For the constant and dynamic shear stress experiments, we calculated the differences in PAS between 0 and 10 min, PAS, which was compared between ASA-treated platelets and

control. The Platelet Activation Rate (PAR) for each experiment was obtained from the slopes of lines fit to normalized PAS values. For the *in vivo* ASA treatment, differences in PAR were obtained by subtracting the PAR calculated for ASA-treated platelet experiments from PAR obtained for paired control experiments. The percentage change in the PAR was calculated by dividing this difference by the control PAR and multiplying by 100. Parametric or non-parametric (Kruskal-Wallis) one-way ANOVA was performed, depending on the normality of the data, with Tukey's *post hoc* test used to compare the PAR for the different groups tested. Paired samples Student's t-tests were used to compare the ASA-treated and control PAR values for each set of VAD experiments, while differences between the PAR for control and ASA-treated experiment were compared to a value of 0, which represents the condition where PAR for ASA-treated and untreated platelets are identical. Significance was achieved for *p* < 0.05. Results are presented as the mean ± standard error of the mean (S.E.M.), unless otherwise stated.

# Results

As a first step we examined the ability of the PAS assay to detect platelet activation via arachidonic acid (AA) and inhibition of activation via addition of ASA – i.e. biochemical activation and inhibition of activation. We selected this as our starting point as the PAS assay has largely been utilized for quantifying shear-mediated activation (14, 18, 25). AA-treated platelets revealed a clear increase in PAS between 0 and 10 min (Figure 2). In contrast, ASA-pretreated platelets demonstrated inhibition of activation. Both mean PAS (0.12 vs 0.04, p < 0.01) and PAR between 0 and 10 min (Table 1) demonstrated the protective effect and maintenance of the inhibitory effect of ASA after 10 min of incubation with AA. These results served to establish as a baseline the efficacy of the PAS assay for examining the effect of ASA in the outlined shear studies of this investigation.

#### Effect of Aspirin in Modulating Shear-Mediated Platelet Activation In Vitro

We then investigated the effect of constant shear stress on platelets pre-treated with 25 and 125 µM ASA. These ASA concentrations correspond to clinical use dosages of 81 mg/day or 325 mg/day, respectively (4). For constant shear conditions, a significant reduction in the PAS after 10 min (Table 2) was observed for 30 dyne/cm<sup>2</sup> exposure for both ASA concentrations when compared to control (Figure 3a, n = 10, p < 0.004). This corresponds to a 31.8% and 45.4% reduction in PAS after 25 and 125 µM ASA pre-treatment, respectively. However, no significant reduction was observed for the 70 dyne/cm<sup>2</sup> condition (Table 2, Figure 3b, n = 10, p > 0.1). Similarly, platelets treated with 125  $\mu$ M ASA and exposed to the 30<sup>th</sup> percentile DeBakey VAD waveform showed a 35.2% reduction in PAS compared to untreated platelets (Table 2, Figure 4a, n = 10, p < 0.05), However, 25  $\mu$ M ASA-treated platelets showed no significant reduction compared to the control at 30<sup>th</sup> percentile shear stress waveform exposure (Figure 4a, n = 10, p > 0.5). Furthermore, ASA treatment had no effect on platelets exposed to the 50<sup>th</sup> percentile shear stress waveform (Table 2, Figure 4b, n = 10, p > 0.5). We also observed that platelets exposed to either the 30 dyne/cm<sup>2</sup> constant shear stress condition or the 30<sup>th</sup> percentile dynamic VAD waveform showed a convex PAS behavior with respect to exposure time, whereas concave behavior

was observed for the 70 dyne/cm<sup>2</sup> constant shear condition and  $50^{\text{th}}$  percentile dynamic VAD waveform condition.

#### Effect of Aspirin in Modulating Shear-Induced Platelet Sensitization

We evaluated whether *in vitro* treatment with ASA modulated shear-induced platelet sensitization, or the priming of platelets for further activation subsequent to high shear stress exposure.(18) Platelets exposed to 70 dyne/cm<sup>2</sup> for 40 s, followed by 1 dyne/cm<sup>2</sup> showed a significant increase in the subsequent PAR during this follow-on exposure when compared to platelets only exposed to 1 dyne/cm<sup>2</sup> for a similar time period (Figure 5, n = 10, p < 0.01). However, treatment with 20  $\mu$ M ASA yielded a non-significant PAR reduction of 9.4% and 15.7% after 70 dyne/cm<sup>2</sup> and 1 dyne/cm<sup>2</sup> pre-exposure, respectively (Figure 5b, n = 10, p >0.5). This indicates that 20  $\mu$ M ASA does not significantly attenuate shear-induced platelet sensitization after exposure to constant pathological shear stress.

# Effect of Aspirin in Modulating VAD-mediated (Elevated Shear) in Vitro

*In vivo* ASA treated-platelets (1000 mg ASA loading dose), sampled 2h after ASA ingestion, showed only a  $0.46 \pm 0.14$  (×  $10^{-4}$ ) min<sup>-1</sup>, or 25.6%, reduction in PAR following exposure to shear imparted by a clinical VAD when compared with paired control experiments (Figure 6, n = 7, p < 0.001). This reduction in platelet activation was observed to be 3-fold less than that achieved in prior work by our group through design optimization of the original DeBakey VAD (16).

# Discussion

The overall goal of the present study was to examine the ability of ASA - a traditional antithrombotic and anti-platelet agent, operating via biochemical pathway inhibition, to limit shear-mediated platelet activation. In the present study, we utilized a "deconstructionist strategy," - i.e. utilizing pure, gel-filtered platelets, to examine the efficacy of ASA to limit shear-mediated platelet activation under conditions devoid of other potentially prothrombotic blood constituents. Further, we utilized the HSD – affording exact control of the shear exposure history – to examine the effects of both constant and dynamic shear. As such, we demonstrate that ASA has a dichotomous effect with regard to its ability to limit shearmediated platelet activation. At the low shear stress levels tested, i.e. 30 dynes/cm<sup>2</sup> constant shear stress or 30th percentile of the PDF (stress accumulation of 1.25 dyne-s/cm<sup>2</sup> per 545 ms passage (dynamic shear stress)). ASA demonstrated a clear ability to limit shearmediated activation. In contrast at elevated shear levels tested, i.e. 70 dynes/cm<sup>2</sup> constant shear stress or 50th percentile of the PDF (stress accumulation of 2.94 dyne-s/cm<sup>2</sup> per 545 ms passage (dynamic shear stress)), ASA was unable to limit shear-mediated platelet activation. Furthermore, ASA did not significantly reduce platelet sensitization - i.e. subsequent activation following an initial high shear exposure. Finally, ASA had limited ability to prevent shear-mediated platelet activation for platelets subjected to elevated shear via cyclic passage through a cfVAD operating under normal clinical conditions (speed, flow rate) in vitro.

#### Ability of Aspirin to Modulate Shear-Mediated Platelet Activation

There are few studies in the literature which have examined the ability of ASA to limit shear mediated-platelet activation (11, 22, 26–28). Konstantopoulos et al. utilized a simple cone and plate viscometer system to demonstrate that the platelet response to shear stress was insensitive to ASA, rather being limited by agents that elevated platelet cyclic AMP levels (29). In their study, shear stress profiles used were those of constant shear with a maximum shear stress level tested of 140 dynes/cm<sup>2</sup>. The present study extends these observations along two lines. Herein we have utilized dynamic shear stress exposure, in addition to constant shear stress, and demonstrated the limited efficacy of ASA in this more aggressive setting. Furthermore in the present study, we utilize actual hyper-shear levels as experienced clinically via utilization of a clinical VAD – the DeBakey VAD, with peak shear stress > 800 dynes/cm<sup>2</sup> (16). In this emulation of a clinical scenario, ASA offers no significant protective effect as to limitation of platelet activation.

ASA was also examined as to its ability to prevent shear-induced platelet aggregation mediated by ADP and vWF multimers (11). Here, the authors showed that shear-induced aggregation is mediated by either large plasma type vWF multimers, endogenous released platelet vWF forms, or unusually large vWF multimers derived from endothelial cells. Furthermore, they showed that aggregation requires ADP and is not inhibited significantly by ASA.

Due to its poor protective action on shear-mediated platelet aggregation, ASA has been used as control to prove the effectiveness of other more recent antiplatelet agents. In a study presented by Tsuchikane et al., 211 patients with 273 lesions who underwent successful percutaneous transluminal coronary angioplasty (PTCA) were randomly assigned to the cilostazol (200 mg/d) group or ASA (250 mg/d) control group (28). Cilostazol appeared to significantly reduce restenosis and target lesion revascularization rates after successful PTCA compared to ASA. More recently, an *in vitro* study conducted by Sheriff et al. compared the efficacy of ASA on platelets subjected to shear stress, proving that *in vitro* treatment with antiplatelet drugs such as ASA is as effective as *in vivo* metabolized ASA in testing the effect of reducing shear-induced platelet activation (22).

The advance afforded by the present study is the utilization of the HSD for shear stress exposure. In the HSD, shear exposure histories may be very finely regulated (15, 21, 30), with a dynamic response time of 4 ms and with defined control of shear stress magnitude (up to 108 dyne/cm<sup>2</sup> at 1 cP viscosity). Furthermore, the HSD uniformly exposes a small sample volume (2.5 ml) to shear stress waveforms extracted from computational fluid dynamics (CFD) simulations of cardiovascular devices, including mechanical heart valves (14, 31) and cfVADs. In addition, the HSD set-up allows real-time sampling to examine the evolution of PAS over time.

Two strategies of shear stress exposure were chosen for this study – constant (continuous) and dynamic shear stress. The logic of this approach was to first examine the inhibitory efficacy of ASA under a simple, constant stress and then to follow with examination of the effect of dynamic varying conditions, i.e. those experienced by platelets with actual flight trajectories derived from passage through a VAD. Under constant low level shear, i.e. that

within the normal physiological range experienced in the arterial vasculature (8 - 60)dynes/cm<sup>2</sup>) (32), ASA demonstrates some inhibition. Our results are consistent with studies that observed non-significant reduction in ASA-treated platelet aggregation after 30 s exposure to 30 and 60 dyne/ $cm^2$  in a cone-plate viscometer (11), and significant reduction in thrombus volume after 5 min exposure of canine blood to 56 dyne/cm<sup>2</sup> (1600 s<sup>-1</sup>) in a parallel-plate flow chamber (33). However, when shear stress exposure was elevated to levels experienced with cardiovascular pathologies, such as arterial stenosis, or at elevated shear regions within a cfVAD, ASA was unable to prevent shear-mediated platelet activation. This reflects prior observations with aggregation in cone-and-plate viscometers at 108 and 120 dyne/cm<sup>2</sup> (11, 34), collagen-induced thrombus formation above 80 dyne/cm<sup>2</sup> in a perfusion chamber (35), and collagen- or vWF-induced platelet adhesion at 50 dyne/cm<sup>2</sup> (36). Moreover, as with constant shear stress exposure, when platelets were exposed to pathologic dynamic shear stress levels, with net stress accumulation of 3235 dyne-s/cm<sup>2</sup> (10 min at 110 passages/min for 50<sup>th</sup> percentile waveform), ASA afforded no protection for shear-mediated activation. Inhibition of activation was only observed after pre-treatment with 125 uM for platelets exposed to a net stress accumulation of 1378 dyne-s/cm<sup>2</sup> (10 min at 110 passages/min for 30<sup>th</sup> percentile waveform).

#### Inability of Aspirin to Prevent Platelet Sensitization

We previously observed that platelets briefly exposed to elevated magnitudes of constant or dynamic shear stress, such as those found in cardiovascular devices or pathologies, continue to activate during subsequent low shear stress exposure (15, 18). This behavior, termed as shear-induced platelet sensitization, has been observed in purified platelets independent of coagulation factors typically present in plasma (18). In addition, sensitized platelets may activate quiescent platelets that have not been exposed to pathological conditions (18). In the present study, we observed that pre-treatment with 20 µM ASA yielded non-significant attenuation of this sensitization effect (Figure 5). Both ADP (released during the minimal lysis during the high shear stress phase) and microparticles generation were previously found to play a role in shear-induced platelet sensitization (18). While the effect of COX-1 pathway modulation on platelet sensitization is not yet understood, it has been shown that shear-induced platelet aggregation is significantly dependent on the presence of ADP, whereas ASA, and therefore COX-1 inhibition, has a minimal effect (11). Therefore, it appears that ASA pre-treatment is unlikely to inhibit the shear-induced sensitization response. This may partially explain why approximately 26% of VAD patients show aspirin resistance or persistent platelet activation despite antithrombotic therapy (37).

#### Efficacy of in vivo ASA in Limiting in vitro cfVAD Shear-mediated Platelet Activation

Our results overall demonstrate that subject-ingested *in vivo* ASA has limited ability to prevent and reduce shear-mediated platelet activation in our *in vitro* cfVAD loop model. In the present study we observed that treatment with maximum strength ASA (1000 mg, sampled 2h after ingestion) reduced the platelet activation rate by 25.6% after shear exposure with a DeBakey VAD. However, an earlier study by our group showed that 20 h after ASA ingestion, this reduction was all but absent (22). These results highlight the necessity of continuous monitoring and administration of ASA therapy to control the level of platelet activation under shear stress exposure. Unfortunately, this continuous administration

of drugs could lead to other complications, such as bleeding and hemorrhage (4, 5). This finding has clinical relevance as present mechanical circulatory support systems, i.e. cfVADs, rely primarily on ASA as the main antiplatelet agent of current clinical anti-thrombotic regimens, with warfarin providing anticoagulant effects (4, 5). While our studies are strictly *in vitro*, utilizing gel-filtered platelets alone rather than whole blood, and must be viewed within that context, they do suggest to the clinical community that relying on ASA alone as the clinical "insurance" to prevent shear-mediated platelet activation may be very limited. Further, these results highlight the impact of shear for situations such as a cfVAD with high degrees of platelet exposure, in contradistinction to an arterial stenosis. In the case of a VAD, the entire blood volume, with contained platelets, circulates through regions of high shear within a short exposure time. In contrast, for a high-grade isolated arterial stenosis, as is seen in coronary artery disease, only a small fraction of platelets within the blood volume are actually exposed to elevated shear.

#### Limitations of the Present Study

In the present study we utilized isolated gel-filtered platelets in order to examine the direct effect of fluid shear stress on platelet activation, and ASA potential to modulate this process. By using purified platelets instead of whole blood (WB), or platelet-rich plasma we neglect the contribution of red blood cells (RBCs), white cells and plasma proteins to the platelet activation process. In particular, RBCs have been shown to increase platelet diffusivity as a function of 1) shear rate and hematocrit through platelet margination and 2) shear rate through localized mixing and cell-cell collisions (38–42). In our experimental protocols, we assumed that platelet margination played a limited role during our tests (absence of RBCs) and that the platelet concentration used (20000 per  $\mu$ l) minimized platelet collisions and cross-talk. RBCs can also contribute to thrombosis and hemostasis by releasing substances that act as platelet agonists. In fact, when hemolysis occurs, RBCs mainly release hemoglobin, ADP and LDH in the blood plasma. These elements have variable and contributory effects on thrombosis and platelet activation (43).

Whole blood also includes plasma proteins that contribute to platelet activation. Some of the prothrombinase complex factors (factor Xa, Ca<sup>2+</sup>), which are normally present in blood plasma in their inactive form, play a key role in the platelet activation process by enhancing the conversion of prothrombin to thrombin. In our study, due to the absence of these factors in GFP, this mechanism of activation was not considered. Nonetheless, the absence of the positive feedback on platelet activation provided by prothrombinase complex factors was necessary for the correct performance of the PAS assay, and these factors were reintroduced during the assay. It is worth clarifying that the main goal of our work was not to study platelet behavior through replication of the biological environment present *in vivo*. Rather, our goal was to assess the effect of ASA on platelet activation by measuring its ability to protect platelets under a range of shear stress conditions. To this end, GFP was considered the best platelet preparation for the detection of activation using the PAS assay.

#### **Future perspectives**

In recent years, a combinational approach consisting of coupling low dose ASA with other antiplatelet agents has been introduced for the clinical management of VAD-patients (4).

Several research groups have begun evaluating the effect of ASA in combination with other drugs (8, 12, 13, 44–49). Nonetheless, the effectiveness of such combined therapeutic approaches after exposure to defined dynamic shear stress profiles has been poorly studied and defined. The results described herein provides a base upon which future studies examining the effects of combinational therapies may be examined. Further, future studies are planned to contrast the efficacy of ASA in limiting shear-mediated platelet activation in whole blood with that observed herein with GFP. Finally, our findings suggest that mechanotransduction of shear leading to platelet activation operates via mechanisms that are independent or insensitive to prostaglandin/thromboxane inhibition (50).

# Conclusions

The present study utilizing purified gel-filtered platelets demonstrates that ASA, a routine, basal component of clinical antithrombotic therapy for prevention of platelet activation in patients with a variety of cardiovascular pathologies, has limited efficacy at best in modulating shear-mediated platelet activation under flow conditions and shear levels existent in mechanical circulatory support devices such as cfVADs. Our study goes beyond what has been termed "aspirin resistance" (50) to demonstrate, in circumstances of supra-physiologic shear stress exposure and accumulation, a domain of "limited or lack" of ASA effect. ASA demonstrated only moderate efficacy under conditions of low shear and with no significant efficacy under high shear. Similarly, ASA was unable to limit platelet sensitization -i.e.subsequent activation following an initial high shear exposure. Finally, ASA had limited ability to prevent shear-mediated platelet activation for platelets subjected to elevated shear via cyclic passage through a cfVAD. While our study is performed under *in vitro* conditions, it provides potential mechanistic insight for the persistent thrombosis rates experienced clinically in cfVAD patients despite ASA therapy. Utilizing ASA with cfVADS remains the present clinical standard-of-care. However, our results reveal the need for future studies aimed at consideration of combinational drug strategies or new agents or means for limiting shear-mediated platelet activation under elevated "hyper-shear" conditions as experienced in patients with cfVADs with persistent thrombotic risk.

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# Highlights

- ASA has limited efficacy in modulating high shear-mediated platelet activation (SMPA)
- ASA is unable to limit shear-mediated platelet sensitization
- ASA has limited efficacy in modulating SMPA for shear associated with cfVADs
- Need exists for strategies to modulate SMPA with "hypershear" (600–1000 dynes/cm<sup>2</sup>)



# Figure 1. Constant and dynamic shear stress waveforms

Gel-filtered platelets (GFP) were exposed to **a**) variable magnitudes of constant shear stress for variable durations and **b**) dynamic shear stress waveforms representing a single exposure in the DeBakey VAD.



Figure 2. The effect of ASA on platelets exposed to arachidonic acid (AA) a) Platelet activation in time after treatment with AA alone (black), ASA and then AA (gray) or ASA alone (white). b) Platelet activation rate (PAR) after 10 min in the same conditions as a) (n = 4, \*p < 0.01).



Figure 3. The effect of ASA on constant shear-mediated platelet activation The effect of ASA (25 or 125  $\mu$ M) was investigated after exposure to **a**) 30 dyne/cm<sup>2</sup> and **b**) 70 dyne/cm<sup>2</sup> (n = 10).



Figure 4. The effect of ASA on dynamic shear-mediated platelet activation The effect of ASA (25 or 125  $\mu$ M) was investigated after exposure to the dynamic waveforms extracted from simulation in the DeBakey VAD corresponding to the **a**) 30<sup>th</sup> (Dynamic\_30%) and **b**) 50<sup>th</sup> percentile (Dynamic\_50%) of the PDF function (n=10).



### Figure 5. Platelet sensitization after in vitro ASA treatment

**a)** For both 20  $\mu$ M ASA-treated and control platelets, PAS was measured after initial 40 s exposure to 70 dyne/cm<sup>2</sup>, and during subsequent exposure 1 dyne/cm<sup>2</sup>. **b**) Sensitization PAR rates for ASA-treated and control platelets were calculated from PAS values subsequent to 70 dyne/cm<sup>2</sup> and 1 dyne/cm<sup>2</sup> pre-exposure (n = 10, \**p* < 0.01).



**Figure 6.** Platelet activation in DeBakey VAD 2h post-*in vivo* ASA treatment a) PAS was measured for 1000 mg ASA-treated platelets and untreated platelets recirculated for 30 min through the VAD, with b) PAR determined from the slope of lines fit to PAS values (n = 7, p < 0.001).

 Table 1

 Platelet Activity Rate (PAR) after static exposure to aspirin (ASA) and arachidonic acid (AA)

Mean PAR values were obtained from the slope of lines fit to PAS values for the first 10 min of platelet exposure to ASA and AA.

Experimental conditions	PAR, 0–10 min (×10 <sup>-4</sup> min <sup>-1</sup> )	<i>p</i> vs. 25 μM AA
25 µM AA	$57\pm16$	-
$25 \ \mu M \ AA + 125 \ \mu M \ ASA$	$5.5 \pm 7.4$	0.001
125 μM ASA	$1.1 \pm 1.6$	0.004

#### Table 2

# Mean normalized PAS for control and ASA-treated platelets subjected to different shear stress profiles

Mean PAS values were calculated from the difference in PAS between the 0 and 10 min samples obtained from the HSD.

Experimental conditions	Normalized	PAS, 0 – 10 min	p vs. control
a) 30 dyne/cm <sup>2</sup>			
control	$0.44\pm0.03$		-
25 µM ASA	$0.30\pm0.03$		< 0.001
125 µM ASA	$0.24\pm0.04$		0.004
b) 70 dyne/cm <sup>2</sup>			
control	$0.83\pm0.02$		-
25 µM ASA	$0.89\pm0.02$		0.12
125 µM ASA	$0.77\pm0.05$		0.43
c) Dynamic_30%			
control	$0.54\pm0.04$		-
25 µM ASA	$0.54\pm0.05$		0.94
125 µM ASA	$0.35\pm0.04$		0.002
d) Dynamic_50%			
control	$0.82\pm0.04$		-
25 µM ASA	$0.87\pm0.03$		0.29
125 µM ASA	$0.73\pm0.04$		0.15

#### Table 3

#### Summary.

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#### What is known on this topic

- ASA is the primary antithrombotic drug for patients with cfVADs
  - Pathological shear stress is the primary activator of platelets in cfVADs
- ASA efficacy has been studied under static, low, high and non-physiological flow conditions, however its efficacy under dynamic, device-related conditions is poorly understood.

#### What this paper adds

- ASA has limited efficacy in modulating shear-mediated platelet activation under both constant and dynamic levels of elevated shear stress and overall shear stress accumulation experienced in cfVADs
- ASA is unable to limit shear-mediated platelet sensitization, or continued activation after brief high shear stress exposure
- A clear need exists for the development of strategies of agents able to modulate shear-mediated platelet activation associated with the "hypershear" levels (600–1000 dyns/cm<sup>2</sup>) associated with mechanical circulatory support devices such as cfVADs